

Impact of Taguchi Optimization in Fiber Surface Plasmon Resonance Sensors Based on Si₃N₄ Layer

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Abstract

This article exhibits a fiber plasmonic sensor based on a silver (Ag) layer and a silicon nitride ($Si₃N₄$) layer with a wide dynamic range of refractive index sensing. The Taguchi (L9) orthogonal array method is applied to optimize the design parameters such as fiber core, sensing region length, and the thickness of $Ag/Si₃N₄$ layers. The performance of the structure is investigated for the full-width half maxima (FWHM) as the smaller the better (STB). The smaller FWHM favors accurate detection, high-quality factor, and better sensitive detection of biomolecules. With the use of analysis of variance (ANOVA), it is evident that for the normalized transmitted power, the Ag layer thickness contributes 47.36%, while the Si_3N_4 layer thickness contributes 0.06% only. Furthermore, the length of the sensing region has the highest dominating factor efect of 53.26% whereas the thickness of the Si_3N_4 layer has the least dominating factor effect of 6.90% on FWHM. This work has shown the highest sensitivity of 6287 nm/RIU whereas the quality factor and detection accuracy are 873.19 RIU⁻¹ and 87.31 respectively. Hence, Taguchi's optimization approach is suitable in multilevel optimization of diferent control factors that lead to the robust design of the fber SPR sensor.

Keywords Taguchi optimization · Surface plasmon resonance · Silver · Silicon nitride · Sensor

1 Introduction

Surface plasmon resonance (SPR) is a well-known technique with potential sensing applications in a variety of domains, including biomedical science and environmental science [[1,](#page-8-0) [2](#page-8-1)]. In recent years, the SPR sensor has gained popularity because of its label-free and real-time sensing [\[3](#page-8-2), [4](#page-8-3)]. In traditional SPR sensing, a glass prism along with a thin metal flm is employed to excite the surface plasmons (SPs) at the metal–dielectric interface. This phenomenon was frst

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described in 1968 by Kretschmann using a high refractive index (RI) prism to couple light at the metal–dielectric interface surrounded by the sensing medium, in which angular interrogation method was used to see the sharp dip in the refectivity spectrum [\[5](#page-8-4)]. However, the bulky and movable prism setup limits the prism-based sensing approach. The growing expectation for miniaturized, low-cost sensors suitable for remote sensing has been attracting researchers to propose new fber-based sensors. Lidberg et al. originally presented SPR technology in a fber-based sensor in 1983, which initiated this technology in the SPR sensing applications. These types of sensors have been widely employed in biomedical science, food safety, biomolecules detection, and environmental protection, etc. $[6–10]$ $[6–10]$ $[6–10]$ $[6–10]$. In the fiber sensing approach, a glass prism is replaced with the fber core that is used to guide light waves and a small portion of fber cladding is removed. Over unclad fber, a metal layer is produced. For the evaluation of sensor performance, the sample to be detected is positioned around the layer of metal, and the resonance wavelength shift with the RI change is observed [\[11,](#page-8-7) [12\]](#page-8-8). Silver, copper, and gold are the most common plasmonic active metals. These are produced on the

unclad fber core's surface. In comparison to these materials, gold is extremely stable. Because silver and copper have weak chemical stability and these are supposed to oxidize fast. This makes them lesser stable for the SPR sensor. As a result, applying a protective layer on the surface of these layers is a feasible option for making an SPR sensor more durable [[13](#page-8-9)[–15](#page-8-10)]. In recent times, the use of transition metal dichalcogenide (TMDC) materials such as WSe2, MoS2, MoSe2, and WS2 is seen in SPR sensing. These materials serve as supporting materials for enhancing plasmons in SPR sensing $[16–21]$ $[16–21]$ $[16–21]$.

In this work, a protective layer of silicon nitride (Si3N4) has been deposited over the surface of the Ag layer that makes this structure more stable. Si3N4 has a huge bandgap $({\sim}5 \text{ eV})$ and received interest due to its excellent chemical and thermal stability [[22](#page-8-13), [23](#page-8-14)]. Here, we have used the Taguchi method to optimize the designing parameters employed in the proposed fber SPR sensor. In the traditional approach, one factor at a time is optimized such that when the thickness of one layer is optimized, the thickness of the other layer is kept fxed. This process makes the high numbers of optimization tests. Due to this reason, the parameters generated with this approach are not sufficient for the designing of such sensors. The Taguchi technique aids in the creation of a robust design by taking into account all of the sensor's control elements. As a result, a high-performance SPR biosensor can be made with a small number of tests.

2 Sensor Design Parameters

Taguchi's optimized design of the proposed fber-based SPR sensor is represented in Fig. [1.](#page-1-0) Here, the fused silica fber core having a diameter of 600 µm is utilized to carry light waves from one side of the fiber to another side, in which a 10-mm length of fber cladding is removed. Fiber optic probe with 600 µm of core diameter can be fabricated by removing 10-mm cladding portion from the middle region of a fber using a sharp blade. After that, acetone and deionized water can be used to clean the unclad area of the

Fig. 1 Plasmonic fber-based sensor structure

fber [[24\]](#page-8-15). The RI of the fused silica core (ncore) may be calculated using the given dispersion equation [[25](#page-8-16)] :

$$
n_{\text{core}}(\lambda) = \left(1 + \frac{a_1 \lambda^2}{\lambda^2 - b_1^2} + \frac{a_2 \lambda^2}{\lambda^2 - b_2^2} + \frac{a_3 \lambda^2}{\lambda^2 - b_3^2}\right)^{1/2} \tag{1}
$$

Here, $a_1 = 0.6961663$, $b_1 = 0.0684043$, $a_2 = 0.4079426$, $b_2 = 0.1162414$, $a_3 = 0.8974794$, and $b_3 = 9.896161$ are the Sellmeier coefficients and " λ " is the wavelength in nm [\[26](#page-8-17)]. Ag metal layer of the thickness of 50 nm is grown over the unclad portion of the fber. Liquid-phase deposition technique can be used to deposit silver layer over the unclad surface of optical fiber [\[27](#page-8-18)]. The dielectric constant of this layer (ϵ_{Ag}) is computed using the given Drude relation [[28\]](#page-8-19) :

$$
\epsilon_{Ag}(\lambda) = 1 - \frac{\lambda^2 \lambda_c}{\lambda_p^2(\lambda_c + i\lambda)}
$$
 (2)

here, λ_c stands for collision (damping) wavelength and is defned as the wavelength corresponding to the damping of the oscillations of the electron density because of the collision among the electrons. The value of λ_c is 1.7614 × 10⁻⁵m. Furthermore, λ_p stands for plasma wavelength. It is the wavelength that corresponds to the frequency of the electron density oscillations in the metal. The value of λ_n is 1.4541×10^{-7} m [\[29](#page-8-20)]. Next, to protect the silver layer from oxidation, a thin layer of $Si₃N₄$ of the thickness of 5 nm is grown over the covered region of the Ag layer. Magnetron sputtering technique can be used to deposit $Si₃N₄$ film on the surface of silver layer [\[30](#page-8-21)]. The dielectric constant for this can be computed using following relation [\[31](#page-8-22)] :

$$
\epsilon_{\text{Si3N4}}(\lambda) = \left(1 + \frac{3.0249\lambda^2}{\lambda^2 - 0.1353406^2} + \frac{40314\lambda^2}{\lambda^2 - 1239.842^2}\right) \tag{3}
$$

At the transmitting end of the fber, light is incident and propagates through the fber. The evanescent wave is generated at the metal surface that excites the SPs wave when the light wave is completely refected in the detecting area. Lastly, we chose water as the detecting medium, which has a RI of 1.33 and measured the change in RI from 1.33 to 1.43

which is suitable for most of the biological reaction. We are restricted to this range because the resonance curve does not follow standardization after this range.

3 Mathematical Modeling

When p-polarized light is emitted into the transmitting end, it travels to the receiving end. In this, light propagates through the mechanism of total internal refection (TIR). So the evanescent wave of the propagating ray can be used to excite the SPs [[32](#page-8-23)]. The surface plasmon wave vector (β_{sp}) and incident light wave vector (k_x) should be identical for resonance. In terms of mathematics [[33\]](#page-8-24), the equation is as follows:

$$
\beta_{\rm sp} = k_{\rm x} \tag{4}
$$

$$
\left\{\frac{2\pi}{\lambda}\text{Re}\sqrt{\frac{\varepsilon_{\text{m}}\,\varepsilon_{\text{die}}}{\varepsilon_{\text{m}}+\varepsilon_{\text{die}}}}\right\} = \frac{2\pi}{\lambda}n_{\text{core}}\,\sin\theta\tag{5}
$$

where $\varepsilon_{\rm m}$ and $\varepsilon_{\rm die}$ signify the dielectric constant of metal and sensing medium respectively, n_{core} denotes the RI of the fiber core and λ denotes the incident light wavelength.

For p-polarized wave incident at transmitting end at angle θ, the normalized transmitted power (P_{trans}) at the receiving end of the fber can be computed as follows [[34\]](#page-8-25) :

$$
P_{trans} = \frac{\int_{\theta_{cr}}^{\pi/2} R_p^{N_{ref}(\theta)} \left(n_1^2 \sin \theta \cos \theta / \left(1 - n_1^2 \cos^2 \theta \right)^2 \right) d\theta}{\int_{\theta_{cr}}^{\pi/2} \left(n_1^2 \sin \theta \cos \theta / \left(1 - n_1^2 \cos^2 \theta \right)^2 \right) d\theta}
$$
(6)

where $N_{ref} = L/D$ tan θ denotes the total number of reflections performed by the incident wave in the sensing region, *D* and *L* denote the core diameter and the sensing region length respectively, $\theta_{cr} = \sin^{-1} n_{cl} / n_{core}$ denotes the critical angle at the interface of the core-cladding while n_{cl} and n_{core} denote the RI of the cladding and core of the fiber respectively.

The Fresnel multilayer refection theory is used to compute the reflectance (R_n) of this multilayer structure (core/ metal/Si3N4/sensing medium) and is provided by [[35\]](#page-9-0).

$$
R_p = \mathbf{r_p r_p}^* = \left| \mathbf{r_p}^2 \right| \tag{7}
$$

For p-polarized light, the reflection coefficient (r_p) is as follows:

$$
r_{p} = \frac{q_{1}(M_{11} + M_{12}q_{N}) - (M_{21} + M_{22}q_{N})}{q_{1}(M_{11} + M_{12}q_{N}) + (M_{21} + M_{22}q_{N})}
$$
(8)

here, for the j^{th} layer, $M_j =$ $\int \cos \beta j \frac{-i}{q_j} \sin \beta_j$ −iqj sin *𝛽*^j cos *𝛽*^j] is the characteristic matrix, in which transverse RI $q_j = \sqrt{\frac{1}{6}}$ ϵ _j λ $\cos \theta_j = \sqrt{(\epsilon_j - n_1^2 \sin^2 \theta_1)/\epsilon_j}$ and phase factor $\beta_j = (\frac{2\pi}{\epsilon})$ $n_j \cos \theta_j (z_j - z_{j-1})$; where $(z_j - z_{j-1})$ is the thickness of the *j* th layer.

4 Sensor Performance Parameters

The sensor performance in this study is evaluated for sensitivity, quality factor, and detection accuracy. The sensitivity (S_{λ}) is expressed in terms of resonance wavelength change $(\delta \lambda)$ and RI change (δn) and can be expressed as follows [[36\]](#page-9-1) :

$$
S_{\lambda} = \frac{\delta \lambda}{\delta n} \left(\frac{nm}{RIU} \right) \tag{9}
$$

The quality factor (Q) is determined by the ratio of sensitivity to FWHM and can be written as follows [[37](#page-9-2)] :

$$
Q = S_{\lambda}/FWHM(\text{RIU}^{-1})
$$
\n(10)

The FWHM of an SPR curve is the spectral width that corresponds to the 50% value of transmission spectra. The third important performance parameter is the detection accuracy which can be given by the ratio of $\delta\lambda$ to FWHM, mathematically [\[38](#page-9-3)] :

$$
Detection accuracy = \delta\lambda / FWHM
$$
 (11)

5 Result Analysis and Discussion

The Taguchi technique is a popular tool for increasing efficiency in research and development. It uses a unique design of orthogonal arrays to examine control parameters with only the few trials, greatly reducing the number of tests and increasing efficiency. It aids in determining the impact of a variety of control elements on the device quality characteristics. Furthermore, signal to noise (SNR) ratio in the Taguchi technique aids researchers to quickly identifying the best combinations of the desired design specifcations [[39](#page-9-4)]. In the presented work, Taguchi L9 orthogonal array is used to optimize the diferent control parameters of this structure. The diameter of the fber core, length of the sensing region, and the thickness of the silver layer and the silicon nitride layer are taken as control factors that mainly afect the performance of the designed

Table 1 Studied control factors and level representation

Level 1	Level 2	Level 3	
400	500	600	
10	15	20	
40	50	60	
3	↖		

structure. These control factors are listed in Table [1.](#page-3-0) With these control factors, the appropriate orthogonal array is L9. FWHM and normalized transmitted power for all nine experiments can be calculated from Fig. [2](#page-3-1). With the Taguchi array structure, the number of simulation trials has been cut from 81 (34) to 9 only. This saves cost, time, and the number of attempts while optimizing the SPR sensor's design parameters.

FWHM is the important parameter in designing of sensor that mainly gives the spectral width of the SPR curve. If the FWHM of the SPR curve is large, the quality factor and detection accuracy decrease as expressed in Eqs. [10](#page-2-0) and [11](#page-2-1) respectively. Here, we have optimized the performance for smaller the better SNR. Furthermore, SNR for the FWHM with the Si3N4 layer and without the Si3N4 layer is shown in Tables [2](#page-4-0) and [3](#page-4-1) respectively. It is seen that adding the Si3N4 layer reduces the FWHM which is the primary prerequisite for designing for such an SPR sensor. In Table [2,](#page-4-0) FWHM is calculated from the SPR curve that can plot with the help of Fresnel multilayer refection theory and transfer matrix method. Furthermore, Taguchi L9 orthogonal array is used to calculate SNR for the desired control factors that we can consider smaller the better for FWHM.

Mean and SNR are calculated for FWHM and normalized transmitted power for all nine experiments. In Taguchi design analysis, SNR can be categorized as larger the better, nominal the best, and smaller the best. In designing of fber SPR sensor, small FWHM and large normalized transmitted power are the prerequisites. Normalized transmitted power with SNR (smaller the better) for diferent experiments is shown in Table [4](#page-4-2). Here, SNR is selected for smaller the better for best performance of the proposed sensor that can be calculated by the following equation [[40\]](#page-9-5) :

$$
SNR_{Smaller\ the\ better} = -10\log_{10}(\frac{1}{n}\sum_{i=1}^{n}Y_i^2)
$$
 (12)

here, *n* represents the number of trials and Y_i denotes the response for a specifc factor-level combination.

5.1 Interpretation of Response Table for FWHM

The response table is utilized to determine the appropriate level for each control factor. Response characteristics of diferent control factors with SNR for FWHM are depicted in Table [5.](#page-5-0) In this, the factors with the greatest efect on FWHM are identifed using rank values and delta. The rank

Fig. 2 SPR spectra of normalized transmitted power for different numbers of experiment

Table 3 FWHM with their SNR without the $Si₃N₄$ layer for diferent experiment

no.	Experiment Control factors			FWHM (nm)	SNR
	Core diameter (μm) region (mm)	Length of sensing	Thickness of silver $layer$ (nm)		
1	400	10	40	21.2	-26.5267
$\overline{2}$	400	15	45	27.6	-28.8182
3	400	20	50	28.5	-29.0969
4	500	10	45	16.8	-24.5062
5	500	15	50	11.7	-21.3637
6	500	20	40	33.5	-30.5009
7	600	10	50	12.4	-21.8684
8	600	15	40	21.2	-26.5267
9	600	20	45	27.6	-28.8182

Table 4 Normalized transmitted power with their SNR for diferent experiments

of sensing region length is one while the rank of silver layer thickness, core diameter, and Si3N4 layer is 2, 3, and 4 respectively. This means that the length of the sensing region has the highest contributing efect of smaller SNR for FWHM. The overall mean value of SNR for FWHM from Fig. 3 is obtained at -23.365 .

5.2 Interpretation of Response Table for Normalized Transmitted Power

The response table for diferent control factors for the normalized transmitted power is shown in Table [6.](#page-5-2) In this, the thickness of the Ag layer with a delta value of 19.80 and

Level	Core diameter (μm)	Length of sensing region (mm)	Thickness of silver laver (nm)	Thickness of Si ₃ N ₄ layer (nm)
	-25.41	-20.72	-25.19	-23.79
$\mathcal{D}_{\mathcal{L}}$	-22.35	-22.61	-24.47	-23.75
3	-22.34	-26.76	-20.43	-22.55
Delta	3.06	6.04	4.76	1.23
Rank	3		2	4

Table 5 Response table for SNR for diferent control factors for FWHM; smaller the better

rank 1 has the highest factor in optimizing normalized transmitted power in designing the proposed SPR sensor. Furthermore, the length of the sensing region and thickness of the Si3N4 layer are having ranks 2 and 3 respectively. Here, the diameter of the fber core had the lowest factor with rank 4 in optimizing the normalized transmitted power. The main efect plot of SNR representation for normalized transmitted power with diferent control factors is shown in Fig. [4](#page-6-0). This plot indicates that the thickness of the silver layer has the highest factor effect on SNR for the normalized transmitted power.

5.3 Analysis of Variance (ANOVA) Interpretation

The analysis of variance (ANOVA), a popular statistical approach, is used to see which of the control factors had a signifcant impact on the performance parameters. ANOVA interpretation for FWHM and normalized transmitted power is given in Tables [7](#page-6-1) and [8](#page-6-2) respectively. The contribution of control factor was chosen to indicate the importance of a

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Table 6 Response table for diferent control factors for normalized transmitted power; smaller the better

control factor. The high percentage value of a contribution has the greatest impact on the FWHM and normalized transmitted power. From Table [7](#page-6-1), it is clear that the length of the sensing region has the highest contribution factor efect of 53.27% on FWHM followed by thickness of the silver layer and core diameter with 29.83% and 10% respectively while the thickness of the Si3N4 layer has least contribution efect of 6.90% on optimization of the FWHM. ANOVA analysis for normalized transmitted power depicted in Table [8](#page-6-2) shows that the thickness of the silver layer has the highest contribution factor efect of 47.36% on optimization of the normalized transmitted power followed by the length of sensing region and the core diameter with 31.58% and 21% respectively while the thickness of Si3N4 layer has the least contribution factor efect of 0.06% on optimization of the normalized transmitted power.

In conclusion, the best selection of control parameters with the Taguchi optimization method for designing the proposed SPR sensor is given in Table [9.](#page-6-3) Based on these

Table 7 Analysis of variance (ANOVA) for FWHM with diferent control factors

Table 8 Analysis of variance (ANOVA) for normalized transmitted power with diferent control factors

parameters, we have a designed a fber SPR sensor for the RI ranging from 1.33 to 1.43. The plot for normalized transmitted power with RI of sensing medium is shown in Fig. [5a](#page-7-0). In

Table 9 Best selection of control parameter with Taguchi method

this, when we are increasing the RI of the sensing medium, the resonance wavelength shifts to a higher value. The value of resonance wavelength for respective RI of sensing medium is plotted in Fig. [5b](#page-7-0) and also depicted in Table [10.](#page-7-1) The values of sensitivity, quality factor, and detection accuracy which are given in Table [10](#page-7-1) can be calculated by using Eqs. [9,](#page-2-2) [10](#page-2-0), and [11](#page-2-1) respectively. Here, the maximum sensitivity of 6287 nm/RIU is achieved for the varying RI from 1.33 to 1.43 while the maximum quality factor and detection accuracy are 873.19 RIU−1 and 87.31 respectively. As a result, the Taguchi approach can be utilized to optimize the designing parameters and can assist in designing the fber SPR sensor.

Fig. 5 (a) Plot of the SPR spectra and (b) the shift of resonance wavelength for the core-Ag-Si₃N₄ configuration with different RI of the sensing medium

Table 10 Performance characteristics of proposed structure for diferent RI of sensing medium

6 Conclusion

In a nutshell, this study focused on the use of numerical analysis, specifcally transfer matrix method (TMM) and Taguchi's method, as an appropriate and reliable approach for improving the control parameters of a $Si₃N₄$ -based fiber plasmonic sensor. Signal to noise ratio is kept smaller the better (STB) for both the FWHM and the normalized transmitted power. Using ANOVA analysis, frstly the thickness of the silver layer has the highest contribution of 47.36% while the thickness of $Si₃N₄$ has the least contribution of 0.06% for the normalized transmitted power. Secondly, on the FWHM, the length of the sensing region has the largest dominant factor effect of 53.26%, while the thickness of the $Si₃N₄$ layer has the least dominating factor effect of 6.90%. With Taguchi optimization, the best control

parameters which contribute maximum normalized transmitted power and minimum FWHM are 600 µm of core diameter, 10 mm of the length of sensing region, 50 nm thickness of the silver layer, and 5 nm thickness of $Si₃N₄$ layer. Considering all these optimized parameters, the maximum sensitivity of 6287 nm/RIU is obtained while the quality factor and detection accuracy are 873.19 RIU−1 and 87.31 respectively. Hence, the Taguchi optimization method is strongly suggested in nanotechnology due to its ability to optimize control factors in the endeavor to design efective fber SPR sensors.

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Declarations

Conflict of Interest The authors declare competing interests.

References

- 1. K.N. Shushama, M.M. Rana, R. Inum, M.B. Hossain, Graphene coated fber optic surface plasmon resonance biosensor for the DNA hybridization detection: simulation analysis. Opt. Commun. **383**, 186–190 (2017)
- 2. M.S. Rahman, M.R. Hasan, K.A. Rikta, M.S. Anower, A novel graphene coated surface plasmon resonance biosensor with tungsten disulfde (WS2) for sensing DNA hybridization. Opt. Mater. **75**, 567–573 (2018)
- 3. R. Zafar, S. Nawaz, G. Singh, A. d'Alessandro, M. Salim, Plasmonics based refractive index sensor for detection of hemoglobin concentration. IEEE Sens. J. **18**(11), 4372–4377 (2018)
- 4. Y. Saylan, S. Akgönüllü, D. Çimen, A. Derazshamshir, N. Bereli, F. Yılmaz, A. Denizli, Development of surface plasmon resonance sensors based on molecularly imprinted nanoflms for sensitive and selective detection of pesticides. Sens. Actuators B Chem. **24**, 446–454 (2017)
- 5. E. Kretschmann, H. Raether, Radiative decay of non-radiative surface plasmons excited by light. ZeitschriftfürNaturforschung A **23**(12), 2135–2136 (1968)
- 6. N. Mudgal, P. Yupapin, J. Ali, G. Singh, BaTiO3-graphene-afnity layer–based surface plasmon resonance (SPR) biosensor for pseudomonas bacterial detection. Plasmonics (2020)
- 7. A.A. Kolomenskii, P.D. Gerson, H.A. Schuessler, Sensitivity and detection limit of concentration and adsorption measurements by laser-induced surface plasmon resonance. Appl. Opt. **36**, 6539– 6547 (1997)
- 8. L. Liu, M. Wang, L. Jiao, T. Wu, F. Xia, M. Liu, W. Kong, L. Dong, M. Yun, Sensitivity enhancement of a graphene–barium titanate-based surface plasmon resonance biosensor with an Ag– Au bimetallic structure in the visible region. J. Opt. Soc. Am. B **36**(4), 1108–1116 (2019)
- 9. N. Mudgal, M. K. Falaswal, T. Ismail, I. S. Fahim, M. Tiwari, G. Singh, *Study of approaches to implement the prism-based surface plasmon resonance sensors* ed. by. V. Janyani, G. Singh, M. Tiwari, T. Ismail. Optical and Wireless Technologies (Lecture Notes in Electrical Engineering, 2020) p. 648
- 10. A.S. Kushwaha, A. Kumar, R. Kumar, M. Srivastava, S.K. Srivastava, Zinc oxide, gold and graphene-based surface plasmon resonance (SPR) biosensor for detection of pseudomonas like bacteria: A comparative study. Optik **172**, 697–707 (2018)
- 11. A. Sharma, R. Jha, B.D. Gupta, Fiber-optic sensors based on surface plasmon resonance: a comprehensive review. Sens. J. IEEE **7**(8), 1118–1129 (2007)
- 12. Y. Zhao, R.J. Tong, X. Feng, P. Yun, Current status of optical fber biosensor based on surface plasmon resonance. Biosens. Bioelectron. **142**, 111505 (2019)
- 13. S. Franzen, Surface plasmon polaritons and screened plasma absorption in indium tin oxide compared to silver and Gold. J. Phys. Chem. **112**(15), 6027–6032 (2008)
- 14. B. Liedberg, C. Nylander, M.I. Lunstro, Surface plasmon resonance for gas detection and biosensing. Sens Actuators **4**, 299–304 (1993)
- 15. L. Xia, S. Yin, H. Gao, Q. Deng, C. Du, Sensitivity enhancement for surface plasmon resonance imaging biosensor by utilizing gold-silver bimetallic flm confguration. Plasmonics **6**(2), 245–250 (2011)
- 16. S. Zeng, D. Baillargeat, H.P. Ho, K.T. Yong, Nanomaterials enhanced surface plasmon resonance for biological and chemical sensing applications. Chem. Soc. Rev. **43**, 3426–3452 (2014)
- 17. A.K. Mishra, S.K. Mishra, R.K. Verma, Graphene and beyond graphene MoS2: a new window in surface-plasmon-resonancebased fber optic sensing. J. Phys. Chem. C **120**(5), 2893–2900 (2016)
- 18. J.B. Maurya, Y.K. Prajapati, V. Singh, J.P. Saini, R. Tripathi, Performance of graphene MoS2 based surface plasmon resonance sensor using silicon layer. Opt. Quant. Electron **47**, 3599–3611 (2015)
- 19. Y. Luo, C. Chen, K. Xia, S. Peng, H. Guan, J. Tang, H. Lu, J. Yu, J. Zhang, Y. Xiao, Z. Chen, Tungsten disulfde (WS2) based all-fber-optic humidity sensor. Opt. Express **24**(8), 8956 (2016)
- 20. H. Shi, H. Pan, Y. W. Zhang, B.I. Yakobson, Quasiparticle band structures and optical properties of strained monolayer MoS2 and WS2. Phys. Rev. B **87**, 155304 (2013)
- 21. S. Kaushik, U.K. Tiwari, S.S. Pal, R.K. Sinha, Rapid detection of Escherichia coli using fber optic surface plasmon resonance immunosensor based on biofunctionalized molybdenum disulfde (MoS2) nanosheets. BiosensBioelectron **126**, 501–509 (2019)
- 22. S.-L. Ku, C.-C. Lee, Optical and structural properties of silicon nitride thin flms prepared by ion-assisted deposition. Opt. Mater. **32**, 956–960 (2010)
- 23. N. Mudgal, A. Saharia, K.K. Choure, A. Agarwal, G. Singh, Sensitivity enhancement with anti-refection coating of silicon nitride (Si3N4) layer in silver-based surface plasmon resonance (SPR) sensor for sensing of DNA hybridization. Appl. Phys. A **126**(946), (2020)
- 24. V. Kapoor, N.K. Sharma, V. Sajal, Efect of zinc oxide overlayer on the sensitivity of fber optic SPR sensor with indium tin oxide layer. Optik **185**, 464–468 (2019)
- 25. R.K. Verma, B.D. Gupta, Surface plasmon resonance based fber optic sensor for the IR region using a conducting metal oxide flm. J. Opt. Soc. Am. A **27**(4), 846–851 (2010)
- 26. C.Z. Tan, Determination of refractive index of silica glass for infrared wavelengths by IR spectroscopy. J. Non-Cryst. Solids **223**(1–2), 158–163 (1998)
- 27. X. Zhang, X. Zhu, Y. Shi, Fiber optic surface plasmon resonance sensor based on a silver-coated large-core suspended-core fber. Opt. Lett. **44**, 4550–4553 (2019)
- 28. M.A. Ordal, L.L. Long, R.J. Bell, S.E. Bell, R.R. Bell, R.W. Alexander, C.A. Ward, "Optical properties of metals Al Co, Cu, Au, Fe, Pb, ni, Pd, pt, Ag, Ti, and w", Pure Appl. Opt. J. Eur. Opt. Soc. A **11**, 1099–1119 (1983)
- 29. A.K. Sharma, G.J. Mohr, Theoretical understanding of an alternating dielectric multilayer-based fber optic SPR sensor and its application to gas sensing. New J. Phys. **10**, 023039 (2008)
- 30. J. Kulczyk-Malecka, P.J. Kelly, G. West, G.C.B. Clarke, J.A. Ridealgh, Difusion studies in magnetron sputter deposited silicon nitride flms. Surf. Coat. Technol. **255**, 37–42 (2014)
- 31. K. Luke, Y. Okawachi, M.R.E. Lamont, A.L. Gaeta, M. Lipson, Broadband mid-infrared frequency comb generation in a Si3N4 microresonator. Opt. Lett. **40**, 4823–4326 (2015)
- 32. B.D. Gupta, S.K. Srivastava, R. Verma, Fiber optic sensors based on plasmonics, World Scientifc Publishing. Chapter 4, 93–95 (2015)
- 33. N. Mudgal, A. Saharia, A. Agarwal, G. Singh, ZnO and Bimetallic (Ag–Au) layers based surface plasmon resonance (SPR) biosensor with BaTiO3 and graphene for biosensing applications. IETE J. Res. (2020). [https://doi.org/10.1080/03772063.2020.](https://doi.org/10.1080/03772063.2020.1844074) [1844074](https://doi.org/10.1080/03772063.2020.1844074)
- 34. X. Zhou, X. Li, T.L. Cheng, S. Li, G. An, Graphene enhanced optical fber SPR sensor for liquid concentration measurement. Opt. Fiber Technol. **43**, 62–66 (2018)
- 35. N. Mudgal, A. Saharia, A. Agarwal, J. Ali, P. Yupapin, G. Singh, Modeling of highly sensitive surface plasmon resonance (SPR) sensor for urine glucose detection. Opt. Quant. Electron. **52**, 307 (2020)
- 36. L. Wu, J. Guo, Q. Wang, S. Lu, X. Dai, Y. Xiang, D. Fan, Sensitivity enhancement by using few-layer black phosphorus-graphene/ TMDCs heterostructure in surface plasmon resonance biochemical sensor. Sens. Actuat. B Chem. **249**, 542–548 (2017)
- 37. Y. Saad, M. Selmi, M.H. Gazzah, A. Bajahzar, H. Belmabrouk, Performance enhancement of a copper-based optical fber SPR sensor by the addition of an oxide layer. Optik **190**, 1–9 (2019)
- 38. A. Sharma, B.D. Gupta, Fiber optic sensor based on surface plasmon resonance with Ag–Au alloy nanoparticule flms. Photon. Nanostruct.-Fundam. Appl. **3**, 30–37 (2005)
- 39. N.R. Mohamad, M.F.M.R. Wee, M.A. Mohamed, A.A. Hamzah, P.S. Menon, Multi-response optimization of chromium/goldbased nanoflm Kretschmann-based surface plasmon resonance glucose sensor using fnite-diference time-domain and Taguchi method. Nanomater. Nanotechnol. (2020). [https://doi.org/10.1177/](https://doi.org/10.1177/1847980420982119) [1847980420982119](https://doi.org/10.1177/1847980420982119)
- 40. S. Sahu, J. Ali, P. Yupapin, G. Singh, Efectiveness of Taguchi method for the optimization of narrowband optical flters based on grating waveguides. MicrosystTechnol **25**, 789–795 (2019)

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