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Assessment of brain beta-amyloid deposition in transgenic mouse models of Alzheimer's disease with PET imaging agents ^{18}F -flutemetamol and ^{18}F -florbetaben

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Abstract

Background: Although amyloid beta (A β) imaging is widely used for diagnosing and monitoring Alzheimer's disease in clinical fields, paralleling comparison between ^{18}F -flutemetamol and ^{18}F -florbetaben was rarely attempted in AD mouse model. We performed a comparison of A β PET images between ^{18}F -flutemetamol and ^{18}F -florbetaben in a recently developed APPsw mouse model, C57BL/6-Tg (NSE-hAPPsw) Korl.

Results: After an injection (0.23 mCi) of ^{18}F -flutemetamol and ^{18}F -florbetaben at a time interval of 2–3 days, we compared group difference of SUVR and kinetic parameters between the AD (n = 7) and control (n = 7) mice, as well as between ^{18}F -flutemetamol and ^{18}F -florbetaben image. In addition, bio-distribution and histopathology were conducted. With visual image and VOI-based SUVR analysis, the AD group presented more prominent uptake than did the control group in both the ^{18}F -florbetaben and ^{18}F -flutemetamol images. With kinetic analysis, the ^{18}F -florbetaben images showed differences in K1 and k4 between the AD and control groups, although ^{18}F -flutemetamol images did not show significant difference. ^{18}F -florbetaben images showed more prominent cortical uptake and matched well to the thioflavin S staining images than did the ^{18}F -flutemetamol image. In contrast, ^{18}F -flutemetamol images presented higher K1, k4, K1/k2 values than those of ^{18}F -florbetaben images. Also, ^{18}F -flutemetamol images presented prominent uptake in the bowel and bladder, consistent with higher bio-distribution in kidney, lung, blood and heart.

Conclusions: Compared with ^{18}F -flutemetamol images, ^{18}F -florbetaben images showed prominent visual uptake intensity, SUVR, and higher correlations with the pathology. In contrast, ^{18}F -flutemetamol was more actively metabolized than was ^{18}F -florbetaben (Son et al. in *J Nucl Med* 58(Suppl 1):S278, 2017).

Keywords: PET/CT imaging, Alzheimer's disease, transgenic mouse model, ^{18}F -flutemetamol, ^{18}F -florbetaben

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Background

Recently, A β imaging with ^{18}F labeled radiotracers has been widely used for patients with Alzheimer's disease (AD). ^{18}F -flutemetamol is ^{18}F labeled analogue of ^{11}C -PiB produced by GE Healthcare (Buckinghamshire, UK) [2]. It has been useful in differentiating between patients with AD and healthy subjects with high specificity (96%) and sensitivity (93%) in the detection of AD, as well as high test–retest reliability [3, 4]. ^{18}F -florbetaben is an ^{18}F labeled polyethylene glycol stilbene derivative showing high in vitro affinity and specificity for β -amyloid plaques [3].

^{18}F -florbetaben and ^{18}F -flutemetamol are widely used for the diagnosis and monitoring of AD in a routine medical field. However, there are many unknown issues regarding the difference in tracer dynamics and biodistribution between ^{18}F -flutemetamol and ^{18}F -florbetaben. Because of the difficulty conducting the direct comparison between two tracers for humans due to the weighted exposure to radiation, a preclinical animal study is a good alternative option for a baseline study.

Recently, several imaging studies using newly developed ^{18}F labeled A β PET tracers were reported in AD mouse models. In a previous study, the in vivo ^{18}F -flutemetamol binding of A β deposits was tested in various AD mouse models [5]. In old APP23 mice, significant ^{18}F -flutemetamol retention was observed in the brain. But, ^{18}F -flutemetamol did not show a outstanding advantage in APPswe-PS1dE9 and Tg2576 mice.

However, transgenic mice with various genetic backgrounds have been related with different pathologies, which make it difficult to interpret the overlapping study results [6]. Therefore, comparisons between β -amyloid imaging regarding AD mouse have to be accomplished with some caution as brain sizes and anatomic landmarks of target VOIs greatly affect accurate PET signal quantification. Until now, there has been no antecedent report comparing between ^{18}F -flutemetamol and

^{18}F -florbetaben images in an AD mouse model, so comparative conclusions draw special interest.

Herein, we tested a recently developed APPsw mouse model (C57BL/6-Tg(NSE-hAPPsw)Korl) enhancing expressing Swedish double mutation form of human APP (K670 N, M671L) under regulation of the neuron specific enolase (NSE) promoter. For this mouse model, there has been no attempt regarding its application for the evaluation of new A β imaging ligands. Hence, we performed a small animal study conducting direct comparisons between two ^{18}F labeled A β PET tracers, ^{18}F -flutemetamol and ^{18}F -florbetaben in (C57BL/6-Tg(NSE-hAPPsw)Korl) mouse model in terms of following aspects: the ability to discriminate a transgenic from a control mouse, intensity of uptake and distribution pattern in visual images, difference of static ratio and kinetic parameters, bio-distribution and correlation with neuropathologic findings.

Methods

Animals

Experiments were conducted with 7 APPsw transgenic mice (genetic background C57BL/6-Tg(NSE-hAPPsw)Korl) augmenting human APP with the Swedish double mutation (K670N, M671L) under regulation of the NSE promoter. As controls, 7 littermates with the corresponding genetic background, C57BL/6J, were used. Age and sex were matched between the two groups (mean age and mean weight: 18 weeks and 24.84 \pm 1.01 g for APPsw mice and 18 weeks and 29.20 \pm 3.49 g for C57BL/6 J control mice). The mice used in the study were donated from the Division of Laboratory Animal Resources, Korea FDA (Food and Drug safety administration, National Institute of Toxicological Research, registration number: KNL-HYD-TG0615). Details on number of animals per study group, sex, mean age and mean body weight are summarized in Table 1. Two mice from each AD and control group were sacrificed for pathology at 18 weeks

Table 1 Basic characteristics of AD transgenic and control mouse model

ID	AD transgenic			Control		
	Age (weeks)	Sex	Weight (g)	Age (weeks)	Sex	Weight (g)
1	18	Male	23.41	18	Male	27.20
2	18	Male	26.34	18	Male	27.68
3	18	Male	25.12	18	Male	31.32
4	18	Male	24.16	18	Male	26.27
5	18	Male	24.12	18	Male	36.26
6	18	Male	25.68	18	Male	27.74
7	18	Male	25.11	18	Male	27.99
Mean \pm SD	18	Male	24.84 \pm 4.8	18	Male	29.20 \pm 3.4

and correlated with imaging. The remaining mice were sacrificed for pathology at 48 weeks. Animal experiments were conducted with the approval of the institutional animal care committee (IRB number: LML 16-970, Dong-A university, Busan, Korea).

PET/CT imaging

Seven transgenic and 7 control mice underwent sequential PET imaging for direct comparison of the two tracers (total 28 scans). The time interval between ^{18}F -florbetaben and ^{18}F -flutemetamol PET imaging was 2–3 days. Inhalation anesthesia was maintained by 3.5 L/min oxygen and 0.6–2% isoflurane, 15 min prior to scanning. The body temperature was kept at 37 °C with a temperature-controlled heating pad, and the respiratory rate stayed at 80–100/min. Small animal PET data was acquired with a nanoscan PET scanner (Mediso Medical Imaging Systems, USA). After the induction of anesthesia, the animals were positioned with their heads in the center of the field of view and were fixed in the PET scanner in the prone head first position (HFP). At the beginning of the PET scanning procedure, computed tomography (CT) scans were acquired for attenuation correction and anatomical reference (50 kVp, 250 mA). Next, simultaneous with an i.v. injection of 8.51 MBq (0.23 mCi) of ^{18}F -flutemetamol or ^{18}F -florbetaben, a 90-min dynamic emission scan was started. Dynamic acquisition was performed in the 3D list mode for 90 min. The emission data were normalized and corrected for decay and dead time. The sinograms were reconstructed with FBP (filtered back-projection using a ramp filter with a cut-off at the Nyquist frequency). Static images and dynamic images with 20 imaging frames were generated.

Radiosynthesis

The radiosynthesis of ^{18}F -florbetaben (4-ethoxyphenyl vinyl)-N-methylaniline, commercial name: Neuraceq) was performed using an auto-synthesizer according to the protocol of Piramal Enterprises Ltd. The radiochemical purity was >99%, as determined by analytical HPLC. The radiochemical yield averaged 45% (decay-corrected) at the end of synthesis (EOS) based on ^{18}F -fluorine. The specific activity averaged 774 GBq/umol at the EOS. The commercial products were purchased from the company (Duchem Bio, South Korea). The radiosynthesis of ^{18}F -flutemetamol (6-Benzothiazolol, 2-[3-(^{18}F) fluoro-4-(methylamino) phenyl], commercial name: Visamyl) was performed to using an auto-synthesizer according to the protocol of GE Healthcare. The radiochemical purity was >96% as determined by analytical HPLC. The radiochemical yield averaged 27% (decay-corrected) at the end of synthesis (EOS) based on ^{18}F -fluorine. The specific activity averaged 1862 GBq/umol at the EOS. The

commercial products were purchased from the company (Carecamp Co., Ltd., South Korea).

Analysis of PET data

PET data was analyzed with the fusion toolbox embedded in PMOD version 3.7.0 software (PMOD Technologies, Zurich, Switzerland). The CT image was thresholded at 2/3 of the maximal value (approximately 1340 Hounsfield units), and the skull image was obtained. For the shape of an atlas to properly fit with the skull CT, the thresholded CT image was manually fused with the magnetic resonance brain template, called M.Mirrione. Then, the transformation information was saved in a MAT-file format. Using the Initialize/Match function of the fusion toolbox, the PET image was re-sliced to match M.Mirrione template [7]. Then, the transformation information between the thresholded CT and the mouse magnetic resonance template was loaded on re-sliced PET image. Then, the re-sliced PET image was co-registered manually using the shift, rotate and scale functions and normalized to the mouse MR brain template (M. Mirrione) [7, 8]. The final co-registered PET image was masked with the M. Mirrione brain mask. The corresponding template and mask files can be found in the resources/usertemplates directory embedded in PMOD version 3.7.0 software (Pmod Technologies, Zurich, Switzerland). The same step was applied to all frames of dynamic data.

Volumes of interest (VOIs) of embedded mouse brains are presented in Fig. 1. The areas of the VOIs are the cortex (Cor), right hippocampus (Rhip), left hippocampus (Lhip), thalamus (Thal), right striatum (Rstr), left striatum (Lstr) and the cerebellum (Crbl). To investigate the difference between ^{18}F -florbetaben and ^{18}F -flutemetamol images, different images using the image algebra option embedded in PMOD fusion tool (version 3.7.0; Pmod Technologies, Zurich, Switzerland) were created. For the analysis of static PET image, the standardized uptake value (SUV) and the standardized uptake value ratio (SUVR) between the cortex and cerebellum was calculated with a VOI based method.

To determine the optimal compartment model for amyloid specific tracers, the 2 tissue compartment model from previous studies was used [9–11]. For the 2 tissue compartment model analysis with the Image Derived Input Function (IDIF) method, 1 mm³ volumes of interest (VOIs) were drawn on the center of the left ventricle on the initial time frame image.

Pathology

Sample preparation

The animals were deeply anesthetized with zoletil and xylazine and were sacrificed by intra-cardiac perfusion with 4% paraformaldehyde (pH 7.4). The brains were

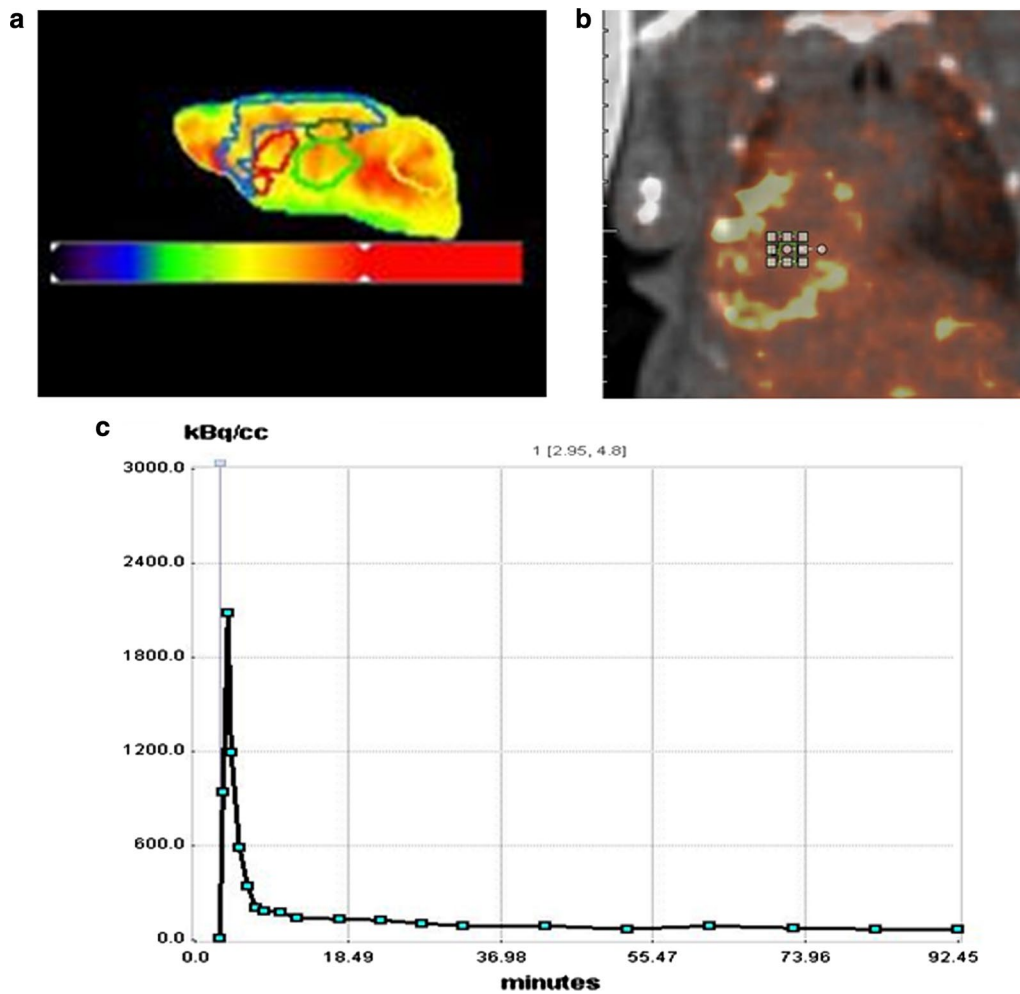


Fig. 1 **a** Volume of interest (VOI) of mouse brain. VOI was drawn under guidance of the PMOD embedded mouse brain atlas (Mouse (M. Mirrione)-T2 MRI atlas) to cover the cortex (Cor: blue), right hippocampus (Rhip: dark green), left hippocampus (Lhip: dark green), thalamus (Thal: light green), right striatum (Rstr: red), left striatum (Lstr: red) and the cerebellum (Crb: yellow), **b** volume of interest in blood input area, **c** time activity curve of blood input area

embedded in paraffin wax for 48 h. The tissue samples were serially sectioned at a thickness of 10 μ m on a rotary microtome for immuno-histochemical analysis.

Thioflavin S staining

The sections were deparaffinated and rehydrated before staining. The sections were incubated in a 1% (1 g per 100 ml water) thioflavin S (Tfs, T1892, Sigma Aldrich, St. Louis, MI, USA) solution for 30 min. The sections were washed with water three times for 2 min, 80% ethanol for 6 min, washed again with water and cover slip mounted with VectaShield as the mounting medium. The slides were stored for 4 $^{\circ}$ C. The sections were washed with water three times for 2 min and with 80% ethanol for fluorescence microscopy using filter sets for

DAPI and GFP. The DAPI (contained in the mounting medium) fluorescence was used by the scanner to set the optical focus, and the GFP contained the specific signal of thioflavin S.

Immunohistochemistry for amyloid beta 40

Non-specific reactions were blocked with 3% fetal bovine serum in phosphate buffered saline (PBS) for 1 h. Slides were incubated with mouse monoclonal primary amyloid beta 40 antibody (diluted 1:150; Millipore, USA). The secondary antibody was Streptavidin Alexa fluor 594 conjugated anti-mouse IgG (1:400, Invitrogen, USA). The fluorescence was observed using Nikon-80i fluorescence microscopy using filter sets for

DAPI and RFP. The DAPI (contained in the mounting medium) fluorescence was used by the scanner to set the optical focus, and the RFP contained the specific signal of amyloid beta 40.

Bio-distribution

The ¹⁸F-florbetaben and ¹⁸F-flutemetamol binding to different brain regions and peripheral organs in AD transgenic (N=1) and control mice (N=1) using ex vivo gamma counting. Mice were anaesthetized with isoflurane and injected with 0.23 mCi of ¹⁸F-florbetaben and ¹⁸F-flutemetamol. The tracer was allowed to distribute for 90 min. Mice were sacrificed by cervical dislocation and the brain was rapidly removed. Then, the blood, heart, lung, liver, kidney, medulla, cerebellum, right cortex, left cortex, olfactory bulb were dissected. ¹⁸F-radioactivity was measured with a gamma counter.

Statistics

For the analysis of static PET data, group comparison of SUVR and kinetic parameters were conducted with the

Mann–Whitney U. A threshold of P less than 0.05 was considered significant. All statistical analyses were performed using IBM SPSS Statistics (version 20.0; SPSS) and Medcalc 16.8.4.

Results

Comparative overview of representative visual brain PET image

A comparative overview of the representative brain PET images is presented in Fig. 2. On the ¹⁸F-florbetaben PET image, the AD transgenic mice showed significantly higher tracer retention in the cortical regions than did the control mice. On the ¹⁸F-flutemetamol PET image, the transgenic mice showed mild, focal uptake in cortical brain regions; however, higher uptake was shown in the transgenic mice than in the control mice. Overall, regardless of the AD transgenic and control group, ¹⁸F-florbetaben imaging showed much higher retention than did ¹⁸F-flutemetamol imaging. Both the AD transgenic and control groups showed high tracer retention in the cerebellum and pons than did the cortical regions.

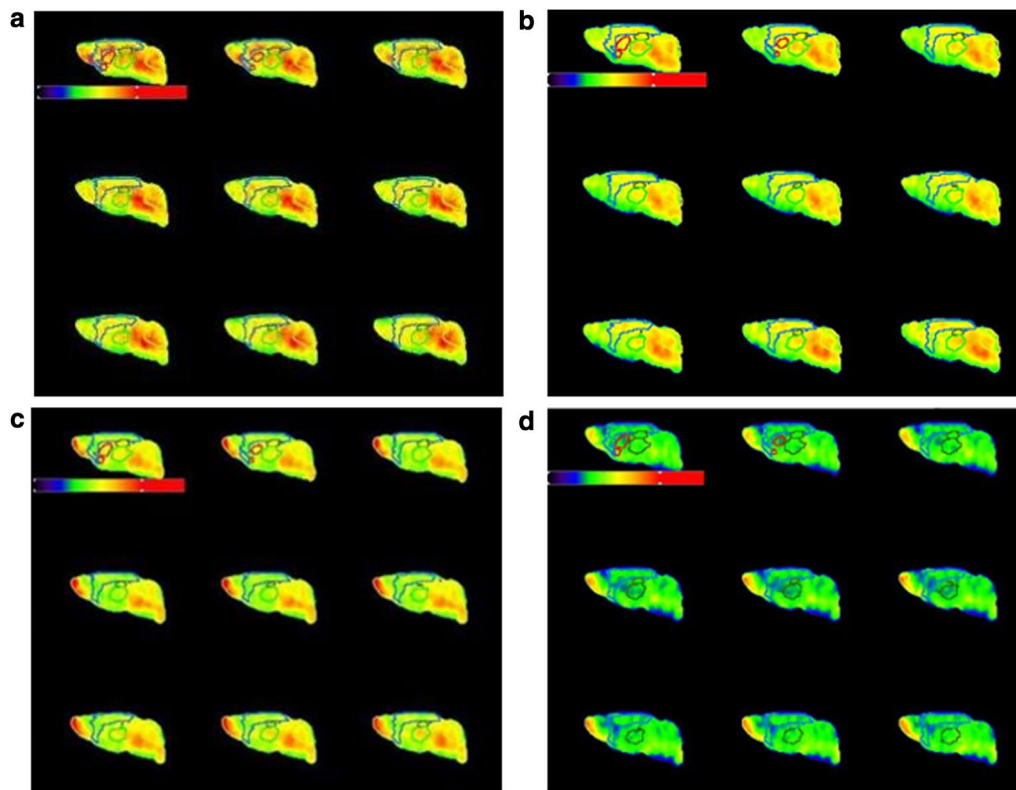


Fig. 2 Overview of PET images sorted by study group. In both AD transgenic and control group, ¹⁸F-florbetaben imaging showed much higher cortical retention than did ¹⁸F-flutemetamol imaging. Color scale bar represents (from black to red) 0–340 percentage of injected dose per cubic centimeter in ¹⁸F-florbetaben image. Color scale bar represents (from black to red) 0–259 percentage of injected dose per cubic centimeter in ¹⁸F-flutemetamol image. **a** ¹⁸F-florbetaben image of AD mouse, **b** ¹⁸F-florbetaben image of control mouse, **c** ¹⁸F-flutemetamol image of AD mouse, **d** ¹⁸F-flutemetamol image of control mouse

Difference image obtained from image algebra calculation: (^{18}F -florbetaben- ^{18}F -flutemetamol)

A visual representation of comparisons of the difference between ^{18}F -florbetaben and ^{18}F -flutemetamol is presented in Fig. 3. In the AD transgenic group, ^{18}F -florbetaben showed higher and more extensive cortical uptakes compared with ^{18}F -flutemetamol.

Comparative overview of representative visual whole body PET image

Figure 4 provides a comparative overview of the representative whole body PET images. The color bar of

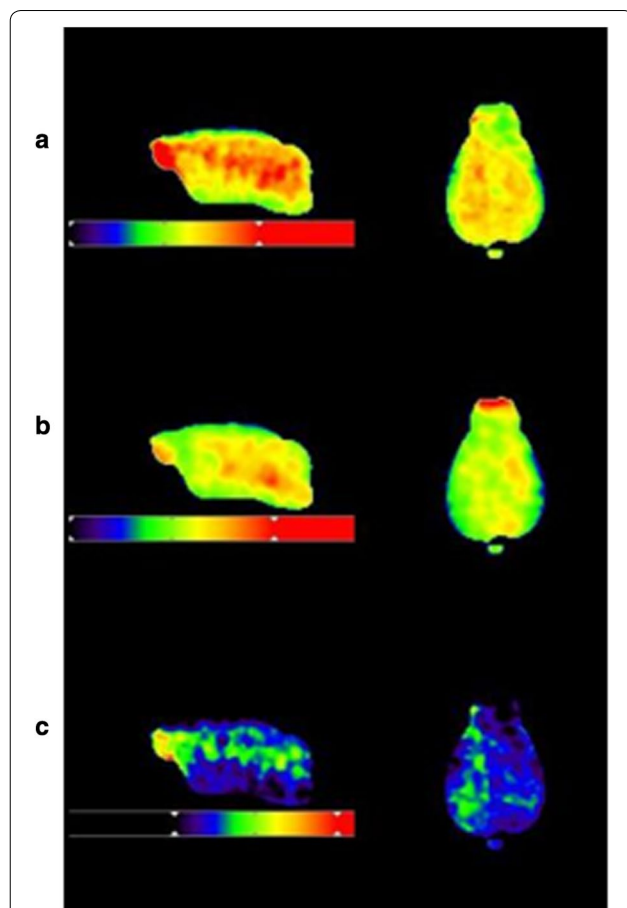


Fig. 3 Difference between ^{18}F -florbetaben and ^{18}F -flutemetamol in AD transgenic group. Each image represents PET image of **a** ^{18}F -florbetaben (upper column), **b** ^{18}F -flutemetamol (middle column) and **c** algebra calculation (^{18}F -florbetaben- ^{18}F -flutemetamol, lower column). In the AD transgenic group, ^{18}F -florbetaben showed higher and more extensive cortical uptakes compared with ^{18}F -flutemetamol. Color scale bar represents 0–340 percentage of injected dose per cubic centimeter in ^{18}F -florbetaben image. Color scale bar represents 0–270 percentage of injected dose per cubic centimeter in ^{18}F -flutemetamol image. Color scale bar represents 0–280 percentage of injected dose per cubic centimeter in difference image

the PET image was adjusted to (0–30% ID/g) to optimize for visualization of the peripheral organ uptakes. ^{18}F -flutemetamol PET imaging showed much more intense uptake in the bowel and bladder than did ^{18}F -florbetaben.

Bio-distribution

Bio-distribution data of both ^{18}F -florbetaben and ^{18}F -flutemetamol are presented in Fig. 5. The highest radioactivity in the brain was measured in the cortex, followed by the medulla and cerebellum. ^{18}F -florbetaben (Rt. cortex: 1.39 ID/g (%), Lt. cortex: 1.209 ID/g (%)) showed higher absolute differences between AD transgenic mice and control mice than did ^{18}F -flutemetamol (Rt. cortex: 0.619 ID/g (%), Lt. cortex: 0.608 ID/g (%)). In AD transgenic mouse, ^{18}F -florbetaben showed higher uptake in the cortex than did ^{18}F -flutemetamol. In addition, for both ^{18}F -florbetaben and ^{18}F -flutemetamol, the right cortex in the AD mouse showed higher uptake, showing right side laterality. In terms of the visceral distribution of ^{18}F -florbetaben, the highest radioactivity was measured in the liver, followed by the kidney, lung, blood and heart in both transgenic and control mice. In terms of visceral distribution of ^{18}F -flutemetamol, the highest radioactivity was measured in the kidney, followed by the liver, lung, blood and heart in transgenic mice. In control mice, the highest radioactivity was measured in the kidney, followed by the lung, liver, blood and heart. Comparative analysis of ^{18}F -florbetaben and ^{18}F -flutemetamol biodistribution revealed that ^{18}F -florbetaben imaging showed higher radioactivity in the cortex than did ^{18}F -flutemetamol. In contrast, ^{18}F -flutemetamol showed higher radioactivity in the kidney, lung, blood and heart, although the liver showed higher radioactivity with ^{18}F -florbetaben. In contrast with the imaging findings, the bio-distribution data showed higher uptake in the cortex than in the cerebellum.

SUVmean and SUVR based analysis of static PET image

The SUVmean and SUVR values of PET images in both the AD transgenic and control groups are presented in Tables 2, 3. The mean SUVmean values of the ^{18}F -florbetaben images in the AD and control mice were 0.804 and 0.699, respectively. In contrast, the mean SUVmean values of the ^{18}F -flutemetamol images in the AD and control mice were 0.332 and 0.297, respectively. The mean SUVR values of the ^{18}F -florbetaben images in the AD and control mice were 0.926 and 0.829, respectively. In contrast, the mean SUVR values of the ^{18}F -flutemetamol images in the AD and control mice were 0.854 and 0.687, respectively. On both the ^{18}F -florbetaben and ^{18}F -flutemetamol scans, the mean SUVmean and SUVR values of the AD transgenic group showed higher values

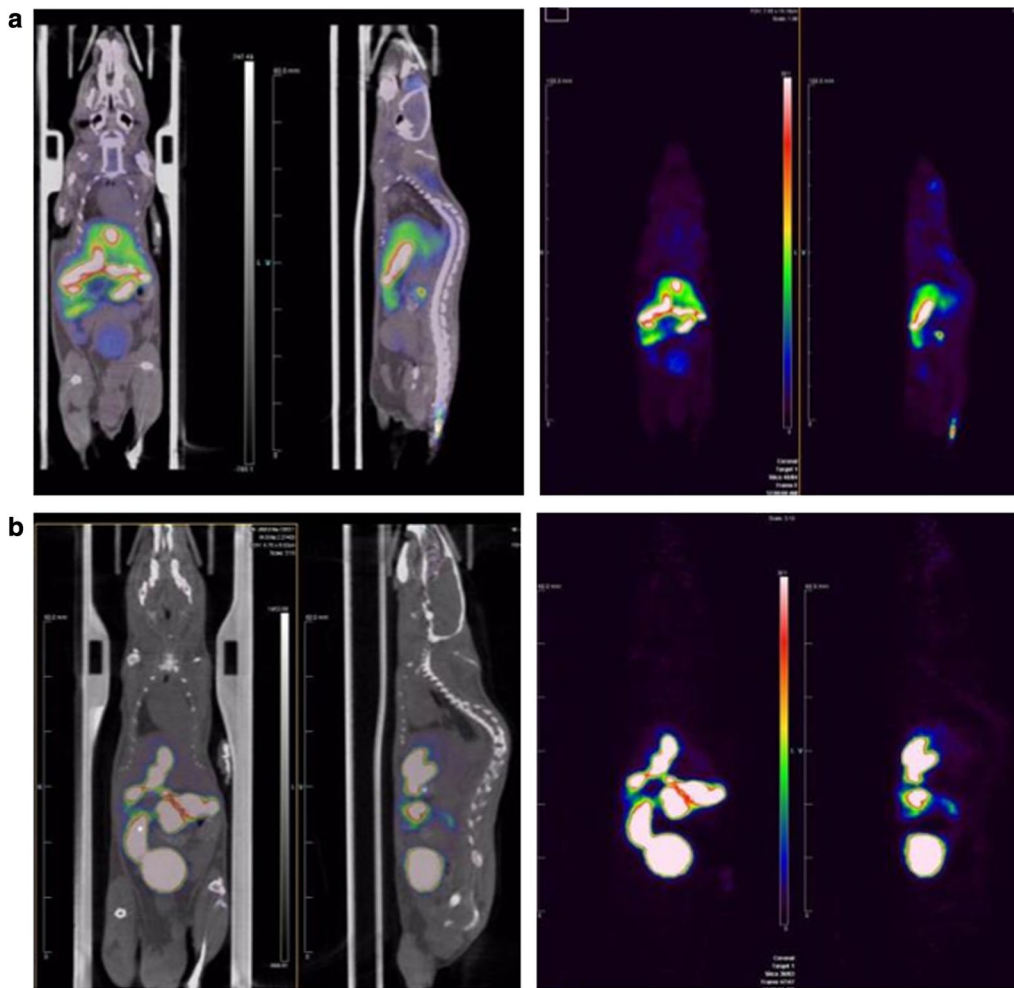


Fig. 4 Overview of representative whole body PET images of **a** ^{18}F -florbetaben and **b** ^{18}F -flutemetamol in AD transgenic mouse. ^{18}F -flutemetamol PET imaging showed much more intense uptake in the bowel and bladder than did ^{18}F -florbetaben. Each row represents a representative PET image of the study group in sagittal view (middle column) and axial view (right column). Color scale bar represents (from black to white) 0–30% ID/g (percentage of injected dose per g) in both ^{18}F -florbetaben and ^{18}F -flutemetamol image

than those of the control group. The mean SUVmean and SUVR of ^{18}F -florbetaben showed higher values than those of ^{18}F -flutemetamol in the AD transgenic and control groups, respectively. The mean of the differences in the SUVmean between the AD and control group was 0.106 for ^{18}F -florbetaben and 0.03 for ^{18}F -flutemetamol.

Statistical analysis of static PET data: AD vs. control

The quantitative parameters of the static PET images (SUVR) in the AD transgenic and control groups were tested. On the ^{18}F -florbetaben images, the AD transgenic group showed significantly higher SUVR values ($p=0.011$) than did the control group. On the ^{18}F -flutemetamol images, the AD group showed significantly higher SUVR values ($p=0.001$) than did

the control group. Moreover, on the ^{18}F -flutemetamol images, the AD group showed significantly higher SUVR values than did the control group in all brain areas. However, on the ^{18}F -florbetaben images, the AD group showed significantly higher SUVR values than did the control group only in the cortex.

Statistical analysis of static PET data: ^{18}F -florbetaben vs. ^{18}F -flutemetamol

The quantitative parameters of the static PET images (SUVR) between the ^{18}F -florbetaben and ^{18}F -flutemetamol groups are presented in Table 4. The significant differences of the SUVR (cortex/cerebellum) between the scans of the two tracers in each AD and control group were compared. ^{18}F -florbetaben presented a higher

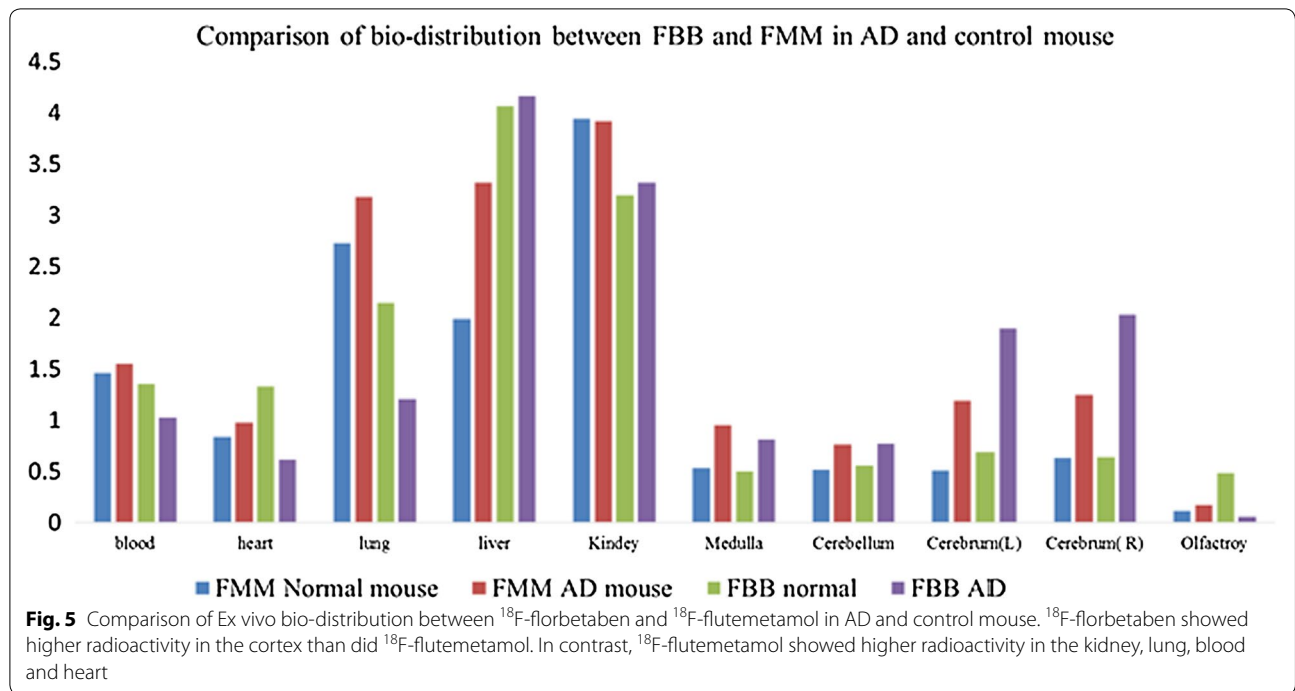


Table 2 SUVR values of ¹⁸F-florbetaben image in both AD transgenic and control group

Group	ID	Cor	Rhip	Lhip	Thala	Rstr	Lstr
<i>(a) SUVR values of ¹⁸F-florbetaben image in AD transgenic group</i>							
AD	1	0.879	0.912	0.941	1.017	0.917	0.979
	2	0.958	0.843	0.808	0.932	0.883	0.878
	3	0.929	0.988	1.004	1.083	1.015	1.014
	4	0.838	0.955	1.009	1.084	0.978	1.000
	5	0.966	0.996	0.966	1.030	0.870	0.856
	6	0.919	1.121	1.133	1.258	1.161	1.187
	7	0.994	1.074	1.133	1.216	1.071	1.144
Average		0.926	0.984	0.999	1.089	0.985	1.008
SD		0.054	0.094	0.113	0.114	0.106	0.123
<i>(b) SUVR values of ¹⁸F-florbetaben image in control group</i>							
Control	1	0.663	0.901	0.966	1.023	0.948	0.956
	2	0.852	0.964	0.957	1.025	0.932	0.962
	3	0.872	0.944	1.006	1.098	1.016	1.035
	4	0.854	1.780	1.775	1.997	1.762	1.752
	5	0.876	0.894	1.003	1.054	0.960	0.988
	6	0.822	1.000	0.989	1.085	1.000	1.012
	7	0.862	0.918	0.972	1.084	0.966	1.007
Average		0.829	1.057	1.095	1.195	1.084	1.102
SD		0.070	0.297	0.278	0.329	0.278	0.267

Cor cortex, Rhip Rt. hippocampus, Lhip Lt. hippocampus, Thala Thalamus, Rstr Rt. striatum, Lstr Lt. striatum

Table 3 SUVR values of ^{18}F -flutemetamol image in both AD transgenic and control group

Group	ID	Cor	Rhip	Lhip	Thala	Rstr	Lstr
(a) SUVR values of ^{18}F -flutemetamol image in AD transgenic group							
AD	1	0.872	0.997	1.037	1.116	1.038	1.094
	2	0.849	0.913	0.882	1.086	0.978	0.974
	3	0.922	0.991	1.064	1.147	1.035	1.144
	4	0.782	0.922	0.939	1.016	0.897	0.889
	5	0.814	0.989	0.950	1.129	0.995	0.899
	6	0.946	0.989	1.003	1.134	1.035	1.123
	7	0.792	0.880	0.933	0.933	0.791	0.837
Average		0.854	0.954	0.973	1.080	0.967	0.994
SD		0.063	0.048	0.064	0.078	0.092	0.125
(b) SUVR values of ^{18}F -flutemetamol image in control group							
Control	1	0.589	0.623	0.633	0.720	0.650	0.638
	2	0.674	0.718	0.784	0.839	0.738	0.779
	3	0.765	0.839	0.862	0.940	0.814	0.829
	4	0.684	0.743	0.773	0.837	0.764	0.762
	5	0.706	0.904	0.912	1.015	0.923	0.950
	6	0.685	0.822	0.848	0.873	0.752	0.771
	7	0.703	0.736	0.864	0.928	0.818	0.850
Average		0.687	0.769	0.811	0.879	0.780	0.797
SD		0.053	0.093	0.092	0.094	0.084	0.095

Cor cortex, Rhip Rt. hippocampus, Lhip Lt. hippocampus, Thala Thalamus, Rstr Rt. striatum, Lstr Lt. striatum

Table 4 Comparison of SUVR values between ^{18}F -florbetaben and ^{18}F -flutemetamol in AD transgenic group

Group	Cor	Rhip	Lhip	Thala	Rstr	Lstr
^{18}F -flutemetamol	0.851 ± 0.063	0.950 ± 0.051	0.972 ± 0.064	1.081 ± 0.080	0.970 ± 0.092	0.9910 ± .092
^{18}F -florbetaben	0.931 ± 0.050	0.980 ± 0.090	1.000 ± 0.110	1.090 ± 0.113	0.991 ± 0.113	1.010 ± 0.124
p value	0.049**	0.805	0.456	0.805	1.000	0.805

Cor cortex, Rhip Rt. hippocampus, Lhip Lt. hippocampus, Thala Thalamus, Rstr Rt. striatum, Lstr Lt. striatum, ** p < 0.05 considered as significant

SUVR value in the cortex than did ^{18}F -flutemetamol in both the AD ($p = 0.049$) and control groups ($p = 0.017$).

Quantitative compartment model dynamic analysis of ^{18}F -florbetaben and ^{18}F -flutemetamol image

Statistical analysis of dynamic PET data: AD versus. control

In the ^{18}F -florbetaben group, there was a significant difference in the K1 ($p = 0.011$) and k4 ($p = 0.017$) parameters between the AD transgenic and control groups. However, in the ^{18}F -flutemetamol group, there was no significant difference in K1, k2, k3, k4, K1/k2, or k3/k4 between the AD transgenic and control groups.

Statistical analysis of dynamic PET data: ^{18}F -florbetaben and ^{18}F -flutemetamol

In the AD transgenic group, there were significant differences of K1 (Table 5), k4 (Table 6), and K1/k2 between ^{18}F -florbetaben and ^{18}F -flutemetamol. In the control

group, there were differences in k3 and k3/k4 between ^{18}F -florbetaben and ^{18}F -flutemetamol.

Difference in the time-activity curve between ^{18}F -florbetaben and ^{18}F -flutemetamol

Dynamic PET time activity curves of the cortex-VOI and cerebellum-VOI for the two tracer images in representative AD and control mice are illustrated in Fig. 6. Visual inspection of the time-activity curves revealed that ^{18}F -florbetaben showed higher initial uptake and later retention than did ^{18}F -flutemetamol. In contrast, ^{18}F -flutemetamol showed lower initial upstroke and faster washout than did ^{18}F -florbetaben.

Neuropathologic findings (at 18 weeks)

Hematoxylin and eosin (H & E) staining

In Fig. 7, the AD mice show a more immature pattern as a result of disarrangement of hippocampal cell migration

Table 5 Comparison of K1 values (2 compartment model) between ¹⁸F-florbetaben and ¹⁸F-flutemetamol in AD transgenic group

Group	Rstr	Lstr	Cor	Rhip	Lhip	Thal	Crbl
¹⁸ F-flutemetamol							
Mean + SD	7.380 ± 1.032	7.331 ± 1.103	6.861 ± 1.331	6.972 ± 1.303	7.3 ± 0.900	7.841 ± 0.240	7.400 ± 1.410
Median (IQR)	7.98 (6.95–8)	8 (6.84–8)	7.52 (5.85–7.95)	7.29 (6.38–8)	7.92 (6.31–8)	7.95 (7.61–8)	8 (7.66–8)
¹⁸ F-florbetaben							
Mean + SD	4.991 ± 3.091	4.581 ± 2.960	3.561 ± 2.160	4.182 ± 2.160	4.802 ± 2.160	4.891 ± 2.160	5.060 ± 2.160
Median (IQR)	4.9 (1–8)	4.51 (1–8)	3.92 (1–4.63)	3.84 (1–7.63)	4.78 (1–7.95)	4.88 (1.18–8)	5.84 (1.65–7.61)
p-value	0.128	0.053	0.011**	0.073	0.128	0.038**	0.073

Cor cortex, Crbl cerebellum, Rhip Rt. hippocampus, Lhip Lt. hippocampus, Thala Thalamus, Rstr Rt. striatum, Lstr Lt. striatum, ** p < 0.05 considered as significant

Table 6 Comparison of k4 values (2 compartment model) between ¹⁸F-florbetaben and ¹⁸F-flutemetamol in AD transgenic group

Group	Rstr	Lstr	Cor	Rhip	Lhip	Thal	Crbl
¹⁸ F-flutemetamol							
Mean + SD	2.281 ± 3.510	1.622 ± 2.793	2.950 ± 3.210	4.551 ± 3.982	2.432 ± 3.982	1.281 ± 3.982	2.403 ± 3.982
Median (IQR)	0.331 (0.18–6.77)	0.561 (0.35–1.06)	1.752 (0.37–7.23)	7.460 (0.32–7.87)	0.340 (0.13–7.71)	0.273 (0.11–0.44)	0.374 (0–7.28)
¹⁸ F-florbetaben							
Mean + SD	0.713 ± 1.010	1.327 ± 2.290	0.161 ± 0.150	0.321 ± 0.331	0.902 ± 1.880	2.190 ± 3.102	0.140 ± 0.141
Median (IQR)	0.312 (0.22–0.92)	0.283 (0.25–2.03)	0.240 (0–0.29)	0.282 (0–0.41)	0.281 (0–0.35)	0.383 (0.21–6.15)	0.110 (0–0.3)
p-value	0.902	0.383	0.017**	0.053	0.383	0.535	0.165

Cor cortex, Crbl cerebellum, Rhip Rt. hippocampus, Lhip Lt. hippocampus, Thala Thalamus, Rstr Rt. striatum, Lstr Lt. striatum, ** p < 0.05 considered as significant

(pathogenic sign of AD) along the dentate gyrus of the hippocampus compared with the wild type.

Thioflavin S staining image

On thioflavin S staining images, Aβ deposits were found broadly in various brain regions including the cortex, hippocampus and thalamus in AD mice. Thioflavin S positive plaque areas predominantly diffuse in a morphologic characteristic nature rather than in a compact nature (Fig. 8).

Immunohistochemistry for Aβ₄₀ staining

The results of immunohistochemistry for Aβ₄₀ staining in AD transgenic and wild type were represented in Figs. 9, 10. In wild type mouse, there was no Aβ₄₀ expression in the cortex and hippocampus. In contrast, the Aa₄₀ expression of AD transgenic mouse significantly increased, correlating our H & E staining findings.

Correlation with neuropathologic findings and visual PET image

Finally, as shown in Fig. 11, the ¹⁸F-florbetaben PET images more closely correlated with the thioflavin S

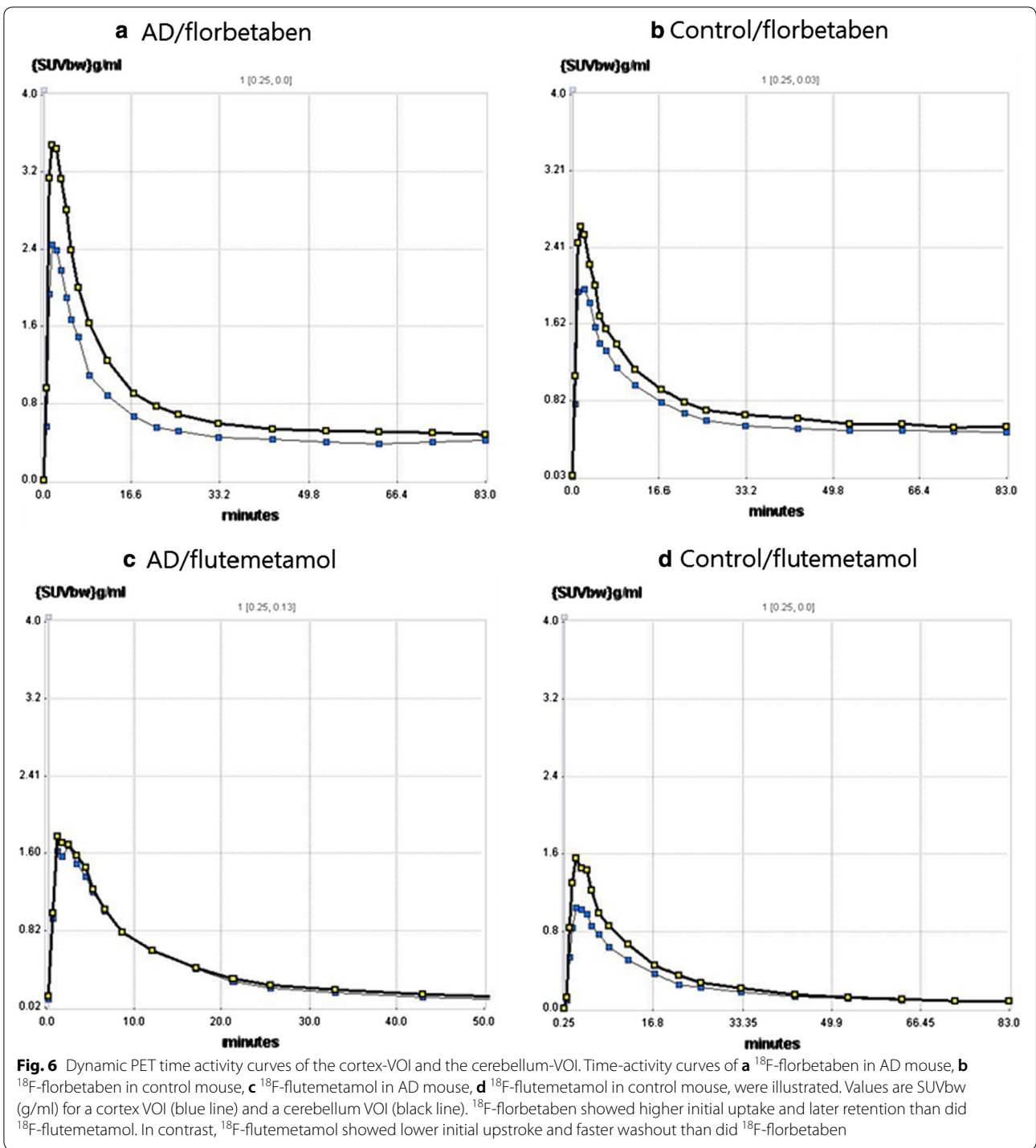
staining image in terms of spatial distribution pattern. However, the ¹⁸F-flutemetamol images revealed less prominent signal intensity and poor correlation of spatial distribution with neuropathologic plaque distribution shown in thioflavin S staining images.

Follow-up neuropathologic findings (at 48 weeks)

The results of the follow-up immunohistochemistry for Ai₄₀ staining in AD mice at 48 weeks are shown in Figs. 12, 13. At 48 weeks, AD mice showed extensive At₄₀ expression in dentate gyrus of hippocampus (CA1, CA2, CA3) and cortex, compared with the images at 18 weeks.

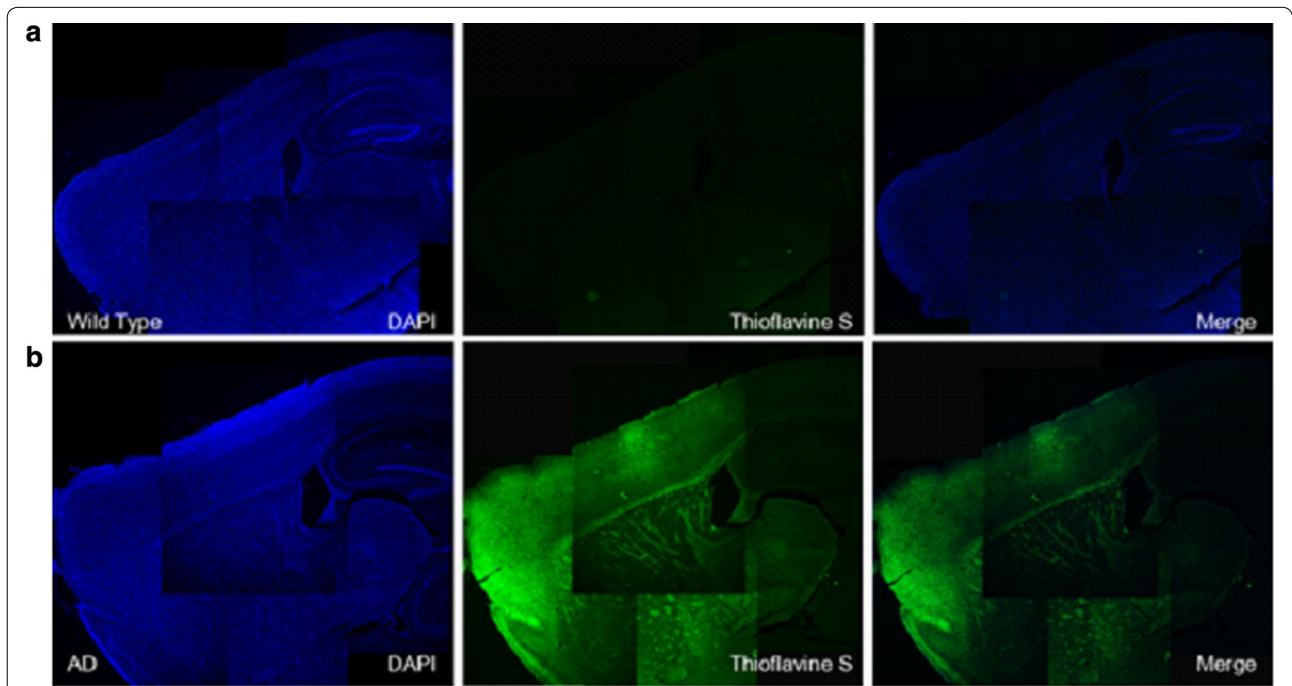
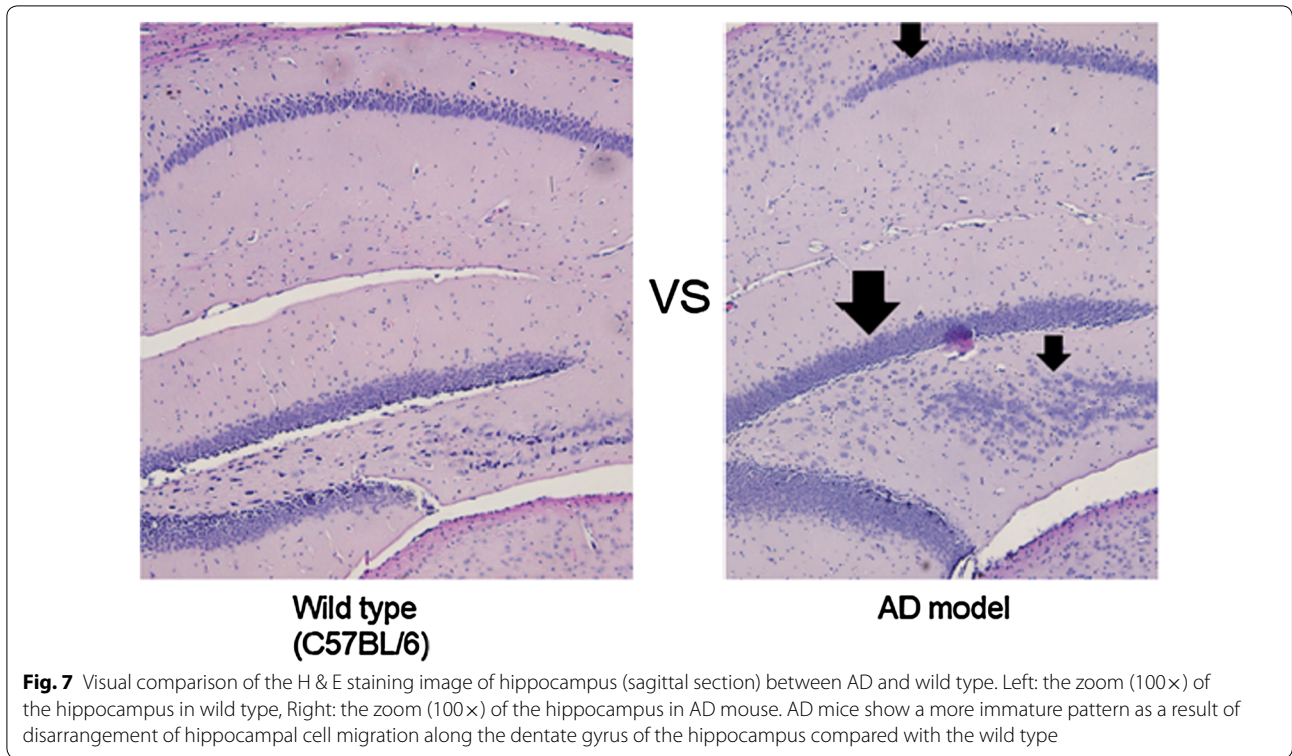
Discussion

In this study, ¹⁸F-florbetaben and ¹⁸F-flutemetamol images could differentiate AD and control group on visual and SUVR analysis. The ¹⁸F-florbetaben group presented differences in K1 and k4 kinetic parameters between AD and control groups, although ¹⁸F-flutemetamol did not show difference. Several differences emerged between ¹⁸F-florbetaben and ¹⁸F-flutemetamol. ¹⁸F-florbetaben images showed more prominent visual uptake intensity and higher SUVR than the ¹⁸F-flutemetamol images did. Moreover, ¹⁸F-florbetaben PET images more correlated well with the thioflavin S staining. However, according



to bio-distribution and kinetic results, ^{18}F -flutemetamol is more actively metabolized than is ^{18}F -florbetaben, suggesting that ^{18}F -flutemetamol has faster transport from arterial plasma into the first tissue compartment and faster dissociation from the amyloid tracer complex.

In the static analysis data, the results were grossly consistent with a previous study [12]. In another ^{18}F -florbetaben PET study, the SUVR in APPsw/PS2 at 5 months was 0.95 ± 0.04 , and the SUVR in APPsw/PS1G384A mice at 5 months was 0.93 [12]. The traditional SUVR method measures the radioactivity ratio of brain target



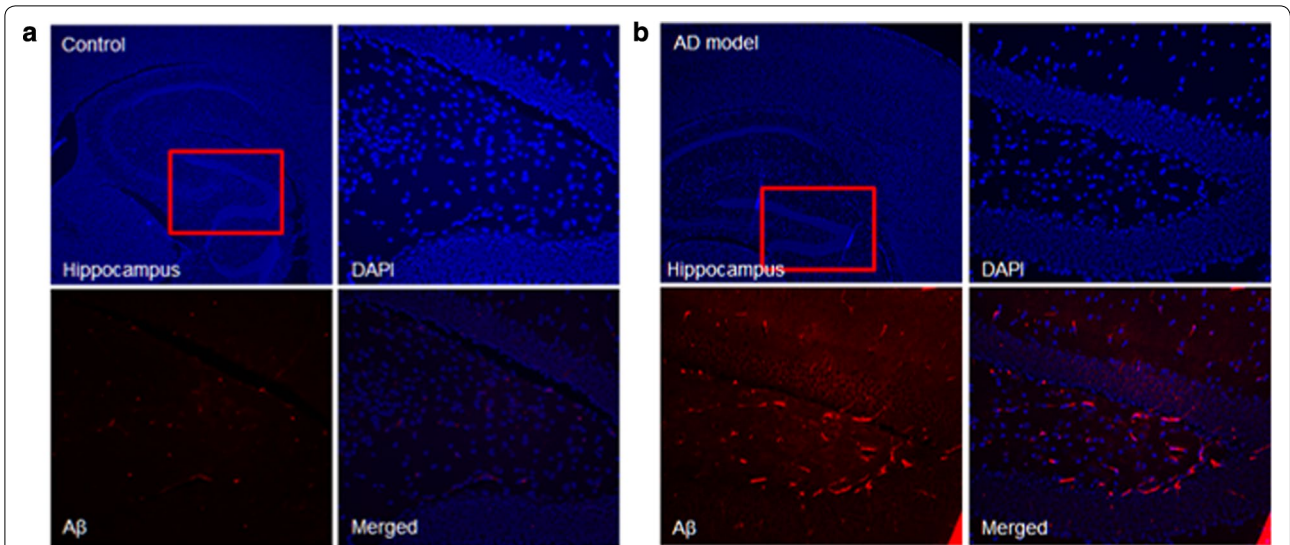


Fig. 9 Visual overview of the $A\beta_{40}$ staining images of hippocampus in **a** wild type and **b** AD mouse. In each group, right upper row shows DAPI (blue channel), Left lower panel shows $A\beta_{40}$ (RFP red channel with specific staining signal) and Right column shows merged image. In wild type mouse, there was no $A\beta_{40}$ expression in the hippocampus. In contrast, the $A\beta_{40}$ expression of AD transgenic mouse significantly increased

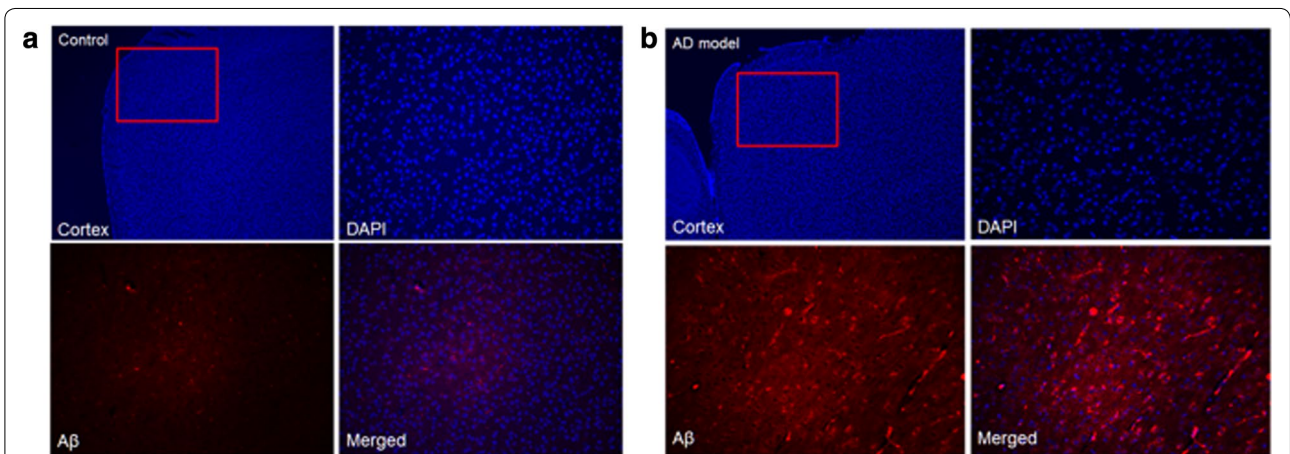


Fig. 10 Visual overview of the $A\beta_{40}$ staining images of cortex in **a** wild type and **b** AD mouse. In each group, right upper row shows DAPI (blue channel), Left lower panel shows $A\beta_{40}$ (RFP red channel with specific staining signal) and Right column shows merged image. In wild type mouse, there was no $A\beta_{40}$ expression in the cortex. In contrast, the $A\beta_{40}$ expression of AD transgenic mouse significantly increased

regions to reference tissue during a fixed time interval after injection of the tracer [11]. This relative quantitative approach for static PET data is practical for routine clinical setting. However, due to the kinetic compartment model for reversible binding radiotracers such as ^{18}F -florbetaben or ^{18}F -flutemetamol, the kinetic model reflects the available binding site density and also the perfusion signal and tracer clearance to and from brain tissue [11]. In this study, the 2 tissue compartment model with IDIF method was used, and the IDIF appears to be an attractive non-invasive alternative option obviating the need

for arterial cannulation, blood handling and analysis [13–15]. Furthermore, to avoid the effects of non-specific binding, we prolonged the uptake time, resulting in a longer wash-out of non-specifically bound tracer. A clinical protocol for ^{18}F -florbetaben involves a 90 min uptake periods [14]. A similar protocol was used in the previous APPPS1-21 mouse cohort study, allowing a 90-min uptake time [15].

The reasons for the disparity in imaging characteristics between ^{18}F -florbetaben and ^{18}F -flutemetamol are related to their chemico-physiological properties.

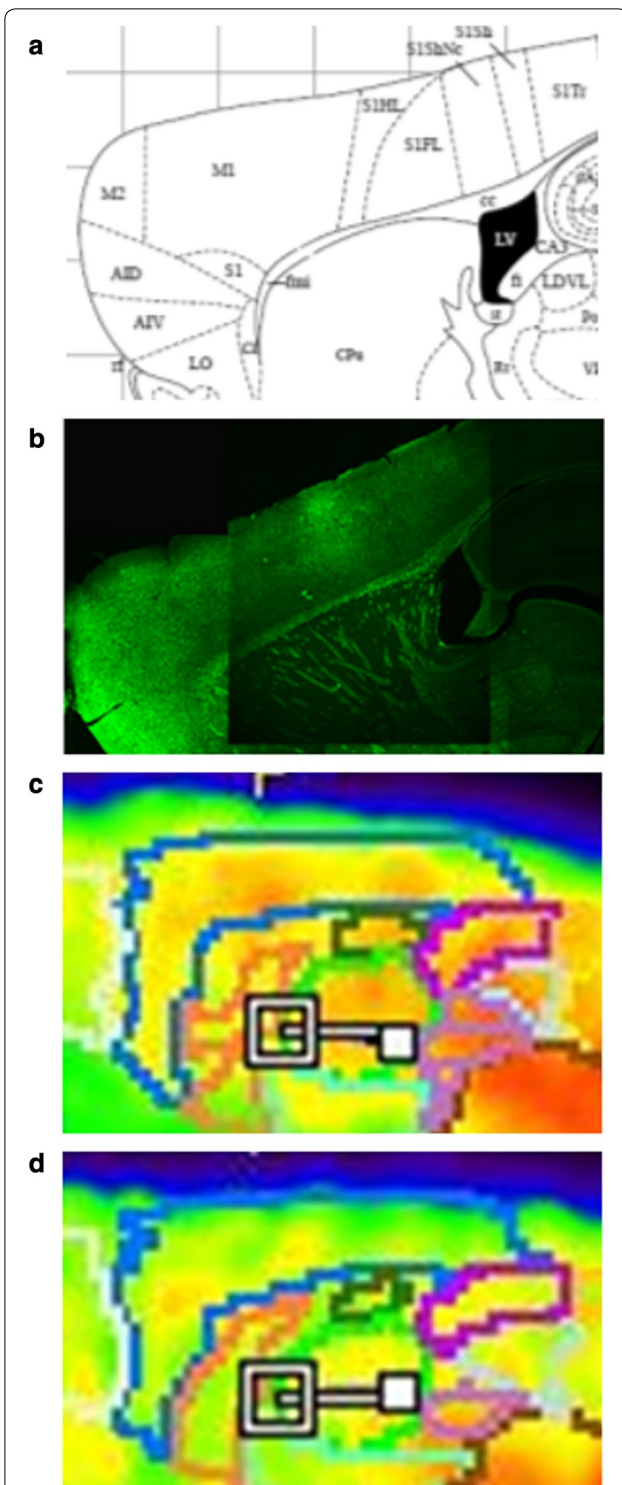


Fig. 11 Correlation with neuropathologic finding and visual PET images. **a** Paxinos and Franklin's Mouse Brain in stereotaxic coordinates atlas representing our pathological section, **b** Thioflavin S staining image, **c** ^{18}F -florbetaben image, **d** ^{18}F -flutemetamol image. The ^{18}F -florbetaben PET images matched well to the thioflavin S staining image in aspects of signal intensity and spatial distribution pattern in cortical brain regions, compared with ^{18}F -flutemetamol images

^{18}F -florbetaben and ^{18}F -flutemetamol belong to different families of imaging probes. ^{18}F -flutemetamol is a member of the thioflavin derivatives imaging probe family [16], and ^{18}F -florbetaben belongs to a different branch of imaging probe family, the trans-stilbene derivatives [16]. Because these two tracers belong to distinct chemical families, they showed differences in binding affinity. In the bio-distribution data, ^{18}F -flutemetamol showed lower brain and higher peripheral organ uptake responsible for metabolite excretion compared with ^{18}F -florbetaben. These findings and kinetic parameter results suggest that ^{18}F -flutemetamol is more actively metabolized than is ^{18}F -florbetaben. The tracer metabolites were more polar than were the parent molecules and therefore less able to enter the brain [17]. In a preclinical study comparing the pharmacokinetic characteristics of ^{18}F -flutemetamol with that of ^{11}C -PiB, the metabolism of ^{18}F -flutemetamol was faster than that of ^{11}C -PiB [18]. This finding can be explained by the higher lipophilicity of ^{18}F -flutemetamol ($\log\text{PC}_{18}=1.7$) than that of ^{11}C -PiB ($\log\text{PC}_{18}=1.2$) [19]. In another study, the lipophilicity of ^{18}F -florbetaben ($\text{Log Doct/PBS}=1.58$) was higher than that of ^{11}C -PiB ($\text{Log Doct/PBS}=1.50$) [20]. These results indirectly demonstrate that the rapid metabolism of ^{18}F -flutemetamol could be explained by the higher lipophilicity of ^{18}F -flutemetamol ($\log\text{PC}_{18}=1.7$) than of ^{18}F -florbetaben ($\text{Log Doct/PBS}=1.58$).

Previous studies reported that various transgenic animal models showed differences in binding affinity with imaging tracers and this phenomenon was thought to be related with variations in plaques configurations. In this study, 18-week-old AD transgenic mice carrying NSE-controlled APP_{swe}, C57BL/6-Tg (NSE-hAPP_{swe}) Korl were selected due to their rapid and robust amyloid plaque development at that early age [21]. In contrast, Tg2576 mice showed late onset and slower accumulation [5]. In another previous report using APP_{PS1} mice co-expressing L166P mutated Presenilin 1 under the control of a neuron-specific Thy1 promoter and KM670/671NL mutated amyloid precursor protein, cortical amyloidosis was reported at the age of 6–8 weeks [22]. In APP_{PS1}-21 mice, amyloid was known to accumulate in a 4-week and cortical microglia increased threefold from 1 to 8 months of age [22]. Hence, APP_{PS1} mice are good for investigating the mechanism of amyloidosis and treatment strategies because of their early onset of amyloid deposition and convenient cross-breeding with other genetically engineered mouse models.

In humans, the APP_{swe} gene caused early presentation of familial AD [23]. In the NSE-controlled APP_{swe} mouse model, the Swedish double mutation at the 670/671 codon in the human APP gene under the control of the NSE promoter caused increased cleavage by

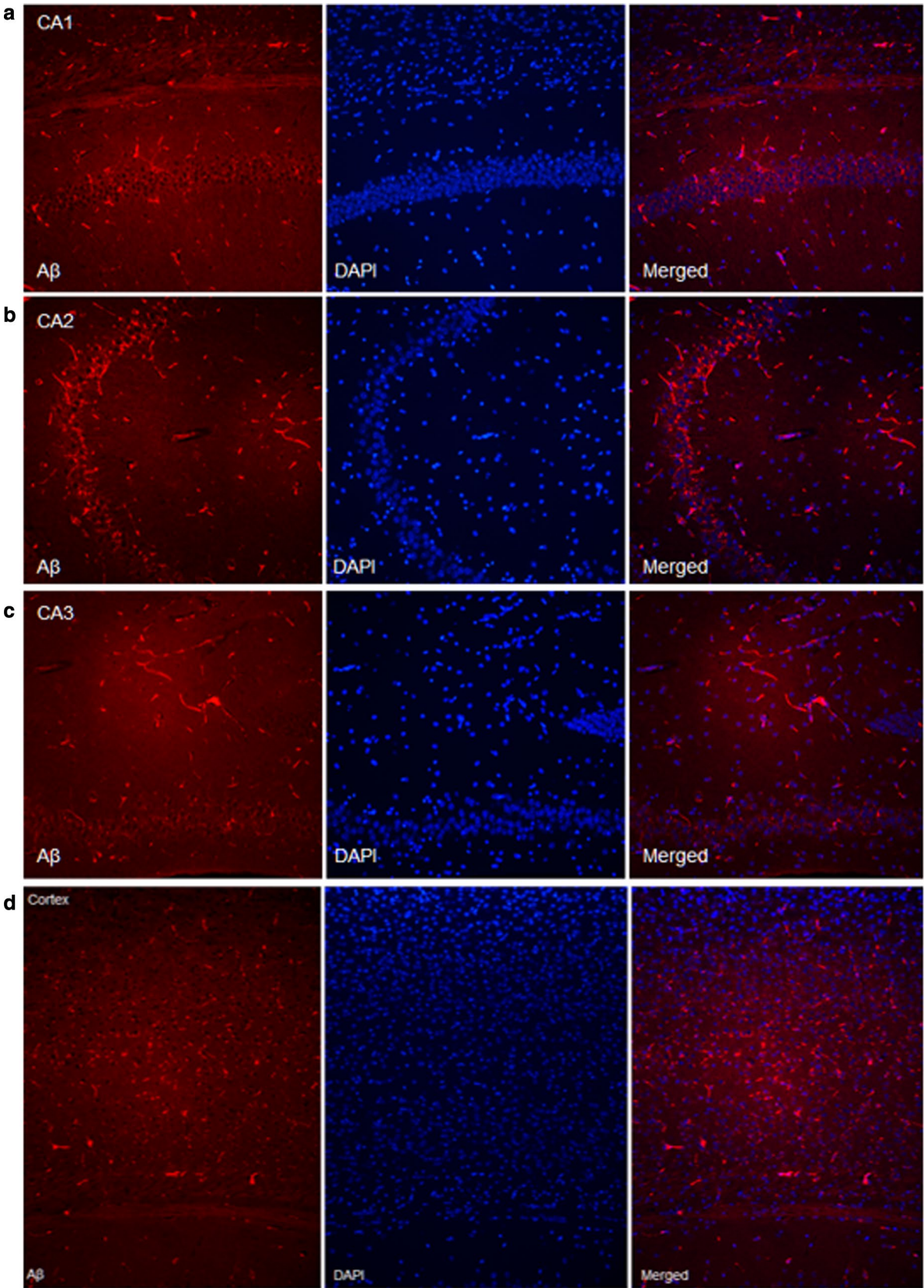
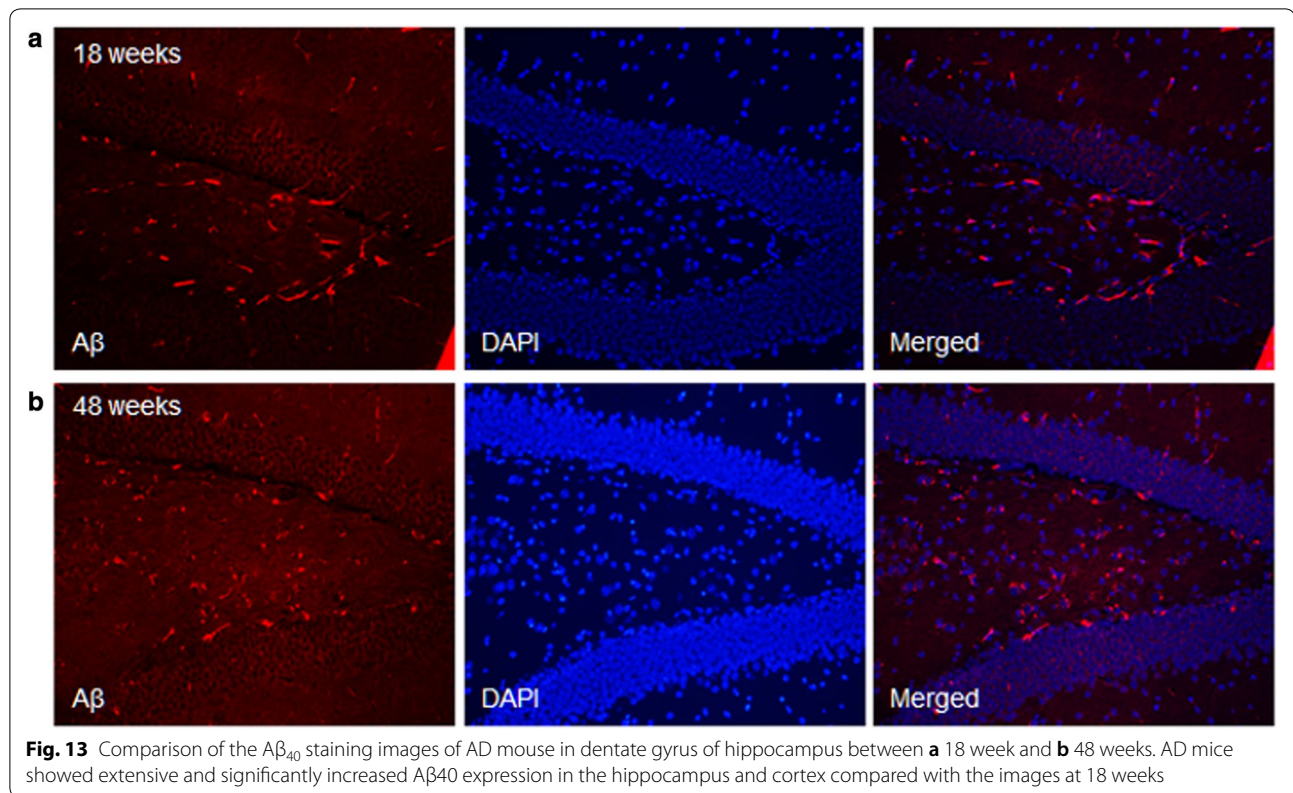


Fig. 12 Aβ₄₀ staining images of AD mouse at 48 weeks in **a** CA1, **b** CA2, **c** CA3 area of hippocampus and **d** cortex



the beta secretase and accelerated amyloid accumulation at young age [24]. Amyloid deposition in the NSE-controlled APPsw mouse induces subsequent neuronal apoptosis through the mechanisms of the mitogen-activated protein kinase (MAPK) and c-Jun N-terminal kinase (JNK) pathway or caspase-3 pathway [25, 26]. Although the mouse model in our study was relatively young, compelling evidence from previous studies regarding the dynamics of cerebral amyloidosis using a young APP mouse model indicates that NSE-augmented APPsw mice are suitable for the neuropathological phenotype of AD [27]. Moreover, we selected only male mice to control the effect of sex. Several studies reported the effect of sex on β -amyloid accumulation and AD phenotype. Latest studies have investigated the effects of sex on hippocampal atrophy in normal aging, MCI and AD [28]. Sex could regulate the relation of amyloid positivity and cognition [28]. Also, significant sex differences in pathology of 3xTg-AD mice suggested these differences may be due to organizational actions of sex hormones during development [29].

The results of this study are in contrary to those of antecedent ^{18}F -FDDNP study that presented affinity for both amyloid and neurofibrillary tangles [30]. There was no increase in cortical uptake even in 13–15-month-old Tg2576 mice, even if technical issues, such as low spatial

resolution, were regarded as the reasons for this negative PET finding [30]. However, in another ^{18}F -FDDNP study in triple-transgenic rats, previous partial volume effects were overcome and contrasting results were observed; prominent uptake was presented in the frontal cortex and hippocampus [31]. In an ^{11}C -PiB study, old Tg2576 mice showed prominent cortical binding than did control mice [9]. Those paradoxical results were explained by the confounding effects of cortical perfusion and the low distribution of ^{11}C -PiB binding sites per plaque [32]. However, following the ^{11}C -PiB study with high specific activity overcame such confounding effects, so significant cortical uptake and excellent correlation between PET uptake and a pathologic amyloid burden were observed in APP23 mice compared with age-matched healthy controls [33]. Additionally, in a recent ^{11}C -PiB PET study of APP/PS1 mice, an outstanding correlation can be found between imaging results and the plaque burden measure obtained ex vivo and in vitro in the same animals [34]. In a previous preclinical imaging study comparing ^{18}F -florbetaben and ^{11}C -PiB, which is of the same thioflavin T derivative family with ^{18}F -flutemetamol, two aged AD mouse models with contrasting levels of amyloid deposition to high (APPPS 1-21) and low (BRI 1-42) target state were investigated [15]. Compared with control mice, APPPS 1-21 mice (high target state) presented prominent

fibrillary amyloid accumulation in both ^{11}C -PiB and ^{18}F -florbetaben, but the difference of uptake between AD and control mice was higher for ^{11}C -PiB than for ^{18}F -florbetaben [15]. However, BRI1-42 mice (low target state) did not show enhanced tracer uptake [15]. Taking into consideration the difference in the mouse ages, our results broadly resemble their findings. Another ^{18}F -florbetaben study using the same mouse cohort reported only a 14.5% difference between control and transgenic mice (5XFAD) found with ^{18}F -florbetapir in comparison to a 21% difference found with ^{11}C -PiB [35].

Before the interpretation of ^{18}F -florbetaben or ^{18}F -flutemetamol images in clinical settings, preclinical approaches can provide baseline information regarding differences in the kinetic and metabolic properties of two tracers. The visual image and SUVR of ^{18}F -florbetaben showed extensive cortical uptake in the same cohorts compared with ^{18}F -flutemetamol images in both the AD and control groups. On the ^{18}F -flutemetamol images, high lipophilicity and fast metabolism might complicate the analysis of PET data. In this study, the metabolism and kinetics of the tracer also have a great influence on the visual uptake of the amyloid tracers. Using these points, the human amyloid image should be read in consideration of the pharmacokinetic and metabolic properties of the tracer. Therefore, preclinical imaging might provide valuable information about the possibilities and limits of a given approach in humans by helping to better understand the *in vivo* binding characteristics of an imaging agent. The results of this study suggest that appropriate outcome measures are important in monitoring disease progression and response to therapeutic approaches in human settings. In this study, both tracers for VOI-based ratio analysis could discriminate the AD transgenic and control groups. However, on kinetic parameters from dynamic data, ^{18}F -flutemetamol images could not be used as an indicator to distinguish between AD transgenic and control groups. Moreover, the detection of amyloid PET signal in this early aged mouse model used in this study suggests the sensitivity of the PET imaging bio-marker, suggesting the possibility of early detection of amyloid pathology before the manifestation of behavioral abnormalities.

There are several limitations that should be mentioned. First, the distribution patterns between ^{18}F -florbetaben and ^{18}F -flutemetamol were compared at a single time point. Therefore, the current data are insufficient to judge the superiority between the two tracers based. In a follow-up study, the scope of the analysis should be extended to cover the comparison of serial and chronological accumulation pattern between ^{18}F -florbetaben and ^{18}F -flutemetamol.

Second, there are some issues regarding methodological perspectives. Herein, for the shape of the merged atlas to match well with the skull CT, the thresholded CT image was manually fused with the magnetic resonance template. However, limitations could exist regarding the method of manual registration. More accurate, automatic algorithm is required in the further study. Additionally, partial volume correction was not conducted when defining the VOI in the blood input area, because the VOI size of the blood input area was larger than the volumetric PET spatial resolution (0.343 mm^3). Therefore, the effect of the partial-volume correction should be investigated in a further study.

Moreover, in further studies, the different amyloid isoform structures and the range of fibrillarity influencing PET imaging results should be investigated. Amyloid plaques can be sub-classified according to the presence of dystrophic neuritis or reactive astrocytes and the morphological features as either diffuse, fibrillary or dense core types [36, 37]. In the thioflavin S image in our study, the thioflavin S positive plaque areas were predominantly diffuse rather than compact in terms of morphologic characteristic nature. Diffuse plaques are known to occur early in the disease course and to progress towards typical cored plaques [27, 38]. Dense-core plaques are often observed in AD mouse models, at an advanced age [39]. Morphological and biochemical compositional differences of plaques can influence the affinity binding sites for amyloid imaging tracers. Between ^{18}F -florbetaben and ^{18}F -flutemetamol, which tracer has higher binding affinity to diffuse type plaques? The answer to this question should be investigated in a further study including an *in vitro* binding assay. In addition, as plaques are amorphous three-dimensional configurations, further three-dimensional analysis of plaque structures with more precise detection stringency should be required.

Moreover, we have not performed A β 1-42 staining along with the A β 1-40 staining, in the follow-up of immunohistochemistry, because we simply wanted to demonstrate the establishment of AD mouse model and regarded A β 1-40 was better choice. A β 1-40 presents the most prominent A β isoform in the AD brain, while the A β 1-42 shows a substantial increase with specific forms of AD [40, 41]. Moreover, extraordinary expressions in AD mice carrying NSE-controlled APPsw presented that A β 1-40 was more prominent than A β 1-42 in the APPsw mice [42].

Conclusion

^{18}F -florbetaben and ^{18}F -flutemetamol images could distinguish between the AD and control group by both visual and SUVR-based analysis. The ^{18}F -florbetaben

and ^{18}F -flutemetamol images showed disparate character in aspects of visual uptake intensity, quantitative parameters, bio-distribution and relations with neuropathological finding. ^{18}F -flutemetamol was more actively metabolized than was ^{18}F -florbetaben, although ^{18}F -florbetaben presented higher visual uptake intensity, SUVR and close correlation with the pathology.

Additional file

Additional file 1. SUVR values of ^{18}F -florbetaben and ^{18}F -florbetaben images in both AD transgenic and control group. (1) Basic characteristics of AD transgenic and control mouse model (2) SUVR values of ^{18}F -florbetaben image in AD transgenic group, (3) SUVR values of ^{18}F -florbetaben image in control group, (4) SUVR values of ^{18}F -flutemetamol image in AD transgenic group, (5) SUVR values of ^{18}F -flutemetamol image in control group.

Abbreviations

FBB: ^{18}F -florbetaben; FMM: ^{18}F -flutemetamol; AD: Alzheimer's disease; A β : amyloid plaque; APP: amyloid precursor protein; CSF: cerebrospinal fluid; FDG: fludeoxyglucose; MRI: magnetic resonance image; MCI: mild cognitive impairment; ND: neurodegenerative diseases; NFT: neurofibrillary tangles; PiB: Pittsburgh compound B; PET: positron emission tomography; RFP: red fluorescent protein; GFP: green fluorescent protein; APP^{swe}: Swedish APP mutation; DAPI: diamidino-2-phenylindole.

Authors' contributions

HJS got the original idea, designed the study, analyzed and interpreted data, ran the statistics and wrote the draft. HJS, SYL, GEC, JAP, MHK, KCL, YJL, MKK, YJJ, HJY, KC, DYK performed the experiments and collected the data, revised and approved the final manuscript. Also, they agreed to be accountable for all aspect of the work in ensuring that questions related to the accuracy of the work are appropriately investigated. All authors read and approved the final manuscript.

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Competing interests

The authors declare that they have no competing interests.

Availability of data and materials

All data generated or analyzed during this study are included in this published article and its additional files.

Consent for publication

Not applicable.

Ethical approval and consent to participate

Not applicable since this research did not involve human participants. All experimental procedures were approved by the institutional animal care committee (IRB number: LML 16-970, Dong-A university, Busan, Korea) and carried out in strict accordance with the Animal Welfare Act, the European

Communities Council Directive of November 24, 1986 (86/609/EEC) and the ARRIVE (Animals in Research: Reporting In Vivo Experiments) guidelines.

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References

1. Son HJ, Kang DY, Jeong YJ, Yoon HJ, Lee YJ, Kim MH, et al. Comparison analysis of brain beta-amyloid deposition in transgenic mouse models of Alzheimer's disease with PET imaging agents ^{18}F -flutemetamol and ^{18}F -florbetaben. *J Nucl Med*. 2017;58(Suppl 1):S278.
2. Henriksen G, Yousefi BH, Drzezga A, Wester HJ. Development and evaluation of compounds for imaging of beta-amyloid plaque by means of positron emission tomography. *Eur J Nucl Med Mol Imaging*. 2008;35(Suppl 1):S75–81.
3. Rinne JO, Wong DF, Wolk DA, Leinonen V, Arnold SE, Buckley C, et al. [(18)F]Flutemetamol PET imaging and cortical biopsy histopathology for fibrillar amyloid beta detection in living subjects with normal pressure hydrocephalus: pooled analysis of four studies. *Acta Neuropathol*. 2012;124:833–45.
4. Hatashita S, Yamasaki H, Suzuki Y, Tanaka K, Wakebe D, Hayakawa H. [(18)F]Flutemetamol amyloid-beta PET imaging compared with [(11)C]PiB across the spectrum of Alzheimer's disease. *Eur J Nucl Med Mol Imaging*. 2014;41:290–300.
5. Snellman A, Rokka J, Lopez-Picon FR, Eskola O, Salmona M, Forloni G, et al. In vivo PET imaging of beta-amyloid deposition in mouse models of Alzheimer's disease with a high specific activity PET imaging agent [(18)F]flutemetamol. *EJNMMI Res*. 2014;4:37.
6. Ashe KH, Zahs KR. Probing the biology of Alzheimer's disease in mice. *Neuron*. 2010;66:631–45.
7. Saigal N, Bajwa AK, Faheem SS, Coleman RA, Pandey SK, Constantinescu CC, et al. Evaluation of serotonin 5-HT(1A) receptors in rodent models using [(11)C]mefway PET. *Synapse*. 2013;67:596–608.
8. PMOD Technologies. PMOD Image fusion (PFUS): II.PMOD. version 3.8. Switzerland: PMOD Technologies Ltd; 2016.
9. Su Y, Blazey TM, Snyder AZ, Raichle ME, Hornbeck RC, Aldea P, et al. Quantitative amyloid imaging using image-derived arterial input function. *PLoS ONE*. 2015;10:e0122920.
10. Price JC, Klunk WE, Lopresti BJ, Lu X, Hoge JA, Ziolkowski SK, et al. Kinetic modeling of amyloid binding in humans using PET imaging and Pittsburgh Compound-B. *J Cereb Blood Flow Metab*. 2005;25:1528–47.
11. Becker GA, Ichise M, Barthel H, Luthardt J, Patt M, Seese A, et al. PET quantification of ^{18}F -florbetaben binding to beta-amyloid deposits in human brains. *J Nucl Med*. 2013;54:723–31.
12. Brendel M, Jaworska A, Griessinger E, Rotzer C, Burgold S, Gildehaus FJ, et al. Cross-sectional comparison of small animal [(18)F]-florbetaben amyloid-PET between transgenic AD mouse models. *PLoS ONE*. 2015;10:e0116678.
13. Zanotti-Fregonara P, Chen K, Liow JS, Fujita M, Innis RB. Image-derived input function for brain PET studies: many challenges and few opportunities. *J Cereb Blood Flow Metab*. 2011;31:1986–98.
14. Villemagne VL, Mulligan RS, Pejoska S, Ong K, Jones G, O'Keefe G, et al. Comparison of ^{11}C -PiB and ^{18}F -florbetaben for Abeta imaging in ageing and Alzheimer's disease. *Eur J Nucl Med Mol Imaging*. 2012;39:983–9.
15. Waldron AM, Verhaeghe J, Wyffels L, Schmidt M, Langlois X, Van Der Linden A, et al. Preclinical comparison of the amyloid-beta radioligands [(11)C]Pittsburgh compound B and [(18)F]florbetaben in Aged APP^{PS1-21}

- and BRI1-42 mouse models of cerebral amyloidosis. *Mol Imaging Biol*. 2015;17:688–96.
16. Rinne JO, Brooks DJ, Rossor MN, Fox NC, Bullock R, Klunk WE, et al. 11C-PIB PET assessment of change in fibrillar amyloid-beta load in patients with Alzheimer's disease treated with bapineuzumab: a phase 2, double-blind, placebo-controlled, ascending-dose study. *Lancet Neurol*. 2010;9:363–72.
 17. Snellman A, Rokka J, Lopez-Picon FR, Eskola O, Wilson I, Farrar G, et al. Pharmacokinetics of [(1)(8)F]flutemetamol in wild-type rodents and its binding to beta amyloid deposits in a mouse model of Alzheimer's disease. *Eur J Nucl Med Mol Imaging*. 2012;39:1784–95.
 18. Koivunen J, Verkoniemi A, Aalto S, Paetau A, Ahonen JP, Viitanen M, et al. PET amyloid ligand [11C]PIB uptake shows predominantly striatal increase in variant Alzheimer's disease. *Brain*. 2008;131:1845–53.
 19. Mathis C, Lopresti B, Mason N, Price J, Flatt N, Bi W, et al. Comparison of the amyloid imaging agents [F-18]3'-F-PIB and [C-11]PIB in Alzheimer's disease and control subjects. *J Nucl Med*. 2007;48:56.
 20. Yousefi BH, von Reutern B, Scherubl D, Manook A, Schwaiger M, Grimmer T, et al. FIBT versus florbetaben and PiB: a preclinical comparison study with amyloid-PET in transgenic mice. *EJNMMI Res*. 2015;5:20.
 21. Darvesh S, Cash MK, Reid GA, Martin E, Mitnitski A, Geula C. Butyrylcholinesterase is associated with beta-amyloid plaques in the transgenic APPSWE/PSEN1dE9 mouse model of Alzheimer disease. *J Neuropathol Exp Neurol*. 2012;71:2–14.
 22. Radde R, Bolmont T, Kaeser SA, Coomaraswamy J, Lindau D, Stoltze L, et al. Abeta42-driven cerebral amyloidosis in transgenic mice reveals early and robust pathology. *EMBO Rep*. 2006;7:940–6.
 23. Mullan M, Crawford F, Axelman K, Houlden H, Lilius L, Winblad B, et al. A pathogenic mutation for probable Alzheimer's disease in the APP gene at the N-terminus of beta-amyloid. *Nat Genet*. 1992;1:345–7.
 24. Irizarry MC, McNamara M, Fedorchak K, Hsiao K, Hyman BT. APPSw transgenic mice develop age-related A beta deposits and neuropil abnormalities, but no neuronal loss in CA1. *J Neuropathol Exp Neurol*. 1997;56:965–73.
 25. Troy CM, Rabacchi SA, Xu Z, Maroney AC, Connors TJ, Shelanski ML, et al. beta-Amyloid-induced neuronal apoptosis requires c-Jun N-terminal kinase activation. *J Neurochem*. 2001;77:157–64.
 26. Gamblin TC, Chen F, Zambrano A, Abraha A, Lagalwar S, Guillozet AL, et al. Caspase cleavage of tau: linking amyloid and neurofibrillary tangles in Alzheimer's disease. *Proc Natl Acad Sci USA*. 2003;100:10032–7.
 27. Hefendehl JK, Wegenast-Braun BM, Liebig C, Eicke D, Milford D, Calhoun ME, et al. Long-term in vivo imaging of beta-amyloid plaque appearance and growth in a mouse model of cerebral beta-amyloidosis. *J Neurosci*. 2011;31:624–9.
 28. Caldwell JZK, Berg JL, Cummings JL, Banks SJ. Moderating effects of sex on the impact of diagnosis and amyloid positivity on verbal memory and hippocampal volume. *Alzheimers Res Ther*. 2017;9(1):72.
 29. Carroll JC, Rosario ER, Kreimer S, Villamagna A, Gentzschlein E, Stanczyk FZ, et al. Sex differences in beta-amyloid accumulation in 3xTg-AD mice: role of neonatal sex steroid hormone exposure. *Brain Res*. 2010;1366:233–45.
 30. Kuntner C, Kesner AL, Bauer M, Kremslehner R, Wanek T, Mandler M, et al. Limitations of small animal PET imaging with [18F]FDDNP and FDG for quantitative studies in a transgenic mouse model of Alzheimer's disease. *Mol Imaging Biol*. 2009;11:236–40.
 31. Teng E, Kepe V, Frautschy SA, Liu J, Satyamurthy N, Yang F, et al. [F-18] FDDNP microPET imaging correlates with brain Abeta burden in a transgenic rat model of Alzheimer disease: effects of aging, in vivo blockade, and anti-Abeta antibody treatment. *Neurobiol Dis*. 2011;43:565–75.
 32. Saido TC, Iwatsubo T, Mann DM, Shimada H, Ihara Y, Kawashima S. Dominant and differential deposition of distinct beta-amyloid peptide species, A beta N3(pE), in senile plaques. *Neuron*. 1995;14:457–66.
 33. Maeda J, Ji B, Irie T, Tomiyama T, Maruyama M, Okauchi T, et al. Longitudinal, quantitative assessment of amyloid, neuroinflammation, and anti-amyloid treatment in a living mouse model of Alzheimer's disease enabled by positron emission tomography. *J Neurosci*. 2007;27:10957–68.
 34. Manook A, Yousefi BH, Willuweit A, Platzer S, Reder S, Voss A, et al. Small-animal PET imaging of amyloid-beta plaques with [11C]PiB and its multi-modal validation in an APP/PS1 mouse model of Alzheimer's disease. *PLoS ONE*. 2012;7:e31310.
 35. Rojas S, Herance JR, Gisbert JD, Abad S, Torrent E, Jimenez X, et al. In vivo evaluation of amyloid deposition and brain glucose metabolism of 5XFAD mice using positron emission tomography. *Neurobiol Aging*. 2013;34:1790–8.
 36. Thal DR, Capetillo-Zarate E, Del Tredici K, Braak H. The development of amyloid beta protein deposits in the aged brain. *Sci Aging Knowledge Environ*. 2006;2006:re1.
 37. Dickson TC, Vickers JC. The morphological phenotype of beta-amyloid plaques and associated neuritic changes in Alzheimer's disease. *Neuroscience*. 2001;105:99–107.
 38. Iwatsubo T, Odaka A, Suzuki N, Mizusawa H, Nukina N, Ihara Y. Visualization of A beta 42(43) and A beta 40 in senile plaques with end-specific A beta monoclonals: evidence that an initially deposited species is A beta 42(43). *Neuron*. 1994;13:45–53.
 39. Guntert A, Dobeli H, Bohrmann B. High sensitivity analysis of amyloid-beta peptide composition in amyloid deposits from human and PS2APP mouse brain. *Neuroscience*. 2006;143:461–75.
 40. Mori H, Takio K, Ogawara M, Selkoe DJ. Mass spectrometry of purified amyloid beta protein in Alzheimer's disease. *J Biol Chem*. 1992;267(24):17082–6.
 41. Naslund J, Schierhorn A, Hellman U, Lannfelt L, Roses AD, Tjernberg LO, et al. Relative abundance of Alzheimer A beta amyloid peptide variants in Alzheimer disease and normal aging. *Proc Natl Acad Sci USA*. 1994;91(18):8378–82.
 42. Hwang DY, Cho JS, Lee SH, Chae KR, Lim HJ, Min SH, et al. Aberrant expressions of pathogenic phenotype in Alzheimer's diseased transgenic mice carrying NSE-controlled APPsw. *Exp Neurol*. 2004;186(1):20–32.

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