

## Modulation of Blood Flow in the Skin of Human Legs during Transcutaneous Electrical Stimulation of the Spinal Cord

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**Abstract**—Changes in blood supply to the skin of the anterior-lateral surface of the shin of 12 healthy subjects were detected. The analysis was performed using laser Doppler flowmetry during transcutaneous electrical spinal cord stimulation (TSCS) by subthreshold bipolar pulses with a frequency of 30 Hz. The TSCS at  $T_7$  and  $L_1$  vertebrae level leads to a significant increase in cutaneous blood flow. With a stimulus intensity of 90% of the motor threshold, the increase in skin perfusion during stimulation at  $L_1$  was about 74%, and during stimulation at  $T_7$ , 38%, relative to the baseline. We suggest that vasodilation and hyperemia of the skin during TSCS occur mainly due to the antidromic stimulation of sensory nerve fibers. Nitric oxide (NO) is an important modulator that promotes vasodilation in TSCS. It is released by the nerve endings and the layer of endothelial cells. Inhibition of cystathionine- $\gamma$ -lyase significantly reduces the increase in skin blood flow during TSCS. Therefore, it was concluded that  $H_2S$ , as well as NO, is also involved in the vasodilation in the skin during TSCS.

**Keywords:** cutaneous blood flow, transcutaneous electrical stimulation of the spinal cord, microcirculation index, nitric oxide, hydrogen sulfide

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The spinal level of regulation of vascular tone is critical for regulating the metabolism of organs and tissues and for the functioning of the cardiovascular system (CVS) in general. The centers of the sympathetic nervous system are located in the thoracic and lumbar spinal cord, innervating the smooth muscle cells of blood vessels, as well as modulating the activity of neurons of the cervical nodes and affecting the work of the heart. A spinal cord injury in humans is accompanied by severe multiple dysfunctions of CVS functions: hypotension, hypothermia, dysregulation of coronary blood flow, orthostatic hypotension, and circulatory disorders in the skin [1].

Experimental studies of spinal mechanisms of regulation of peripheral blood circulation in humans, as a rule, are carried out exclusively in clinical conditions, with the participation of patients. Such studies involving healthy people were unavailable for ethical reasons until recently. The development of the method of transcutaneous electrical spinal cord stimulation (TSCS) of a person [2] removed this limitation, since the most important advantage of this method is the absolute non-invasiveness and, consequently, the absence of infectious and hardware complications [3]. It has been proven that TSCS selectively affects neural networks at different levels of the spinal cord [4].

Previously, we examined the mechanisms of regulation of peripheral blood flow in humans, in which neural networks of the lumbar spinal cord are involved. For this purpose, TSCS was used at the level of the  $T_{11}$ – $T_{12}$  and  $L_1$ – $L_2$  vertebrae and blood flow was recorded in the skin of the toes and the skin of the shin [5, 6]. The skin as a tissue for assessing the effects of TSCS on blood flow was chosen not only because of the convenience of the study, but also because all types of microcirculatory blood flow regulation are present in the skin and the local mechanisms of its modulation are well studied [7]. It has been proved that nitric oxide (NO) is involved in the dilatation of skin vessels during electrical stimulation of the spinal cord [6, 8]. However, the question of the source of this NO is not yet resolved: there is no convincing evidence whether NO has neuronal or endothelial origin.

In recent years, it has been shown that in addition to NO, an important role in modulating blood flow in the skin is played by hydrogen sulfide ( $H_2S$ ), which is a potent vasodilator [9]. Two enzymes producing  $H_2S$  were found in the wall of skin vessels: cystathionine- $\gamma$ -lyase and 3-mercaptopyruvate sulfurtransferase. These enzymes are localized in the cytosol or in the mitochondria of blood vessel cells [10]. In addition, the level of  $H_2S$  in the skin can also be increased non-enzymatically from various forms of storage of sulfur,

such as thiosulfate, thiocysteine and sulfite [10]. In addition, it became known that there are complex relationships between these two gas transmitters (NO and H<sub>2</sub>S) that can increase or decrease the vasodilation effect [9].

It was shown that electrical stimulation of the spinal cord at the lumbar [11] and at the thoracic level [12] causes the same vasomotor effect in patients with spinal cord injury. It prevents orthostatic hypotension and normalizes blood circulation in the cerebral vessels. One of our tasks was to compare the spinal mechanisms of regulation of peripheral blood circulation in humans, implemented at the lumbar and thoracic level.

In this connection, the following tasks were set in this study: (1) to study the characteristics of the reactions of the microcirculatory bed of the tibial skin in healthy volunteers during TSCS of the segments located at different levels of the spinal cord: in the thoracic region (level of the  $T_7$ – $T_8$  vertebrae) and in the lumbar region (level of the  $L_1$ – $L_2$  vertebrae), (2) to determine the source (s) of NO in the skin, which promotes vasodilation and hyperemia in TSCS, and (3) to study the role of H<sub>2</sub>S in TSCS-induced skin hyperemia.

## METHODS

The study involved 12 volunteers aged 24–45 years (7 men, 5 women). All of them were healthy, had no cardiovascular or metabolic diseases, did not take any medications, and did not smoke during the previous day. The temperature in the room in which the study was conducted was maintained at 22–23°C.

Stimulating electrodes (cathodes) were placed cutaneous, along the midline of the spine, at two levels between the spinous processes of the adjacent vertebrae  $T_7$ – $T_8$  (hereinafter, level  $T_7$ ) and  $L_1$ – $L_2$  (hereinafter, level  $L_1$ ); the anodes were placed above the iliac crests. The technique of carrying out TSCS and the equipment used were described in detail earlier [6]. At the first stage, the motor threshold (MT) was determined. MT is the minimum intensity of the current causing motor responses of the leg muscles to single monopolar impulses of 1 ms duration upon stimulation of each of the two levels of the spinal cord. The MT varied from 45 to 110 mA in different volunteers. Surface electromyography (EMG) was used to determine the motor response. The activity of m. biceps femoris, m. rectus femoris, m. gastrocnemius lateralis, and m. tibialis anterior was registered in both legs. EMG activity was recorded using H124SG electrodes (Covidien-ARBO-Kendall, Germany), A-M Systems (AM-Systems, United States) and the Lab Chart software (ADInstruments, United States).

After evaluating the MT using the multifunctional LACC M laser diagnostic complex (LAZMA, Russia), we determined the microcirculation index (MI, which

is blood flow (perfusion of tissue by blood) per unit time in the probed volume, measured in perfusion units, units PU). This is initial blood flow in the skin of the anterolateral surface of the lower third of the shin. Laser Doppler flowmetry (LDF) has a number of advantages compared to other methods for assessing blood flow in the skin: the signal is continuous, has a good temporal resolution, the measurement area is very small (high spatial resolution), the method measures blood flow at a shallow depth, i.e. only in the skin, without affecting the subcutaneous structures with their specific blood supply [7, 13]. The impact of the continuous TSCS on the  $T_7$  and  $L_1$  levels on the blood flow was registered after the recording of the initial blood flow. The bipolar pulses with a frequency of 30 Hz, filled with a frequency of 5 kHz, were used; the duration of the series is 1 min. A current intensity of 30, 60, and 90% of the individual MT was used.

In the final part of the work, the mechanisms of blood flow regulation activated in TSCS were investigated. The following substances were used: 7-nitroindazole (7-NI) (Sigma-Aldrich, United States), which is a selective inhibitor of neuronal synthase NO, and DL-propargylglycine (PAG) (Sigma-Aldrich, United States), which is an irreversible inhibitor of the cystathionine- $\gamma$ -lyases. 7-NI and PAG were dissolved in distilled water. The drugs were introduced into the skin iontophoretically, and the Elfor-Prof electrophoresis apparatus (Nevoton, Russia) was used. The current strength during iontophoresis was 1 mA, the duration of iontophoresis was 2 minutes. The effect of the iontophoresis with 0.9% NaCl solution with the indicated current strength on the skin blood flow was analyzed previously. Iontophoresis of a 0.9% NaCl solution for 2–3 min did not cause significant changes in skin blood flow parameters. Upon completion of 7-NI or PAG iontophoresis, continuous TSCS was performed according to the protocol used in the second stage of the study. LDF-gram (LDF recording of blood flow in the skin) was recorded for 2 min before iontophoresis and for 1 min after 7-NI or PAG iontophoresis.

The LDF-grams were mathematically analyzed with the standard software provided with the LACC M complex (version 3.0.2.376). To analyze the amplitude-frequency characteristics, a wavelet transform was used, which was carried out by a program supplied by the manufacturer with the device. The wavelet analysis of LDF-grams allows us to estimate the amplitude of blood flow fluctuations in different frequency ranges and to calculate the values of neurogenic, myogenic, or endothelium-dependent components in the general tone of the studied blood vessels of the skin [13]. Statistical data processing was performed using Microsoft Excel tables and the Statistica for Windows v.10 software package. The results of the analysis are presented by mean values of data (M) and values of standard error. The normality of the distribution of the obtained data was determined by the Shap-

**Table 1.** Microcirculation index (MI) in the shin skin during the continuous TSCS at the  $T_7$  and  $L_1$  levels

TSCS intensity	MI in the rest, pf units	MI, $T_7$ , pf units	MI, $L_1$ , pf units
30% MT	$7.24 \pm 0.37$	$8.02 \pm 0.51$	$8.95 \pm 0.43^*$
60% MT	$7.24 \pm 0.37$	$8.77 \pm 0.54^*$	$10.19 \pm 0.53^\#$
90% MT	$7.24 \pm 0.37$	$9.97 \pm 0.54^\#$	$12.63 \pm 0.62^\#$

Blood flow in the skin is presented in perfusion units (pf. unit); the differences are significant: \*  $p < 0.05$  compared to the level of perfusion at rest,  $^\# p < 0.01$  compared to the level of perfusion at rest.

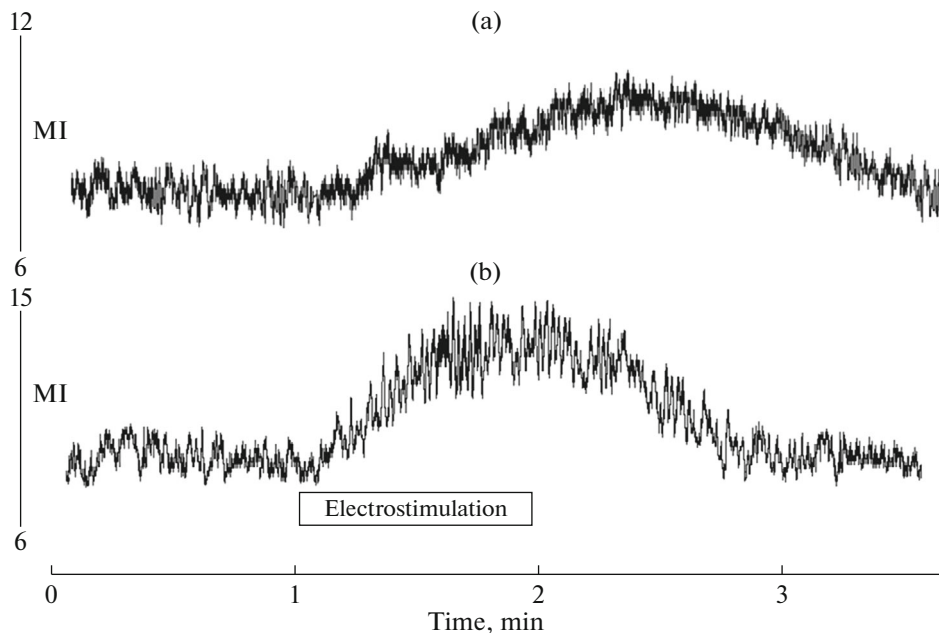
iro–Wilk  $W$  test. The statistical significance of differences in the means was estimated basing on Student's  $t$  test. The results were considered statistically significant for  $p < 0.05$ .

## RESULTS

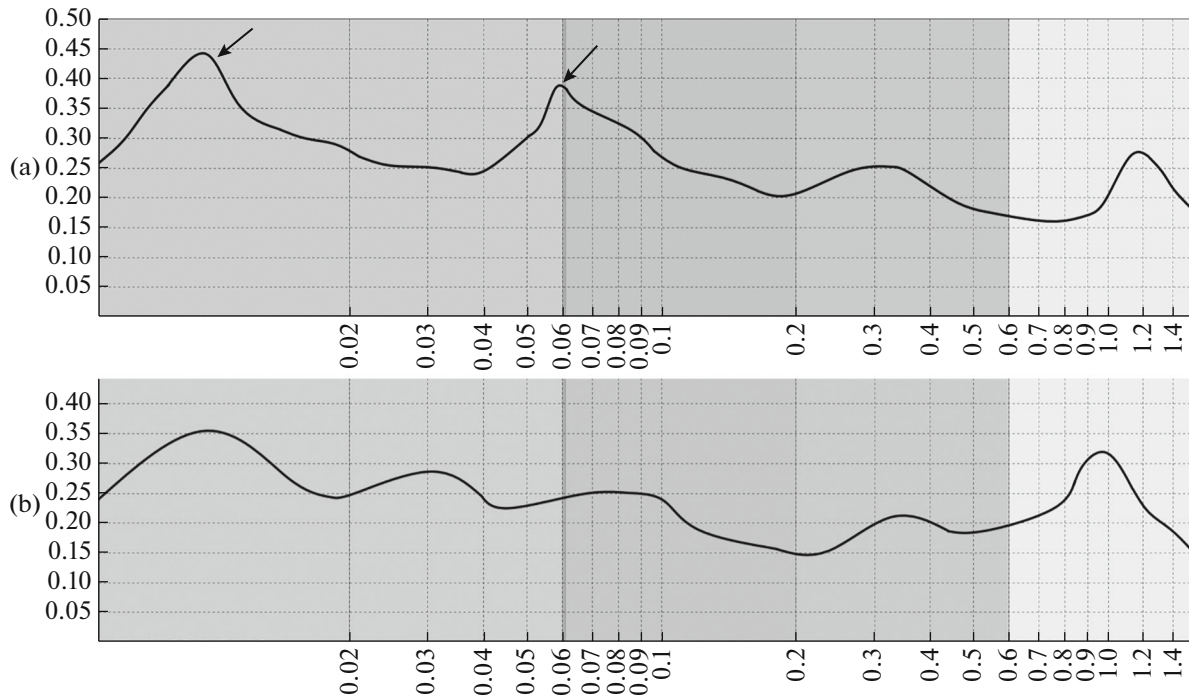
Continuous TSCS with a current amplitude of 30% of the MT was accompanied by a relatively slow and low amplitude increase in MI in the shin skin. At this magnitude of the current, the MI increase rate and its amplitude at continuous TSCS at the  $T_7$  and  $L_1$  levels differed insignificantly. An increase in the stimulating current up to 60% of the MT led to an increase in the amplitude of the increase in the MI of the tibial skin (Table 1). At the same time, the MI increase rate and its amplitude at TSCS at the  $L_1$  level were significantly higher compared to TSCS at the  $T_7$  level. The maximum changes in the amount of blood flow in the shin skin were recorded with TSCS, which was 90% of MT. It is important to note that during stimulation at the  $L_1$

level, the growth rate of MI and its amplitude were significantly higher compared to the speed obtained during stimulation of SC at the  $T_7$  level. At the same time, it should be emphasized that in all subjects with TSCS at the  $L_1$  level, despite the high growth rate of MI, blood flow began to decrease immediately after the termination of TSCS, and at TSCS at the  $T_7$  level, the increase in blood flow continued for another 15–20 s after termination of TSCS (Fig. 1).

Processing of the LDF-gram data recorded during the TSCS by means of wavelet analysis showed a pronounced increase in the amplitude of blood flow oscillations at frequencies of  $\sim 0.01$  and  $\sim 0.06$  Hz (Fig. 2). The first high-amplitude wave is of endothelial origin, and the second is caused by activation of sensory nerve fibers [13]. The most pronounced increase in the amplitude of oscillations in the neurogenic range was recorded with TSCS with an amplitude of 90% MT both during stimulation in the  $L_1$  region and during stimulation in the  $T_7$ .



**Fig. 1.** The dynamics of the microcirculation index (MI) in the skin of the antero-lateral part of the shin during TSCS with a current intensity of 90% of the MT for 1 min. (a) Stimulation at the  $T_7$  level; (b) stimulation at the  $L_1$  level. MI is presented in perfusion units (pf units).



**Fig. 2.** The amplitude-frequency spectrum of blood flow fluctuations in the shin skin of patient B. (a) At rest and (b) with TSCS at the  $L_1$  level with a current intensity of 90% of MT. The arrows indicate the oscillation peaks with a frequency of  $\sim 0.01$  Hz (endothelial genesis) and  $\sim 0.06$  Hz (caused by activation of sensory nerves). The abscissa axis is the frequency of blood flow oscillations (Hz), the ordinate axis is the oscillation amplitude (conventional units).

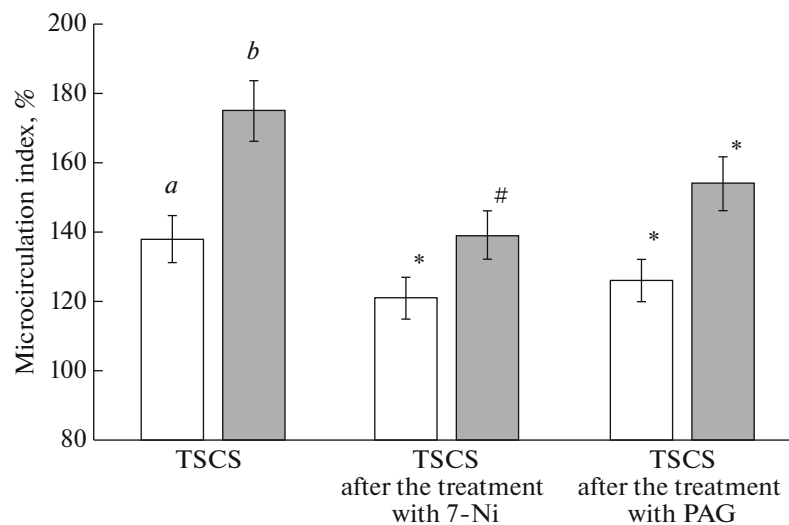
The local mechanisms promoting vasodilation in ESM, as already indicated in the introduction, are complex and not sufficiently studied. As for the mechanisms activated in the skin with TSCS, such information is practically absent. In order to identify the source of NO released in the wall of the blood vessels of the skin during TSCS, a selective inhibitor of neuronal synthase NO, 7NI, was used. The results of electrical stimulation after 7NI iontophoresis are presented in Fig. 3. The same figure shows blood flow data for TSCS after PAG iontophoresis. In both cases, the increase in blood flow during TSCS significantly decreased after the use of inhibitors.

## DISCUSSION

As in our previous study of changes in blood flow in the shin skin with lumbar TSCS [6], in this study, continuous TSCS with subthreshold stimuli was accompanied by an increase in blood flow in the shin skin, while the degree of increase in MI correlated with the amplitude of the applied current. As in [6] stimulating electrodes were placed at the close distance from each other ( $T_{11}$  and  $L_1$ ), the TSCS results after the stimulation of the neighboring regions of the spinal cord differed insignificantly. In the present study, the stimulating electrodes were located far enough from each other ( $T_7$  and  $L_1$ ), therefore, in TSCS, the increase in blood flow in the first or second region was very differ-

ent (Table 1). During TSCS in the  $L_1$  region with a current of 90% of the MT, the increase in blood flow was 74% compared to the initial one, while during TSCS in the  $T_7$  region with a current of the same magnitude, only 38%. It can be assumed that the difference in the reactions of the skin blood supply system is explained by the fact that, by stimulating different segments of the spinal cord, we affected different parts of the regulation of vascular blood flow. The sympathetic neurons located in the ganglia in the  $T_7$  region innervate mainly the organs of the lower part of abdominal cavity and the pelvis and produce a relatively small number of nerve fibers going to the vessels of the lower extremities. The sympathetic nerve fibers (including cholinergic) of the lower ganglia "connect to the lumbosacral plexus and are distributed along the lower limb along the main nerves, sciatic and femoral, and from this the innervation extends to the vessels of the thigh and shin" [14]. A similar distribution is observed for sensory nerve fibers. Due to the innervation characteristics of the vessels of the lower extremities, the stimulation effect of the lower segments of the spinal cord is more pronounced.

The second feature identified during the study is the differences in the rate of increase in MI during TSCS in  $T_7$  and  $L_1$  regions. However, to answer the question, what is the reason for the differences in the rate of increase in MI and the duration of the increase in blood flow with TSCS at  $T_7$  and  $L_1$  at the present



**Fig. 3.** Changes in the microcirculation index in the skin of the anterior-lateral part of the shin during TSCS with a current intensity of 90% of MT after iontophoresis of inhibitors: *a*, during stimulation in the  $T_7$  region; *b*, during stimulation in the  $L_1$  region. MI is presented in % of the initial level in intact skin. Significant differences: \*  $p < 0.05$ ; #  $p < 0.01$ .

time is not possible. An additional special series of studies is needed.

An analysis of the literature indicates that the local mechanisms leading to an increase in blood flow in the skin with ESSC and thermal exposure are not well understood [15, 16]. Several studies have found that part of reflex vasodilation in human skin is caused by the release of NO at the ends of sensory nerves [17]. At the same time, other authors prefer the role of endothelial synthase NO in the mechanisms of cutaneous reflex vasodilation [18]. Previously, we have also shown the important role of NO in increasing blood flow in the skin during TSCS. In the previous work, we used L-NAME, which is a non-specific inhibitor of all NO synthases, which created certain difficulties in identifying the source of NO produced during TSCS [6]. In this work, in order to determine the role of nerves in the formation and release of NO during TSCS, we used 7-Nitroindazole, which is a selective inhibitor of neuronal synthase NO. 7-NI was injected into the skin by electrophoresis immediately before TSCS and blood flow measurement. In the skin treated with 7-NI, TSCS led to a decrease in the rate of hyperemia development compared to intact skin; the amplitude of MI increase was also lower (Fig. 2). However, if we compare the decrease in MI growth during TSCS with an intensity of 90% of MT after pretreatment with L-NAME [6] and with 7-NI under the same experimental conditions, it is clearly seen that L-NAME had a greater inhibitory effect on the growth of MI at TSCS in the  $L_1$  region. L-NAME inhibits both types of NO synthases and this leads to a decrease in blood flow by ~40% relative to the increase upon stimulation of 90% of MT [6]. 7-NI, which selectively inhibits only neuronal synthase, causes a decrease in

blood flow by ~20% relative to growth at 90% of MT (Fig. 2). Thus, we can conclude that in TSCS, NO formed in the wall of blood vessels has both neurogenic and endothelial origin. As is known, activation of sensory nerves stimulates the release of neuronal NO and the calcitonin gene related peptide (CGRP) in the nerve endings [19], and the latter can activate endothelial synthase NO, as was found in the culture of some tissues [20] and directly in the wall of microvessels [21]. Direct interaction of neuronal and endothelial synthases NO is also possible, as was shown in the myocardium [22]. The NO synthesis blockade in our experiments, both with L-NAME and with 7-NI, only reduced the value of the TSCS-induced vasodilation in the shin skin, but did not cancel it, which implies the activation of other signaling pathways during the TSCS smooth muscle cells of blood vessels of the skin, vasodilation and hyperemia.

In the final series of experiments, we tested the hypothesis that  $H_2S$  may be involved in the implementation of the vasodilation effect of TSCS. As mentioned earlier,  $H_2S$  is found in many tissues and is believed to be one of the gas transmitters [23].  $H_2S$  has a rather low barrier to intercellular transport and can function well as a paracrine signaling molecule. In the last decade,  $H_2S$  has been shown to have many physiological effects on the vessel wall.  $H_2S$  is produced by vascular cells and has antioxidant, antiapoptotic, anti-inflammatory, and vasoactive properties [24].

The main mechanism by which  $H_2S$  affects the activity of signaling proteins is the persulfidation of reactive cysteine residues on target proteins to form a persulfide group (-SSH) [23]. Depending on the nature of the target protein, the effect of  $H_2S$  may take from a few seconds to several days. For example, per-

sulfidation of ATP-sensitive K-channels leads to hyperpolarization and relaxation of smooth muscle cells, which occurs within a few seconds. It is recognized that the main effect of H<sub>2</sub>S in the vasculature is vasodilating, although in some cases a vasoconstrictor effect has been identified [25].

In our study, we performed TSCS after iontophoresis in the shin skin of the DL-Propargylglycine, which is an irreversible inhibitor of cystathionine- $\gamma$ -lyase, the main enzyme that produces H<sub>2</sub>S in the vascular wall. After PAG iontophoresis, the amplitude of MI growth was significantly lower compared to intact skin (Fig. 3). The data obtained undoubtedly indicate the involvement of H<sub>2</sub>S in the vasodilation process during TSCS, but it is rather difficult to explain the activation of cystathionine- $\gamma$ -lyase during TSCS. In this regard, [23] is extremely interesting, in which it was shown that NO donors increase the relaxation of smooth muscles caused by H<sub>2</sub>S. We can consider the following hypothetical scheme explaining the participation of H<sub>2</sub>S in TSCS-induced vasodilation of the shin skin vessels: through antidromic activation of the sensory nerve endings TSCS leads to the release of neuronal NO (proved [19]), which, acting on cystathionine- $\gamma$ -lyase, leads to its activation. In addition, NO produced by endothelium can also stimulate cystathionine- $\gamma$ -lyase (discussed above). Activation of cystathionine- $\gamma$ -lyase leads to the formation of H<sub>2</sub>S, which has an additional vasodilation effect, using other signaling pathways other than signaling pathways activated by NO [26, 27].

## CONCLUSIONS

(1) TSCS at the T<sub>7</sub>–T<sub>8</sub> vertebrae level, as well as during stimulation at the L<sub>1</sub>–L<sub>2</sub> level, by continuous electric pulses with a frequency of 30 Hz and an intensity of 30–90% of the motor threshold, leads to an increase in perfusion of the shin skin.

(2) The magnitude and rate of change in blood flow during stimulation in the L<sub>1</sub>–L<sub>2</sub> region significantly differ from that in stimulation in the T<sub>7</sub>–T<sub>8</sub> region, which demonstrates the possibility of using TSCS for targeted exposure to different sections of blood flow regulation.

(3) The increase in the microcirculation in the shin skin during TSCS has been proven to be caused mainly by antidromic activation of the sensor nerve fibers, producing NO by their endings.

(4) It was found that, along with neuronal NO, the vasodilation effect in the skin of the shin during TSCS is modulated by endothelial NO.

(5) It has been shown for the first time that H<sub>2</sub>S produced by cystathionine- $\gamma$ -lyase is involved in the process of vasodilation in the skin with TSCS.

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## COMPLIANCE WITH ETHICAL STANDARDS

*Conflict of interests.* The authors declare no apparent or potential conflicts of interest related to the publication of this article.

*Statement of compliance with standards of research involving humans as subjects.* All studies were carried out in accordance with the principles of biomedical ethics formulated in the Helsinki Declaration of 1964 and its subsequent updates and approved by the local bioethical committee of the Institute of Physiology, RAS (St. Petersburg). Each study participant submitted voluntary written informed consent, signed by him after explaining to him the potential risks and benefits, as well as the nature of the forthcoming study.

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