



# A Generic Model for Quantitative Prediction of Interactions Mediated by Efflux Transporters and Cytochromes: Application to P-Glycoprotein and Cytochrome 3A4

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## Abstract

**Background and Objective** The In Vivo Mechanistic Static Model (IMSM) is a powerful method used to predict the magnitude of drug–drug interactions (DDIs) mediated by cytochromes. The objective of this study was to extend the IMSM paradigm to DDIs mediated by efflux transporters and cytochromes.

**Methods** First, a generic model for this kind of interaction was devised. A flexible approach was then developed to estimate the characteristic parameters [the contribution ratios (CRs) and inhibition or induction potencies (IXs)] from clinical data by non-linear regression. Next, this approach was applied to the DDIs mediated by P-glycoprotein (P-gp) and cytochrome P450 (CYP) 3A4/3A5 in a large set of victim drugs and interactors. Lastly, the model and associated parameters were used to identify the DDIs most at risk of overexposure.

**Results** A total of 25 substrates and 26 interactors (three inducers, 23 inhibitors) could be considered in the regression analysis. The number of observations [area under the plasma concentration–time curve ratios or renal clearance ratios (Robs)] was 138. Fifty CRs and 57 IXs were estimated. The proportions of predictions within 0.67- to 1.5-fold Robs and within 0.5- to 2-fold Robs were 79% and 93% for the internal validation and 76% and 88% for the external validation, respectively. The median fold error was 0.98 (the ideal value is 1) and the interquartile range of the fold error was 0.36. The relative standard error of parameter estimates was a maximum of 15%.

**Conclusions** The IMSM approach was successfully extended to DDIs mediated by P-gp and CYP3A4/3A5. The method revealed good predictive performances by internal and external validation.

## Key Points

Pharmacokinetic drug–drug interactions mediated by membrane transporters and cytochromes may result in large variations of drug exposure.

A new approach is presented to predict the variation of exposure due to interactions mediated by P-glycoprotein and cytochrome P450 3A4/3A5.

This approach was applied to a large set of substrates and inhibitors or inducers. The predictive performances were suitable for clinical applications.

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## 1 Introduction

Pharmacokinetic drug–drug interactions (DDIs) are well-known to be a major factor of inter-individual variability in drug exposure [1]. As a result, drug agencies have issued guidelines to evaluate the potential DDIs during drug development [2, 3]. The strongest interactions are mediated by cytochromes and membrane transporters. Much effort has been put into devising quantitative methods to predict the impact of DDIs on drug exposure in order to reduce the experimental burden, duration, and cost of drug development. Currently, the favored approach relies on in vitro–in vivo extrapolation, using a physiologically based pharmacokinetic (PBPK) model [4, 5]. This approach is mainly used for metabolic, cytochrome-mediated DDIs. However, the importance of DDIs mediated by membrane transporters is now widely recognized [6]. These interactions may involve influx transporters such as organic anion transporter polypeptides (OATPs) [7–9] and efflux transporters such as P-glycoprotein [P-gp, also known as multidrug resistance 1 (MDR1) coded by the *ABCB1* gene] [10] or breast cancer resistance protein (BCRP, also known as ABCG2) [11], among others.

The PBPK approach allows complete description of the pharmacokinetics of the interaction, but this remains complex, time-consuming, and requires determination of the empirical scaling factors for application to clinical data [12, 13]. As a result, the PBPK approach is mainly used in the context of drug development. Besides this approach, when estimation of the variation of drug exposure in plasma at steady state is the major goal (such as in clinical settings), a static model is an attractive approach because of its simplicity. Static models for transporter-mediated DDIs have previously been described [14–16]. All of these approaches rely on some in vitro–in vivo extrapolations to estimate the parameters of the model.

Another approach to static models for predicting DDIs has been developed, which is based solely on clinical data. For this reason, the method is called the In vivo Mechanistic Static Model (IMSM). One feature of the IMSM is that the victim drugs and interactors are characterized by dimensionless parameters [the contribution ratios (CRs) and the inhibition or induction potencies (IXs)] that are easy to interpret. This approach was introduced by Ohno et al. [17, 18] to predict cytochrome P450 (CYP) 3A4-mediated DDIs. We extended the method to other cytochromes [19–22], the combined impact of DDIs and cytochrome polymorphism [23, 24], and, recently, the prediction of the inter-individual variability of DDIs [25]. The predictions made using the IMSM have proven to be accurate in a large dataset of more than 600 DDIs [26] and also for DDIs involving inhibitory metabolites [27].

In this study, the IMSM paradigm was extended to describe DDIs mediated by efflux transporters and cytochromes. First, a generic model for this kind of interaction was devised. A flexible approach was then developed to estimate the characteristic parameters (the CRs and IXs) from clinical data. Next, this new approach was applied to the DDIs mediated by P-gp and CYP3A4 in a large set of victim drugs and interactors. Lastly, the model and associated parameters were used to identify the DDIs with high risk of overexposure.

## 2 Methods

### 2.1 Generic Model

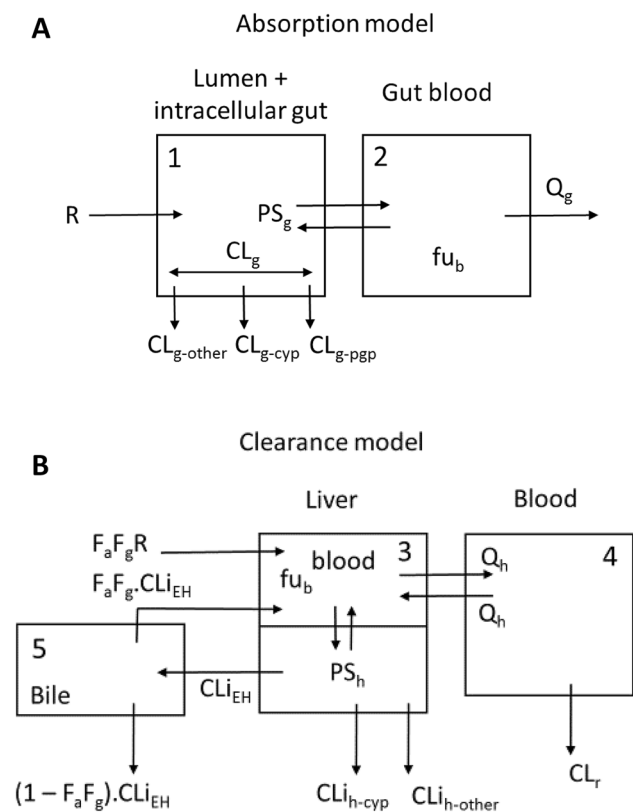
The goal of our model is to describe the impact of DDIs mediated by a single efflux membrane transporter and one or several cytochromes quantitatively. The victim drug, which is a substrate of the transporter and possibly of the cytochromes, is assumed to be administered by the oral route. The interactor, inhibitor, and/or inducer of the transporter, and possibly of the cytochromes, is also given by the oral route. The impact of the interaction is mainly characterized by the variation in exposure [area under the plasma concentration–time curve (AUC)] of the substrate in plasma. In this study, we do not attempt to model the variation of exposure in tissues (e.g., in brain).

The transporter is assumed to be present in the gut wall, liver (on the apical canalicular membrane), and kidney (on the apical membrane), resulting in drug secretion in the gut lumen, bile, and urine. The cytochromes are assumed to be located in the gut wall and liver. For simplicity here, we consider a single cytochrome (CYP3A4/A5) in the equations, but extension of the model to drugs metabolized by several cytochromes is straightforward.

A semi-physiologic, compartmental model is used to describe the pharmacokinetics of the victim drug. The two parts of the model are shown in Fig. 1a, b.

The first part is the absorption model, which is composed of two compartments: the lumen of the gastrointestinal tract combined with the intracellular space of the enterocytes and the gut blood. The second part is the clearance (CL) model, which is composed of four compartments: the liver blood, the intracellular space of hepatocytes, the bile compartment, and the blood of the systemic circulation. To derive the model, we assumed that the victim drug is given as a continuous zero-order input at rate  $R$  (e.g., in mg/h) in the lumen and that the system is at steady state. However, the final equations do not rely on this assumption.

The drug in compartment 1 may disappear with an apparent clearance of the gut ( $CL_g$ ), which is due to CYP3A4 metabolism ( $CL_{g-cyp}$ ), elimination by the lumen flow of the



**Fig. 1 a, b** Representation of the semi-physiologic compartmental model of drug absorption (a) and clearance (b).  $CL_{EH}$  enterohepatic cycle with an intrinsic clearance,  $CL_g$  clearance of the gut,  $CL_{h-cyp}$  clearance of the drug in the liver by cytochromes,  $CL_{h-other}$  clearance of the drug in the liver by other metabolites,  $CL_r$  renal clearance,  $CL_{g-cyp}$  clearance of the gut due to cytochromes,  $CL_{g-other}$  clearance of the gut due to other metabolites,  $CL_{g-pgp}$  clearance of the gut due to P-glycoprotein,  $F_a F_g$  fraction of drug that escapes from the gut,  $fu_b$  unbound drug concentration in blood,  $Q_g$  blood flow rate in gut blood,  $Q_h$  blood flow rate in liver blood,  $PS_g$  permeability surface product of the gut,  $PS_h$  permeability surface product of hepatocytes,  $R$  dosing rate

drug that has been effluxed from the enterocyte to the lumen and not reabsorbed ( $CL_{g-pgp}$ ), and elimination by the lumen flow before absorption ( $CL_{g-other}$ ). The drug in compartment 1 is transferred by passive diffusion to the gut blood with a gut permeability surface product  $PS_g$  (which has a clearance dimension). The concentration of drug in gut blood is  $C_2$ , and the blood flow rate is  $Q_g$ . The output rate of the drug from compartment 2 is  $Q_g \cdot C_2$ , which is by definition equal to  $F_a F_g \cdot R$ , where  $F_a F_g$  is the fraction of drug that escapes from the gut.

In the liver blood, part of the drug is transported into the systemic circulation with a blood flow rate  $Q_h$ , while the other part is eliminated by secretion into the bile or metabolism. The level of permeability of drug through the hepatocyte membrane is assumed to be high and there is no active transport of drug between liver blood and

hepatocyte intracellular water. Hence, the concentrations in liver blood and the intracellular space of hepatocytes are in rapid equilibrium. The rate of elimination from liver blood is  $fu_b \cdot C_3$  (drug concentration in compartment 3)  $\cdot CL_{i_h}$  (total hepatic intrinsic clearance), where  $fu_b$  is the unbound drug concentration in blood. The drug in the liver may undergo metabolism by cytochromes ( $CL_{i_h-cyp}$ ) and an enterohepatic cycle with an intrinsic clearance ( $CL_{i_{EH}}$ ), which is the sum of  $CL_{i_{h-pgp}}$  (the intrinsic clearance for efflux of the parent drug in bile) and  $CL_{i_{h-mr}}$  (the intrinsic clearance for metabolites that may be recycled, e.g., glucuronides, plus efflux by other transporters). The intact drug eliminated by active efflux and recycling metabolites goes into the bile compartment and a fraction ( $F_a F_g$ ) returns to the liver blood. From the systemic circulation ('blood' compartment), the drug may return to the liver or eventually be eliminated by the renal route (renal clearance [ $CL_r$ ]). The pharmacokinetics of the victim drug are assumed to be linear, i.e., the clearances are independent of the substrate dose.

As shown in "Appendix A", the drug concentration in blood ( $C_4$ ) may be calculated by solving the following system of equations:

$$F_a F_g = \frac{1}{1 + R_g} \tag{1a}$$

$$V_3 \cdot \frac{dC_3}{dt} = F_a F_g \cdot R + (F_a F_g \cdot fu_b \cdot CL_{i_{EH}} - fu_b \cdot CL_{i_h} - Q_h) \cdot C_3 + Q_h \cdot C_4 = 0 \tag{1b}$$

$$V_4 \cdot \frac{dC_4}{dt} = Q_h \cdot C_3 - (Q_h + CL_r) \cdot C_4 = 0 \tag{1c}$$

where  $R_g$  is the ratio of gut clearance ( $CL_g$ ) to the apparent gut permeability surface product ( $PS_{g-app}$ ) escaping from the gut, and  $V_3$  and  $V_4$  are the volume of compartments 3 and 4, respectively. This parameter is actually a tuning parameter that accounts for the fact that a high level of extraction may be reached in the gut, although the number of cytochromes and transporters is much less than in the liver. A high extraction (low  $F_a F_g$ ) may be understood as high  $R_g$ , i.e., a low  $PS_{g-app}$  compared with  $CL_g$ . In this system of equations, the parameters ( $R_g$ ,  $fu_b$ ,  $CL_{i_h}$ ,  $Q_h$ , and  $CL_r$ ) are fixed in accordance with the literature.

In DDI studies, non-compartmental analysis is frequently applied. Estimates of total apparent clearance ( $CL/F$ ) and possibly  $CL_r$  (drug amount in urine/AUC) are obtained in each arm of the studies (subjects who receive the victim drug alone and subjects who receive the victim drug and the interactor). Hence, the ratio of AUCs ( $R_{AUC} = AUC^*/AUC$ ) and the ratio of  $CL_r$  values ( $R_{CL_r} = CL_r^*/CL_r$ ) may be obtained (where \* denotes the parameter value for the substrate combined with the

interactor). These metrics of the interaction have been expressed as a function of a number of parameters characteristic of the substrate (the CRs) and the perpetrator (the IXs). The CR of each pathway that may be impacted by the interaction are defined as follows:

$$CR_{g-cyp} = \frac{CL_{g-cyp}}{CL_g} \quad CR_{g-pgp} = \frac{CL_{g-pgp}}{CL_g} \quad (2a)$$

$$CR_{h-cyp} = \frac{CL_{h-cyp}}{CL_{i_h}} \quad CR_{h-pgp} = \frac{CL_{h-pgp}}{CL_{i_h}} \quad CR_{h-mr} = \frac{CL_{h-mr}}{CL_{i_h}} \quad (2b)$$

$$CR_{r-pgp} = \frac{CL_{r-pgp}}{CL_r} \quad (2c)$$

where  $CR_{g-cyp}$  and  $CR_{g-pgp}$  are the contributions of CYP and Pgp to gut clearance,  $CR_{h-cyp}$ ,  $CR_{h-pgp}$  and  $CR_{h-mr}$  are the contributions of CYP, Pgp and recycling metabolites to hepatic intrinsic clearance, and  $CR_{r-pgp}$  is the contribution of Pgp secretion to renal clearance. Each CR may range from 0 to 1. In addition, the sum of CRs in the gut and the sum of CRs in the liver must each be less than or equal to 1.

The characteristic parameters of the interactor are defined as follows:

$IX_{g-cyp}$  and  $IX_{h-cyp}$  are the inhibition or induction potency of the interactor on CYP metabolism in the gut and the liver, respectively.

$IX_{g-pgp}$ ,  $IX_{h-pgp}$ , and  $IX_{r-pgp}$  are the inhibition or induction potency of the interactor on the efflux transporter in the gut, liver, and kidney, respectively.

For inhibitors, each IX may range from 0 (no inhibition) to  $-1$  (complete inhibition). For inducers, each IX may range from 0 (no induction) to  $\infty$  in theory. In practice, IX estimates of the most potent inducers have been  $\leq 10$ .

In case of interaction, the value of the parameters is modified as follows:

$$F_a F_g^* = \frac{1}{1 + R_g \cdot [1 + CR_{g-cyp} \cdot IX_{g-cyp} + CR_{g-pgp} \cdot IX_{g-pgp}]} \quad (3a)$$

$$CL_{i_h}^* = [1 + CR_{h-cyp} \cdot IX_{h-cyp} + CR_{h-pgp} \cdot IX_{h-pgp}] \cdot CL_{i_h} \quad (3b)$$

$$CL_{i_{EH}}^* = [CR_{h-pgp} \cdot (1 + IX_{h-pgp}) + CR_{h-mr}] \cdot CL_{i_{EH}} \quad (3c)$$

$$CL_r^* = [1 + CR_{r-pgp} \cdot IX_{r-pgp}] \cdot CL_r \quad (3d)$$

The drug concentration in blood in case of interaction  $C_4^*$  can be calculated by solving the system of Eqs. (2a)–(2c) with the parameters modified according to Eqs. (3a)–(3d). The predicted AUC ratio is  $C_4^*/C_4$ , although it is not computed exactly in this way (see “Appendix A”).

This procedure may be used to estimate the characteristic parameters by regression, using data from clinical studies of DDIs, and then to predict the magnitude of DDIs that have not been studied so far.

## 2.2 Estimation Method

For a given DDI, there are up to ten parameters (five CRs and five IXs) involved in the AUC ratio. Hence, it is not possible to estimate these parameters from a single clinical study; it is necessary to combine the results of several clinical studies involving a number of victim drugs and interactors. The parameters (the CRs and IXs) can then be estimated by regression. Even in this case, the number of datapoints will be hardly any larger than the number of parameters to be estimated, eventually leading to a large uncertainty regarding parameter estimates. To overcome this difficulty, we propose the following approach.

First, we use all available data, i.e., the AUC ratios (Eq. 1a–1c) and the  $CL_r$  ratios (Eq. 3a–3d).

Second, the parameters are estimated by weighted non-linear least squares. The weights are defined as the inverse of the expected standard error of the AUC ratio (see “Appendix B”).

Third, all the constraints of the parameters, defined earlier, are accounted for in the regression in order to improve the consistency (avoid unrealistic values) and the identifiability of the model. The constraints are enforced by penalization in the objective function.

Fourth, some parameters are fixed using available data for drug interactions involving only cytochromes but not transporters (see Sect. 2.3).

The objective function to be minimized with respect to the parameters is finally as follows:

$$OBJ(\hat{P}) = \sum_{i=1}^{ns} \left[ \frac{\ln(Rpred_i) - \ln(Robs_i)}{SE(\ln Robs_i)} \right]^2 + \sum_{i=1}^{ns} pen_i \quad (4)$$

where  $\hat{P}$  represents the current estimates of CRs and IXs, Rpred and Robs are the predicted and observed AUC and  $CL_r$  ratios, ns is the number of observations (number of AUC ratios and number of  $CL_r$  ratio), and pen is the value of the penalty if some constraints are violated (see “Appendix B”). The expected standard error of Robs is calculated according to our previous work [25] (see “Appendix B”).

To minimize the objective function, the simplex algorithm is used; this is a local optimizer, based on a derivative-free

method. This choice was made because the algorithm works well even with a complex set of constraints such as ours. The model was coded in Matlab® R2014b (MathWorks, Natick, MA, USA) and the function *fminsearch* was used for the simplex minimization of the objective function.

A confidence interval for the parameter estimates was obtained using a parametric bootstrap of the observations (see “Appendix B”).

### 2.3 Application to P-Glycoprotein

To evaluate and illustrate our approach, we considered the DDIs mediated by P-glycoprotein and CYP3A4/3A5.

A literature search was conducted in PubMed using the key words P-glycoprotein, drug interaction, and pharmacokinetics, with the results restricted to human studies in the period 1980–2017. After elimination of irrelevant or incomplete studies, a set of substrates and interactors was defined. Interactions studies with midazolam and alprazolam, which are CYP3A4/A5 substrates but not P-gp substrates, were also included in order to increase the precision of the estimates of IX of some interactors acting on CYP3A4/A5 and P-gp. Midazolam and alprazolam were chosen because (1) their  $F$  and  $F_g$  (1) their bioavailability ( $F$ ) and bioavailability in the gut ( $F_g$ ) are known, allowing the contribution of the gut and the liver to their pharmacokinetics to be disentangled; (2) a wide range of interaction studies have been published with each of them; and (3) their pharmacokinetics are appropriate for our purpose. Midazolam is highly metabolized by CYP3A4 in the gut ( $F_g = 0.51$ ) and in the liver, while alprazolam is weakly metabolized by CYP3A4 in the gut ( $F_g = 0.94$ ) but highly metabolized in the liver [28–30]. The interactions with midazolam and alprazolam allowed estimation of the  $IX_{g-cyp}$  and  $IX_{h-cyp}$  values for several interactors by root finding in Eq. (40) (see “Appendix A”).

To estimate the  $CR_{g-pgp}$ , we need at least one interactor whose  $IR_{g-pgp}$  is known or fixed. Itraconazole  $IR_{g-pgp}$  was fixed to  $-0.99$ . The reasons for this are that (1) itraconazole is responsible for the strongest known interaction with aliskiren, a P-gp substrate; (2) inhibition of P-gp in the gut was deemed to be the unique mechanism for this interaction; and (3) the concentration of drug producing 50% inhibition ( $IC_{50}$ ) of itraconazole for P-gp is 1.4 mg/L [31], a value far lower than the expected concentration of itraconazole in the gut lumen after a 200 mg dose.

The data were divided into two parts: the learning dataset was made up of the most informative studies with respect to the parameters to be estimated, given the assumed mechanisms of interaction; and the validation dataset consisted of the rest of the published data, involving a substrate and an interactor whose CRs and IXs had been estimated in the learning study.

The CRs and IXs were estimated as described earlier using the learning set. The goodness of fit was evaluated by several criteria. First, a plot of  $R_{pred}$  versus  $R_{obs}$  was examined and visually compared with the identity line. Second, the proportions of predictions within 0.67- to 1.5-fold  $R_{obs}$  and within 0.5- to 2-fold  $R_{obs}$  were calculated. Third, the median and the interquartile range of  $R_{pred}/R_{obs}$ , denoted as median fold error (MFE) and interquartile fold error (IQFE), were computed. Fourth, the confidence intervals of the parameter estimates were examined to ensure that all parameters were estimated with a good precision [the relative standard error (RSE) should be less than 30%]. Last, an external validation was carried out using the validation dataset. The  $R_{pred}$  was compared with  $R_{obs}$  for a range of interactions not included in the learning dataset.

A sensitivity analysis was conducted to assess the impact of fixing the pharmacokinetic parameters ( $R_g$ ,  $fu_b$ ,  $CL_{ih}$ ,  $Q_h$ , and  $CL_r$ ) to a single common value for all predictions with a given substrate. Because all of the pharmacokinetic parameters are derived from the oral clearance and the fraction of dose absorbed for the substrate given alone, the impact of the variation of these two parameters on the predicted AUC ratio was evaluated by simulation under different assumptions regarding the CR and IX values.

## 3 Results

Following the literature search, some data had to be excluded before analysis. The fexofenadine–carbamazepine interaction [32] was excluded because the interaction was deemed to be due in part to the transporter multidrug resistance protein 2 (MRP2) in addition to P-gp. The interactions of verapamil as a substrate with atorvastatin [33] and lovastatin [34] were discarded because the pharmacokinetics of verapamil are strongly non-linear.

A total of 25 substrates (including midazolam and alprazolam) and 26 interactors (three inducers, 23 inhibitors) were retained in the regression analysis. The number of observations  $n_s$  was 138, with 123 AUC ratios and 15  $CL_r$  ratios. The total number of parameters in the model was  $(25 + 26) \times 5 = 255$ . The number of parameters to be estimated was 107 (50 CRs and 57 IXs). The rest of the parameters were fixed either to zero (e.g., for midazolam and alprazolam,  $CR_{g-pgp} = CR_{h-pgp} = CR_{r-pgp} = 0$ ) or, for  $CR_{h-cyp}$  and  $IX_{h-cyp}$ , to the value determined previously [17, 18, 35]. The data are shown in Table 1. The fixed parameters are shown in Electronic Supplementary Material Table 1. In Table 1, comparison of the AUC ratio with the elimination half-life ( $t_{1/2}$ ) ratio provides information on the site of the interaction. Indeed, the AUC ratio is equal to  $(CL/CL^*) \times (F^*/F)$ , while

**Table 1** Data from drug–drug interaction studies used for the regression analysis

Substrate	Interactor	AUC ratio	$t_{1/2}$ ratio	CL <sub>r</sub> ratio	Assumed mechanism of interaction	Site of interaction	Reference
Aliskiren 75 mg	Cyclosporine 200 mg/day	4.28	1.77	NA	P-gp + OATP2B1 <sup>a</sup>	GI + liver	[45]
Aliskiren 75 mg	Cyclosporine 600 mg/day	4.99	1.81	NA	P-gp + OATP2B1 <sup>a</sup>	GI + liver	[45]
Aliskiren 300 mg	Ketoconazole 400 mg/day	1.76	NA	NA	P-gp	GI	[46]
Aliskiren 300 mg	Atorvastatin 80 mg/day	1.47	NA	NA	P-gp	GI	[46]
Aliskiren 300 mg	Verapamil 240 mg/day	1.88	0.84	NA	P-gp	GI	[47]
Aliskiren 150 mg	Itraconazole 200 mg/day	6.54	1.06	1.21	P-gp	GI	[48]
Aliskiren 300 mg	Amlodipine 10 mg/day	1.29	NA	NA	P-gp	GI	[49]
Apixaban 10 mg	Ketoconazole 400 mg/day	1.99	1.22	NA	P-gp + 3A4	GI + liver	[50]
Apixaban 10 mg	Diltiazem 360 mg/day	1.31	1.06	NA	P-gp + 3A4	GI + liver	[50]
Apixaban 10 mg	Naproxen 500 mg	1.54	1.00	NA	P-gp	GI	[51]
Apixaban 10 mg	Rifampicin 600 mg/day	0.46	0.61	NA	P-gp + 3A4	GI + liver	[52]
Atorvastatin 20 mg	Telaprevir 750 mg tid	7.88	0.72	NA	P-gp	GI	[53]
Atorvastatin 20 mg	Itraconazole 200 mg	2.50	1.30	NA	P-gp + 3A4	GI + liver	[54]
Atorvastatin 40 mg	Itraconazole 200 mg	3.31	2.90	NA	P-gp + 3A4	GI + liver	[55]
Atorvastatin 20 mg	Lopinavir/ritonavir 400/100 mg bid	5.90	NA	NA	P-gp + 3A4	GI + liver	[56]
Celiprolol 100 mg	Itraconazole 400 mg/day	1.80	1.00	NA	P-gp	GI	[57]
Cyclosporine 10 mg	Telaprevir 750 mg tid	4.60	4.38	NA	P-gp + 3A4	GI + liver	[58]
Cyclosporine 100 mg	Boceprevir 800 mg	2.70	1.38	NA	P-gp + 3A4	GI + liver	[59]
Cyclosporine <sup>b</sup>	Ketoconazole 200–400 mg/day	4.39	NA	NA	P-gp + 3A4	GI + liver	[60]
Cyclosporine 300 mg	Itraconazole 400 mg/day	2.00	NA	NA	P-gp + 3A4	GI + liver	[61]
Colchicine 0.6 mg	Atorvastatin 40 mg/day	1.24	1.13	NA	P-gp	Bile	[62]
Colchicine 0.6 mg	Ketoconazole 400 mg/day	2.86	4.15	NA	P-gp	Bile + kidney	[63]
Colchicine 0.6 mg	Cyclosporine 100 mg	3.17	3.05	NA	P-gp	Bile + kidney	[63]
Colchicine 0.6 mg	Ritonavir 200 mg/day	3.45	3.38	NA	P-gp	Bile + kidney	[63]
Colchicine 0.6 mg	Clarithromycin 500 mg/day	3.39	3.40	NA	P-gp	Bile + kidney	[63]
Colchicine 0.6 mg	Diltiazem 240 mg/day	1.77	2.27	NA	P-gp	Bile	[63]
Colchicine 0.6 mg	Verapamil 240 mg/day	1.99	2.75	NA	P-gp	Bile	[63]
Dabigatran 150 mg	Amiodarone 600 mg	1.60	NA	NA	P-gp	GI	[64]
Dabigatran 150 mg	Clarithromycin 1000 mg/day	1.55	NA	NA	P-gp	GI	[65]
Dabigatran 150 mg	Dronedarone 800 mg/day	2.40	NA	NA	P-gp	GI	[64]
Dabigatran 150 mg	Ketoconazole 400 mg/day	1.53	NA	NA	P-gp	GI	[64]
Dabigatran 150 mg	Quinidine 200 mg/2 h	1.53	NA	NA	P-gp	GI	[64]
Dabigatran 150 mg	Verapamil IR 240 mg	2.50	NA	NA	P-gp	GI	[66]
Dabigatran 150 mg	Ticagrelor 180 mg/day	1.46	NA	NA	P-gp	GI	[64]
Dabigatran 150 mg	Rifampicin 600 mg/day	0.33	NA	NA	P-gp	GI	[64]
Digoxin 0.75 mg	Clarithromycin 500 mg/day	1.7	NA	0.8	P-gp	GI + kidney	[67]
Digoxin 0.25 mg	Diltiazem 180 mg/day	1.51	1.29	NA	P-gp	GI + kidney	[68]
Digoxin <sup>b</sup>	Dronedarone 800 mg/day	2.5	NA	NA	P-gp	All	[69]
Digoxin 0.25 mg	Fostamatinib 200 mg/day	1.37	NA	NA	P-gp	GI	[70]
Digoxin 0.5 mg	Itraconazole 200 mg/day	1.5	1.25	0.80	P-gp	GI + kidney	[71]
Digoxin	Quinidine 200 mg/2 h	1.76	NA	0.69	P-gp	All	[72]
Digoxin 1 mg	Rifampicin 600 mg/day	0.70	1.00	1.00	P-gp	GI	[73]
Digoxin 0.5 mg IV	Ritonavir 300 mg/day ss	1.86	2.56	0.65	P-gp	Bile + kidney	[74]
Digoxin 0.4 mg	Ritonavir 400 mg/day ss	1.22	NA	1.00	P-gp	GI + bile	[75]
Digoxin 0.5 mg	Lopinavir/ritonavir 400/100 mg bid	1.81	NA	NA	P-gp	All	[76]
Digoxin C <sub>ss</sub> = 1 ng/mL	St John's wort 900 mg/day	0.71	1.00	1.00	P-gp	GI	[77]
Digoxin 0.5 mg	Telaprevir 750 mg tid	1.85	1.30	0.83	P-gp	GI + kidney	[78]
Digoxin 0.5 mg	Ticagrelor 400 mg/day	1.28	1.24	1.00	P-gp	Bile	[79]

**Table 1** (continued)

Substrate	Interactor	AUC ratio	$t_{1/2}$ ratio	$CL_r$ ratio	Assumed mechanism of interaction	Site of interaction	Reference
Digoxin 0.25 mg	Vandetanib 300 mg	1.23	1.00	0.91	P-gp	GI	[80]
Digoxin <sup>b</sup>	Verapamil	1.60	NA	1.00	P-gp	GI + bile	[81]
Digoxin 0.38 mg	Verapamil 240 mg/day	1.44	NA	1.00	P-gp	GI + bile	[82]
Edoxaban 60 mg	Ketoconazole 400 mg/day	1.87	1.00	NA	P-gp	GI	[83]
Edoxaban 60 mg	Erythromycin 2000 mg/day	1.85	1.00	NA	P-gp	GI	[83]
Edoxaban 60 mg	Cyclosporine 500 mg	1.73	1.00	NA	P-gp	GI	[83]
Edoxaban 60 mg	Dronedarone 400 mg	1.84	1.00	NA	P-gp	GI	[84]
Edoxaban 60 mg	Quinidine 300 mg	1.77	1.00	NA	P-gp	GI	[84]
Edoxaban 60 mg	Verapamil 240 mg	1.53	1.00	NA	P-gp	GI	[84]
Everolimus 2 mg	Cyclosporine 175 mg/day	2.68	1	NA	P-gp + 3A4	GI + liver	[85]
Everolimus 2 mg	Erythromycin 1500 mg/day	4.4	1.39	NA	P-gp + 3A4	GI + liver	[86]
Everolimus 2 mg	Ketoconazole 400 mg/day	15.3	1.87	NA	P-gp + 3A4	GI + liver	[87]
Everolimus 2 mg	Verapamil 240 mg/day	3.5	1.2	NA	P-gp + 3A4	GI + liver	[88]
Fexofenadine 60 mg	Itraconazole 200 mg/day	1.80	1.00	1.00	P-gp	GI	[89]
Fexofenadine 180 mg	Itraconazole 200 mg	2.29	1.00	0.72	P-gp	GI	[90]
Fexofenadine 180 mg	Itraconazole 200 mg	3.01	1.00	0.84	P-gp	GI	[90]
Fexofenadine 60 mg	Itraconazole 200 mg	2.97	1.00	1.00	P-gp	GI	[91]
Fexofenadine 120 mg	Lopinavir/ritonavir 400/100 mg bid	2.94	1.00	NA	P-gp	GI	[92]
Fexofenadine 120 mg	Lopinavir/ritonavir 400/100 mg	4.00	1.00	NA	P-gp	GI	[92]
Fexofenadine 120 mg	Ritonavir 100 mg	2.23	1.00	NA	P-gp	GI	[92]
Fexofenadine	Ritonavir 800 mg/day	1.4	1.00	NA	P-gp	GI	[93]
Fexofenadine	Rifampicin 600 mg/day	0.42	1.00	1.00	P-gp	GI	[94]
Fexofenadine 180 mg	St. John's wort 900 mg/day	0.86	1.00	NA	P-gp	GI	[95]
Fexofenadine 180 mg	St John's wort 900 mg/day	0.54	1.00	1.00	P-gp	GI	[96]
Fexofenadine 60 mg	Fluvoxamine 50 mg/day	1.78	1.00	1.00	P-gp	GI	[97]
Ledipasvir <sup>b</sup>	Verapamil 240 mg/day	1.60	NA	NA	P-gp	GI	[98]
Ledipasvir <sup>b</sup>	Rifampicin 600 mg/day	0.40	NA	NA	P-gp	GI	[98]
Ledipasvir <sup>b</sup>	Simeprevir <sup>b</sup>	1.80	NA	NA	P-gp	GI	[98]
Ledipasvir <sup>b</sup>	Cyclosporine 300 mg	1.00	NA	NA	P-gp	GI	[99]
Loperamide 16 mg	Quinidine 600 mg	2.20	1.00	NA	P-gp	GI	[100]
Loperamide 4 mg	Itraconazole 100 mg/day	3.81	1.57	1.00	P-gp + 3A4	GI + liver	[101]
Nadolol 30 mg	Itraconazole 100 mg/day	2.24	1.00	NA	P-gp	GI	[102]
Nadolol 30 mg	Rifampicin 450 mg/day	0.78	0.84	NA	P-gp	GI	[102]
Naloxegol 25 mg	Quinidine 600 mg	1.40	0.39	NA	P-gp	GI + bile	[103]
Rivaroxaban 10 mg	Ketoconazole 200 mg/day	1.82	0.78	0.66	P-gp + 3A4	Liver + kidney	[104]
Rivaroxaban 10 mg	Ketoconazole 400 mg/day	2.58	1.35	0.64	P-gp + 3A4	Liver + kidney	[104]
Rivaroxaban 10 mg	Ritonavir 600 mg bid	2.53	1.21	0.25	P-gp + 3A4	Liver + kidney	[104]
Sirolimus 10 mg	Diltiazem 120 mg/day	1.6	0.85	NA	P-gp + 3A4	GI + liver	[105]
Sirolimus 2-5 mg	Ketoconazole 400 mg/day	5	1.5	NA	P-gp + 3A4	GI + liver	[106]
Sirolimus <sup>b</sup>	Verapamil 240 mg/day	1.16		NA	P-gp + 3A4	GI + liver	[107]
Tacrolimus 0.5 mg	Boceprevir 800 mg	17.00	1.67	NA	P-gp + 3A4	GI + liver	[59]
Tacrolimus 0.5 mg	Telaprevir 750 mg tid	70.00	4.82	NA	P-gp + 3A4	GI + liver	[58]
Tacrolimus <sup>b</sup>	Ketoconazole 200–400 mg/day	2.39	NA	NA	P-gp + 3A4	GI + liver	[60]
Tacrolimus 7 mg	Ketoconazole 200 mg/day	2 <sup>c</sup>	NA	NA	P-gp + 3A4	GI	[108]
Tacrolimus 4 mg	Itraconazole 200 mg/day	5.6	NA	NA	P-gp + 3A4	GI + liver	[109]
Talinolol 100 mg	Carbamazepine 600 mg/day	0.85	1.00	1.50	P-gp + MRP2	GI + kidney	[110]
Talinolol 100 mg	Rifampicin 600 mg/day	0.65	0.85	1.00	P-gp + MRP2	GI + bile	[111]
Talinolol 50 mg	St John's wort 900 mg/day	0.69	0.81	1.00	P-gp	GI + bile	[112]

**Table 1** (continued)

Substrate	Interactor	AUC ratio	$t_{1/2}$ ratio	$CL_r$ ratio	Assumed mechanism of interaction	Site of interaction	Reference
Talinolol 50 mg	Verapamil 120 mg	1.31	NA	NA	P-gp	GI	[113]
Venetoclax 50 mg	Ketoconazole 200–400 mg/day	6.4	3.19	NA	P-gp + 3A4	GI + liver	[114]
Venetoclax 200 mg	Rifampicin 600 mg/day	0.27	0.37	NA	P-gp + 3A4	GI + liver	[115]
Venetoclax 200 mg	Rifampicin 600 mg	1.71	1.00	NA	P-gp	GI	[115]
Quinidine 200 mg	Itraconazole 100 mg	2.58	1.35	0.40	P-gp + 3A4	All	[116]
Quinidine 100 mg	Itraconazole 200 mg/day	2.4	1.60	0.50	P-gp + 3A4	All	[117]
Quinidine 200 mg	Rifampicin 600 mg/day	0.11	0.30	1.27	P-gp + 3A4	All	[118]
Midazolam	Clarithromycin 1000 mg/day	6.98	NA	NA	3A4	GI + liver	[119]
Midazolam	Erythromycin 1000 mg/day	3.77	NA	NA	3A4	GI + liver	[120]
Midazolam	Fluvoxamine 50–200 mg/day	1.66	NA	NA	3A4	GI + liver	[121]
Midazolam	Itraconazole 100–200 mg/day	7.97	NA	NA	3A4	GI + liver	[122]
Midazolam	Ketoconazole 200–400 mg/day	9.51	NA	NA	3A4	GI + liver	[123]
Midazolam	Lopinavir/ritonavir 400/100 mg bid	13	NA	NA	3A4	GI + liver	[56]
Midazolam	Rifampicin 600 mg/day	0.12	NA	NA	3A4	GI + liver	[123]
Midazolam	Ritonavir 600 mg/day	10.5	NA	NA	3A4	GI + liver	[124]
Midazolam	Simeprevir 150 mg/day	1.45	NA	NA	3A4	GI + liver	[125]
Midazolam	St John's wort 900 mg/day	0.48	NA	NA	3A4	GI + liver	[126]
Midazolam	Telaprevir 750 mg tid	8.96	NA	NA	3A4	GI + liver	[127]
Alprazolam	Carbamazepine 300 mg/day	0.42	NA	NA	3A4	Liver	[128]
Alprazolam	Erythromycin 1000 mg/day	2.37	NA	NA	3A4	Liver	[129]
Alprazolam	Fluvoxamine 50–200 mg/day	2	NA	NA	3A4	Liver	[130]
Alprazolam	Itraconazole 100–200 mg/day	2.66	NA	NA	3A4	Liver	[131]
Alprazolam	Ketoconazole 200–400 mg/day	3.75	NA	NA	3A4	Liver	[132]
Alprazolam	Rifampicin 600 mg/day	0.12	NA	NA	3A4	Liver	[133]
Alprazolam	St John's wort 900 mg/day	0.68	NA	NA	3A4	Liver	[134]
Alprazolam	Telaprevir 750 mg tid	1.35	NA	NA	3A4	Liver	[127]

3A4 cytochrome P450 3A4, AUC area under the plasma concentration–time curve, bid twice daily,  $CL_r$  renal clearance,  $C_{ss}$  steady-state plasma concentration, GI gastrointestinal tract, IR immediate release, IV intravenous, MRP2 multidrug resistance protein 2, NA not available, OATP organic anion transporter polypeptide, P-gp P-glycoprotein, ss steady state,  $t_{1/2}$  elimination half-life, tid three times daily

<sup>a</sup>OATP1B1 is not taken into account in the model

<sup>b</sup>Dose not reported

<sup>c</sup>Ratio of absolute bioavailabilities

the  $t_{1/2}$  ratio is equal to ( $CL/CL^*$ ) if the volume of distribution is not altered by the interaction. If the AUC ratio is different from unity while the  $t_{1/2}$  ratio is close to unity, then the site of interaction is the gut, not the liver.

The goodness-of-fit plots are shown in Fig. 2. These plots did not show any particular trend, as expected, but there is an outlier at (Rpred 16, Robs 70) corresponding to the tacrolimus–telaprevir interaction. The same plot in log–log scale with the 2-fold prediction error limits confirms the lack of trend, but there are ten values outside these 2-fold error limits (one outside the 3-fold error limits). The outliers are described in Table 2.

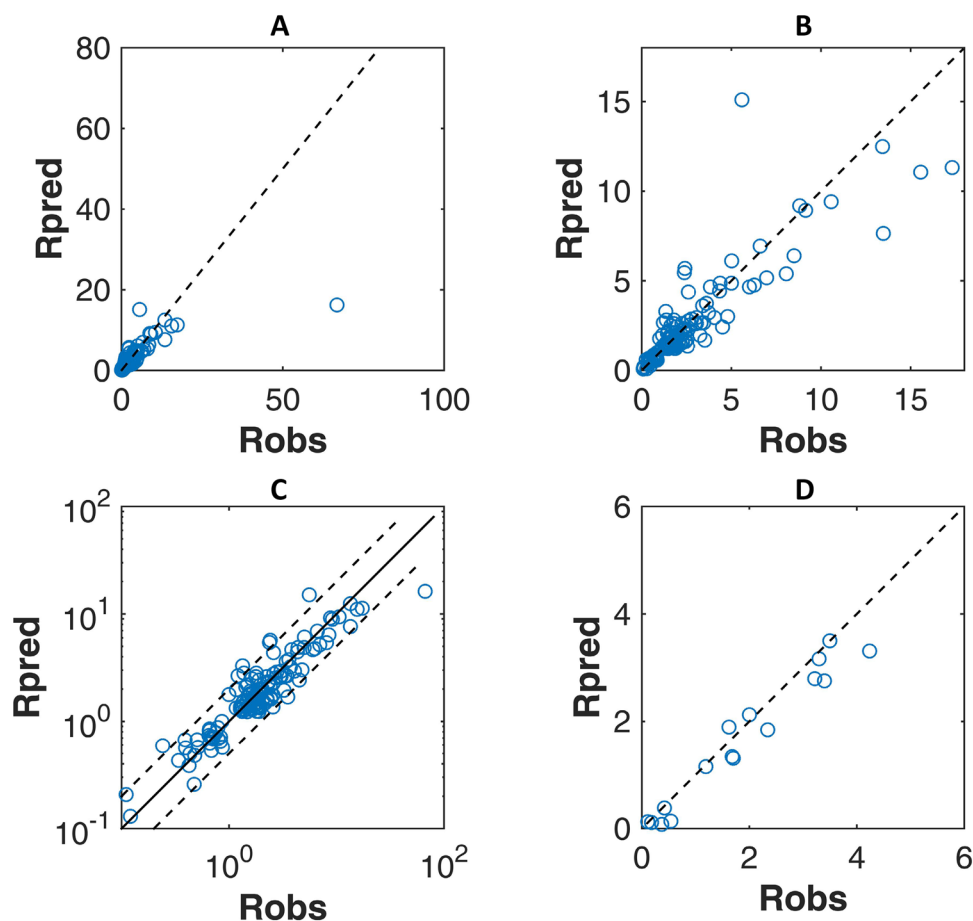
The proportions of predictions within 0.67- to 1.5-fold Robs and within 0.5- to 2-fold Robs were 79% and 93%, respectively. The MFE was 0.98 (the ideal value is 1). The

interquartile range of the fold error was 0.36. Regarding the confidence interval of the parameter estimates, the highest RSE was 15% for CRs and 10% for IXs (data not shown). Hence, the model was deemed acceptable.

The parameter estimates are shown in Tables 3 (CRs) and 4 (IXs). The substrates with a  $CR_{g-pgp}$  greater than 0.9 are digoxin and edoxaban. The substrates with the highest  $CR_{h-pgp}$  are colchicine (0.60) and fexofenadine (0.66). The substrates with a major elimination by tubular secretion are dabigatran ( $CR_{k-pgp} = 0.5$ ) and celiprolol (0.50). The major inhibitors of gut efflux are telaprevir, boceprevir, itraconazole, cyclosporine (ciclosporin), and lopinavir/ritonavir ( $IX_{g-pgp} < -0.9$ ). The strongest inhibitors of efflux in bile are ketoconazole and ritonavir ( $IX_{h-pgp} < -0.9$ ). Finally,



**Fig. 2** **a** Predicted ratio ( $R_{AUC}$  or  $R_{CL_r}$ ) versus observed ratio for the learning set. The dashed line is the identity line ( $y=x$ ). **b** Same plot as in **a** but the axes range is 0–18. **c** Predicted ratio ( $R_{AUC}$  or  $R_{CL_r}$ ) versus observed ratio in log–log scale. The continuous line is the identity line ( $y=x$ ), the lower dashed line is  $y=0.5x$ , and the upper dashed line is  $y=2x$ . **d** Predicted ratio ( $R_{AUC}$  or  $R_{CL_r}$ ) versus observed ratio for the validation set. The dashed line is the identity line ( $y=x$ ). An outlier at ( $R_{obs}=13.1$ ,  $R_{pred}=7.1$ ) is not in the figure.  $AUC$  area under the plasma concentration–time curve,  $CL_r$  renal clearance,  $R_{AUC}$  ratio of AUCs,  $R_{CL_r}$  ratio of  $CL_r$  values,  $R_{pred}$  predicted AUC and  $CL_r$  ratio,  $R_{obs}$  observed AUC and  $CL_r$  ratio



**Table 2** List of predictions with  $R_{pred}/R_{obs}$  outside of the 0.5–2 interval

Substrate	Interactor	$R_{pred}$	$R_{obs}$
Atorvastatin	Itraconazole 200 mg	5.7	2.5
Colchicine	Clarithromycin 500 mg/day	1.7	3.4
Tacrolimus	Telaprevir 750 mg tid	16.2	70
Venetoclax	Rifampicin 600 mg/day	0.09	0.27
Rivaroxaban	Ritonavir 600 mg bid	0.59	0.25
Alprazolam	Telaprevir 750 mg tid	3.3	1.35
Tacrolimus	Ketoconazole 200–400 mg/day	5.4	2.4
Tacrolimus	Itraconazole 200 mg/day	15.1	5.6
Sirolimus	Verapamil 240 mg/day	2.7	1.2
Fexofenadine	Ritonavir 800 mg/day ss	2.8 <sup>a</sup>	1.4 <sup>a</sup>

$AUC$  area under the plasma concentration–time curve, *bid* twice daily,  $CL_r$  renal clearance,  $R_{obs}$  observed AUC and  $CL_r$  ratio,  $R_{pred}$  predicted AUC and  $CL_r$  ratio, *ss* steady state, *tid* three times daily

<sup>a</sup>Ratio of renal clearances

cyclosporine and ritonavir are major inhibitors of tubular secretion ( $IX_{r-pgp} < -0.9$ ).

The results of the external validation on 17 DDIs are shown in Fig. 2d and Table 5. The MFE was 0.90 (the ideal value is 1) while 76% and 88% of the predicted values were

within 0.67- to 1.5-fold and within 2-fold of the observed values, respectively.

Some examples of predictions of the AUC ratio for several associations of drugs are shown in Fig. 3.

The results of the sensitivity analysis are shown in Electronic Supplementary Material Figs. 1 and 2. The main result is that the predicted AUC ratio is weakly sensitive to a small variation of the oral clearance and the fraction of dose absorbed in most regions of the plot. Hence, the choice of the reference values of the fixed parameters is not critical.

## 4 Discussion

In this study, a general model for analyzing and predicting DDIs mediated by an efflux transporter and a cytochrome was derived and evaluated. This a static (i.e., steady-state) mechanistic model, in the framework of CRs and IXs calculated solely from clinical data. This model, which we propose to call the ‘second-generation model’, is an improvement over our first-generation model, which did not (1) separate the intestine and the liver and (2) consider the impact of P-gp [35]. Although the model was applied only to P-gp as an efflux transporter, it could also apply to other

**Table 3** Contribution ratio estimates of the substrates

Substrate	CR <sub>g-pgp</sub>	CR <sub>g-cyp</sub>	CR <sub>h-pgp</sub>	CR <sub>h-cyp</sub>	CR <sub>r-pgp</sub>
Aliskiren 75 mg	0.87	0.00	0.00	0.00	0.00
Apixaban 10 mg	0.67	0.00	0.30	0.25	0.25
Atorvastatin 20 mg	0.66	0.28	0.00	0.27	0.00
Atorvastatin 40 mg	0.28	0.31	0.00	0.23	0.00
Celiprolol 100 mg	0.81	0.00	0.50	0.00	0.50
Cyclosporine 100 mg	0.29	0.14	0.00	0.53	0.00
Cyclosporine 10 mg	0.52	0.30	0.00	0.44	0.00
Colchicine 0.6 mg	0.00	0.00	0.60	0.25	0.15
Dabigatran 150 mg	0.85	0.00	0.00	0.00	0.50
Digoxin 0.75 mg	0.90	0.00	0.33	0.00	0.26
Edoxaban 60 mg	0.93	0.00	0.08	0.10	0.11
Fexofenadine 60 mg	0.45	0.00	0.66	0.00	0.35
Ledipasvir <sup>a</sup>	0.57	0.00	0.20	0.00	0.00
Loperamide 16 mg	0.76	0.00	0.00	0.35	0.00
Nadolol 30 mg	0.54	0.00	0.00	0.00	0.00
Naloxegol 25 mg	0.89	0.00	0.57	0.41	0.00
Rivaroxaban 10 mg	0.39	0.00	0.00	0.28	0.41
Tacrolimus 0.5 mg	0.85	0.14	0.10	0.57	0.00
Talinolol 100 mg	0.47	0.00	0.34	0.00	0.24
Venetoclax 50–200 mg	0.41	0.29	0.07	0.60	0.00
Quinidine 100–200 mg	0.52	0.05	0.17	0.43	0.40
Midazolam	0.00	0.90	0.00	0.86	0.00
Alprazolam	0.00	0.90	0.00	0.75	0.00
Sirolimus	0.35	0.55	0.20	0.36	0.00
Everolimus	0.36	0.54	0.20	0.58	0.00

CR<sub>g-cyp</sub> contribution ratio of the substrate on cytochrome P450 metabolism in the gut, CR<sub>h-cyp</sub> contribution ratio of the substrate on cytochrome P450 metabolism in the liver, CR<sub>g-pgp</sub> contribution ratio of the substrate on the efflux transporter in the gut, CR<sub>h-pgp</sub> contribution ratio of the substrate on the efflux transporter in the liver, CR<sub>r-pgp</sub> contribution ratio of the substrate on the efflux transporter in the kidney

<sup>a</sup>The dose was not reported

transporters with the same pattern of actions such as BCRP. Likewise, we considered a single cytochrome (CYP3A4/A5) in this study, but the extension to a model with several cytochromes is straightforward. Extension to multiple transporters would be more problematic because the number of parameters to estimate would be very large. Incorporation of the impact of transporter or cytochrome polymorphism in this framework is also quite simple; see Tod et al. [24] for a description of how to proceed. Consideration of the impact of polymorphism is useful to increase the identifiability of the model when the genetic variations have a strong impact on the activity of the transporter or cytochromes.

Relying solely on in vivo data for the computations has the advantage that (1) there is no need to extrapolate from in vitro data and to make all the assumptions associated with this approach [36]; and (2) the impact of all the molecular

species generated by the interactor (enantiomers, metabolites) is accounted for in the estimation of IXs [27]. The drawback is that for a new substrate or interactor, clinical data are required to be able to compute the CRs or IXs before other DDIs can be predicted. In addition, in vitro data, although not used in the computations, remain useful to ascertain the mechanisms of the interaction, or to fix some parameters at zero before applying the model.

The CR–IX framework is attractive because its parameters have an immediate physiological or pharmacological interpretation. Especially for inhibitors, the value of IX is more informative than an inhibition constant ( $K_i$ ) value, because the  $K_i$  by itself cannot be interpreted if the concentration of the inhibitor facing the enzyme or the transporter is unknown. However, the CRs (for the transporter) and IXs depend on the dose of the substrate and interactor, respectively. As the dose increases, the CRs might decrease (if the transporter is saturated) while the IXs increase (in absolute value). For example, the CR<sub>g-pgp</sub> of atorvastatin was 0.66 at 20 mg but 0.28 at 40 mg, while the CR<sub>g-pgp</sub> of cyclosporine was 0.52 at 10 mg but 0.29 at 100 mg. Another advantage of the CR–IX framework is that any kind of inhibition (competitive or not) is handled in the same way. On the other hand, the IXs are estimated at steady state (e.g., for inducers or mechanism-based inhibitors of cytochromes), and thus the time course of the interaction cannot be described.

Despite its assumptions (for the substrate: linear pharmacokinetics, no active influx, rapid equilibrium between blood and intracellular water, no variation of binding in blood, no variation of blood-to-plasma ratio; for the interactor: the value of IX is independent of the substrate) and approximations (the CR<sub>h-mr</sub> is fixed and the recycling metabolites are assumed to be completely back transformed to the parent drug), the goodness-of-fit criteria and predictive performance metrics did not invalidate the model. Of note, our approach performed better than the in vitro–in vitro extrapolation method using digoxin as a probe for P-gp-mediated DDIs [37].

Using such a model requires an appropriate method for estimating the parameters. We proposed a flexible strategy that allows all available data to be treated at once and to enforce a complex set of constraints on the parameters to be estimated. Depending on how informative the data at hand is, the parameter estimates might be precise or not. If some parameter estimates are imprecise, more data should be incorporated. In our case, the addition of data obtained with selective substrates of intestinal and hepatic CYP3A4 (alprazolam and midazolam), which are not substrates of P-gp, improved the precision of the estimated potency of several mixed interactors [e.g., ketoconazole, clarithromycin, rifampicin (rifampin)]. As a result, the confidence interval of the parameter estimates expressed as RSE was quite narrow (see “Results”).

**Table 4** Inhibition or induction potency estimates of the interactors

Interactor	$IX_{g-pgp}$	$IX_{g-cyp}$	$IX_{h-pgp}$	$IX_{h-cyp}$	$IX_{r-pgp}$
Amiodarone 600 mg	-0.60	0.00	0.00	0.00	0.00
Amlodipine 10 mg/day	-0.27	0.00	0.00	0.00	0.00
Atorvastatin 40–80 mg/day	-0.38	0.00	-0.30	0.00	0.00
Boceprevir 800 mg	-1.00	-0.44	-0.36	-0.98	0.00
Carbamazepine 300–600 mg/day	1.08	<i>4.31</i>	0.99	<i>1.42</i>	0.99
Clarithromycin 500–1000 mg/day	-0.46	-0.63	-0.28	-0.88	-0.48
Cyclosporine 100–600 mg/day	-0.93	-0.42	-0.53	-0.78	-0.91
Diltiazem 180–360 mg/day	-0.36	-0.57	-0.28	-0.80	-0.37
Dronedarone 400–800 mg/day	-0.65	0.00	-0.74	0.00	-0.65
Erythromycin 2000 mg/day	-0.42	-0.79	-0.61	-0.74	0.00
Fluvoxamine 50 mg/day	-0.87	0.00	0.00	-0.53	0.00
Fostamatinib 200 mg/day	-0.80	0.00	0.00	0.00	0.00
Itraconazole 100–400 mg/day	-1.00	-1.00	-0.63	-0.89	-0.83
Ketoconazole 200–400 mg/day	-0.51	-1.00	-0.99	-0.97	-0.45
Lopinavir/ritonavir 400/100 mg bid	-0.96	-0.87	-0.95	-0.95	0.00 <sup>a</sup>
Naproxen 500 mg	-0.75	0.00	0.00	0.00	0.00
Quinidine 200–600 mg	-0.45	0.00	-0.57	0.00	-0.58
Rifampicin 450–600 mg/day	1.26	<i>1.30</i>	1.11	8.83	0.91
Ritonavir 100 mg	-0.88	0.00	0.00	0.00	0.00
Ritonavir 200–600 mg/day ss	-0.73	-1.00	-0.84	-0.98	-1.00
Simeprevir	-0.64	-0.59	0.00	0.00	0.00
St John's wort 900 mg/day	1.09	<i>1.46</i>	0.94	<i>0.44</i>	0.00
Telaprevir 750 mg tid	-1.00	-0.88	-0.69	-0.99	0.00
Ticagrelor 180–400 mg/day	-0.45	0.00	0.00	0.00	0.00
Vandetanib 300 mg	-0.49	0.00	0.00	0.00	0.00
Verapamil 240 mg/day	-0.55	-0.48	-0.58	-0.71	0.00

All zero values and italicized values were fixed in the regression. All other parameters are estimates

*bid* twice daily,  $IX_{g-cyp}$  inhibition or induction potency of the interactor on cytochrome P450 metabolism in the gut,  $IX_{g-pgp}$  inhibition or induction potency of the interactor on the efflux transporter in the gut,  $IX_{h-cyp}$  inhibition or induction potency of the interactor on cytochrome P450 metabolism in the liver,  $IX_{h-pgp}$  inhibition or induction potency of the interactor on the efflux transporter in the liver,  $IX_{r-pgp}$  inhibition or induction potency of the interactor on the efflux transporter in the kidney, *ss* steady state, *tid* three times daily

<sup>a</sup>Could not be estimated due to the lack of data, but should be similar to the ritonavir value

Treating a large amount of data all at once might reveal some outliers, which requires close examination. An outlier might sometimes suggest that the mechanisms of the interaction are not those assumed. For example, an additional transporter might be involved. Alternatively, some subjects might have a genetic variant resulting in different activity of the transporter or the CYPs. Lastly, the assumption of independence of IX with respect to the substrate may be violated. In particular, the DDIs with tacrolimus are not well-predicted with this model; this issue with tacrolimus has been observed by others [38, 39]. The interactions with tacrolimus are better predicted when the  $K_i$  values of the inhibitors are measured with tacrolimus as the substrate [39]. In our paradigm, this is equivalent to considering that the IXs of the inhibitors are specific to tacrolimus. In other

words, the interactions with tacrolimus are poorly predicted with our approach, which should not be used in this case.

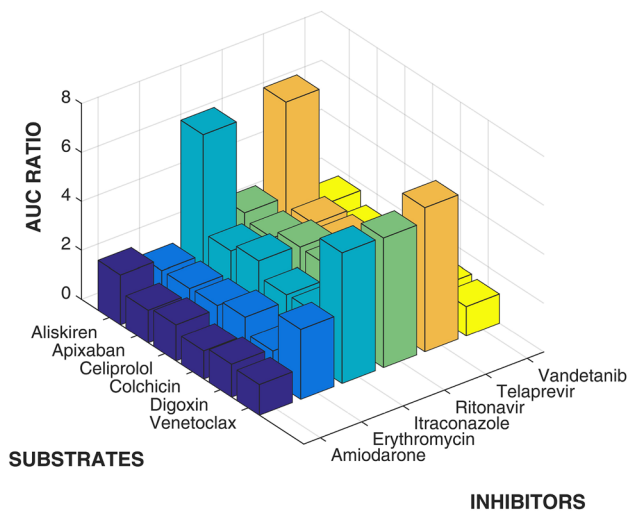
Despite these encouraging results, we do not pretend that all estimates obtained in this study are definitive. When new data become available, some estimates might be revised. For atorvastatin, some CYP3A4 metabolism was found ( $CR_{h-cyp} = 0.27$  and  $0.23$  from two different studies), although it is considered that the hepatic clearance of atorvastatin depends only on OATP influx at microdose [40].

From a practical point of view, the interactions involving efflux transporters at risk of overexposure are those involving (1) a substrate with a high CR for efflux combined with a strong efflux inhibitor; or (2) a substrate with mixed elimination (P-gp plus cytochrome) combined with a strong mixed inhibitor. According to the model and the parameter values (Tables 3 and 4), the following interactions, which

**Table 5** Validation dataset

Substrate	Interactor	Robs	Rpred	Reference
Atorvastatin	Dronedarone	1.7	1.31	[69]
Cyclosporine	Simeprevir	1.19	1.15	[125]
Cyclosporine	Diltiazem	1.62	1.89	[135]
Cyclosporine	Erythromycin	2.34	1.84	[136]
Cyclosporine	St John's wort	0.54	0.14	[137]
Digoxin	Amiodarone	1.68	1.34	[138]
Digoxin	Cyclosporine	2	2.13	[139]
Everolimus	Verapamil	3.50	3.50	[140]
Everolimus	Rifampicin	0.37	0.08	[141]
Loperamide	Ritonavir	3.22	2.79	[142]
Naloxegol	Diltiazem	3.4	2.75	[143]
Naloxegol	Rifampicin	0.11	0.13	[143]
Sirolimus	Rifampicin	0.18	0.11	[144]
Sirolimus	Cyclosporine	3.3	3.16	[107]
Sirolimus	Erythromycin	4.24	3.31	[107]
Sirolimus	Telaprevir	13.1	7.09	[145]
Tacrolimus	St. John's wort	0.42	0.38	[146]

AUC area under the plasma concentration–time curve,  $CL_r$  renal clearance, Robs observed AUC and  $CL_r$  ratio, Rpred predicted AUC and  $CL_r$  ratio



**Fig. 3** Prediction of the area under the plasma concentration–time curve (AUC) ratio for several associations of drugs

have not been studied so far, are expected to exhibit the highest  $R_{AUC}$ : aliskiren–telaprevir 6.5, venetoctax–ritonavir 5.3, venetoctax–telaprevir 5.9, venetoctax–itraconazole 5.3, naloxegol–lopinavir/ritonavir 15.6.

A limitation of the model is that only the impact of the interaction on exposure in plasma is described. However, efflux transporters such as P-gp and BCRP are also present at the blood–brain barrier. Inhibition of these transporters at

the blood–brain barrier leads to a higher drug concentration in the brain parenchyma [41–44]. This increased penetration in the brain may have beneficial or adverse consequences that cannot be predicted solely by the  $R_{AUC}$  in plasma. This is a limitation that can seldom be overcome, because measurements of drug concentration in the brain are generally not available in clinical trials. Hence, establishing a predictive model seems out of reach. Another limitation is that the description of the renal elimination of the drug is simplistic. Renal tubular secretion is taken into account through its contribution to  $CL_r$  by the parameter  $CR_{r-pgp}$ , and the interaction on tubular secretion is described through the potency of the interactor  $IX_{r-pgp}$ ; however, additional mechanisms of interaction due to modifications of renal blood flow, glomerular filtration rate, and tubular reabsorption, if present, are not taken into account.

## 5 Conclusions

In this study, the IMSM approach was successfully extended to DDIs mediated by P-gp and CYP3A4/3A5. The method revealed good predictive performances by internal and external validation, with the exception of tacrolimus. However, because clinical data are required to train the algorithm, the method cannot be applied at the stage of preclinical drug development. The IMSM approach is more useful during the clinical phase of development and in hospital settings, e.g., in the context of prescription analysis to optimize treatments. Currently, the IMSM approach is implemented for CYP-mediated DDIs on the free DDI-Predictor website (<https://www.ddi-predictor.org>). Extension to incorporate P-gp-mediated DDIs will occur in the future.

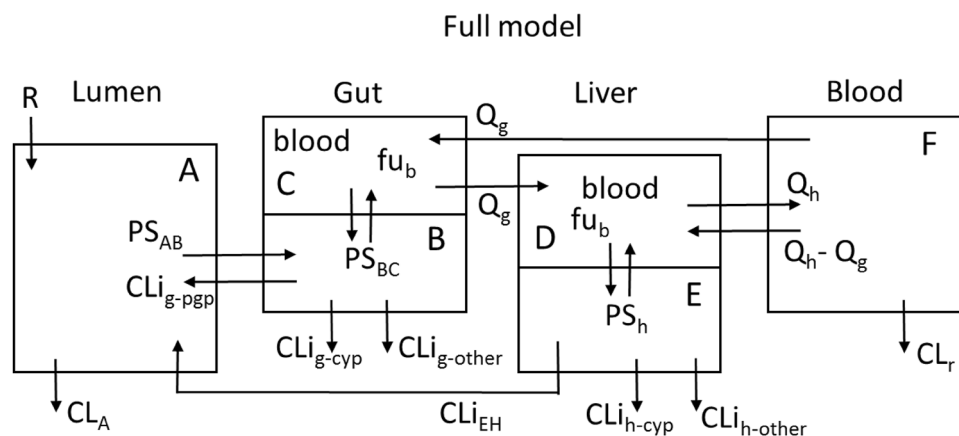
## Compliance with Ethical Standards

**Funding** No external funding was used in the conduct of this study.

**Conflict of Interest** Michel Tod, Nathalie Bleyzac, Sylvain Goutelle, and Laurent Bourguignon do not have any potential conflicts of interest that might be relevant to the content of this article.

## Appendix A: Derivation of the Model Equations

We need to derive the expression of (1) the concentration of the victim drug in blood; (2) its value when the interactor is co-administered; and (3) the metrics of the interaction: the AUC ratio and the ratio of renal clearances.



**Fig. 4** Full model.  $CL_A$  clearance in compartment A,  $CLi_{EH}$  intrinsic clearance of the enterohepatic cycle,  $CLi_{g-cyp}$  intrinsic clearance of the drug in the gut due to cytochromes,  $CLi_{g-other}$  intrinsic clearance of the gut due to other metabolism,  $CLi_{g-pgp}$  intrinsic clearance of the gut due to P-glycoprotein metabolism,  $CLi_{h-cyp}$  intrinsic clearance of the drug in the liver by cytochromes,  $CLi_{h-other}$  intrinsic clearance

of the drug in the liver by other metabolism,  $CL_r$  renal clearance,  $f u_b$  unbound drug concentration in blood,  $Q_g$  blood flow rate in gut blood,  $Q_h$  blood flow rate in liver blood,  $PS_{AB}$  permeability surface product in compartments A and B,  $PS_{BC}$  permeability surface product in compartments B and C,  $PS_h$  permeability surface product in the intercellular space of hepatocytes,  $R$  dosing rate

### Model with No Interaction (Substrate Alone)

The full model (Fig. 4) is the starting point of our approach. It is not the model ultimately used, but it allows understanding of the derivation of the final model. Because we are only interested by the impact of drug interaction on substrate clearance, the non-eliminating organs need not be considered in the model. In the gut and the liver compartment, the upper compartment represents blood, while the lower compartment represents the intracellular fluid. In compartment A (the gut lumen), the drug may be passively absorbed (with a permeability surface product  $PS_{AB}$ ) or eliminated by lumen fluid flow in the feces, with a flow rate  $CL_A$ . The drug is absorbed in the intracellular space of the gut (compartment B), where it may diffuse passively in the blood ( $PS_{BC} = PS_{CB}$ ) or undergo metabolism by CYP3A4 (with an intrinsic clearance  $CLi_{g-cyp}$ ) or efflux in the lumen ( $CLi_{g-pgp}$ ). The drug in the gut blood (compartment C) flows to the liver blood (compartment D) where it may diffuse in the intracellular space of hepatocytes (compartment E,  $PS_h$ ). In this study,  $PS_h$  is a passive process and the permeability of the drug is assumed to be high. Hence, the unbound drug concentrations in compartments D and E are considered to be equal, and compartment E is ignored in the equations.

The drug in the liver may undergo metabolism by CYP3A4 ( $CLi_{h-cyp}$ ) and an enterohepatic cycle with an intrinsic clearance  $CLi_{EH}$  that is the sum of  $CLi_{h-pgp}$  (the intrinsic clearance for efflux in bile mediated by P-gp) and  $CLi_{h-mr}$  (the intrinsic clearance for metabolites that may be recycled, e.g., glucuronides, plus efflux by other transporters).

The total intrinsic clearance in the liver is as follows:

$$CLi_h = CLi_{h-pgp} + CLi_{h-mr} + CLi_{h-cyp} + CLi_{h-other}$$

The drug that escapes the liver reaches the systemic circulation (compartment F) where it may be eliminated by renal route (with renal clearance  $CL_r$ ).

This model is not useful in practice for our purpose because it contains too many parameters, some of which cannot be easily measured or calculated. A more useful model is obtained by splitting the full model into two sub-models: the absorption model and the clearance model.

The absorption model represents the lumen and the gut. Because we are not interested in the pharmacokinetics of the drug, but rather only in the steady-state concentrations, the concentration in the lumen and in the intracellular space of the gut need not be distinguished. The enterohepatic cycle will be considered in the clearance model and does not appear in the absorption model. Therefore, compartment A and B are lumped together and the absorption model is represented by Fig. 1a.

From compartment 1, the drug may disappear with an apparent clearance  $CL_g$ , which is due to CYP3A4 metabolism ( $CL_{g-cyp}$ ), elimination by the lumen flow of the drug that has been effluxed and not reabsorbed ( $CL_{g-pgp}$ ), and elimination by the lumen flow before absorption ( $CL_{g-other}$ ). The passive diffusion between compartment 1 and 2 ( $PS_g$ ) is actually a tuning parameter that controls the residence time of the drug in compartment 1. A slow  $PS_g$  results in a long residence time in compartment 1, allowing more drug to be eliminated before reaching the liver, for a given  $CL_g$  value. The output rate of the drug from compartment 2 is  $Q_g \cdot C_2$ , which is by definition  $F_a \cdot F_g \cdot R$ , the rate of drug input to the liver that may be measured in a subject in whom the enterohepatic cycle has been interrupted by mechanical or

pharmacological means. Note that the systemic blood returning to the gut (from compartment F to compartment C in the full model) that would lead to a clearance from the gut is neglected, because the amount of CYP3A4 and P-gp in the gut is 90- and 41-fold lower, respectively, than in the liver [147, 148].

The clearance model represents the liver and the systemic blood compartment (Fig. 1b).

The fraction of drug that undergoes an enterohepatic cycle goes into the bile compartment, where it returns eventually in the liver after reabsorption in the gut. The corresponding rate of input is  $F_a \cdot F_g \cdot \text{CLi}_{\text{EH}} \cdot C_5$ . If the recycling is not fully efficient (e.g., because the glucuronides are not completely hydrolyzed in the lumen), an additional parameter must be introduced, but its value has to be fixed.

The model corresponding to Fig. 1a, b is described as a set of five differential equations [Eqs. (5)–(9)]. Since the system is considered at steady state, each equation is equal to zero:

$$V_1 \cdot \frac{dC_1}{dt} = R - (\text{CL}_g + \text{PS}_g) \cdot C_1 + \text{PS}_g \cdot \text{fu}_b \cdot C_2 = 0 \quad (5)$$

$$V_2 \cdot \frac{dC_2}{dt} = \text{PS}_g \cdot C_1 - (\text{fu}_b \cdot \text{PS}_g + Q_g) \cdot C_2 = 0 \quad (6)$$

$$V_3 \cdot \frac{dC_3}{dt} = F_a \cdot F_g \cdot R - (\text{fu}_b \cdot \text{CLi}_h + Q_h) \cdot C_3 + Q_h \cdot C_4 + F_a \cdot F_g \cdot \text{CLi}_{\text{EH}} \cdot C_5 = 0 \quad (7)$$

$$V_4 \cdot \frac{dC_4}{dt} = Q_h \cdot C_3 - (Q_h + \text{CL}_r) \cdot C_4 = 0 \quad (8)$$

$$V_5 \cdot \frac{dC_5}{dt} = \text{fu}_b \cdot \text{CLi}_{\text{EH}} \cdot C_3 - \text{CLi}_{\text{EH}} \cdot C_5 = 0 \quad (9)$$

Equation (9) implies that, at steady state,  $C_5 = \text{fu}_b \cdot C_3$ . Hence, the bile compartment may be omitted in the system provided that Eq. (7) is rewritten as follows:

$$V_3 \cdot \frac{dC_3}{dt} = F_a \cdot F_g \cdot R - (\text{fu}_b \cdot \text{CLi}_h + Q_h) \cdot C_3 + Q_h \cdot C_4 + F_a \cdot F_g \cdot \text{CLi}_{\text{EH}} \cdot \text{fu}_b \cdot C_3 = 0 \quad (10)$$

The system of equations may be further simplified by deriving an expression for  $F_a \cdot F_g$ .

Rearranging Eq. (6) yields:

$$C_1 = \frac{\text{fu}_b \cdot \text{PS}_g + Q_g}{\text{PS}_g} \cdot C_2 \quad (11)$$

Let's define the apparent  $\text{PS}_g$  as follows:

$$\text{PS}_{g-\text{app}} = \frac{Q_g}{\text{fu}_b \cdot \text{PS}_g + Q_g} \cdot \text{PS}_g \quad (12)$$

Using this definition, the concentration  $C_2$  is expressed as follows:

$$C_1 = \frac{Q_g}{\text{PS}_{g-\text{app}}} \cdot C_2 \quad (13)$$

The sum of Eqs. (5) and (6) yields:

$$R = \text{CL}_g \cdot C_1 + Q_g \cdot C_2 \quad (14)$$

Replacing  $C_1$  with its expression and rearranging, we get the following:

$$R = \frac{Q_g \cdot (\text{CL}_g + \text{PS}_{g-\text{app}})}{\text{PS}_{g-\text{app}}} \cdot C_2 \quad (15)$$

The output rate of the drug escaping from the system is  $Q_g \cdot C_2$ . By definition the product  $F_a \cdot F_g$  is as follows:

$$F_a \cdot F_g = \frac{Q_g \cdot C_2}{R} \quad (16)$$

Substituting  $R$  with Eq. (14) yields:

$$F_a \cdot F_g = \frac{\text{PS}_{g-\text{app}}}{\text{PS}_{g-\text{app}} + \text{CL}_g} = \frac{1}{1 + (\text{CL}_g / \text{PS}_{g-\text{app}})} = \frac{1}{1 + R_g} \quad (17)$$

With this expression, Eqs. (5) and (6) are no longer needed to compute  $C_3$  and  $C_4$ .

The system of equations reduces to its final form:

$$F_a \cdot F_g = \frac{1}{1 + R_g} \quad (18)$$

$$V_3 \cdot \frac{dC_3}{dt} = F_a \cdot F_g \cdot R + (F_a \cdot F_g \cdot \text{fu}_b \cdot \text{CLi}_{\text{EH}} - \text{fu}_b \cdot \text{CLi}_h - Q_h) \cdot C_3 + Q_h \cdot C_4 = 0 \quad (19)$$

$$V_4 \cdot \frac{dC_4}{dt} = Q_h \cdot C_3 - (Q_h + \text{CL}_r) \cdot C_4 = 0 \quad (20)$$

This system is solved in matrix form by matrix inversion to obtain  $(C_3, C_4)$ .

In Eqs. (18)–(20), the drug is assumed to be administered at a constant rate  $R$  and  $C_4$  is the steady-state concentration. In case of repeated administration by oral route at intervals ( $\tau$ ),  $C_4$  would be the time-average concentration, the ratio of AUC from time zero to  $\tau$  on  $\tau$ . Because the pharmacokinetics of the victim drug are assumed to be linear,  $\text{AUC}_\tau$  is equivalent to the AUC from time zero to infinity ( $\text{AUC}_\infty$ ) after the first dose. Hence, Eqs. (18)–(20) may be used to characterize the AUC after single or repeated dosing.

### Model with Interaction (Substrate + Interactor)

The DDI is assumed to alter the efflux by P-gp (in the gut, liver, and kidney) and the metabolism by cytochromes (in the gut and liver).

To describe the DDI, we define the CR of each pathway that may be impacted by the interaction as follows:

$$CR_{g-cyp} = \frac{CL_{g-cyp}}{CL_g} \quad CR_{g-pgp} = \frac{CL_{g-pgp}}{CL_g} \quad (21)$$

$$CR_{h-cyp} = \frac{CL_{h-cyp}}{CL_{i_h}} \quad CR_{h-pgp} = \frac{CL_{h-pgp}}{CL_{i_h}} \quad CR_{h-mr} = \frac{CL_{h-mr}}{CL_{i_h}} \quad (22)$$

$$CR_{r-pgp} = \frac{CL_{r-pgp}}{CL_r} \quad (23)$$

where each CR may range from 0 to 1. In addition, the sum of CRs in the gut and the sum of CRs in the liver must both be  $\leq 1$ .

The characteristic parameters of the interactor are defined as follows:

$IX_{g-cyp}$  and  $IX_{h-cyp}$  are the inhibition or induction potency of the interactor on CYP metabolism in the gut and the liver, respectively.

$IX_{g-pgp}$ ,  $IX_{h-pgp}$ , and  $IX_{r-pgp}$  are the inhibition or induction potency of the interactor on the efflux transporter in the gut, liver, and kidney, respectively.

For inhibitors, each IX may range from 0 (no inhibition) to  $-1$  (complete inhibition). For inducers, each IX may range from 0 (no induction) to  $\infty$  in theory. In practice, IX estimates of the most potent inducers have been  $\leq 10$ .

Using these definitions, the expression of the parameters impacted by the interaction may be derived. The superscript \* denotes the parameters whose value is changed by the interaction.

In case of interaction, the value of  $CL_g$  becomes  $CL_g^*$ , which is expressed as follows:

$$CL_g^* = \left[ CR_{g-cyp} \cdot (1 + IX_{g-cyp}) + CR_{g-pgp} \cdot (1 + IX_{g-pgp}) + (1 - CR_{g-cyp} - CR_{g-pgp}) \right] \cdot CL_g \quad (24)$$

which becomes the following after simplification:

$$CL_g^* = [1 + CR_{g-cyp} \cdot IX_{g-cyp} + CR_{g-pgp} \cdot IX_{g-pgp}] \cdot CL_g \quad (25)$$

And:

$$F_a F_g^* = \frac{1}{1 + R_g \cdot [CR_{g-cyp} \cdot (1 + IX_{g-cyp}) + CR_{g-pgp} \cdot (1 + IX_{g-pgp}) + (1 - CR_{g-cyp} - CR_{g-pgp})]} \quad (26)$$

which becomes the following after simplification:

$$F_a F_g^* = \frac{1}{1 + R_g \cdot [1 + CR_{g-cyp} \cdot IX_{g-cyp} + CR_{g-pgp} \cdot IX_{g-pgp}]} \quad (27)$$

The value of  $CL_{i_h}$  becomes  $CL_{i_h}^*$ , which is expressed as follows:

$$CL_{i_h}^* = [1 + CR_{h-cyp} \cdot IX_{h-cyp} + CR_{h-pgp} \cdot IX_{h-pgp}] \cdot CL_{i_h} \quad (28)$$

while

$$CL_{i_{EH}}^* = [CR_{h-pgp} \cdot (1 + IX_{h-pgp}) + CR_{h-mr}] \cdot CL_{i_{EH}} \quad (29)$$

with

$$CL_{i_{EH}} = [CR_{h-pgp} + CR_{h-mr}] \cdot CL_{i_h}$$

The value of  $CL_r$  becomes  $CL_r^*$ :

$$CL_r^* = [1 + CR_{r-pgp} \cdot IX_{r-pgp}] \cdot CL_r \quad (30)$$

The value of the substrate concentration in blood in case of interaction,  $C_4^*$ , is calculated by solving the system of Eqs. (18)–(20) with  $CL_g^*$ ,  $CL_{i_h}^*$ ,  $CL_{i_{EH}}^*$ , and  $CL_r^*$  replacing  $CL_g$ ,  $CL_{i_h}$ ,  $CL_{i_{EH}}$ , and  $CL_r$ , respectively. The predicted AUC ratio is therefore as follows:

$$R_{AUC} = \frac{C_4^*}{C_4} \quad (31)$$

But, as explained in the following section, the AUC ratio is not obtained exactly in this way.

### Calculation of the Substrate Parameters and the Area Under the Plasma Concentration–Time Curve (AUC) Ratio

The goal is to estimate the CRs (other than  $CR_{h-mr}$ ) and the IXs by regression, given the data (the AUC ratios).

For a given substrate, the values of oral clearance from plasma in the control group ( $CL_{oral,p}$ ), bioavailability ( $F$ ),  $CL_r$ ,  $fu_b$ , blood-to-plasma concentration ratio (BPR),  $Q_h$ , and  $CR_{h-mr}$  are common to all interactions with this substrate. These values are extracted or imputed from the literature.

When there is an enterohepatic cycle, it is necessary to distinguish the ‘effective’ fraction of dose absorbed are oral administration, which will be denoted  $F^+$ , from the fraction of dose absorbed when the enterohepatic cycle is suppressed

by pharmacological or mechanical means,  $F_{\text{noEHC}}$ . Following Tse et al. [149], the relationship between  $F^+$  and  $F_{\text{noEHC}}$  may be derived as follows:

$$F^+ = \frac{F_{\text{noEHC}}}{1 - E_b \cdot F_{\text{noEHC}}} \quad \text{so that} \quad F_{\text{noEHC}} = \frac{F^+}{1 + E_b \cdot F^+} \quad (32)$$

where  $E_b$ , the coefficient of extraction of the drug to the bile, is approximated by  $(\text{CR}_{\text{h-pgp}} + \text{CR}_{\text{h-mr}})$ . For our purpose, the values of the pharmacokinetic parameters without an enterohepatic cycle need to be derived in order to calculate the impact of the interaction properly.

The rest of the parameters are therefore calculated as follows:

$$\text{CLiv} = F_{\text{noEHC}} \cdot \text{CLoral}_p / \text{BPR} \quad (33)$$

$$\text{CL}_h = \text{CLiv} - \text{CL}_r \quad (34)$$

where  $\text{CL}_r$  is renal clearance from blood.

$$F_h = 1 - (\text{CL}_h / Q_h) \quad (35)$$

where  $Q_h$  is set to 89 L/h [150].

$$\text{CLi}_h = \text{CL}_h / (f_{\text{ub}} \cdot F_h) \quad (36)$$

$$F_a F_g = F_{\text{noEHC}} / F_h \quad (37)$$

$$R_g = (1 - F_a F_g) / F_a F_g \quad (38)$$

Using the current estimate of  $\text{CR}_{\text{h-pgp}}$ :

$$\text{CLi}_{\text{EH}} = [\text{CR}_{\text{h-pgp}} + \text{CR}_{\text{h-mr}}] \cdot \text{CLi}_h \quad (39)$$

Using the current estimates of CRs and IXs,  $F_a F_g^*$ ,  $\text{CLi}_h^*$ ,  $\text{CL}_{\text{EH}}^*$ , and  $\text{CL}_r^*$  are calculated according to Eqs. (27)–(30), allowing  $C_4^*$  to be calculated by solving Eqs. (18)–(20). In the computations, the dosing rate  $R$  is fixed to an arbitrary value (e.g.,  $R = 100$ ). The output of the model is expressed as  $\text{CLoral} = R/C_4$  and  $\text{CLoral}^* = R/C_4^*$ . The AUC ratio is  $\text{CLoral}/\text{CLoral}^*$ . Assuming that the BPR of the victim drug concentration is unchanged by the interactor, the ratio of blood clearances is equal to the ratio of clearances from plasma, because the BPR cancels each of these clearances out in the ratio.

### Calculation of the Inhibition or Induction Potencies (IXs) of Interactors with Midazolam and Alprazolam as Substrates

Midazolam and alprazolam are not effluxed by P-gp. Hence, all parameters pertaining to the efflux may be removed from the model. After rearrangement, the following expression for the AUC ratio is obtained:

$$R_{\text{AUC}} = \frac{(1 + R_g)}{1 + R_g [1 + \text{CR}_{\text{g-cyp}} \text{IX}_{\text{g-cyp}}]} \cdot \frac{1}{[1 + \text{CR}_{\text{h-cyp}} \cdot \text{IX}_{\text{h-cyp}}]} \quad (40)$$

where the  $\text{CR}_{\text{h-cyp}}$  values are known from our previous work [35] and  $\text{CR}_{\text{g-cyp}}$  values are fixed to 0.9 because no other metabolic pathways are known in the intestine for these substrates. If the AUC ratios of the interaction of midazolam and alprazolam are known for an interactor, then we have two equations with two unknowns ( $\text{IX}_{\text{g-cyp}}$  and  $\text{IX}_{\text{h-cyp}}$ ). The solution may be obtained by root finding or regression. The values of  $\text{IX}_{\text{g-cyp}}$  and  $\text{IX}_{\text{h-cyp}}$  were obtained in this way for carbamazepine, ketoconazole, itraconazole, erythromycin, fluvoxamine, rifampicin, ritonavir, and St John's Wort. These values are weakly sensitive to the value assumed for  $\text{CR}_{\text{g-cyp}}$  (i.e., 0.9).

### Calculation of the IXs of Interactors with Aliskiren as Substrate

The interactions with aliskiren are assumed to arise solely by P-gp inhibition in the gut. Therefore:

$$R_{\text{AUC}} = \frac{(1 + R_g)}{1 + R_g [1 + \text{CR}_{\text{g-pgp}} \text{IX}_{\text{g-pgp}}]} \quad (41)$$

where  $\text{CR}_{\text{g-pgp}} = 0.87$ . Hence, the  $\text{IX}_{\text{g-pgp}}$  values of amlodipine, atorvastatin, cyclosporine, ketoconazole, and verapamil were fixed by solving Eq. (41).

## Appendix B: Objective Function

The objective function to be minimized with respect to the parameters is finally as follows:

$$\text{OBJ}(\hat{P}) = \sum_{i=1}^{ns} \left[ \frac{\text{Ln}(\text{Rpred}_i) - \text{Ln}(\text{Rob}_i)}{\text{SE}(\text{Ln Rob}_i)} \right]^2 + \sum_{i=1}^{ns} \text{pen}_i \quad (42)$$

where  $\hat{P}$  are the current estimates of CRs and IXs,  $\text{Rpred}$  and  $\text{Rob}$  are the predicted and observed AUC and  $\text{CL}_r$  ratios (i.e.,  $\text{AUC}^*/\text{AUC}$  and  $\text{CL}_r^*/\text{CL}_r$ ),  $ns$  is the number of observations (number of AUC ratio and number of  $\text{CL}_r$  ratio),  $np$  is the number of parameters to be estimated, and  $\text{pen}$  is the value of the penalty if some constraints are violated. The expected standard error of  $\text{Rob}$  is calculated according to our previous work [25].



The constraints and the penalties associated with violation of the constraints are as follows: For each substrate:

$$\text{if all CRs} > 0 \text{ and } < 1 \text{ then pen} = 0 \text{ else pen} = 1000 \quad (43)$$

$$\text{if } \sum(\text{CR}_g) < 1 \text{ and } \sum(\text{CR}_h) < 1 \text{ then pen} = 0 \text{ else pen} = 1000 \quad (44)$$

For each inhibitor:

$$\text{if all IXs} > -1 \text{ and } < 0 \text{ then pen} = 0 \text{ else pen} = 1000 \quad (45)$$

For each inducer:

$$\text{if all IXs} > 0 \text{ then pen} = 0 \text{ else pen} = 1000 \quad (46)$$

The expected standard error of  $\bar{R}_{\text{Obs}}$  is calculated as follows. When the AUC ratio is  $> 1$ :

$$\text{SE}(\text{Ln } \bar{R}_{\text{Obs}}) = \left( \frac{1}{\text{nsuj}} \left[ 0.191 \left( \frac{\bar{R}_{\text{Obs}} - 1}{\bar{R}_{\text{Obs}}} \right)^2 + 0.0289 \right] \right)^{0.5} \quad (47)$$

When the AUC ratio is  $< 1$ :

$$\text{SE}(\text{Ln } \bar{R}_{\text{Obs}}) = \left( \frac{1}{\text{nsuj}} \left[ 0.191 (1 - \bar{R}_{\text{Obs}})^2 + 0.0289 \right] \right)^{0.5} \quad (48)$$

where  $\text{nsuj}$  is the number of subjects in the clinical study from which the geometric mean ratio  $\bar{R}_{\text{Obs}}$  was calculated. These equations reflect the larger uncertainty associated with  $\bar{R}_{\text{Obs}}$  values far from unity.

A confidence interval for the parameter estimates was obtained by a parametric bootstrap of the observations. Based on these equations for  $\text{SE}(\text{Ln } \bar{R}_{\text{Obs}})$ , a synthetic dataset is generated by sampling  $\text{Ln } \bar{R}_{\text{Obs}}$  values in a normal distribution with mean  $\text{Ln } \bar{R}_{\text{Obs}}$  and standard deviation  $\text{SE}(\text{Ln } \bar{R}_{\text{Obs}})$ . The parameters are estimated with this synthetic dataset. This procedure is repeated 30 times. The final point estimate of each parameter and its standard error are taken as the mean and standard deviation of the 30 estimates. A higher number of replicates did not result in significant variations of the standard deviation.

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