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Magnetic Poly(N-isopropylacrylamide) Nanocomposites: Effect of Preparation Method on Antibacterial Properties

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Abstract

The most challenging task in the preparation of magnetic poly(N-isopropylacrylamide) (Fe₃O₄-PNIPAAm) nanocomposites for bio-applications is to maximise their reactivity and stability. Emulsion polymerisation, in situ precipitation and physical addition were used to produce Fe₃O₄-PNIPAAm-1, Fe₃O₄-PNIPAAm-2 and Fe₃O₄-PNIPAAm-3, respectively. Their properties were characterised using scanning electron microscopy (morphology), zeta-potential (surface charge), thermogravimetric analysis (stability), vibrating sample magnetometry (magnetisation) and dynamic light scattering. Moreover, we investigated the antibacterial effect of each nanocomposite against Gram-negative *Escherichia coli* and Gram-positive *Staphylococcus aureus*. Both Fe₃O₄-PNIPAAm-1 and Fe₃O₄-PNIPAAm-2 nanocomposites displayed high thermal stability, zeta potential and magnetisation values, suggesting stable colloidal systems. Overall, the presence of Fe₃O₄-PNIPAAm nanocomposites, even at lower concentrations, caused significant damage to both *E. coli* and *S. aureus* DNA and led to a decrease in cell viability. Fe₃O₄-PNIPAAm-1 displayed a stronger antimicrobial effect against both bacterial strains than Fe₃O₄-PNIPAAm-2 and Fe₃O₄-PNIPAAm-3. *Staphylococcus aureus* was more sensitive than *E. coli* to all three magnetic PNIPAAm nanocomposites.

Keywords: Magnetic poly(N-isopropylacrylamide), PNIPAAm, Bio-application, Escherichia coli, Staphylococcus aureus

Background

Magnetic thermoresponsive polymer nanocomposites have been used for a wide range of applications, including water treatment and nanomedicine [1-4]. Each nanocomposite is specifically designed to benefit from the combination of features inherent in both components, i.e. magnetic particles and temperature-responsive polymers, thus creating a nanocomposite that is more specific and controllable. Magnetite (Fe₃O₄) nanoparticles impart magnetic properties that allow for rapid and easy separation following application of an external magnetic field [5]. Poly(N-isopropylacrylamide) (PNIPAAm) forms a three-dimensional hydrogel that undergoes a reversible lower critical solution temperature (LCST) phase transition from a single coil with a swollen hydrated state to a collapsed and shrunken dehydrated

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state [6] when heated in water above 32 °C. Capping of the magnetic nanoparticles with a PNIPAAm layer not only provides colloidal stability in water but also allows for surface functionality by binding with other molecules, such as drugs, proteins or enzymes [7]. Construction of dual responsive nanocomposites is achieved by combining two properties that respond simultaneously to a combination of temperature and magnetism. The most common methods used for synthesis of Fe₃O₄-PNIPAAm nanocomposites are physical addition, in situ precipitation and emulsion polymerisation. Physical addition, the simplest method, requires the physical mixing of previously synthesised magnetic nanoparticles and PNIPAAm particles. The second method, in situ precipitation, involves precipitation of magnetic nanoparticles in the presence of the PNIPAAm nanopolymer [8]. The third (and most common) route, emulsion polymerisation, requires polymerisation of the (N-isopropylacrylamonomer in the presence of magnetic mide) nanoparticles [9-11]. Fe₃O₄-PNIPAAm nanocomposites have found widespread use in biomedical and



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biotechnological applications. Highly stable, controlled and well-dispersed magnetic nanoparticles will be required in order to increase the suitability of such nanocomposites for future applications. One recent innovation involves an external magnetic field that creates a local heat source for self-heating particles, causing the PNIPAAm to shrink and in turn allowing release of encapsulated drugs [12]. This phenomenon, coupled with magnetic beads targeted on tumours, opens up other potential cancer therapies such as hyperthermia. Hyperthermia can be initiated by oscillating nanoparticles in an oscillating magnetic field at frequencies ranging from kilohertz to megahertz. Other Fe₃O₄-PNIPAAm nanocomposites have recently been synthesised to control the release of bio-active molecules, such as myoglobin or vitamin B12, and for drug delivery [13]. A recent study using PNIPAAm-coated superparamagnetic Fe₃O₄ nanoparticles was able to show that thermally induced aggregation of iron oxide nanoparticles greatly increases T2 contrast during magnetic resonance imaging [14]. Clearly, Fe₃O₄-PNIPAAm shows great promise for future developments in both biomedical and biotechnological applications. Consequently, it is important that further studies are undertaken on the biocompatibility of this material and its antibacterial effect.

In this study, we investigated the effect of three preparation methods on the physical-chemical properties of Fe_3O_4 -PNIPAAm nanocomposites. In doing so, we aim to assess the most convenient preparation method for producing nanocomposites displaying enhanced properties for biological applications. For the first time, we also describe the antibacterial effects of the three Fe_3O_4 -PNI-PAAm nanocomposites using a multi-endpoint approach, bacterial growth rate, viability, cell morphology and level of DNA damage.

Methods

Chemicals

Iron(III) chloride hexahydrate (FeCl₃.6H₂O, \ge 98%), Iron(II) chloride tetrahydrate (FeCl₂.4H₂O, \ge 99%), ammonium hydroxide (26% NH₃ in H₂O), N-isopropylacrylamide (NiPAM, \ge 99%), N,N-methylenebis(acrylamide) (BIS, \ge 99%), sodium dodecyl sulphate (SDS, \ge 99%) and ammonium persulphate (APS, \ge 98.5%) were all purchased fresh from Sigma-Aldrich, Germany.

Preparation of PNIPAAm by Emulsion Polymerisation

NiPAM (4 g), BIS (0.2 g) and SDS (0.3 g) were dissolved in 350 ml of deionised water (DI) at 70 °C under atmospheric nitrogen. APS (0.0035 g) was dissolved in 1 ml of DI and added to the reaction vessel to start the reaction. After 4 h, the reaction was stopped and the prepared particles washed with DI water. Finally, the PNIPAAm nanoparticles were separated by centrifugation (12,000 rpm for 30 min) and used in further reactions.

Preparation of Magnetite (Fe₃O₄) Nanoparticles

FeCl₂·4H₂O (1.9 g) and FeCl₃·6H₂O (5.4 g) (molar ratio 1:2) were dissolved in DI (100 ml) and heated to 70 °C. Ammonium hydroxide (NH₄OH; 6 ml) was quickly added to the solution, which immediately produced a deep black magnetic precipitate. Finally, the Fe₃O₄ nanoparticle suspension was stirred for 30 min at 70 °C. The product was washed several times with DI, following which the Fe₃O₄ nanoparticles were dried in a rotary evaporator (25 mbar at 40 °C) until a fine powder was formed. This was used in all further reactions.

Preparation of Magnetic PNIPAAm Nanocomposite by Emulsion Polymerisation (Fe₃O₄-PNIPAAm-1)

NiPAM (0.4 g), freshly prepared Fe_3O_4 nanoparticles (0.2 g), BIS (0.2 g) and SDS (0.3 g) were dissolved in 350 ml of DI and heated to 70 °C under a nitrogen atmosphere. APS (0.0035 g) was then dissolved in 1 ml of DI and added to the reaction vessel to start the reaction. After 4 h, the reaction was stopped and the prepared nanocomposite washed with DI. Finally, Fe₃O₄-PNI-PAAm-1 separated by was out centrifugation (12,000 rpm for 30 min) and then dried using a rotary evaporator (25 mbar at 40 °C). The powdered material was stored in the dark at room temperature.

Preparation of Magnetic PNIPAAm Nanocomposite Through In Situ Precipitation (Fe₃O₄-PNIPAAm-2)

FeCl₂ (0.148 g), FeCl₃ (0.4 g) and 10 ml DI were mixed well and added to 1 g of PNIPAAm. NH₄OH (3 ml) was then quickly added to the solution, which immediately produced a deep black magnetic precipitate. The suspension was then stirred for 30 min at 70 °C. The prepared nanocomposite was washed with DI, following which the Fe₃O₄-PNIPAAm-2 was separated out by centrifugation (12,000 rpm for 30 min) and dried using a rotary evaporator (25 mbar at 40 °C). The resultant powder was stored in the dark at room temperature.

Preparation of Magnetic PNIPAAm Nanocomposite Through Physical Addition (Fe₃O₄-PNIPAAm-3)

Freshly prepared PNIPAAm (1 g), freshly prepared Fe_3O_4 nanoparticles (0.5 g) and DI (5 ml) were mixed well, and the resultant suspension stirred for 30 min at 70 °C. The nanocomposite thus prepared was washed with DI, following which the Fe_3O_4 -PNIPAAm-3 was separated out through centrifugation (12,000 rpm for 30 min) and dried using a rotary evaporator (25 mbar at 40 °C). The powdered material was stored in the dark at room temperature.

Nanocomposites Characterisation

The size and zeta potential of the Fe_3O_4 -PNIPAAm nanocomposites were measured following complete

dissolution of the nanoparticles in DI (dispersal in DI followed by sonification for 2 min at room temperature). Zeta potential measurements were performed using a Zetasizer Nano analyser (Malvern Instruments, USA) at pH 7. A Zetasizer Nano dynamic light scattering (DLS) unit was employed to measure the hydrodynamic diameter of particle aggregates in DI. Thermogravimetric analysis (TGA) was undertaken in order to quantify the amount of coating and to determine the nanocomposite's thermal stability. Thermal studies were undertaken on 3-4 mg of dry sample at temperatures ranging from 25 to 900 °C, using a TGA Q500 (TA Instruments, USA) under a nitrogen atmosphere (heating rate 10 °C/min). The material's magnetic properties were measured using a MicroMag[™] 2900 vibrating sample magnetometer (Princeton measurements corporation, USA). Microscopy images were obtained using a scanning electron microscope (SEM), the particles being first thoroughly dissolved in DI and a drop of the solution placed on the copper grid of a Zeiss ULTRA Plus field-emission SEM equipped with a Schottky cathode. All images were analysed using Smart SEM software v 5.05 (Zeiss, Germany) for imaging operated at 1.5 kV.

Bacterial Strains and Media

Gram-negative *Escherichia coli* CCM3954 and Grampositive *Staphylococcus aureus* CCM 3953 (Brno, Czech Republic) were used for all experiments. Detailed information on the strains is provided on the web page of the 'Czech Collection of Microorganisms' (http://www.sci.muni.cz/ccm/). Each bacterial culture was freshly prepared and held overnight in a soya nutrient broth (Sigma-Aldrich) before performing the biological experiments.

DNA Damage

Comet assays were performed following the methodology of Singh et al. [15] and Solanky et al. [16]. All chemicals were purchased from PENTA (Czech Republic) unless otherwise noted. A fresh bacterial culture (adjusted to 10^7 cells/ml) was grown overnight and then incubated with two concentrations (0.1 and 1 g/l) of PNIPAAm and each of the Fe₃O₄-PNIPAAm nanocomposites for 30 min at 37 °C.

A microgel was prepared by putting 100 ml of agarose onto the frosted surface of a slide and covering it with a 24 × 50 mm cover glass (ThermoFisher Scientific, USA). The slides were left at room temperature for 5 min, then the cover glasses were removed and the slides allowed to dry. This dried agarose layer (first layer) provided a firm base for subsequent layers. After exposing the bacteria to the PNIPAAm and Fe₃O₄-PNIPAAm nanocomposites for 30 min, 2 μ l (containing approximately 10,000 exposed cells) was taken and mixed with 100 μ l of freshly prepared 0.5% agarose. This mixture was pipetted onto

frosted slides and immediately covered with a cover glass (second layer). The slides were then cooled in a steel tray over ice. The cover glasses were removed after 1 min, and a third layer of 100 µl of lysis agarose (including 0.5% agarose with 5 µg/ml RNAse A [Ameresco, USA], 0.25% sodium N-lauroylsarcosine and 0.5 mg/ml lysozyme) was produced, again using a cover glass. The slides were then left on ice for 10 min then placed into a humid chamber for 30 min at 37 °C. After removing the cover glass, the slides were immersed in a lysing solution containing 2.5 M of NaCl, 100 mM of EDTA tetrasodium salt, 10 mM tris buffer of pH 10, 1% sodium lauroyl sarcosine and 1% triton X-100. After 1 h of lysis at room temperature, the slides were transferred to an enzyme digestion solution containing 2.5 M of NaCl, 10 mM of EDTA and 10 mM tris pH 7. Four buffer with 1 mg/ml of proteinase K. The slides were then incubated at 37 °C for 2 h, following which they were placed on the horizontal slab of an electrophoretic unit (Scie-plas, UK) and equilibrated with 300 mM of sodium acetate and 100 mM pH 9 tris buffer for 20 min then electrophoresed at 12 V (0.4 V/cm, approximately 100 mA) for 30 min. Following electrophoresis, the slides were immersed in 1 M ammonium acetate in ethanol (5 ml of 10 M ammonium acetate and 45 ml of absolute ethanol) for 20 min, absolute ethanol for 0.5 h and 70% ethanol for 10 min, after which the slides were air-dried at room temperature. To achieve uniform staining, the slides were pretreated with 50 ml of a freshly prepared solution of 5% TE buffer and 10 mM of NaH₂PO₄. The slides were then stained with 50 µl of a freshly prepared 1 mM solution of SYBR stain (Sigma-Aldrich, USA) in TE buffer for 30 min. Migration of DNA strand breaks (comets) was visualised using an AxioImager fluorescence microscope at × 400 magnification and AxioVision v 4 software (Zeiss, Germany). Typically, a tail length of 50 comets was individually measured for each sample.

Bacterial Growth Rate, Cell Viability and Morphology

The experimental protocol followed that described in Darwish et al. [17]. Briefly, a Fe_3O_4 -PNIPAAm nanocomposite stock suspension (10 g/l) was added to fresh bacterial culture in order to obtain final concentrations of 0.01, 0.05, 0.5 and 1 g/l. Each concentration was produced in triplicate in a 24-well plate. Negative controls, consisting of bacterial cells only in growth media and Fe_3O_4 -PNIPAAm nanocomposite only in growth media, were run in parallel. The plate was then incubated at 37 °C, following which the sample's optical density was measured at 600 nm (OD600) every 2 h for 6 h using a SynergyTM HTX plate reader (Biotek, USA). Bacterial growth rate was defined as the R linear regression of the OD600 measurement (absorbance units, AU) versus incubation time in hours. Preliminary measurements of nanocomposite samples without cells (6 h at 600 nm) showed constant absorbance values that did not interfere with absorbance values of nanocomposites measured with bacterial cells.

The effective concentration of nanocomposite at 10% inhibition (EC10) on bacterial growth rate (μ) was calculated for each form of Fe₃O₄-PNIPAAm based on the equation: $I(\%) = (\mu_C - \mu_T)/\mu_C \times 100$, where *I* is inhibition, μ_C

is the mean control growth rate value and μ_T is the growth rate of the culture affected by the nanocomposite [18].

After 24-h incubation, 100 µl aliquots of each sample were stained using the L7007 Bacterial Viability Kit (Molecular Probes, Invitrogen, USA) in the dark for 15 min. Determination of the proportion of live (Ex/Em 485/528 nm) and dead cells (Ex/Em 485/645 nm) was performed using a Synergy[™] HTX plate reader (Biotek, USA). The percentage of dead cells was calculated as the



Fig. 1 Scanning electron microscope images and histograms of PNIPAAm (a), Fe_3O_4 -PNIPAAm-1 (b), Fe_3O_4 -PNIPAAm-2 (c) and Fe_3O_4 -PNIPAAm-3 (d). Scale bar = 200 nm

ratio of dead to live cells. At the same time, images of *E. coli* and *S. aureus* were obtained using an AxioImager fluorescence microscope (Zeiss, Germany) with Ex/Em 470/490–700 nm. The length of *E. coli* cells and area of *S. aureus* cell clusters were determined at \times 600 magnification using AxioVision v 4 software (Zeiss, Germany).

Statistical Analysis

Differences between bacterial strains incubated in PNI-PAAm, different Fe_3O_4 -PNIPAAm nanocomposites and control samples without nanocomposites were tested using ANOVA and Dunnett's test (GraphPad PRISM, USA).

Results

In this study, we synthesised Fe_3O_4 -PNIPAAm nanocomposite employing three different protocols: emulsion polymerisation (Fe_3O_4 -PNIPAAm-1), in situ precipitation (Fe_3O_4 -PNIPAAm-2) and physical addition (Fe_3O_4 -PNIPAAm-3). SEM imaging showed that the type of protocol used had a clear effect on sample morphology and particle size, with Fe_3O_4 -PNIPAAm-1, Fe_3O_4 -PNI-PAAm-2 and Fe_3O_4 -PNIPAAm-3 showing a broad size distribution, agglomeration due to high surface energy between nanoparticles and presence of magnetic dipolar interactions (Fig. 1).

TGA indicated that the Fe₃O₄-PNIPAAm samples became relatively stable at temperatures above 400 °C (Fig. 2). Overall, PNIPAAm nanoparticles showed lower residual content than the Fe₃O₄-PNIPAAm nanocomposites. Zeta potential values for surface charge were – 1.58 mV for PNIPAAm, – 15.6 mV for Fe₃O₄-PNIPAAm1, – 16.4 mV for Fe₃O₄-PNIPAAm-2 and – 1.8 mV for Fe₃O₄-PNIPAAm-3. Vibrating sample magnetometer values for magnetisation saturation were 50.4 emu/g for Fe₃O₄-PNIPAAm-1, 53.7 emu/g for Fe₃O₄-PNIPAAm-2 and 21.0 emu/g for Fe₃O₄-PNIPAAm-3. Dynamic light scattering above (45 °C) and below (25 °C) LCST indicated a hydrodynamic size for PNIPAAm of 50 nm at 25 °C and 27 nm at 45 °C; 412 nm at 25 °C and 197 nm at 45 °C for Fe₃O₄-PNIPAAm-1; 212 nm at 25 °C and 130 nm at 45 °C for Fe₃O₄-PNIPAAm-2 and 122 nm at 25 °C and 60 nm at 45 °C for Fe₃O₄-PNIPAAm-3 (Fig. 3).

$\ensuremath{\mathsf{Fe}_3\mathsf{O}_4}\xspace{-}\ensuremath{\mathsf{PNIPAAm}}\xspace$ Nanocomposite Effect on the Bacterial DNA

Following a short exposure of 30 min, DNA strand breaks were determined for both *E. coli* and *S. aureus* in cells treated with the Fe_3O_4 -PNIPAAm nanocomposites, 40% EtOH (positive control) and untreated cells (negative control). All Fe_3O_4 -PNIPAAm nanocomposites showed a similarly significant effect (P < 0.001) on mean *E. coli* and *S. aureus* comet tail length at all concentrations (Fig. 4), compared with control cells incubated without nanocomposites.

Fe₃O₄-PNIPAAm Nanocomposite Antibacterial Effect

Growth rates indicated that Gram-positive *S. aureus* was less resistant than Gram-negative *E. coli* to all nanocomposites after 6 h exposure. Fe₃O₄-PNIPAAm-1 and Fe₃O₄-PNIPAAm-2 both strongly inhibited bacterial growth, compared with PNIPAAm and Fe₃O₄-PNIPAAm-3, with *E. coli* growth rate significantly reduced from 0.08 to 0.028 (P < 0.001) with



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Fe₃O₄-PNIPAAm-2 and 0.005 (P < 0.001) with Fe₃O₄-PNIPAAm-1 (1 g/l). No effect was observed on *E. coli* growth rate by either PNIPAAm or Fe₃O₄-PNIPAAm-3 (Fig. 5a). In comparison, the growth rate of *S. aureus* was affected by all Fe₃O₄-PNIPAAm nanocomposites and by the PNIPAAm nanoparticles. At lower concentrations (0.01 g/l and 0.05 g/l), growth rate was only slightly reduced from 0.07 to 0.06 (P < 0.05). At higher concentrations (0.5 and 1 g/l), however, there was a significant reduction from 0.07 to 0.001 with PNIPAAm, 0.0 with Fe₃O₄-PNIPAAm-1, 0.01 with Fe₃O₄-PNIPAAm-2 and 0.009 with Fe₃O₄-PNIPAAm-3 (all P < 0.001; Fig. 5b). In addition, the EC10 for all Fe₃O₄-PNIPAAm nanocomposites and

the PNIPAAm nanoparticle control was lower for *S. aureus* than that for *E. coli* (Table 1).

The percentage of dead E. coli cells increased with increasing concentration of Fe₃O₄-PNIPAAm nanocomposite after 24 h. PNIPAAm (0.5 and 1 g/l), for example, caused a significant increase in E. coli dead cells (20%) compared to cultures without Fe₃O₄-PNIPAAm nanocomposite (12%). Fe₃O₄-PNIPAAm-1 (0.5 g/l) resulted in up to 28% of dead E. coli cells and 32% at 1 g/l (P < 0.001). The effect of Fe₃O₄-PNIPAAm-2 was lower than that of Fe₃O₄-PNIPAAm-1 and Fe₃O₄-PNIPAAm-3, with the percentage of dead cells increasing from 13 to 25% when exposed to concentrations of 0.01 and 1 g/l, respectively (P < 0.001). At both 0.5 and 1 g/l, Fe₃O₄-PNI-PAAm-3 resulted in around 25% dead cells (P < 0.001; Fig. 6a). The percentage of dead S. aureus cells was only significantly affected by 1 g/l Fe₃O₄-PNIPAAm-1 and Fe₃O₄-PNIPAAm-3, with dead cells reaching up to 50 and 48%, respectively (P < 0.001). The control without nanocomposites contained approximately 18% of dead cells while in lower concentrations of PNIPAAm, Fe₃O₄-PNI-PAAm-1 and Fe₃O₄-PNIPAAm-3, the proportion of dead cells was even lower. PNIPAAm at concentrations of 0.5 and 1 g/l resulted in 25 and 30% (P < 0.005) dead cells, respectively. Fe₃O₄-PNIPAAm-2 had no effect on S. aureus cultures (Fig. 6b).

There was no difference in average *E. coli* cell length (5 µm) and average *S. aureus* cell cluster area (200 µm²) for any nanocomposite or the PNIPAAm control at lowest concentrations (0.1 g/l; Fig. 7). At higher concentrations, *E. coli* length did not change in the presence of Fe₃O₄-PNIPAAm-2, nor did *S. aureus* cell group area in the presence of Fe₃O₄-PNIPAAm-1. However, *E. coli* length was significantly increased in the presence of 1 g/l of PNIPAAm (5.4 µm, P < 0.005), Fe₃O₄-PNIPAAm-1 (6 µm, P < 0.001) and Fe₃O₄-PNIPAAm-3 (10 µm, P < 0.001) (Fig. 7a), while *S. aureus* formed larger clusters when exposed to PNIPAAm (1937 µm², P < 0.001), Fe₃O₄-PNIPAAm-2 (924 µm², P < 0.001) and Fe₃O₄-PNIPAAm-3 (1722 µm², P < 0.001) (Fig. 7b).

Discussion

Both the method of synthesis and the means by which magnetic nanoparticles were added to the polymer matrix had a clear effect on the intrinsic physical-chemical properties of the magnetic Fe_3O_4 -PNIPAAm nanocomposites. Stepwise synthesis had a strong impact on nanocomposite properties, resulting in changes to particle shape, size distribution, size and surface chemistry, along with subsequent changes in magnetic properties [19, 20]. Emulsion polymerisation (Fe₃O₄-PNIPAAm-1), an easy and precise method, produced the stable nanocomposites with narrow particle size distribution and lowest aggregation tendency,



qualities particularly important in biomedical applications [17]. Produced as a result of both steric and coulombic repulsion, the particle dimensions were sufficiently small that precipitation was avoided [21]. The least effective method was physical addition (Fe₃O₄-PNIPAAm-3). Not only was it produced via three distinct steps, and hence took longer to prepare, the resulting nanocomposite showed higher aggregation than either of the other two production methods. Moreover, our results indicated that Fe₃O₄-PNIPAAm-3 produced in this way may have contained undesirable PNIPAAm and Fe₃O₄ nanoparticle residuals.

Polymers can become attached to magnetic nanoparticles by either physical (noncovalent) or covalent bonds, with the resulting hybrid material displaying specific properties depending on the synthetic route taken. Significant re-suspension of magnetic nanoparticles takes place when preparation proceeds in the solvent in which hybrid nanoparticle formation occurs, whereupon aggregation and segregation may become a problem. In this case, in situ formation of magnetic nanoparticles may be a better alternative in many cases. In addition, if the surfactant concentration is too low, coalescence will change the size of



Table 1 The effective concentration of PNIPAAm, Fe_3O_4 -PNIPAAm-1, Fe_3O_4 -PNIPAAm-2 and Fe_3O_4 -PNIPAAm-3 nanoparticles (g/l) at 10%growth inhibition (EC10) determined for Gram-negative Escherichiacoli and Gram-positive Staphylococcus aureus

	PNIPAAm	Fe ₃ O ₄ - PNIPAAm-1	Fe ₃ O ₄ - PNIPAAm-2	Fe ₃ O ₄ - PNIPAAm-3
E. coli	0.43	0.11	0.14	0.67
S. aureus	0.10	0.05	0.04	0.06

the droplets, whereas micelles can form if the concentration is too high, leading to micellar nucleation. In this respect, it is important that the surfactant concentration is chosen carefully based on precise characterisation of surface properties and extent of particle modification, in order to ensure the inorganic particle surface is compatible with the polymer matrix.

In order to evaluate the magnetic properties of Fe_3O_4 -PNIPAAm nanocomposites, it is important to know the content of MNPs in the nanocomposite. TGA was employed to quantify amount of MNP and to investigate thermal stability of Fe_3O_4 -PNIPAAm nanocomposites compared with PNIPAAm nanoparticles alone. All three Fe_3O_4 -PNIPAAm nanocomposites displayed higher thermal stability than PNIPAAm nanoparticles, presumably due to the presence of Fe_3O_4 particles in the matrix (Fig. 2). Higher residues in magnetic nanocomposites could be attributed to the presence of inorganic Fe_3O_4 compounds in the samples, which were sustained even at higher temperatures.

 $\rm Fe_3O_4$ -PNIPAAm-1 showed highest thermal nanocomposite stability, along with the lowest weight lost. Up to 200 °C, the main source of weight loss was through loss of water and physical adsorption of the polymer layer [22]; above 200 °C, however, losses were mainly due to decomposition of the chemical layer bonding the PNIPAAm. The sample residue, which became stable above 400 °C, represented 87% of the original weight, which corresponds with the amount of magnetic nanoparticles in the nanocomposite. One aim of this preparation process was to produce a nanocomposite with magnetic properties preventing aggregation and enabling it to re-disperse rapidly as soon as the magnetic field is turned off. Such properties would allow its use in a range of different fields, including hyperthermic treatment of tumours, as contrasting agents in magnetic resonance imaging, in tissue repair, biomedical device coating, immunoassay, cell separation and biomagnetic separation of biomolecules [18, 23-26]. We tested our nanomaterials through magnetisation saturation, which assesses the maximum possible magnetisation of the substance beyond which no further change takes place despite an increase in the magnetic field. Our results showed Fe₃O₄-PNIPAAm-2 to have the highest magnetisation saturation level of the three nanocomposites tested. Our values were lower (53.7 emu/g) than those previously reported for uncoated Fe₃O₄ nanoparticles (92 emu/g) [27], however, presumably due to surface order/disorder interactions in the magnetic spin moment and an increase in

ence of the PNIPAAm polymer layer. Of special interest as regards biomedical application is the behaviour of polymer-water solutions stable below a LCST [28]. After heating the prepared Fe_3O_4 -PNIPAAm nanomaterials above the transition temperature, a coilto-globule transition occurred, followed by intermolecular association. All three Fe_3O_4 -PNIPAAm nanomaterials displayed very similar behaviour, with all shrinking as temperature increased. PNIPAAm is widely used as a thermoresponsive polymer due to the proximity of its LCST (~ 30-32 °C) to physiological temperature. Furthermore, the thermo-responsibility of PNIPAAm has proved useful for drug release in vivo [28]. Nanoscale magnetic hydrogels based on PNIPAAm

nanocomposite weight and volume due to the pres-





have now been developed for the ranostic application, with those embedded with low concentrations of Fe₃O₄ magnetic nanostructures resulting in an LCST of $\sim 40~^\circ$ C, making Fe₃O₄-PNIPAAm of especial interest for controlled drug release application [29].

SEM nanoparticle histograms displayed a broader size distribution than those using DLS (Fig. 1). Interpretation of DLS data involves the interplay of multiple parameters, however, including the size, concentration, shape, polydispersity and surface properties of the particles. Measurement of the hydrodynamic size of thermoresponsive samples in relation to temperature is a common method of characterising LCST behaviour, with nanoparticles shrinking as temperatures increase, soluble polymers precipitating and particle size increasing. As expected, PNIPAAm had a lower hydrodynamic size than the Fe_3O_4 -PNIPAAm nanocomposites. Of the nanocomposites, Fe_3O_4 -PNIPAAm-3 displayed the lowest hydrodynamic size and a narrow size distribution.

Table 2 Summary of the antimicrobial effect of PNIPAAm and three nanocomposites on *Escherichia coli* and *Staphylococcus aureus*

Endpoint Strain	PNIPAAm	Fe ₃ O ₄ - PNIPAAm-1	Fe ₃ O ₄ - PNIPAAm-2	Fe ₃ O ₄ - PNIPAAm-3
Growth rate				
E. coli	0		-	0
S. aureus	-			-
Viability				
E. coli				
S. aureus			0	
DNA damage				
E. coli	-			
S. aureus	-			

0 no effect, - significant negative effect, - - strong negative effect

Variability in hydrodynamic size is likely to be due to the presence of Fe_3O_4 nanoparticles in the PNIPAM matrix, which increases both the particle dimension and aggregation in water (Fig. 3) [8].

All Fe₃O₄-PNIPAAm nanocomposites displayed antimicrobial properties (Table 2), with both Gram-negative and Gram-positive bacteria negatively affecting *E. coli* growth rate in the order Fe₃O₄-PNIPAAm-1 > Fe₃O₄-PNIPAAm-2 > Fe₃O₄-PNIPAAm-3 = PNIPAAm and *S. aureus* growth rate as Fe₃O₄-PNIPAAm-1 > Fe₃O₄-PNI-PAAm-2 > Fe₃O₄-PNIPAAm-3 > PNIPAAm. Similarly, the antibacterial properties desired for medical applications such as biomedical device coatings and wound dressing materials have been confirmed for a number of new PNIPAAm composites, including ZnO-PNIPAAm, Ag-PNIPAAm and chitosan-PNIPAAm [23–26].

In comparison with the modified Fe₃O₄ nanomaterials described in our earlier studies, the PNIPAAm-1, PNIPAAm-2 and PNIPAAm-3 nanocomposites all showed a stronger effect on both E. coli and S. aureus, with S. aureus EC10 growth inhibition ranging from 0.04 to 0.06 g/l for the three nanomaterials, while modified APTS-, PEG- and TEOS-MNPs ranged between 0.1 and 0.25 g/l [17], and polymer-coated Fe₃O₄ (PEI-mC-, PEI- and OA-MNPs) had a value of 0.15 g/l [18]. Inhibition of bacterial growth could have been caused by several factors, including cell membrane damage, oxidative stress and cell elongation, resulting in the production of lethal cells. The cells could, on the other hand, survive such unfavourable conditions by employing repair enzymes, antioxidants and/or transient growth arrest. This could partly explain the phenomenon that in lower concentrations (0.01 and 0.05 g/l) of PNIPAAm, Fe₃O₄-PNI-PAAm-1 and Fe₃O₄-PNIPAAm-3, the proportion of dead cells of S. aureus was lower after 24-h incubation than in control where no such factor inducing mobilisation of the



defence/repair system was present. Higher concentrations of PNIPAAm and nanocomposites caused indeed significant increase in dead cells of *E. coli* and *S. aureus* corresponding well with significant decrease in growth rate of the cell cultures.

Exposure to 1 g/l of the nanocomposite resulted in changes to bacterial cell morphology, with greatest change to E. coli cell length caused by Fe₃O₄-PNIPAAm-3 > Fe₃O₄-PNIPAAm-1 > PNIPAAm > Fe₃O₄-PNIPAAm-2, and Fe₃O₄-PNIPAAm-3 > Fe₃O₄-PNIPAAm-2 > PNI- $PAAm > Fe_3O_4$ -PNIPAAm-1 for *S. aureus* clustering. This effect was also observed previously when the same bacteria were exposed to different functional magnetic nanoparticles [17]. Elongation of *E. coli* cells in the presence of nanocomposites is indicative of transient growth arrest and is evidence of an adaptive response to oxidative stress or DNA damage [30]. In the case of S. aureus, which is a biofilm formation species, the cells became embedded over a larger area than the nanocomposite-free control when exposed to PNIPAAm, Fe₃O₄-PNIPAAm-2 and Fe₃O₄-PNIPAAm-3 (Fig. 8). No S. aureus biofilm was produced when in contact with Fe₃O₄-PNIPAAm-1, possibly due to its stronger antibacterial properties. S. aureus usually produces a biofilm in harsh environments to protect the cells [31]; however, this could also have an adverse effect on the bacteria as nanocomposites can integrate through the biofilm and harm the cells, as has already been described for Pseudomonas sp. [32].

Iron could lead to DNA damage in bacterial cells as described in previous reviews [33, 34]; hence, we attempted to test whether our MNPs caused DNA damage to bacteria. The presence of Fe_3O_4 -PNIPAAm nanocomposites at both low and high concentrations (0.01 or 1 g/l) caused significant damage to *E. coli* and *S. aureus* DNA, even after short exposures (30 min). To the best of our knowledge, this is the first acute genotoxicity study of magnetic composites on bacteria; as a result, we cannot compare our results with those of other authors directly. Previous

studies have shown no genotoxicity attributable to PNIPAAm nanoparticles, however, and no decrease in cell viability when tested against two kinds of mammalian cell at nanoparticle concentrations of up to 800 mg/l [30]. On the other hand, previous genotoxicity studies on MNPs (γ -Fe₃O₄) have shown a negative effect on human fibroblast cells at 100 mg/l [35]. Studies performed with mammalian cell lines, however, cannot be directly compared to studies done with bacterial cells, due to significant differences in eukaryotic and prokaryotic cells.

Conclusions

Magnetic poly(N-isopropyl-acrylamide) nanocomposites were prepared through emulsion polymerisation (Fe₃O₄-PNIPAAm-1), in situ precipitation (Fe₃O₄-PNIPAAm-2) and physical addition (Fe₃O₄-PNIPAAm-3). Both Fe₃O₄-PNIPAAm-1 and Fe₃O₄-PNIPAAm-2 showed higher values for surface charge and thermal stability, indicating a stable colloidal system. At room temperature, Fe₃O₄-PNIPAAm-3 displayed highest magnetisation saturation. Presence of Fe₃O₄-PNIPAAm nanocomposites at both low and high concentrations caused significant damage to both E. coli and S. aureus DNA, even after short exposure, and led to a decrease in cell viability. Overall, we suggest that Fe₃O₄-PNIPAAm-1, prepared through emulsion polymerisation, is the most appropriate method for producing a magnetic nanocomposite with high antimicrobial activity towards Gram-negative E. coli and Gram-positive S. aureus.

Abbreviations

 ${\rm Fe}_3{\rm O}_4\text{-}{\rm PNIPAAm}:$ Magnetic poly(N-isopropylacrylamide); MNPs: Magnetite nanoparticles

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Authors' Contributions

NHAN designed and performed the antimicrobial tests and wrote the majority of the manuscript. MSAD performed the synthesis and characterisation of magnetite composites and participated on the manuscript text. PK assisted with SEM analysis. AŠ and IS supervised the conceptual framework and corrected the manuscript. All authors read and approved the final manuscript.

Ethics Approval and Consent to Participate

Not applicable.

Competing Interests

The authors declare that they have no competing interests.

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