RESEARCH PAPER

Relation of arterial stifness with postural control in older people

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Key summary points

Purpose This study aimed to compare postural control without or with dual task, in patients over 65 years,depending on the degree of arterial stifness, measured using the carotid-femoral pulse.

Findings Sway path traveled and surface covered by the center of foot pressure were measured on a forceplatform in diferent postural conditions, i.e. eyes open, eyes closed and eyes open with a dual task, allowing to calculate the length function of surface (LFS), this ratio providing information about the precision (surface) of postural control and the efort made (length) by the participant. After an age-adjustment, LFS was higher in participants with high pulse wave velocity in diferent postural conditions especially dual task condition.

Message The difculties in maintaining the equilibrium under a dual task condition being more pronounced inpeople with increased arterial stifness, it is necessary to avoid or to limit its aggravation to reduce the number ofalls, one of the main causes of mortality in the elderly.

Abstract

Purpose Arterial stifness generates vascular alterations that may cause balance disorders and falls. This study aimed to investigate the possible link between arterial stifness and postural control under diferent sensorial conditions in patients over 65 years.

Methods Carotid-femoral pulse wave velocity (PWV) was measured in 47 participants aged over 65 years to evaluate their arterial stiffness (high PWV). Twenty-seven participants (mean age = 70.52 ± 4.02 years, 22 females) had a normal PWV $(< 10 \text{ m s}^{-1})$ and 20 participants (mean age = 75.93 \pm 6.11 years; 15 females) had a high PWV (\geq 10 m s⁻¹). Postural control was evaluated using a force platform in four postural conditions: eyes open (EO) 1, eyes closed (EC), eyes open with a dual task (DT) and eyes open again (EO2). Using sway path traveled and surface covered by the center of foot pressure,

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we calculate the length function of surface (LFS). This ratio provides information about the precision (surface) of postural control and the effort made (length) by the subjects.

Results After an age-adjustment, LFS was lower in EO than in EC and DT in both groups ($p \le 0.001$). LFS was higher in participants with high PWV both in eyes open and eyes closed conditions (*p*<0.05). LFS increased when PWV increased in EO ($p < 0.01$) and EC conditions ($p < 0.001$) but not when a dual task was performed.

Conclusion Difficulties in maintaining equilibrium under a dual-task condition are more pronounced in people with increased arterial stifness. These data suggest that understanding of the infuence of the arterial stifness level on specifc balance control parameters could contribute to propose better balance-oriented rehabilitation programs in older adults in an attempt to prevent fall.

Keywords Postural control · Arterial stifness · Older adult · Posturography

Introduction

Physiological aging is accompanied by deterioration in the quality of movement [[1\]](#page-6-0) and impairment in postural control causing loss of balance [\[2](#page-6-1)]. Thus, all these age-related changes, without any pathology, put older adults in a precarious situation in walking, gradually resulting in a loss of autonomy in addition to an increased risk of falling [[3\]](#page-6-2).

Clinical practice shows that balance disorders which could promote falls are frequent in older patients [[4,](#page-6-3) [5](#page-6-4)]. Indeed, older patients with systolic hypertension, which is a clinical manifestation of the arterial stifness, are particularly susceptible to the risk of variability in blood pressure and to orthostatic hypotension which can result in falls [\[6](#page-6-5), [7](#page-7-0)].

Moreover, arterial stifness is a recognized risk factor of subcortical vascular lesions that may promote the occurrence of dementia syndromes [\[8](#page-7-1)[–12\]](#page-7-2). Falls and postural disorders can be related to cerebrovascular attacks [[13](#page-7-3)]. Arterial stifness can also cause vascular alterations of the vestibular system, generating vertigo, dizziness and falls. Finally, arterial stifness can be responsible for balance disorders through proprioceptive disorders secondary to atherosclerosis. However, few studies in the literature have addressed the direct association of arterial stifness and balance control impairment [[4,](#page-6-3) [5\]](#page-6-4). Due to this, we decided to evaluate the possible impairment of postural control using sensitive tests, such as the dual-task situations in older adults according to arterial stifness. Balance evaluation in hypertensive older patients subjected to multiple tasks is even more interesting because arterial stifness can lead an alteration of central information processing through the nervous system lesions it causes.

Several studies examined the efect of a cognitive task on posture, which compared the motor task posture stabilization during a cognitive task between non-hypertensive older subjects and to younger subjects. Most studies have shown that an additional cognitive task signifcantly worsens a balance disorder, evaluated by the increase in the movement of the center of foot pressure in the older adults $[14, 15]$ $[14, 15]$ $[14, 15]$ $[14, 15]$. These fndings are possibly consistent with electromyography data which showed a signifcant decrease in muscle activity, in the older adults, during this same dual task [\[16](#page-7-6)]. However, the other authors either found no efect or showed a positive efect of cognitive task on the balance of presumed healthy older adults depending on the type of cognitive task [[17\]](#page-7-7).

Arterial stifness could can be caused by lesions in the white subcortical matter, or through dizziness associated with postural hypotension or vascular alterations of the vestibular system, balance disorders and walking. Stifness can occur without clinically overt cerebral vascular disease. A cognitive task can be a destabilizing factor which will become even more important in the context of accelerated aging that can cause a cognitive weakness. This can result in balance disorders, which can cause impaired central processing information through the central nervous system.

This study aimed to compare the postural control without or with dual task, in patients over 65 years, depending on the degree of arterial stifness, measured using the carotidfemoral [Pulse Wave Velocity (PWV)].

Materials and methods

Participants

Forty-seven volunteers over the age of 65 years participated in this study. The exclusion criteria were: musculoskeletal disorder, chronic neurological disorder (dementia, stroke, Parkinson's disease, and diabetic neuropathy), uncorrected visual pathology, vestibular pathology, progressive organic pathology, psychotropic drug use, opposing personality, low motivation or any other emotional or intellectual problem which may invalidate the consent or limit the possibilities of the participant to cooperate with the protocol requirements. Subjects were assigned into two groups function of degree of arterial stifness, measured using the carotid-femoral PWV. The PWV was considered as normal ($\leq 10 \text{ m s}^{-1}$) in the frst group (Gr1), composed of 27 patients (mean $age = 70.52 \pm 4.02$ years; 22 females). The PWV was considered as high (>10 m s⁻¹) in the second group (Gr2), composed of 20 patients (mean age = 75.93 ± 6.11 years; 15

females). Age, gender, and body mass index were recorded in each group.

All participants gave their written informed consent before the study, which was approved by the French Medical Ethical Committee (Comité de Protection des Personnes Est III de Lorraine).

Measurement of carotid‑femoral pulse wave velocity

Carotid-femoral PWV was measured in the supine position after lying for 10 min. The PulsePen device (Diatecne, Milan, Italy) was used for measuring carotid-femoral PWV $[18]$ $[18]$. The delay between pulse waves was determined by a single high-fdelity applanation tonometer to obtain the carotid and femoral pulse recorded sequentially in highly rapid succession, using the ECG trace as reference [[19](#page-7-9)]. Carotid-femoral PWV was calculated as the distance divided by the time delay measured between pressure upstroke at each site. Distance was determined using a sliding caliper subtracting the distance from the carotid location to the sternal notch from the distance between the sternal notch and the femoral site of measurement. The time delay was measured between the feet of the femoral and carotid waveforms. The foot of the wave was defned at the end of diastole, at the onset of the steep rise of the wavefront for the PulsePen.

A study group on behalf of the Artery Society, the European Society of Hypertension Working Group on Vascular Structure and Function, and the European Network for Noninvasive Investigation of Large Arteries suggested a critical cutoff value of carotid-femoral PWV of 10 m s⁻¹ [[20,](#page-7-10) [21](#page-7-11)]. The same cutoff value has also adopted by the European Society of Hypertension guidelines for hypertension management $[22]$ $[22]$. This cutoff value has been estimated while considering the additive value of arterial stifness beyond traditional risk factors to predict the occurrence of a cardiovascular event.

Cognitive assessment

The Folstein Mini-Mental State Examination (MMSE) was used to assess the patient's level of general cognitive domains (temporal and spatial orientation, learning ability and recall, attention, language and visual-constructive praxis) [[23](#page-7-13)]. A score higher than 25 was considered as normal [[24](#page-7-14)].

The short form of the Geriatric Depression Scale (GDS) [\[25\]](#page-7-15) was used to rule out depression, which can affect the cognitive state. A score equal or higher than 10 was considered to be a sign of depression, in which case patients were not included in the study.

The evaluation of autonomy was assessed by the activities of daily living (ADL) scale [[26\]](#page-7-16) and the instrumental

activities of daily living (IADL) scale [[27\]](#page-7-17). For both scales, the higher the score is, the higher the dependency.

Posturography

A vertical force platform, ftted with three strain-gauge force transducers (Satel, Blagnac, France) was used to perform posturography and to provide a measurement of the body sway in terms of displacement of the center of foot pressure (CoP) in a two-dimensional horizontal plane (recording time: 25.6 s, acquisition frequency: 40 Hz). Each participant was asked to stand upright on the platform, barefoot, feet abducted at 30°, heels separated by 3 cm, arms along the body, remaining as stable as possible and breathing normally [[28,](#page-7-18) [29\]](#page-7-19). Sway path traveled and area covered by the CoP were used to calculate the LFS (length function of surface).

The LFS, providing information about the precision of postural control and the effort made (efficiency), is calculated using the following equation: LFS = sway path/396 \times exp^(0.0008 \times area) [\[30](#page-7-20)[–32](#page-7-21)].

The analysis was carried out under four conditions, alternating with periods of rest for 1 min. In the third condition (the "dual task" condition), a cognitive task was included. This task consisted of serial subtraction by 7 from a random number between 100 and 200.

The four posturographic conditions consisted of:

- Eyes open 1 condition (EO1);
- Eyes closed condition (EC);
- Eyes open with dual task (DT); the number and precision of the answer were recorded.
- The eyes open condition was repeated at the end of the sequence (EO2) to assess possible learning or fatigue effects

A diference between the LFS obtained in each condition was also calculated $(Δ$ LFS) to show the improvement or deterioration of the postural control between each condition.

Statistical analysis

The SPSS statistical software package (version 23.0) was used in this study for data analysis. Qualitative data were expressed as number (*n*) and percentage (%) and were compared using χ^2 test. Quantitative data were expressed as mean with standard deviation (SD) and non-parametric Mann–Whitney test were performed to compare characteristics of patients (age, sex, body mass index, systolic blood pressure, diastolic blood pressure, heart rate, MMSE, ADL, IADL, and GSD) and the LFS in the four postural conditions of the two groups. Statistically signifcant diferences were accepted for a probability level of $p \leq 0.05$. Comparisons between the four conditions (EO1, EC, DT, and EO2) were

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Table 1 Characteristics of the sample in the two groups (normal PWV: Gr 1; high PWV: Gr2) function of degree of arterial stifness

Mini-Mental State Examination (MMSE): normal cognition > 25; Activity of daily life (ADL): independent<6; Instrumental activity of daily living (IADL): independent>5 for men and=8 for women; Geriatric depression scale (GDS): no depression≤5; standard deviation (STDEV)

Signifcant value (in bold)

Inter-situation	Normal wave velocity	High wave velocity
comparisons		
$E01$ <i>vs.</i> EC	$***$	$***$
EO1 vs. DT	$***$	NS
EO1 vs EO2	\ast	\ast
EC vs DT	NS	\ast
EC $vs.$ EO2	$***$	$**$
DT vs. EO2	$***$	\ast

Fig. 1 Intergroup (above) and inter-situation (below) comparisons. Values of LFS eyes open (EO), eyes closed (EC) and in dual task (DT) situations in normal wave velocity and high wave velocity patients. $\frac{*p}{0.05}$; $\frac{**p}{0.001}$

produced using a non-parametric Wilcoxon test. The Bonferroni–Dunn procedure was applied to pairwise comparisons by adjusting "family-wise alpha" to a signifcance level of $p \le 0.05/6 = 0.0083$ in accordance with the six possible comparisons. A Student *T* test was used to evaluate the impact of the gap between eyes open and eyes closed or PWV on LFS, a highest T absolute value indicating the parameters having a higher impact on LFS.

For the comparison between the two groups with adjustment to age, a Mann–Whitney test was used. This test was also used to compare the Δ LFS between the two groups. Statistically signifcant diferences were accepted for a probability level of $p \leq 0.05$.

The relationship between PWV and LFS, without and with adjustment to age, was tested using a linear regression model. Statistically signifcant relationships were accepted for a probability level of $p < 0.05$.

The effect size of PWS on LFS can be estimated using two coefficients: the coefficient of determination, square of the Pearson correlation *R* (*R*2 < 0.2 as weak effect; $0.2 < R$ 2 < 0.5 as moderate effect; R 2 > 0.5 as strong effect), and the Cohen's d measuring the standardized diference between the two means of LFS in normal PWV and high PWV.

Results

Participants with a high PWV were older than participants with normal PWV $(p=0.001)$ $(p=0.001)$ (Table 1). Due to this signifcant diference, an adjustment to age was made before comparing the characteristics of the populations. No other baseline characteristic was diferent between the two groups except for the resting heart rate which was higher in the participant with high PWV ($p < 0.001$). Participants were autonomous and did not have depression.

The LFS was signifcantly higher in participants with high PWV than in participants with normal PWV in EO1 condition ($p = 0.031$ $p = 0.031$) and in EC condition ($p = 0.017$) (Fig. 1). No diference between the two groups was observed in EO with DT condition and EO2 condition. In both groups, LFS was higher in eyes closed condition than in both eyes open conditions ($p < 0.0083$). LFS in EO with DT was higher than in both EO1 conditions in participants with normal PWV (*p*<0.0083) but was only higher than in EO2 condition in participants with high PWV ($p < 0.0083$). For the intragroup diference in LFS between YO and YC, evaluated by the paired Student T between these groups, we observed $t = 6.84$. For the inter-group difference in LFS between the two PWV groups, estimated by the usual T, we observed $t = 2.41$ in EO condition and $t = 2.55$ in EC condition. Therefore, we can conclude that the diference between EO and EC is larger than the diference between the two PWV groups.

Δ LFS between EC and DT condition was higher in participants with high PWV than in participants with normal PWV $(p=0.014)$.

Δ LFS between EC and EO2 condition was higher in participants with high PWV than in participants with normal PWV $(p=0.007)$.

Figure [2](#page-6-6) shows the linear regression models for the relationship between LFS and PWV. The LFS increased when the PWV increased in EO1 condition $(p < 0.001)$, EC condition ($p < 0.001$), EO with DT condition ($p = 0.003$), EO2 condition $(p=0.001)$. The LFS increased when the ageadjusted PWV increased in EO1 condition $(p < 0.001)$, EC condition ($p < 0.001$), EO2 condition ($p = 0.01$). PWV has a medium effect on LFS. After age-adjustment, we observed r^2 = 0.269 in EO condition and r^2 = 0.445 in EC condition. For the Cohen's d measuring the standardized diference between the two means of LFS in normal PWV and high PWV, we observed $d = 0.31$ in EO condition and $d = 0.51$ in EC condition.

Discussion

This study showed higher values of LFS in postural performances for patients with increased arterial stifness. Depending on the postural condition, the values of the LFS varied in the same way in patients with normal or higher arterial stifness. LFS values increased in the following order: (1) eyes open on frm support, (2) dual tasking in eyes open and (3) eyes closed. LFS was lower when condition with eyes open has been reproduced at the end of the evaluation, indicating a learning efect in both groups. The LFS increased when the PWV increased in eyes open and eyes closed.

During the fulfllment of a cognitive task or in eyes closed condition, the LFS increased, indicating more energetic expenditure requirement and/or lower precision of balance [\[31](#page-7-22)]. Jamet et al. (2004) [\[14](#page-7-4)] showed that the achievement of a cognitive task could induce postural perturbations. A cognitive task requires attention to maintain balance control and needs to share attentional resources between counting task and postural control [[14\]](#page-7-4). In this context and depending on the limited attentional resources available, subjects could be forced to grade their mental activities and focus their attention on relevant information [\[14](#page-7-4)]. To perform a backward counting task, the subject mentally uses visual mental images of the calculation and so is partly disconnected from external visual landmarks, reducing the visual anchorage required to control balance [\[14\]](#page-7-4). Older adults are more dependent in visual information to maintain postural control [\[29](#page-7-19), [33](#page-7-23)]. This loss of external visual anchorage when older adults perform a cognitive task can explain the balance perturbation observed [\[14](#page-7-4)].

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 \blacktriangleleft **Fig. 2** Linear regression models between pulse wave velocity (PWV) and length function of surface (LFS) without and with adjustment to age in four postural conditions (eyes open 1, eyes closed, dual task, eyes open 2)

A signifcant poorer postural stability in eyes closed conditions compared with eyes open confrms the importance of the visual system for body balance [\[34,](#page-7-24) [35](#page-7-25)]. Vision facilitates head stabilization in older adults to compensate for age-related decrease in vestibular and proprioceptive systems involved in maintenance of postural control [\[36](#page-7-26)]. The modulation of the somatosensory and visual pathway by eye closure diminishes with age and the dominance of the visual system is more pronounced in the aging brain [\[37](#page-8-0)].

Higher LFS was observed in participants with increased arterial stifness compared to the participants with lower values of PWV. PWV has a moderate efect on LFS in eyes open (frst condition) and eyes closed and a weak efect on LFS in dual task and eyes open (last condition). The gap between eyes open and eyes closed has a higher impact on LFS than PWV. During the fulfllment of eyes open or closed conditions, more energetic expenditure is required for patients with arterial stifness to maintain balance and its precision compared to participants with normal wave velocity. Arterial stifness may be explained by gradual loss of the cushioning capacity of the aorta and early wave refection from the periphery, resulting in lesion of small vessels and thus, a lower irrigation of various organs [[38](#page-8-1)]. Wong et al., (2004) [\[39](#page-8-2)] showed that multiorganic and multisystemic manifestations arising from arterial stifness could increase the risk of falls through impaired cognitive function and postural control or peripheral neurological changes. In older adults, aortic stifness may be detrimental to mobility.

This study has several limitations. Limited sample size of mostly female population needs to be highlighted. There are no data available on the ftness state or muscle mass of the population. It is well known that exercise capacity and muscle mass play a signifcant role in modulating arterial stifness [\[40](#page-8-3)]. We do not have information on the extent to which participants practice physical and sport activities other than ADL and IADL questionnaire responses. In particular, combined aerobic and low-intensity resistance exercise training increases basal nitric oxide production and could have a benefcial efect on arterial stifness in older adults [[41\]](#page-8-4).

Conclusion

Postural control efficiency is better in people with normal pulse wave velocity than in patients with higher pulse wave velocity. The impact of arterial stifness on diferent organs, more particularly through a deficit in irrigation, can increase the risk of falls through impaired cognitive function and postural control. More energetic expenditure is required for patients with arterial stiffness to maintain balance and its precision. These data suggest that understanding of the infuence of the arterial stifness level on specifc balance control parameters could contribute to propose better balance-oriented rehabilitation programs in older adults in an attempt to prevent fall.

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Author contributions All the authors contribute to the study concept and design. LP-C, AL and SB realized the posturography recordings. GW and AB realized the cardiovascular investigations determining the assignment in a given group. Statistical analyses were made under the supervision of RG, statistician. PhP is principal investigator of the study. All the authors contribute to the writing of the manuscript.

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Compliance with ethical standards

Conflict of interest The authors declare that they have no confict of interest.

Ethics approval The study was approved by the French Medical Ethical Committee (Comité de Protection des Personnes Est III de Lorraine) and by the National Agency for Medicines and Health Products Safety.

Informed consent All the participants gave their written informed consent prior to the study.

Consent for publication All the authors consent for publication.

Availability of data and material The Direction for Research of the Nancy University Hospital, as study Promoter (which is not Investigator of the study), is the owner of the data and may allow their transmission according to the terms of an agreement.

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