ORIGINAL ARTICLE



¹⁸F-FPYBF-2, a new F-18 labelled amyloid imaging PET tracer: biodistribution and radiation dosimetry assessment of first-in-man ¹⁸F-FPYBF-2 PET imaging

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Abstract

Objective Recently, a benzofuran derivative for the imaging of β -amyloid plaques, 5-(5-(2-(2-(2-18F-fluoroethoxy)ethoxy)) ethoxy) benzofuran-2-yl)- *N*-methylpyridin-2-amine (¹⁸F-FPYBF-2) has been validated as a tracer for amyloid imaging and it was found that ¹⁸F-FPYBF-2 PET/CT is a useful and reliable diagnostic tool for the evaluation of AD (Higashi et al. Ann Nucl Med, https://doi.org/10.1007/s12149-018-1236-1, 2018). The aim of this study was to assess the biodistribution and radiation dosimetry of diagnostic dosages of ¹⁸F-FPYBF-2 in normal healthy volunteers as a first-in-man study.

Methods Four normal healthy volunteers (male: 3, female: 1; mean age: 40 ± 17 ; age range 25–56) were included and underwent ¹⁸F-FPYBF-2 PET/CT study for the evaluation of radiation exposure and pharmacokinetics. A 10-min dynamic PET/ CT scan of the body (chest and abdomen) was performed at 0–10 min and a 15-min whole-body static scan was performed six times after the injection of ¹⁸F-FPYBF-2. After reconstructing PET and CT image data, individual organ time–activity curves were estimated by fitting volume of interest data from the dynamic scan and whole-body scans. The OLINDA/EXM version 2.0 software was used to determine the whole-body effective doses.

Results Dynamic PET imaging demonstrated that the hepatobiliary and renal systems were the principal pathways of clearance of ¹⁸F-FPYBF-2. High uptake in the liver and the gall bladder, the stomach, and the kidneys were demonstrated, followed by the intestines and the urinary bladder. The ED for the adult dosimetric model was estimated to be $8.48 \pm 1.25 \,\mu$ Sv/MBq. The higher absorbed doses were estimated for the liver (28.98 ± 12.49 and $36.21 \pm 15.64 \,\mu$ Gy/MBq), the brain (20.93 ± 4.56 and $23.05 \pm 5.03 \mu$ Gy/MBq), the osteogenic cells (9.67 ± 1.67 and $10.29 \pm 1.70 \,\mu$ Gy/MBq), the small intestines (9.12 ± 2.61 and $11.12 \pm 3.15 \,\mu$ Gy/MBq), and the kidneys (7.81 ± 2.62 and $8.71 \pm 2.90 \,\mu$ Gy/MBq) for male and female, respectively. **Conclusions** The ED for the adult dosimetric model was similar to those of other agents used for amyloid PET imaging. The diagnostic dosage of 185–370 MBq of ¹⁸F-FPYBF-2 was considered to be acceptable for administration in patients as a diagnostic tool for the evaluation of AD.

Keywords Alzheimer disease · Amyloid imaging · Normal healthy volunteers · Positron emission tomography · Biodistributtion · Radiation dosimetry · OLINDA/EXM

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Introduction

For diagnosing Alzheimer's disease (AD) which is the most common neurodegenerative disorder and the most common cause of dementia in the elderly with steadily increasing numbers [1], the ability to detect deposition of amyloid beta (A β) protein is an area of active research in molecular imaging. Developing imaging probes to evaluate amyloid deposition is an ongoing pursuit that could be helpful in the diagnosis of AD. Several imaging tracers, especially for positron emission tomography (PET), has been developed and reported to evaluate amyloid deposition, such as ¹¹C-Pittsburgh compound B (PiB) [2], ¹¹C-BF227 [3], ¹⁸F-AZD4694 [4], ¹⁸F-FACT [5], ¹⁸F-BAY-949172 (¹⁸F-florbetaben) [6], ¹⁸F-AV-45 (¹⁸F-florbetapir) [7], and ¹⁸F-GE067 (¹⁸F-Flutemetamol) [8]. PiB, the first amyloid imaging PET tracer, has been reported with successful results and used widely as a research tool [9].

Recently, we developed a benzofuran derivative for the imaging of A β protein, 5-(5-(2-(2-(2-¹⁸F-fluoroethoxy)ethoxy)benzofuran-2-yl)- *N*-methylpyridin-2-amine (¹⁸F-FPYBF-2) [10, 11]. This new fluorinated benzofuran derivative, which is like ¹⁸F-AZD4694 but has a fluoropolyethylene glycol side chain, is promising PET probes for cerebral A β plaques imaging, and the specific labeling of A β plaques was observed in autoradiographic sections of autopsied AD brain. It should be noted that ¹⁸F-FPYBF-2 has a stable chemical structure which does not photodegrade. ¹⁸F-FPYBF-2 is a ¹⁸F-labeled analog, which has the much longer half-life of ¹⁸F (*t*1/2 = 110 min), should offer a more manageable manufacturing and delivery process for clinical practice, as compared to ¹¹C labeled tracers.

In a clinical setting using healthy volunteers and patients with dementia, ¹⁸F-FPYBF-2 has been already validated as a tracer for amyloid imaging and it was found that ¹⁸F-FPYBF-2 PET/CT is a useful and reliable diagnostic tool for the evaluation of AD [12]. However, evaluation regarding biodistribution of ¹⁸F-FPYBF-2 and radiation dosimetry of ¹⁸F-FPYBF-2 PET imaging were not assessed and reported to the full.

Therefore, to facilitate clinical application of ¹⁸F-FPYBF-2 PET/CT, we have conducted studies aimed at assessing the biodistribution and radiation dosimetry of diagnostic dosages of ¹⁸F-FPYBF-2 in normal healthy volunteers as a first-in-man study.

Materials and methods

Automated radiosynthesis and preparation of ¹⁸F-FPYBF-2

¹⁸F-FPYBF-2 was prepared in-house as described before [12]. Briefly, the ¹⁸F-fluoride was produced with a cyclotron, CYPRIS HM18 (Sumitomo Heavy Industries (SHI), Ltd., Japan) by the ¹⁸O(p, n)¹⁸F reaction on 98% enriched ¹⁸O water. The radiosynthesis of ¹⁸F-FPYBF-2 was performed using a modification of the methods described by Ono et al. [10] and on a hybrid synthesizer, cassette-type multipurpose automatic synthesizer module (JFE Engineering Corporation, Japan).

Normal healthy volunteers

From March 2013 to October 2017, normal healthy volunteers were recruited for this dynamic PET study and finally 4 normal healthy volunteers (male: 3, female: 1; mean age: 40 ± 17 ; age range 25–56) (Table 1) were included and underwent ¹⁸F-FPYBF-2 PET/CT study for the evaluation of radiation exposure and pharmacokinetics. Eligibility criteria for healthy volunteers (20 years old or older) in the present study were follows; 1) who did not give any subjective complaint about cognitive problem, and (2.1) who made a declaration of their healthy status without medication, or (2.2) who had underlying non-neurological illness, such as hypertension, diabetes, hyperlipidemia, but controlled them well by medication as an out-patient based medical practice. Exclusion criteria were follows; (1) who had a subjective complaint or objective symptom of cognitive problem, (2) who were treated with or had past history of neurological disorder and related diseases, (3) who were treated with or had past history of brain or head injury. Each volunteer gave a written informed consent form defined by our institutional review boards with the information about the expected radiation exposure. The tracer study for normal healthy volunteers was approved by our institutional review boards, the Human Study Committee (approved on Mar. 28, 2013) and the Committee for the Clinical Use of Short-Half Life Radioactive Materials (approved on Mar. 1, 2013), where our protocol was investigated according to the results of animal studies of safety performed in 2012 as an extended single intravenous dose toxicity study, which was based on the protocol of Guidance for the Performing of Microdose Clinical Trials announced by the Ministry of Health, Labour and Welware of Japan.

PET/CT data acquisition

In first-in-man volunteer study for newly developed ¹⁸F-FPYBF-2, all normal healthy volunteers underwent ¹⁸F-FPYBF-2 PET/CT. PET/CT scans were performed by a whole-body PET/CT scanner, Siemens True Point Biograph 16 (pixel size: 1.34 mm) (Siemens/CTI, Erlangen,

 Table 1
 Profile of normal healthy volunteers and injected radioactivity of ¹⁸F-FPYBF-2

Subjects	Gender	Age	Injected dose (MBq)
#1 (TTT)	Male	53	199
#2 (AAA)	Male	26	236
#3 (KKK)	Male	25	220
#4 (HHH)	Female	56	199
Mean \pm SD		40 ± 17	213 ± 18

Germany) after the intravenous injection of ¹⁸F-FPYBF-2 (213 \pm 18 MBq). A 10-minutes dynamic PET/CT scan of the body (chest and abdomen) was performed at 0–10 min and a 15-minutes whole-body static scan was performed six times; 15–30, 30–45, 45–60, 60–75, 75–90 and 90–105 min, after the injection of ¹⁸F-FPYBF-2. For the image data processing in PET/CT scanner, the trans-axial effective field of view of the scanner was 342 mm in diameter, and the matrix size was 256 × 256. All acquisition data were reconstructed by 2 iterations and 21 subsets by the PET/CT scanner, using the three-dimensional ordered subset expectation maximization, OS-EM. The CT data were used for attenuation correction.

Imaging analysis

Regional dynamic and whole-body reconstructed PET and CT data were stored in the DICOM file format and were analyzed using PMOD software version 3.3 (PMOD Technologies Ltd., Zurich, Switzerland). Three-dimensional volumes of interest (VOIs) of individual source organs were constructed on the PET images to include all organ activity. The following source organs, the heart, aorta (blood), lung, liver, gallbladder, kidneys, pancreas, spleen, vertebral bone, muscle, small intestine, large intestine were analyzed for dynamic images. For the whole-body image analysis, the brain and salivary glands, urinary bladder, and whole body in addition to the above organ were analyzed. VOIs were manually drawn and corrected around the tissues referring CT images and mean activity concentration was expressed as Bq/cm³. Tissue distribution in organs of ¹⁸F-FPYBF-2 expressed SUV was plotted against time to obtain timeactivity curves (TACs) of measured organs.

Time-integrated activity coefficient and absorbed radiation dose Calculations

Individual organ time-activity curves were estimated by fitting volume of interest data from the dynamic scan and whole-body scans for the four subjects. The whole-body time-activity curves were constructed by taking the activity in the entire whole-body (including the urinary bladder) in the first 3 whole-body scans and decay-correcting them to the time of administration. This was assumed to represent the entirety of the administered activity. The remaining 2 whole-body scans were constructed by taking the activity in the entire whole body excluding those of the urinary bladder at the time of the third whole-body scan, assuming a 1-h voiding interval to estimate the residence time of urine in the bladder. Radiation absorbed doses and effective doses were calculated based on the RADAR method [13] using OLINDA/EXM2.0 software (HERMES Medical Solutions and Vanderbilt University, Stockholm Sweden) [14, 15]. The time-integrated activity coefficient (formerly called the residence time) was calculated by dividing the fractional uptake parameter of the exponential fit to the original data (not corrected for decay) by the decay constant of the fit. Each organ volume obtained by the PET/CT images was converted to organ masses according to the International Commission on Radiological Protection Publication 89 (ICRP-89) male and female phantom-models [16]. Organ absorbed doses and effective dose (ED) per absorbed activity in μ Gy/MBq and μ Sv/ MBq, were calculated, respectively, using the ICRP-103 tissue weighting factors [17].

Statistics

All values are expressed as mean \pm SD. All the statistical analysis was performed using statistical software, JMP 8J version.

Results

PET imaging of pharmacokinetics and biodistribution of ¹⁸F-FPYBF-2

None of the subjects injected with 213 ± 18 MBq of ¹⁸F-FPYBF-2 demonstrated observable adverse events or clinically detectable pharmacologic effects, and any apparent changes in standard vital signs during three months follow-up period. Dynamic PET imaging demonstrated that the hepatobiliary and renal systems were the principal pathways of clearance of ¹⁸F-FPYBF-2 (Fig. 1). High uptake in the liver and the gall bladder, the stomach, and the kidneys were demonstrated, followed by the intestines and the urinary bladder. Some accumulation of ¹⁸F-FPYBF-2 was observed in the brain (Table 2). No significant accumulation or retention of ¹⁸F-FPYBF-2 was observed in the lung, the genital organs. There were mild depositions of radioactivity in the skeletal structures, the muscle, salivary glands. The time-activity curves of ¹⁸F-FPYBF-2 radioactivity concentration in different organs and tissues were determined from PET/CT images (Fig. 2). Within 1 min, the level of radioactivity in the aorta (blood) reached SUVmax; 12.6 ± 5.34 and then cleared bi-exponentially with the fast phase between 1 and 10 min and then a slow phase until 90 min. Accumulation of the radioactivity into the liver and kidney was observed, reaching concentrations of SUVmax; 9.29 ± 1.60 at 10 min and SUVmax; 13.12 ± 52.13 at 1 min, respectively. There was a relatively low level of uptake in the lung, the pancreas, the spleen and the muscle throughout the 90 min of the study.

Fig. 1 Time-activity curve of ¹⁸F-FPYBF-2 uptake (SUV) in selected organs and tissues determined from dynamic and whole-body PET images of four normal healthy volunteers. Data were expressed in mean±s.d



Table 2 Uptake of ¹⁸F-FPYBF-2 in the Brain obtained from whole-body PET images of four normal healthy volunteers

Time (min)	15	30	45	60	75	90
Blood (Aorta)	1.12 ± 0.20	1.05 ± 0.17	0.95 ± 0.15	0.98 ± 0.16	0.95 ± 0.16	0.92 ± 0.12
Brain (Cortex)	1.68 ± 0.31	1.57 ± 0.33	1.48 ± 0.28	1.35 ± 0.27	1.33 ± 0.22	1.21 ± 0.19

Radiation dosimetry

To assess human radiation exposure due to diagnostic dosages of ¹⁸F-FPYBF-2, the radiation absorbed doses to organs were estimated using organ time-integrated activity coefficients from each individual (Table 3). The mean organ doses and EDs normalized to the unit-injected activity applied to ICRP-89 male and female phantom models are given in Table 4 and 5. The ED for the adult dosimetric model was estimated to be $8.48 \pm 1.25 \ \mu\text{Sv}/\text{MBq}$ ($3.14 \pm 0.46 \ \text{mSv}/370 \ \text{MBq}$). The higher absorbed doses were estimated for the liver ($28.98 \pm 12.49 \ \text{and} 36.21 \pm 15.64 \ \mu\text{Gy}/\text{MBq}$), the brain ($20.93 \pm 4.56 \ \text{and} 23.05 \pm 5.03 \ \mu\text{Gy}/\text{MBq}$), the small intestines ($9.12 \pm 2.61 \ \text{and} 11.12 \pm 3.15 \ \mu\text{Gy}/\text{MBq}$), and the kidneys ($7.81 \pm 2.62 \ \text{and} 8.71 \pm 2.90 \ \mu\text{Gy}/\text{MBq}$) for male and female, respectively.

Discussion

This study was conducted to facilitate the clinical imaging study with ¹⁸F-FPYBF-2, a benzofuran derivative for the imaging of A β protein. Previously, ¹⁸F-FPYBF-2 showed high binding affinity for A β aggregates in ex-vivo autoradiograms of brain sections from Tg2576 mice and for amyloid plaques in sections of autopsied AD brain [10]. Recently, we reported the usefulness of ¹⁸F-FPYBF-2 imaging for the evaluation of AD [12]. In that study, static head PET image acquisition for 20-minutes was performed 50–70 min after the intravenous injection of ¹⁸F-FPYBF-2 (200 \pm 22 MBq).

In this first-in-man study, the pattern of biodistribution and clearance of ¹⁸F-FPYBF-2 were similar to those reported before in mice study [10]. ¹⁸F-FPYBF-2 was mainly excreted by the liver and substantial intestinal discharge of the radioactive material was observed. This radiotracer also showed considerable renal excretion. The slight uptake in the brain in normal healthy volunteers was observed from the early phase after the injection of ¹⁸F-FPYBF-2, which was supposed to be suitable for neuro imaging for diagnosis of AD.

Based on the results of the present study in normal healthy volunteers, the estimated ED in human patients after administration of 185–370 MBq of ¹⁸F-FPYBF-2 is 1.57–3.14 mSv ($8.48 \pm 1.25 \ \mu$ Sv/MBq). Previous studies of ¹¹C-PiB PET imaging showed ED estimation (Adult Phantom Model) as 4.74 μ Sv/MBq [18] or 5.29 μ Sv/MBq [19]. As anticipated, whole-body ED for ¹⁸F-FPYBF-2 was greater than those for ¹¹C-PiB because of the longer decay

Fig. 2 Representative wholebody coronal maximum intensity projection (MIP) PET images obtained at 15, 30, 45, 60, 75 and 90 min. Different organs are indicated by arrows and labeled as; Br brain, Hrt heart, Liv liver, Int intestine, Bl urinary bladder





60 min

75 min

90 min

Table 3 Time-integrated activity coefficients of each organ calculated from biodistribution data of FPYBF2 in healthy subjects

Organ	#1 (TTT)	#2 (AAA)	#3 (KKK)	#4 (HHH)	Mean	S.D.
Brain	1.18E-01	1.16E-01	1.70E-01	1.05E-01	1.27.E-01	2.91.E-02
Gallbladder Wall	1.72E-03	1.52E-03	1.69E-03	2.65E-03	1.90.E-03	5.11.E-04
Small Intestine	1.33E-01	1.88E-01	1.45E-01	2.58E-01	1.81.E-01	5.65.E-02
Right colon	1.86E-02	1.26E-02	1.01E-02	1.19E-02	1.33.E-02	3.69.E-03
Heart Contents	1.85E-02	1.82E-02	1.70E-02	1.90E-02	1.82.E-02	8.50.E-04
Heart Wall	1.45E-02	1.03E-02	1.07E-02	1.76E-02	1.33.E-02	3.45.E-03
Kidneys	2.28E-01	1.28E-01	1.98E-01	1.07E-01	1.65.E-01	5.71.E-02
Liver	3.30E-01	1.16E-01	1.53E-01	1.90E-01	1.97.E-01	9.35.E-02
Lungs	1.16E-02	1.23E-02	1.85E-02	1.05E-02	1.32.E-02	3.59.E-03
Pancreas	1.35E-02	1.88E-02	1.05E-02	9.62E-03	1.31.E-02	4.14.E-03
Trabecular Bone	1.75E-01	1.82E-01	1.06E-01	1.24E-01	1.47.E-01	3.75.E-02
Spleen	1.00E-02	1.05E-02	1.31E-02	1.39E-02	1.19.E-02	1.92.E-03
Urinary Bladder Contents	5.57E-03	1.19E-02	1.33E-02	1.21E-02	1.07.E-02	3.49.E-03

half-life of 18 F (t1/2 = 110 min) than of 11 C (t1/2 = 20 min). In ¹¹C-PiB PET imaging study, however, patients usually supposed to receive a relatively higher radioactive dose of ¹¹C-PiB (i.e. 555 MBq) to obtain appropriate image quality. Thus, it implies that ED of ¹¹C-PiB PET imaging in

a clinical setting is around 2.6 to 2.9 mSv. Therefore, the radiation exposure of ¹⁸F-FPYBF-2 PET can be considered allowable for clinical PET study for dementia. Concerning the radiation exposure of other amyloid imaging agents, the estimated EDs were reported as follows; 14.67 µSv/MBq for Table 4Mean organ absorbeddoses to the ICRP 89 adult (a)male and (b) female phantommodel in OLINDA/EXM 2.0using time-integrated activitycoefficients from normal healthyvolunteers after intravenousinjection of ¹⁸F-FPYBF-2

Organ	#1 (TTT)	$\#2(\Delta \Delta \Delta)$	#3 (KKK)	#4 (HHH)	(uGy/MBa)	mGy/370 MBa
organ	#1(111)	#2 (IUIII)	#5 (IXIXIX)	<i>"</i> - (IIIII)	$(\mu O y/MBq)$ Mean + SD	Mean + SD
<i>(a)</i>						
Adrenals	1.93	1.08	1.47	1.13	1.40 ± 0.39	0.52 ± 0.14
Brain	19.60	19.20	27.60	17.30	20.93 ± 4.56	7.74 ± 1.69
Esophagus	5.20	3.30	3.63	3.90	4.01 ± 0.83	1.48 ± 0.31
Gallbladder wall	1.41	0.76	0.88	1.12	1.04 ± 0.28	0.39 ± 0.11
Left colon	3.19	3.05	2.83	3.58	3.16 ± 0.31	1.17 ± 0.12
Small intestine	7.00	9.38	7.38	12.70	9.12 ± 2.61	3.37 ± 0.96
Stomach wall	5.98	4.38	4.42	4.72	4.87 ± 0.76	1.80 ± 0.28
Right colon	7.23	5.00	4.46	5.31	5.50 ± 1.21	2.04 ± 0.45
Rectum	0.53	0.60	0.52	0.72	0.59 ± 0.09	0.22 ± 0.03
Heart wall	1.26	0.93	0.95	1.28	1.10 ± 0.19	0.41 ± 0.07
Kidneys	10.75	6.07	9.25	5.19	7.81 ± 2.62	2.89 ± 0.97
Liver	46.75	18.10	23.33	27.75	28.98 ± 12.49	10.72 ± 4.62
Lungs	5.53	3.98	5.03	4.26	4.70 ± 0.71	1.74 ± 0.26
Pancreas	2.00	2.36	1.55	1.60	1.88 ± 0.38	0.69 ± 0.14
Prostate	0.09	0.09	0.08	0.10	0.09 ± 0.01	0.03 ± 0.00
Salivary glands	2.34	2.24	2.90	1.97	3.36 ± 0.39	0.87 ± 0.14
Red marrow	7.97	7.28	5.50	6.71	6.86 ± 1.04	2.54 ± 0.39
Osteogenic cells	10.50	10.30	7.18	10.70	9.67 ± 1.67	3.58 ± 0.62
Spleen	1.45	1.30	1.63	1.60	1.50 ± 0.15	0.55 ± 0.06
Testes	0.22	0.24	0.20	0.22	0.22 ± 0.02	0.08 ± 0.01
Thymus	0.23	0.16	0.17	0.20	0.19 ± 0.03	0.07 ± 0.01
Thyroid	1.51	1.17	1.23	1 14	1.26 ± 0.17	0.07 ± 0.01 0.47 ± 0.06
Urinary bladder wall	3 975	7.025	7 55	7 35	6.48 ± 1.68	240 ± 0.62
(<i>h</i>)	5.975	1.025	1.55	1.55	0.10 - 1.00	2.10 - 0.02
Adrenals	1 78	1.03	1 33	1 12	1.31 ± 0.33	0.49 ± 0.12
Brain	21.60	21.00	30.40	19.00	1.51 ± 0.55 23.05 ± 5.03	0.49 ± 0.12 8 53 ± 1 86
Breasts	1.00	1 23	1 31	1 44	1.48 ± 0.32	0.55 ± 0.12
Ecophague	7.13	1.25	4.70	5.08	1.40 ± 0.52	0.35 ± 0.12
Collbladdor well	1.52	4.10	4.70	1.22	5.27 ± 1.29	1.93 ± 0.48
Laft colon	2.84	2.52	2.46	2.00	1.20 ± 0.25	0.47 ± 0.08
Small intesting	2.04	11.42	0.02	15.00	2.70 ± 0.20	1.00 ± 0.10
Stamook wall	0.30	5.46	5.60	6.22	11.12 ± 3.13	4.11 ± 1.17
Dight color	7.14	5.40	J.00	5.66	0.12 ± 0.73	2.27 ± 0.28
Right colon	1.23	5.29 0.52	4.81	5.00 0.50	3.73 ± 1.03	2.13 ± 0.39
Rectum Least wall	0.45	0.52	0.47	0.39	0.31 ± 0.06	0.19 ± 0.02
Heart wall	12.00	1.15	1.14	1.34	1.32 ± 0.21	0.49 ± 0.08
Kidneys	12.00	6.78	10.25	5.83	8.71 ± 2.90	3.22 ± 1.07
Liver	58.50	22.60	29.25	34.50	36.21 ± 15.64	13.40 ± 5.79
Lungs	6.58	4.76	6.05	5.05	5.61 ± 0.85	2.08 ± 0.31
Ovaries	1.71	1.85	1.63	2.24	1.86 ± 0.27	0.69 ± 0.10
Pancreas	2.54	2.78	1.92	1.93	2.29 ± 0.44	0.85 ± 0.16
Salivary glands	2.64	2.53	3.24	2.23	2.66 ± 0.42	0.98 ± 0.16
Red marrow	10.08	9.33	6.88	8.67	8.74 ± 1.37	3.23 ± 0.51
Osteogenic cells	11.20	10.90	7.76	11.30	10.29 ± 1.70	3.81 ± 0.63
Spleen	1.83	1.61	2.03	1.95	1.85 ± 0.18	0.69 ± 0.07
Thymus	0.25	0.18	0.19	0.21	0.20 ± 0.03	0.08 ± 0.01
Thyroid	1.79	1.39	1.47	1.35	1.50 ± 0.20	0.55 ± 0.07
Urinary bladder wall	4.83	8.50	9.00	9.03	7.84 ± 2.02	2.90 ± 0.75
Uterus	0.15	0.18	0.15	0.22	0.17 ± 0.03	0.06 ± 0.01

Effective dose	#1 (TTT)	#2 (AAA)	#3 (KKK)	#4 (HHH)	Mean ± SD
(µSv/MBq)	10.30	7.46	7.93	8.23	8.48 ± 1.25
(mSv/370MBq)	3.81	2.76	2.93	3.05	3.14 ± 0.46

Table 5 Effective doses to the ICRP 89 adult female phantom model in OLINDA/EXM 2.0 using time-integrated activity coefficients from normal healthy volunteers after intravenous injection of ¹⁸F-FPYBF-2

¹⁸F-BAY94-9172 [19], 18.0 μSv/MBq for ¹⁸F-AV-45 [20], and 33.8 μSv/MBq for ¹⁸F-GE067 [21]. It was considered that our study protocol with the 1-hour voiding interval in this study may result in lower ED value of ¹⁸F-FPYBF-2 PET study than those of other PET studies. Therefore, as for the radiation exposure control of patients, urination before and after scan should be encouraged.

The critical organs for ¹⁸F-FPYBF-2 were the liver, kidneys, and the brain which are relatively high uptake organs of this radiotracer. Intestines were also one of critical organ, which is due to combined radiation exposure from the surrounding organs such as the liver, kidney, and urinary bladder. For comparison, the reported radiation absorbed doses after the administration of ¹¹C-PiB in humans were 19.0-19.88 µGy/MBg in the liver, 3.10-3.92 µGy/MBg in the brain, 12.6-12.92 µGy/MBq in the kidneys, 3.62-4.65 μ Gy/MBq in the small intestine [18, 19]. Furthermore, the reported radiation absorbed doses after the administration of 18 F-AV-45 in 3 humans were 44.4 μ Gy/MBq in the liver, 13.8 µGy/MBq in the brain, 16.6 µGy/MBq in the kidneys, 55.2 μ Gy/MBq in the small intestine [20]. These results suggest that the diagnostic dosage of 185-370 MBq of ¹⁸F-FPYBF-2 may be acceptable for administration in human patients and that its radiation exposure is well below the limit of 50 mSv per organ per year, which is set forth in the FDA regulations (21 CFR 361.1) [22-24].

Our clinical study with healthy volunteer and dementia patients clearly indicated that ¹⁸F-FPYBF-2 is a safe amyloid PET tracer with longer half-life with F-18 and is comparable to ¹¹C-PiB in the detectability of amyloid deposition [12]. In this report, PET study with healthy volunteers showed that ¹⁸F-FPYBF-2 uptake was mainly observed in cerebral white matter and that average Mean Cortical Index was low and stable basically independent from age or gender. In patients with AD, ¹⁸F-FPYBF-2 uptake was observed both in cerebral white and gray matter and Mean Cortical Index was significantly higher than those of volunteers and other dementia. In comparative study, the results of 18F-FPYBF-2 PET/CT were comparable with those of 11C-PiB, and the Mean Cortical Index showed direct proportional relationship with each other. Although ¹⁸F-FPYBF-2 is a "late" amyloid PET tracer after the appearance of several tracers in clinical practice with comparable diagnostic ability, we would like to show the potential of ¹⁸F-FPYBF-2 as diagnostic abilities as an amyloid imaging tracer and expand the utilization of this tracer further in various fields of research and clinical practice.

There are several issues in terms of the study limitation. First, the pharmacokinetics and metabolic analysis of ¹⁸F-FPYBF-2 were not determined in this present study, however another report about those data is in preparation. Second, the present first-in-man study reports for the radiation dosimetry assessment of ¹⁸F-FPYBF-2 PET imaging using recently released OLINDA/EXM version 2.0 [14] implemented the RADAR (Radiation Dose Assessment Resource) method, which is conceptually the same as the MIRD method and is a U.S. FDA approved software tool. Since previously reported dosimetric data used for comparison in this study were calculated by former version of OLINDA/EXM 1.0 or 1.1, those data might be slightly different from present results, and the direct comparison might not be appropriate. But this version 2.0 is reported to adopts the modified algorithm to the previous version 1.0 and 1.1 to match the organ masses shown in ICRP publication 89 [16].

Conclusions

The radiation dosimetry for amyloid imaging agents 18 F-FPYBF-2 was determined in this first-in-man study. The ED for the adult dosimetric model is $8.48 \pm 1.25 \ \mu$ Sv/MBq that is similar to those of other agents used for amyloid PET imaging. The diagnostic dosage of $185-370 \ MBq$ of 8 F-FPYBF-2 is considered to be acceptable for administration in patients as a diagnostic tool for the evaluation of Alzheimer's disease.

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Compliance with ethical standards

Conflict of interest No potential conflicts of interest were disclosed with regard to this study.

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