## ORIGINAL RESEARCH

# Differential mobility spectrometry with nanospray ion source as a compact detector for small organics and inorganics

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Abstract Electrospray ionization (ESI) is an important tool in chemical and biochemical survey and targeted analysis in many applications. For chemical detection and identification electrospray is usually used with mass spectrometry (MS). However, for screening and monitoring of chemicals of interest in light, low power field-deployable instrumentation, an alternative detection technology with chemical selectivity would be highly useful, especially since small, lightweight, chip-based gas and liquid chromatographic technologies are being developed. Our initial list of applications requiring portable instruments includes chemical surveys on Mars, medical diagnostics based on metabolites in biological samples, and water quality analysis. In this report, we evaluate ESI-Differential Mobility Spectrometry (DMS) as a compact, low-power alternative to

MS detection. Use of DMS for chemically-selective detection of ESI suffers in comparison with mass spectrometry because portable MS peak capacity is greater than that of DMS by 10X or more, but the development of light, fast chip chromatography offers compensating resolution. Standalone DMS provides the chemical selectivity familiar from DMS-MS publications, and exploits the sensitivity of ion detection. We find that submicroliter-per-minute flows and a correctly-designed interface prepare a desolvated ion stream that enables DMS to act as an effective ion filter. Results for a several small organic biomarkers and metabolites, including citric acid, azelaic acid, n hexanoylglycine, thymidine, and caffeine, as well as compounds such as dinitrotoluene and others, have been characterized and demonstrate selective detection. Waterquality-related halogen-containing anions, fluoride through bromate, contained in liquid samples are also isolated by DMS. A reaction-chamber interface is highlighted as most practical for portable ESI-DMS instrumentation.

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Center of Excellence In Genomic Medicine Research, King Abdulaziz University, Jeddah, Saudi Arabia  $\begin{tabular}{ll} \textbf{Keywords} & Ion\ mobility \cdot Nanospray \cdot Electrospray \cdot \\ Differential\ ion\ mobility \cdot DMS \cdot FAIMS \\ \end{tabular}$ 

# Introduction

Instrumentation for chemical analysis is essential for many scientific, environmental and clinical applications but the range of tools available for field deployment is limited. For high sensitivity and selectivity, mass spectrometry (MS) is often the method of choice, while optical spectroscopy is competitive in selectivity, but cannot equal MS sensitivity. The detection of ion signals, as in mass spectrometry, is highly sensitive and electrospray ionization (ESI) is efficient at broad-spectrum ionization from liquid samples with little fragmentation. Chemical selectivity can be provided by a back-end mass spectrometer, but at a cost of added power consumption, and increased



weight and cost, although progress continues to be made in reducing that burden [5,12,13,34,50].

As chip-based liquid chromatography (LC) systems with integrated trap, column, and emitter operating at nano-flow levels become available [2,4,14,15], new field-deployable devices should combine components of similarly reduced physical and electrical parameters and sufficient chemical selectivity. We have tested differential mobility ion separation with ion current detection (DMS) as a more compact alternative to MS detection. DMS provides selectivity and chemical noise suppression that can be used with low-flow ESI sources such as chip-LC with integrated emitter.

Our intended applications for portable instruments include chemical analysis on Mars and other planetary environments, medical diagnostics based on metabolites in a biological matrix such as urine, and water quality analysis, all of which can benefit from improved instrumentation. Gas chromatography (GC)-DMS has already been applied by NASA in Air Quality Monitoring on the International Space Station, with excellent results reported by Limero et al. [29]. We want to extend DMS technology to the broader range of targets accessible through ESI.

Ion mobility is well known as a method of separating ions by size, charge, conformation, polarity, and other physical, chemical, and electrical properties. The ion mobility group of techniques is used for ion separation in two primary forms. The first is a low mobility separation in drift-time ion mobility spectrometry (DT-IMS) or in traveling-wave ion mobility (TW-IMS) (generically, IMS). The second form depends on the field-dependence of ion mobility, and is known as differential mobility spectrometry (DMS), or field-asymmetric ion mobility spectrometry (FAIMS), or ion-mobility-increment spectrometry (IMIS), here generically DMS. Ion mobility is used in standalone form and in combination with other selective detection methods, especially mass spectrometry. Both ion mobility and differential ion mobility have been described from historical and technical perspectives in monographs [11,43], and technical improvements and new applications and reviews [26] appear regularly in the literature.

Ion mobility techniques are capable of operating with almost any atmospheric-pressure ionization source, and can easily be used with standard LC technology. As a fast ion selector or as a detector for fast chromatography, DMS generally has several useful properties, as summarized here, and detailed elsewhere [9,21,44].

 Continuous operation. DMS operates in continuous mode as an ion filter while IMS methods intermittently gate ions into the mobility cell for analysis, resulting in either lower sensitivity due to ion gate losses, the extra complexity of an intermediate ion trap [20,36] or the use of the Hadamard transform[1].

- Low loss. The planar configuration for DMS has a loss profile that is efficient and essentially independent of ion mobility coefficient [21]. In a commercial implementation, ion losses have been shown to be on the order of 20 % under low flow conditions [39]. In the prototype designs appropriate for small instruments tested here, the transmission coefficient is typically about 20 %.
- High speed. DMS operates at atmospheric pressure for high speed and resolution, with transit time delays on the order of 10 msec.
- Modifier-enhanced resolution. Addition of low concentrations of polar modifiers to the drift (IMS) or transport (DMS) gas increases selectivity by chemically-specific ion-neutral clustering [25,28,37,40,48]. Modifiers also suppress interfering species and clusters with lower proton affinity (positive mode) or electron affinity (negative mode) than the target analyte through charge competition [17,27,28,40,42]. Similar effects are familiar IMS [10].
- Adapted to small molecules. DMS techniques have optimum performance for small molecular weight compounds, as in our intended applications. DMS selectivity typically decreases with molecular weight, while IMS is more selective for higher masses.

In this communication, planar DMS is employed in small-molecule, low-flow electrospray applications. Ion mobility in lab-scale mass spectrometry, as in the AB SCIEX SelexION or Waters Synapt systems, is designed without regard to gas flows, heater power consumption, and complexity (for instance, the AB SCIEX ion source may use desolvation temperatures as high at 750 °C). Our goal in this work is to characterize ESI-DMS as a simplified miniature electrospray detector that provides an extra level of resolution for infused samples or for a nano-flow chip-LC system. As mentioned, our intended applications include astrobiology (traces of life, including amino acids and peptides [31]), metabolic biomarker detection [8,9], as well as environmental monitoring.

A comparison of the power and weight characteristics of portable mass spectrometers, and an ESI-DMS system, shown in Table 1, indicates that the ESI-DMS system can be very much lighter and lower in power than MS systems, but with lower peak capacity. Except in special cases, additional methods like chromatography may be necessary, but that is often necessary in MS applications as well.

### **DMS** selectivity

The ion separations used in differential mobility spectrometry (DMS) are determined by the differential mobility parameter,  $\alpha(E)$ , which describes the relative change with



**Table 1** Power and weight requirements. A nano-ESI-DMS system operates at atmospheric pressure with a diaphragm micropump weighing 20 g providing flow of 300 ccm. Vacuum pumps and complex electronics increase the power and weight of MS systems.

Resolutions listed for MS systems are approximate and do not include any chromatographic resolution. Sources (Griffin: http://gs.flir.com/griffin-400, Torion: http://www.torion.com/products/24, Cooks/Purdue: Sokol et al. [45,46])

Instrument	Commercial production	Weight	Power	Battery option	Resolution	Туре	Sample intro
Griffin 400/460 MS Torion TRIDION 9 MS	Yes Yes	37–45 kg 15 kg	400–600 W 60–120 W	Yes Yes	~400 ~400	trap MS, GC-MS trap MS, GC-MS	GC SPME, needle trap
Mini 10.5 MS (Cooks, Purdue)	No	10 kg	50 W	Yes	~300	Ion trap MS	Membrane, sorbent, D-API
ESI-DMS	No	1 kg	< 10 W	Yes	~40	DMS	Nanospray to reaction chamber

electric field amplitude of the ion mobility coefficient [3], K(E):

$$\alpha \quad (E) = \frac{K(E) - K(0)}{K(0)}, \quad \text{where}$$

$$K(E) = v(E) / E, \quad \text{or} \quad NK(E) = \frac{v(E)}{\left(E / N\right)} = \frac{v(E)}{E_{Td}}.$$
(1)

v(E) is the field-induced ion drift speed, E the electric field strength, N the buffer gas density, and  $E_{Td}$  is E/N, which is the ion mobility field in Townsend units [32]. The mobility coefficient, K(E), acquires a dependence on field strength that is dependent on properties of the ion [30], interactions of the ion with its chemical environment [25,28,40], and the pressure, and temperature in the DMS analytical region [23,32]. This field dependence is dominated by ion-neutral chemical affinity (except in the case of helium transport gas), which is the basis of the high small-molecule selectivity of DMS.

The ion mobility coefficient in Townsend units, NK(E), can be written in terms of an effective cross-section for the interaction of the ion with all the neutrals in the local chemical environment.

$$NK(E) \cong \frac{1}{\Omega(T_{eff})} \left[ \frac{3}{4} \frac{q}{\mu \langle v_{rel} \rangle_0} \right], \text{ where } \langle v_{rel} \rangle_0 \equiv \sqrt{\frac{8kT}{\pi \ \mu}}$$
 (2)

The quantities in square brackets ([]) can be disregarded in a qualitative view because they are constant at a particular bulk gas temperature, T, and independent of the ion for heavier ions. Thus, all the variation in ion mobility in Townsend units, NK(E), is contained in the ion-neutral cross-section,  $\Omega$ , controlled by the effective temperature,  $T_{eff}$ . Other symbols in the equation have their usual meanings. The effective temperature,  $T_{eff}$ , is the bulk gas temperature, T, plus a heating term from the applied field,  $\varsigma m(K(E)E)^2/3k$  [23] ( $\zeta$  is an ion-specific parameter, typically 0.5 to 1.0).

From the above expression for ion mobility, it can be concluded that temperature and pressure have only weak effects on practical DMS resolution, but that modifiers, which decluster synchronously with the DMS waveform, can increase differential mobility by modulating the cross-section. The dissociation of ion-neutral clusters is required for the highest field dependence and thus the highest DMS selectivity and that can be facilitated by lower pressure and higher temperature. In the case of Mars, since the ambient pressure is 4.56 Torr, clusters will be reduced, and ESI at low pressure has been developed in the Smith group at PNNL [35].

The configuration of a DMS system with integrated detectors is shown in Fig. 1. The fields applied in the DMS region are also shown. The separation voltage/field (SV) is an AC waveform (time average zero) and the compensation voltage (CoV) is a DC offset that tunes the waveform trajectory to pass selected ions. The waveform properties and generation are discussed in more detail in [24]. The DMS filtration process is specified by these two electrical parameters, SV, and CoV, in addition to environmental variables pressure, temperature, and transport gas composition.

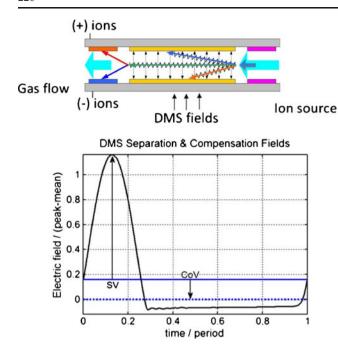
Peak capacity in DMS has been discussed in a recent publication by Schneider et al. [42] and in a data-rich Pittcon presentation available from the AB-SCIEX website [38]. As shown in those works, peak capacity without chemical modifiers is typically on the order of 20, and about 40 or higher with modifiers.

# **Experimental**

## Chemicals

Electrospray solvents, acetonitrile, methanol, and water were Fisher Scientific Optima LC/MS grade. Other chemicals include thymidine ( $C_{10}H_{14}N_2O_5$ , MW=242.09027, CAS 50-89-5) from Alfa Aesar (L12490), azelaic acid ( $C_9H_{16}O_4$ , MW=188.10485 CAS 123-99-9) from Alfa Aesar (36308), Citric acid monohydrate ( $C_6H_8O_7$ , MW=192.027 CAS 77-92-6) from Alfa Aesar (22869), n hexanoylglycine ( $C_8H_{15}NO_3$ , MW=173.10519 CAS 24003-67-6), from Dr.





**Fig. 1** Schematic of the DMS analytical region and notation for the waveform used in these experiments. The DMS ion filter is a simple planar region (typ. 0.5 mm gap, 10. mm length, 3 mm width, 300–600 ccm flow) with Faraday plate ion detection. The field applied across the channel is of the "flyback" type, with a period of 800 nsec. The *solid horizontal line* is the waveform time-average. DMS separation field (SV) is measured as waveform mean to peak voltage (SV), and compensation field (CoV) is measured as mean voltage difference

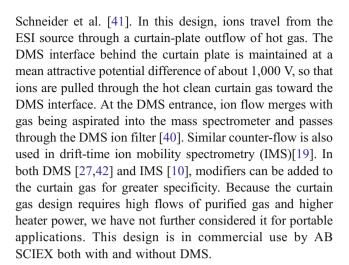
Herman J. ten Brink, VU Medical Center Metabolic Laboratory, Amsterdam, The Netherlands, and other chemicals were obtained from Sigma-Aldrich, including caffeine, formic acid, ammonium acetate, DL-trisodium isocitrate, and 2,4-dinitrotoluene. Anion solutions for fluoride, chloride, and bromate were provided in the form of ion-chromatography test solutions by Dionex as ion standard solutions (www.dionex.com).

## ESI interface to DMS

Compact instrumentation designs are constrained by available power, gas flow rates, and size requirements. We have considered three interface types: (1) Curtain gas: a fully-desolvating curtaingas interface with ions desolvated in a hot gas counter-flow, (2) Reaction chamber: a reaction/desolvation chamber design with hot-gas dilution, and (3) Capillary or skimmer: a heated capillary or simple orifice design with thermal declustering only. The three configurations are briefly described below.

# Curtain-gas interface

The fully-desolvating curtain-gas interface used in commercial lab-scale instrumentation is illustrated in Fig. 6 in



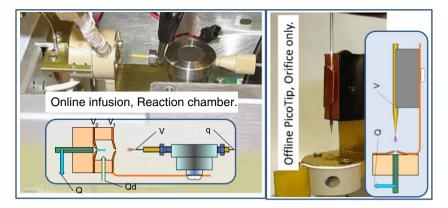
#### Reaction chamber

The reaction chamber interface is simpler to implement, requires lower gas flows, and uses lower voltages on the interface than the curtain gas system. Rather than supplying a flow exceeding the transport flow of the DMS, dilution with a 10-20 % flow of heated gas, which may contain modifier, is used. This design is illustrated in Fig. 2 (left). Pre- and post-reaction-chamber orifices reduce the entry of droplets, and the reaction chamber allows additional time for heating and desolvation of the electrospray plume, and the equilibration of charge-transfer and modifier-clustering reactions. An attractive potential of 40 to 400 V is applied between the reaction chamber orifice and a similar orifice at the DMS entrance. DMS SV and CoV values for ion transmission in this system are modified by ESI solvent vapors, and the additional concentration of any added modifiers. Room air provides the bulk of the gas flow, which may add trace contaminants extracted in the reaction chamber, but that effect is minimized by the short emitter-to-orifice distance, and they are usually removed by DMS filtration. In difficult environments, chemical filter cartridges may be used to purify the desolvation gas and to supply an electrospray chamber.

## Simple orifice or heated capillary

Use of an entry orifice with low nano-flow is the simplest of the three designs, with no added desolvation gas or region (Fig. 2, right). A heated tube 0.8 mm ID or smaller can also be used with similar performance. Heating in the tube is used for desolvation, and emitter approach angle and distance aid in the separation of solvent droplets and clusters in both cases. This method is less effective because the ESI solvent vapors remain undiluted. Since equilibration time is short, evaporative cooling can fight desolvation. However, the presence of solvent vapors improves DMS resolution





**Fig. 2** Two configurations have been tested which are suitable for field-portable instrumentation. The system at left uses a reaction chamber for ion desolvation. In the reaction chamber design, total gas flow, Q (400–800 sccm) includes a heated desolvation and modifier gas flow, Qd, of about 100 sccm at about 100 °C, with the balance of gas aspirated from the ESI plume region. The ESI liquid infusion, q, is 50-600 nL/min, with an emitter voltage drop  $V-V_1$  in the  $\pm 1,400-2,000$  V range for Proxeon metal emitter tips. The voltage across the reaction chamber,  $V_2-V_1$  (not

critical) is typically  $\pm 40$  to 100 V, and  $V_2$  is set to the mean DMS potential. At right is shown the configuration with very low flow and no additional desolvation. The reaction chamber allows more complete breakup of ion-solvent clusters, provides more stable intensities, and works at higher liquid flows. A full curtain-gas system (Qd>Q, for net outflow toward the ESI source for complete control of desolvation and modifier effects) is not discussed here, but is used in the AB SCIEX commercial DMS-MS and is shown in Schneider et al. [39]

through the modifier effect, but only on the desolvated fraction of ions since the modulation of ion mobility depends on the ratio of clustered and unclustered molecular sizes. Testing described below indicate that this design is less effective than might be expected, even at the lowest flows because of instability in the droplet fraction and the tendency to deposit charges on inlet surfaces which decrease ion flow.

#### Equipment

Electronics for generation of DMS voltages, detection of DMS ion currents, and serial communication with a controlling PC were derived from components from a Sionex Corp. SVAC microDMx system [23,33]. The electronics provide the fly-back DMS waveform shown in Fig. 1, with peak-to-mean separation voltage (SV) amplitude from 500 V to 1,500 V for DMS-filter mode and 0 V for DMS transparent mode (SV=0 V), and compensation voltage (CoV) ranging from -43 V to + 15 V. The dual detection circuits for positive and negative ions have gains of 166 pA/V, bandwidth of 15 kHz, and RMS noise below 1 mV in 10 msec averaging time. The system was operated, and data was acquired using Sionex Expert software, and data analysis done in MATLAB (Mathworks, Natick, MA).

In the two experimental configurations shown in Fig. 2, gas flows from 300 to 600 sccm are used. The DMS analytical region is (0.5 mm H, 3.0 mm W, 10 mm L). DMS resolution can be shown to be proportional to the height dimension at constant diffusion loss [22], but practical sensor design is limited by available gas flow rate and electrical breakdown field. Waveform

shapes are described in more detail elsewhere [24]. We employ a frequency of approximately 1.25 MHz (800 nsec period) for the asymmetric waveform. For an ion mobility of K=1.5 cm<sup>2</sup>/( $V\cdot sec$ ), the predicted loss due to diffusion at 300 K, 1 atm., is 30 % (SV=0), increasing to 35 % with SV=100 Td (1,223 V), with a predicted transmission peak width of 1.1 V (CoV), based on a custom MATLAB application containing DMS design principles.

The three sections of the sensor, desolvation/reaction chamber (if any), DMS analytical region holder, and detection region holder were machined from PEEK, while the electrodes of the DMS analytical and detector regions were manufactured as gold-metal traces on alumina ceramic or on circuit board. Nitrogen or air, dried through an Ailtech Hydropurge cartridge, was provided for desolvation and modifier introduction, with the desolvation gas heated to ~90 °C by passage through a 4" long, 1/16" stainless tube wrapped with a heating element (~4 W). Total DMS transport gas flow was controlled at the sensor outlet by a needle valve connected to a micro KNF diaphragm pump or to a vacuum source. Data for comparison with DMS-MS acquired on an AB SCIEX API 3000 with a prototype DMS curtain-gas interface, and a nebulized micro-spray ESI source with Proxeon ES563 emitter. This data is not shown, but had similar DMS characteristics.

Infused sample was delivered at flow rates from 20 to 800 nL/min by a Harvard Apparatus Syringe pump with Hamilton gas-tight syringes of 10  $\mu$ L and 25  $\mu$ L sizes. Stainless steel emitters from Proxeon (ES561, www.proxeon.com) were used, as well as off-line Econo12 PicoTip emitters from New Objective (www.newobjective.com).



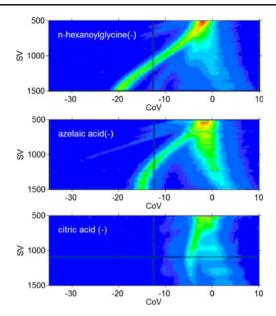


Fig. 3 ESI-DMS of three reported urine biomarkers of radiation exposure are shown across the entire DMS tuning range in these topographic or dispersion plots. N-hexanoylglycine, azelaic acid, and citric acid are shown in (–). It is adventageous to use negative ion mode for biological samples. In positive mode, ion concentrations are diluted by the occurence of Na and K adducts, by proton and Na-bound dimers, and by the more facile proton attachment of matrix ions. These ions are successfully resolved, but a gas-phase modifier or liquid chromatography will be necessary to resolve other targets. (See next two figures)

#### Results and discussion

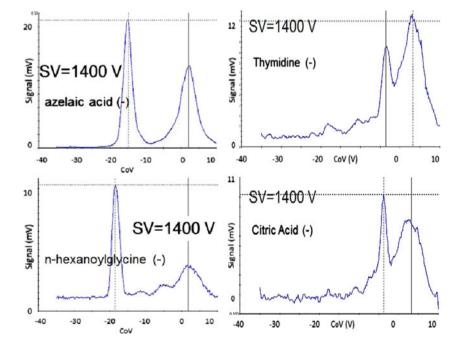
Metabolic biomarker analysis

A reaction chamber interface shown in Fig. 2 (left) was used to record the DMS-detected negative ion electrospray of

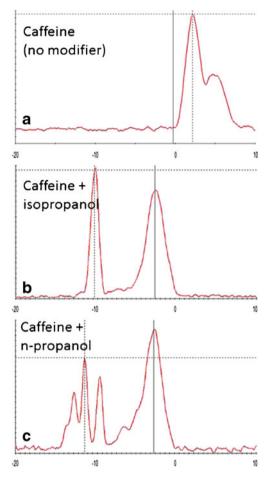
several small organic molecules, including azelaic acid ([M-H]-, 1 87.097), n-hexanoylglycine ([M-H]-, 172.097), citric acid([M-H]-, 1 91.019), DL-isocitric acid([M-H]-, 191.019), and thymidine([M-H]-, 241.082). Topographic or dispersion 2-D plots (Fig. 3) show the complete DMS-detected transmission profile for all SV and CoV for three of these compounds (n-hexanoylglycine, azelaic acid, and citric acid). These molecules have previously been identified as candidate urinary biomarkers for radiation exposure [49], and are associated with stress response. Each compound was prepared in 50/50 methanol/water at 100  $\mu$ M, and was supplied at 500 nL/min to a Proxeon ES561 emitter at -1.7 kV. DMS total transport gas flow was 0.6 LPM, and desolvation flow was 0.1 LPM dry nitrogen heated to approximately 100 °C.

All of the compounds can be detected as deprotonated anions at specific DMS SV/CoV. Negative ion mode is usually preferred for detection of polar urine biomarkers in biological matrices because fewer interferents appear in negative electrospray than in positive. Positive ion mode has additional complexity from Na and K adducts as well as proton or Na-bound dimers, and a number of less polar compounds attach a proton (PA) but have low electron affinity (EA). Figure 4 shows DMS signals as a function of compensation voltage for azelaic acid, n hexanoylglycine, thymidine, and citric acid at SV 1,400 V. The signals for azelaic acid and n-hexnoylglycine can be resolved from the remaining ion-solvent cluster peak near zero CoV at the highest voltages. The background peak is a bit large in these data, and may be due to two effects: excessive concentration (100 uM) leading to dimer ions, and relatively high liquid flow and low desolvation flow. Compensation

Fig. 4 Radiation-exposure biomarkers thymidine and citrate are not resolved under the conditions of Fig. 3 although azelaic acid and n-hexanoylglycine are. Citric acid is shifted to more negative compensation voltage by alcohol gas-phase modifiers while thymidine is not (DMS-MS data, not shown), thereby allowing them to be resolved. Examples of modifier effects are shown in Fig. 5

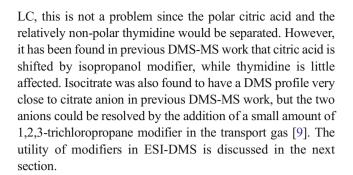






**Fig. 5** Caffeine is used here to illustrate modifier-enhanced DMS resolution in reaction-chamber DMS. Peaks are shifted and separated by the introduction of about 1 % v/v isopropanol or n-propanol in the transport gas stream in the reaction chamber. The caffeine concentration (100 uM) is large, resulting in a significant cluster peak (rightmost peak). **a** no modifier, **b** 1 % isopropanol, **c** 1 % n-propanol. The multiple peaks with n-propanol may indicate multiple conformations

voltages, -15 V for azelaic acid, and -19 V for n-hexanoylglycine at 1,400 V SV are quite distinct, but peaks for thymidine and citric acid are at the same CoV. If used with

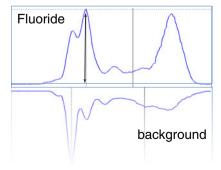


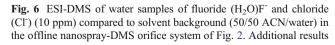
#### ESI-DMS modifier-enhanced resolution

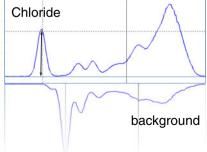
The use of modifiers in the transport gas stream to increase the DMS field modulation of the effective cross-section has been described in a number of publications [28,40,42]. We illustrate this method in ESI-DMS with the most generically-effective modifier for positive ions, isopropanol (other alcohols are also effective). For negative ions, methylene chloride is often used, and 1,2,3-trichloropropane has been found to be especially effective, even at low concentrations.

ESI-DMS in positive ion mode was tested for caffeine with and without transport gas modifiers. Modifiers isopropyl alcohol, and n propyl alcohol were introduced at about 1 % by volume with the desolvation flow in the reaction chamber. These results are shown in Fig. 5. For caffeine in Fig. 5(a), at the maximum SV of 1,500 V, the caffeine peak is only partially separated from the cluster peak, but could be used for detection in combination with LC with a stable solvent background level. Figures 5(b) and (c) show that the addition of alcohol modifiers isopropyl alcohol or n propyl alcohol provide much higher resolution at lower SV (650 V). The caffeine sample was 100 μM in 50/50 acetonitrile/water, and the infusion rate 300 nL/min.

The multiple caffeine peaks for n-PA may indicate multiple cluster structures or multiple cluster numbers. The mechanism, kinetics, and thermochemistry of DMS modifier effects have been considered briefly in earlier publications [25,27], but a number of mechanistic, kinetic, and thermochemical questions remain on the modifier effect.







are shown in Table 2. The rightmost peak in each case is a dimer and solvent cluster peak that would be decreased with heated reaction chamber desolvation and lower concentrations



**Table 2** Experimental results for halogen anions important for water quality. Samples concentrations were in the 1–10 ppm range, diluted in 50/50 acetonitrile/water. Bromate (BrO<sup>3-</sup>) is a common result of water treatment. Ion identities were determined by DMS-MS. Formate occurs as an anion and a proton-bound dimer. Acetate is not distinguished

from ACN under these conditions. Data was taken on the off-line emitter system without additional desolvation of Fig. 2 (left). This results in some signal instability that is avoided in the reaction chamber design

Sample	Ion	CoV(500 V SV)	CoV(550 V SV)	CoV(600 V SV)
Chloride	Cl <sup>-</sup>	-15.5 V	-20.2 V	Weak
Fluoride	$(H2O)F^-$	-10.6 V		-16.9 V
Bromate	BrO3 <sup>-</sup>	−3 V		-4.8 V
Formate	CHO2 <sup>-</sup> , ((CHO2)2H) <sup>-</sup>			−12 V, −4.4 V
Acetate		-12.3 V		−19.5 V
ACN/water only	CH3CN <sup>-</sup>	-12.3 V		−19.5 V

Molecular and cluster structures have been calculated, as well as entropy and enthalpy values for correlation with DMS behavior, and work is ongoing.

Water quality: halogen-containing anions

We have also tested DMS-detected electrospray for ion chromatography detection for common anions, fluoride, chloride, bromate, formate, and acetate. This kind of analysis is essential in the monitoring of water contaminants for industrial and public health applications. Some of these results are shown in Fig. 6, comparing chloride and fluoride with the solvent background. Fluoride anion was identified by DMS-MS as the hydrated fluoride anion,  $F^-(H2O)$ , m/z=-37, while chloride is carried by Cl<sup>-</sup>, m/z=37 and 35. Table 2 lists DMS characteristics of several other species important for water quality, such as BrO3<sup>-</sup>, generated in water treatment. The estimated LOD for chloride and fluoride was computed as 100 ppb based on the observed S/N in a survey scan with 10 msec averaging time. Many volatile organic compounds (VOCs) in water have previously been detected using GC-DMS (Sionex data, not shown), and should similarly be observable in ESI-DMS. The use of reclaimed and recycled water in environments with limited storage space and no continuous water supply, such as the International Space Station, has many advantages but requires broad-spectrum monitoring of contaminants.

Simple orifice/capillary interface: ESI-DMS signal stability

Ion streams generated by ESI are monopolar and can be intense. ESI may be contrasted with the bipolar ion stream generated by some other sources, such as radioactive ionization (such as <sup>63</sup>Ni) and UV photoionization. In DMS, contact of the ions with the walls of the analytical region is part of the selectivity of the system, allowing only one ion species to pass out of the DMS analytical region unneutralized. This characteristic can lead to charge buildup, even on metal surfaces (as is familiar in vacuum in mass spectrometry under heavy ion loads). This charge buildup can lead to intensity changes, or even to transmission pinchoff. As indicated in Table 3, this effect is greatest in systems without a desolvation gas stream. A DMS system with a simple orifice sample introduction has the least ion losses and the greatest signal levels but is prone to charge buildup and loss of intensity. The large signals are illustrated by the signals over a volt in amplitude, corresponding to nearly 250 pA of ion current in a system with a noise floor on the order of 0.1 pA with 10 msec averaging time (Fig. 7). Introducing too many ions into an inlet without desolvation

**Table 3** Immediate ion desolvation at atmospheric pressure is more important for DMS than for MS because expansion to vacuum is strongly desolvating. These three designs are discussed in the text, with results summarized here. Although the curtain gas interface is

most effective, the reaction chamber design is effective with lower gas flows, and provides some modifier-effect resolution enhancement. The simplest heated capillary/orifice interface can be used at flows from 20 to 80 nL/min, but is still occasionally unstable

Desolvation method	Flow ratio desolvation/DMS	liquid flow	modifier effect from ESI solvent	Intensity instability
Curtain gas	1.0 to 2.0	<20 uL/min	No	None
Reaction chamber	0.1 to 0.5	<600 nL/min	Yes	Occasional
Capillary or orifice, no reaction chamber	No added flow	<80 nL/min	Yes	Frequent, esp. for orifice



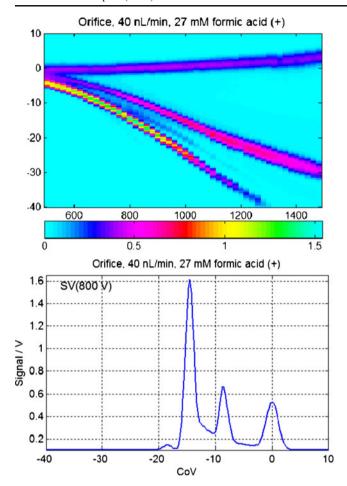


Fig. 7 Nanoflow with orifice interface can provide very large signals, but is weak in desolvation and prone to instability. The bottom trace show  $\sim\!\!250$  nA peak (166 pA/V gain) at SV 800 V. The S/N exceeds 2000:1 averaged 10 msec per point (27 mM formic acid in MeOH/water, 40 nL/min). Without the reaction chamber heated desolvation gas, charge build-up and ion flow pinch-off can result, preventing ion transmission. A low-flow online infusion system was used for these results

leads to enormous signals followed by amplitude instability and, finally, complete loss of ion transmission.

# **Conclusions**

General guidelines for the three interface types that we have described (curtain gas, reaction chamber, and capillary or skimmer) are given in Table 3. The higher liquid flows require the more effective desolvation methods. The efficiency values given for the curtain gas interface on lab-scale DMS-MS systems (SelexION, AB SCIEX) are generally consistent with the results for DMS losses observed in Schneider et al. [39]. The reaction chamber interface is clearly the most practical for use in NASA applications and for other portable applications, due to acceptable performance and modest flow requirements. The capillary or skimmer interface can be used effectively

only for off-line disposable emitter applications, but this method is the most economical in sample usage and among the highest in ionization efficiency. A simple interface of the latter type was used in recent work in the Cooks group at Purdue on interfacing DMS to a small ion trap mass spectrometer with discontinuous sample introduction [47]; it is likely that a reaction chamber or curtain gas interface could improve the performance and flexibility of DMS interfaces to this type of device, as it does for independent DMS detection.

We conclude that a heated reaction chamber is the minimum needed for desolvation and stability of chemical effects. A simple orifice is not effective, even at very low nano-flows in the range of 20-80 nL/min. A heated tube without reaction chamber under similar conditions was also found to give approximately the same behavior. Problems with the use of a small tube for desolvation prior to DMS at near atmospheric pressure do not imply any difficulty with a heated capillary in the atmosphere to vacuum transition common on Thermo Scientific instruments, which is effective due to expansion into low pressure. The reaction chamber design is lower in ion transmission than a full curtain gas interface (15-20 %) [16,18] versus 60-80 % at low flow [39], but requires up to a factor of ten less scrubbed gas, less heater power, shows improved DMS resolution due to solvent modifier effects, and requires fewer and lower voltages in the interface. As a result (Table 3), it is the preferred design for further development.

DMS filtration is known to remove chemical noise that arises from low-level contaminants, fragments, instrumental contamination and solvents (for example, see Figure 17 in [7], which shows the elimination of chemical noise after DMS selection for 2'-deoxycytidine). This is a significant advantage, because most atmospheric pressure ion sources have frequent interferents in the low mass range [6]. This reduced noise floor is evident in the ESI-DMS figures through the zero signal level seen at high CoV values. As a result, DMS is much superior to a total current detector, because total ion current is approximately independent of chemical content when samples are dilute, and TIC noise, which is large due to the high detected ion current, will mask weaker features.

The development of integrated single-chip nano-flow LC systems opens up the possibility of smaller-scale instrumentation for a range of NASA mission and for clinical diagnostic applications. Operation at reduced pressure may also be possible, leading to improved declustering based on the Smith group results [35]. As a next step, we would like to test performance with a commercial nano-LC and with custom chip-LC units that have been provided to JPL by Agilent, Santa Clara, CA.

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