SHORT COMMUNICATION

In vivo evaluation of a microtubule PET ligand, [11C]MPC‑6827, in mice following chronic alcohol consumption

J. S. Dileep Kumar1,2 [·](http://orcid.org/0000-0001-6688-3991) Andrei Molotkov3 · Michael C. Salling⁴ · Patrick Carberry³ · Jaya Prabhakaran1,5 · John Castrillon3 · Akiva Mintz1,3

Received: 8 April 2021 / Revised: 8 July 2021 / Accepted: 13 July 2021 / Published online: 7 September 2021 © Maj Institute of Pharmacology Polish Academy of Sciences 2021

Abstract

Background Excessive alcohol consumption is a global health burden and requires a better understanding of its neurobiology. A lower density of brain microtubules is found in alcohol-related human brain disease postmortem and in rodent models of chronic alcohol consumption. Here, we report in vivo imaging studies of microtubules in brain using our recently reported Positron Emission Tomography (PET) tracer, [¹¹C]MPC-6827, in chronic alcohol-consuming adult male C57BL/6 J mice and control mice.

Methods In vivo PET imaging studies of $\binom{11}{1}$ MPC-6827 (3.7 \pm 0.8 MBq) were performed in two groups of adult male mice: (1) water-consuming control mice $(n = 4)$ and (2) mice that consumed 20% alcohol (w/v) for 4 months using the intermittent 2-bottle choice procedure that has been shown to lead to signs of alcohol dependence. Dynamic 63 min PET images were acquired using a microPET Inveon system (Siemens, Germany). PET images were reconstructed using the 3D-OSEM algorithm and analyzed using VivoQuant version 4 (Invicro, MA). Tracer uptake in ROIs that included whole brain, prefrontal cortex (PFC), liver and heart was measured and plotted as %ID/g over time (0–63 min) to generate timeactivity curves (TACs).

Results In general, a trend for lower binding of $[$ ¹¹C]MPC-6827 in the whole brain and PFC of mice in the chronic alcohol group was found compared with control group. No group diference in radiotracer binding was found in the peripheral organs such as liver and heart.

Conclusions This pilot study indicates a trend of loss of microtubule binding in whole brain and prefrontal cortex of chronic alcohol administered mice brain compared to control mice, but no loss in heart or liver. These results indicate the potential of $[{}^{11}C]$ MPC-6827 as a PET ligand for further in vivo imaging investigations of AUD in human.

Keywords PET · Microtubule · Alcoholism · Tubulin · Brain

Abbreviations

- Aβ Amyloid beta
- AD Alzheimer's disease

 \boxtimes J. S. Dileep Kumar dkumar7@northwell.edu

- Area of Molecular Imaging and Neuropathology, New York State Psychiatric Institute, Manhattan, NY, USA
- Feinstein Institutes for Medical Research, North Shore University Hospital, Manhasset, New York, USA
- ³ Department of Radiology, Columbia University Medical Center, Manhattan, NY, USA
- ⁴ Department of Cell Biology and Anatomy, Louisiana State University Health Sciences Center, New Orleans, LA, USA
- ⁵ Department of Psychiatry, Columbia University Medical Center, New York, NY, USA
- ALS Amyotrophic lateral sclerosis
- AUD Alcohol use disorder
- BBB Blood brain barrier
- IA Intermittent access
- ID/g Injected dose/gram
- MBq Mega becquerel
- MT Microtubule
- PET Positron emission tomography
- PFC Prefrontal cortex
- PTM Post-translational modifcations
- TAC Time-activity curves
- SEM Standard error of the mean
- SUV Standardized uptake values
- W/v Weight per volume

Introduction

Over 14 million adults aged 18 and older, representing 5.8% of this population in the US sufer from Alcohol Use Disorder (AUD) [1]. Nearly half a million adolescents aged 12–17 years have AUD [1]. An estimated that 88,000 people die from alcohol-related causes annually, making alcohol the third leading preventable cause of death in the United States and ffth leading risk factor for premature death and disability globally [1]. Major efects of alcohol in the body are observed in brain, liver, heart, pancreas, and immune responses [[2](#page-5-0)]. Chronic alcohol consumption is a risk factor for cancer and dementia $[2-4]$ $[2-4]$ $[2-4]$. There is an unmet need for identifying new drug targets for this disease [\[5](#page-5-2)–[7\]](#page-5-3). The lack of a validated biomarker for mapping clinical state of AUD also hamper drug development.

Loss of tubulins, the major repeating protoflament units of α - and β -tubulin heterodimers of the microtubule (MT) cytoskeleton has been reported in brain in response to chronic excessive alcohol exposure and is a potential biomarker for AUD [[8](#page-5-4)[–11\]](#page-5-5). Loss of α - and β -tubulins and spectrin *β*-II proteins are reported in human postmortem brain in AUD [[8](#page-5-4)]. However, no changes were found in actin proteins in alcoholic subjects compared with controls [[8\]](#page-5-4). Among the tested regions in alcohol group, prefrontal cortex (PFC) shows highest α - and β -tubulin loss (50 and 47%), followed by hippocampus (54%, 36%), cerebellum (54%, 34%), and caudate nucleus (30%, 31%) in compar-ison to control group [[6\]](#page-5-6). However, this effect was not observed with non-alcoholic suicide patients. Similar to the fndings in postmortem human brain, 47% reduction of *α*-tubulins and 38% reduction of *β*-tubulin brain protein levels are reported in chronic alcohol administered rodents $[8-11]$ $[8-11]$ $[8-11]$. Although alcohol-related pathology in brain differs from that of peripheral organs, tubulin alterations are also reported in liver and heart of AUD patients [[12,](#page-5-7) [13](#page-5-8)].

Postmortem tubulin disruption may compromise fndings in brain and periphery organs in AUD. Positron Emission Tomography (PET) imaging of MT with radiolabeled and blood brain barrier (BBB) penetrating MT ligands may ofer a direct approach for detecting and quantifying the changes in MT density, in vivo*,* in brain and other organs. $[$ ¹¹C]MPC-6827 is a high affinity, selective MT ligand that binds to tubulins at the colchicine site [\[14](#page-5-9), [15](#page-5-10)]. It is the frst PET ligand that showed BBB penetration and specifc binding in brain and periphery organs in rodents [\[14,](#page-5-9) [15](#page-5-10)]. Our pilot preclinical PET imaging studies of $[^{11}C]MPC-$ 6827 in and Alzheimer's Disease (AD) mice model of Aβ pathology (5×FAD), tau pathology (rTg4510), and Amyotrophic Lateral Sclerosis (ALS) pathology (SOD1*G93A) detected lower binding in brain compared to wild type mice [[16\]](#page-5-11). This finding indicates that disease-related

tubulin loss may be measurable by PET imaging. We now report use of $[{}^{11}C]$ MPC-6827 to determine MT alterations in mice following long-term consumption of alcohol compared to age-matched water-consuming control mice using microPET imaging (Fig. [1\)](#page-1-0).

Materials and methods

All commercial chemicals and solvents used in the synthesis were purchased from Sigma–Aldrich Chemical Co., (St. Louis, MO), or Fisher Scientifc Inc., (Springfeld, NJ) and were used without further purifcation. Gamma-ray detector (Bioscan Flow-Count ftted with a NaI detector) coupled in series with the UV detector (Waters Model 996 set at λ 254 nm) was used for detection of radiolabeled products. Data acquisition for both the analytical and preparative systems was accomplished using a Waters Empower Chromatography System. MPC-6827 and desmethyl-MPC-6827 were synthesized according as previously reported [[14](#page-5-9)]. $[{}^{11}$ C]CO₂ was produced from a Siemens Eclipse cyclotron. Radiosynthesis of $[$ ¹¹C]MPC-6827 was achieved by reacting corresponding desmethyl-MPC-6827 phenolate with $[$ ¹¹C]CH₃I in a GE-FX2MeI/FX2M radiochemistry module using our established procedure [\[14](#page-5-9)[–16](#page-5-11)]. All animal experimental procedures were carried out in accordance with the Institutional Animal Care Committee ethical guidelines of Columbia University Medical Center. All experiments were performed in male C57BL⁄6 J mice (Jackson Laboratories, Bar Harbour, ME) during adolescence and adulthood (postnatal day 35–120).

Chronic alcohol treated mice

The chronic intermittent alcohol consumption model used was based on a previously reported and widely used procedure [[17\]](#page-5-12). This method of alcohol exposure was chosen as it is a voluntary, approximates binge drinking levels and states of withdrawal, can lead to signs of alcohol dependence, and is known to model alcohol induced neuroadaptations observed in humans like increased glutamatergic neurotransmission [\[17\]](#page-5-12). In short, mice were given either two bottles of water $(n = 4)$ or intermittent access to alcohol

Fig. 1 Chemical structure of $[^{11}C]$ MPC-6827

 (IA) $(n = 4)$ which consisted of one bottle of water and one bottle of increasing concentrations of alcohol (5, 10, 15% w/v) over the frst three sessions and then maintained on 20% (w/v) alcohol throughout the rest of the experiment. A cage with bottles and no mice was placed on the rack to estimate loss of fuid. Mice and bottles were weighed daily to calculate alcohol dose consumed (g/kg) and alcohol preference (%) after subtracting bottle drip. This procedure is known to result in elevated blood alcohol levels and signs of withdrawal in C57BL/6 J mice $[17]$ $[17]$. Both mice groups ($n =$ 4) underwent PET scans and imaging occurred one day after last session of alcohol consumption.

microPET imaging

microPET imaging studies were performed in anesthetized (by isoflurane 5% induction; O_2 rate: 2 L/min) mice using our established procedure [[14](#page-5-9)–[16](#page-5-11)]. PET imaging studies were conducted on a Siemens Inviorn microPET by tail vein administration of $[{}^{11}C]$ MPC-6827 (1.85 \pm 0.37 MBq, 20 µL volume) and dynamic acquisition was for 63 min in multiple frames (2 \times 30 s, 4 \times 60 s, 3 \times 120 s, 4 \times 180 s, and 4 \times 300 s). Using VivoQuant (ver 4, Invicro, MA) software (version 4.0, Switzerland), three-dimensional ellipsoid volume of interests (VOIs) ranging from 2 to 6 $mm³$ were placed manually at the center of the brain, heart (blood-pool), and liver. The percentage of injected dose/gram (%ID/g) was estimated using a calibration factor calculated from a phantom study, and time-activity curves (TACs) and standardized uptake values (SUV) were derived from VOIs.

Statistical analyses

All data reported are as mean \pm standard error of the mean (SEM), unless otherwise stated. Statistical analyses of

Fig. 2 Ethanol consumption (g/ kg) over 24 h for C57BL⁄6 J mice given intermittent access to alcohol. Values are reported as the mean \pm standard error of the mean (SEM) from four of mice per time point

radiotracer binding in the whole brain, PFC, heart and liver regions in control and chronic alcohol treated mice groups were analyzed using an Mann–Whitney nonparametric test. Statistical analyses were performed using Graphpad Prism version 9.1.0. Graphs were made using Graphpad Prism version 9.1.0. A *p* value less than 0.05 was considered statistically signifcant.

Results

Radiosynthesis of $[$ ¹¹C]MPC-6827 was accomplished with $45 \pm 5\%$ radiochemical yield and molar activity of 100 \pm 37 GBq/μmol at end of synthesis. After 2 weeks, mice given IA to ethanol achieved > 15 g/kg/24 h on average, which is likely to lead to blood alcohol concentrations above 80 mg/ dl [[18\]](#page-6-0) (Fig. [2\)](#page-2-0). We also found a similar trend for ethanol consumption throughout the remaining sessions $\left(\sim 12-20 \text{ g/s}\right)$ $kg/24 h$) (Fig. [2](#page-2-0)).

The dynamic microPET images of $[$ ¹¹C]MPC-6827 showed BBB penetration and retention of radiotracer in brain of both chronic alcohol administered mice and waterconsuming control mice (Fig. [3\)](#page-3-0).

As evident from Fig. [3,](#page-3-0) alcohol-consuming mice showed a lower binding in whole brain (right image) compared to control (left image). Similarly, whole brain TACs also demonstrate reduced binding of $[{}^{11}C]$ MPC-6827 in alcohol mice group compared to control mice (Fig. [4A](#page-3-1)). The radioligand exhibited somewhat heterogeneous distribution in brain with a higher retention in cortical regions. TACs in PFC indicate reduced binding of the tracer (Fig. [4](#page-3-1)B) in the alcohol group compared to control. The peak uptake of tracer is comparable for whole brain and PFC in both groups. SUV analyses show lower binding of tracer (-20%) in whole brain and PFC in alcohol group than control

Fig. 3 Representative microPET (sagittal) image, computed from 0 to 63 min, summed images of $[$ ¹¹C]MPC-6827 in control male white mice $(n = 4, \text{ left})$ and alcohol-consuming mice group $(n = 4, \text{ left})$ right). Image represents our observation that the alcohol treated group exhibited less binding of tracer compared to controls

group (Fig. [5](#page-4-0)A, B). Statistical analyses of whole brain SUV data show no signifcantly diferent binding of radiotracer between water (median $= 0.88$, $n = 4$) and chronic alcohol (median = 0.75 , $n = 4$) conditions (Mann–Whitney test, $U = 3$, $p = 0.2$), whereas, a noticeable trend for significance of PFC SUV data between water (median $= 1.07$, $n = 4$) and chronic alcohol (median = 0.89, $n = 4$) groups (Mann–Whitney, $U = 1$, $p = 0.0571$).

Subsequently, we examined the binding of $[$ ¹¹C]MPC-6827 in heart and liver of chronic alcohol treated and water treated mice. The uptake of $\binom{11}{1}$ MPC-6827 in heart was peaked at 1 min followed by a fast washout for both groups (Fig. [6](#page-4-1)A). Whereas, liver uptake was peaked at 3 min, followed by a fast washout up to 18 min, then a slow decline in activity throughout the remaining scan period (Fig. [6B](#page-4-1)). The uptake and SUV of $[{}^{11}C]$ MPC-6827 in heart and liver did not show any statistically signifcant group binding differences (Mann–Whitney test, heart: $U = 8$, $p > 0.99$; liver: $U = 8, p > 0.99$.

Discussion

The present study reports the frst preclinical in vivo imaging of chronic alcohol-consuming mice and control waterconsuming mice with PET using an MT targeting radioligand. We adopted an established intermittent access method to induce high chronic ethanol intake in mice because this model mimics the features of human alcohol dependence [[17,](#page-5-12) [18](#page-6-0)]. Similar to rodents, the intermittent access procedure also results in an escalation of voluntary alcohol drinking in non-human primates [[19\]](#page-6-1). This procedure is relatively simple, highly valid, and offers translational value among other models and appears to be a useful procedure for preclinical evaluation of potential therapeutic approaches against AUD. Several PET tracers of diferent imaging targets are being evaluated for PET imaging of human AUD [[20–](#page-6-2)[22](#page-6-3)]. Although these tracers show proof of concept of imaging AUD in human, most of them show moderate to minumum efect size, as well as mixed or conficting results. The above tracers also are not proven successful in correlating with clinical fnding to predict treatment responses, and no/less data available diferentiate the various stages of AUD. Since loss of cortical thickness due to reduced MT stability is a pathogenic fnding in AUD, visualizing this efect in vivo via PET imaging in various stages of AUD could have signifcant value in terms of studying pathophysiology and identifying treatment targets. If MT density quantifed by PET imaging were correlated with symptomatology in future human research, further studies could examine this biomarker in relationship to treatment outcome in treatment studies, and potentially as a biomarker for drug development. A large number of epigenetic, post-translational

Fig. 4 Time-activity curves of [11C]MPC-6827 binding in control water-consuming and chronic alcohol-consuming mice. **A** Whole brain; **B** prefrontal cortex. Values are reported as the mean (solid line) \pm SEM (dotted line) from four pairs of mice per group. Radioactivity in whole brain and prefrontal cortex of alcohol treated mice group suggest less binding of tracer compared to controls

Fig. 5 Standardized uptake values of $\binom{11}{1}$ C]MPC-6827 binding in control and chronic alcohol-consuming mice. **A** Whole brain; **B** prefrontal cortex. Values are reported as a box and whisker plot where from four pairs of mice per group. Whole brain SUV values were not significantly different between water (median $= 0.88$, $n = 4$) and chronic alcohol (median = 0.75 , $n = 4$) conditions (Mann–Whitney test, $U = 3$, $p = 0.2$). However, PFC, there was a nearly significant reduction in SUV (Mann–Whitney, $U = 1$, $p = 0.057$) between water (median $= 1.07$, $n = 4$) and chronic alcohol (median $= 0.89$, $n = 4$) groups

modifcations (PTM) and environmental factors contribute to MT or tubulin loss in AUD [[9,](#page-5-13) [23,](#page-6-4) [24\]](#page-6-5). Therefore, cumulative loss of MT is a common pathway for a variety of biochemical pathologies leading to AUD. Furthermore, MTs and tubulins are highly expressed in brain compared to other currently available PET imaging targets for AUD. This offers a likelihood of higher brain uptake and significant binding diference of MT targeted PET tracer in AUD compared to control group. Hence monitoring the changes in MT, in vivo, in brain may also be advantageous for understanding its involvement in the pathophysiology of AUD. Imaging experiments were performed with $[{}^{11}$ C]MPC-6827, a PET tracer that exhibited specifc binding to MT in brain, developed by our group [\[14](#page-5-9)[–16\]](#page-5-11). MPC-6827 is a known MT

depolymerization inhibitor which binds mostly to the colchicine sites of α , and β -tubulin at MT exchangeable site and to sites of α -tubulin residues at non-exchangeable sites [[25,](#page-6-6) [26\]](#page-6-7). A large number of epigenetic, post-translational modifcations (PTM) and environmental factors contribute to MT or tubulin loss in AUD [[9,](#page-5-13) [25,](#page-6-6) [26\]](#page-6-7).

The PET scans (Figs. [3,](#page-3-0) [4,](#page-3-1) [5](#page-4-0)) show a trend of lower binding of $[{}^{11}C]$ MPC-6827 in whole brain and PFC of chronic ethanol administered mice compared with water-administered control mice. This fnding is in agreement with lower binding to tubulins determined by in vitro postmortem studies and also the fndings in animal models of AUD [\[8](#page-5-4)[–11](#page-5-5)]. However, in vitro studies show tubulin loss in heart and liver in contrast to our fndings with in vivo PET imaging. This may be partially due to a methodological diference, because MT lose structure in vitro and so PET may offer a diferent in vivo result to postmortem brain tissue. In vitro methods measure binding of tubulins based on specifc antibodies, whereas, PET detects the sum of the available *α*and *β*-tubulin variants and PTM of MT which may be up or down regulated in AUD. For example, acetylated-tubulins are upregulated in AUD compared to α - and β -tubulins [\[8](#page-5-4)]. Currently, we do know whether binding of $[{}^{11}C]$ MPC-6827 is to all tubulin variants and or MT-PTMs. It is also difficult to determine the in vivo selectivity of $[{}^{11}C]$ MPC-6827 for tubulins and MT-PTMs due to the lack of specifc brain penetrating ligands to use as nonspecifc binding agents. Furthermore, the sensitivity of in vitro methods may be higher compared with in vivo PET.

Apart from PFC binding, we did not perform regional binding analysis of the tracer in other brain regions due to low spatial resolution of microPET coupled with the high retention of $[$ ¹¹C]MPC-6827. This microPET imaging study on mice also lacks arterial input function measurements and partial volume correction derived measurement of tracer binding in brain. Such methods are not practical for mice studies due to smaller brain size and volume of blood.

Fig. 6 Time-activity curves of $[$ ¹¹C]MPC-6827 in control mice and chronic alcohol consuming mice in heart (**A**) and liver (**B**). Values are reported as the mean \pm SEM from four pairs of mice per group. Radiotracer did not show any signifcant differences of binding in the heart and liver

Since both mice group and conditions exhibited comparable peak uptake of radiotracer in whole brain and PFC, the %ID/g as outcome measurement for tracer binding comparison is acceptable. In addition to brain, heart also exhibited comparable peak uptake of the tracer in both groups further support the validity of %ID/g as the tracer binding outcome.

Although tubulin pathology is present in liver and heart of AUD patients, we did not fnd signifcant diference in [11C]MPC-6827 binding in the hearts of alcohol treated mice and control group. This is likely due to the duration of alcohol exposure (months in a mouse versus decades in a human) and potentially be accelerated using intermittent alcohol vapor exposure known to accelerate signs of dependence in mice. It also may be due to diferent variants of tubulins and or PTM of tubulins in periphery organs compared to brain. We found modest specific binding of $[$ ¹¹C]MPC-6827 in liver in both groups of mice. There was very less specifc binding of the radioligand in heart, and, therefore, most of the cardiac binding may also be partially due to a blood flow effect of radiotracer $[14]$ $[14]$. The higher retention of radiotracer in liver may also be due to an accumulation of radioactive metabolites of $\left[$ ¹¹C]MPC-6827 [\[14](#page-5-9)].

Conclusions

In conclusion, our pilot preclinical imaging studies show a trend of reduction of whole brain and PFC uptake with MT targeted PET tracer $[$ ¹¹C]MPC-6827 in chronic alcohol-consuming mice group compared to water-consuming control mice. This result supports the previous report of lower binding of *α*- and *β*-tubulins in AUD in human brain (postmortem) and also in vitro fndings in animal models of alcoholism. The major limitations of these studies are the variations of alcohol uptake in mice, the lack of plasma input data and large sample size. Therefore, further PET imaging studies with AUD in non-human primates or human subjects and control with arterial input functions are required to establish the potential of $[{}^{11}C]$ MPC-6827 as a potential PET tracer for mapping brain MT in AUD and related diseases.

Author contributions JSDK conceived the idea. JSDK, MCS, and AM designed the experiments. JSDK, MCS, AM, PC, JP, and JC performed the experiments. JSDK, AM, and MCS performed all analyses. JSDK, AM, MCS, and AM analyzed and interpret the data. JSDK drafted the manuscript. The manuscript was written through contributions of all authors and all authors have given approval to the fnal version of the manuscript.

Funding This work was Funded by NCATS UL1TR001873 (Reilly) Irving Institute/CTSA Translational Therapeutics Accelerator.

Declarations

Conflicts of interest The authors declare no conficts of interest.

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