



Synthesis and Characterization of Hollow Mesoporous Silica Spheres and Studying the Load and Release of Dexamethasone

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Abstract

Hollow mesoporous silica (HMS) spheres were synthesized using cetyltrimethylammonium bromide (CTAB) and carbon nanospheres as a hard template through a hydrothermal procedure. The prepared HMS was characterized by UV-Vis, FT-IR, TG, XRD, BET and SEM measurements. HMS was functionalized using aminopropyltriethoxysilane (APTES) and amino groups were linked on its surface. Synthesized mesoporous material consists of homogenous particles with a size about 500–600 nm. Channels on the shell have hexagonal arrangements. In comparison with MCM41 and SBA15, spherical HMS provides more volume for drug loading, for its hollow cores. Thereby, the ability of obtained mesoporous materials to load and release of dexamethasone as a drug was studied.

Keywords Hollow mesoporous silica (HMS) · Carbon nanospheres · Dexamethasone · Drug release

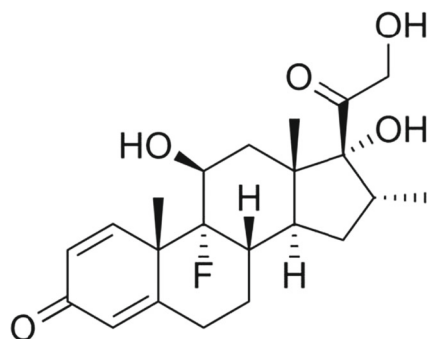
1 Introduction

Future nanotechnology hinges on the ability to synthesize new nanomaterials possessing distinct structural and functional features. Among them, hollow nanospheres possess “tunable” void volume, excellent flow performance, and large surface area [1]. Also, Hollow micro/nanostructural materials are a large family of functional materials and have attracted much research and industrial interest due to their special shape, low density, and large fraction of voids, large hollow cavities, intact shells, and uniform morphologies [2]. There have been reports about synthesis of silica hollow spheres by several methods such as sonochemical, solid particle templates, surfactant/vesicle templates, and emulsion templating technology. However, only several reports have occasionally involved the synthesis of hollow spheres with ordered porous wall structures. Moreover, their particles sizes are usually not uniform [3]. Previously, mesoporous hollow spheres have been synthesized by self-assembly of silica precursors with surfactant templates at oil–water, or

air–water droplet interfaces, or using the vesicle approach. As these soft templates generally represent low stability and poor uniformity in solution, the obtained hollow materials are often ill-defined in shape and poly-dispersed in size. Also, the hollow core size and shell thickness cannot be easily and independently controlled by these techniques. To overcome these problems, the hard templating methods have been used to fabricate mesoporous silica hollow spheres by using polymer or inorganic beads as sacrificial core templates [4]. During the past three decades, controllable drug release system which can deliver the therapeutic drugs to the targeted cells or tissues in a controlled manner and enhanced drug efficiency with reduced toxicity has attracted much attention. So far, a large variety of materials, such as biodegradable polymers, hydroxyapatite, calcium phosphate cement, hydrogels, and mesoporous silica have been employed in controlled drug release systems [5]. It has been speculated that HMS spheres are more suitable as drug carriers compared to the conventional mesoporous silica, because HMS spheres exhibit the similar drug release kinetics, but hollow cores provide more volume for drug loading. Therefore, many efforts have been made to develop drug release systems based on the HMS spheres as carriers [6]. Recently, there has been a growing interest in synthesizing HMS with penetrating channels from the wall surface to its hollow core, and its *in vitro* drug release performances have also been studied. Compared to conventional

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Scheme 1 Chemical structure of dexamethasone

solid porous materials, these hollow spheres show higher adsorption capacity for the drug molecules, which are also favorable for applications in confined nanocatalysts, biosensors, targeted drug and gene release, enzyme encapsulation, and nanoreactors [7].

In this work, we have prepared HMS spheres using CTAB and carbon nanospheres as a hard template to achieve spherical morphology. HMS was functionalized using aminopropyltriethoxysilane (APTES) and the load and release of dexamethasone drug (Scheme 1) on the product was studied.

2 Experimental Section

2.1 Materials and Reagents

Cetyltrimethylammonium bromide (CTAB), tetraethoxysilane (TEOS), 3-aminopropyltriethoxysilane (APTES),

ammonium hydroxide (28.0–30.0%), ethanol, hydrochloric acid, nitric acid, glucose monohydrate, acetone and acetonitrile were purchased from Merck. All materials were used as obtained without further purification.

2.1.1 Preparation of Carbon Nanospheres by Hydrothermal Method

Glucose monohydrate (4.752 g) was dissolved in distilled water (60 mL) and stirred by magnetic stirrer. Then, it was placed in an autoclave for 12 h at 180 °C. After a while, a two-phase solution was formed that was brown in color. In order to separate the unreacted monomers and solvent, sample was centrifuged for 15 minutes at a speed of 6000 rpm. Then, ethanol was added to it and placed in an ultrasonic bath for 20 minutes. This cycle is called centrifuge-ultrasonic-washing and the cycle was repeated ten times using double distilled water and ethanol. After that, obtained mixture was placed in a 70 °C oven.

2.1.2 Synthesis of SiO₂ Hollow Nanospheres with the Carbon Core

At First, carbon template (100 mg) and cetyltrimethylammonium bromide (CTAB) (170 mg) were added to distilled water (30 mL) and dispersed for 30 minutes in an ultrasonic bath. Then, ethanol (13 mL) and ammonia (28 wt%, 0.45 mL) were added and redispersed for 30 minutes. After that, tetraethylorthosilicate (TEOS) (0.3 mL) was added dropwise and resulted solution dispersed for 2 h. It was filtered by centrifuge and washed six times using ethanol and double

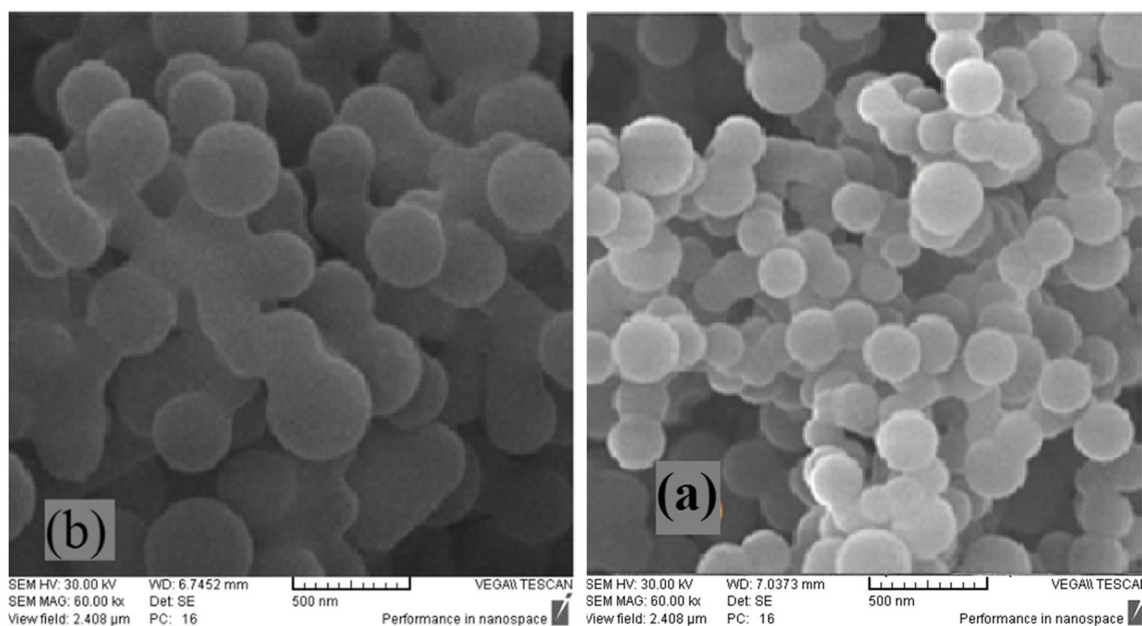


Fig. 1 SEM images of carbon nanospheres obtained from glucose **a** 0.4 M and **b** 0.6 M

distilled water. The pH of solution was 7 by washing. In order to remove the solvent, the final product was placed in an oven at 80 °C. Finally, for calcination and removal of the carbon core, the obtained precipitate was placed in a furnace at 500 °C with the rate of 2 °C/min.

2.1.3 Preparation of SiO₂ Nanoparticle Modified with Aminopropyltriethoxysilane (APTES)

Aminopropyltriethoxysilane (1mL) was transferred to a flask (50 mL) containing toluene (30 mL) and equipped to refrigerant. Then, SiO₂ hollow nanospheres (1 g) were added to balloon and the mixture refluxed under nitrogen

atmosphere for 24 h. After completion of the reaction, the product is separated by centrifuge and washed with methanol. Finally, the product was placed in a 100 °C oven.

2.1.4 Preparation of Simulated body Fluid (SBF)

At first, the container including double distilled water (960 mL) and sodium chloride (6.5456 g) was stirred for 3 minutes at room temperature. Then, Sodium bicarbonate (2.2682 g), potassium chloride (0.3730 g) and disodium phosphate (0.1419 g) were added to it and stirred for 3 minutes. The solution was heated at 37 °C. After that, magnesium chloride hexahydrate (0.3049 g) was added

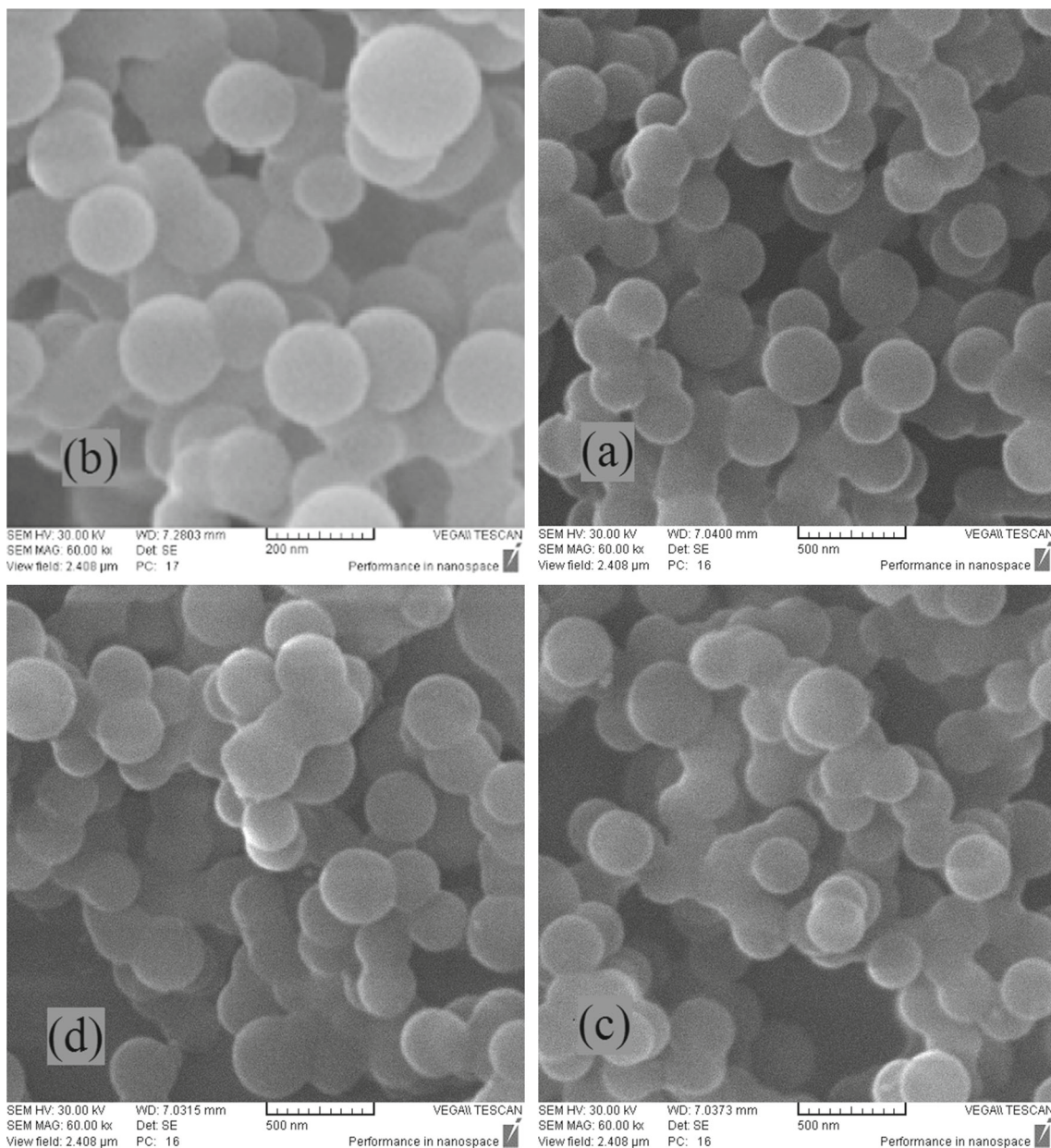


Fig. 2 SEM images of carbon nanospheres (0.4 M) in the times **a** 8, **b** 12, **c** 14 and **d** 16 h

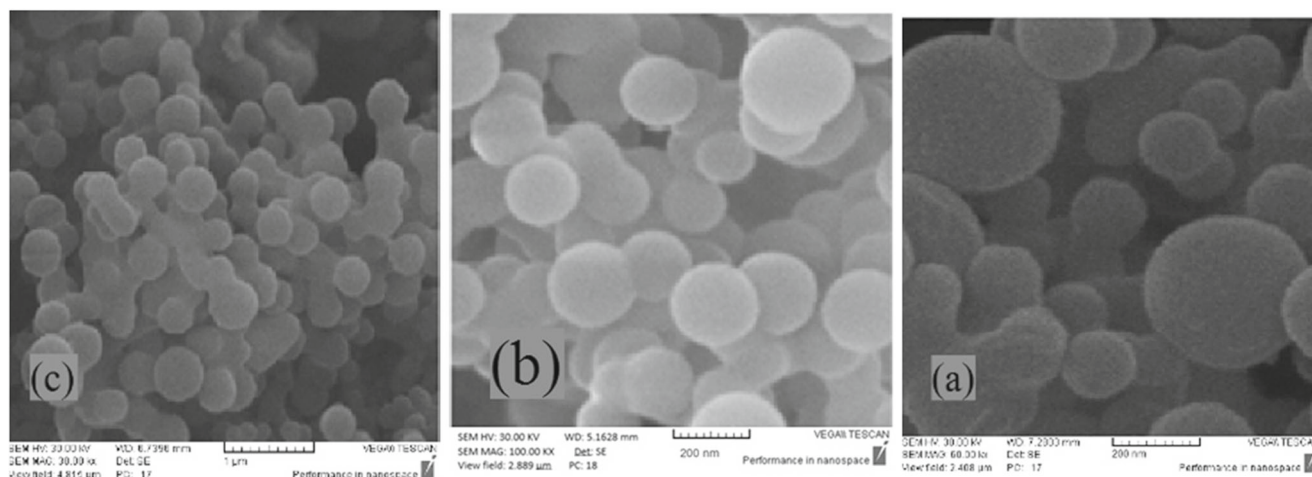


Fig. 3 SEM images of carbon nanospheres at temperatures: **a** 150, **b** 180 and **c** 210°C

to it and the solution was stirred for 3 minutes. Then hydrochloric acid (9 mL, 1 M) was added drop wise and again stirred for 3 minutes. Calcium chloride (0.3675 g) and sodium sulfate (0.071 g) were added and stirred for 3 minutes. Finally, trishydroxymethylaminomethane (6.057 g) was added to the solution and immediately the solution became dull. On stirring at 37 °C, the pH of solution reached to 7.4 by adding hydrochloric acid (30 mL, 1 M). Finally, the color of solution turned transparent and the resulting solution (SBF) was kept in a refrigerator at 4 °C [8].

2.1.5 Absorption of Drug by Hollow and Porous Nanospheres

The drug used in this research was dexamethasone and its structure was given in Scheme 1. At first, the solution of drug (250 ppm) was prepared and poured in the two separate containers. To one of them was added SiO₂ nanoparticles and to another SiO₂ nanoparticles modified with aminopropyltriethoxysilane was added and the mixture stirred. In order to evaluate the absorption of the drug, every

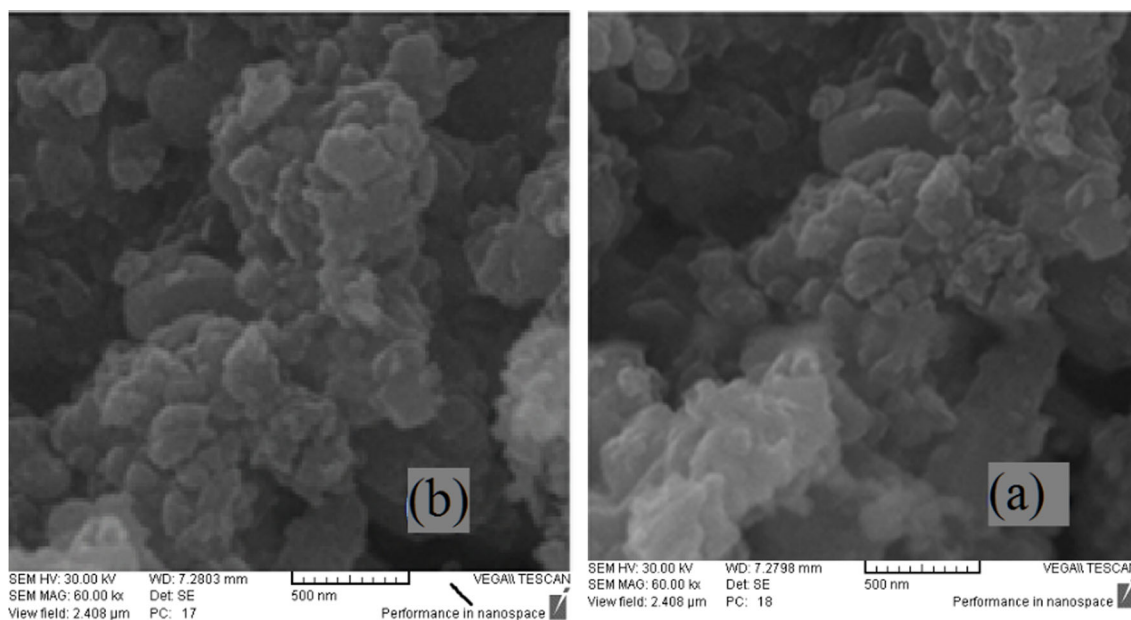


Fig. 4 SEM images after calcination of C@SiO₂ at **a** 650 and **b** 600 °C

6 hours, the mixture of drugs and nanospheres were sampled for 10 min and centrifuged at 14,000 rpm.

2.1.6 Drug Release from Nanospheres Loaded in Simulated Body Fluid

In this study, the drug was allowed to place in the vicinity of nanospheres for 72 hours. Then, using centrifuge, nanospheres were separated from the drug solution. After separating the hollow nanospheres, to obtain the loaded drug, was taken UV-Vis absorption spectrum from the remaining solution of the drug. Then, the loaded nanospheres were washed using deionized water and the final product dried in a vacuum oven for 4 h at 50 °C. After that, obtained nanospheres was poured in SBF (100 mL) and at the onset of drug release, sampled at 30 minutes, 1, 2, 5, 8 and 24 h, respectively. After centrifuging the samples, UV-Vis absorption spectra were measured in the range 190 to 800 nm.

2.2 Instrumentation

Powder X-ray diffraction (PXRD) patterns were measured on a JEOL diffractometer with monochromatized Cu K α radiation ($\lambda = 1.5418 \text{ \AA}$) [9]. Thermogravimetric analysis (TGA) was carried out with a STA-409 PC Luxx. The N₂ adsorption/desorption isotherms were acquired at liquid nitrogen temperature (77 K) using a Belsorp mini II instrument, and the specific surface area was calculated by the Brunauer- Emmett-Teller (BET) method. The pore size distribution was determined using the Barret-Joner-Halenda (BJH) method [10]. The UV-Vis absorption spectra

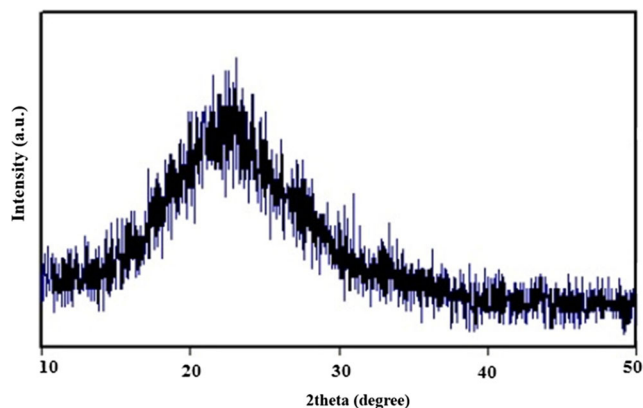


Fig. 6 XRD pattern of SiO₂ nanospheres

were acquired using a Shimadzu, mini 1240 single beam. Scanning electron microscopy (SEM) images were obtained on a LEO-1455 VP with gold coating. Fourier transform infrared (FT-IR) spectra were recorded on a Shimadzu-8400S spectrometer in the range of 450–4000 cm⁻¹ using KBr pellets [11].

3 Results and Discussion

3.1 SEM Images of Carbon Nanospheres

The effect of parameters such as concentration, time and temperature on the morphology and size of the nanospheres and also uniform size distribution of the nanospheres were examined. The claim can be proved with SEM images obtained from different samples.

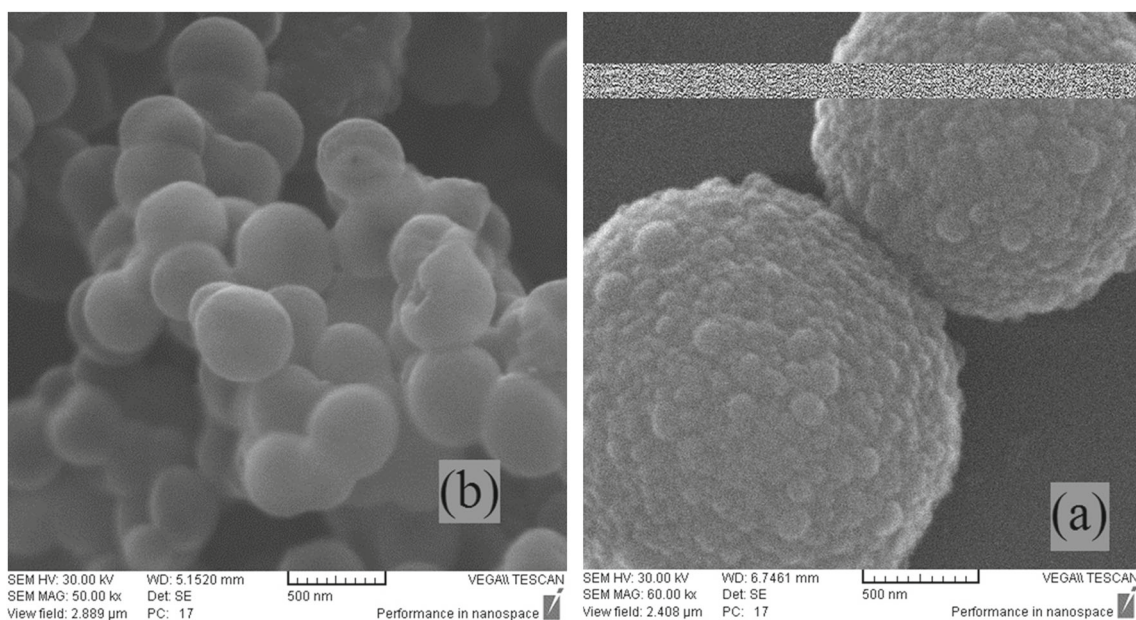
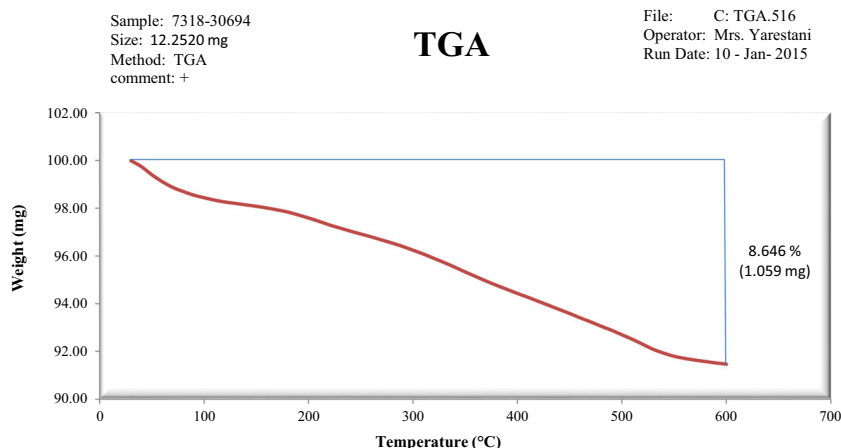


Fig. 5 SEM images of C@SiO₂ a before and b after calcination

Fig. 7 TG curve of C@SiO₂@APTES



3.1.1 Effect of Concentration

SEM images of Fig. 1a and b are related to two samples with the same synthesis procedure and only different in glucose concentration. It was found that for uniform carbon spheres, the optimal concentration of glucose monohydrate solution is 0.4 M, because nanospheres obtained at higher concentrations are agglomerated. SEM images in Fig. 1 show that samples at glucose concentration of 0.4 M contain carbon nanospheres more uniform and separated, but in 0.6 M glucose, nanospheres are agglomerated and become unsuitable templates for producing hollow nanospheres.

3.1.2 Effect of Time

SEM images in Fig. 2a–d are related to the four samples with the same synthesis procedures, differing only in reaction time. The time parameter is also an important factor in the synthesis of carbon nanospheres, because it is a polymerization reaction, and if the time is insufficient, a major part of it was converted to unreactive monomers or led to very small and non-uniform distributed nanospheres. To obtain the separated carbon nanospheres, the optimal time is 12 h. If the time increases, agglomeration occurs and if the

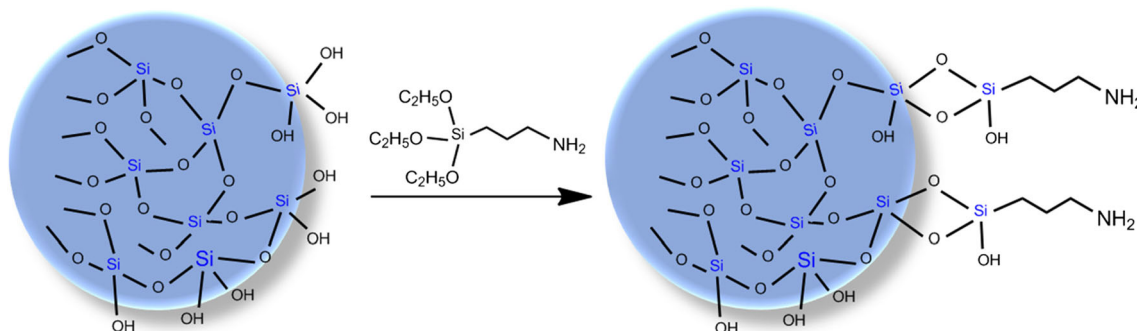
time decreases, the growth of nanospheres is not completed and some of glucose particles remains non-spherical.

3.1.3 Effect of Temperature

SEM images in Fig. 3a–c are attributed to three samples prepared in different temperatures, 150, 180 and 210 °C. The best temperature for synthesis of these nanospheres was estimated 180 °C. Because at higher temperatures, the samples were agglomerated samples and at lower temperatures, complete reaction does not take place.

3.2 FT-IR Spectrum of Carbon Nanospheres

FT-IR spectroscopy was used to confirm the chemical bonds. According to Fig. S1 of ESI, it can be noted that in different times and temperatures of hydrothermal reaction, significant changes were not created in surface functional groups of carbon nanospheres. The more the time of reaction, the smaller the peak intensity in the region of 3400 cm⁻¹, representing a loss of more water [12]. Figure S1 shows the FT-IR spectrum of carbon nanospheres. The observed bands at 1620 and 1695 cm⁻¹ are related to C=C and C=O stretching vibrations, respectively. The bonds are



Scheme 2 Functionalization of SiO₂ spheres by APTES

created as a result of glucose aromatization process during hydrothermal reaction have been created. The decrease of frequency may be caused by the hydrogen bonding between the hydroxyl group and oxygen of carbonyl groups. The peaks at $1000\text{--}1400\text{ cm}^{-1}$ are attributed to stretching vibrations of C–OH and bending of OH, respectively, of course the broad peak in the range of 3400 cm^{-1} confirms that there are hydroxyl groups covalently bonded to the surface of spheres.

3.3 SEM Images of Core/Shell Nanostructures

SEM images in Fig. 4a and b are related to calcination of C@SiO₂ at 650 and 600 °C. To remove carbon spheres and organic parts from SiO₂, the optimum temperature were determined 500 °C. The SEM images of C@SiO₂ before and after calcination are illustrated in Fig. 5a and b. It seems that good nanospheres obtained at this temperature and they are suitable for drug release. At temperature less than 500 °C, the pores of sample are not suitable for the absorption of the drug. Above 500 °C, nanospheres are broken and converted into nanoparticles.

3.4 FT-IR Spectrum of Nanospheres Core/Shell

3.4.1 C@SiO₂ before Calcination

The FT-IR spectrum of C@SiO₂ before calcination is given in Fig. S2 of ESI. The observed bands at 462 and 1099 cm^{-1} are related to Si–O bending and Si–O stretching vibrations respectively, which represents the synthesis of SiO₂. Due to strong interaction of carbonyl group with silicon, carbonyl bond has converted to a single bond, and creates an additional peak in the range of 1100 cm^{-1} , which belongs to C–O stretching frequencies. Also, the peak intensity was reduced in the range of 1600 cm^{-1} [13].

3.4.2 C@SiO₂ after Calcination

Figure S3 of ESI shows the FT-IR spectrum of C@SiO₂ after calcination. The observed bands at 462 and 1099 cm^{-1} correspond to Si–O bending and Si–O stretching vibrations, respectively and represent removal of organic parts from SiO₂ [14].

3.4.3 FT-IR Spectrum of APTES

In Fig. S4 of ESI, the observed bands at 2935 cm^{-1} is attributed to C–H stretching vibrations of CH₂ group of propyl chain and represents attaching of aminopropyltriethoxysilane on the surface. The observed band in the range of $1020\text{--}1220\text{ cm}^{-1}$ is related to C–N stretching vibrations

Table 1 BET measurements for SiO₂

Nanoporous specific area	916.82 m ² /g
Pore size	3.72 nm
Absorption desorption diagram	mesopore type 4

which covered by a broad peak related to the asymmetric stretching vibration of Si–O–Si group [15].

3.5 Powder X-ray Diffraction Patterns of SiO₂

Figure 6 shows the X-ray diffraction pattern of SiO₂ nanoparticles. There is a broad peak at $2\theta = 23^\circ$, which is characteristic for amorphous SiO₂ [16].

3.6 Thermal Analysis of C@SiO₂@APTES

The TG curve of C@SiO₂@APTES is shown in Fig. 7. In the TG curves, there are three weight losses. The initial weight loss observed up to 30–190 °C is attributed to physically adsorbed water molecules [17, 18]. The next weight loss occurred at 190–350 °C which was related to surface groups of OH or in the other words, chemically adsorbed water molecules [19]. The latest weight loss observed up to 350–600 °C is attributed to propyl chain [20]. Formation of SiO₂ nanoparticles modified with aminopropyltriethoxysilane are illustrated in Scheme 2.

3.7 Textural Properties of SiO₂ Nanospheres

The textural properties such as surface area and pore volume of SiO₂ nanospheres are given in Table 1. According to the

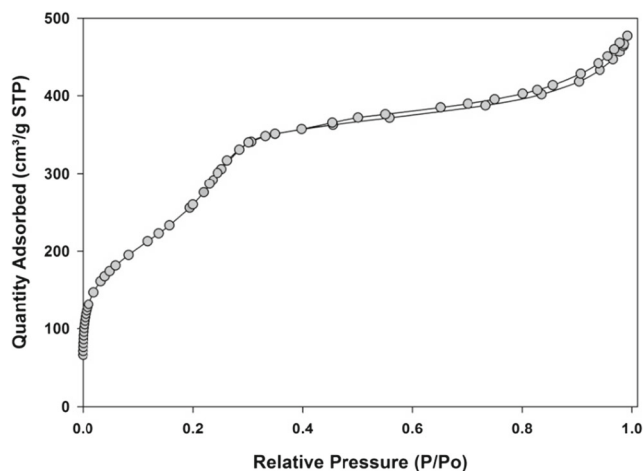
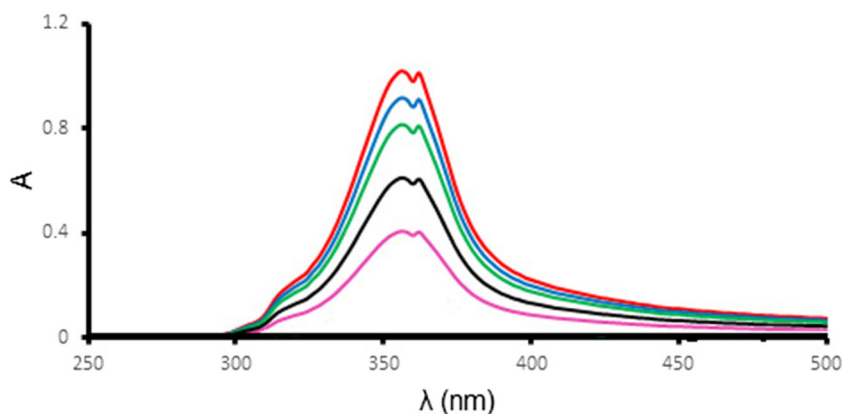


Fig. 8 N₂ adsorption/desorption isotherms of SiO₂ nanospheres

Fig. 9 UV-Vis absorption spectrum of solution of dexamethasone (250 ppm) and SiO₂ nanospheres: 0 (the bottom curve), 1, 2, 6 and 12h (top curve) after start of tests



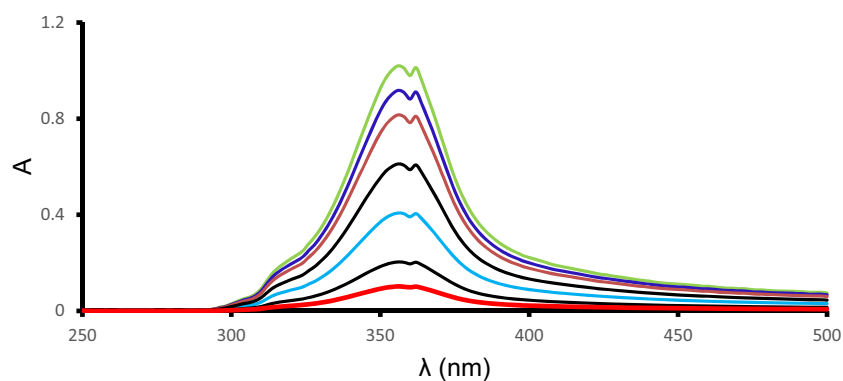
results of BET measurements, it was found that synthesized SiO₂ containing porous structure of the mesoporous type. The specific surface area of SiO₂ nanospheres is 916.82 nm and the pore size is 3.72 nm, so it is desirable for the drug release [21]. The nitrogen adsorption–desorption isotherms obtained at 77 K are shown in Fig. 8. The isotherms obtained for the porous nanospheres are of Type IV, which is the characteristic feature of the mesoporous materials [9].

3.8 Drug Load and Release

3.8.1 Absorption of Drug by SiO₂ Nanospheres

To study the amount of drug absorbed by nanospheres and drug release in the simulated body fluid was applied UV-Vis absorption spectrum. By comparing the peak intensity of drug, efficiency of nanospheres in the drug absorption and release can be obtained. Figure 9 is related to UV-Vis absorption spectrum of dexamethasone solution (250 ppm) in the presence of SiO₂ nanospheres (0.01 g). Over time, the amount of drug absorption by nanospheres is increased. It should be noted that in this test, pH was 6 and is not used no acidic or alkaline agent to alter and control of pH. Molecular structure of dexamethasone is brought in Scheme 1. The $\pi \rightarrow \pi^*$ and $n \rightarrow \pi^*$ was the most likely transition.

Fig. 10 UV-Vis absorption spectrum of solution of drug (250 ppm) and SiO₂ nanospheres modified with aminopropyltriethoxysilane 0 (the bottom curve), 1, 2, 6, 12, 24 and 48h (the top curve) after starting the tests



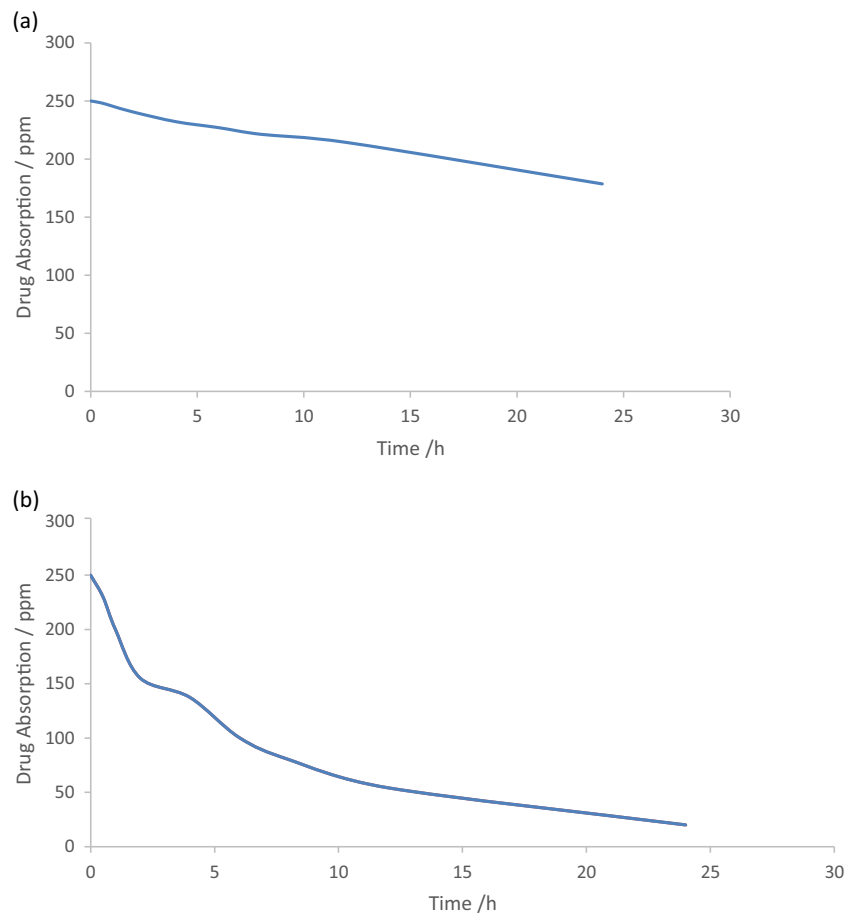
3.9 Absorption of Drug by SiO₂ Nanospheres Modified with Aminopropyltriethoxysilane

Absorption spectrum of SiO₂ nanospheres modified with aminopropyltriethoxysilane is similar to the spectrum of SiO₂ nanospheres, only the difference is that the amount of drug absorbed by SiO₂ nanospheres modified with aminopropyltriethoxysilane is more than SiO₂ nanospheres. Figure 10 shows UV-Vis absorption spectrum of solution of drug (250 ppm) and SiO₂ nanospheres modified with aminopropyltriethoxysilane. Figure 11a and b show the amount of drug absorbed by SiO₂ nanospheres and SiO₂ nanospheres modified with aminopropyltriethoxysilane.

3.10 Study of Drug Release in SBF

In order to study the drug release absorbed by SiO₂ nanospheres modified with aminopropyltriethoxysilane and SiO₂ nanospheres were used the simulated body fluid. The solution containing 250 ppm of dexamethasone drug (50 mL) and porous nanospheres (0.01 g) were stirred for 72 h. After separation of nanospheres by centrifuge and washing with acetone, final product dried in a vacuum oven at 40 °C for 3 h. Obtained nanospheres were poured in SBF (100 mL) and placed at 37 °C. The amount of

Fig. 11 Graph of the amount of drug absorbed by **a** SiO₂ nanospheres **b** SiO₂ nanospheres modified with aminopropyltriethoxysilane vs. time



drug release from nanospheres into simulated body fluid was sampled at different times. After separation of the loaded nanospheres using centrifugation for 20 minutes at 6000 rpm, UV-Vis absorption spectra of the loaded drug from the remaining solution were measured in the range 250 to 500 nm. UV-Vis absorption spectra related to the release of dexamethasone from SiO₂ nanospheres modified

with aminopropyltriethoxysilane and SiO₂ nanospheres at different times are illustrated in Fig. 12. As seen in the figure, an increase in the intensity of absorption is related to increased concentrations of dexamethasone in simulated body fluid. It is noteworthy that no difference in the peak related to UV-Vis molecular absorption spectra of drug release from SiO₂ nanospheres modified with

Fig. 12 UV-Vis absorption spectra of dexamethasone release from SiO₂ nanospheres modified with aminopropyltriethoxysilane: 0 (the bottom curve) 1, 2, 6, 12, 24, 48 and 72 h (the top curve) after starting

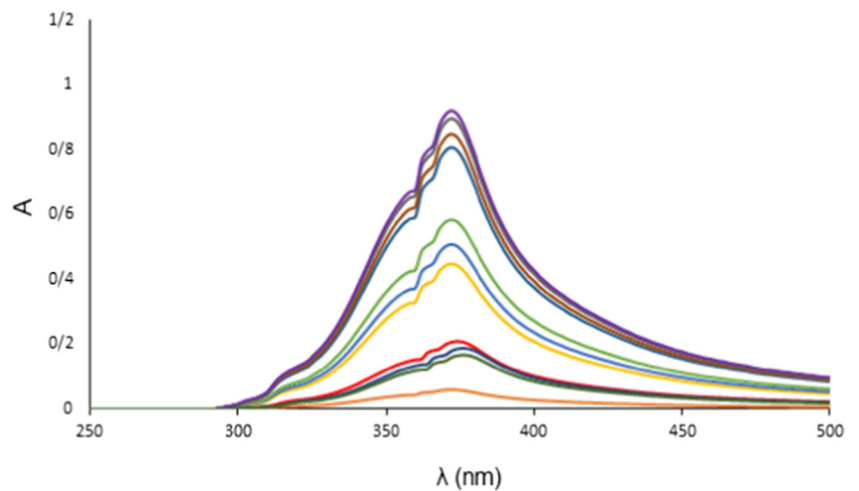
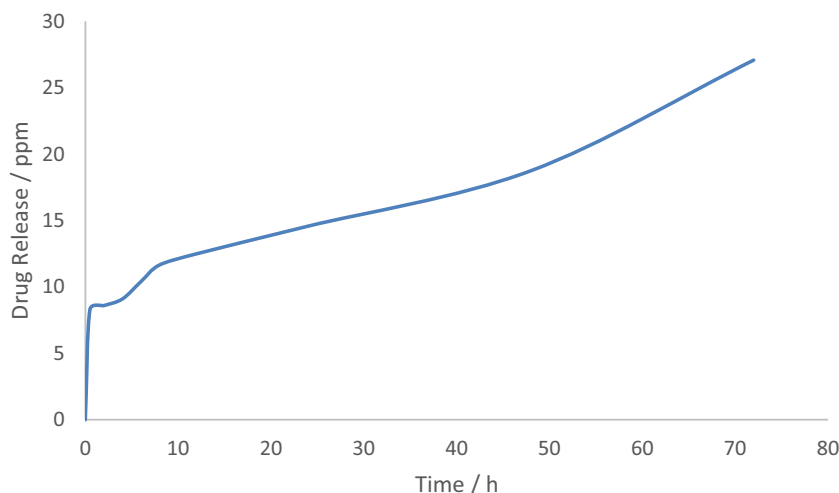


Fig. 13 Graph of the release of dexamethasone drug from SiO₂ nanospheres modified with aminopropyltriethoxysilane in SBF versus time



aminopropyltriethoxysilane and SiO₂ nanospheres were not observed. Figure 13 shows the amount of drug release from nanospheres in SBF and also drug release lasted for 72 hours.

4 Conclusions

In this work, hollow mesoporous silica (HMS) spheres were synthesized using glucose as a carbon precursor and CTAB. The SiO₂ nanoparticles were functionalized using aminopropyltriethoxysilane. Obtained mesoporous material was studied for the load and release of a drug. The amount of drug adsorption was increased with functionalizing of SiO₂ nanospheres and drug release lasted for 72 hours. Synthesized carriers do not need to adjust pH for absorption and release of the drug and this is considered as an advantage.

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