

The Efect of Annealing Temperature and Immersion Time on the Active–Passive Dissolution of Biomedical Ti₇₀Zr₂₀Nb₇₅Ta_{2.5} Alloy in Ringer' s Solution

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Abstract

Because of their superior biocompatibility, chemical stability, and mechanical strength, Ti and Ti-based alloys are commonly utilized in orthopedic dentistry. In Ringer's solution (RS), the corrosion behavior of the $Ti_{70}Zr_{20}Nb_{7.5}Ta_{2.5}$ alloy was examined as an alternative potential material for Ti and Ti_6A_4V (T_6A_4V) in medical applications. The corrosion resistance was evaluated utilizing potentiodynamic polarization curves (PPCs), electrochemical impedance spectroscopy (EIS), and open-circuit potential techniques (OCP), supplemented by XRD and SEM surface analysis. The $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy has the highest resistance to corrosion since it has the most stable passive state in addition to the lowest corrosion current $(I_{corr}=11.8 \mu A \text{ cm}^{-2})$ and lowest CR (6.1 mpy) in comparison with that of T₆A₄V (I_{corr}=13.7 µA cm⁻², CR=7.13 mpy) and Ti (I_{corr}=29.5 µA cm⁻², CR=15.3 mpy). Furthermore, it was also looked at how different annealing temperatures (600, 800, and 1000 °C) and immersion times (one, two, and three weeks) affected the corrosion behavior of $T_{70}Z_{20}N_7$, T_2 , In comparison to the other samples, the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy annealed at 800 °C demonstrated superior resistance to corrosion (the lowest I_{corr}=1.53 × 10⁻⁶ A cm⁻²) and I_{pass}=0.009 mA cm⁻². While that annealed at 1000 °C has the lowest resistance to corrosion (highest I_{corr}=4.49×10⁻⁵ A cm⁻² and I_{pass}=0.611 mA cm⁻²) as a result of the passive layer dissolution. The passive flm is composed of an inner and outer oxide layer, according to the EIS measurements. Meanwhile, the PPCs data demonstrate that the resistance to corrosion of the alloy is higher without immersion than it is with immersion and for a shorter immersion time. It was found that the $T_{70}Z_{20}N_{7.5}T_{2.5}$ system consisted of α and β phases. An X-ray structural study indicated a mixture of body-centered cubic β-Ti and hexagonal close-packed α-Ti (main phase, with a grain size of about 5.35 nm). Therefore, among all the materials evaluated in this work, the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy can be considered a promising material suitable for use as a biomaterial.

Keywords Ringer's solution · Biomedical $Ti_{70}Zr_{20}Nb_{7.5}Ta_{2.5}$ alloy · Passivity · Annealing · Immersion time

1 Introduction

Ti and Ti-based alloys are widely utilized for orthopedic and dental purposes as a result of their superior chemical stability, mechanical strength, and biocompatibility [[1](#page-12-0)[–4](#page-12-1)]. For surgical implants, Ti_6AI_4V , TiNi, and Ti_6AI_7Nb alloys are currently the most frequently utilized. Nevertheless, the toxicity of aluminum and vanadium as well as the high sensitivity of Ni leads to the formation of non-toxic Ti-based alloys [[5–](#page-12-2)[8\]](#page-12-3). Several binary or ternary Ti-based alloys have reportedly been used to create implants, including TiNb [\[9](#page-12-4)], TiTa [\[10\]](#page-12-5), TiZr [[11](#page-12-6)], Ti₃₅Nb₇Zr₅Ta [[12\]](#page-12-7), and Ti₁₃Zr₁₃Nb [[13\]](#page-12-8). One of them, $Ti_{13}Nb_{13}Zr$ has recently gained attention due to its superbly comprehensive properties, which include superior corrosion resistance and a lower elastic modulus (70 GP) [\[6](#page-12-9), [7](#page-12-10)]. To improve the compatibility and interaction between the implanted alloys and the tissues, the porosity and surface shape of the alloys should be modifed. However, the sintering environment had a signifcant impact on the pore size and alloy homogeneity [[14\]](#page-12-11). The most crucial characteristics for an implant in the human body are biocompatibility and resistance to corrosion, which increase the

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usage of alloys as biomaterials [[15\]](#page-12-12). Niobium (Nb) addition may improve a material's ability to resist corrosion [[16](#page-12-13)]. Acceptable mechanical strength is displayed by zirconium (Zr) [\[17\]](#page-12-14), and in vivo research has shown that zirconium implants have good osteointegration [[18,](#page-12-15) [19](#page-12-16)]. Tantalum (Ta) has more resistant to corrosion than Nb due to the increase in its oxide stability [\[20,](#page-12-17) [21](#page-12-18)]. Both the biocompatibility of Ta and its superior corrosion resistance have undergone rigorous evaluation [\[22\]](#page-12-19). TiZrNbTa alloys are therefore anticipated to have great corrosion resistance and excellent biocompatibility due to the unique properties of Ta, Zr, and Nb. On the other hand, Zr, Nb, and Ta were chosen as intensifcation elements because they are toxicology-free elements that have been thoroughly studied and found to have no undesirable effects on tissue [[23\]](#page-12-20). Comprehensive ion production from a prosthesis can have undesirable biological effects that cause mechanical failure of the device. In general, it is preferable to use corrosion-resistant materials to reduce the amount of metal ions released, which mostly rely on the stable passive flm that forms on the alloy surface to act as a barrier between the alloy substrate and the bio-environment [[24\]](#page-12-21). Even so, other protection techniques can be applied [\[25](#page-13-0)[–27\]](#page-13-1). The literature did not have any thorough information regarding the corrosion behavior of the $T_{70}Z_{20}N_7$, T_{25} alloy in a RS. The aim of the research was to examine the $T_{70}Z_{20}N_{7.5}T_{2.5}$ corrosion behavior compared with Ti and T_6A_4V in RS using various electrochemical techniques: PPCs, EIS, and OCP measurements. Also, the corrosion behavior of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy in RS at diferent immersion times and at diferent annealing temperatures was studied, along with the passive flm structure analysis by an X-ray difraction analysis.

2 Experimental Details

The corrosion behavior of the three materials Ti, T_6A_4V , and $T_{70}Z_{20}N_{7.5}T_{2.5}$ in RS was compared using an electrochemical analysis (their compositions are given in Table [1](#page-1-0)). Using epoxy cold resin mounting of alloys, the Ti, T_6A_4V , and $T_{70}Z_{20}N_{7.5}T_{2.5}$ electrodes were prepared, allowing 1.0 cm² of the electrode surface to be exposed to RS. In electrochemical studies, the Ti, T_6A_4V , and $T_{70}Z_{20}N_{7.5}T_{2.5}$ electrodes were employed as the working electrodes (Japan Coating Center Co. Ltd., Kanagawa, Japan, provided the electrode specimens). The electrode is mechanically polished with fne

sandpaper of various grades, beginning with 500, moving up to 800, and ending with 1200, before being washed with acetone and distilled water. After activating the electrode in 1.0-M hydrogen fuoride for 1.0 min, it is carefully cleaned with double-distilled H_2O . The counter electrode was a platinum electrode. For all potential measurements, a reference electrode was silver/silver chloride. For each experiment, measurements were made at 37 °C using freshly generated RS as the electrolyte to simulate the conditions that a biological component might encounter. The chemical components of RS were dissolved in 1.0 L of distilled $H_2O:9.00-g$ sodium chloride, 0.40-g potassium chloride, 0.20-g sodium bicarbonate, and 0.25-g calcium chloride dissolved in 1.0 L of distilled H_2O [[23\]](#page-12-20). All solutions were freshly prepared from analytical-grade chemicals and doubly distilled water. The solution was kept at pH 7.4. In an electric heat furnace, the annealing procedure was perfected at temperatures of 600 °C, 800 °C, and 1000 °C. Two hours were spent holding the substance, and air conditioning was used to cool it.

The electrochemical investigations used a 1000 Gamry Instrument Potentiostat/Galvanostat/ZRA. All the electrochemical parameters were derived using the Echem Analyst software supplied by Gamry Instruments. The PPCs were done using a voltage range of -1.2 to $+3.0$ V and a $5-mV s^{-1}$ scan rate. The EIS diagrams were plotted after 1800s of immersion in a RS with a frequency range from 100,000 Hz to10.0 mHz with an amplitude of 5 mV peak to peak. The tests were done after 30 min of immersion. The electrochemical experiments were evaluated in accordance with the accepted test procedure to identify the tiny implant's sensitivity to corrosion. Each test was carried out twice. The samples surface morphology under test was investigated utilizing the scanning electron microscopy (SEM) model JEOL JEM-1200EX II Electron Microscope. An X-ray diffraction analysis was applied (Panalytical Empyrean, the Netherlands) with a CuKa radiation (λ = 1.54045 Å) at an accelerating voltage of 40 kV and current 35 mA.

3 Results and Discussion

3.1 Corrosion Resistance Resulted from PPCs

Figure [1](#page-2-0) shows PPCs of $T_{70}Z_{20}N_{7.5}T_{2.5}$, T_6A_4V , and Ti electrodes in a RS, at 37 °C with a 5-mVs⁻¹ scan rate. The related corrosion parameters obtained are shown in Table [2.](#page-2-1)

Fig. 1 Potentiodynamic polarization curves of $T_{70}Z_{20}N_{7.5}T_{2.5}T_6A_4V$, and Ti electrodes in a RS recorded with a sweep rate of 5 mVs−1 at 37 °C

There are five zones (I-V) in the PPCs of the $T_{70}Z_{20}N_{7.5}T_{2.5}$, T_6A_4V , and Ti. Because the Ti element and alloying elements are oxidized into ions of varying valences and the production of the passive layers happens simultaneously with the reactions, the first region (I) demonstrates that the electrodes are in the active–passive state. As a result of reactions dominating passive layer production, the current density rises as potential rises. The current densities (I_{pass}^1) stay very stable as the potential increases in the zone (II), reaching about 87.7, 98.28, and 160.3 µA cm⁻² for T₇₀Z₂₀N_{7.5}T_{2.5}, T_6A_4V , and Ti, respectively. This depicts that as the voltage approached E_L^{-1} (the low limit voltage in the first passive zone) (II), the passive layers gradually produced on the electrode surface. For the three materials $T_{70}Z_{20}N_7$, T_2 , T_6A_4V , and Ti at various voltages (E_H^{-1}) , about 1.46, 1.47, and 1.55 V correspondingly, with an increase in the voltage, the current density rises (III). This could be accounted for by the reality that chloride ions from the RS destroyed the passive layers. Some electrode areas that had previously been passively protected from corrosion by flms are exposed to the solution

once again, and the elements of alloying like Zr, Al, and Ti participate in the charge transfer when the voltage is raised. The highest current densities (I°) (region IV), 132.4, 189.3, and 262.4 mA cm⁻², are reached for $T_{70}Z_{20}N_{75}T_{25}$, $T_{6}A_{4}V$, and Ti when the potentials E° (the voltage corresponding to the greatest current density) increase to approximately 1.99, 2.04, and 2.06 V, respectively. As the voltage increases and gradually replaces the reactions, the breakdown parts on the passive flms are restored.

Restoring the breakdown parts on the passive layers continues along with the voltage increase and gradually supplants the reactions. Ultimately, the three electrodes, $T_{70}Z_{20}N_{7.5}T_{2.5}$, T_6A_4V , and Ti, have respective current densities (I_{pass}^2) (region V) of 134.1, 176.9, and 276.9 µA cm⁻², all of which are quite steady values. This indicates a formal transition into the re-passive condition for the electrodes.

The potentiodynamic polarization approach can be used to analyze the passive behaviors to determine the relative stability of the passive layers in the specifc medium as well as the passivity tendency of the materials. Three parameters, including (E_L^{-1}) for the first passive zone and I° and E° for the re-passive zone, are correlated to the previous. E_L^{-1} distinguishes the difficulty in the first passive case. The system can become passive more easily, and the closer the materials are to the E_{corr} (corrosion potential) the more quickly they are protected from corrosion.

The regions exposed to localized corrosion are small as $I[°]$ is low, and the restoration times for passive films are very fast. Therefore, from the active stage to the re-passive stage, the electrodes are easier to convert. In a similar vein, when E° is low relative to I° , it is favorable for the system to enter the re-passive state. As can be seen in Fig. [1](#page-2-0) and Table [2,](#page-2-1) the $T_{70}Z_{20}N_{7.5}T_{2.5}$ has the lowest values of E_L^1 , E° , and I° in comparison to the other materials investigated. Based on the results already mentioned, it can be said that $T_{70}Z_{20}N_7$, $T_{2.5}$ enters the passive stage more readily.

Two factors—the voltage range and the I_{pass} in the passive stage—distinguish the stability of passive flms. The more expansive the voltage range, the harder it is for the passive layers to transfer from the passive stage to the active stage. Furthermore, the passive coatings appear to be more

Material					$\begin{array}{ccccccccc} I_{Corr} & E_{corr} & E_L^{-1} & E_H^{-1} & E^{\circ} & E_L^{-2} & I_{pas}^{-1} & I^{\circ} & I_{pass}^{-2} & CR \\ \mu A\,cm^{-2} & V & V & V & V & \mu A\,cm^{-2} & \mu A\,cm^{-2} & \mu A\,cm^{-2} & mpy \end{array}$	
$T_{70}Z_{20}N_{7,5}T_{2,5}$ 11.8 -0.558 0.336 1.46 1.99 2.13 87.7 132.4 134.1 6.10						
T_6A_4V	13.7				-0.524 0.606 1.47 2.04 2.14 98.28 189.3 176.9	7.13
Ti	29.5				-0.786 0.711 1.55 2.06 2.16 160.3 262.4 276.9	15.3

 E_{corr} is the corrosion potential, I_{corr} is the corrosion current density, E_L^{-1} and E_H^{-1} are the low limit and high limit potentials in the first passive region, respectively, I_{pass}^{-1} is the current density in the first passive region, *E*° is the potential in correspondence with the highest current density, *I* ° is the highest current density during the whole scanning range, E_L^2 is the low limit potential in the re-passive region, and (I_{pass}^2) is the current density in the re-passive region

stable because their dissolution rate is comparatively slow and their I_{pass}^{-1} , I_{pass}^{-2} values are low, regardless of whether they are in the primary passive stage or the re-passive stage, suggesting that the passive layers are more stable. The frst passive area voltage ranges are 1.124, 0.864, and 0.839 V for $T_{70}Z_{20}N_{7.5}T_{2.5}$, T_6A_4V , and Ti, respectively. Certainly, $T_{70}Z_{20}N_{7.5}T_{2.5}$ has the widest potential range. Similar to this, $T_{70}Z_{20}N_{75}T_{25}$ also exhibits low passive current densities, with values of 87.7 and 134.1 mA cm^{-2} in the initial passive and re-passive regions, respectively.

According to the study presented above, the passive layer that has developed on the $T_{70}Z_{20}N_{75}T_{25}$ surface is the most stable among the remnants. Because of the presence of alloying elements, like vanadium, aluminum, zirconium, niobium, and tantalum, that help to reduce anode activity and promote passivity, $T_{70}Z_{20}N_{7.5}T_{2.5}$ and T_6A_4V alloys have better passive characteristics than Ti.

3.2 Corrosion Resistance Resulted from EIS

The Nyquist plots of the samples $T_{70}Z_{20}N_{7.5}T_{2.5}$, T_6A_4V , and Ti after 1800s of immersion in a RS at 37 °C are shown in Fig. [2a](#page-3-0). Due to the frequency dispersion, it is revealed that all of the diagrams are portions of the imperfect semicircles [\[28](#page-13-2)]. It is evident from impedance diagrams' depressed semi-circular shape that a charge transfer process controls how readily titanium and its alloys corrode.

According to Bode plots (Fig. [2b](#page-3-0)), the Z_{mod} value (modulus of impedance) for $T_{70}Z_{20}N_{7.5}T_{2.5}$ (28.18 k Ω cm²) is larger than that for T₆A₄V alloy (16.60 kΩ cm²) and Ti (6.92 kΩ cm^2), respectively. The high impedance values show the typical passive flm capacitive response behavior [[29](#page-13-3)[–33](#page-13-4)].

The highest Z_{mod} value for $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy in RS suggests improved resistance to corrosion of the spontaneous oxide layer compared to T_6A_4V alloy and Ti. Additionally, the highest value of phase angle for the $T_{70}Z_{20}N_{75}T_{25}$ alloy (-76.88) compared to the T_6A_4V alloy (-75.85) and Ti (-67.02) shows that the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy may have a passive flm protecting it in the RS. Consequently, two layers of passive flm were modeled: the outer porous layer, which is in charge of the dissolution processes through the passive flm, and the inner compact barrier layer, which is in charge of the alloy's resistance [[29–](#page-13-3)[34](#page-13-5)].

An electric equivalent circuit with two time constants was used to describe the dual-outer/inner oxide layers [\[35](#page-13-6)]. The electrical circuit models were used to analyze the impedance spectra collected at the OCP, and the results were successfully used to ft the whole set of data for all materials under test $(T_{70}Z_{20}N_{7.5}T_{2.5}, T_6A_4V$, and Ti) utilizing the equivalent circuit (EC) shown in Fig. [3](#page-4-0). The elements of this equivalent circuit are as follows: Rs is the resistance of electrolyte, R_p and CPE_p are the resistance and capacitance of the porous oxide film, and R_b and CPE_b are the resistance and capacitance of the barrier oxide film $[29-34]$ $[29-34]$. To obtain effective compatibility between the results of the simulations and those of the experiments, pure capacitors were replaced with constant phase elements (CPE) in the ftting process.

The impedance of CPE was determined by [\[35](#page-13-6)]:

$$
Z_{\rm CPE} = \left[C(j\omega)^n\right]^{-1},\tag{1}
$$

where *C* is the capacitance, ω is the angular frequency, and n is the non-uniform current distribution attributed to surface inhomogeneity or roughness. Table [3](#page-4-1) displays the

Fig. 2 Nyquist plots (**a**) and Bode plots (**b**) of EIS data of $T_{70}Z_{20}N_{75}T_{2.5}$, T_6A_4V , and Ti electrodes after 30 min of immersion in a RS at 37 °C

Fig. 3 The equivalent circuit used for the EIS data ftting

Table 3 Fitting parameters of EIS obtained for a $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy, T_6A_4V alloy, and Ti in a RS at 37° C

main parameters for all studied samples (R_s, R_b, CPE_b, R_p) , and CPE_p) of the recommended EC. According to the fitting parameters, the inner flm has a stronger resistance to charge and species transport than the outer flm, which is confirmed by the largest values of R_b relative to R_p . The CPE_p values are superior to the CPE_b values, suggesting that the barrier layer is what gives the corrosion resistance. These data prove that the protection offered by the passive film is mostly attributed to the inner compact film $[36]$ $[36]$. As a result, the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy was discovered to have the highest resistance of the inner compact film. The n_1 and n_2 values are lower than 1. This refers to faults caused by surface heterogeneity, roughness, the creation of porous layers, and adsorption flms [\[37\]](#page-13-8).

3.3 Corrosion Resistance Resulted from OCP

The variations in the free corrosion potential with time for $T_{70}Z_{20}N_{7.5}T_{2.5}$, T_6A_4V , and Ti samples in a RS at 37 °C are shown in Fig. [4](#page-4-2). The nobility of the materials can be compared using the OCP values [\[38](#page-13-9), [39\]](#page-13-10). It is common knowledge that a high open-circuit potential value corresponds to a strong resistance to corrosion. In the case of Ti, the potential decreased for a short time (300 s) (the dissolution of the natural oxide layer), then quickly rose in the OCP to the greater positive potentials to indicate its capability to re-passivate, and a steady-state value of − 0.48 V was even-tually reached [\[40](#page-13-11), [41\]](#page-13-12). In the case of $T₆A₄V$, the potential appears to be more negative (-0.58 V) . However, with time, it starts to increase gradually to more positive potentials, indicating its ability to re-passivate, and a steady-state value

Fig. 4 Open-circuit potential behavior as a function of time of $T_{70}Z_{20}N_{7.5}T_{2.5}$, T_6A_4V , and Ti electrodes in a RS at 37 °C

at − 0.35 V was eventually reached. After a short time of decreasing potential (200 s), in comparison with Ti, the OCP values became more positive with time for $T_{70}Z_{20}N_7$, T_7 , This indicates the rapid re-passivation and reaching a steadystate potential of − 0.30 V. According to this characteristic, protective passive flms quickly form and serve as a barrier to metal disintegration, reducing the rate of corrosion. The results for PPCs are consistent with the steady-state potential of OCP, which highlights the order in which the longterm corrosion resistance of the samples reduces as follows: $Ti_{70}Zr_{20}Nb_{7.5}Ta_{2.5}$ > TiAlV > Ti.

3.4 Efect of Annealing Temperature

For titanium alloys, there are numerous diferent kinds of heat treatments. Annealing, aging, deformation heat treating, and chemical heat treating are frequently used processes. Diferent titanium alloys can beneft from annealing, which primarily serves to reduce stress, enhance alloy plasticity, and stabilize the structure. The recrystallization temperature should be higher than the stress-relieving annealing temperature, which should be in the extent of 450 to 650 °C. The characteristics of the alloy will decrease if the temperature rises above the phase transition point. Therefore, our studied alloy sample was subjected to annealing in the temperature range of 600–1000 °C.

3.4.1 Corrosion Resistance Resulted from PPCs

Figure [5](#page-5-0) shows the PPCs of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy without and with annealing at various temperatures in a RS with a $5-mVs^{-1}$ scan rate. The polarization curves for the unannealed and annealed samples at 600, 800, and 1000 °C showed active–passive behavior. The polarization curves without annealing are pushed toward a less noble potential, suggesting that the resistance to corrosion of the $T_{70}Z_{20}N_{75}T_{25}$ sample reduces. Table [4](#page-5-1) displays the electrochemical parameters deduced from the polarization curves. The sample annealed at 1000 $^{\circ}$ C showed the lowest E_{corr} $(-5.51 \times 10^{-1} \text{ V})$, the largest I_{corr} $(4.49 \times 10^{-5} \text{ A cm}^{-2})$, the worst resistance to corrosion, and the largest CR (corrosion rate) (23.30 mpy). However, the alloy annealed at 800ºC exhibited the highest E_{corr} (−2.45 × 10⁻¹ V), the lowest I_{corr} (1.53 × 10⁻⁶ A cm⁻²), the best resistance to corrosion,

Fig. 5 Potentiodynamic polarization curves of $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy in a RS after annealing at diferent temperatures with a sweep rate of 5 mVs^{-1}

Table 4 Electrochemical parameters obtained for a $T_{70}Z_{20}N_{75}T_{25}$ alloy in a RS annealed at diferent temperatures

Temperature $\rm ^{\circ}C$	$\frac{I_{\text{Corr}}}{A \text{ cm}^{-2}}$	- $\mathrm{E_{Corr}}$ v	$\frac{I_{\text{pass}}}{mA \text{ cm}^{-2}}$	CR. mpy
Unannealed	1.18×10^{-5}	0.558	0.114	6.10
600	2.49×10^{-6}	0.313	0.036	1.292
800	1.53×10^{-6}	0.245	0.009	0.795
1000	4.49×10^{-5}	0.551	0.611	23.30

and the least CR (0.795 mpy). The E_{corr} (−3.13×10⁻¹ V), the I_{corr} (2.49 × 10⁻⁶ A cm⁻²) and the CR (1.292 mpy) of the sample that was annealed at 600ºC were between those of the annealed samples at 800 and 1000 $\,^{\circ}$ C, as well as the unannealed sample ($E_{corr} = -6.46 \times 10^{-1}$ V, $I_{corr} = 1.18 \times 10^{-5}$, and CR = 6.10 mpy). Additionally, the I_{pass} of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample after annealing at various temperatures was seen to vary after the activation–passivation transition. The sample that was annealed at 1000ºC had the highest I_{pass} (0.611 mA cm⁻²), followed by the sample that was annealed at 600 °C (0.036 mA cm⁻²). The sample that was annealed at 800 °C had the lowest passivation current density (0.009 mA cm⁻²), although the difference was extremely tiny.

3.4.2 Corrosion Resistance Resulted from EIS

In Figs. [6](#page-6-0)a and b, the EIS examinations of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy at the OCP with 30 min of immersion in a RS without and with annealing at various temperatures are shown. According to Nyquist plots (Fig. [6a](#page-6-0)), the capacitive semicircle value of the unannealed sample is greater than that of the annealed sample at 1000 °C but lower than that of the annealed sample at 600 and 800 °C. The above findings demonstrate that the resistance to corrosion of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample without annealing and the annealed sample at a crucial temperature (1000 °C) reduces attributed to the dissolution of the passive layer, whereas the resistance to corrosion of the annealed sample at a crucial temperature rises (up to 800 °C). In Bode plots (Fig. [6b](#page-6-0)), as the annealing temperature rises from 600 to 800 $^{\circ}$ C, the Z_{mod} values sharply increase from 32.36 to 63.06 kΩ cm², and the maximum phase angles rise from -62.08 to -71.45° , but at very high annealing temperatures (1000 °C), the Z_{mod} values and maximum phase angles sharply decrease to 3.311 kΩ cm^2 and -17.38° , respectively, as they move slightly to a higher-frequency zone. These data indicate that at high annealing temperatures (600, 800 $^{\circ}$ C) the oxide layer on the surface of the alloy has high resistance, but at a higher annealing temperature 1000 °C, the oxide film suffers from the dissolution process. It was found that the EC

Fig. 6 Nyquist diagrams (**a**) and Bode plots (**b**) of $T_{70}Z_{20}N_{7.5}T_{2.5}$ at open-circuit potential in a RS after annealing at different temperatures

shown in Fig. [3](#page-4-0) could satisfactorily match the entire set of data for the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy. According to fitting parameters, the values of R_p and R_b rise as the annealing temperature rises (600–800 $^{\circ}$ C), indicating that the produced oxide layer on the surface of the alloy is more protected. Additionally, they reveal that the values of R_b are higher than R_p at the same annealing temperatures (Table [5](#page-6-1)), suggesting that the barrier layer has a high resistance to transporting both the charge and the species across it. Because there are slightly more processes of corrosion, R_p and R_b values are lower at annealing temperatures (1000 °C) than they are at 600 and 800 °C. When the annealing temperature is raised (between 600 and 800 °C), the CPE_p and CPE_b drop, suggesting that the two oxide films thickness has risen. At the same temperatures, the CPE_p is higher than the CPE_p, proving that the barrier oxide layer is in charge of the resistance to corrosion. The CPE_p and CPE_b values at annealing temperatures of 1000 °C are higher than they are between 600 and 800 °C, showing that the two oxide layers thickness is reduced. This outcome indicates that the two oxide layers thickness decreases at higher annealing temperatures as a result of their dissolution [[42](#page-13-13)].

3.4.3 Corrosion Resistance Resulted from OCP

Figure [7](#page-7-0) depicts the OCP of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy without and with annealing at various temperatures in a RS as a function of time. Generally, annealed samples at 600 and 800 °C possess a higher positive potential in comparison with those that are unannealed or annealed at 1000 °C. For the unannealed sample, shortly after the potential decreases, the OCP rapidly rises to a more positive potential, indicating that it may re-passivate rapidly. A steady-state value of -0.31 V was eventually reached. And for those annealed at 800 °C, the OCP increases in the positive trend, reaching a maximum steady-state value at -0.03 V, a very long and stable passive region. During the immersion of the annealed samples at 600 and 1000 °C, the potential initially changed in a negative direction. The local breakdown of the passive flm, which in turn resulted from the initial the initial dissolving of the native passivation layer on the titanium alloy surface, was most likely what caused this change in the negative trend. The curves fnally attain a stable state after a certain amount of time. This might be as a result of the development of a new passivation coat in RS, which slowed down the rate of OCP change. The potential was stabilized when the passivation layer dissolved and produced a prorated balance [[43\]](#page-13-14). At varying annealing temperatures, the $T_{70}Z_{20}N_{7.5}T_{2.5}$

Table 5 Fitting parameters of EIS obtained for the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy annealed at diferent temperatures in a RS

Temperature $\rm ^{\circ}C$	$R_{\rm c}$ $(\Omega \text{ cm}^2)$	R _b $(k\Omega \text{ cm}^2)$	CPE _b $(F cm2 H71-n1)$	n ₁		R_p CPE _p (Ω cm ²) (F cm ² H _z ¹⁻ⁿ²)	n ₂
Unannealed	44.56	31.59×10^3	45.60×10^{-6}	0.842	45.79	147.2×10^{-6}	0.895
600	24.93	64.05×10^3	34.20×10^{-6}	0.803	51.98	88.18×10^{-6}	0.872
800	18.55	112.3×10^3	28.69×10^{-6}	0.821	68.56	60.45×10^{-6}	0.852
1000	33.54	9.78×10^{3}	134.17×10^{-6}	0.758	14.24	277.35×10^{-6}	0.741

Fig. 7 Open-circuit potential behavior as a function of time for $T_{70}Z_{20}N_{7.5}T_{2.5}$ samples without and with annealing at different temperatures

alloy has a varied fnal steady-state potential. Figure [7](#page-7-0) shows that the OCP of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy ranges from -0.03 to − 0.55 V after being annealed at various temperatures. In spite of the fact that the trends of change of OCP for sample $T_{70}Z_{20}N_{7.5}T_{2.5}$ annealed at various temperatures were comparable, they varied in the time required to attain steady state. Additionally, the alloy that was annealed at 800 °C exhibited the highest potential, attaining − 0.03 V. The potential value of the sample annealed at 600 °C was lower, at − 0.27 V, while the sample annealed at 1000 °C had the lowest potential, at approximately $- 0.55$ V. These data demonstrate that the sample $T_{70}Z_{20}N_{7.5}T_{2.5}$ annealed at 800 °C had the greatest resistance to corrosion when compared to the samples annealed at 600 °C and unannealed, and when it was annealed at 1000 °C the resistance to corrosion was the worst. Therefore, it is recommended to anneal the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy at 800 °C to improve its corrosion resistance.

3.5 Impact of Immersion Time

3.5.1 Corrosion Resistance Resulted from PPCs

Figure [8](#page-7-1) illustrates the PPCs of the $T_{70}Z_{20}N_{75}T_{25}$ alloy in a RS without and with various immersion times, at 37 °C with a 5 -mVs⁻¹ scan rate. As the immersion time increases from one week to three weeks, the dissolution of the passive flm generated on the surface of the alloy becomes easier. Without immersion, the polarization curves behave in an active–passive manner and are moved toward a less noble potential, which indicates a reduction in the resistance to corrosion of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample. The active–passive

Fig. 8 Potentiodynamic polarization curves of $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy in a RS at various immersion times with a scan rate of 5 mVs⁻¹ at 37 °C

transition behavior may be seen in the polarization curves of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy at various immersion times. The current density rises quickly when the potential rises. This is probably attributed to the destruction of the native passive layer of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy, which led to the active dissolution behavior of the alloy. When the potential was greater than 0.20 V, the current density rose and entered the stable passive area. This may be the result of the surface producing a new passive flm to protect the alloy. The current density has reached a stable state, when the balance between the production and degradation of the passive layer has been achieved [[44\]](#page-13-15). The polarization curves with immersion are moved toward nobler potentials comparable to the polarization curves without immersion. This might be explained by the rapid cathodic reaction. (The right branch of the polarization curve). Using the following parameters, the corrosion behavior was estimated: I_{corr} , E_{corr} , I_{pass} , and CR (Table [6](#page-7-2)). It could be deduced that the resistance to corrosion of the alloy is greater without immersion than it is with immersion because the values of I_{corr} , I_{pass} , and CR are lower without immersion than they are with immersion. The sample at one

Table 6 Electrochemical parameters obtained for a $T_{70}Z_{20}N_{75}T_{25}$ alloy in a RS with various immersion times at 37 °C

Immersion time Week	I_{Corr} A cm ⁻²	$\frac{E_{\text{Corr}}}{V}$	I_{pass} mA cm ⁻²	Corr Rate mpy
Without immersion 1.18×10^{-5} 0.558 0.114				6.10
One week	2.47×10^{-5} 0.416		0.336	12.18
Two weeks	2.82×10^{-5} 0.435		0.594	14.65
Three weeks	3.31×10^{-5} 0.400		0.886	17.15

week of immersion time exhibits an I_{corr} value (3.76 \times 10⁻⁵ A cm⁻²) lower than the values of the other two samples $(4.70 \times 10^{-5}$ and 5.80×10^{-5} Acm⁻², respectively) and, as a result, this sample is therefore more resistant to corrosion than the other two samples. The lower I_{pass} implies that a stable passive flm is formed. At the one week of immersion, the sample exhibit the lowest I_{pass} value, indicating the formation of a highly stable passive flm. The CR value of the sample at three weeks of immersion is higher than that of the two other samples (at one and two weeks of immersion times), which indicates that this sample has the lowest corrosion resistance and displays that the CR enhances with longer immersion times.

3.5.2 Corrosion Resistance Resulted from EIS

Figures [9](#page-8-0)a and b report the EIS examinations of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy, without and with various immersion times in a RS at 37 °C. According to Nyquist plots (Fig. [9a](#page-8-0)), the capacitive semicircle value is higher without immersion than it is with immersion and the semicircle values get smaller with an increase in the immersion time. These outcomes show that the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample's resistance to corrosion reduces as the time of immersion increases and is higher without immersion than with immersion. Bode plots (Fig. [9b](#page-8-0)) show that without immersion, the Z_{mod} value $(28.18 \text{ k}\Omega \text{ cm}^2)$ and phase angle (-67.88°) are greater than when immersed. This suggests that the passive oxide coating is more protective without immersion than it is with immersion. As the immersion time increased, the Z_{mod} values fell from 14.45 to 0.776 kΩ cm². In addition, phase angles fall from -68.59° to -50.96° . These outcomes show that the oxide layer on the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy dissolves rapidly as immersion time in a RS is increased. In the examination of the EIS acquired at the OCP, it was observed that the entire data collection for the sample could be successfully ftted with the equivalent circuit shown in Fig. [3](#page-4-0) after evaluating a variety of various electrical circuit models. A two-layer model of the surface coating is used to support this. Table [7](#page-8-1) contains the parameters (Rs, Rp, CPEp, Rb, and CPEb) of the suggested equivalent circuit obtained for $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy without and with various immersion times in a RS. The results show that R_p and R_b decrease as immersion time in RS increases, indicating that the developed oxide coating on $T_{70}Z_{20}N_7$, T_2 , becomes less resistant as immersion time in RS increases. However, R_b is significantly larger than R_p . This suggests that the protection is supplied by the inner layer and is comparable with what Assis et al. reported for

Fig. 9 Nyquist diagrams (**a**) and Bode plots (b) of $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy at open-circuit potential in a RS at various immersion times at 37 °C

Ti alloys [[45](#page-13-16)]. The CPE_p and CPE_b enhance with longer times of immersion, showing that the thickness of two oxide coatings has reduced as a result of their dissolution at high immersion times. CPE_p is greater than CPE_b , indicating that the inner oxide coating is in charge of resistance to corrosion.

3.5.3 Corrosion Resistance Resulted from OCP

Figure [10](#page-9-0) shows the variations in the free corrosion potential of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy in a RS at various immersion times. The behavior of the potential time is completely changed with immersion. For the studied alloy, the OCP changed dramatically from -0.49 V at the beginning to − 0.34 V at the end of the measurement. As the immersion time is increased from one week to three weeks, it is possible that the dissolution of the passive layer becomes easier. The steady-state potential is achieved in a short time after immersion in RS, in comparison with those without immersion time. In all the samples within the frst several minutes of immersion, the potential was initially slightly negative. The local passive layer on the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy surface was dissolved at the initial step, which led to this shift in the negative trend. Eventually, after a certain amount of time, the curves reach a steady state. This might be attributed to the production of a new passive coating, slowing the rate at which the OCP changes. The potential becomes stable when the passivation coating disintegration rate and production are relatively balanced [[43](#page-13-14)].

At various immersion times, the fnal steady-state potential of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy varies. Additionally, the alloy that had been submerged for one week had the highest potential, measuring about -0.35 V. The alloy immersed for two weeks

Fig. 10 Variation of $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy open-circuit potential in a RS at various immersion times at 37 °C

had a lower potential, measuring about − 0.38. The alloy immersed for three weeks had the least potential, measuring about − 0.42 V. These data reveal that the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy immersed for one week has greater resistance two corrosions compared to the alloys immersed for two and three weeks, suggesting that the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy corrosion resistance increases as the immersion time decreases.

3.6 Microstructural Properties

An XRD structural investigation was carried out to understand the composition of phases and the microstructure of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample. In Fig. [11,](#page-9-1) the X-ray diffractograms for $T_{70}Z_{20}N_{75}T_{25}$ samples without and with annealing at various temperatures are displayed. The relationship between the diffraction angle (2θ) and the relative intensity (counts per second) is graphed. The peaks of the unannealed $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy are indexed to the (100), (002), (101), (102), (110), and (103) planes at 2θ values of 34.1, 37.6, 38.7, 50.0, 61.6, and 68.6°, respectively. These peaks correspond to those of the hexagonal α-Ti. The two peaks that appeared at $2θ = 37.6$ and 68.6° are due to the (110) and (211) levels of the β-Ti phase, respectively $[46]$. The results also found that the (101) plane was the most common crystallographic orientation for the hexagonal Ti phase. Using Scherrer formula ([2](#page-9-2)) [[47](#page-13-18)] and the (101) peak, the grain size of α phase was calculated to be 5.35 nm. Other TiZrNbTa alloys showed comparable results [\[48](#page-13-19)].

$$
D = \frac{0.9\lambda}{\beta \cos \theta},\tag{2}
$$

where *D* is the grain size, λ is the wavelength of the diffraction X-ray, β is the full-width at half-maximum of the diffraction peak, and θ is the angle of diffraction. There were

Fig. 11 The X-ray diffraction analysis obtained for the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy without and with annealing at diferent temperatures

no oxide peaks found in the unannealed sample, and all of the difraction peaks were connected to body-centered Ti and hexagonal close-packed Ti, indicating that the naturally produced Titania flms were amorphous, despite the tendency of titanium alloys to generate $TiO₂$ films at ambient temperature [\[49](#page-13-20)].

When the alloy samples were compared after being annealed at 600, 800, and 1000 °C, it was revealed that annealing at 600 °C resulted in the appearance of new peaks at 2θ values of 25.4, 31.5, 36.2, 53.71, and 63.7° (JCPDS No. 00-027-0911), which are consistent with those of the orthorhombic TiO₂ (JCPDS No. 01-084-1750), as well as two peaks of orthorhombic $Ti₂ZrO$ at 36.2 and 63.7° (JCPDS No. 00-027-0911). However, when annealing at 800 $^{\circ}$ C, additional peaks that are compatible with those of rutile, syn tetragonal TiO₂, and cubic $ZrO₂$ are formed (JCPDS) No. 01-076-0320 and 00-027-0997, respectively). However, annealing at 1000 °C, the same peaks that are comparable with those of rutile, syn tetragonal $TiO₂$, and cubic $ZrO₂$ appeared, as well as new peaks which are comparable with those of $ZrTiO₄$ (JCPDS No. 00-034-0415). Figure [11](#page-9-1) shows that the annealing altered the crystallization of the oxide, i.e., the amorphous oxide turns into the crystalline rutile TiO₂. Better corrosion resistance and biocompatibility would be provided by implants with a crystalline rutile layer rather than an amorphous $TiO₂$ layer [\[50](#page-13-21)].

3.7 Surface Morphology

The surface morphology of the polished (Fig. [12a](#page-11-0)) as well as the alloy samples at diferent immersion times and at diferent annealing temperatures is shown in Fig. [12.](#page-11-0) Increasing the immersion times (Fig. $12b$, c, d) leads to surface defects as a result of possible dissolution of the passive layer, especially after three weeks in comparison with the unimmersed sample. Increasing the annealing temperatures from 600 to 800 °C, on the other hand, changed the morphology from amorphous to crystalline, as confrmed by the XRD patterns (Fig. [10\)](#page-9-0). Annealing at 1000 °C causes microcracks to form, resulting in a less proactive (i.e., less corrosion resistant) surface. The presence of some small pits on the surface does not represent a big problem since there is less tendency for the alloy to pit, as shown from the polarization curves studied in Figs. [5](#page-5-0) and [8](#page-7-1), which do not refer to pitting in the potential range studied.

4 Conclusion

In this study, the in vitro corrosion resistance of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy has been evaluated and contrasted with that of T_6A_4V and Ti in RS. Electrochemical studies were used to examine the corrosion behavior of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy when it was annealed at 600, 800, and 1000 °C and immersed for various immersion times. The data in this work led to the following conclusions:

- 1) The Z_{mod} and R_b values of $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy (28.18) $kΩ$ cm² and 31.59 × 10³ kΩ cm², respectively) is greater than those of T₆A₄V alloy (16.60 kΩ cm² and 28.46×10^3 k Ω cm², respectively) and Ti (6.92 k Ω cm² and 17.14×10^3 k Ω cm², respectively), indicating that the spontaneous oxide coating for $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy has improved in its ability to resist corrosion. According to PPC's results, the I_{corr} value of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy (I_{corr} =11.8 µA cm⁻²) is also smaller compared to T₆A₄V (I_{corr}=13.7 µA cm⁻²) and Ti (I_{corr}=29.5 µA cm⁻²). Both EIS and PPCs data show that $T_{70}Z_{20}N_7$, $T_{2,5}$ has the highest level of corrosion resistance comparable to those of the T_6A_4V alloy and Ti.
- 2) In contrast to the T_6A_4V (OCP = 0.35 V) and Ti (OCP=− 0.48 V) samples, the values of OCP for the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample became more positive with time (-0.30 V) indicating that the $T_{70}Z_{20}N_{7.5}T_{2.5}$ is in a state of greatly stable passivation and is highly resistant to corrosion.
- 3) In comparison to the other samples, including annealed and unannealed ones, the $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy showed the best corrosion resistance when it was annealed at a temperature of 800 °C. The $T_{70}Z_{20}N_{7.5}T_{2.5}$ alloy annealed at 1000 \degree C had the greatest I_{pass}, $(0.611 \text{ mA cm}^{-2})$, whereas the alloy annealed at 800 °C had the lowest I_{pass} (0.009 mA cm⁻²).
- 4) The EIS results display that the passive flm is composed of a dual-outer and inner oxide layer and that at a critical high temperature (up to 800 °C) the resistance of corrosion of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample increases, but above this critical temperature (at 1000 °C) and without annealing, the resistance of corrosion decreases due to the dissolution process of the passive flm on the $T_{70}Z_{20}N_7$, T_2 , sample surface.
- 5) The OCP data show that the resistance to corrosion of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample treated at 800 °C (-0.03 V) was the best in comparison to the untreated and annealed samples at $600 \degree C$ (-0.31, -0.27 V, respectively) and the resistance to corrosion was the least when the alloy was treated at 1000 °C (-0.55 V).
- 6) The PPCs data show that without immersion, the alloy corrosion resistance is higher than its value both with immersion and with decreasing the immersion time. These results agree with the EIS and OCP data of the alloy at the same immersion times.
- 7) The $T_{70}Z_{20}N_{7.5}T_{2.5}$ system was discovered to have a structure made up of alpha- and beta-phases. An examination of the X-ray structure found a combination of hexagonal close-packed α-Ti (main phase, with 5.35-nm

Fig. 12 SEM images of the $T_{70}Z_{20}N_{7.5}T_{2.5}$ sample surface at different immersion times in RS at 37 °C **a** blank, **b** one week, **c** two weeks, **d** three weeks, and samples annealed at diferent temperatures **e** 600, **f** 800 °C, and **g** 1000 °C

grain size) and body-centered Ti. Of all the materials investigated in this work, the alloy $T_{70}Z_{20}N_{7.5}T_{2.5}$ can be regarded as a promising material appropriate for use as a biomaterial.

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Declarations

Conflict of interest The authors declare that they have no conficts of interest.

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