



Tissue Section Image-Based Liver Scar Detection

Yung-Kuan Chan¹ · Ming-Jen Chang² · Yi-Wen Hung^{3,4} · Ching-Lin Wang⁵ · Chun-Fu Hong⁶ · Kwong-Chung Tung³ · Shyr Shen Yu²

Received: 14 November 2016 / Accepted: 22 May 2017 / Published online: 12 December 2017
© Taiwanese Society of Biomedical Engineering 2017

Abstract

Liver cirrhosis is a major cause of liver cancer. Traditionally, the diagnosis of stages of liver cirrhosis depends on doctors' examination of large numbers of images acquired from clinical specimens, which is a relatively time-consuming and labor-intensive task. To avoid this extensive effort and possible error of human judgment, it is necessary to develop an automatic system to recognize the liver scar stages based on clinical liver tissue section images. In this study, a tissue section image-based liver scar stage (TSILSS) diagnosis system is proposed to detect liver scar stages. In this system, a local cross-thresholding method is provided to separate the scar liver tissues from normal liver tissues on a liver tissue section image. Moreover, a two-layer recognition algorithm is presented to identify the scar stage of liver tissue. Furthermore, a parameter decider genetic algorithm is proposed to determine the most suitable values of the parameters used in the TSILSS diagnosis system. The experimental results show that in segmenting scar tissues and normal tissues on liver cirrhosis images, the average precision, average recall rate, and average F-measure that the TSILSS diagnosis system obtains are greater than 94%, and the average accuracy is close to 90%. The TSILSS diagnosis system can help doctors recognize the liver tissue scar stage more efficiently.

Keywords Liver cancer · Liver cirrhosis · Liver tissue section · Image segmentation · Pattern recognition

1 Introduction

Liver cancer was the second leading cause of cancer-related death worldwide in 2012 [1]. Liver cancer is a malignant tumor that grows rapidly and commonly occurs after the age of 45 [2]. There may be no obvious symptoms in the early stage of liver cancer. As advanced cancer grows, symptoms

may include weight loss, loss of appetite, nausea or vomiting, and yellowing of the skin and eyes [3]. Without early diagnosis and proper medical treatment, a patient often dies within 6 months after liver cancer has been initially diagnosed [2]. The survival rate of liver cancer has gradually improved in recent decades. For example, in Korea, the 5-year survival rate of liver cancer has slightly improved

✉ Chun-Fu Hong
cfhong@nqu.edu.tw

Yung-Kuan Chan
ykchan@nchu.edu.tw

Ming-Jen Chang
d102056001@mail.nchu.edu.tw

Yi-Wen Hung
hongiw@yahoo.com.tw

Ching-Lin Wang
clwang@ncut.edu.tw

Kwong-Chung Tung
kctung1@mail.nchu.edu.tw

Shyr Shen Yu
pyu@nchu.edu.tw

¹ Department of Management Information System, National Chung Hsing University, Taichung 40227, Taiwan, ROC

² Department of Computer Science and Engineering, National Chung Hsing University, Taichung 40227, Taiwan, ROC

³ Department of Veterinary Medicine, National Chung Hsing University, Taichung 40227, Taiwan, ROC

⁴ Department of Education and Research, Taichung Veterans General Hospital, Taichung 40705, Taiwan, ROC

⁵ Department of Information Management, National Chin-Yi University of Technology, Taichung 41170, Taiwan, ROC

⁶ Department of Long-Term Care, National Quemoy University, Kinmen County 89250, Taiwan, ROC

from 11.0% in 1993–1997 to 14.7% in 1998–2002 [4]; in a study cohort of 1115 liver cancer patients who underwent hepatectomy between 1981 and 2008 at five hepatobiliary centers in France, China, and the USA, the results showed that after major hepatectomy, the 5-year overall survival rate was 40%, and the 5-year survival rates were 30, 40, and 51% in 1981–1989, 1990–1999, and 2000–2008, respectively [5]. The prevention and treatment of liver cancer have become important issues.

Liver cirrhosis is one of the major causes of liver cancer [6–8]. The cause of liver cirrhosis can be attributed to several factors, including alcoholic liver diseases, chronic viral hepatitis, obesity, and nonalcoholic fatty liver disease. These factors may lead to chronic liver inflammation [6, 7, 9]. Evidence shows that the inflammatory response of liver parenchymal injury leads to hepatic fibrosis [10]. Liver inflammation will stimulate the proliferation of fibrous tissue in the liver, and these fibrous tissues then become scar tissues. They surround the normal liver cells, transform into the fake hepatic lobule, and then lead to liver cirrhosis and eventually liver cancer [6, 7]. For example, excess fat accumulation in the liver cells results in a fatty liver. The cells of normal liver tissues and tissues around the liver will be transformed into fat organizations for storing fat. In these circumstances, the liver cells cannot obtain a sufficient blood supply, nutrients and oxygen and become prone to inflammation or necrosis [6].

To understand the pathology of liver fibrosis and cirrhosis, animal models such as rats, have been introduced to examine the pathogenesis of liver cirrhosis and liver cancer. Different chemical substances were given to animals to induce liver diseases. For example, carbon tetrachloride (CCl_4) is a common chemical substance used to induce rat liver fibrosis, liver cirrhosis, and subsequent liver cancer progression. In these experiments, CCl_4 was repeatedly given to rats by gavage at different time points, and their livers were then extracted and observed by a microscope. The results showed that the area and quantity of the scar tissues increased when the treatment time was expanded [11, 12].

Traditionally, judging the phases of liver cirrhosis or liver cancer usually takes a considerable amount of time for doctors to observe many medical images. Current technologies, such as X-ray and magnetic resonance imaging (MRI), are applied to observe the roughness of the liver surface and check whether cirrhosis or tumors exist. In some serious circumstances, a surgical puncture is used to remove the liver slices, and the scar tissues are examined under a microscope [13].

For liver cirrhosis pathology, the areas of scar tissues are different in various stages of liver cirrhosis. In a liver cirrhosis tissue image, the area of the scar tissues from the first to the third stages will become more numerous and larger. Figure 1 shows a healthy liver tissue image and a scar liver

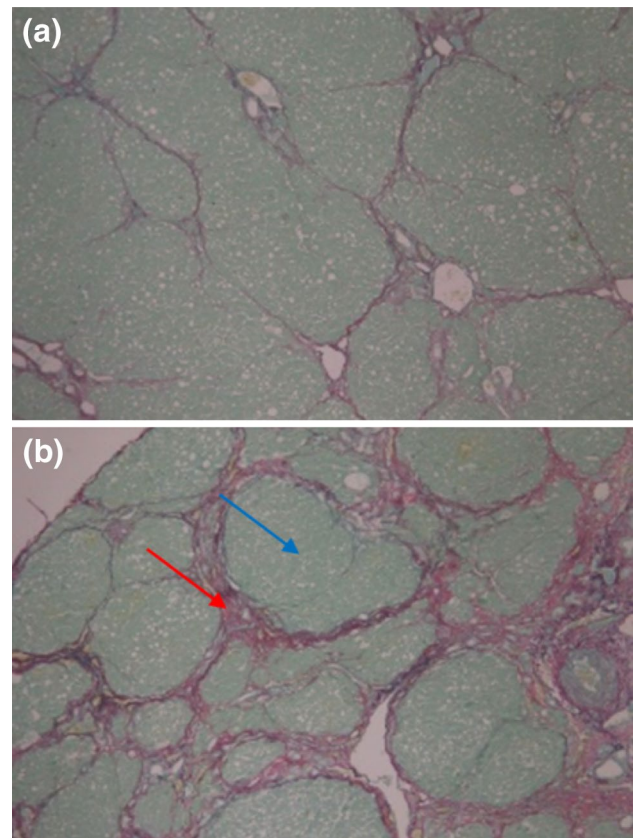


Fig. 1 Two liver tissue section images. **a** Healthy rat liver tissue section. **b** Injured rat liver tissue section. The blue arrow indicates the healthy liver tissue region and the red arrow indicates the scar liver tissue

tissue image, on which the blue arrow indicates the healthy liver tissue region and the red arrow indicates the liver scar tissue region. However, it is difficult for the human eye to justify the severity of liver tissue injury from a liver tissue section image, especially for a junior physician. Therefore, developing an automatic system to identify the scar stages of liver tissue is necessary.

In this study, a tissue section image-based liver scar stage (TSILSS) diagnosis system was proposed to diagnose the liver scar stage from the liver tissue section images. The TSILSS diagnosis system automatically segments the scar regions on the liver tissue section image, extracts the features from the segmented the scar regions, and then identifies the liver scar stage based on the extracted features. The TSILSS diagnosis system can reduce the processing time, error of human judgment, and human resources. It can also efficiently assist a doctor in diagnosing the liver scar stages.

In this study, the rat liver tissue section images were used as the test data for investigating the performance of the TSILSS diagnosis system. In these experiments, CCl_4 was administered to rats for a period of time. After that, the TSILSS diagnosis system was employed to extract the scar

tissue regions from a liver tissue section image, compute the features of the segmented scar tissues, and then recognize the scar stage of the liver based on the extracted features to assist the doctor in determining the stage of liver cirrhosis. In this study, a genetic-based algorithm is also proposed to determine the fittest values of the parameters used in the TSILSS diagnosis system.

2 Methods

2.1 Animals and Treatment

Male Sprague–Dawley rats were purchased and housed in cages under constant conditions of temperature (22 °C) and humidity (60%) with light illumination for a 12-h light/dark cycle. CCl₄ was prepared as a 50% solution by mixing with an equal volume of olive oil. All rats were divided into four groups (each group has 8 rats). The negative control group remained untreated for 20 weeks. Rats 8, 12, and 16 weeks of age were treated with 50% CCl₄ solution for 12, 8 and 4 weeks, respectively. Then, 0.2 ml 50% CCl₄ solution was administered per 100 g rat weight by gavage twice a week. After all rats had reached the age of 20 weeks, rats were euthanized by CO₂. Adequate size liver samples were fixed with 10% buffer-formaldehyde solution and then embedded in paraffin blocks. The paraffin-embedded liver samples were sectioned and stained with hematoxylin and eosin (H&E) and Sirius red following standard procedures. The stages of rat liver scars were determined according to the methods proposed by Ruwart et al. [14]. All animal experiments were carried out following the guidelines of the Laboratory Animal Center of Taichung Veterans General Hospital, ROC.

2.2 TSILSS Diagnosis System

The TSILSS diagnosis system contains three approaches, respectively to segment the scar liver tissue regions from the liver tissue section images, compute the features of the extracted scar liver tissue regions, and discriminate the stage of liver scars based on the extracted features. This subsection will describe these three approaches in detail.

2.2.1 Liver Scar Tissue Segmentation

2.2.1.1 Pre-processing To make scar liver tissue region segmentation easier, the TSILSS diagnosis system transforms each color liver tissue section image I_{RGB} into a gray-level one. The TSILSS diagnosis system first separates the RGB color mode liver tissue section image I_{RGB} into R, G, and B color components images R-, G-, and B-images, respectively, composed of the red, green, and blue color components of all the pixels in I_{RGB} . It also transforms I_{RGB} into an

HSV color mode image I_{HSV} , isolates the H, S, and V color components from I_{HSV} , and then respectively combines the H, S, and B color components into H-, S-, and B-images [15, 16]. Figure 2 shows a color liver tissue section image and its R-, G-, B-, H-, S-, and B-images.

Obviously one can observe that the difference in the contrast of the health and scar liver tissue regions is large in the G-image. The difference in the contrast of the health and scar liver tissue regions in the H-image is also large, but some pixels in the healthy liver tissue region may be lost, i.e., the regions indicated by red arrows. To facilitate scar liver tissue region segmentation, the TSILSS diagnosis system will isolate the scar liver tissue regions from the healthy liver tissue regions on the G-image of each color liver tissue section image. We can consider the G-image as a gray-level image I_0 .

2.2.1.2 Contrast Enhancement The TSILSS diagnosis system then uses Gamma equalization [17] to enhance the contrast of I_0 to make the liver tissues clearer. Let $I_0(x, y)$ be the gray level of the pixel located at the coordinates (x, y) on I_0 . Gamma equalization is then adopted to transfer I_0 into I_r by:

$$I_r(x, y) = \left(\frac{I_0(x, y) - \min_0}{\max_0 - \min_0} \right)^{r_G} \times 255, \quad (1)$$

where \max_0 and \min_0 are the maximal and minimal gray levels of all the pixels in I_0 , and r_G is a given constant. Figure 3b is the image obtained by running the Gamma equalization operation on the image in Fig. 3a.

2.2.1.3 Local Cross Thresholding Figure 3b shows that the healthy liver tissue is brighter than the region of the scar liver tissue. The TSILSS diagnosis system intends to use bi-level thresholding method to label the scar liver tissue. Figure 3d demonstrates the binary image I_O obtained by

$$I_O(x, y) = \begin{cases} 1, & \text{if } I_r(x, y) > T_O, \\ 0, & \text{otherwise.} \end{cases} \quad (2)$$

where T_O is the threshold provided by the Otsu thresholding method [18, 19] on image I_r .

The areas on the right side and at the bottom left corner of the image in Fig. 3d are almost resemble the scar liver tissue, which was caused by uneven lighting. Usually, the global thresholding method cannot produce a proper result for the unevenly lit images [20]. In this study, an adaptive thresholding method was hence provided; we call it the local cross-thresholding method.

For each pixel $I_r(x, y)$ in I_r , a cross region R_C is given, where R_C consists of all the pixels in $\{I_r(x+i, y) \mid -\frac{m_c-1}{2} \leq i \leq \frac{m_c-1}{2}\}$ and $\{I_r(x, y+j) \mid -\frac{m_c-1}{2} \leq j \leq \frac{m_c-1}{2}\}$. Let

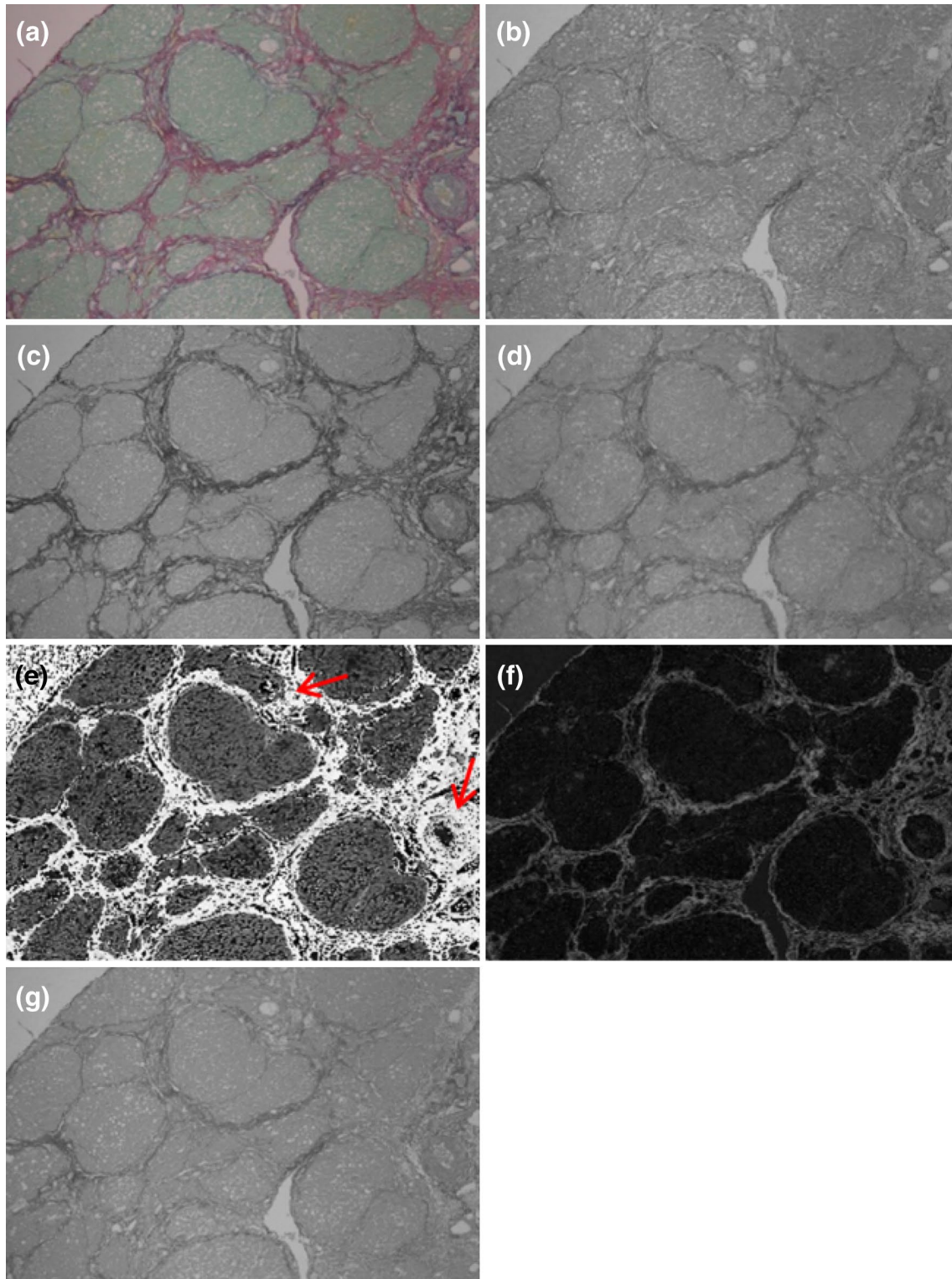


Fig. 2 An original color liver tissue section image and its derivative images. **a** Original image. **b** R-image. **c** G-image. **d** B-image. **e** H-image. **f** S-image. **g** B-image. The arrow indicates the liver scar tissue

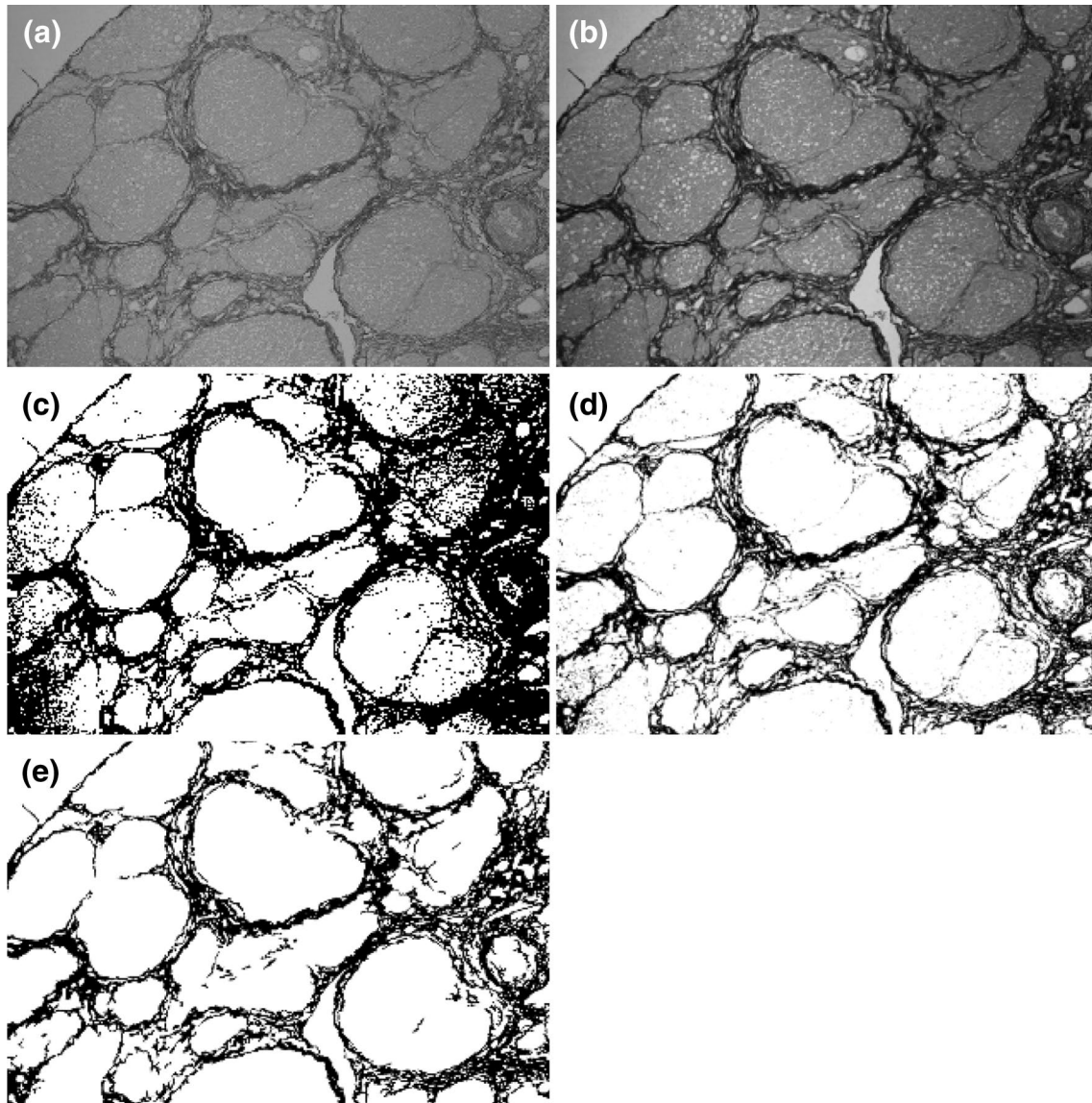


Fig. 3 The procedures of the image preprocessing approach. **a** G-Image, **b** Image of I_r , **c** I_0 , **d** I_b , and **e** I_b after removing noise

$Mean_g$ and Std_g be the mean and standard deviation of the gray levels of all the pixels in I_r and $Mean_l$ and Std_l be the mean and standard deviation of the gray levels of all the pixels in R_C . If $\frac{Mean_l}{Mean_g} > 1$, $I_r(x, y)$ is located at a bright area, and a bigger threshold $T_b = \frac{Mean_l}{Std_g}$ is given; otherwise, a smaller threshold $T_s = \frac{Mean_l}{Std_s}$ is specified. The local cross thresholding method transfers I_r into a binary image I_b as follows:

$$I_b(x, y) = \begin{cases} 1 & \text{if } I_r(x, y) > T_b, \\ 0 & \text{otherwise;} \end{cases} \quad (3)$$

else

$$I_b(x, y) = \begin{cases} 1, & \text{if } I_r(x, y) > T_s, \\ 0, & \text{otherwise.} \end{cases} \quad (4)$$

Figure 3d displays the I_b obtained by the local cross thresholding method on I_r , where the white pixels represent the healthy liver tissue pixels, while the black pixels signify the liver scar tissue pixels.

There are tiny scar liver tissue regions with very small areas on I_b in Fig. 3d. The tiny regions are considered as noise and are removed. The TSILSS diagnosis system uses a closing operation to eliminate the noise. It performs the dilation operation [21] twice and then the erosion operation twice on I_b based on the 3×3 structure element,

including 9 1-bits. Figure 3e illustrates the I_b after removing noise.

2.2.2 Feature Extraction

Figure 4 presents the liver scar tissue section images with stages I, II, and III, respectively. The G-image of the liver tissue sliced from a healthy liver contains a few large uniform color regions, while the liver tissue sliced from a scarred liver consists of some healthy tissue regions and many small scar tissue regions scattered throughout the image, where the healthy tissue regions are brighter than the scar tissue regions.

The TSILSS diagnosis system, therefore, adopts five features, μ_G , σ_G , R_A , D_h , and D_s , to characterize a liver tissue section image I_0 to identify the scar stage of the liver. μ_G and σ_G are the average and standard deviation of the gray levels of the G-image of the liver tissue section image. R_A is the ratio of the areas of scar tissue regions to the areas of the healthy tissue regions.

Let $h(x_i, y_j)$ be the gray-level of the i th pixel located at coordinates (x_i, y_j) on all the healthy tissue regions. Additionally, let (x_h, y_h) be the central pixel of all the $h(x_i, y_j)$ s, which is defined as:

$$\begin{cases} x_h = \frac{\sum_{i=1}^{n_h} x_i}{n_h}, \\ y_h = \frac{\sum_{i=1}^{n_h} y_i}{n_h}, \end{cases} \quad (5)$$

where n_h is the number of pixels in all of the healthy tissue regions. D_h is defined as follows:

$$D_h = \frac{\sum_{i=1}^{n_h} \sqrt{(x_i - x_h)^2 + (y_i - y_h)^2}}{n_h}. \quad (6)$$

Let $s(x_i, y_j)$ be the gray-level of the i th pixel located at coordinates (x_i, y_j) on all the scar tissue regions. Additionally, let (x_s, y_s) be the central pixel of all the $s(x_i, y_j)$ s, which is defined as:

$$\begin{cases} x_s = \frac{\sum_{i=1}^{n_s} x_i}{n_s}, \\ y_s = \frac{\sum_{i=1}^{n_s} y_i}{n_s}, \end{cases} \quad (7)$$

where n_s is the number of pixels in all of the healthy tissue regions. D_s is defined as follows:

$$D_s = \frac{\sum_{i=1}^{n_s} \sqrt{(x_i - x_s)^2 + (y_i - y_s)^2}}{n_s}. \quad (8)$$

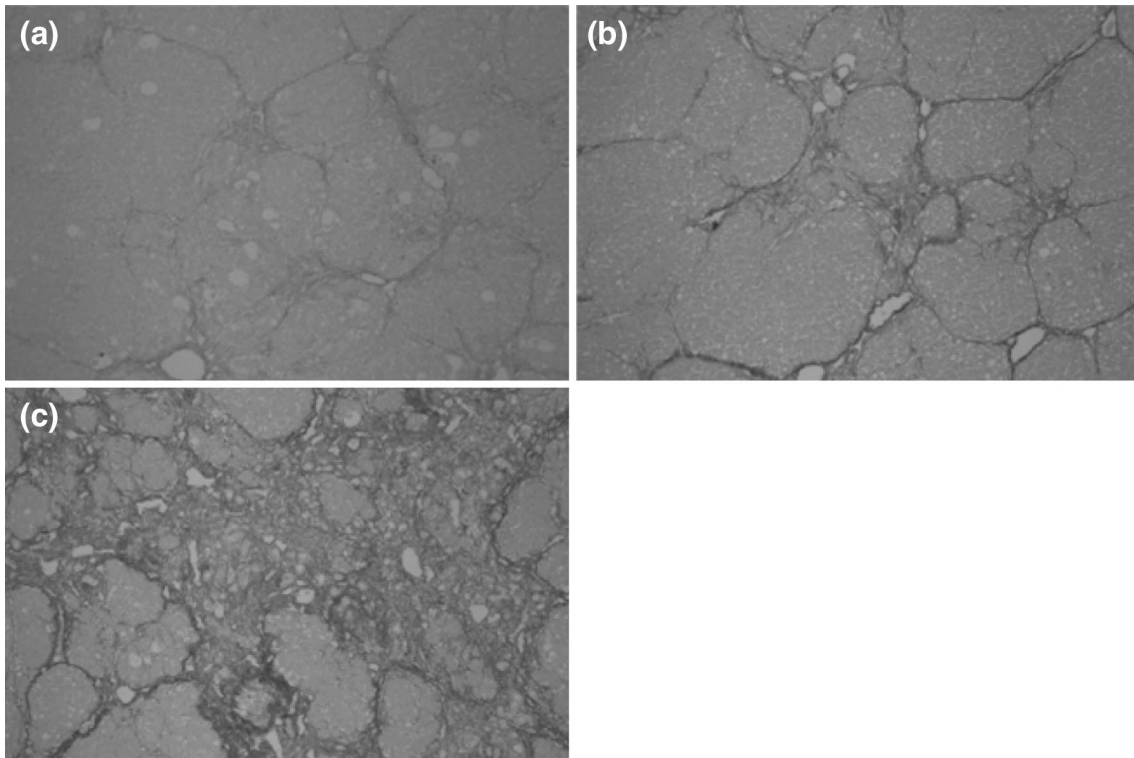


Fig. 4 The examples of the tissue section images with different liver scar stages. **a** Scar liver tissue at Stage I. **b** Scar liver tissue at Stage II. **c** Scar liver tissue at Stage III

2.2.3 Liver Tissue Scar Stage Identification

In pattern recognition, a set of historical data is collected in advance. Let f_{cik} be the k th feature of the i th datum in the c th cluster. Assume that there are N_c clusters in the set of historical data. The center $(\bar{f}_{c1}, \bar{f}_{c2}, \dots, \bar{f}_{cK})$ of the c th cluster is often used to represent each datum in the cluster, where

$$\bar{f}_{ck} = \frac{\sum_{i=1}^{N_c} f_{cik}}{N_c}, \tag{9}$$

and N_c is the number of data in cluster c . Each liver section image can be described by five features, $\mu_G, \sigma_G, R_A, D_h$, and D_s . For the i th liver section image in cluster c , $(f_{ci1}, f_{ci2}, \dots, f_{ci5})$ maps to the five features $(c, \mu_G, \sigma_G, R_A, D_h, D_s)$ of the image.

When given a liver section image I_0 has five features (f_1, f_2, \dots, f_5) , the TSILSS diagnosis system computes the distance d_c between (f_1, f_2, \dots, f_5) and each cluster center as follows:

$$d_c = \sum_{k=1}^K w_k |f_k - \bar{f}_{ck}|^{r_k} \tag{10}$$

Here, w_k and r_k are the given constants. The TSILSS diagnosis system then considers I_0 to the cluster (stage) c' , while $c' = ARG(MIN_{c=1}^C d_c)$.

If the data in a cluster are quite different, the cluster center cannot precisely depict the data in the cluster. For example, there are two clusters C_1 and C_2 . The data in C_1 are very distinct, and the data in C_2 are similar. For datum X in C_1 farther from the cluster center of C_1 but closer to that of C_2 , X will be mistakenly regarded as a datum in C_2 , i.e., the datum X in Fig. 5a. When the data in C_1 are categorized into smaller sub-clusters, X will be specified to one of the sub-clusters in C_1 as Fig. 5b; then, one can correctly assign X to cluster C_1 . Based on this property, in this paper, a two-layer recognition algorithm is provided. In the two-layer recognition algorithm, the k -means algorithm [22] is used to separate the data in each cluster into sub-clusters.

The two-layer recognition algorithm uses the k -means algorithm to classify the data in the c th cluster into N_{cs} sub-clusters. When given a liver section image I_0 has five features (f_1, f_2, \dots, f_5) , the TSILSS diagnosis system computes the distance between (f_1, f_2, \dots, f_5) and the center of each sub-cluster by:

$$d_c = MIN_{s=1}^{N_{cs}} \sum_{k=1}^K w_k |f_k - \bar{f}_{csk}|^{r_k} \tag{11}$$

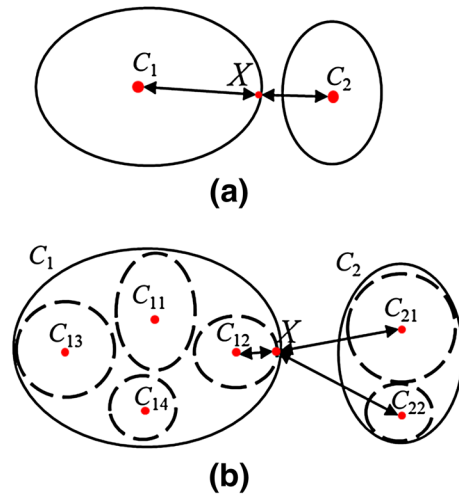


Fig. 5 Illustrations of two clusters, C_1 and C_2 , and datum X . **a** Two clusters, C_1 and C_2 . **b** C_1 and C_2 are re-clustered into sub-clusters

where \bar{f}_{csk} is the k th feature of the center of the s th sub-cluster in cluster c . The two-layer recognition algorithm then considers I_0 to one element of c' , where $c' = ARG(MIN_{c=1}^{N_c} d_c)$.

2.3 Parameter Decider Genetic Algorithm (PDGA)

The performance of the TSILSS diagnosis system is deeply affected by the parameters $r_G, m_c, r_b, r_s, r_1, w_1, r_2, w_2, \dots, r_5$, and w_5 . In this study, a parameter decider genetic algorithm (PDGA) is presented to give the fittest values of $r_G, m_c, r_b, r_s, r_1, w_1, r_2, w_2, \dots, r_5$, and w_5 .

A genetic algorithm [23–25] is a heuristic optimization method where a set of possible solutions represents a population of individuals. The fitness of an individual describes its degree of adaptation to the environment. A chromosome is the coordinate of an individual in the search space. A gene, encoding the value of a parameter, is a subsection of a chromosome being optimized. When given a certain population, only the individuals that adapt well to their environment can survive and transmit their characteristics to their descendants. Generally, a genetic algorithm alternatively and repetitively performs three operations, crossover, mutation, and selection, to derive the best solution.

In PDGA, each chromosome, represented by a binary string concatenated by 15 binary substrings $s_G, s_c, s_b, s_s, s_{r_1}, s_{w_1}, s_{r_2}, s_{w_2}, \dots, s_{r_5}, s_{w_5}$, and s_d , consisting of $n_G, n_c, n_b, n_s, n_{r_1}, n_{w_1}, n_{r_2}, n_{w_2}, \dots, n_{r_5}, n_{w_5}$, and n_d binary bits, respectively, are designated to describe $r_G, m_c, r_b, r_s, r_1, w_1, r_2, w_2, \dots, r_5, w_5$, and dum , respectively. Here dum is a dummy value which is not a parameter in the TSILSS diagnosis system but will

be used to determine the values of r_G , r_b , and r_s . Let $v_G, v_c, v_b, v_s, v_{r_1}, v_{w_1}, v_{r_2}, v_{w_2}, \dots, v_{r_5}, v_{w_5}$, and v_d be the decimal values that $s_G, s_c, s_b, s_s, s_{r_1}, s_{w_1}, s_{r_2}, s_{w_2}, \dots, s_{r_5}, s_{w_5}$, and s_d describe. For each chromosome Ch , a set of $r_G, m_c, r_b, r_s, r_1, w_1, r_2, w_2, \dots, r_5, w_5$ can be encoded as

$$r_G = \frac{v_G}{v_G + v_b + v_s} \times v_d, \tag{12}$$

$$m_c = 2 \times v_c + 1, \tag{13}$$

$$r_b = \frac{v_b}{v_G + v_b + v_s} \times v_d, \tag{14}$$

$$r_s = \frac{v_s}{v_G + v_b + v_s} \times v_d, \tag{15}$$

$$r_i = \frac{v_{r_i}}{v_{r_1} + v_{r_2} + \dots + v_{r_5}} \times v_d, \text{ for } i = 1 \text{ to } 5, \tag{16}$$

$$w_i = \frac{v_{w_i}}{v_{w_1} + v_{w_2} + \dots + v_{w_5}}, \text{ for } i = 1 \text{ to } 5. \tag{17}$$

Based on the $r_G, m_c, r_b, r_s, r_1, w_1, r_2, w_2, \dots, r_5, w_5$, the TSILSS diagnosis system can be used to identify the liver scar stages and the obtained accurate rate is regarded as the fitness of the chromosome. Initially, PDGA randomly creates N_c chromosomes, and we call them initial chromosomes. Then, PDGA alternatively and repeatedly performs mutation, crossover, and selection operations to determine the optimal solution:

- (A) In mutation operation:
 - (a) For each chromosome Ch in the N_c initial chromosomes, PDGA randomly selects one bit b from each substring in Ch .
 - (b) Set each $b = \bar{b}$, where \bar{b} is the logical complement of b .
- (B) In the crossover operation:
 - (a) PDGA randomly selects N_c chromosome pairs from the N_c initial chromosomes.
 - (b) A binary string S_M is given for each selected chromosome pair Ch_1 and Ch_2 , and $|S_M| = |Ch_1| = |Ch_2|$, where $|S_M|$ is the number of bits in S_M .
 - (c) $|S_M|/2$ bits in S_M are randomly selected.
 - (d) The selected bits in S_M are set to 1, while the other bits in S_M are set to 0.
 - (e) After that, a new chromosome Ch is created by:

$$Ch = (Ch_1 \wedge S_M) \vee (Ch_2 \wedge \overline{S_M}), \tag{18}$$

where \wedge and \vee are ‘‘AND’’ and ‘‘OR’’ bit-logic operators.

- (C) In the selection operation: a chromosome set S'_c with N_c chromosomes is created.
 - (a) Eighty percent of the chromosomes in S'_c are the chromosomes with the highest fitness, selected from the N_c initial chromosomes, the N_c chromosomes created in the mutation operation, and the N_c chromosomes produced in the crossover operation.
 - (b) Twenty percent of the chromosomes in S'_c are generated by a random number generator. S'_c then replaces S_c as the new initial chromosome set.

Furthermore, PDGA alternatively and repeatedly executes the mutation, crossover, and selection operations until the related fitnesses of the chromosomes in the initial chromosome set are very close to one another or until the number of iterations is equal to a specified constant.

3 Results and Discussion

The performances of the TSILSS diagnosis system were investigated in these experiments. In total, 108 rat liver tissue section images were used as the test data, provided by Laboratory Animal Center of Taichung Veterans General Hospital, ROC, in which 36 images were taken from the liver tissue sections of the rats in the first stage (GCI), 37 images from the liver tissue sections of the rats in the second stage ($GC2$), and 35 images from the liver tissue sections of the rats in the third stage ($GC3$).

Three experiments, A, B , and C , are performed by PDGA to probe the fittest values of the parameters used in the TSILSS diagnosis system. In experiment A , the image set S_A , including all 108 images, was used as the training data; in experiment B , the image set S_B , consisting of 18, 19, and 17 images randomly selected from $GCI, GC2$, and $GC3$, respectively, was applied as the training data; in experiment C , the image set S_C , comprising all the images in S_A but not in S_B , was employed as the training data. Table 1 demonstrates the fittest values of the parameters used in the TSILSS diagnosis system, which were derived by PDGA. In this study, the following experiments adopted these obtained parameter values.

Precision, recall, F-measure, and accuracy are frequently used statistical measures of the performance of a binary classification test [26, 27]. A true positive (TP) occurs when the condition is detected, and the condition is also actually

Table 1 The fittest parameter values derived by PDGA

Parameters	Exp. A	Exp. B	Exp. C	Average
r_G	2	2.1	2.1	2.1
r_b	0.2	0.25	0.25	0.25
r_s	0.15	0.15	0.2	0.175
m_s	5	5	5	5
w_1	0.45	0.4	0.4	0.4
w_2	0.25	0.25	0.2	0.225
w_3	0.35	0.35	0.35	0.35
w_4	0.4	0.4	0.4	0.4
w_5	0.45	0.45	0.4	0.25
r_1	0.9	0.8	1	0.9
r_2	0.9	0.9	0.9	0.9
r_3	0.7	0.7	0.7	0.7
r_4	0.7	0.8	0.8	0.8
r_5	0.9	1	1.1	1.05

present. A true negative (TN) occurs when the condition is not detected, and the condition is actually absent. A false positive (FP) occurs when the condition is detected, but the condition is actually absent. A false negative (FN) occurs when the condition is not detected, but the condition is actually present. Precision (P), recall (R), F-measure (F), and accuracy (ACC) can be defined as:

$$P = TP / (TP + FP), \tag{19}$$

$$R = TP / (TP + FN), \tag{20}$$

$$F = 2 \times P \times R / (P + R), \text{ and} \tag{21}$$

$$Acc = (TP + TN) / (TP + TN + FP + FN). \tag{22}$$

In this study, precision, recall, F-measure, and accuracy were used to measure the performances of the TSILSS diagnosis system.

Next, three experiments A' , B' , and C' were performed to scrutinize the performances of the TSILSS diagnosis system. In experiment A' , the parameters in column Exp. A in Table 1 were adopted, and the data in S_A were used as the testing data. In experiment B' , the parameters in column Exp. B in Table 1 were used and the data in S_C were used as the testing data. In experiment C' , the parameters in column Exp. C in Table 1 were employed and the data in S_B were used as the testing data. Table 2 shows that

Table 2 The experimental results obtained by the TSILSS diagnosis system

	Exp. A'	Exp. B'	Exp. C'		Average	Otsu	Region
P (%)	93.48	93.14	98.20	96.49	92.71	94.80	77.78
R (%)	92.59	92.59	98.15	96.30	92.59	94.44	77.52
F (%)	93.00	92.74	98.13	96.24	92.61	94.54	77.34
ACC (%)	86.96	86.21	96.36	92.86	86.21	89.72	63.66

all the precision, recall, and F-measures provided by the TSILSS diagnosis system were over 92%, and the accuracy was over 86%. The Average column in Table 2 displays the averages of the precision, recall, F-measure, and accuracy obtained by the TSILSS diagnosis system. On average, the precision, recall, and F-measure offered by the TSILSS diagnosis system were greater than 94.80, and the accuracy was close to 90%.

To investigate the performance of the local cross-thresholding method, in this study, the Otsu thresholding method was also used to derive the threshold on image I_r to transform I_r into I_b . Column Otsu in Table 2 shows that the average results obtained by the method were identical to the TSILSS diagnosis system, except that the local cross-thresholding method was replaced by the Otsu thresholding method.

In this experiment, I_r was partitioned into 5×5 regions, shown in Fig. 6. For each pixel in $R(i, j)$, the threshold T_R was set to the average gray-level of all the pixels in all the regions $R(x + i, y + j)$, for $-1 \leq i, j \leq 1$. Then, I_r was converted into I_b by

$$I_b(x, y) = \begin{cases} 1, & \text{if } I_r(x, y) > T_R, \\ 0, & \text{otherwise.} \end{cases} \tag{23}$$

We call this method the local region thresholding method. The Region column in Table 2 illustrates that the experimental results obtained by the method were identical to the TSILSS diagnosis system, except that the local region thresholding method was substituted for the local cross-thresholding method. Obviously, one can observe

R(-2, -2)	R(-1, -2)	R(0, -2)	R(1, -2)	R(2, -2)
R(-2, -1)	R(-1, -1)	R(0, -1)	R(1, -1)	R(2, -1)
R(-2, 0)	R(-1, 0)	R(0, 0)	R(1, 0)	R(2, 0)
R(-2, 1)	R(-1, 1)	R(0, 1)	R(1, 1)	R(2, 1)
R(-2, 2)	R(-1, 2)	R(0, 2)	R(1, 2)	R(2, 2)

Fig. 6 Partitioning I_r into 5×5 regions

that the local cross-thresholding method can provide much better results than the Otsu thresholding method and the local region thresholding method.

4 Conclusions

In this study, the TSILSS diagnosis system was used to identify the liver scar stage from liver tissue section images. In the TSILSS diagnosis system, the local cross-thresholding method is proposed to determine the fittest threshold. The TSILSS diagnosis system employs five features, μ_G , σ_G , R_A , D_h , and D_s , to characterize a liver scar tissue section image. In addition, a two-layer recognition algorithm is proposed to distinguish the liver scar stage. A genetic-based algorithm, PDGA, is presented to derive the most suitable parameters used in the TSILSS diagnosis system as well. The experimental results also show that the TSILSS diagnosis system can provide impressive results.

The traditional manual stage detection of liver cirrhosis or liver cancer is an expensive, time-consuming, labor-intensive, and subjective task for doctors to observe a large number of medical images. The scar liver tissue areas are distinct in different liver cirrhosis stages; nevertheless, for the human eye, it is difficult to verify the severity of liver tissue injury from a liver tissue section image, especially for an inexperienced physician. The TSILSS diagnosis system will be of great assistance for doctors if the method is used in medical diagnoses. It is also helpful for exploring the effects of a new medicine in animals.

References

- Douglas, S. S., Matthew, A. F., Courtney, L. S., & Sean, J. M. (2016). Biomarkers in pancreatic adenocarcinoma: Current perspectives. *OncoTargets and Therapy*, 9, 7459–7467.
- Chow, J. H., & Chow, C. (2006). *The encyclopedia of hepatitis and other liver diseases*. New York: Infobase Publishing.
- Al-Sarraf, M., Go, T., Kithier, K., & Vaitkevicius, V. (1974). Primary liver cancer. A review of the clinical features, blood groups, serum enzymes, therapy, and survival of 65 cases. *Cancer*, 33(2), 574–582.
- Jung, K. W., Yim, S. H., Kong, H. J., Hwang, S. Y., Won, Y. J., Lee, J. K., et al. (2007). Cancer survival in Korea 1993–2002: A population-based study. *Journal of Korean Medical Science*, 22(Suppl), S5–S10.
- Andreou, A., Vauthey, J. N., Cherqui, D., Zimmiti, G., Ribero, D., Truty, M. J., et al. (2013). Improved long-term survival after major resection for hepatocellular carcinoma: A multicenter analysis based on a new definition of major hepatectomy. *Journal of Gastrointestinal Surgery*, 17(1), 66–77.
- Tsochatzis, E. A., Bosch, J., & Burroughs, A. K. (2014). Liver cirrhosis. *The Lancet*, 383(9930), 1749–1761.
- Qian, Y., & Fan, J. G. (2005). Obesity, fatty liver and liver cancer. *Hepatobiliary Pancreat Dis Int*, 4(2), 173–177.
- Lin, T., Tsu, W., & Chen, C. (1986). Mortality of hepatoma and cirrhosis of liver in Taiwan. *British Journal of Cancer*, 54(6), 969.
- Schuppan, D., & Afdhal, N. H. (2008). Liver cirrhosis. *The Lancet*, 371(9615), 838–851.
- Iredale, J. P. (2007). Models of liver fibrosis: Exploring the dynamic nature of inflammation and repair in a solid organ. *The Journal of Clinical Investigation*, 117(3), 539–548.
- Dai, L., Ji, H., Kong, X. W., & Zhang, Y. H. (2010). Antifibrotic effects of ZK14, a novel nitric oxide-donating biphenyldicarboxylate derivative, on rat HSC-T6 cells and CCl4-induced hepatic fibrosis. *Acta Pharmacologica Sinica*, 31(1), 27–34.
- Fujii, T., Fuchs, B. C., Yamada, S., Lauwers, G. Y., Kulu, Y., Goodwin, J. M., et al. (2010). Mouse model of carbon tetrachloride induced liver fibrosis: Histopathological changes and expression of CD133 and epidermal growth factor. *BMC Gastroenterology*, 10(1), 79.
- Bruix, J., Sherman, M., Llovet, J. M., Beaugrand, M., Lencioni, R., Burroughs, A. K., et al. (2001). Clinical management of hepatocellular carcinoma. Conclusions of the Barcelona-2000 EASL conference. *Journal of Hepatology*, 35(3), 421–430.
- Ruwart, M. J., Wilkinson, K. F., Rush, B. D., Vidmar, T. J., Peters, K. M., Henley, K. S., et al. (1989). The integrated value of serum procollagen III peptide over time predicts hepatic hydroxyproline content and stainable collagen in a model of dietary cirrhosis in the rat. *Hepatology*, 10(5), 801–806.
- Chaves-González, J. M., Vega-Rodríguez, M. A., Gómez-Pulido, J. A., & Sánchez-Pérez, J. M. (2010). Detecting skin in face recognition systems: A colour spaces study. *Digital Signal Processing*, 20(3), 806–823.
- Hanbury, A. (2008). Constructing cylindrical coordinate colour spaces. *Pattern Recognition Letters*, 29(4), 494–500.
- Park, C. W., & Ryu, J. Y. (2008). Development of a new automatic gamma control system for mobile LCD applications. *Displays*, 29(4), 393–400.
- Otsu, N. (1975). A threshold selection method from gray-level histograms. *Automatica*, 11(285–296), 23–27.
- Samet, H., & Tamminen, M. (1988). Efficient component labeling of images of arbitrary dimension represented by linear bintrees. *Pattern Analysis and Machine Intelligence, IEEE Transactions on*, 10(4), 579–586.
- Booth, S., & Clausi, D. A. (2001). Image segmentation using MRI vertebral cross-sections. *IEEE Proceedings of the IEEE Canadian Conference on Electrical and Computer Engineering*, 2, 1303–1307.
- Gonzalez, R. C., & Woods, R. E. (2008). *Digital image processing* (4th ed.). Upper Saddle River: Pearson-Prentice-Hall.
- MacQueen, J. (1967). Some methods for classification and analysis of multivariate observations. In *Proceedings of the Fifth Berkeley Symposium on Mathematical Statistics and Probability*, 1967 (Vol. 1, pp. 281–297). Oakland, CA.
- Man, K. F., Tang, K. S., & Kwong, S. (2012). *Genetic algorithms: Concepts and designs*. New York: Springer.
- Sanchis, J., Martínez, M. A., & Blasco, X. (2008). Integrated multiobjective optimization and a priori preferences using genetic algorithms. *Information Sciences*, 178(4), 931–951.
- Yun, Y. (2006). Hybrid genetic algorithm with adaptive local search scheme. *Computers & Industrial Engineering*, 51(1), 128–141.
- Raghavan, V., Bollmann, P., & Jung, G. S. (1989). A critical investigation of recall and precision as measures of retrieval system performance. *ACM Transactions on Information Systems (TOIS)*, 7(3), 205–229.
- Makhoul, J., Kubala, F., Schwartz, R., & Weischedel, R. (1999). Performance measures for information extraction. In *Proceedings of DARPA Broadcast News Workshop, 1999* (pp. 249–252)