

RESEARCH

Open Access



Oral solid self-nanoemulsifying drug delivery systems of candesartan cilexetil: formulation, characterization and in vitro drug release studies

Halah Hussein Ali* and Ahmed Abbas Hussein

Abstract

Candesartan cilexetil is an ester prodrug antagonist to angiotensin II receptor type 1 (AT1) used in management of many cardiovascular diseases. The absolute bioavailability of candesartan cilexetil is about (14–40%). Therefore, the paper aim was to prepare and evaluate solid self-nanoemulsifying drug delivery systems for candesartan cilexetil in order to improve its solubility, dissolution and stability. Solubility study was run in different vehicles to select the best excipients for dissolving candesartan cilexetil. Pseudo-ternary phase diagrams were constructed at 1:1, 2:1, 3:1 and 4:1 ratios and four formulations were prepared using various concentrations of cinnamon oil, tween 80 with poloxamer 407 mixture and transcutool HP as oil, surfactant mixture and co-surfactant, respectively. After this step about (0.2 milliliter) of each formulation was adsorbed on to two different adsorbent mixtures set which were: avicel 101 with aerosil 200 and avicel 101 with dibasic calcium phosphate anhydrous resulted in eight solid nanoformulations. All prepared formulations were evaluated for particle size distribution, polydispersity index, zeta potential, scanning probe microscopy, Fourier transform infrared spectroscopy, differential scanning calorimetry, X-ray powder diffractometry and in vitro drug dissolution. It was found that release rate and extent for all prepared formulations were significantly higher ($p < 0.05$) than marketed tablet as well as plain drug powder. It could be concluded from the study that self-nanoemulsifying drug delivery system is a promising approach to improve solubility, wettability, dissolution and stability of candesartan cilexetil.

Keywords: Candesartan cilexetil, Solubility, Pseudo-ternary phase diagram, Adsorbent mixture, Self-nanoemulsifying drug delivery system, Stability

Background

Two key steps that affect oral bioavailability of drugs are dissolution and gastrointestinal permeation. These two parameters are dictated by the intrinsic physicochemical properties of the drug, i.e., its aqueous solubility and lipophilicity (Jane et al. 2006). The aqueous solubility of the drug in question is a crucial factor because only drug in solution is destined for possible absorption. Dissolution of drug is largely determined by the aqueous solubility of drug, since a drug must be in solution to exert its beneficial effect (Patel et al. 2012). Good drug candidates should have high solubility and high lipophilicity. Unfortunately,

lipophilicity also translates into high hydrophobicity and poor aqueous solubility (Rahman et al. 2011).

Nanotechnology world opens the field of delivering many of therapeutic agents in such a cell-specific manner with a maximum intrinsic activity of drugs. Therefore, to increase drug's efficacy while decreasing their toxic side effects, it has been projected to encapsulate the drug in a nanocarrier (Fathi et al. 2012). Delivery thereby limiting off-target access, improving the bioavailability of poorly soluble drugs and enhancing intracellular delivery (Maravajhala et al. 2012).

Cardiovascular diseases include arterial diseases affecting the blood supply to the heart or to the brain, or to the peripheral regions of the body (Frayn 2005). Thiazide Diuretics, angiotensin converting enzyme inhibitors (ACE

* Correspondence: halahpharma@yahoo.com
Department of Pharmaceutics, College of Pharmacy, Baghdad University, Baghdad, Iraq

inhibitors), AT1 antagonists, β -blockers and calcium antagonists are drugs of first choice aim to prevent organ damage and reduce mortality rate (Bieger et al. 2005). Since it is a chronic disease, it necessitates long term treatment, but most of antihypertensive drugs available today showed extensive first pass metabolism, variable bioavailability and more frequent times of administration make them an ideal candidate for solid self-nanoemulsifying drug delivery (SSNEDDS) (Muhamad et al. 2014).

Self-nanoemulsifying drug delivery system (SNEDDS) is thermodynamically stable isotropic mixed bag of anhydrous nanoemulsion (NE) which when poured to the aqueous medium under gentle agitation, will self-emulsify to yield either oil-in-water (o/w) or water-in-oil (w/o) NE usually with globule size less than 200 nm stabilized by the interfacial film of surfactant/co-surfactant mixture (Smix) (Elgadira and Adam 2014; Soni et al. 2014; Dey et al. 2012). This type of delivery system is expected to improve drug solubility and bioavailability by virtue of their high solubilization and permeation attributes suited for poorly soluble and slowly absorbable drugs (Wadhwa et al. 2012). Indeed, these systems can be converted into solid intermediates by various methods and then filled into capsules or compressed into tablets after mixing with proper tableting excipients (Kalepun et al. 2013).

Candesartan cilexetil (CC) is an ester prodrug antagonist to AT1 receptors used in management of hypertension, heart failure, myocardial infarction and diabetic nephropathy (Sweetman 2009; Kolesar and Vermeulen 2016). It is practically insoluble in water with log P 7.43 and belonging to class II according to biopharmaceutical classification system (BCS) (Darwhekar et al. 2012; Beale et al. 2010). Following oral administration, CC undergoes hydrolysis at the ester linkage to form the active drug, candesartan with absolute bioavailability for candesartan is about 40% when CC is given as a solution and about 14% when given as tablets. Peak plasma concentrations of candesartan occur about 3 to 4 hours (h) after oral doses as tablets (Moffat et al. 2011). Candesartan is more than 99% bound to plasma proteins. It is excreted in urine and bile mainly as unchanged drug and a small amount of inactive metabolites with a terminal elimination half-life of about 9 h (Husain et al. 2011).

The aim of this research was to design and evaluate different formulations of SSNEDDS using various Smix ratios and adsorbent mixtures in order to achieve an enhancement in CC solubility, wettability, dissolution

and stability for better delivery of CC through oral cavity to confront problems associated with chronic cardiovascular diseases old dosage forms.

Materials and Methods

Materials

Candesartan cilexetil, poloxamer 188, poloxamer 407 and, poloxamer 338 were purchased from Shenzhen Nexconn PharmaTechs, LTD. (China). Cinnamon oil was brought from Now food (USA). Tween 80 was purchased from Pure chemistry (Germany). Transcutol HP was purchased from Gattefosse Corporation (USA). Microcrystalline cellulose pH 101(Avicel 101) was provided by Fluka analytical (Ireland). Colloidal silicon dioxide (Aerosil 200) was bought from Hyper-Chem LTD Co. (china). Dibasic calcium phosphate anhydrous was purchased from HiMedia Lab Pvt. LTD (India). All other chemicals used were of analytical grade.

Methods

Construction of pseudo-ternary phase diagrams

Pseudo-ternary phase diagrams of oil, Smix and water were constructed using aqueous titration method. Ratios were chosen in increasing the concentration of surfactant with respect to co-surfactant in 1:1, 2:1, 3:1 and 4:1 ratios. Boundaries of phase diagrams designated the system's three components; one axis representing the aqueous phase, the second for the oil, and the third representing the Smix (Selvam et al. 2013).

Preparation of candesartan cilexetil liquid self-nanoemulsifying drug delivery systems

Four self-nanoemulsifying liquid formulations of CC were prepared using tween 80 with poloxamer 407 mixture and transcutol HP at Smix ratios (1:1, 2:1, 3:1 and 4:1) keeping oil: Smix at 1:9 ratio as presented in (Table 1). Preparation includes dissolving CC in cinnamon oil, mixing with other components at the concentration of (8 milligram (mg) of CC/0.2 milliliter (ml) of SSNEDDS) in screw-capped glass vials. The vials were then sealed and placed in a water bath at (50–60 °C) to facilitate homogenization. The components were mixed by vortex mixer (Labinco L46, CAT.NO.46000, Netherland) for 5 minute (min) to obtain clear uniform mixtures and again cooled to room temperature followed by equilibrating the mixture on a sonicator (VWR ultrasonic

Table 1 Composition of candesartan cilexetil liquid self-nanoemulsifying drug delivery systems (% w/w)

F-code	Smix ratio	Oil:Smix	Cinnamon oil %	Tween 80%	Poloxamer 407%	Transcutol HP %
SNEDDS-1	1:1	1:9	10	36.0	9.0	45.0
SNEDDS-2	2:1	1:9	10	48.0	12.0	30.0
SNEDDS-3	3:1	1:9	10	54.0	13.5	22.5
SNEDDS-4	4:1	1:9	10	57.6	14.4	18.0

cleaner, USC200T model, Copley scientific, U.K.) at room temperature for 10 min, after that the formulations were kept under visual observation for at least 48 h and examined for any signs of turbidity or phase separation prior to particle size distribution studies (Prajapati et al. 2013).

Evaluations of the prepared candesartan cilexetil liquid self-nanoemulsifying drug delivery systems

Thermodynamic stability studies

All of the self-nanoemulsifying liquid formulations were subjected to centrifugation test at 3500 revolutions per minute (rpm) for 30 min. These formulations that keep their clarity were engaged in heating/cooling cycles test with storage time period for about 48 h at 45 °C and 4 °C, respectively. Lastly, freezing/thawing cycles test was achieved via storing each prepared formula at -21 °C and +25 °C for two days at each temperature. All thermodynamically stable formulations were taken for further tests (Kumar et al. 2009; Sureshkumar et al. 2015).

Determination of particle size distribution and polydispersity index value

The mean particle size distribution and the polydispersity index of the selected liquid SNEDDS formulations were performed by laser particle size analyzer instrument (Brookhaven Corp 90 Plus, NY, USA) at 25 °C with an angle of detection of 90° (Tiwari and Amiji 2006).

Measurement of surface charge

To predict the stability of NE pre-concentrate, the electronic charge of particles in liquid SNEDDS was verified using zeta plus instrument (Brookhaven Zeta Plus, Holtsville, NY 11742-1832, USA). Particles with zeta potentials above 30 millivolt (mV) irrespective of their charge are normally considered stable (Gupta et al. 2011).

Determination of self-emulsification efficiency of surfactant mixture and co-surfactant

Surfactant mixture (tween 80 with poloxamer 407 mixture at 4:1 ratio) and co-surfactant (transcutol HP) were screened for their cinnamon oil emulsification ability. Surfactant emulsification efficiency was done on the basis of percentage transparency and ease of emulsification judged by the number of flask inversions required to yield a homogenous NE. Briefly, 300 mg of the surfactant mixture was added to 300 mg of cinnamon oil. The mixtures were gently heated at 50 °C for homogenization of components. From each mixture, 50 mg was then diluted with deionized water to 50 ml in a stoppered conical flask (Yasser et al. 2013).

Formed mixtures were allowed to stand for 2 h and their percentage transparency was evaluated at 650 nm by Ultraviolet/Visible (UV/Vis) spectrophotometer (UV-6100 PC, EMC lab, Germany) using deionized water as a

blank. The resulted combinations were further observed visually for any turbidity or phase separation. Screening of co-surfactant was conducted via preparing a mixture of 100 mg of the co-surfactant, 200 mg of the selected surfactant mixture and 300 mg of the selected oil and evaluated in the same way as the surfactant mixture (Yasser et al. 2013).

Determination of self-nanoemulsification time

The emulsification times of prepared CC SNEDDSs were determined using united state pharmacopeia (USP) type II dissolution apparatus (UV-6100 PC, EMC lab, Germany). About (0.2 ml) quantity of each formulation was added to 900 ml of 0.1 normal "N" HCl (pH 1.2) at 37 °C. The formed mixtures were gently stirred at 50 rpm and visually monitored (i.e., until a transparent homogenous system was seen) to determine the time (min) for complete nanoemulsification according to the visual observation criteria for self NE formation listed in (Table 2). The upper limit for formation of good (transparent) NE was set as one min, since when nanoemulsification occurs slowly in more than one min, milky NE with dull appearance will be formed (Yadav et al. 2014).

Robustness to dilution

Robustness to dilution was evaluated by diluting all formulations 100 and 1000 times with different dissolution media which were: 0.1 N HCl (pH 1.2), phosphate buffer (pH 6.8) and water. The diluted NEs were stored for 24 h and monitored for any signs of phase separation or drug precipitation. Formulae which give neither drug precipitation nor phase separation and are thus, said to be "robust" to dilution (Elnaggar et al. 2009).

Turbidity measurement

Turbidity of the resultant NEs given in a nephelometric turbidity unit (NTU) was measured using a turbidimeter (Turbidirect, Lovibond, U.K). Turbidity measurements were performed on the NEs stored in screw capped sample vials. A quantity about 0.2 ml of each SNEDDS was introduced into 900 ml of 0.1 N HCl (pH 1.2) under the action of gentle magnetic stirring (CB 162 heat-stir,

Table 2 Visual observation of self- nanoemulsification grades

Grade	Time required for nanoemulsion formation	Appearance
A	Within 1 min	Clear or slightly bluish
B	Within 1 min	Bluish white
C	Within 2 min	Bluish white, similar in appearance to milk
D	Longer than 2 min	Dull, ash emulsion, slightly oily appearance
E	Longer than 2 min	Poor or minimal emulsification, large oil droplets present on the surface

Stuart, Copley scientific, U.K.) rotates under a constant speed at room temperature (Dash et al. 2015).

Preparation of candesartan cilexetil solid self-nanoemulsifying drug delivery systems

self-nanoemulsifying powders (Table 3) for CC were prepared by mixing about (0.2 ml) amount of each liquid SNEDDS with two types of an adsorbent mixture in a fixed ratio (40:1). Adsorbent mixtures used were: avicel pH 101 plus aerosil 200 and avicel 101 plus dibasic calcium phosphate anhydrous for a period of 10 min under gentle magnetic stirring (CB 162 heat-stir, Stuart, Copley scientific, U.K.). Then each prepared mixture was left to dry in an oven at 40 °C for a period of 48 h. After drying, a quantity of this system (310 mg) equivalent to 8 mg of CC was taken and filled into hard gelatin capsule size 0 (Tarkase et al. 2014).

Evaluations of candesartan cilexetil solid self-nanoemulsifying drug delivery systems

Determination of powder flowing properties

1. Measurement of angle of repose

Angle of repose is an angle between the sides of cone and horizontal surface after pouring powder through a funnel onto a horizontal surface (Aulton and Taylor 2013). The angle is a measure of cohesiveness of powder, as it represents the point at which the interparticle attraction exceeds the gravitational pull on a particle and depends on particle size, shape and moisture content (Lachman and Lieberman 1990). A free-flowing powder will form a cone with shallow sides, and hence a low angle of repose, while a cohesive powder will form a cone with steeper sides. The value obtained was calculated using Eq. 1 and compared with ranges sited in (Table 4) (Chavda et al. 2013).

Table 3 Compositions of candesartan cilexetil solid self-nanoemulsifying drug delivery systems

F-code	Smix ratio	Oil: Smix ratio	Avicel 101 (mg)	Aerosil 200 (mg)	Dibasic calcium phosphate anhydrous (mg)
SSNEDDS-1	1:1	1:9	200	5	—
SSNEDDS-2	1:1	1:9	200	—	5
SSNEDDS-3	2:1	1:9	200	5	—
SSNEDDS-4	2:1	1:9	200	—	5
SSNEDDS-5	3:1	1:9	200	5	—
SSNEDDS-6	3:1	1:9	200	—	5
SSNEDDS-7	4:1	1:9	200	5	—
SSNEDDS-8	4:1	1:9	200	—	5

Table 4 Powder flowing properties based on angle of repose

No.	Angle of repose (degrees)	Type of flow
I.	25–30	Excellent
II.	31–35	Good
III.	36–40	Fair (flow aid not needed)
IV.	41–45	Passable (may hang up, flow aid might be needed)
V.	46–55	Poor (agitation or vibration needed)
VI.	56–65	Very poor
VII.	Over 66	Very, very poor

$$\tan \theta = h/r \tag{1}$$

Where: h and r are height and radius of powder cone; respectively.

2. Measurement of poured density and bulk density
 A quantity of 2 gram (g) of SSNEDDS powders was poured into 10 ml measuring graduated cylinder. Initial volume was recorded and the cylinder was allowed to fall under its own weight onto a hard surface from a height of 2.5 centimeter (cm) at 2 second intervals. Tapping was continued until no further change in volume (Reddy and Sowjanya 2015). Both densities were calculated using Eqs. 2 and 3.

$$\text{Poured density (BD)} = \frac{\text{Weight of powder blend}}{\text{Poured volume of powder blend}} \tag{2}$$

$$\text{Tapped density (TD)} = \frac{\text{Weight of powder blend}}{\text{Tapped volume of powder blend}} \tag{3}$$

3. Measurement of Hausner’s ratio and Carr’s index (Compressibility index)

Hausner’s ratio and Carr’s index are two terms give a useful measure of powder flowability and calculated using Eqs. 4 and 5 respectively which are illustrated below. Hausner’s ratio is related to interparticulate friction and varies from about 1.2 for free-flowing powders to 1.6 for cohesive powders (Table 5) (Lachman and Lieberman 1990). Carr’s index is a direct measure of the potential powder arch or bridge strength and stability. It is classified into ranges as listed in (Table 5) (Mohanrao et al. 2011).

$$\text{Hausner’s ratio} = \frac{\text{Tapped bulk density}}{\text{Poured bulk density}} \tag{4}$$

Table 5 Powder flowing properties based on Carr’s index and Hausner’s ratio

No.	Carr’s index %	Hausner’s ratio	Type of flow
I.	1–10	1.00–1.11	Excellent
II.	11–15	1.12–1.18	Good
III.	16–20	1.19–1.25	Fair
IV.	21–25	1.26–1.34	Passable
V.	26–31	1.35–1.45	Poor
VI.	32–37	1.46–1.59	Very poor
VII.	>38	>1.60	Very, very poor

$$\text{Carr's index} = \frac{100 \times (\text{tapped bulk density} - \text{poured bulk density})}{\text{Tapped bulk density}} \quad (5)$$

In vitro drug dissolution and kinetics of release in various media

In vitro dissolution test was conducted to evaluate the impact of various types of adsorbent mixture on the dissolution of CC from solid self-nanoemulsifying capsule formulations. Release of CC from the prepared capsules was determined using USP dissolution apparatus II (DIS 6000, Copley scientific, U.K.) (Paddle type) in 900 ml of 0.1 N HCl solution (pH 1.2) (Vuddisa et al. 2014; Krishna et al. 2013). After that, release medium was changed into phosphate buffer (pH 6.8) and then into the water in order

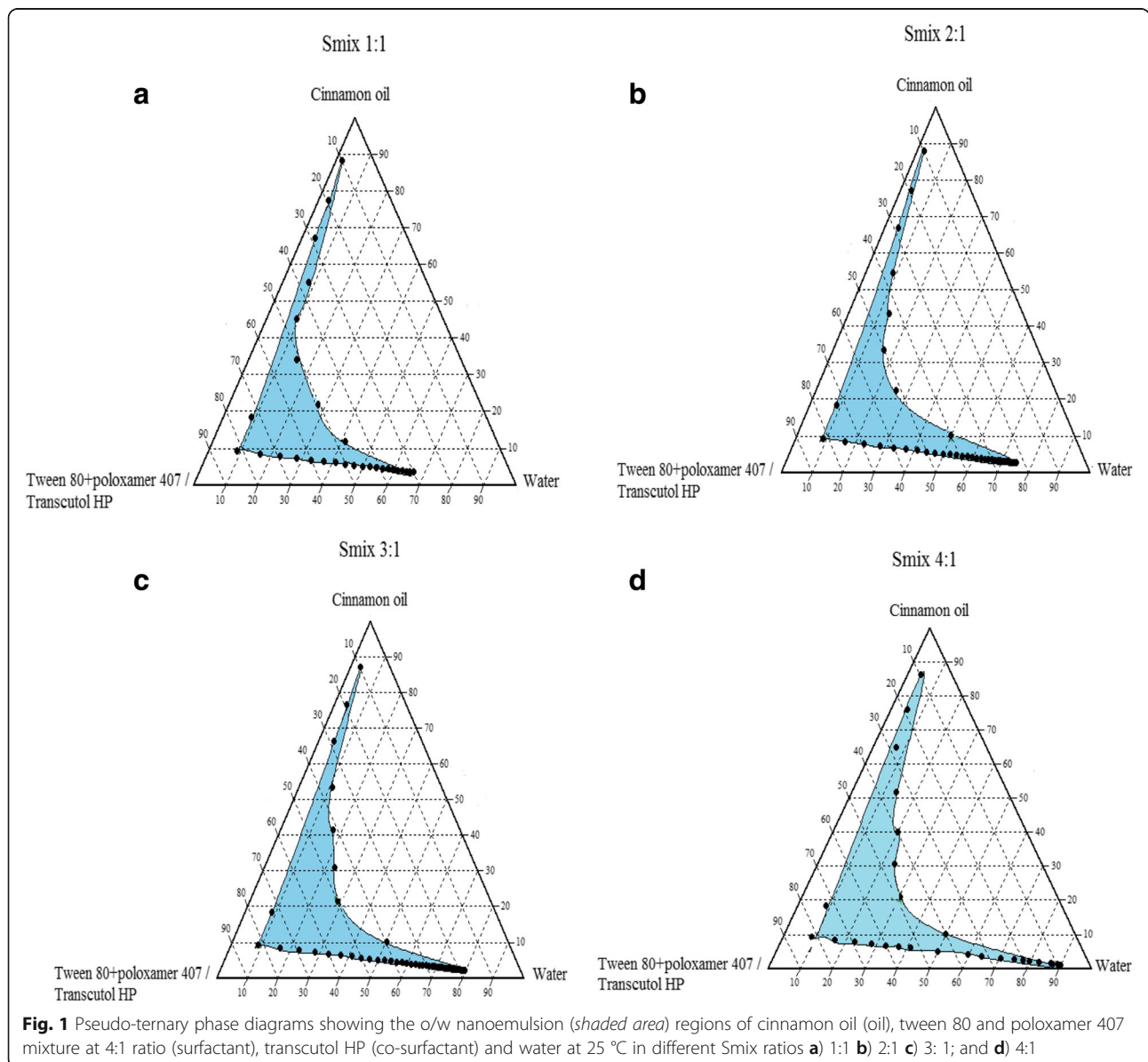


Fig. 1 Pseudo-ternary phase diagrams showing the o/w nanoemulsion (shaded area) regions of cinnamon oil (oil), tween 80 and poloxamer 407 mixture at 4:1 ratio (surfactant), transcutol HP (co-surfactant) and water at 25 °C in different Smix ratios **a**) 1:1 **b**) 2:1 **c**) 3: 1; and **d**) 4:1

Table 6 Particle size distribution and polydispersity index (PDI) of candesartan cilexetil self-nanoemulsifying drug delivery systems

F-code	Particle size (nm)	PDI
SNEDDS-1	39.8	0.281
SNEDDS-2	22.3	0.304
SNEDDS-3	14.1	0.276
SNEDDS-4	46.5	0.328

to study the effect of changing the dissolution medium on drug release from SSNEDDS and evaluate its efficacy.

Selection of optimum candesartan cilexetil solid self-nanoemulsifying drug delivery system

The choice of the best CC SSNEDDS formula was achieved based on the results gained from the evaluation tests including: angle of repose, Hausner's ratio, Carr's index and in vitro drug release study.

Optimum candesartan cilexetil solid self-nanoemulsifying drug delivery system further evaluations

Morphology examination

To visualize the shape and morphology of CC SSNEDDS best formula, the external structure was investigated by a scanning probe microscope (SPM-AA3000, Angstrom Advanced Inc, USA) uses the interaction between a sharp tip and a surface to obtain the image (Thassu et al. 2007).

Fourier transform infrared spectroscopy (FT-IR)

This test was performed at the range of 4000 cm^{-1} to 500 cm^{-1} to detect drug–excipients interaction using FT-IR instrument (FTIR- 8400S, Bruker, Germany). The FT-IR was performed for a pure drug (CC) and optimum SSNEDDS to check if there is any incompatibility between drug and the whole system (Mehta et al. 2014).

Differential scanning calorimetry (DSC)

The DSC technique was used to acquire qualitative information about the physicochemical status of the drug in the solid NE formula and compatibility problems. Moreover, this test was done in order to assess the thermotropic properties and thermal behavior of the drug (CC) and formula. Procedures include taking about 10 mg of each sample, sealing it in an aluminum pan in

Table 7 Surface charge measurement of candesartan cilexetil self-nanoemulsifying drug delivery systems

F-code	Zeta potential (mV)
SNEDDS-1	-88.44
SNEDDS-2	-91.26
SNEDDS-3	-96.50
SNEDDS-4	-98.68

Table 8 Efficiency of surfactant/co-surfactant for cinnamon oil self-emulsification

No.	Surfactant/co-surfactant	Transparency %	No. of flask inversion
I.	Tween 80 with poloxamer 407 mixture at (4:1) ratio	98.6333 ± 0.5507	1
II.	Transcutol HP	99.7000 ± 0.2645	1

DSC instrument (DSC-60 plus Shimadzu, Japan) and heated at the rate of $10\text{ }^{\circ}\text{C}/\text{min}$, covering a temperature range of $40\text{ }^{\circ}\text{C}$ to $300\text{ }^{\circ}\text{C}$ (Kamalakkannan et al. 2013).

X-ray powder diffractometry (XPRD)

It has been shown that polymorphic changes of drug and drug-excipients interaction are important factors, which may affect the drug dissolution rate and bioavailability; therefore XPRD measurements were carried out on two samples include pure CC powder and optimum SSNEDDS using a diffractometer (XRD-6000 Shimadzu, Japan) covering a range of about $0\text{--}50^{\circ}$ (2θ) using the Cu-target X-ray tube and Xe-filled detector and relies on the fact that this radiation has a strong penetrating power in materials with the rate of absorption depending on the density of material (Giannini et al. 2016; Vinay and Ahmed 2015).

Stability study

Optimized CC solid NE formulation was stored at $40\text{ }^{\circ}\text{C}$ and maintained at $75 \pm 5\%$ relative humidity (RH) for 3 months (Mommert oven, W. Germany) and examined for particle size, polydispersity index, zeta potential and in vitro drug dissolution on days 0 and 90. The expiration date was also measured from applying the Arrhenius plot method (Yadav et al. 2014; Selvam and Kulkarni 2014).

Statistics

One-way-analysis of variance (ANOVA) was employed to identify insignificant factors. Data were analyzed and assumed to have an insignificant term when $P > 0.05$ and significant term when $P < 0.05$.

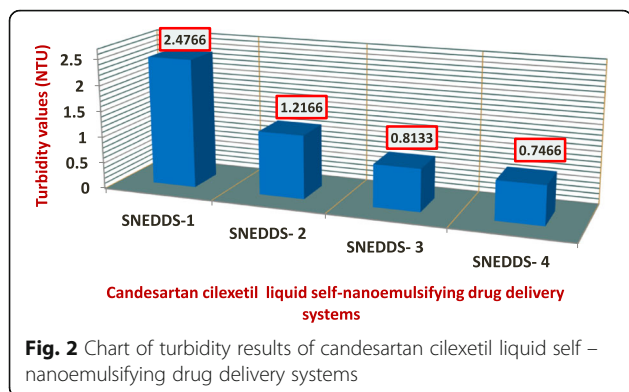
Results and discussion

Construction of pseudo-ternary phase diagrams

Pseudo-ternary phase diagram was used as a useful tool to evaluate the NE domain at Smix ratios: 1:1, 2:1, 3:1 and 4:1. Pseudo-ternary phase diagram results are shown in (Fig. 1).

Table 9 Time of nanoemulsification of candesartan cilexetil liquid self-nanoemulsifying drug delivery systems

F-code	Grade	Emulsification time (second)
SNEDDS-1	A	25
SNEDDS-2	A	22
SNEDDS-3	A	17
SNEDDS-4	A	30



In each Smix ratio, when tween 80 was mixed with poloxamer 407 in 4:1 ratio, it resulted in final hydrophilic/lipophilic balance (HLB) values of 10.150, 12.100, 13.075 and 13.660 for each Smix ratio used respectively.

Preparation of candesartan cilexetil liquid self-nanoemulsifying drug delivery systems

Yellow and clear mixtures were apparently observed without drug precipitation or phase separation. In this study, it was found that lower cinnamon oil and higher tween 80 with poloxamer 407 mixture ratio provided a wide transition window from anhydrous to transparent stable NE upon aqueous dilution under gentle magnetic stirring than did the reverse case and resulted in four successful formulations.

Evaluations of prepared candesartan cilexetil liquid self-nanoemulsifying drug delivery systems

Thermodynamic stability studies

Four CC liquid SNEDDSs have passed the successive cycles of centrifugation, heating-cooling test and freezing-thawing test. It could be concluded that all formulae were found to be thermodynamically/physically stable systems and were selected for further study.

Determination of particle size distribution and polydispersity index value

Results obtained (Table 6) showed that, the average particle size can dramatically decrease with increasing surfactant mixture level due to the presence of more surfactant at the cinnamon oil–water interface, thereby providing stabilized NE (Eid et al. 2013). It was evident from the results that when Smix ratio reached (4:1), there was an increase in particle size distribution.

This finding could be explained by the interfacial break up introduced by the extensive aqueous penetration into cinnamon oil droplets enhanced by the increased surfactant level which lead to the ejection of oil droplets into water have lower critical micelle concentrations (Bandyopadhyay et al. 2013).

Measurement of surface charge

It was found from results illustrated in (Table 7) that the surface charge increased with an increase in surfactant mixture concentration. This could be explained by the fact that higher amount of surfactant (tween 80 with poloxamer 407 mixture) raise the numbers of the hydroxyl group of fatty acid and glycol of tween 80 and poloxamer 407, respectively which further elevate CC SNEDDSs negativity (Ahmad et al. 2014).

Determination of emulsification efficiency of surfactant and co-surfactant

Results are shown in (Table 8). It was seen that although the cinnamon oil, tween 80 with poloxamer 407 mixture and transcitol HP were miscible with each other, upon emulsification in aqueous phase, the co-surfactant (with low HLB) as the oil may have had better interaction with the oil than did the surfactant mixture (with high HLB) and the oil. The polar head groups of both tween 80 and poloxamer 407 may have extended towards the aqueous phase and interacted more efficiently than transcitol HP (Bouchemal et al. 2004).

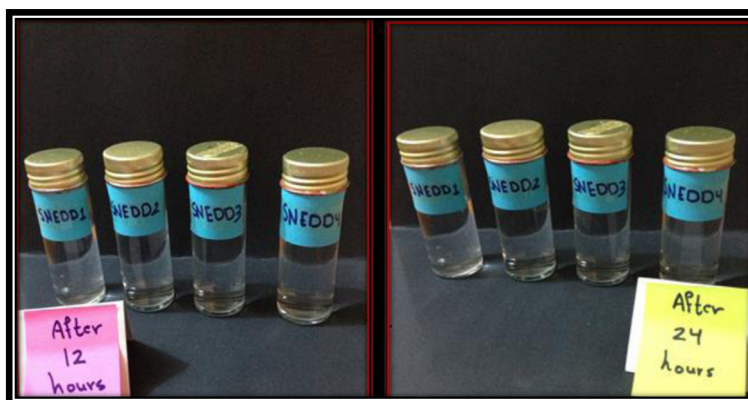


Fig. 3 Photographic picture of turbidity study results of candesartan cilexetil liquid self-nanoemulsifying drug delivery systems

Table 10 Results of candesartan cilexetil self-nanoemulsifying powder flowing properties evaluation

F-code	Angle of repose (Θ)	Result	Hausner's ratio	Result	Carr's index %	Result
SSNEDDS-1	26.5219 ± 0.4177	Excellent	1.0857 ± 0.0084	Excellent	7.6456 ± 0.1869	Excellent
SSNEDDS-2	28.7171 ± 0.1557	Excellent	1.1106 ± 0.0004	Excellent	9.6397 ± 0.3722	Excellent
SSNEDDS-3	27.3802 ± 0.2573	Excellent	1.0489 ± 0.0216	Excellent	6.3017 ± 0.2914	Excellent
SSNEDDS-4	27.6408 ± 0.2956	Excellent	1.1102 ± 0.0010	Excellent	8.0971 ± 0.1610	Excellent
SSNEDDS-5	25.2672 ± 0.0243	Excellent	1.0416 ± 0.0175	Excellent	4.3190 ± 0.0928	Excellent
SSNEDDS-6	25.6616 ± 0.0318	Excellent	1.0643 ± 0.0044	Excellent	6.4776 ± 0.2098	Excellent
SSNEDDS-7	25.1833 ± 0.0060	Excellent	1.0349 ± 0.0043	Excellent	3.4751 ± 0.4301	Excellent
SSNEDDS-8	25.5906 ± 0.2049	Excellent	1.0559 ± 0.0083	Excellent	5.8421 ± 0.0863	Excellent

Determination of self-nanoemulsification time

The spontaneity of the nanoemulsification process depends mainly on the following variables: degree of reduction in the interfacial tension, phase transition region and surfactant concentration (Ebrahimi et al. 2013). The assessment of nanoemulsification time showed that with the increase in surfactant mixture concentration, the time needed for nanoemulsification would be reduced. This could be justified via the increase in surfactant contents availability for adsorption and form a film at the oil/water interface (Shafiq and Shakeel 2009).

The study of emulsification time showed that all four formulations employed could emulsify within the range of (17–30) second and were of grade A class (Table 9).

Robustness to dilution

All CC liquid SNEDDS formulations did not show any signs of phase separation or drug precipitation after 24 h

and 48 h storage. It was warranted that dilution of liquid SNEDDS does not change the rigidity of packing of surfactant mixture layer at the nanodroplet interface (Prabhakar et al. 2013; Raval et al. 2012).

Turbidity measurement

It was noticed from the results presented in (Fig. 2), that increasing Smix ratio leads to a decrease in turbidity values due to a better solubility of drug (Sarkar and Hardenia 2011). The formulation with a high turbidity (2.4766 ± 0.1266 NTU) had Smix ratio of (1:1), whereas minimum turbidity result (0.7466 ± 0.0251 NTU) was found in SNEDDS-4 formulation corresponding to (4:1) ratio. Results showed that all the SNEDDS formulations showed minimum turbidity values (less than 100 NTU) in comparison to water (0.6033 ± 0.0568 NTU) as a result of their small particle size, which indicates good miscibility and self-emulsification of these formulae when introduced into the aqueous acidic medium

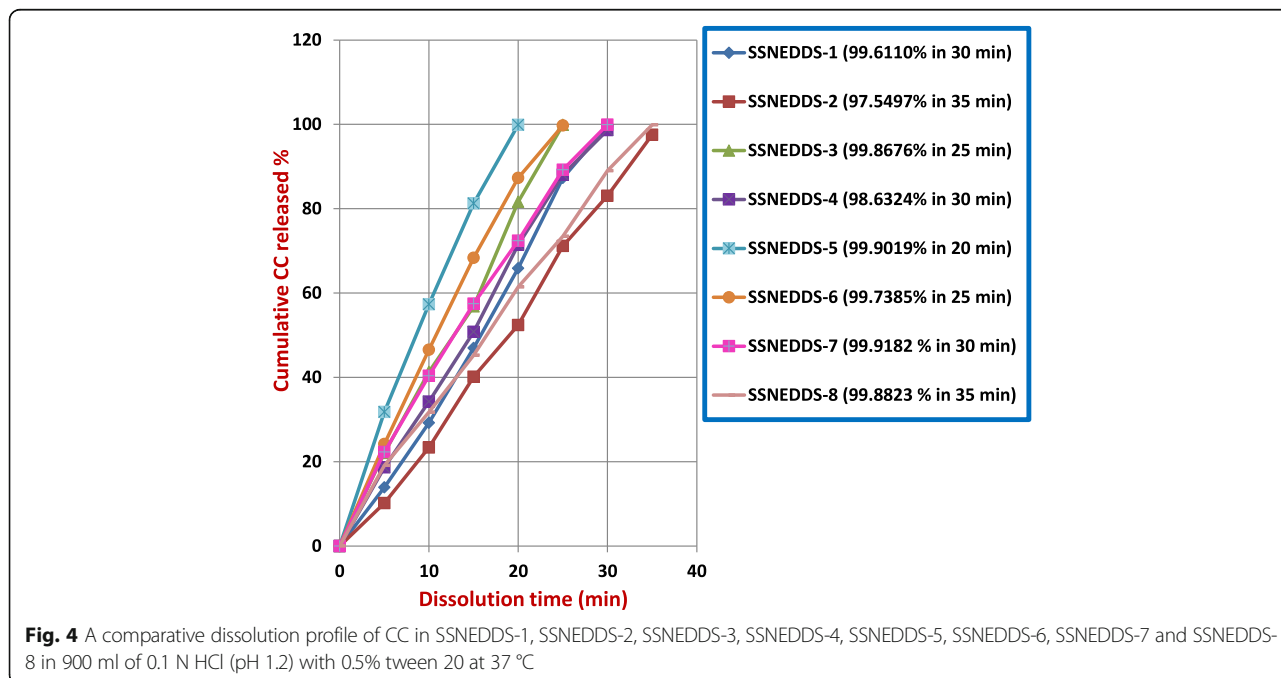


Fig. 4 A comparative dissolution profile of CC in SSNEDDS-1, SSNEDDS-2, SSNEDDS-3, SSNEDDS-4, SSNEDDS-5, SSNEDDS-6, SSNEDDS-7 and SSNEDDS-8 in 900 ml of 0.1 N HCl (pH 1.2) with 0.5% tween 20 at 37 °C

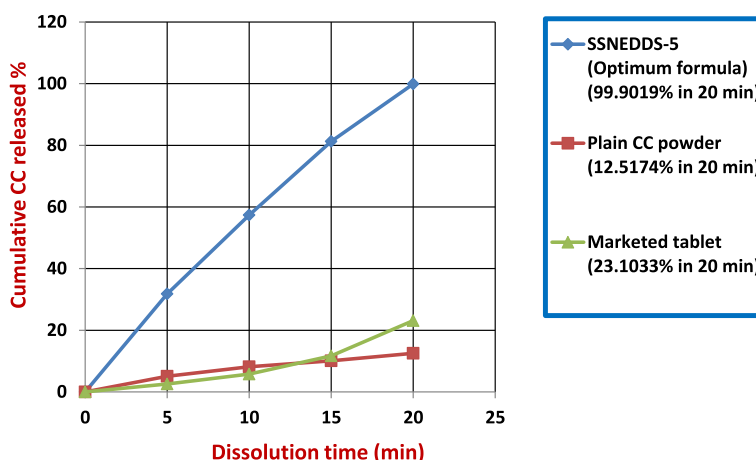


Fig. 5 A comparative dissolution profile of candesartan cilexetil SSNEDDS-5, plain candesartan cilexetil powder and marketed tablet in 900 ml of 0.1 N HCl (pH 1.2) with 0.5% tween 20 at 37 °C

(Czajkowska-Kośnik et al. 2015; Kassem et al. 2010). All prepared liquid formulations maintained their clarity after 24 h and 48 h storage as illustrated in (Fig. 3).

Preparation of candesartan cilexetil solid self-nanoemulsifying drug delivery systems

Adsorbing of four liquid SNEDDS formulations on to two different set of solid adsorbent carrier mixtures resulted in eight white, fluffy and free-flowing powders with a porous structure and this will overcome the problem of stability associated with liquid dosage form and will improve patient compliance.

Evaluations of candesartan cilexetil solid self-nanoemulsifying drug delivery systems

Determination of powder flowing properties

Various micromeritic properties of SSNEDDS formulations of CC are shown in (Table 10). Solid self-nanoemulsifying formulations were prepared to overcome the disadvantages associated with poor flowability of pure CC powder which has an angle of repose about

(67.5683 ± 0.3111), Hausner’s ratio of (1.7701 ± 0.0359) and Carr’s index of (40.3480% ± 0.1589%).

Results showed that all CC SSNEDDS formulations have good flow properties. From results gained, it was found that all powders prepared have angle of repose ranges between 25.1833 ± 0.0060 and 28.7171 ± 0.1557, Hausner’s ratio is in the run of (1.0349 ± 0.0043 to 1.1106 ± 0.0004) and Carr’s index falls into the latitude of (3.4751% ± 0.4301% to 9.6397% ± 0.3722%), which indicate good flowing and compressing properties of powder.

In vitro drug dissolution and kinetics of release in various media

The dissolution of hard gelatin capsules filled with CC SSNEDDS eight formulations in 0.1 N HCl medium (pH 1.2) with 0.5% of tween 20 at 37 °C results are presented in (Fig. 4). It could be speculated from the results gained that all CC SSNEDDS formulations resulted in a spontaneous formation of NEs with a small droplet size in zero order release model. The amount of CC released

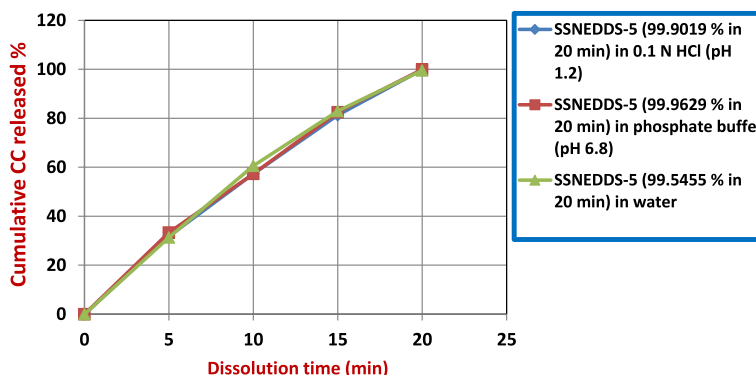


Fig. 6 A comparative dissolution profile of SSNEDDS-5 in different dissolution media

Table 11 Release kinetics of candesartan cilexetil form SSNEDDS-5 in different media

F-code	Zero order (R ²)	First order (R ²)	Higuchi (R ²)	Hixson Crowell (R ²)	Korsmeyer and Peppas		
					R ²	n	Release mechanism
SSNEDDS-5 in 0.1 N HCl (pH 1.2)	0.9909	0.7158	0.9579	0.7776	0.9522	1.5490	Supercase II Transport
SSNEDDS-5 in phosphate buffer (pH 6.8)	0.9885	0.7089	0.9618	0.7708	0.9483	1.5485	Supercase II Transport
SSNEDDS-5 in water	0.9849	0.7142	0.9610	0.7745	0.9527	1.5558	Supercase II Transport

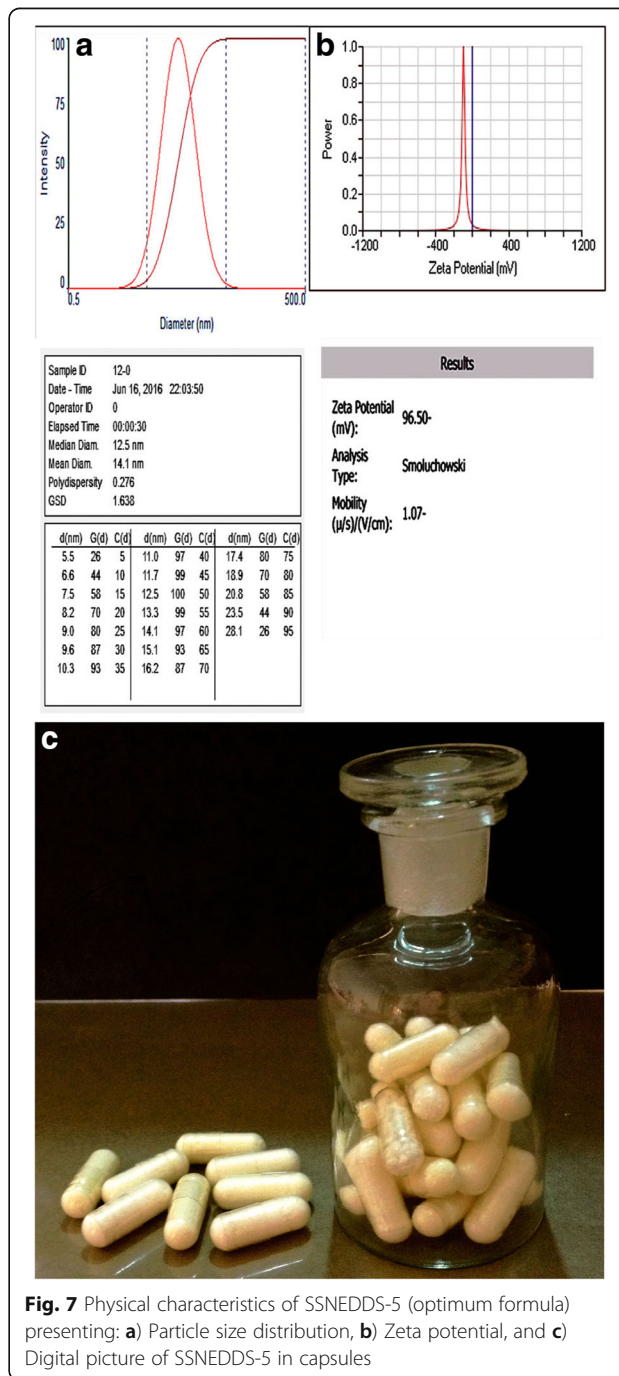
percent from different SSNEDDS formulations varied according to adsorbent mixture type and Smix ratio.

In vitro drug release from CC self-nanoemulsifying capsules prepared by different adsorbent mixture was higher for formulations containing avicel 101 with aerosil 200 mixture than formulations adsorbed onto a mixture of avicel 101 plus dibasic calcium phosphate anhydrous mixture. Adsorbent particle size may be the primary factor that influences drug release from various SSNEDDS formulations (Amrutkar et al. 2014).

The release of drug decreased with increasing adsorbent particle size because of entrapment of drug in deeper voids of larger particles and a narrow surface area interacting with aqueous dissolution medium (Sohn et al. 2012). Small adsorbent particle size with its large surface area exposed and highly porous structure lead to a better soaking of drug and more contact with dissolution medium, which also increases the CC dissolution rate (Krstić et al. 2015).

Moreover, an excipient such as aerosil 200 enhances dissolution of CC to a large extent. It is typical of many fine inorganic powder grades like aerosil 200 has a particle size of about 15 nm diameter in concomitant with large surface area exposed around (100–400 m²/g), whereas dibasic calcium phosphate anhydrous has porous spheres with average particle diameter around 94 μm and surface area of 35 m²/g (Rowe et al. 2006). For this reason, the release of CC adsorbed onto a carrier mixture containing aerosil 200 was better than release from dibasic calcium phosphate anhydrous based formulations, which was slower.

In vitro drug release from CC self-nanoemulsifying capsules prepared by different Smix ratios were found in the following order: (Smix ratio) 4:1 > 3:1 > 2:1 > 1:1. Release of CC was more for higher ratios of Smix used when compared to the lower ratios. This may be rationalized to a better coating of carrier around the drug molecules which leads to improved solubility and dissolution rate of drug (Obitte et al. 2013). Thus, From all the results obtained, it was evident that the usage of tween 80 with poloxamer 407 mixture: transcitol HP at 3:1 and 4:1 ratio were the most advantageous in dissolution term than other ratios, although 4:1 ratio

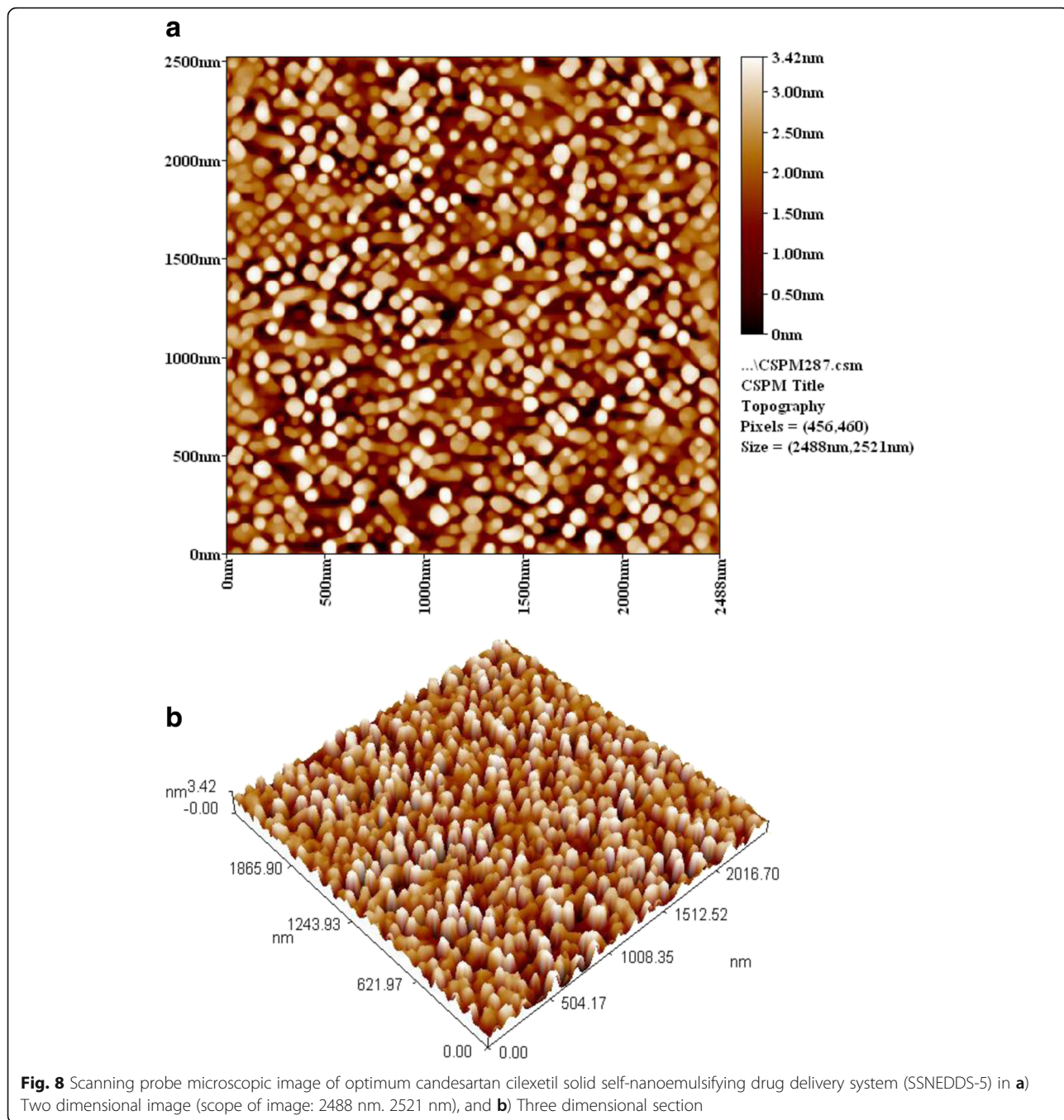


formulations have a higher particle size distribution than 3:1 ratio.

This could be attributed to the higher amount of liquid vehicle of tween 80 and poloxamer 407 which further improve solubility and dissolution of CC in addition to the large surface area of nanometric drug particles. It was clear that, formula (SSNEDDS-5) showed the highest drug released percent (99.9019% after 20 min) and according to ANOVA analysis, there was a substantial

difference ($P < 0.05$) between the mean dissolution rates obtained from this formula, plain CC powder (12.5174% after 20 min) and marketed tablet (Atacand® 8 mg) (23.1033% after 20 min) in dissolution rate and extent (Fig. 5).

In vitro CC release from SSNEDDS-5 formula was done in phosphate buffer (pH 6.8) containing 0.35% of tween 20 and in water with 2% of tween 20 (Fig. 6) and it has shown that release of CC was faster in phosphate



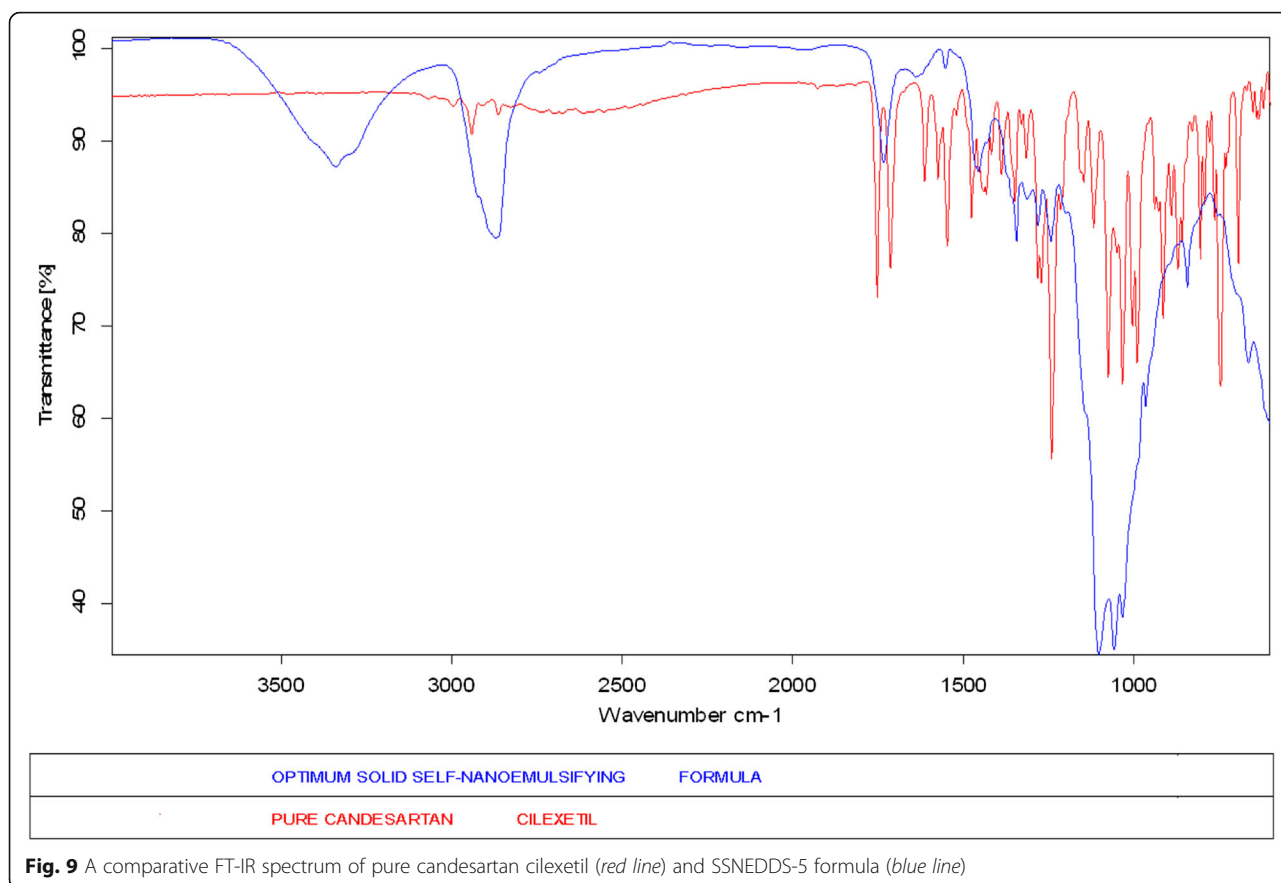


Fig. 9 A comparative FT-IR spectrum of pure candesartan cilexetil (red line) and SSNEDDS-5 formula (blue line)

buffer (pH 6.8) and lower in water compared with their release in 0.1 N HCl medium (pH 1.2). This difference in cumulative release rate and extent in different media was due to the difference in solubility of CC in various media which was following this order of solubility:

Media: phosphate buffer (pH 6.8) > 0.1 N HCl (pH 1.2) > water.

Solubility of CC (mg/ml): $0.0089 \pm 0.0006 > 0.00617 \pm 0.0050 > 0.00034 \pm 0.0001$

Release kinetic studies of CC from the SSNEDDS-5 formulation in all media had shown the highest correlation coefficient (R^2) value was corresponding to zero order model as listed in (Table 11). According to the Korsmeyer-Pepas equation, release exponents (n) were greater than (1.00) in all release media. This indicates that supercase II transport was govern the whole release mechanism; therefore diffusion and convection controlled mechanisms play a role in the release of CC from SSNEDDS formulation. Also, all the results of dissolution of CC were conformed to united state pharmacopeia (USP) and fall within

acceptable criteria (at least 75–80% amount of drug dissolved).

Selection of optimum candesartan cilexetil solid self-nanoemulsifying drug delivery system

The formula (SSNEDDS-5) was selected as an optimum self-nanoemulsifying capsule consisting of 10% w/w of cinnamon oil, 54% w/w of tween 80, 13.5% w/w of poloxamer 407, 22.5% w/w of transcitol HP, 200 mg of avicel 101 and 5 mg of aerosil 200 (Fig. 7), since it has an excellent flowing properties as indicated by having an angle of repose (25.2672 ± 0.0243), Hausner’s ratio (1.0416 ± 0.0175), Carr’s index ($4.3190\% \pm 0.0928\%$) and fast cumulative drug

Table 12 FT-IR Characteristic functional groups of candesartan cilexetil

No.	Functional groups	Peaks (cm ⁻¹)
I.	-O-H Stretching	2800–3380
II.	-C = O- Stretching	1670–1820
III.	-C-O- Stretching	1210–1350
IV.	-O- Substitution	600–750
V.	Aromatic C-H Stretching	2850–2950

release ($99.9019\% \pm 0.0841\%$ in 20 min). Solubility study on this formula has shown a significant improvement in solubility of CC ($p < 0.05$) compared to water and was found to be (524.9692 ± 1.0652 mg/ml). Presenting the drug in a highly solubilized form is expected to induce a cell-specific delivery manner with a maximum intrinsic activity of the drug. Delivery thereby limiting off-target access and improving the bioavailability of poorly soluble drug, CC.

Optimum candesartan cilexetil solid self-nanoemulsifying drug delivery system further evaluations

Morphology examination

The SPM image result in (Fig. 8) showed spherical shape particles with smooth margins and average nanometric particle size of about (57.07 nm) of SSNEDDS-5 optimum formula. The difference in average particle size result from that obtained via particle size analyzer instrument is due to agglomeration of formula powder particles placed on a glass slide of SPM instrument. In addition, small sample loaded also considered as another reason that made SPM probe unable to get precise

statistical determination of particle size distribution (Eyjolfsson 2015).

Fourier transform infrared spectroscopy

The FT-IR spectrum of pure CC powder (Fig. 9) showed characteristic peaks ideal for pure drug powder at 2940.73 cm^{-1} due to aromatic ($-\text{C}-\text{H}$) stretching, 2862.06 cm^{-1} for (O-H) stretching, 1751.37 cm^{-1} and 1713.48 cm^{-1} for ester ($-\text{C}=\text{O}$) stretching vibration, 1270.20 cm^{-1} and 1315.09 due to ($-\text{C}-\text{O}$) stretching of carbonyl group of aromatic ester and 744.56 due to ($-\text{O}$ -substitution). It was found that in SSNEDDS-5 formula (Fig. 9), CC showed major characteristic peaks which were: 1733.28 cm^{-1} corresponding for ester ($-\text{C}=\text{O}$) carbonyl stretching and another peak at 1242.29 cm^{-1} corresponding to ($-\text{C}-\text{O}$) stretching in aromatic ester indicated that there was no interaction between drug and formulation excipients (Sathali and Varun 2012). All obtained peaks were within acceptable range of pure CC shown in (Table 12) (Singh et al. 2015).

Furthermore, there was a shift in the ester ($-\text{C}=\text{O}$) stretching vibration from 1713.48 cm^{-1} to 1733.28 cm^{-1}

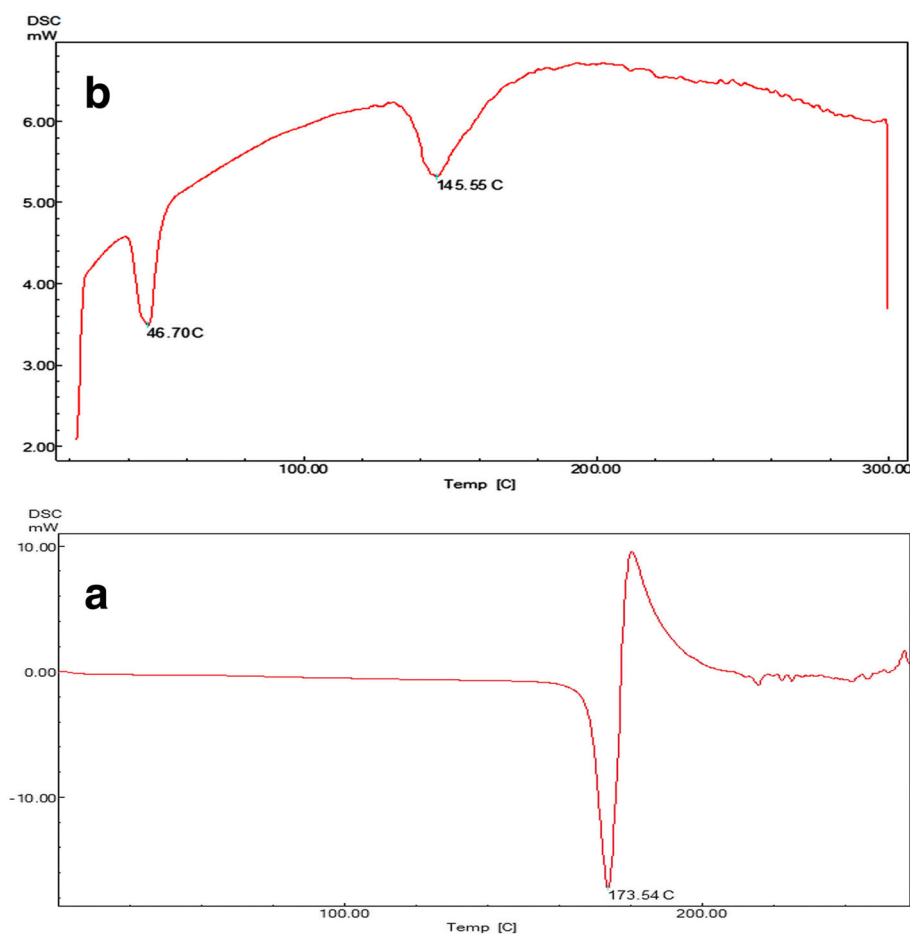


Fig. 10 Thermogram profile of (a) Pure candesartan cilexetil, and (b) Optimum formula (SSNEDDS-5)

which may be attributed to conversion of CC from crystal form to an amorphous form (Panchal et al. 2012). The minor peaks due to CC were absent indicating trapping of CC inside the inner oily core matrix (Raghad and Hind 2015). Corresponding to (-C-H) of CC, it was shifted from 2940.73 cm^{-1} to 2870.92 cm^{-1} , which suggests the presence of hydrogen bonding, resulting in an increase in the solubility of CC (Devi et al. 2014).

Differential scanning calorimetry

Results of DSC pattern for pure CC and the optimum SSNEDDS-5 formula is shown in (Fig. 10). Pure CC showed a characteristic endothermic peak at (173.54 °C)

which indicating its melting point and conforms the reported range of (160 °C–175 °C) (Reddy and Navaneetha 2015). No representative peak of CC was observed for the SSNEDDS-5 formula, indicating that the drug was present in an amorphous form or in a molecularly dissolved state in cinnamon oil core of SSNEDDS-5 (Suresh et al. 2007).

It is important to remind that in the preparation of SSNEDDS-5 formula, CC was dissolved in cinnamon oil and mixed with tween 80, poloxamer 407, transcucol HP and subsequently was adsorbed via a solid carrier mixture. This allowed homogeneous dispersion of the CC in the oily phase and did not allow the drug to crystallize

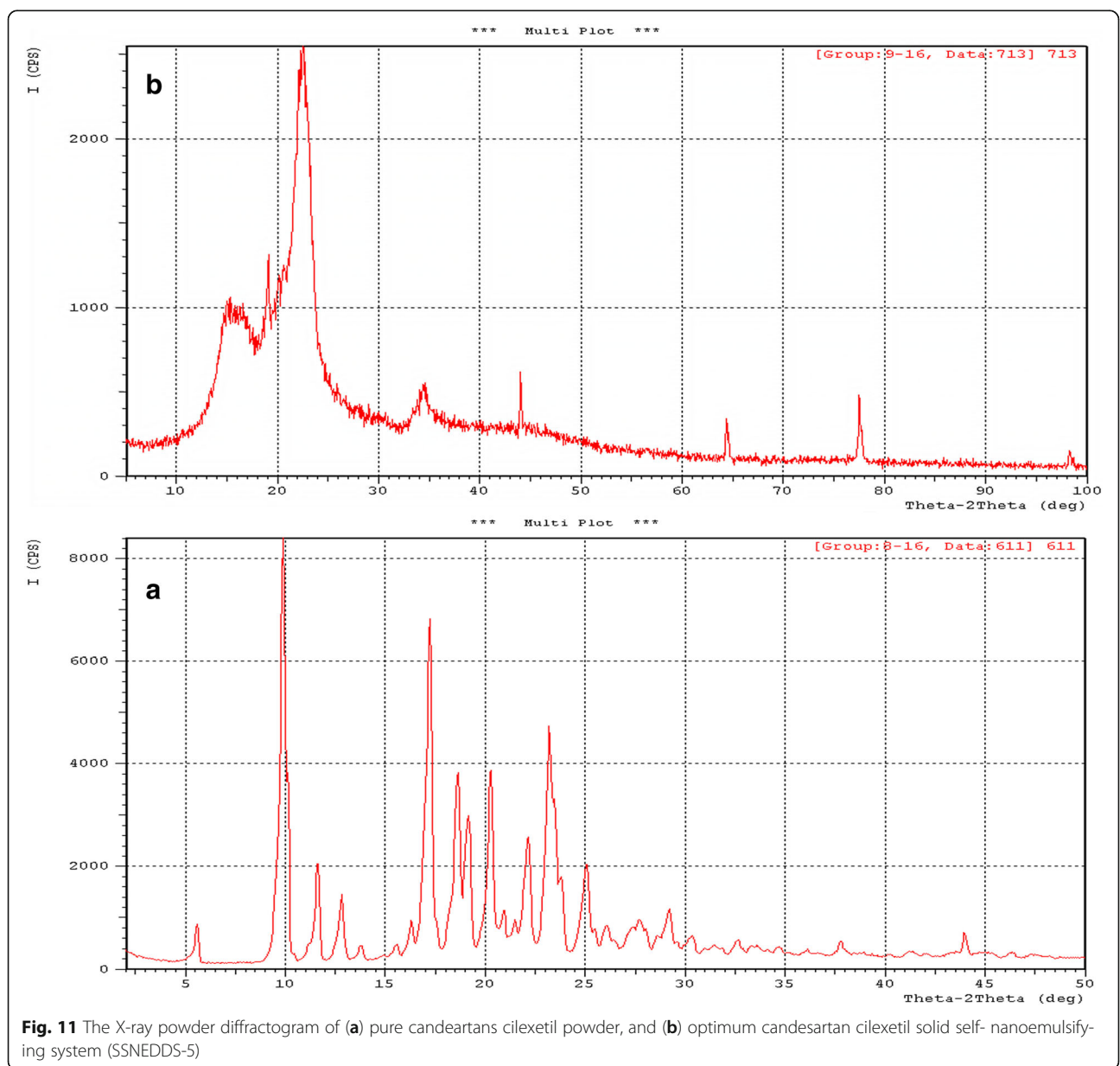


Fig. 11 The X-ray powder diffractogram of (a) pure candesartan cilexetil powder, and (b) optimum candesartan cilexetil solid self-nanoemulsifying system (SSNEDDS-5)

Table 13 Stability of candesartan cilexetil optimum solid self-nanoemulsifying capsule (SSNEDDS-5)

No.	Tests	Results at temperature 40 °C		
		Initial value	After 1 month	After 3 months
I.	Particle size (nm)	14.1	15.1	17.1
II.	PDI	0.267	0.257	0.218
III.	Zeta potential (mV)	-96.50	-95.54	-93.55
IV.	Dissolution	99.9019 ± 0.0841	99.6020 ± 0.0434	98.8514 ± 0.4937

(Selvam and Kulkarni 2014; Cekić et al. 2015). Besides that, a new peak appeared at (145.55 °C) in the optimum SSNEDDS-5 formula. This peak corresponds to melting of the whole system (Patil et al. 2013). Finally, regarding endothermic peak at (46.70 °C) corresponding to avicel 101 was appeared confirming its ability to maintain its crystalline structure, but in a reduced intensity state due to the presence of cinnamon oil, tween 80, poloxamer 407 and transcitol HP.

X-ray powder diffractometry

The X-ray diffractogram of pure CC and SSNEDDS-5 formula is shown in (Fig. 11). It was found that X-ray diffraction pattern of pure CC revealed the presence of the drug in a crystalline state as it showed sharp distinct peaks notably at 2θ diffraction angles of 9.9819°, 17.2137°, 18.6489°, 19.8632°, 21.5225°, 23.8034°, 25.5001°, 27.7464° and 29.1848° which match the reported values (Krishna et al. 2013). The results showed the absence of obvious peaks representing crystals of CC in optimum formula (SSNEDDS-5) indicating that the drug was in an amorphous or disordered crystalline phase in the oily inner core. The XRPD of SSNEDDS-5 formula showed only three sharp diffraction peaks at 2θ angles of 15.6217°, 20.5113° and 22.5252° belonging to avicel 101, indicating that it is the only component which maintained its crystalline structure.

Stability study

The results tabulated in (Table 13) showed that there was no marked difference between initial samples and aged samples of SSNEDDS-5 formula after three months storage. This implying that there was little or no degradation of CC and/or excipients used in the SSNEDDS-5 formula within this period of time and it possesses a good storage capacity and thermodynamic stability for drug delivery. From Arrhenius plot, the expiration date was calculated to be about 4.366 years. It could be judged from the results gained, that inclusion of poloxamer 407 (polymeric surfactant) has been shown to be quite successful regarding stabilization, since there will be a synergistic stabilizing effect together with tween 80 (Li et al. 2016).

Conclusion

Based on all results gained, it has been established that SSNEDDS with its ability to produce a nanometric dispersion of controllable size modulates the encapsulated model drug (CC) solubility, wettability, dissolution and stability in the desired fashion than did the conventional dosage form. The SSNEDDS-5 formula composed of 10% w/w of cinnamon oil, 54% w/w of tween 80, 13.5% w/w of poloxamer 407, 22.5% w/w of transcitol HP adsorbed on a mixture of avicel 101 and aerosil 200 in 40:1 ratio showed good flow properties and best drug release, proving that delivering the drug in a highly solubilized form and rapidly dispersed manner could be achieved through proper design of SSNEDDS formulations.

Abbreviations

ACE: Angiotensin converting enzyme; ANOVA: Analysis of variance; AT1: Angiotensin II type-1; BCS: Biopharmaceutical classification system; CC: Candesartan cilexetil; cm: Centimeter; cm⁻¹: Reciprocal centimeter; DSC: Differential scanning calorimetry; FT-IR: Fourier transform infrared; g: Gram; GRAS: Generally regarded as safe; HLB: Hydrophilic/lipophilic balance; h: Hour; Log P: Base-10 logarithm of the permeability coefficient; m²: Square meter; mg: Milligram; min: Minute; ml: Milliliter; mV: Millivolt; N: Normal; NEs: Nanoemulsions; nm: Nanometer; No.: Number; NTU: Nephelometric turbidity unit; o/w: Oil in water; PDI: Polydispersity index; pH: Minus Logarithm [H⁺]; RH: Relative humidity; RI: Refractive index; rpm: Revolution per minute; Smix: Surfactant/co-surfactant mixture; SNEDDS: Self-nanoemulsifying drug delivery system; SPM: Scanning probe microscopy; SSNEDDS: Solid self-nanoemulsifying drug delivery; USP: United state pharmacopeia; UV/Vis: Ultraviolet/Visible; w/o: Water in oil; w/w %: Weight by weight percent; XRPD: X-ray powder diffractometry; λ_{max}: Wave length with maximum absorbance

Funding

None.

Authors' contributions

Both authors read and approved the final manuscript.

Competing interests

The authors declare that they have no competing interests.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Received: 24 January 2017 Accepted: 9 May 2017

Published online: 15 June 2017

References

- Ahmad J, Mir SR, Kohli K, Chuttani K, Mishra AK, Panda AK, Amin S (2014) Solid-nanoemulsion preconcentrate for oral delivery of paclitaxel: formulation design, biodistribution, and γ scintigraphy imaging. *BioMed Res Inter* 2014:1–12

- Amrutkar C, Salunkhe K, Chaudhary S (2014) Study on self nanoemulsifying drug delivery system of poorly water soluble drug rosuvastatin calcium. *World J Pharm Res* 3(4):2137–2151
- Aulton ME, Taylor KM (2013) *Aulton's pharmaceuticals: the design and manufacture of medicines*, 4th edn. Edinburgh, Elsevier Health Sciences
- Bandyopadhyay S, Bhuria L, Lal D (2013) An explicit review on quantitative estimation of candesartan cilexetil employing various analytical techniques. *Pharma Anal Acta* 4(6):1–7. doi:10.4172/2153-2435.1000254
- Beale JM, Block J, Hill R (2010) *Organic medicinal and pharmaceutical chemistry*, 12th edn. Lippincott Williams and Wilkins, Philadelphia
- Bieger D, Hein L, Lüllmann H, Mohr K (2005) *Color atlas of pharmacology*, 3rd edn. Thieme, Stuttgart
- Bouchamel K, Briançon S, Perrier E, Fessi H (2004) Nano-emulsion formulation using spontaneous emulsification: solvent, oil and surfactant optimization. *Int J Pharmaceutics* 280(1):241–251. doi:10.1016/j.ijpharm.2004.05.016
- Cekić ND, Đorđević SM, Savić SR, Savić SD (2015) A full factorial design in the formulation of diazepam parenteral nanoemulsions: physicochemical characterization and stability evaluation. *Adv Technol* 4(1):69–77
- Chavda H, Patel J, Chavada G, Dave S, Patel A, Patel C (2013) Self-nanoemulsifying powder of isotretinoin: preparation and characterization. *J Powder Technol* 1–9. doi:10.1155/2013/108569
- Czajkowska-Kośnik A, Szełalska M, Amelian A, Szymańska E, Winnicka K (2015) Development and evaluation of liquid and solid self-emulsifying drug delivery systems for atorvastatin. *Molecules* 20(12):21010–21022. doi:10.3390/molecules201219745
- Darwehkar GN, Jain DK, Chouhan J (2012) Biopharmaceutical classification of candesartan and candesartan cilexetil. *Asi J Pharm Life Sci* 2(2):295–302
- Dash RN, Mohammed H, Humaira T, Ramesh D (2015) Design, optimization and evaluation of glipizide solid self-nanoemulsifying drug delivery for enhanced solubility and dissolution. *Saudi Pharmaceutical J* 23(5):528–540. doi:10.1016/j.jsps.2015.01.024
- Devi S, Peddinti D, Pinnika A (2014) Formulation and evaluation of solid dispersion tablets of poorly water soluble drug candesartan cilexetil using poloxamer 407. *Int J Pharm Sci Res* 29(1):67–73
- Dey S, Jha SK, Malakar J, Gangopadhyay A (2012) Improvement of bioavailability of poorly soluble drugs through delivery system. *J Pharm SciTech* 1(2):6–11
- Ebrahimi P, Ebrahim-Magham B, Pourmorad F, Honary S (2013) Ferulic acid lecithin-based nano-emulsions prepared by using spontaneous emulsification process. *Iran J Chem Chem Eng* 32(3):17–25
- Eid AM, Elmarzugi NA, El-Enshasy HA, Arafat OM (2013) A novel Swietenia macrophylla oil self-nanoemulsifying system: development and evaluation. *Int J Pharm Pharm Sci* 5(Suppl 3):639–644
- Elgadira MA, Adam A (2014) Selected drug delivery systems based on nanoemulsion. *World J Pharm Res* 3(2):1796–1809
- Elnaggar YS, El-Massik MA, Abdallah OY (2009) Self-nanoemulsifying drug delivery systems of tamoxifen citrate: design and optimization. *Int J Pharm* 380(1):133–141. doi:10.1016/j.ijpharm.2009.07.015
- Eyjolfsson R (2015) *Design and manufacture of pharmaceutical tablets*. Elsevier, London
- Fathi M, Mozafari MR, Mohebbi M (2012) Nanoencapsulation of food ingredients using lipid based delivery systems. *Trends Food Sci Technol* 23(1):13–27. doi:10.1016/j.tifs.2011.08.003
- Frayn K (2005) Cardiovascular disease: diet, nutrition and emerging risk factors. The report of a british nutrition foundation task force. Blackwell, Oxford
- Giannini C, Ladisa M, Altamura D, Siliqi D, Sibillano T, De Caro L (2016) X-ray diffraction: a powerful technique for the multiple-length-scale structural analysis of nanomaterials. *Crystals* 6(87):1–22. doi:10.3390/cryst6080087
- Gupta AK, Mishra DK, Mahajan SC (2011) Preparation and in-vitro evaluation of self emulsifying drug delivery system of antihypertensive drug valsartan. *Int J Pharm Life Sci* 2(3):633–639
- Husain A, Azim M, Mitra M, Bhasin PS (2011) A review on candesartan: pharmacological and pharmaceutical profile. *J Appl Pharma Sci* 1(10):12–17
- Jane PFB, Guo JH, Chaubal MV (2006) *Excipient development for pharmaceutical biotechnology and drug delivery systems*, 3rd edn. Informa Healthcare, USA
- Kalepun S, Manthina M, Padavala V (2013) Oral lipid-based drug delivery systems—an overview. *Acta Pharm Sin B* 3(6):361–372. doi:10.1016/j.apsb.2013.10.001
- Kamalakkannan V, Puratchikody A, Ramanathan L (2013) Development and characterization of controlled release polar lipid microparticles of candesartan cilexetil by solid dispersion. *Res Pharm Sci* 8(2):125–136
- Kassem AA, Marzouk MA, Ammar AA, Elosaily GH (2010) Preparation and in vitro evaluation of self-nanoemulsifying drug delivery systems (SNEDDS) containing clotrimazole. *Drug Discoveries Therapeutics* 4(5):373–379
- Kolesar JM, Vermeulen LC (2016) *Top 300 pharmacy drug cards—2016/2017*. McGraw-Hill Education, New York
- Krishna HP, Srinivasan B, Rajamanickam D, Veerabhadraiah BB, Varadharajan M (2013) Solubility and dissolution enhancement of candesartan cilexetil by liquisolid compacts. *Pharmaceutics Drug Deliv Res* 2(2):1–10. doi:10.4172/2325-9604.1000115
- Krstić M, Ražić S, Vasiljević D, Spasojević Đ, Ibrić S (2015) Application of experimental design in the examination of the dissolution rate of carbamazepine from formulations. Characterization of the optimal formulation by DSC, TGA, FT-IR and PXRD analysis. *J the Serb Chem Soc* 80(2):209–222. doi:10.2298/JSC030814114K
- Kumar M, Pathak K, Misra A (2009) Formulation and characterization of nanoemulsion-based drug delivery system of risperidone. *Drug Dev Ind Pharm* 35(4):387–395. doi:10.1080/03639040802363704
- Lachman L, Lieberman HA (1990) *Pharmaceutical dosage forms, parenteral medications*. M. Dekker, New York
- Li M, Azad M, Davé R, Bilgili E (2016) Nanomilling of drugs for bioavailability enhancement: a holistic formulation-process perspective. *Pharmaceutics* 8(17):1–35. doi:10.3390/pharmaceutics8020017
- Maravajhala V, Papishetty S, Bandlapalli S (2012) Nanotechnology in development of drug delivery system. *Int J Pharm Sci Res* 3(1):84–96
- Mehta MR, Machhaliya RY, Patel CN, Daraji HM (2014) Formulation and evaluation of sublingual tablet of candesartan cilexetil. *Int J Pharm Res BioSci* 3(2):900–925
- Moffat AC, David Osselton M, Brian W (2011) *Clarke's analysis of drugs and poisons*, 4th edn. Pharmaceutical Press, London
- Mohanrao BM, Sundar PS, Nagsen S (2011) Preparation and characterization of solid self microemulsifying drug delivery system by adsorbent technique to improve dissolution profile of poorly aqueous soluble drug Ramipril. *Int Res J Pharm* 2(6):85–90
- Muhamad II, Selvakumaran S, Lazim NA (2014) Designing polymeric nanoparticles for targeted drug delivery system. *Nanomedicine* 287–313
- Obitte NC, Rohan LC, Adeyeye CM, Parniak MA, Esimone CO (2013) The utility of self-emulsifying oil formulation to improve the poor solubility of the anti HIV drug CSiC. *AIDS Res Ther* 10(1):1–9
- Panchal D, Patel U, Bhimani B, Daslaniya D, Patel G (2012) Formulation and evaluation of sustained release matrix tablets of candesartan cilexetil. *Int J Pharm Res BioSci* 1(4):75–101
- Patel ND, Patel YB, Mankad AU (2012) Techniques to improve the solubility of poorly soluble drugs. *Int J Pharm Life Sci* 3(7):1828–1832
- Patil S, Patil V, Shete A, Doijad R (2013) Design, development and *in vitro* characterization of self emulsifying drug delivery system for Irbesartan. *Iran J Pharm Sci* 9(2):67–80
- Prabhakar K, Afzal SM, Surender G, Kishan V (2013) Tween 80 containing lipid nanoemulsions for delivery of indinavir to brain. *Acta Pharm Sin B* 3(5):345–353
- Prajapati ST, Joshi HA, Patel CN (2013) Preparation and characterization of self-microemulsifying drug delivery system of olmesartan medoxomil for bioavailability improvement. *J Pharmaceutics* 2013:1–9. doi:10.1155/2013/728425
- Raghad AN, Hind EZ (2015) Enhancement of candesartan cilexetil dissolution rate by using different methods. *Asi J Pharm Clin Res* 8(1):320–326
- Rahman MA, Harwansh R, Mirza MA, Hussain S, Hussain A (2011) Oral lipid based drug delivery system (LBDDS): formulation, characterization and application: a review. *Curr Drug Deliv* 8(4):1–16. doi:10.2174/156720111795767906
- Raval C, Joshi N, Patel J, Upadhyay UM (2012) Enhanced oral bioavailability of olmesartan by using novel solid self emulsifying drug delivery system. *Int J Adv Pharmaceutics* 2(2):82–92
- Reddy BV, Navaneetha K (2015) Formulation and evaluation of orodispersible tablets of candesartan. *Pharm Innov J* 4(1):25–32
- Reddy MS, Sowjanya N (2015) Formulation and in-vitro characterization of solid self nanoemulsifying drug delivery system (s-SNEDDS) of simvastatin. *J Pharm Sci Res* 7(1):40–48
- Rowe RC, Sheskey PJ, Weller PJ (2006) *Handbook of pharmaceutical excipients*, 6th edn. Pharmaceutical press, London
- Sarkar B, Hardenia S (2011) Microemulsion drug delivery system: for oral bioavailability enhancement of glipizide. *J Adv Pharm Educ Res* 1(4):195–200
- Sathali AA, Varun J (2012) Formulation, development and in vitro evaluation of candesartan cilexetil mucoadhesive microbeads. *Int J Curr Pharm Res* 4(3):109–118

- Selvam RP, Kulkarni PK (2014) Design and evaluation of self nanoemulsifying systems for poorly water soluble HIV Drug. *J PharmaSciTech* 4(1):23–28
- Selvam PR, Kulkarni PK, Dixit M (2013) Preparation and evaluation of self-nanoemulsifying formulation of efavirenz. *Ind J Pharm Edu Res* 47(1):47–54
- Shafiq S, Shakeel F (2009) Effect of labrasol on self-nanoemulsification efficiency of ramipril nanoemulsion. *Die Pharmazie-An Int J Pharm Sci* 64(12):812–817. doi:10.1016/j.japsb.2013.08.001
- Singh J, Umadevi SK, Vardhan S, Lachoriya M, Rajeswari G, Kasturibai B (2015) Solubility enhancement of candesartan cilexetil by using different hydrotropic agents. *Eur J Pharm Med Res* 2(1):339–353
- Sohn Y, Lee SY, Lee GH, Na YJ, Kim SY, Seong I, Lee BJ, Kuh HJ, Lee J (2012) Development of self-microemulsifying bilayer tablets for pH-independent fast release of candesartan cilexetil. *Die Pharmazie-An Int J Pharm Sci* 67(11): 917–924
- Soni GC, Prajapati SK, Chaudhari N (2014) Self nanoemulsion: advance form of drug delivery system. *World J Pharm Pharm Sci* 3(10):410–436
- Suresh G, Manjunath K, Venkateswarlu V, Satyanarayana V (2007) Preparation, characterization, and in vitro and in vivo evaluation of lovastatin solid lipid nanoparticles. *AAPS PharmSciTech* 8(1):E1–E9
- Sureshkumar R, Gowthamarajan K, Bhavani P (2015) Nanoemulsion for lymphatic absorption: investigation of fenofibrate nanoemulsion system for lymphatic uptake. *Int J ChemTech Res* 7(2):832–841
- Sweetman SC (2009) *Martindale: the complete drug reference*, 36th edn. Pharmaceutical press, London
- Tarkase KN, Damale PS, Kapare PS, Lagad VA (2014) Formulation and evaluation of supersaturable self nano-emulsifying drug delivery system of poorly water soluble atorvastatin calcium. *Asi J Pharm Res Dev* 2(4):22–33
- Thassu D, Deleers M, Pathak YV (2007) *Nanoparticulate drug delivery systems*. Informa Healthcare, New York
- Tiwari SB, Amiji MM (2006) Improved oral delivery of paclitaxel following administration in nanoemulsion formulations. *J Nanosci Nanotechnol* 6(8):1–7. doi:10.1166/jnn.2006.440
- Vinay CH, Ahmed MG (2015) Formulation and evaluation of mucoadhesive buccal tablets of candesartan. *J Drug Deliv Therapeutics* 1(4):369–386. doi:10.1155/2013/583536
- Vuddisa SK, Subramanian S, Raavi S (2014) Preparation and characterization of candesartan cilexetil solid lipid nanoparticulate capsules. *Int J Pharma Res Rev* 3(12):26–31
- Wadhwa J, Nair A, Kumria R (2012) Emulsion forming drug delivery system for lipophilic drugs. *Acta Pol Pharm* 69(2):179–191
- Yadav PS, Yadav E, Verma A, Amin S (2014) Development, characterization, and pharmacodynamic evaluation of hydrochlorothiazide loaded self-nanoemulsifying drug delivery systems. *Sci World J* 1–10. doi:10.1155/2014/274823.
- Yasser M, Gad S, El-sayed M, Ghorab M (2013) The effect of converting liquid valsartan SNEDDS into solid SNEDDS using different solid carriers on its performance. *Int J Bio Pharm Res* 4(12):1015–1026

Submit your manuscript to a SpringerOpen[®] journal and benefit from:

- Convenient online submission
- Rigorous peer review
- Open access: articles freely available online
- High visibility within the field
- Retaining the copyright to your article

Submit your next manuscript at ► springeropen.com
