



Recent Advances and Prospects in Silicon Nanowire Sensors: A Critical Review

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Abstract

Due to the distinctive optical, mechanical and electrical characteristics, silicon nanowire (SiNW), one of the one dimensional nanostructures, has become a potential sensing nanomaterial. SiNWs have drawn interest in high-sensitive sensor fabrication, primarily because of their large surface-volume ratios, which significantly enhanced the detection limit to femtomolar concentrations and also provided high sensitivity. Due to its high charge sensitivity, SiNW FET-based sensors had been employed extensively for sensing various chemical as well as biological species. In this work, the sensing performance and applications of different SiNW biosensors, gas sensors, chemical and metal ion sensors were studied. In this study, we have also elaborated the most current developments as well as the sensing performance of various SiNW-based Covid-19 sensors.

Keywords Silicon nanowire sensors · Silicon nanowire bio-sensors · Gas sensors · Chemical sensors · pH sensors · Silicon nanowire humidity sensors · Metal-ion sensors · Covid-19 sensors

1 Introduction

Nanowires are structures which facilitate both flexibility as well as miniaturization, have exhibited substantial potential as sensor component in various electronic sensing devices. SiNW being key nanostructure has been a subject of research since 1950s, have emerged as an ideal candidate to be used as sensing element due to its 1-dimensional quasi electronic structure and their large surface-volume ratio. SiNWs also find application in photovoltaics, lithium-ion battery anodes, field-effect transistors, thermoelectrics etc. [1–5]. By varying the doping process condition, the conductance of SiNW can be adjusted so as to enhance its sensitivity. As a way to enhance surface area which is exposed to target molecules, SiNW can be made suspended, which

will further improve its sensitivity. Another advantage of using SiNW is its compatibility with classical Sil technology as easy integration of peripheral circuitry on the same chip can be achieved [6–15]. SiNWs are usually fabricated using two approaches namely bottom up and top down. In top down fabrication approach SiNW is fabricated using lithographic process by scaling down bulk Sil wafer to the desired size and shape. Fig. 1 represents the schematic of a top-down SiNW device fabrication process. The fabrication of SiNW devices is carried out on the SOI (Sil on insulator) platform having oxide buried layer. In order to pattern the nanowire structure on the silicon-on-insulator layer, electron beam lithography was used. By applying anisotropic and isotropic etching, SiNWs can be made suspended. Bottom up method (metal assisted chemical etching, oxide assisted growth, vapour liquid solid) is a SiNW synthesize or growth technique from bulk Sil wafer via catalyzed metal-free or catalyzed metal -assisted process. Metal assisted chemical etching has been reported as an easy and low-cost process for SiNWs array manufacturing. This process consists of two major steps namely deposition of electroless metal on Sil wafer as well as chemical etching using solution based on fluoride-ion. In oxide assisted SiNW growth, SiO was used as a starting material to enhance the growth and nucleation of SiNWs without catalyzed metal assistance and resulted in high purity SiNWs devoid of metal contamination.

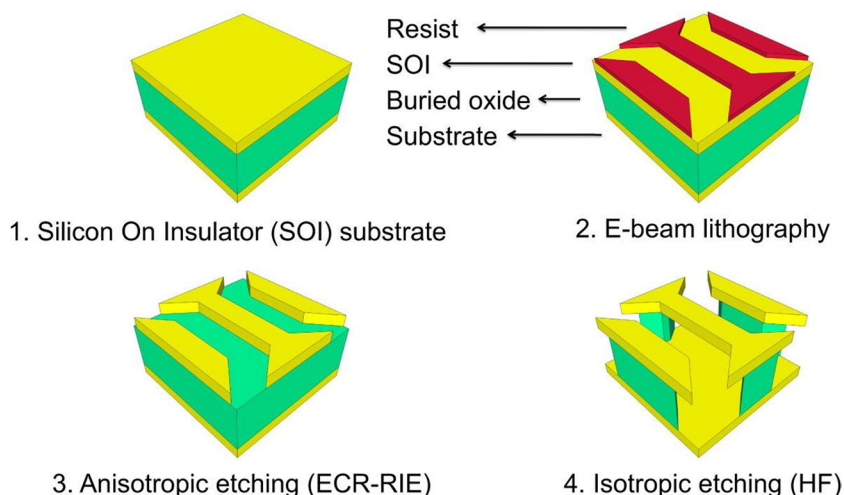
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Fig. 1 Top-Down SiLNW device fabrication process [25] (Copyright @ Elsevier)



Metal-catalyzed (Al, Fe, Pt, Au etc.) would be placed on the SiLNW wafer first in vapour liquid solid method and laser ablation or chemical vapour deposition procedures are used to accelerate SiLNW development. [16–25].

In this article, we had elaborated briefly the sensing performance of various SiLNW based biosensors, gas sensors, chemical and metal ion sensors, pH sensors, humidity sensors, strain and pressure sensors and photonic sensors. The emerging application of SiLNW sensors in rapid Covid-19 virus detection was also reviewed critically.

2 Silicon Nanowire Based Bio-Sensors

SiLNW sensors are generally FET based sensors having gate, drain and source electrodes (Fig. 2). SiLNW biosensor works by varying the current that flows through the SiLNW channel, influenced by the variation in surface charges due to binding reaction of biomolecule. Due to its benefits like capability to

integrate with complementary metal-oxide semiconductors, direct electrical readouts and good sensitivity, FET based SiLNW sensors have exhibited a lot of potential in bio-sensing applications. [28–30].

In the year 2008, A.Cattani-Scholz et al. [31] investigated PNA functionalized organophosphonate-based SiLNW sensor with self-assembled hydroxyalkylphosphonate monolayer interface system for label-free DNA sensing. Upon electrolyte 1µM DNA buffer solution injection, a decline in wire resistance value corresponding to variation in surface potential of approximately 1.5 mV was reported. In the year 2010, Guo-Jun Zhang et al. [32] reported SiLNW sensor functionalized with reverse-transcription-polymerase chain reaction technique for label free, quick and high sensitive identification of dengue virus using electrical detection and nucleic acid hybridization (Fig. 3).

By computing the change of resistance in SiLNW after and before the binding of the DEN-2 reverse-transcription-polymerase chain reaction product to the PNA sequence,

Fig. 2 Schematic representation of SiLNW FET based biosensor [26, 27]

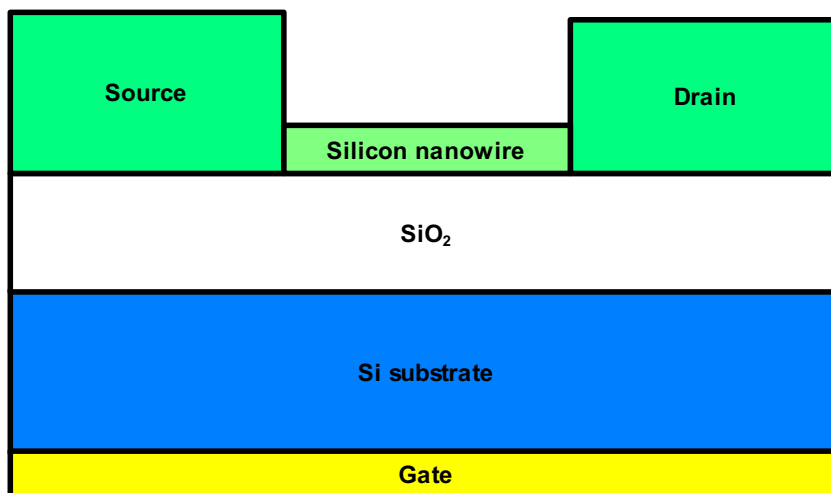
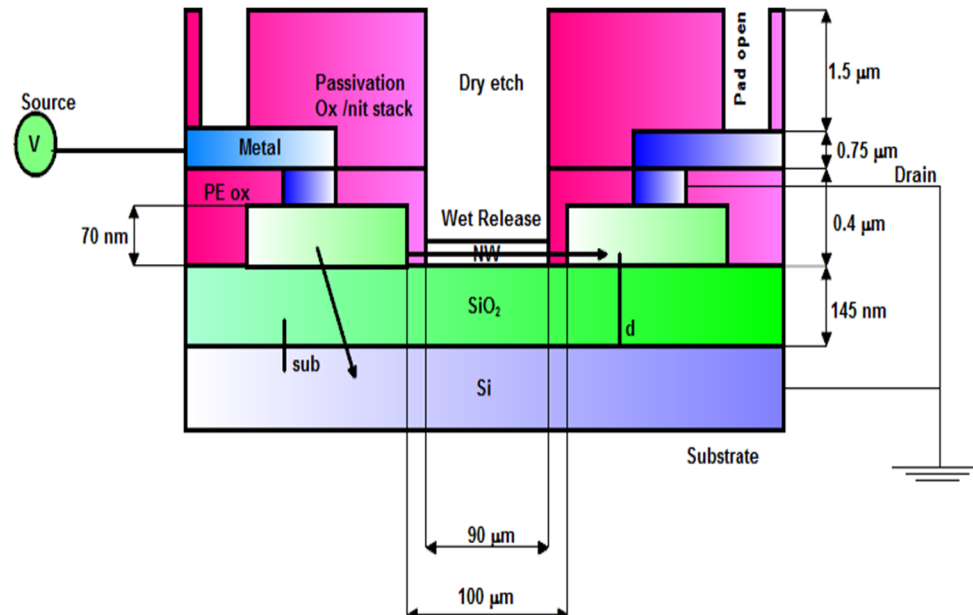


Fig. 3 Schematic illustration of Si/nW FET based dengue virus detection biosensor [32]



detection limit below 10 fM for amplicons concentration in thirty minutes was reported. In the year 2010, Seong-Wan Ryu et al. [33] reported Si/nW biosensor embedded with gold nanoparticle for high sensitive DNA label free sensing. In order to measure the probe oligonucleotides immobilization as well as its oligonucleotides target hybridization, the flow of electric current in between drain and source electrodes were measured. At a concentration of 1 pM, 23-mer oligonucleotide complementary target analogous to the DNA of breast cancer was reported in Si/nW gold nanoparticle embedded biosensor. In the same year, Guo-Jun Zhang et al. [34] reported Si/nW biosensor functionalized with Morpholino for label free and sequence specific DNA detection. Fluorescence microscopy and photoelectron X-ray spectroscopy were used for DNA-Morpholino hybridization and Morpholino attachment on to the surface of Si/nW. High specificity for DNA recognition was reported in Morpholino-modified surface and the Si/nW sensor reported DNA detection in hundreds of femtomolar range. In 2011, D.H.Kwon et al. [35] reported Si/nW modified by gold NPs using aminopropyltriethoxysilane self-assembled monolayer for sensing albumin. It was reported that the reliability of sensor got increased by repeated thermal treatment in vacuum, as it improves the conductivity from aminopropyltriethoxysilane molecule carbonization and also by making gold NPs in close contact to Si/nW surface. Si/nW modified with gold NPs array sensor reported range of detection of 1-7 μ M for bovine serum albumin. In the same year, Guo-Jun Zhang et al. [36] reported monolayer-assisted self-assembled Si/nW biosensor for DNA-protein interaction detection in breast cancer cells nuclear extracts. A self-assembled vinyl-terminated monolayer was applied to the Si/nW surface, and oxidation transformed

the surfaces termination into carboxylic acid. Atomic force microscopy and photoelectron X-ray spectroscopy were used to observe protein-DNA interaction on the Si/nW surface and to characterize the step-by-step functionalization of the self-assembled monolayer and DNA on bare Si/nW surface. (ERE, dsDNA) estrogen receptor element and (ER α , protein) estrogen receptor alpha binding were used in the research. The sensor reported limit of detection as low as 10fM for detecting ER α . In the year 2012, A. Kulkarni et al. [37] reported Si/nW array based sensor for selective and sensitive detection of as synthesized two dimensional DNA lattices with biotins. Top down approach was used to fabricate Si/nW array which contains two fifty nanowires of twenty μ m length spaced equally with an interval of 3.2 μ m (Fig. 4).

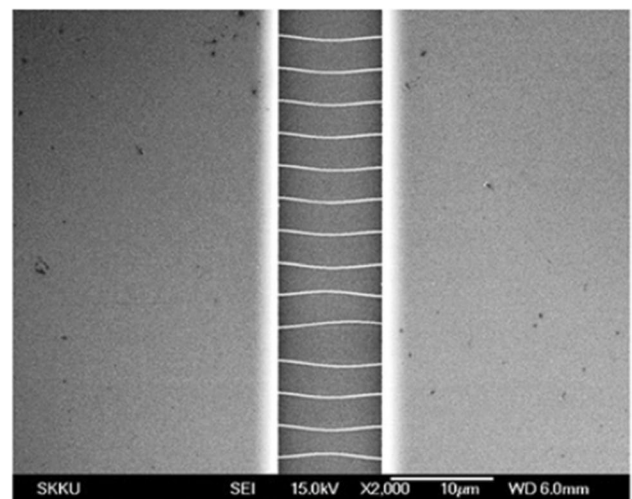


Fig. 4 Fabrication result of Si/nW array [37] (Copyright @Elsevier)

It was reported that the SiNW responsivity peak, caused by optical local field enhancement linked to the dielectric periodic structure of the NWs exist at 480 nm in the photocurrent spectrum (Fig. 5). Further the photo-resistivity of the SiNW array device reported significant changes as a result of conductivity in DNA lattices with protein streptavidin, making it an ideal device for DNA detection and applications like toxic detection, DNA forensics and in immunological assays

In the year 2012, X. Duan et al. [38] investigated use of SiNW biosensors to study the ligand-protein binding affinities as well as kinetics and reported sensitivity down to fM concentrations. An analytical model was formed by combining device solution trans-conductance that can normalize the sensor response with Langmuir isotherms which can be used to measure binding-affinities of molecules (Eq. 1) [38].

$$\frac{\Delta I_{ds}}{g_m} = \Delta V_T = \frac{q_A}{C_0} [B]_{max} \times \frac{[A]}{[A] + K_D} \quad (1)$$

where g_m represents trans-conductance, ΔV_T represents threshold voltage shift, q_A represents electric charge that is contributed by adsorbed analytes, K_D represents equilibrium constant, C_0 represents channel/analyte capacitive coupling, $[A]$ represents bulk solution analyte concentration and $[B]_{max}$ represent the maximum functional binding sites surface density on the SiNW. In the year 2013, P. Serre et al. [39] reported DNA sensor in which random network based on SiNW was fabricated through low cost, versatile and simple vacuum filtration technique. The fabricated nanowire density can be monitored easily and also were homogeneous and reproducible. At room temperature these networks can be deposited on to various types of substrates. Through fluorescence it was demonstrated

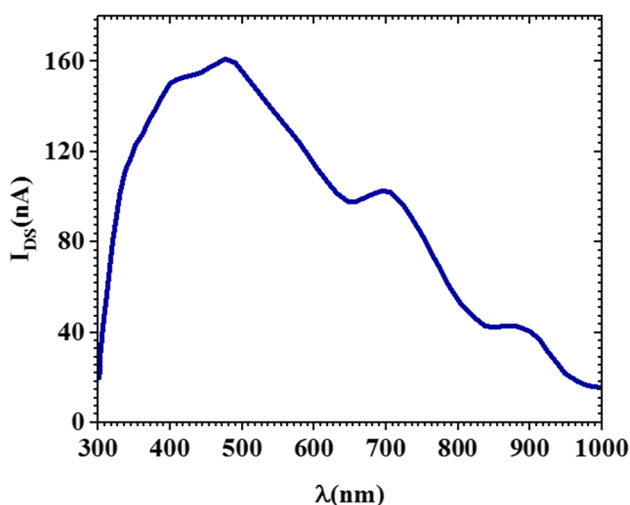


Fig. 5 Photocurrent spectral response of SiNW array chip [37]

that due to the nano-wire geometry, SiNW networks when compared to Si_3N_4 surface are extremely selective to DNA hybridization with an improved sensitivity and selectivity. In the same year Jia-Yo Wu et al. [40] reported SiNW back-gated FET based sensor for detecting a fragment of cancer-related (IL-1 β) interleukin-1 β gene. Plasma modification treatment was employed on device surface with various parameters to increase SiNW sensor sensitivity and it was reported that after one minute of N_2O plasma treatment, the sensitivity of SiNW FET sensor can be enhanced because after N_2O plasma treatment the detection region morphology was rougher. From the normalized current shift value, N_2O plasma-treated SiNW FET sensor reported sensitivity of 0.12/decade in sensing IL-1 β 20-mer target DNA with 2.5 fM limit of detection. The normalized current shift was computed as [40]

$$I_{d,normalized\ current\ shift} = (I_{d,after} - I_{d,before})/I_{d,before} \quad (2)$$

where $I_{d,after}$ represents drain current after injecting target DNA and $I_{d,before}$ represents drain current before injecting target DNA.

In the year 2014, H. Wang et al. [41] reported SiNW based fluorescent sensor for alkaline phosphatase detection. A number of phosphate compounds are hydrolyzed and transphosphorylated by alkaline phosphatase, which is a hydrolase phosphomonoester enzyme, to produce the appropriate alcohols and phosphate ions. Several diseases like prostatic and breast cancer, diabetes, liver dysfunction, bone disease etc. can be caused due to abnormal level of serum alkaline phosphatase. SiNW sensor was fabricated by immobilizing fluorescein molecules covalently on the surface of SiNWs along with phosphorylation of the fluorescein immobilized group. The SiNW fluorescent biosensor demonstrated a linear range of detection of 0.0175 U/mL–0.3U/mL with 0.0175 U/mL detection limit. The sensor also reported a response time of 20 minutes. The potential of SiNW fluorescent biosensor in measuring alkaline phosphatase was evident from the relative fluorescence intensity time curves (Fig. 6) in which by increasing the concentration of alkaline phosphatase, SiNW fluorescent biosensor exhibited higher level of fluorescence enhancement and faster enzymatic reaction rate. In the year 2014, G. Jayakumar et al. [42] reported pixel based fully electronic SiNW based biosensor with back gate and fluid gate on chip integrated with CMOS circuits. The side wall transfer lithography process were used to fabricate nanowires as it was time and cost efficient. The sensor consists of eight output-input pins and N by N pixel matrix. Single crystalline SiNW with cross-section area 75 by 20 nm was defined in each pixel. This design facilitates sequential readout of individual SiNWs and can be utilized for charge based instantaneous detection of molecules in gases or liquids. In the year 2015,

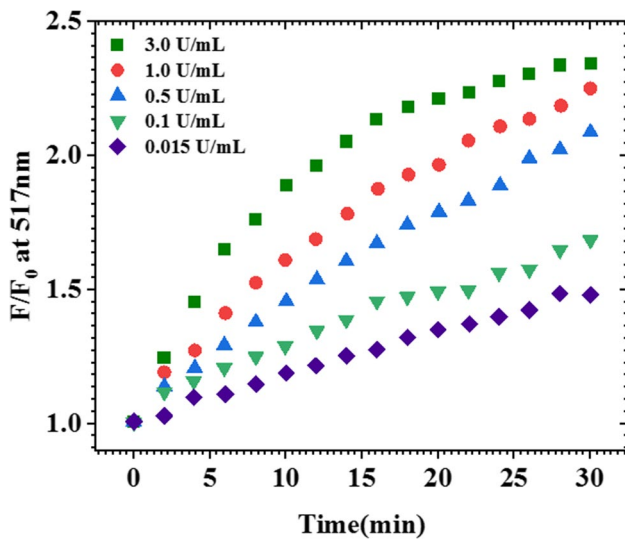
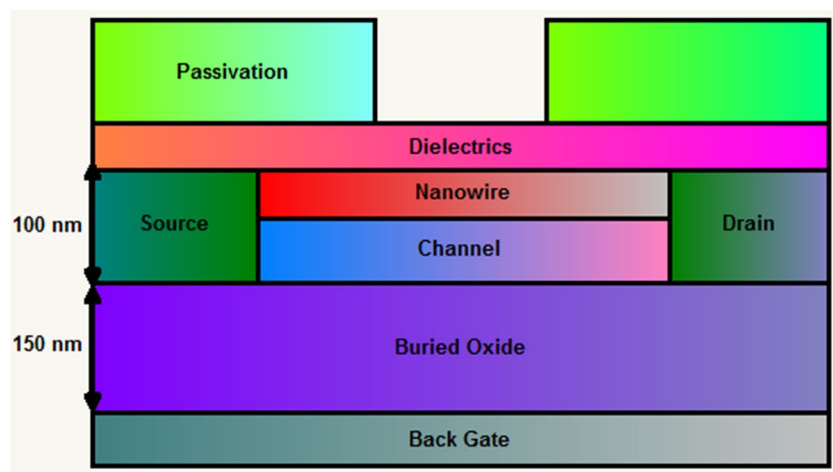


Fig. 6 Fluorescence-intensity time plot at 517 nm with different alkaline phosphatase concentrations [41]

Shih-Hsiang Shen et al. [43] reported multi-channel SiNW cardiac troponin I biosensor with stacked dielectric structure (Fig. 7) coated with high-k dielectric materials namely HfO_2 and Al_2O_3 for enhancing the sensing property. When compared to the performance of sensor with only high-k dielectric devices, SiO_2 ultrathin sensing membrane structure stacked with 10 nm HfO_2 and 14 nm Al_2O_3 reported enhanced sensing property of 1.4 and 3.8 times. The sensor reported 320 fM limit of detection along with 20% signal enhancement.

In the year 2015, T. Adam et al. [44] reported liquid gate control SiNW sensor for specific single-stranded DNA molecule detection which can be used in liquid environment. Conventional photolithography was used to fabricate the sensor and was coupled inductively with plasma dry etching process. In order to create a molecular binding chemistry,

Fig. 7 Schematic illustration of SiNW cardiac troponin I biosensor [43]



the sensor surface was salinized and subjected to (3-aminopropyl) triethoxysilane amination. The sensor reported high reusability and 0.1 nM limit of detection with a detection range of 100 pM to 25 nM. However it was observed that surface composition and nanowire size can limit the sensor response. The sensor response was computed as [44]

$$\text{Device response} = \frac{G_{25} - G_{0.1}}{G_{25}} \times 100 \tag{3}$$

where G_{25} represents current response at 25 nM and $G_{0.1}$ represents current response at 0.1 nM. In the same year J. Lee et al. [45] reported SiNW based hybrid biosensor integrated with amplifier MOSFET fabricated via classical CMOS technology. It was observed that amplifier MOSFET integration will enhance FET based biosensors current response. The hybrid SiNW sensor for pH detection reported 5.74 decades per pH current response which when compared to single SiNW biosensor is 2.5×10^5 times larger. The sensor also exhibited 4.5×10^5 high current change for 500 nM concentration of poly(allylamine hydrochloride) charged polymer detection.

In the year 2016, Li-Chen Yen et al. [46] reported horn-like polycrystalline-SiNW FET biosensor for label free and real time sensing of ferritin protein. Spacer wire method was used to create a dummy gate trapezoidal-shaped structure that is used to fabricate nanowires which resemble horns. It was reported that horn-like poly-SiNW FET having 2 μm channel length exhibited good electrical characteristics (Fig. 8), increased $I_{\text{on}}/I_{\text{off}}$ value of 3.47×10^5 and lesser threshold voltage value of 1.1 V in comparison with other channel lengths. Additionally, the sensor also exhibited 133.47 mV/pH high sensitivity value due to the large capacitive coupling ratio, exceeding Nernst limit. In the year 2016, S.F.A.Rahman et al. [47] reported oxygen plasma treated SiNW biosensor functionalized with standard complementary metal oxide- semiconductor process for detecting

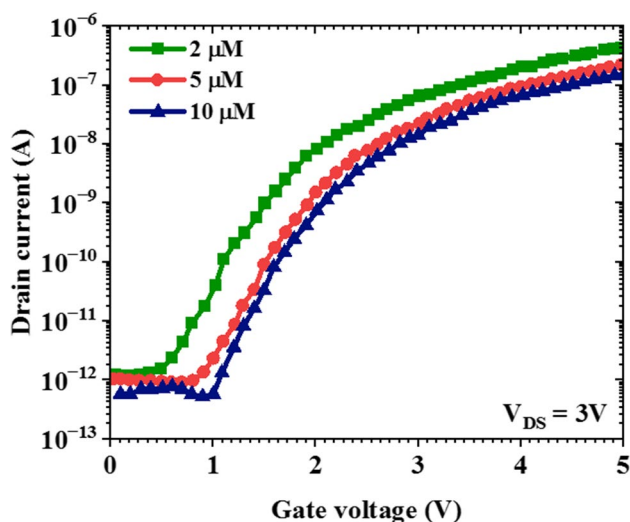


Fig. 8 Transfer characteristics plot of horn-like polycrystalline-SiNW FET biosensor for different channel length [46]

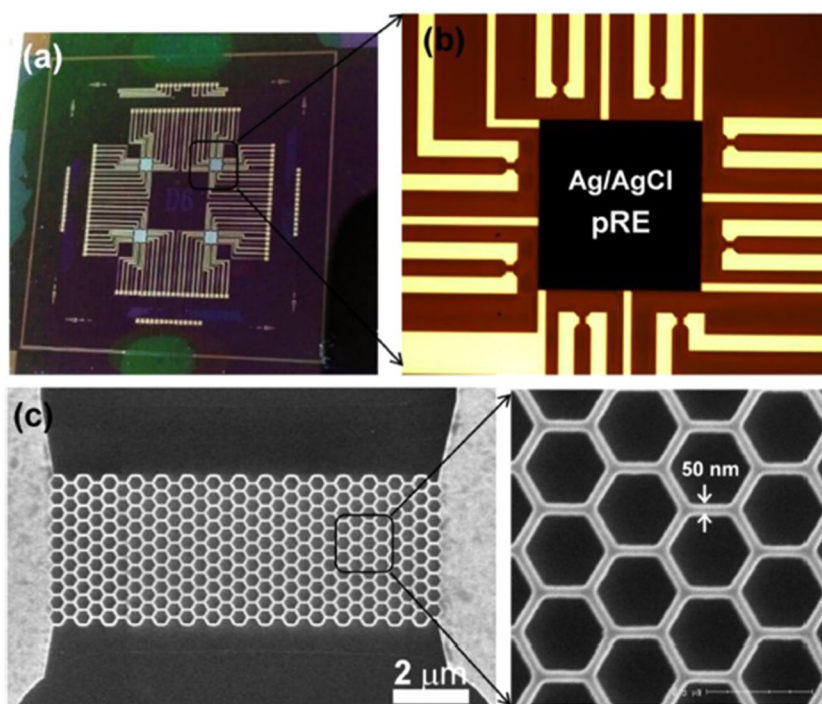
dengue virus DNA with enhanced sensitivity. Three step process namely surface modification of SiNW, immobilization of DNA and DNA hybridization was employed to make the device as a functional sensing element. It was suggested that altering the SiNW surface with oxygen plasma treatment would be an efficient way to increase the amount of target DNA binding. When compared to untreated SiNW device, oxygen plasma treated-SiNW device reported enhancement in current measurement. From the IV characteristics, improved efficiency was evident in SiNW device with 60

second of oxygen plasma treatment which will degrade after 90 second of treatment. 1.985×10^{-14} M detection limit was reported in plasma oxygen treated SiNW sensor with a linear range of detection 1.0×10^{-9} M to 1.0×10^{-13} M.

In 2016 K. Kim et al. [48] reported SiNW biosensor for label free recognition of biomarker cTnI-cardiac troponin-I. The nanowire configuration of the fabricated SiNW cardiac troponin biosensor utilized a honeycomb structure embedded with Ag/AgCl/pRE (Fig. 9) and exhibited enhanced electrical performance for various cardiac troponin-I concentration (Fig. 10) along with improved sensing area. The sensor reported n-type behaviour with less sub threshold swing, small leakage current at gate and high OFF-ON current ratio. The detection limit as low as 5 pg/mL, high sensitivity with low ion concentrations under buffer solutions along with excellent specificity for sensing cardiac troponin-I biomarker were also reported in the fabricated honeycomb SiNW biosensor. In the same year, M.Nuzaihan.M.N et al. [49] reported p-type molecular gate control based SiNW biosensor (Fig. 11) for sensing dengue virus related DNA. A three-step process that involved DNA immobilization, surface modification and hybridization were used to functionalize the surface of the fabricated SiNW. $45.0 \mu\text{AM}^{-1}$ sensitivity and 2.0 fM detection limit were reported in the fabricated p-type dengue virus SiNW biosensor.

In the year 2017, G. Presnova et al. [50] reported gold nanoparticles functionalized SiNW FET biosensor for label free and instantaneous detection of prostate specific antigen in human serum. The SiNW FET exhibited enhanced electrical performance and improved sensitivity to pH when

Fig. 9 (a) and (b) Optical images of SiNW honeycomb FET (c). Scanning electron microscopy image of SiNW honeycomb FET [48] (Copyright @ Elsevier)



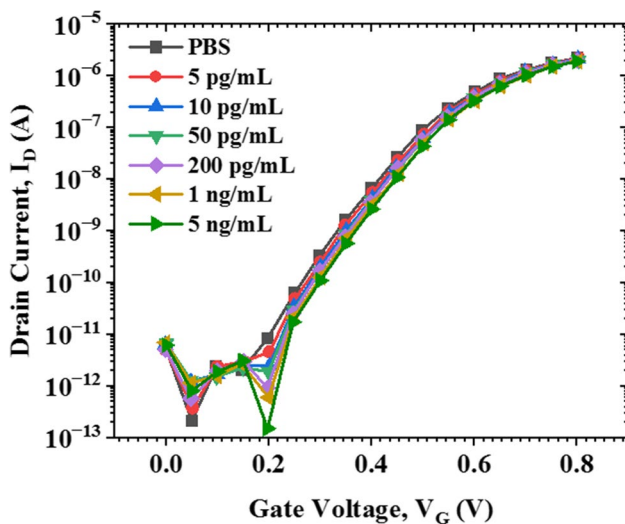


Fig. 10 V-I characteristics of honeycomb SiNW cardiac troponin-I biosensor [48]

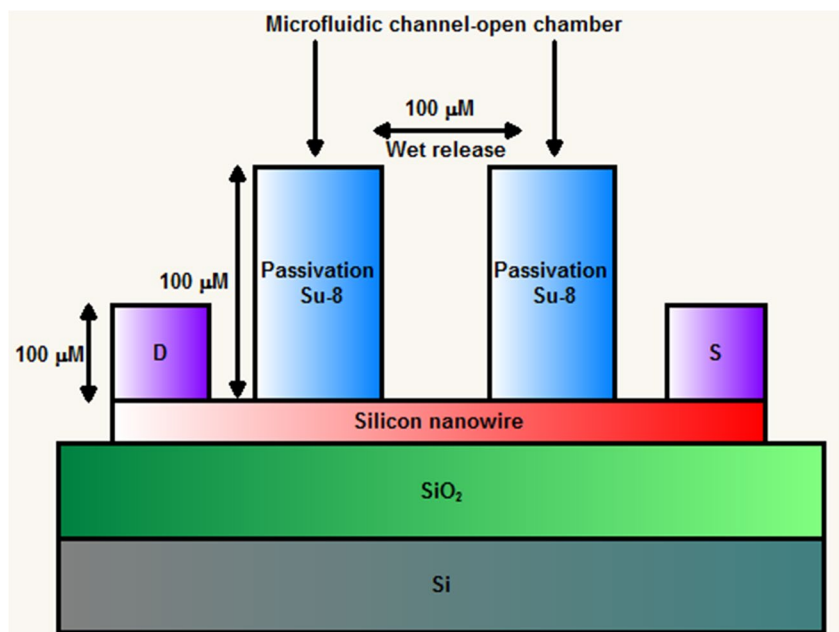
the gold nanoparticles were used. The SiNW FET biosensor reported a response time of 5s to 10s and one minute analysis time per sample. 23 fg/mL detection limit and the prostate specific antigen detection range of 23 fg/mL to 500 ng/mL were also reported.

In the year 2018, B. L. Borgne et al. [51] reported three dimensional SiNW based resistor (Fig. 12) for real time sensing of Escherichia coli bacteria. Using gold as catalyst, vapour liquid solid process is used to synthesize SiNWs. Through electrical measurement, resistor exhibited Escherichia coli bacteria detection ability at lower concentration of 6×10^3 CFU/mL. In the year 2019, K. Zhou et al. [52]

reported SiNW pH sensor fabricated using side wall mask technology via CMOS compatible process. Instead of using advanced lithography facilities, side wall mask technology facilitate in obtaining 10s or 100s of nano-meter feature sizes through film deposition method. This will help in the fabrication of SiNW with easy availability, low cost and high output. The sensor reported high sensitivity of 54.5 mV/pH, stability as well as repeatability in the pH range of 1 to 12. From the repeatability test measured for three times, 8 nA largest deviation was reported corresponding to 2.3%FS (Fig. 13).

In the year 2020, H. Zhang et al. [53] investigated the design as well as fabrication of SiNW biosensor through integration of critical factors for high sensitive detection of bio-molecules. Critical factors which affect the sensing performance of SiNW sensors namely functional interface, detection target and structure were analysed so as to enhance the sensing performance. It was reported that n-type narrow SiNWs with modest doping concentrations for impurities are useful for superior sensitive detection of negatively charged molecules. By controlling the thickness of the phosphorus dopant layer and thermal diffusion temperature, an n-type Si layer with a doping concentration of 2×10^{16} cm⁻³ to 6×10^{16} cm⁻³ was synthesized. Through the use of controlled plasma etching and a high-resolution EBL method, high-quality SiNWs of 16.0 nm width were fabricated. In order to transport the trapped charged molecules near the SiNW surface, the layer of native oxide on SiNW was used as the gate-insulator. The SiNW width of 16 nm in the biosensor exhibited exceptional FET properties, demonstrating the biosensor's potential to recognise biomolecules in very low concentrations. Additionally, 2-aminoethylphosphonic

Fig. 11 Schematic illustration of SiNW integrated with microfluidic channel [49]



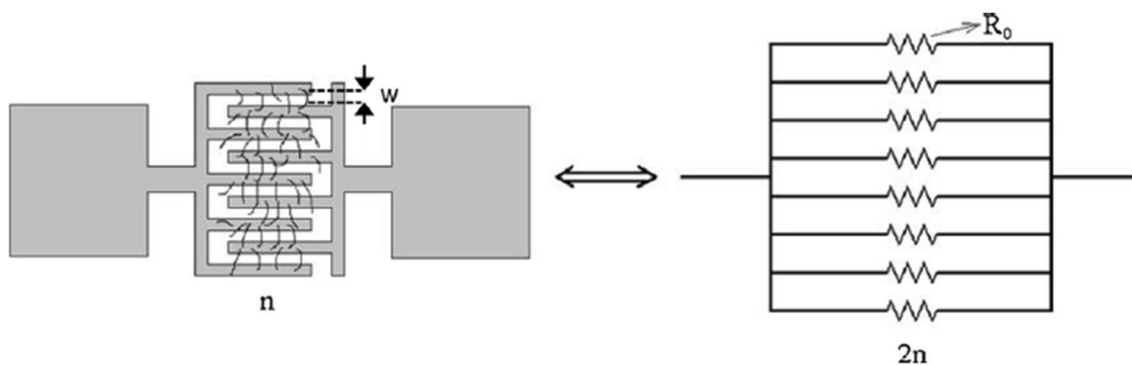


Fig. 12 Equivalent circuit diagram representation of SiLNW resistor [51] (Copyright @ Elsevier)

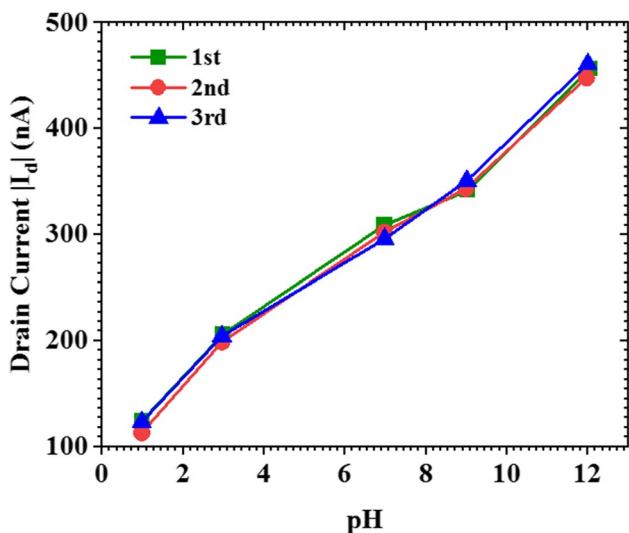


Fig. 13 SiLNW pH sensor repeatability test measured for three times in the pH range of 1 to 12 [52]

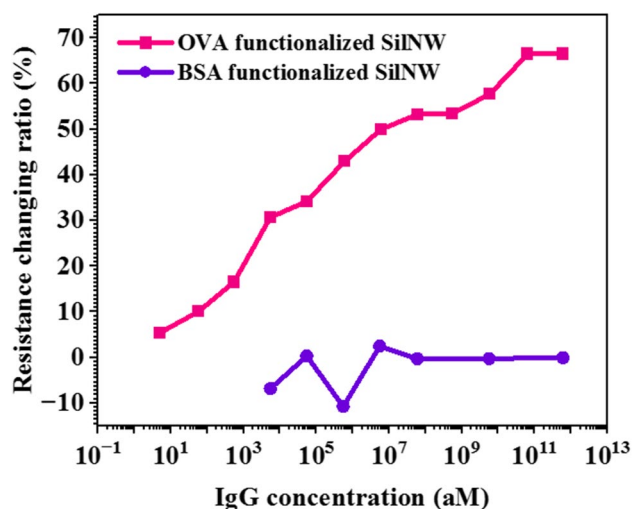


Fig. 14 Resistance changing ratio vs. IgG concentration plot of OVA functionalized and BSA functionalized SiLNWs [53]

acid coupling was used to alter the SiLNWs' surface, and SiLNW surface was functionalized using OVA molecules for target IgG molecules capture and to detect IgG with high specificity (Fig. 14) and sensitivity. 6 aM detection limit and detection range of 6 aM to 600 nM was reported in the optimized SiLNW biosensor towards target IgG.

In the same year, A. Gao et al.[54] reported B-nose based on AgOBP-functionalized SiLNW array for sensing volatile odorant molecules emitted by human. On a commercial SOI (111) wafer, the SiLNW array was fabricated using a low-cost novel top-down fabrication technique. With electric read-outs, the AgOBP-SiLNW device exhibited repeatable and reversible response. Highly specific structural selectivity and excellent sensitivity down to 2 ppb were also reported by the B-nose device. In the year 2021, D. Li et al. [55] reported SiLNW array biosensor for quantitating tumor marker circulating tumor DNA. The 120 SiLNWs served as a molecular gate for identifying the target circulating tumor DNA after

being silanized with the probe DNA. This SiLNW-array FET biosensor exhibited remarkable selectivity in the recognition of complementary target circulating tumor DNA from one, two, or whole base mismatched DNA. The sensor reported 10 aM detection limit and a linear detection range of 0.1 fM to 100 pM. Additionally, SiLNW array FET biosensor successfully identified target circulating tumor DNA in samples of human serum, indicating its promising future clinical application. In 2021, V. Gautam et al. [56] reported SiLNW/reduced graphene oxide nano composite based biosensor for detecting biomarkers of infectious diseases formaldehyde and cyclohexane. MACE (metal-assisted chemical etching process) was used to fabricate SiLNW, which at room temperature was then casted using graphene oxide. Under an inert atmosphere SiLNW/graphene oxide was reduced to SiLNW/reduced graphene oxide nano-composite using argon gas. SiLNW/reduced graphene oxide nano-composite was characterized using scanning electron microscope, energy

dispersive spectrometer, transmission electron microscope, X-ray diffractometer, fourier transform infrared and Raman spectroscopy. At room temperature, the Si/NW/reduced graphene oxide nanocomposite sensor exhibited a response of 1.07 and 0.99 for cyclohexane and formaldehyde concentrations of 1 ppm, respectively. The sensor displayed a quick response time of 30 s under ambient settings as well as detection limit of 1 ppm. The sensor also reported good repeatability (Fig. 15) and reproducibility. For cyclohexane and formaldehyde, the sensor's recovery time was 1–2 min and 3 min, respectively.

In the year 2022, Y. Benserhir et al. [57] reported fabrication of highly sensitive Si/NW based *Escherichia coli* bacteria detection sensor. This research employs a method that quantitatively assesses the contribution of bacteria immobilized on nanowires sandwiched between two electrodes via measuring significant change in current. 83 μA CFU/mL per decade sensitivity due to nanometric dimensions of the nanowires and 10^2 CFU/mL limit of detection to various *Escherichia coli* concentrations along with linear detection range of 10^2 CFU/mL to 10^8 CFU/mL were reported. In the same year, W. Zhao et al. [58] reported Si/NW FET biosensor device modified chemically with special antibodies for label free and electrical detection of exosomes. Using standard microelectronic process, the Si/NW FET was fabricated with 45 nm width NWs and was packed in a polydimethylsiloxane microfluidic channel. Further specific CD63 antibody was used to modify nanowire to form Si/NW FET biosensor. The sensor reported 2159 particles/mL limit of detection for A549 exosomes. Si/NW FET biosensor also reported the ability to sense real time changes in exosomes. The sensor exhibited real time decrease in current with increase in exosome concentration. In the year 2023, J.E.Santana et al.

[59] investigated the effect of amphetamine adsorption on the electronic and structural properties as well as on the work function of pristine and modified Si/NWs. Amphetamine which is one of the most commonly used illicit drug, was also employed in different medicinal therapies. Therefore, accurate tracking of amphetamine in various contexts is essential for its controlled distribution, even inside the human body. The two forms of changes that were investigated were surface functionalization using the same species as well as substitutional doping using boron, aluminium, and gallium atoms. Doped nanowires reported higher adsorption energies for the amphetamine molecule than functionalized ones and undoped Si/NWs. It was also reported that Boron is the best chemical species for enhancing amphetamine adsorption for both doped and functionalized Si/NWs. In the year 2023, J.E.Santana et al. [60] reported Si/NW functionalized with copper, silver and gold transition metal atoms for selective sensing of RNA/DNA nucleobases. The adsorption of single RNA/DNA nucleobases cytosine, adenine, thymine, uracil and guanine was examined using Density Functional Theory first-principles computations. It was observed that guanine, adenine and cytosine were more favourably adsorbed by copper functionalized Si/NWs and uracil and thymine prefer to adsorb on gold functionalized Si/NWs. As a whole, nucleobase adsorption modifies the metal functionalized Si/NWs original band structure by generating new localised states inside the band gap and close to the conduction band border which will enable their optical detection. The work function magnitude of the metal functionalized Si/NW varies as a result of nucleobase adsorption. The copper functionalized Si/NW exhibited the highest work function variation of 0.4 eV upon guanine and adenine adsorption. The sensing performance of different Si/NW bio-sensors was given in Table 1 [31–93].

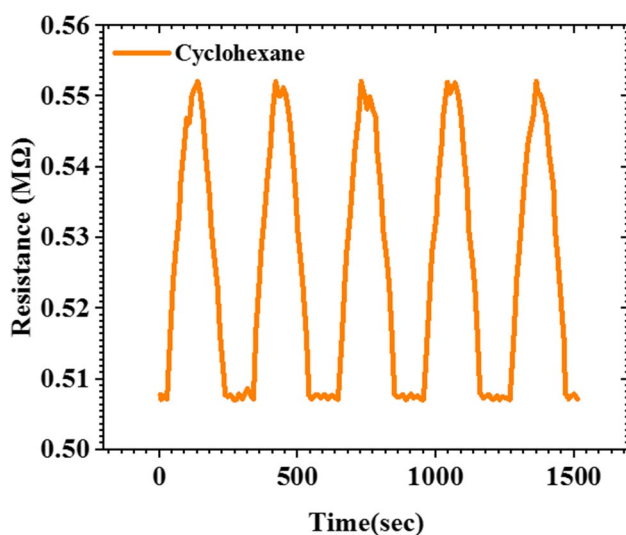


Fig. 15 Si/NW/reduced graphene oxide biosensor repeatability for cyclohexane at 1 ppm concentration [56]

3 Silicon Nanowire Based Covid-19 Sensors

The covid-19 virus outbreak in the year 2019–2020 caused thousands of deaths and widespread fear across the globe. The covid-19 virus has a high rate of transmission and is deadly. In addition to being a health emergency, covid-19 created an adverse financial impact. In March 2020, covid-19 was declared a worldwide pandemic and health emergency. In terms of electrical detection, one of the most promising platforms for covid-19 virus is a biosensor based on semiconductor field-effect devices [94–98]. In 2022, A. Wasfi et al. [99] reported Si/NW FET based covid-19 sensor using a semi-empirical modelling approach integrated with covid-19 anti-spike protein antibody. A. Wasfi et al. investigated the charge transport properties of Si/NW FET which consists of a channel, gate and two electrodes. Significant changes in transmission spectra current, and conductance were seen

Table 1 Sensing performance and application of different SiNW biosensors [31–93]

Ref	SiNW sensor type	Target	LoD	Detection Range	Sensitivity	Response Time
[31]	Organophosphonate based PNA functionalized SiNW	DNA	-	-	-	-
[32]	SiNW sensor	Dengue virus	10 fM	-	-	30 minutes
[33]	Gold nanoparticle embedded SiNW biosensor	DNA	1 pM	-	-	-
[34]	Morpholino functionalized SiNW biosensor	DNA	100 pM	-	-	-
[35]	SiNW modified by gold NPs	Albumin	-	1 to 7 μ M	-	-
[36]	SAM-assisted SiNW biosensor	ER α	10 fM	-	-	-
[37]	SiNW array	DNA	-	-	-	-
[38]	SiNW FET biosensor	DNA-HMGB1 binding	-	-	-	-
[39]	SiNW biosensor	DNA	-	-	-	-
[40]	N ₂ O plasma modified SiNW biosensor	Interleukin-1 β gene	2.5 fM	-	0.12/decade	-
[41]	Modified SiNW sensor	Alkaline phosphatase	0.0175 U/mL	0.0175 to 0.3 U/mL	-	20 minutes
[43]	Multi-channel SiNW biosensor	Cardiac troponin I	320 fM	-	-	-
[44]	Liquid-based gate-control SiNW biosensor	ssDNA	0.1 nM	100 pM to 25 nM	-	-
[45]	SiNW/Amplifier MOSFET Hybrid biosensor	pH detection	-	-	-	-
[46]	SiNW -Polycrystalline FET biosensor	Ferritin	50 pg/mL	50 pg/mL to 500 ng/mL	133.47 mV/pH	-
[47]	O ₂ plasma treated SiNW biosensor	Dengue Virus	1.985 x 10 ⁻¹⁴ M	1.0 x 10 ⁻⁹ M to 1.0 x 10 ⁻¹³ M	-	-
[48]	SiNW FET biosensor	Cardiac troponin I	~5 pg/mL	-	-	-
[49]	SiNW biosensor	Dengue virus DNA	2.0 fM	-	45.0 μ AM ⁻¹	-
[50]	SiNW FET biosensor	PSA	23 fg/mL	23 fg/mL to 500 ng/mL	70 mV/pH	5 to 10 seconds
[51]	3D SiNW based resistor	Escherichia coli bacteria	6 \times 10 ³ CFU/mL	-	-	< 1hour
[52]	SiNW FET	pH detection	-	-	54.5 mV/pH	-
[53]	n-type SiNW	IgG	6aM	6 aM - 600 nM	-	-
[54]	SiNW array	Volatile odorant molecules	-	-	-	-
[55]	SiNW array biosensor	ctDNA	10 aM	0.1 fM to 100 pM	-	-
[56]	rGO/SiNW nanocomposite	Cyclohexane and formaldehyde	1 ppm	-	-	30 seconds
[57]	SiNW biosensor	Escherichia coli bacteria	10 ² CFU/mL	-	83 μ A/decade of CFU/mL	-
[58]	SiNW bio FET	Exosomes	2159 particles/mL	-	-	-
[59]	SiNW sensor	Amphetamine drug detection	-	-	-	-
[60]	Metal functionalized SiNW sensor	RNA/DNA nucleobases	-	-	-	-

Table 1 (continued)

Ref	SiNW sensor type	Target	LoD	Detection Range	Sensitivity	Response Time
[61]	SiNW FET	Cancer biomarker detection	-	-	-	-
[62]	SiNW-ECIS	Cancerous cultured living lung cells detection	-	-	-	-
[63]	SiNW FET	Particle counting	-	-	-	-
[64]	SiNWs/anti-PSA/AgNPs/MCH sensor	Prostate specific antigen	0.1 $\mu\text{g.L}^{-1}$	0.1-20 $\mu\text{g.L}^{-1}$	-	-
[65]	SiNW FET	MMP-9	7.6 pg/ml	-	86.96%	-
[66]	SiNW FET decorated with polyethylene glycol	MicroRNA	10 aM	10 aM to 10 pM	-	-
[67]	SiNW FET	ALT	4.1 \pm 0.4 U/L ALT	-	-	-
[68]	SiNW FET	pH	5nS/pH unit	-	-	-
[69]	SiNW ion sensitive FET	pH	-	-	-	-
[70]	Coaxial structured ZnO/SiNW EGFET	pH	-	-	46.25 mV/pH	-
[71]	SiNW dual gate sensor	pH	-	-	1438.8 mV/pH	-
[72]	Double gate SiNW FET	pH	-	-	720.7 mV/pH	-
[73]	SiNW with SiO ₂ /Al ₂ O ₃ sensing membrane	pH	-	-	60.2 mV/pH	-
[74]	IGZO/SiNW sensor	pH	-	-	50 mV/pH	-
[75]	SiNW	Intracellular biochemical sensing	-	-	-	-
[76]	SiNW PDMS	Prostate specific antigen	1 fg/mL	-	-	-
[77]	SiNW FET	α -fetoprotein	-	500 fg/mL to 50 ng/mL	-	-
[77]	SiNW FET	Carcinoembryonic antigen	-	50 fg/mL to 10 ng/mL	-	-
[78]	SiNW array biosensor	Carcinoembryonic antigen	10 fg/mL	10 fg/mL to 100 pg/mL	-	-
[79]	SiNW FET	Carcino embryonic antigen	1 fg/ml	-	-	-
[79]	SiNW FET	microRNA 126	0.1 fM	-	-	-
[80]	Magnetic graphene composite modified poly-SiNW-FET	APOA2 protein	6.7pgmL ⁻¹	19.5pgmL ⁻¹ -1.95 μgmL^{-1}	-	-
[81]	Silicon on insulator nanowire biosensor	D-NFATc1 protein	10 ⁻¹⁵ M	-	10 ⁻¹⁴ M	-
[82]	SiNW FET	α -fetoprotein	10 ng/ml	-	-	-
[83]	SiNW FET	α -fucosidase	1.3 pM	-	-	-
[84]	SiNW FET	Vascular endothelial growth factor	2.59 nM	-	-	-
[85]	SiNW FET	ALCAM biomarker	15.5 pg/ml	-	-	30 minutes
[86]	SiNW FET	Vascular endothelial growth factor	-	5to 200 fM	-	-
[87]	SiNW FET	DNA	1 fM	-	-	-
[88]	SiNW FET	DNA	0.1 fM	-	-	-
[89]	Silicon on insulator NW biosensor	microRNA	10 ⁻¹⁷ M	-	-	-

Table 1 (continued)

Ref	SilNW sensor type	Target	LoD	Detection Range	Sensitivity	Response Time
[90]	Silicon on insulator nanowire biosensor	Tumor M2-PK	-	10^{-13} to 10^{-15} M	-	-
[91]	SilNW FET Sensor Arrays	CRP proteins	-	-	1.2 nA/dec	-
[92]	SilNW FET	H3N2 virus	10^4 viruses/L	-	-	-
[93]	SilNW sensor	Influenza A viruses	29 viruses/ μ L	-	-	-

in the presence of the covid-19 spike protein. The sensors performance was evaluated using the variation in current. The difference between bare sensors current and the current for the sensor as a result of the positioning of the target molecule was computed. The spike protein which is negatively charged caused extra hole-carriers, which decreased the current from drain of the SilNW-FET sensor during the placement of the target molecule (Fig. 16).

In the year 2022, B. Gao et al. [100] reported vertically oriented SilNW array based sensor for spike protein SARS-Covid-2 detection. Biosensor is based on vertically oriented SilNW arrays coupled to angiotensin converting enzyme-2, has strong selectivity and sensitivity for sensing SARS-Covid-2 spike protein. (Fig. 17). Using a metal-assisted chemical etching method, huge area arrays of vertically oriented SilNW arrays were created. The Sil substrate was transformed into a p-n junction diode that is electrically active following the vertical SilNW metal-assisted chemical etching process. The fabricated SilNW biosensor has 10^{10} vertical SilNWs per cm^2 area density and 350 nm average vertical SilNW length. 100 ng/ml limit of detection and response time of less than one hour have been reported in

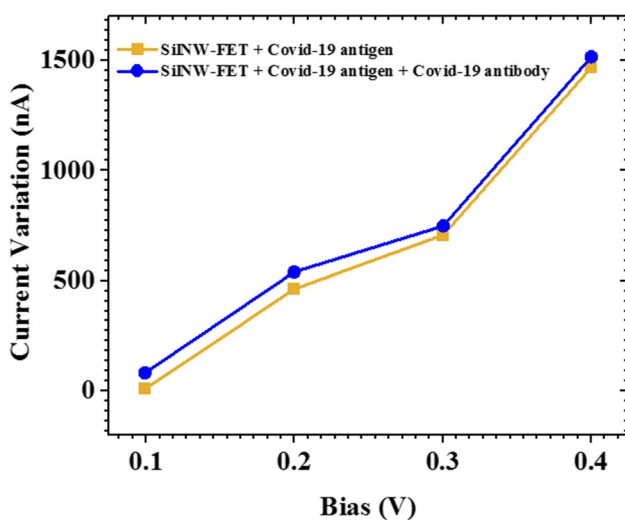


Fig. 16 Drain current variation in SilNW covid-19 sensor due to spike protein [99]

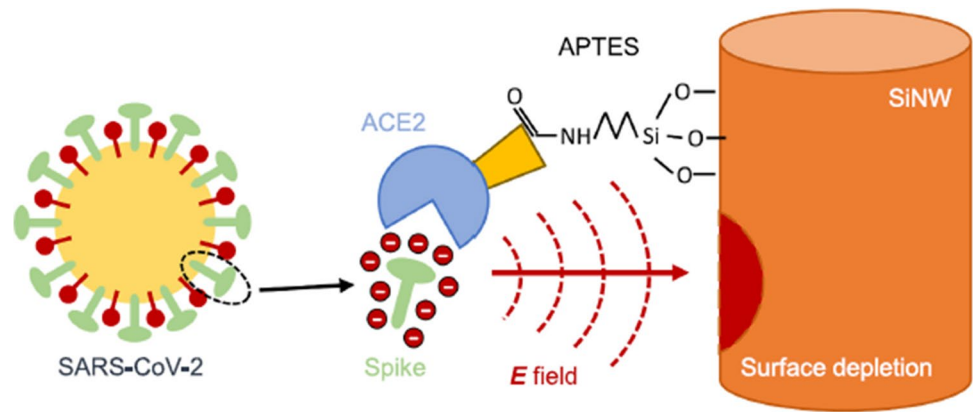
the fabricated vertical SilNW covid-19 biosensor. Offering a viable point-of-care detection approach for SARS-Covid-2 virus, the vertical SilNW sensor exhibited excellent specific response to the spike protein compared to negative controls.

In the year 2022, Chi-Chang Wu [101] reported polycrystalline SilNW FET sensor to detect SARS-Covid-2 spike protein. In order to keep the NW diameter within 100 nm, sidewall spacer etching was used to fabricate SilNW FET. 125 mV/decade sub-threshold swing and 10^6 on-off current ratio were reported in SilNW FET which indicates its strong stability and attributes. Using a pH range of 6 to 9 to evaluate solution, the polycrystalline SilNW FET biosensor exhibited a sensitivity of 59 mV pH^{-1} . The sensor also reported a limit of detection of 0.51 ng ml^{-1} .

4 Silicon Nanowire Based Gas Sensors

For the purpose of identifying different gases that have a harmful environmental impact as well as on people safety, gas sensors play a crucial role in our daily lives. Due to their distinct electrical characteristics, SilNWs finds application in instantaneous, sensitive and label-free detection of different gases. The SilNW based devices used for gas sensing are made up of both vertically standing and in-plane oriented SilNW [102–106]. In the year 2009, J. Wan et al. [107] reported SilNW sensor fabricated using PMMA/SiO₂/SU8 trilayer-nanoimprint method for gas detection. The SOI substrate, which is boron doped at $8 \times 10^{17} \text{ cm}^{-3}$ dopant concentration, was used in the fabrication of SilNW gas sensor. For comparison, a thin-film device and two SilNW sensors with 130 nm and 75 nm nanowire line widths were developed. The fabricated sensors were then used for sensing 250 ppm of NH₃ and NO₂. The carrier traps created during the reactive ion etching process after trilayer imprinting was reported as the reason for substantial increase in resistance of the NW devices. Due to its large surface to volume ratio, the narrower SilNW device in particular exhibited a notable improvement in sensitivity. 61.8% sensitivity for NH₂ gas and -19.7% sensitivity for NH₃ gas were reported in 75 nm SilNW sensor. In the year 2010, C. Gao et al. [108]

Fig. 17 Detection mechanism of vertically oriented SiNW biosensor [100] (Copyright @ Elsevier)



reported SiNW based gas sensor down to 22 nm wide fabricated using wet etching and trilayer nano imprint method. On the Si on insulator substrate, samples with 22 and 75 nm top widths were developed. The fabricated devices were evaluated for NO₂ gas detection in a 250 ppm NO₂ environment. When compared to 75 nm wide one, 22 nm wide NW device reported higher relative sensitivity. Sensor with 22 nm NW width exhibited relative sensitivity of 14.7% for NO₂ while relative sensitivity of 7.0 % for NO₂ was reported in device with 75 nm NW width. In the same year, K. Skucha et al. [109] reported palladium/SiNW schottky barrier FET based hydrogen sensor that functions at ambient temperature. The sensor was made of boron-doped contact-printed SiNW arrays on top of a Si/SiO₂ substrate with palladium contacts onto it that are subsequently evaporated. The sensor reported 6.9%/ppm sensitivity at 1000 ppm and was capable of reversibly and reliably detecting hydrogen concentrations in the range of 3 ppm to 5%. For hydrogen concentrations above 1000 ppm and over 100 ppm, the sensor reported a response that can be distinguished from noise and drift in less than 5 seconds and less than 30 seconds respectively. In the year 2011, C. Gao et al. [110] reported SiNW gas sensor fabricated via angled physical vapour deposition and bilayer nano imprint method with NW width ranging from 22 to 110 nm. This fabrication method was suggested as an alternate method for low-cost, high-resolution, ultra-thin and large-throughput production of NW sensors such that the widths of NW can be adjusted. On the boron-doped top Si layers of the Si on insulator substrate, SiNWs of varying widths were produced and was employed as the sensing components of gas sensor. The sensor with 60 nm SiNW width reported 155% sensitivity and SiNW with 90 nm width reported 44% sensitivity for 250 ppm of NO₂ gas. In the year 2013, L. Yang et al. [111] reported tellurium modified SiNW gas sensor for detecting propylamine and ammonia gas. Solution approach was used to grow tellurium nanoparticles on SiNWs, with an average diameter of 5 nm. Tellurium modified SiNW gas sensor

exhibited low detection limits of 174 ppb and 196 ppb for propylamine and ammonia along with a detection range of 5 ppm to 25 ppm and 10 ppm to 400 ppm respectively. The sensor exhibited response time of 15 second and 5 seconds upon exposure to propylamine and ammonia. The recovery time reported was 6 second and 8 seconds respectively. The tiny size of tellurium nanoparticles has been ascribed as the reason for sensors quick response and high sensitivity. In the year 2014, Y. Wu et al. [112] reported p-porous Si/ p-TeO₂ NW gas sensor for detecting NO₂. Thermal evaporation was used to fabricate porous Si/ p-TeO₂ NW gas sensor using porous Si as growth substrate and Te powder as the source material. At 26°C to 150°C working temperature (Fig. 18) and NO₂ concentrations that range from 0.05 ppm to 3 ppm, the gas sensing characteristics of pure porous Si sensors and composite structure sensors were investigated. The composite structure sensor reported good NO₂ selectivity at room temperature, great repeatability and high responsiveness. In the year 2015, S. Naama et al. [113] reported SiNW based CO₂ gas sensor fabricated in AgNO₃/HF aqueous solution through metal-assisted one-step electroless etching technique. Platinum and gold nanoparticles were added to SiNWs via electroless metal deposition method.

Higher response was reported in gold modified structure biased with less voltages. The sensor response was computed as [113]

$$S = \frac{I_g - I_v}{I_v} \quad (4)$$

where I_v and I_g are the devices responsive current values in presence of primary vacuum and CO₂ gas.

In the year 2017, Y. Qin et al. [114] reported silver modified SiNW NH₃ gas sensor. Metal-assisted chemical etching was used to create SiNWs, and a key anisotropic post etching of TMAH was used to modify the silver NP in situ using the metal assisted chemical etching produced Ag dendrites. When compared to pristine SiNWs, approximately three

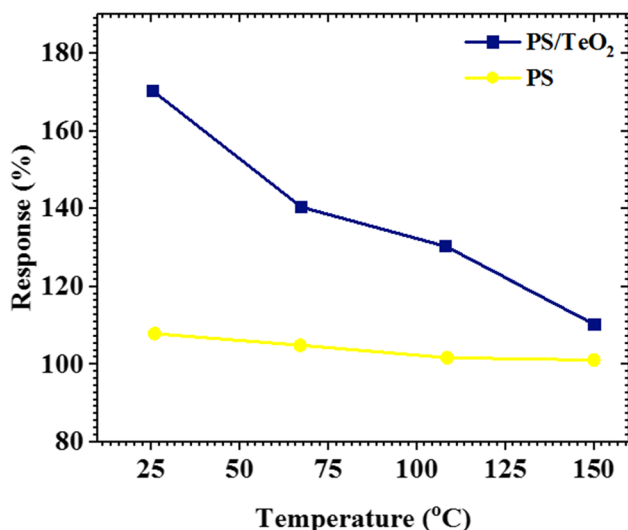


Fig. 18 Response curve to 1 ppm NO₂ of pristine PS and PS/TeO₂ NW gas sensor at various temperatures [112]

fold enhancement in gas response was reported in silver modified SiNWs. Response time, less than 2 seconds and recovery time less than 9 seconds were reported in silver modified SiNWs for 0.33 ppm to 10 ppm of NH₃. In the same year, Y. Qin et al. [115] reported WO₃/SiNWs dendritic composite array based gas sensor for detection of NO₂. From the top section of each SiNW produced by metal-assisted chemical etching, WO₃ well-defined NWs form a hierarchical structure resembling dendrites. The WO₃/SiNWs exhibited response with significant improvement in NO₂ sensing. Exposure to 0.5 ppm to 5 ppm NO₂ resulted in transient response with response time less than 1 second. For the purpose of detecting ammonia at ambient temperature, sensitive porous Si/Pd-loaded WO₃ NWs based resistive-type gas sensor was reported in the year 2018 by X. Qiang et al. [116]. Thermal evaporation of W powder over a porous Si substrate was used to fabricate porous Si/WO₃ NWs, and in-situ reduction was used to decorate the surface of the WO₃ NWs with Pd nanoparticles. The porous Si/Pd-loaded WO₃ NWs exhibited a quick recovery-response time, strong selectivity, and an increased response to ammonia at low concentrations down to 1 ppm when compared to porous Si/WO₃ NWs (Fig. 19). It was observed from the enhanced sensing properties that Pd NP was ideal in enhancing the performance of SiNW gas sensor.

In the year 2019, J. Yun et al. [117] reported high performance H₂ gas sensor with lower power usage and great stability against various environmental noises via suspended, self-heated and palladium decorated SiNWs. SiNWs were produced using standard complementary metal-oxide semiconductor technique, and palladium NPs were then added using a physical vapour deposition method to create the palladium decorated SiNWs. In contrast to existing palladium

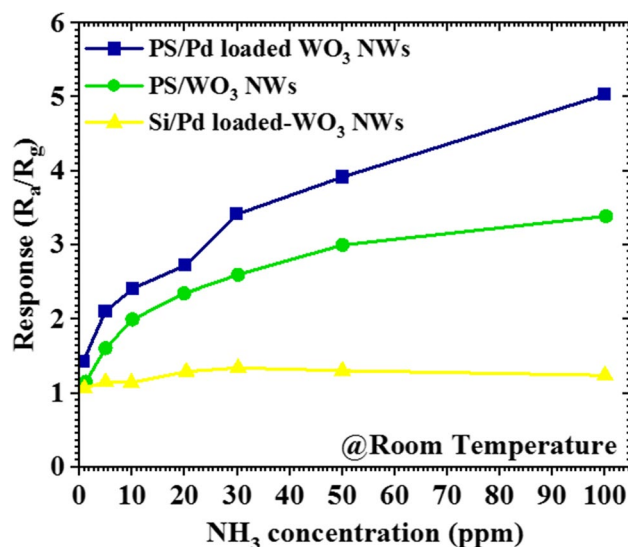


Fig. 19 Response of porous Si/WO₃ NWs, porous Si/Pd-loaded WO₃ NWs and Si/Pd-loaded WO₃ NWs for various NH₃ concentrations in room temperature [116]

based H₂ gas sensors, joule heating of palladium-SiNW (< 1 mW) permits H₂ gas detection with a quicker response time and without a loss of sensitivity. In the year 2020, Y. Qin et al. [118] reported a stable clusters array of SiNWs with a special aggregation interconnection structure. The Cu₂O top-plating process used several spin-coatings of HF solution and Cu²⁺ on SiNWs to produce the stable aggregation interconnection structure. Vertical SiNWs with distinct tip aggregation interconnection structure in various clusters were produced by the top plating procedure in a stable and distinctive clusters array. The as-formed aggregation interconnection array was reported to be a highly efficient gas sensor, delivering a steady response with highly sensitivity and a low detection limit at ambient temperature. The aggregation interconnection-SiNWs sensor demonstrated a response value which is approximately 64 times better to 1 ppm NO₂ when compared to pristine SiNWs sensor. The sensor reported a limit detection of 5.4 ppb to NO₂ gas. In the year 2021, A. Mukherjee et al. [119] reported a high performance ultra-sensitive palladium nanoparticles decorated electrostatically formed SiNW based H₂ sensor. The electrostatically produced NW gate biases were properly tuned resulting in a sensitivity of approximately 400% ppm⁻¹ and exceptional sensor response of 2x10⁶% for 0.8% H₂ (Fig. 20). The sensor also exhibited quick recovery and response times, strong sensing capability even with a relative humidity of 50%, and repeatability across time.

Ethanol is a vital VOC and significantly contributes to the detection of drunk driving. In the year 2021, Y. Qin et al. [120] reported SiNW ethanol sensor modified by ZIF-67 (Fig. 21) with enhanced moisture resistance and

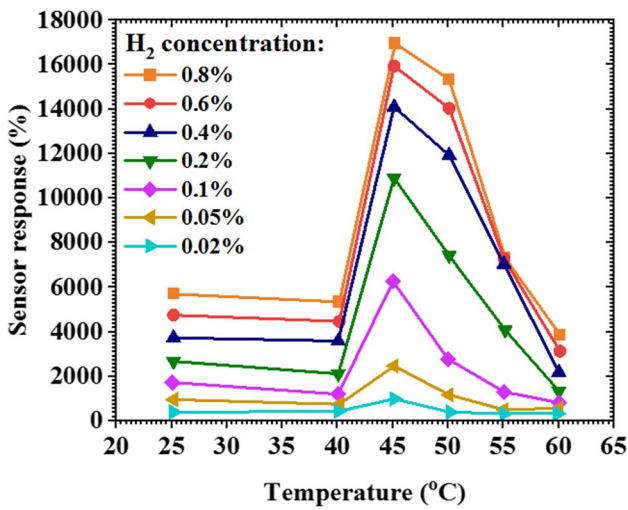


Fig. 20 Temperature vs sensor response plot of electrostatically formed SiLNW sensor at various H₂ concentrations [119]

expanded detection range. The sensor showed a practical ability to detect 250 ppb ethanol with 25% response at room temperature with a 25% relative humidity. The developed ZIF-67 decorated SiLNWs sensor still exhibited a substantial reaction when exposed to ethanol at concentrations between 0.25ppm to 200 ppm at high humidity of 65%. The sensor maintained 95% performance after 30 days and exhibited good concentration stability. In 2021, P. Dwivedi et al. [121] reported SiLNW decorated with indium trioxide sensor for detection of ethanol. Metal assisted chemical etching method was used to fabricate SiLNWs and thin film of indium was used to decorate it followed by annealing. Au-Cr inter-digitated electrode structure which was integrated on the top of the sensing layers was employed to compute the resistance change in order to measure the sensing response. At close to room temperature, the sensor’s responsiveness to ethanol was greatly enhanced by indium trioxide integration in SiLNWs. SiLNWs and indium

trioxide decorated SiLNWs-based sensors reported 50 ppm and 10 ppm minimum ethanol detection respectively. The oxygen species present on indium trioxide NPs on the surface of SiLNWs and the hetero structure generated at the interface was reported as the cause for this superior sensing behaviour. In 2021, X. Song et al. [122] reported integratable fabrication of SiLNW based field effect sensors through in-plane step-guided solid-liquid-solid growth for ammonia gas sensing at room temperature. By tuning the back gated SiLNW sensors into appropriate sub threshold detection regime, 75.8% excellent field-effect sensitivity at 100 ppm NH₃, 100 ppb low limit of detection, rapid response/recovery time of 20 seconds and outstanding stability of over 180 days has been reported. These exceptional sensing abilities are due to the quick charge transfer between adsorbed NH₃ molecules and the exposed SiLNW channels, suggesting a practical method for fabricating and deploying extremely effective gas detectors, which are in great demand in the emerging portable or wearable electronics market. The sensitivity of SiLNW based field effect ammonia sensor was computed as [122]

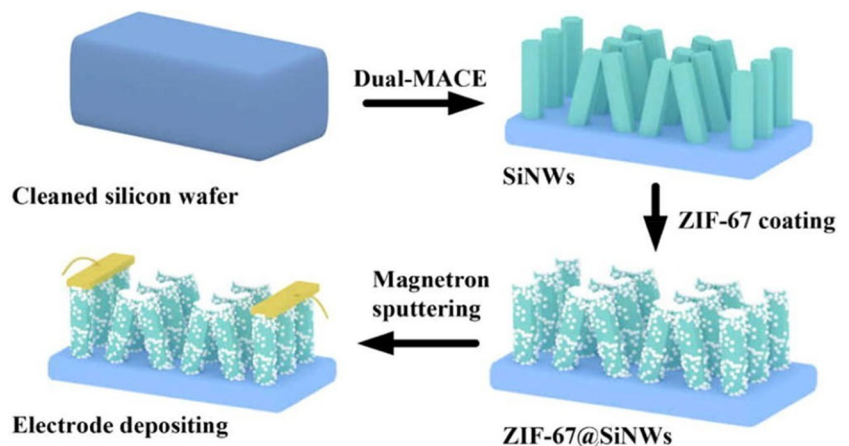
$$S(\%) = \left[\left(\frac{|I_{ds, NH_3}|}{|I_{ds, air}|} \right) - 1 \right] \times 100 \tag{5}$$

where $|I_{ds,air}|$ and $|I_{ds,NH_3}|$ represents I_{ds} when exposed to air ambient gas and ammonia gas.

In the year 2022, V. Kashyap et al. [123] reported SiLNW based nitrogen dioxide gas sensor fabricated through low cost metal assisted chemical etching technique.

The dislocation density of the synthesised SiLNWs decreased concurrently with the rise in crystallite size, according to the structural study. The array of SiLNWs had an approximate average size of 80 ± 0.001 nm and 97 ± 5 nm for the p₄₀ and n₄₀ samples respectively, according to the results of the morphological study. At 50 ppm, maximum sensing capabilities for the n₄₀-type SiLNW based gas sensor was identified to be 68%, 63% and 35%

Fig. 21 Fabrication process of SiLNWs decorated by ZIF-67 [120] (Copyright @ Elsevier)



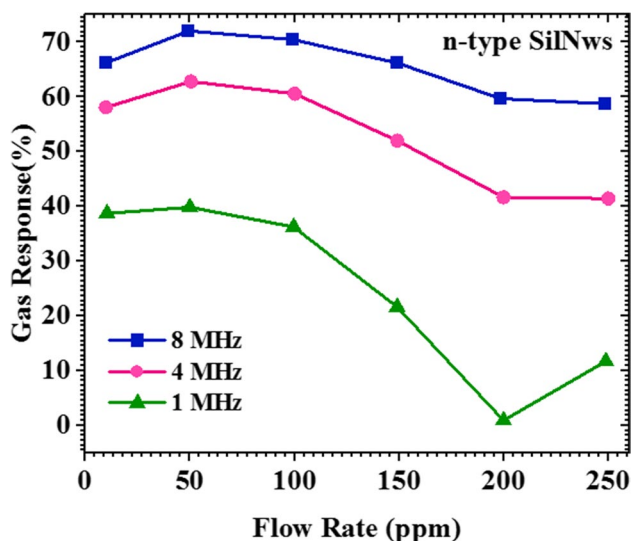


Fig. 22 n-type SiLNW gas sensor response for different NO₂ concentration as a function of frequency [123]

at 8, 4, and 1 MHz, respectively, while it was 62%, 68% and 75% for the p₄₀-type SiLNW based sensor. The results indicate that the n₄₀-type SiLNW-based sensor is optimal in NO₂ gas detection at lower frequencies (Fig. 22) and room temperature, while the p₄₀-type SiLNW-based sensor is ideal for NO₂ gas detection at room temperature and higher frequencies (Fig. 23).

In the year 2022, P. Nath et al. [124] reported SiLNW ammonia sensor fabricated via metal assisted electrochemical etching process. On a Si wafer that has been electroplated with silver, the etching process was carried out with the aid of dc-current delivered by an 6634B Agilent dc-power supply. The technique resulted in ordered SiLNWs with a greater surface area. According to gas sensing tests, SiLNWs exhibit reasonable recovery and response durations with 10 ppm low detection limit and are extremely selective for ammonia when compared to other gases, with improved response sensitivity. In the year 2023, R. Chaujar et al. [125] reported gate-all-around junctionless SiLNW FET based hydrogen sensor. Palladium was used as a gate electrode because of its sensitivity to hydrogen gas. SiO₂ interface oxide and high dielectric oxide were used at the gate to combat electron tunnelling. Enhanced sensitivity was reported in gate-all-around junctionless SiLNW FET hydrogen sensor when compared to bulk MOSFET and gate-all-around MOSFET. The results demonstrate that the gate-all-around junctionless SiLNW FET based hydrogen sensor exhibited sensitivity improvements of 124.51% and 51.65%, respectively, over MOSFET and GAA-MOSFET, as 150mV palladium work function shifts at the gate. Sensing performance of different SiLNW gas sensors was given in Table 2 [107–135].

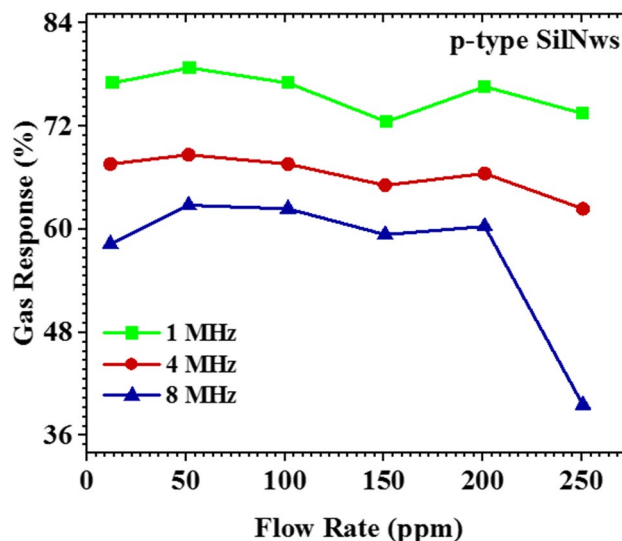


Fig. 23 p-type SiLNW gas sensor response for different NO₂ concentration as a function of frequency [123]

5 Silicon Nanowire Based Chemical and Metal Ion Sensor

SiLNWs were the focus of significant study for high sensitivity chemical sensors due to their surface potential sensitivity to charged species and their high surface to volume ratio [136–139]. In the year 2001, Y. Cui et al. [140] reported the first SiLNW based chemical species sensor for streptavidin detection. SiLNW modified with biotin were able to sense streptavidin in picomolar concentration range (10 pM). Y. Cui et al. also investigated the Ca²⁺ sensing of SiLNWs which are crucial for triggering biological operations including contraction of muscles, cell death, protein release and cell development. The conductance decreased when a 25 μM Ca²⁺ solution was added, according to data obtained from modified SiLNW devices, and then increased when a free buffer Ca²⁺ was subsequently passed through the device. Control trials using unaltered SiLNWs showed no conductance change when Ca²⁺ was introduced, proving that the calmodulin receptor is necessary for detection.

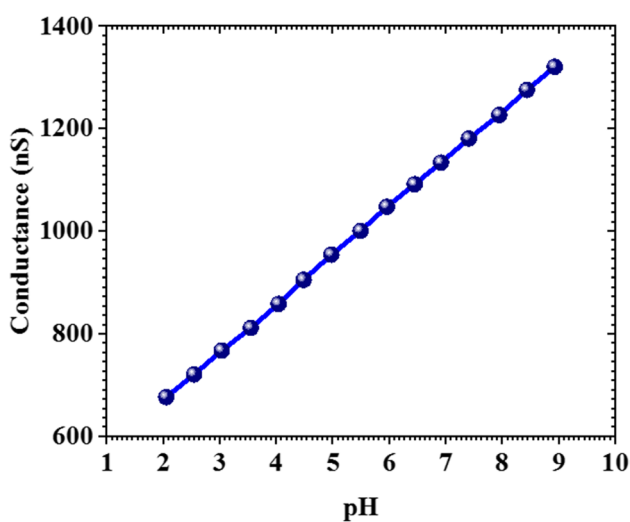
Additionally, 10⁻⁵M-10⁻⁶ M estimated dissociation constant, was compatible with the known K_d for calmodulin, and the observed conductance drop in modified SiLNWs is consistent with predicted chemical gating by positive Ca²⁺. Y. Cui et al. also investigated pH dependent conductance of oxide and amine functionalized SiLNWs. The pH dependency was observed to be linear across the pH range of 2 to 9 (Fig. 24), making modified SiLNWs ideal be used as pH sensors in the nanoscale. In the year 2008, X. Bi et al. [141] reported SiLNW based electrochemical calcium sensor modified with phosphotyrosine. SiLNWs were used as channels in a FET which is chemically gated

Table 2 Sensing performance of different Si/NW gas sensors [107–135]

Ref	Si/NW sensor type	Target	Sensitivity	LoD	Response Time	Recovery Time
[107]	Trilayer nano imprinted Si/NW sensor (75 nm NW)	NH ₂	61.8%	-	-	-
[107]	Trilayer nano imprinted Si/NW sensor Si/NW (75 nm NW)	NH ₃	-19.7%	-	-	-
[108]	22 nm Si/NW gas sensor	NO ₂	14.7%	-	-	-
[109]	Si/NW/Palladium schottky barrier based sensor	H ₂	6.9%/ppm at 1000 ppm.	< 5 second for H ₂ concentrations over 1000 ppm	-	-
[110]	Angle deposition +Bilayer NIL + RIE (60 nm Si/NW)	NO ₂	155% to 250 ppm NO ₂	-	-	-
[111]	Tellurium modified Si/NW	Ammonia	-	196 ppb	5seconds	8 seconds
[111]	Tellurium modified Si/NW	Propylamine	-	174 ppb	15seconds	6 seconds
[112]	p-porous Si/p-TeO ₂ NWs	NO ₂	-	-	-	-
[113]	Au modified Si/NW(0.5mbar)	CO ₂	-	-	303 seconds	311 seconds
[113]	Pt modified Si/NW(0.5mbar)	CO ₂	-	-	143 seconds	120 seconds
[114]	Ag-modified Si/NW	NH ₃	-	-	≤ 2 seconds	≤ 9 seconds
[115]	Si/NWs/WO ₃ NWs	NO ₂	-	-	< 1 seconds to 0.5ppm to 5ppm NO ₂	-
[116]	Porous silicon/Pd-loaded WO ₃ NWs	Ammonia	-	1 ppm	3 second - 10 second	-
[117]	Joule heated and suspended Si/NW	H ₂	-	-	-	-
[118]	Si/NW arrays	NO ₂	-	5.4 ppb	-	-
[119]	Palladium NPs decorated Si/NW	H ₂	~400 % ppm ⁻¹	-	78 seconds	434 seconds
[120]	ZIF-67 modified Si/NW	Ethanol	-	-	-	-
[121]	In ₂ O ₃ decorated Si/NW	Ethanol	-	10 ppm	-	-
[122]	Self-aligned Si/NW FET	Ammonia	75.8% for 100 ppm NH ₃	100 ppb	-	-
[123]	Vertical Si/NW array	NO ₂	-	-	-	-
[124]	Si/NW sensor	Ammonia	-	-	-	-
[125]	Gate-all-around junctionless Si/NW FET	H ₂	-	-	-	-
[126]	Si/NW based resistor	NH ₃ and Smoke	-	-	-	-
[127]	CuO NPs decorated Si/NW	Non-enzymatic H ₂ O ₂	22.27 μA/mM	1.6μM	-	-
[128]	Suspended Si/NW	Ammonia	-	-	-	-
[129]	Bottom-gate Si/NW FET	H ₂	154.5%	-	-	-
[130]	Si/NW/WO ₃ NW	NO ₂	-	-	-	-

Table 2 (continued)

Ref	SilNW sensor type	Target	Sensitivity	LoD	Response Time	Recovery Time
[131]	Si/tungsten oxide NWs	NO ₂	-	-	14 seconds at 250°C	-
[132]	Vertically aligned SilNW/ZnO structures	CO ₂	-	-	2 to 7 seconds	2 to 7 seconds
[133]	SilNW sensor	Petroleum vapor detection	-	-	-	-
[134]	MoS ₂ /porous SilNW	NO ₂	-	1 ppm	-	-
[135]	SilNW/graphene heterostructure molecular sensors	H ₂ and O ₂	-	-	0.15/3.5 seconds	0.15/12 seconds

**Fig. 24** Conductance vs. pH plot of oxide and amine functionalized SilNWs [140]

for the electrical detection of calcium ions. The SilNWs are modified with phosphotyrosine amino acid, which will bind the calcium ions with high affinity, to provide a sensitive and selective layer for calcium sensing. When exposed to aqueous solutions having calcium ions, phosphotyrosine modified SilNW reported increase in conductance with increase in concentration of calcium up to 10 μM. In the same year, X. Bi et al. [142] reported SilNW FET sensor modified with tripeptide for detection of copper ions. Gly-Gly-His modified SilNWs was used as channel in the fabricated FET which reported excellent specificity and sensitivity to detect copper ions. The modified SilNW conductance change exhibits linear increase with logarithm of the copper concentrations and was attributed as the reason for stable complexation between Gly-Gly-His and copper ions. The percentage variation in conductance was computed as [142]

$$G\% = \frac{G_{Cu} - G_{buffer}}{G_{buffer}} \times 100\% \quad (6)$$

where G_{buffer} and G_{Cu} represents Gly-Gly-His modified SilNW conductance without and with copper ions

Even in the presence of Zn, Gly-Gly-His modified SilNWs reported good selectivity and response for copper ions as low as 1 nM in real-time and with reversibility when compared to Gly-His-Gly-modified SilNWs. In the year 2009, X. Bi et al. [143] reported multi-channel ion sensor using oligopeptide modified SilNW arrays. Due to the top-down fabrication method used to create these SilNW arrays, very dense individually addressable SilNW (180 SilNWs organised into thirty six clusters) has been produced on a single chip. Sil-on-insulator wafers with Sil oxide and Sil that are each 50 nm and 80 nm thick, respectively, were employed as substrate. The concentrations of Cu^{2+} and Pb^{2+} in aqueous solutions may also be monitored concurrently and selectively in two separate channels after two distinct SilNW clusters have been modified with Cu^{2+} and Pb^{2+} selective oligopeptide respectively. 10 nM detection limit for Cu^{2+} and 1 nM detection limit for Pb^{2+} were reported in oligopeptide modified SilNW arrays. In the year 2011, J. Yin et al. [144] reported electro chemical hydrogen peroxide sensor based on SilNW arrays decorated with silver NPs. Silver ions can be reduced by the ordered H-terminated SilNW arrays fabricated by electroless etching, resulting in the deposition of silver NPs on SilNW. According to the electrochemical experiment results, the silver nanoparticles decorated SilNW array sensor showed more active areas for chemical reaction processes per unit area and high electrical conductivity. As a result, it has a quick amperometric sensing, a broad linear response spectrum, minimal detection limit and good sensitivity to hydrogen peroxide. The sensor can attain in 4 seconds, 95% of the maximum steady-state current at an applied voltage of 0.45V and a pH of 7.5 with 0.2 μM detection limit. In the year 2012, Q. Yan et al. [145] reported hydrogen peroxide sensor based on SilNW

modified with nickel hydroxide. The SiNWs/ nickel hydroxide electrode was made out of a nickel hydroxide coating layer that was applied using an electroless plating approach along with chemically etched SiNWs. By using amperometry and cyclic voltammetry, the analytical capabilities of the SiNWs/nickel hydroxide electrode for hydrogen peroxide measurement were examined. $3.31 \text{ mA mM}^{-1} \text{ cm}^{-2}$ sensitivity and $3.2 \text{ }\mu\text{M}$ detection limit were reported in the fabricated SiNWs/ nickel hydroxide electrode based hydrogen peroxide sensor. In 2014, Y.M.Georgiev et al. [146] reported a highly precise junctionless SiNW biological and chemical sensing devices with a variety of shapes were made on SOI wafers using a top-down completely CMOS-compatible technique. Advanced PEC, high-resolution electron-beam lithography with the electron resist negative tone HSQ and RIE with Cl-chemistry, were used for the patterning of the devices. A very high level of patterning quality was achieved in produced structures with little roughness between 0.8 nm and 1.6 nm and little variation in the SiNW widths from the intended values. When the devices were electrically characterised, junctionless back gated nanowire transistors with large on-currents in the range of $1\text{ }\mu\text{A}$ to $10\text{ }\mu\text{A}$ depending on the high ratios between the on-state and off-state currents of six-seven orders of magnitude and drain potentials were reported. In the same year, P. Livi et al. [147] reported a chemical sensor system having a chip with an array of SiNW ion sensitive FETs and CMOS readout. Each of the NWs has been interfaced to the CMOS circuitry, which consists of eight sigma-delta modulators and eight current-frequency converters, so as to apply a steady voltage for computing the corresponding current across each NW. Because each NW has its own exclusive readout channel, there is no need for multiplexing, which helps to prevent leakage current problems. In the year 2018, X. Cao et al. [148] reported SiNW based fluorescent facile sensor for dithionite detection. The sensor was fabricated by concurrently immobilising dabsyl group (recognising and quencher group) and dansyl group (fluorescent molecule) on the surface of SiNW and SiNW arrays. High selectivity and a strong linear connection between dithionite concentrations and fluorescence intensities between 0.1 mM and 1 mM were also reported. In the year 2021, Seong-Kun Cho et al. [149] reported sodium ion sensor based on SiNW dual gate FET. Extended gate sodium selective membrane was used as sensing unit and SiNW dual gate structured FET was used as transducer. For the SiNW pattern transfer, using electrospun polyvinylpyrrolidone nanofibers as a template, the Si on insulator substrate was dry etched to create the SiNW channel dual gate FET. For NaCl solution, a sensitivity reading of 1464.66 mV/dec was recorded. The SiNW channel FET based sodium ion sensors outstanding selectivity was proved by the devices low sensitivities to buffer solutions including KCl, pH and CaCl_2 .

In the year 2022, K. Daoudi et al. [150] reported hierarchical Ag nano prism/GO/SiNW arrays as raman scattering surface-enhanced sensors for atrazine detection (Fig. 25). Silver aided chemical etching has been used to successfully fabricate vertically and homogenous aligned SiNWs. Additionally, silver nano prism/GO/SiNW arrays were constructed by drop-casting the silver nano prisms after GO was spin-coated. In order to improve the homogeneous deposition of silver nano prisms, graphene oxide layers have been added to NW bunches. After graphene oxide modification, SERS characteristics significantly improved, with a SERS efficiency of 3.2×10^8 . The sensor reported 2.0×10^{-12} limit of detection for Atrazine. Sensing performance of different SiNW based Chemical and Metal Ion sensors was given in Table 3 [140–153].

6 Silicon Nanowire Based Various Other Sensors

SiNW has grown as an ideal material for sensing in various technological applications like temperature sensing, humidity sensing, pressure and strain sensing etc. In the year 2011, X. Chen et al. [154] reported humidity sensor based on SiNW. The SiNWs were modified using a monolayer self-assembled hexamethyldisilazane. Due to the methyl termination of the generated hexamethyldisilazane monolayer, the SiNWs surface becomes hydrophobic after modification. With its hydrophobic property, the sensors performance was reported to get enhanced by successfully preventing water vapour adsorption, enhancing charge storage stability and lowering surface conductivity. Humidity sensing behaviour of SiNWs based humidity sensors without and with hexamethyldisilazane modification was investigated. The hexamethyldisilazane modified SiNWs based humidity sensor shown enhanced humidity detecting behaviour, such as hysteresis, reaction time and linearity, compared to the SiNWs based sensor, due to the hydrophobic feature of hexamethyldisilazane. In the year 2012, H.Y.Wang et al. [155] investigated the capacitive humidity sensing characteristics of Si carbide NW. On a nanoporous Si pillar array, a catalyst-assisted chemical vapour deposition process was used to generate a significant number of entangled Si carbide NW with 15 nm average diameter. By evaporating interdigital coplanar silver electrodes onto the surface of Si carbide NW/Si nanoporous pillar array, the capacitive humidity sensing capability at room temperature were investigated. At 100 Hz measurement frequency, a capacitance increase of nearly 960% was attained with a change in relative humidity from 11% to 95% (Fig. 26). At 75% relative humidity, the 4.5% maximum humidity hysteresis was measured and the response and recovery durations were recorded to be 105 seconds and 85 seconds respectively.

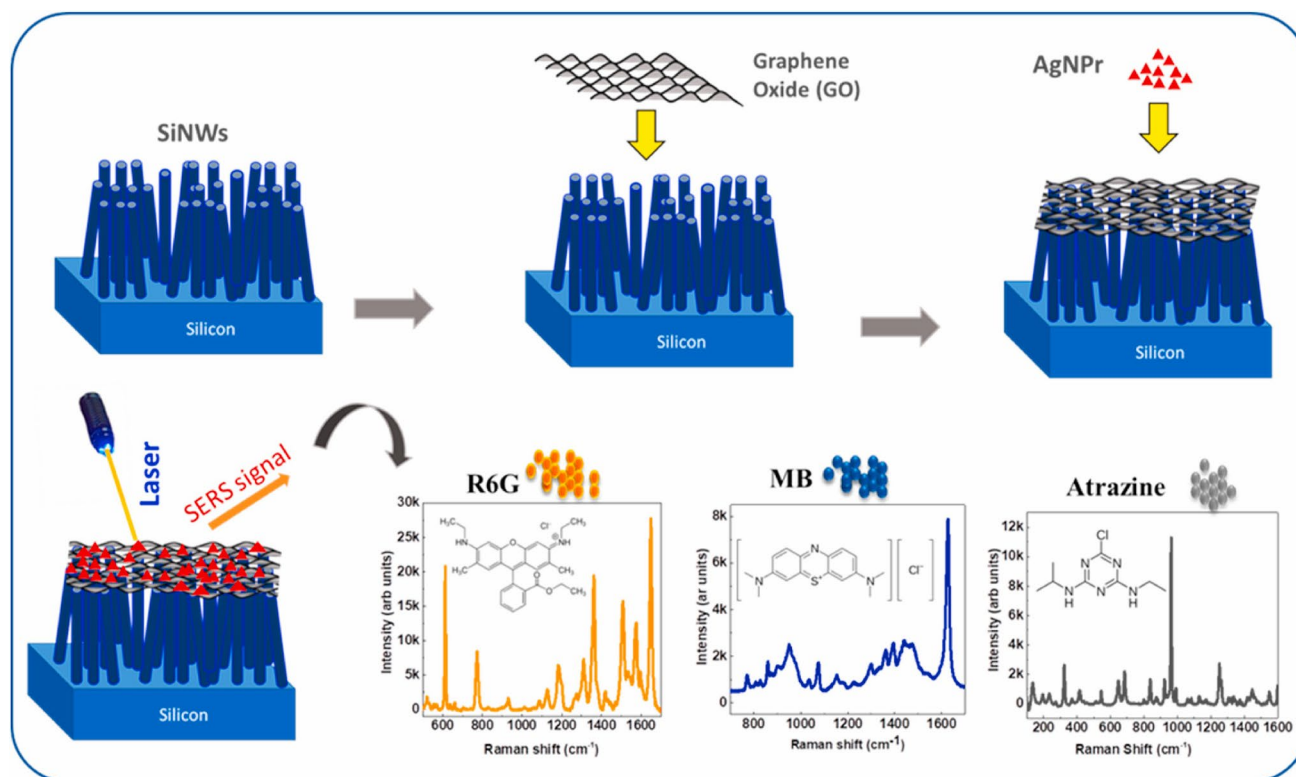


Fig. 25 Schematic representation of Ag nano prism/GO/SiLNW chemical sensor [150] (Copyright @ Elsevier)

Table 3 Sensing performance of different SiLNW based Chemical and Metal Ion sensors [140–153]

Ref	SiLNW sensor type	Target	Sensitivity	LoD	Range of Detection
[140]	Biotin-modified SiLNW	Streptavidin	-	10 pM	-
[141]	SiLNW modified with p-Tyr	Calcium ions	-	1.2 nM	100 nM to 1 mM
[142]	Tripeptide modified SiLNW FET	Copper ions	-	1 nM	-
[143]	Oligopeptide modified SiLNW arrays	Pb ²⁺	-	1nM	-
[143]	Oligopeptide modified SiLNW arrays	Cu ²⁺	-	10 nM	-
[144]	Silver nanoparticles decorated SiLNW	Hydrogen peroxide	57.5 $\mu\text{A mM}^{-1} \text{cm}^{-2}$	0.2 μM	0.2 mM – 20 mM
[145]	Nickel hydroxide modified SiLNW	Hydrogen peroxide	3.31 mA $\text{mM}^{-1} \text{cm}^{-2}$	-	-
[148]	Fluorescent SiLNW sensor	Dithionite	-	-	0.1 to 1 mM
[149]	SiLNW dual gate FET	Sodium ion	1464.66 mV/dec	-	-
[150]	Silver/GO/SiLNW array	Atrazine	-	$2.0 \times 10^{-12} \text{ M}$	-
[151]	MPTES functionalized SiLNW	Cd ²⁺	10^{-4} M	-	-
[151]	MPTES functionalized SiLNW	Hg ²⁺	10^{-7} M	-	-
[152]	SiLNW modified with R6G derivatives	Cu(II)	-	-	0.0 to 7.0 μM
[153]	SiLNW FET	Organophosphorus molecules	-	-	-

A high degree of measurement repeatability and long-term stability were also demonstrated for the humidity sensor. In the year 2013, H. Taghinejad et al. [156] reported humidity sensor based on doped SiLNW. Vapor-liquid-solid method was been used to fabricate SiLNWs. Doping of NWs resulted in a noticeable increase in the device sensitivity. In the year 2014, S. Zhang et al. [157] reported a SiLNW based novel

piezo-resistor pressure sensor with an annularly grooved diaphragm. The advantage of the groove structure, which makes the stress to be localised in the rib area and results in a higher resistance change, was observed by both measurement and FEM data. The device's sensitivity was boosted by 2.5 times in pressure ranges of zero to 120 mmHg compared to flat diaphragm pressure sensor. The sensor reported

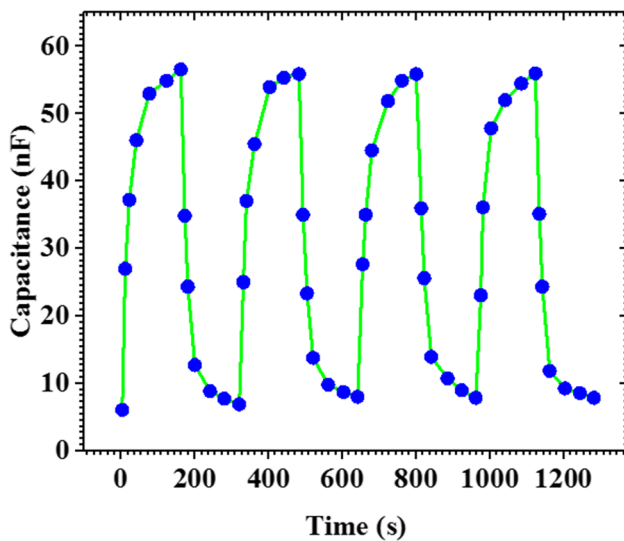


Fig. 26 Silicon carbide NW/Sil nanoporous pillar array time response curve by varying the ambient relative humidity between 11% & 95% at a frequency of 100 Hz [155]

a sensitivity of approximately 8.92×10^{-5} ($\Delta R/R$)/mmHg. In the year 2015, Z. Wang et al. [158] reported humidity sensor (capacitive) based on SiLNW arrays with ZnO nanorods grown on it. Chemical bath deposition and wet chemical etching, respectively, were used to fabricate SiLNWs with a length of about eight μm and zinc oxide nanorods with a length of about two hundred nm. When the relative humidity varies from 11.30% to 97.69%, the sensors maximum response range reported was 2.40 nF to 64.40 nF. The longest recovery and response time of seven seconds and twenty six seconds for 97.69% relative humidity was reported in the fabricated ZnO nanorods/SilNW humidity sensor along with a sensitivity of 0.69 nF/% RH. The sensors have 2.93% maximum relative standard deviation which corresponds to 11.30% relative humidity over the course of nearly a month at room temperature in air, demonstrating their long-term stability (Fig. 27).

In the year 2019, G. Chen et al. [159] reported highly self-assembling CMOS fabricated porphyrin-Sil hybrid NW transistor based photonic sensor. The selective assembly of a large number of porphyrin molecules to the surface of poly-SilNW was accomplished by carefully constructing the hydrophobic isolation structure in the device, which was confirmed by the AFM, SEM, and laser confocal fluorescence microscopy. Selective-assembling porphyrin-SilNW FET reported significantly greater photo-electronic detection sensitivity than classical devices, even at extremely low illumination power densities of $11.2 \mu\text{W}/\text{cm}^2$. In the year 2020, C. Kim et al. [160] reported a SiLNW based pressure sensor fabricated via metal assisted chemical etching process. In order to provide the sensor the necessary

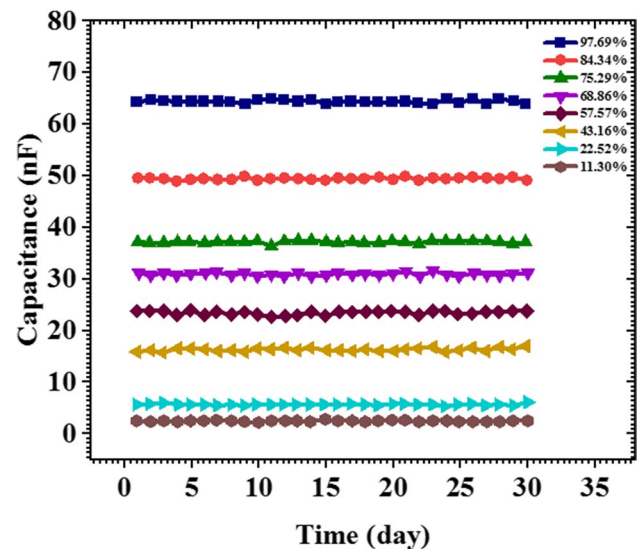


Fig. 27 Stability of ZnO nanorods/SilNW humidity sensor at room temperature for one month [158]

flexibility and high-pressure resistance, polydimethylsiloxane was applied to metal assisted chemical etched NWs, which had a height of 30 μm and a diameter as tiny as 200 nm. As the applied pressure changes from 0 - 4.5 kPa, the piezo-resistance SiLNW sensor reported a quick recovery and response time of 0.3 seconds, and it can differentiate pressure fluctuations as low as 0.3 kPa, which is far lower than the range that human skin can perceive (10 to 40 kPa). In the year 2021, J. Rhee et al. [161] reported SiLNW based optical under display proximity sensor. Due to its strong photo-responsivity, SiLNW can sense distance even when positioned underneath displays without using a significant amount of current for driver operation. Additionally, the read-out integrated circuit in the reported optical proximity sensor will eliminate the dark leakage current produced by SiLNWs. The read-out integrated circuit takes up 0.18 mm^2 of space and the proximity sensor is made using a $0.18 \mu\text{m}$ CMOS technology. The optical proximity sensor can identify an item that is closer than 40 mm in each of the three scenarios with vertical cavity surface emitting laser generating currents of 12 mA, 10 mA and 7 mA. In the year 2022, Y. Yang et al. [162] reported strain sensor fabricated via two-step technique, including water-induced swelling and silver NW deposition, to create stretchable sensors with hierarchical wrinkled architectures. Sodium chloride particles were introduced into the elastomer matrix as highly soluble additives. The elastomer substrate experienced substantial swelling after being soaked in dopamine aqueous solution. The swelling process that occurs along with the dopamine deposition gives the sample surface ultra-hydrophilicity. When exposed to external deformation ranging from 10% to 100% stresses, the sensor exhibited great sensitivity, strong

Table 4 Sensing performance and applications of various other SiNW based sensors [154–171]

Ref	SiNW sensor type	Application	Sensitivity	Response Time	Recovery Time
[154]	Hexamethyldisilazane modified SiNWs	Humidity sensing	-	-	-
[155]	SiC NW/silicon nanoporous pillar array	Humidity sensing	-	105 seconds	85 seconds
[156]	Doped SiNW	Humidity sensing	-	-	-
[157]	SiNW	Pressure sensing	$8.92 \times 10^{-5} (\Delta R/R)/\text{mmHg}$	-	-
[158]	ZnO nanorods/SiNWs	Humidity sensing	0.69 nF/% RH	26 seconds	7 seconds
[159]	Porphyrinoporin-SiNW FET	Photonic Sensor	-	-	-
[160]	SiNW array	Pressure sensing	-	0.3 seconds	0.3 seconds
[161]	SiNW	Proximity sensor	-	-	-
[162]	SiNW with hierarchical wrinkled structures	Strain sensor	-	-	-
[163]	NEMS piezoresistive SiNW	Pressure sensing	0.42% psi^{-1}	-	-
[164]	SiNW array	Humidity sensing	-	-	-
[165]	SiNW	Hydrogen ion sensing	-	-	-
[166]	SiNW based NEMS sensor	Pressure sensing	-	-	-
[167]	SiNW	Optical rectangular waveguide sensor	-	-	-
[168]	SiNW	RFID Humidity Tag Sensor	-	-	-
[169]	High Anisotropy SiNW	Photonic Sensor	-	-	-
[170]	SiNW	Environmental air quality monitoring	-	-	-
[171]	SiNW	Pressure sensing	8.2 kPa^{-1}	3 milliseconds	-

electrical repeatability over 8000 stretch/release cycles, and consistent electrical response at various stretch/release frequencies.

The recent advancements in SiNW devices enable rapid and sensitive analysis in different prospective applications. It is expected that these enhanced sensing devices would be commercially produced and widely employed in our daily lives. Other than for sensing applications, in the last decade, significant advancements had also happened in the use of SiNWs for thermoelectric, photovoltaic, photo electrochemical power generation, energy storage with LIB anodes, photo detection etc. Sensing performance and applications of various other SiNW based sensors was given in Table 4 [154–171].

7 Conclusion

The rapid rise and development of sophisticated nanotechnology has led to the fabrication of several sensing nano materials with specific features, desirable sizes, and chemical compositions. The development SiNW technology will be considered as a very useful augmentation to the present Sil technology. The exceptional physical and chemical capabilities of SiNWs made them a good alternative for a variety of uses that depends on their extraordinary physicochemical qualities. The distinctive properties of SiNW sensor, such as

biocompatibility, adjustable optical and electrical characteristics, and outstanding surface-to-volume ratio, make them a viable choice in the detection of various nucleic acids, viruses, chemicals, metal ions species and gases. However in order ensure the dependability of electrical and electrochemical SiNW sensors, the two broad manufacturing procedures of SiNWs must be developed more effectively. In the promising field of various sensing devices, Sil nanostructures will open way for more networked, smarter and portable platforms.

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Data availability Not applicable.

Declarations

Ethics Approval and Consent to Participate All procedures performed in studies were in accordance with the ethical standards of the institutional and/or national research committee and with the comparable ethical standards.

For this type of study, formal consent is not required.

Consent for Publication Authors give consent for the publication of the Submitted Research article in Silicon.

Competing interests The authors declare no competing interests.

Research Involving Human Participants and/or Animals Not Applicable.

Informed Consent Not Applicable.

Conflicts of Interest The authors declare that there is no conflict of interest reported in this paper.

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