

Continuous Renal Replacement Therapies: A Brief Primer for the Neurointensivist

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Abstract Continuous renal replacement therapy (CRRT) is a renal replacement modality that is often used in the ICU setting, including the neuro-ICU. This form of renal replacement therapy has been used classically for acute renal failure in patients with hemodynamic compromise, but is gaining acceptance as a method to control vascular and extra-vascular volume and mediate cytokines in non-renal diseases. Although these uses are briefly discussed, this review concentrates on the different forms of continuous renal replacement, mainly focusing on the technology of convective versus diffusive modalities and briefly on filter technology. There is also discussion on the various anticoagulation regimes used in CRRT including data on performing CRRT without anticoagulation. This review is not meant to be a discussion on the pros and cons of CRRT versus intermittent dialysis, but rather a primer on the technology of CRRT and how this therapy may affect general care of the ICU patient.

Keywords CRRT · CVVH · CVVHDF · Diffusive clearance · Convective clearance

Introduction

Acute renal failure (ARF) related to critical illness is a significant contributor to poor outcome regardless of the primary diagnoses or condition that warranted ICU care [1–4]. Intermittent or continuous renal replacement therapy (CRRT) remains the cornerstone in treating ARF and/or refractory volume overload in the ICU and has been for over 30 years.

There is ongoing debate as to the type of renal replacement therapy (RRT) that is superior in the intensive care setting. Debates range from who should manage the therapy, what the goals of the therapy should be to what type of therapy are best—intermittent or continuous. Even timing of the initiation of RRT is debated and remains an unsettled issue [5]. The CRRT or intermittent hemodialysis (IHD) debate generates strong biases and opinions in spite of recent studies to suggest equipoise, the controversy remains [6, 7]. Many institutions offer both therapies and have different criteria in choosing which to use. This is a discussion of CRRT technology and not a position paper advocating one therapy over another.

CRRT is a form of RRT that is used continuously to treat not only ARF, but has also been utilized to treat a variety of ICU conditions without ARF such as shock and pancreatitis [8, 9]. CRRT incorporates several modes of RRT utilizing different mechanisms of clearance. The modes include slow continuous ultra-filtration (SCUF), continuous arteriovenous hemofiltration (CAVH), Continuous veno-venous hemofiltration (CVVH), continuous veno-venous hemodiafiltration (CVVHDF), and high volume hemofiltration (HVHF) [10]. Each mode has unique clearance mechanics with some using convective clearance (CVVH) while other modes use diffusive clearance or some combination of convective and diffuse clearance

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(CVVHDF). This complexity extends further to machine configuration, such as pre-filter or post-filter solution replacement in convective modes, to different filter technology. In spite of these numerous modalities, CRRT has been used as a catchall phrase with inference that all continuous modalities are the same. This gives little regard to the specifics and uniqueness of each mode or possible machine configuration. This is equivalent to reporting that a patient is on mechanical ventilation ignoring mode, rate, PEEP, tidal volume or FiO_2 .

CRRT at most institutions resides within the realm of the nephrologist being a natural extension or offshoot of intermittent dialytic therapy. However, the goals of an intensivist utilizing continuous therapy may differ from that of a consulting nephrologist [11]. In specialized units like a Neuroscience ICU, nephrologist may round daily, but are not in charge of adjusting vasopressors or monitoring triple-H therapy, adding new antibiotics, initiating and adjusting nutritional support, giving fluids or colloids for hemodynamic issues or continually monitoring hemodynamic parameters. That is the domain and responsibility of the intensivist. Therefore, understanding CRRT, and the particular modalities, is extremely important since CRRT affects, among other things, drug clearance and dosing [12–14], including antibiotics and vasopressors [15–17], and affects nutritional support [18, 19]. These affects are dependent on CRRT mode, type of clearance, mode configuration, and filter type [20]. In addition, the use of anticoagulation for CRRT opens another area that needs to be controlled and understood by the intensivist.

IHD vs CRRT

Intermittent dialysis provides renal replacement for brief intervals (3–4 h), usually daily or every 2–3 days. CRRT is a therapy that provides continuous 24-h per day therapy. Both IHD and continuous hemodialysis (HD) circuits utilize similar principles. Blood is removed from the patient, pumped through a dialysis filter and returned to the patient following removal of surplus water and waste. The major difference between intermittent and continuous therapies is the speed and mechanism by which water and wastes are removed. IHD removes large amounts of water and wastes in a short period of time using diffusion, whereas, continuous renal replacement therapies remove water and wastes at a slow and steady rate using diffusion, convection or combination thereof. While intermittent dialysis allows chronic renal failure patients to limit the amount of time that they receive dialysis, the rapid removal of water and wastes during intermittent treatments may be poorly tolerated in unstable patients.

Hemodynamically unstable, fluid overloaded, catabolic and septic patients better tolerate CRRT [21]. Because of these advantages, the popularity of CRRT for the treatment of critically ill patients with renal failure has increased considerably. Major advantages of CRRT use in the ICU setting includes: (1) slower rate of solute or fluid removal per unit of time leading to a steady state fluid equilibrium [22]; (2) improved control of body temperature, fluid, and metabolic balance; (3) continuous control of azotemia, electrolytes, and acid–base balance; (4) continuous removal of fluid in volume overload clinical situations; (5) aid in administration of parenteral nutrition and other fluids without concern for volume excess due to continuous ultrafiltration; and (6) can effectively lower intracranial pressure as opposed to routine IHD which can sometimes raise intracranial pressure [23, 24]. CRRT has also demonstrated removal of circulating inflammatory substances including cytokines, activated components of complement, and derivatives of the arachidonic acid [25–28].

Presently, most equipment that performs CRRT is used exclusively for providing CRRT. A few manufactures offered machines that can provide both intermittent and continuous modalities. However, these machines usually have configuration limitations, are more costly and require dedicated dialysis nursing presence. Because of this, most centers maintain separate equipment for both IHD and CRRT for both logistics and cost.

Indications for CRRT

The indications for CRRT can be separated into renal and non-renal indications. The traditional indication for CRRT in the ICU setting has been ARF complicated by hemodynamic instability [22] and ARF associated with heart failure, volume overload, hypercatabolism, acute or chronic liver failure, and/or brain swelling [29–31]. Non-renal indications include systemic inflammatory response (SIRS), sepsis, multiorgan failure (MOF), and adult respiratory distress syndrome to name a few [32–34]. Table 1 list several non-renal diseases processes that have utilized CRRT as part of the therapeutic regime. Although these therapies do not meet rigorous evidence based standards, this technology is broadening its scope and expanded uses are increasingly reported. It will take some time before enough data accumulates to sparse out efficiency and to define which patient populations may benefit from non-renal uses.

Modes and Principles of CRRT

HD refers to the transport process by which a solute passively diffuses down its concentration gradient from one

Table 1 Reported non-renal indications for CRRT

| |
|-------------------------------|
| SIRS [35] |
| Shock [32] |
| Sepsis [27] |
| MODS [36] |
| Pancreatitis [25] |
| Control of volume status [25] |
| Crush syndrome [37] |
| Acute hepatic failure [37] |

fluid compartment (either blood or dialysate) into the other. During HD, urea, creatinine, and potassium move from blood to dialysate, while other solutes, such as calcium and bicarbonate, move from dialysate to blood. The dialysate flows countercurrent to blood flow through the dialyzer to maximize the concentration gradient between the compartments and therefore to maximize the rate of solute removal. The net effect is the desired changes in the plasma concentrations of blood urea nitrogen and plasma creatinine concentration along with an elevation in the plasma calcium and bicarbonate concentrations.

Hemofiltration (HF) refers to the use of a hydrostatic pressure gradient to induce the filtration (or convection) of plasma water across the membrane of the hemofilter [38]. The frictional forces between water and solutes (called solvent drag) results in the convective transport of small and middle molecular weight solutes (<5000 Da) in the same direction as water [39]. To prevent hypovolemia, any water removed during HF is returned to the blood before it reaches the patient. This is called “replacement” fluid or “substitution” fluid. The process of HF itself removes smaller solutes (such as urea and electrolytes) in roughly the same concentration as the plasma. Therefore, little change in the plasma concentrations of these solutes is seen with HF contrasting those achieved by HD. However, the administration of substitution fluid will lower the plasma concentrations of those solutes by dilution since solutes such as urea and creatinine are not present in the substitution fluid.

Original continuous HD circuits required arterial to venous access sites, because they did not utilize a blood pump to pull blood through the filter. Consequently, they were referred to as continuous arterial–venous (CAV) circuits. Today’s technology uses a blood flow pump; therefore, most continuous circuits are continuous venous–venous (CVV).

The following are the different CVV therapies that can be provided:

SCUF. SCUF is the removal of water from the patient’s blood as it travels through the filter. Water removal is referred to as ultrafiltration. Ultrafiltration is the movement of water across a semi-permeable membrane because of a

pressure gradient (hydrostatic, osmotic or oncotic). The increased blood pressure in the hollow fibers of the filter creates a favorable driving pressure to force water across the membrane.

Blood pressure within the hollow fibers is positive, while the pressure outside the hollow fibers is lower. Increased negativity can be generated outside the hollow fibers by an effluent pump thus increasing the fluid removal rate. The difference between the blood pressure in the hollow fibers and the surrounding pressure is the transmembrane pressure (TMP). The TMP determines the ultrafiltrate production.

Different filter membrane properties can produce different ultrafiltration rates at a constant TMP. A filter that is more permeable to water will allow more water to travel across the membrane at a given TMP. A filter with a high permeability to water is called high-flux membranes (Fig. 1) [40].

CVVH. CVVH is the removal of large amounts of water across the filter membrane for the purpose of clearing wastes. When large volumes of water are washed across the membrane, solutes are dragged along with the water (convection). HF is the removal of water over and above the surplus water removed during ultrafiltration. To prevent hypovolemia, water removed during HF must be given back before the blood is returned to the patient. This is referred to as replacement. CVVH is the use of replacement fluid without dialysis fluid, plus or minus fluid

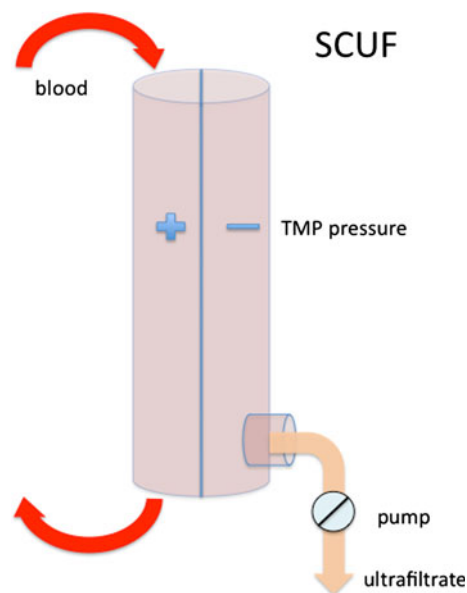


Fig. 1 This diagram shows the basics of SCUF. When blood enters the filter, a TMP gradient is formed by the hydrostatic pressure of the blood and by a negative effluent pressure generated by the effluent pump resulting in ultrafiltration formation

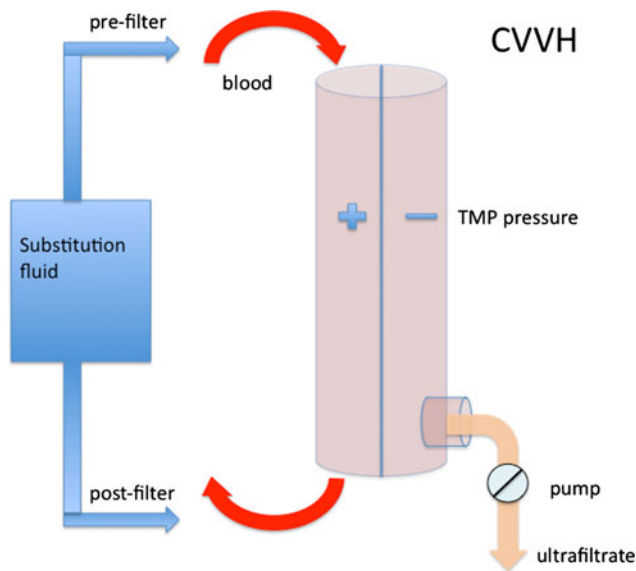


Fig. 2 Configuration of CVVH. The ultrafiltrate is generated as it is in SCUF. However, in CVVH, there is equal amount of fluid put into the circulation. Therefore, there is no net fluid removal. Depending on the equipment used, this fluid can be returned pre- or post-filter or a combination of both

removal (with ultrafiltration, the correct nomenclature would be CVVHF) (Fig. 2).

Continuous venous–venous hemodialysis (CVVHD). CVVHD is the countercurrent infusion of dialysis fluid into the filter canister. The dialysis fluid (dialysate) surrounds the blood filled filter segments. Solutes that are small enough to fit through the membrane of the dialysis filter will move from an area of high concentration to low concentration (diffusion). The dialysate determines the solutes that will be removed. To remove solutes, the concentration in the dialysate is lower than the blood concentration. To give something to the patient, the concentration in the dialysate is higher than the blood. CVVHD is the removal of wastes by diffusion only, without the use of HF (replacement fluid). It can be administered with or without fluid removal from the patient.

CVVHDF. CVVHDF is the use of dialysis and HF. Therapy will include the use of both dialysate and replacement fluids and can be administered with or without fluid removal from the patient (Fig. 3).

Hybrid Therapies

Extended Daily Dialysis

Extended daily dialysis (EDD) is a modality that extends dialysis over a longer than normal period and can be an alternative to CRRT in the ICU. With EDD blood flow

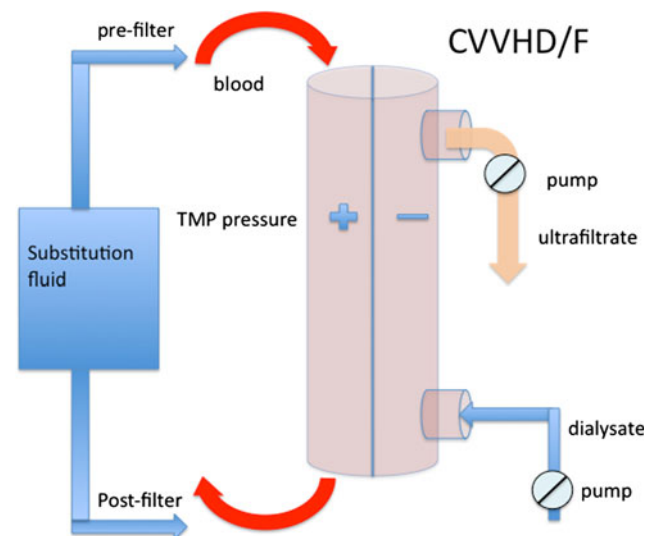


Fig. 3 The configuration for CVVHD and CVVHDF is the addition of counter-current dialysate. This mode utilizes diffusive and convective methods of clearance. If the volume of filtration exceeds the substitution rate (a net negative fluid balance) then the configurations are considered a hemodiafiltration. No net fluid removal CVVHD, net fluid removal CVVHDF

rates are around 200 ml/min with a dialysate flow rate of approximately 300 ml/min for treatment time of 6–8 h. EDD utilizes conventional IHD equipment. EDD in small studies has shown to be safe and effective alternative to CRRT that offers comparable hemodynamic stability and excellent small solute control [40]. EDD uses the principle of diffusion for solute removal. Anticoagulation during the treatment is similar to other modalities. A few reported advantages of EDD include less cumbersome technique, patient mobility, decreased requirements for anticoagulation while providing hemodynamic stability and volume control [41]. In spite of possible advantages, there is insufficient evidence that it offers any clear advantage to the critically ill patient, particularly those with significant hemodynamic compromise.

Slow Low Efficiency Daily Dialysis

Slow low efficiency daily dialysis (SLEDD) is a hybrid technique between CRRT and IHD. It is aimed to reduce rate of ultrafiltration for optimal hemodynamic stability while also providing low efficiency solute removal to minimize solute disequilibrium [42]. SLEDD reportedly provides a sustained treatment duration to maximize dialysis dose but also has periods off therapy that can give an opportunity for therapeutic procedures during scheduled down-time. The disadvantages of SLEDD include lower clearance rates of small and particularly large solutes in comparison to CRRT. SLEDD can be performed using

traditional IHD machines or CRRT machines. The blood flow rate can be set between 50 and 200 ml/min and treatment can last anywhere from 6 to 12 h and can be done nocturnally. There is insufficient data to date to advocate SLEDD over another form of RRT in the ICU setting [43].

Vascular Access

Historically early circuits removed blood from arterial access sites and returned the purified blood via a venous catheter. This promoted blood flow through the filter by utilizing the patients own arterial to venous blood pressure gradient [44]. Advantage to this technique was that there was no pump required and the mean arterial pressure drove the blood into the filter. However, there was increased risk of atheroembolism, ischemia of limb, hematoma formation, hemorrhage, arterial wall injury and spasm of the artery cannulated.

Current CRRT machines have a pump and hence use a veno-venous access. Temporary double-lumen venous dialysis catheters are the most common form of access. They can be inserted quickly at the bedside and used immediately. This method gives rapid and constant blood flow rate, improved dialyzer performance and decreased circuit and dialyzer clotting. Disadvantages include air embolism due to inadvertent disconnection and vein thrombosis and stenosis risk.

Anticoagulation

Anticoagulation is often used to maintain circuit patency. The strategies include systemic anticoagulation and regional anticoagulation. Also, CRRT can be successfully administered without anticoagulation, however, the common strategy is systemic anticoagulation with growing use of regional anticoagulation [45].

Systemic Anticoagulation

Different systemic anticoagulation options include heparin, low-molecular weight heparin (LMWH), nafamostat, prostacyclin, hirudin, argatroban, activated protein C (aPC).

Heparin

Heparin is the most common anticoagulant used for CRRT. Advantages of heparin include low cost, ease of administration, ease of monitoring, short half life, and easily reversible with protamine. Disadvantages include risk of heparin-induced thrombocytopenia, hypoaldosteronism,

dependency of antithrombin III, transaminitis, and hemorrhage [46]. With increased bleeding noted in patients with PTT > 45 s. Strategies include bolus of 2000–5000 units injected into the circuit followed by an infusion of 3–15 units/kg/h to maintain PTT 1.5–2 times upper limit of normal.

LMWH

Advantages of LMWH include lower incidence of HIT, lower affinity for antithrombin III, less platelet activation, constant bioavailability, and less metabolic side effects. Disadvantages include need to monitor anti-Xa levels, which are not readily available, and no reversal agent available for bleeding complications. Goals for anticoagulation are anti-Xa levels between 0.25 and 0.35 U/ml. Their use as an anticoagulant for CRRT is sparse and no recommendation can be made about their use [47, 48].

Prostacyclins

Prostacyclins exert their effects by platelet inhibition. There is inadequate data to suggest use of prostaglandins for anticoagulation in CRRT. However, a few small studies should have efficacy [49, 50]. Disadvantages include cost, vasodilatation, increased ICP, and difficulty in monitoring.

Hirudin

Hirudin is a specific thrombin inhibitor. The safety and efficacy of hirudin as an anticoagulant strategy in CRRT has been demonstrated [51]. Disadvantages include difficulty in monitoring and no effective antidote. It also requires complete dependence on renal function for elimination.

Argatroban

Argatroban is a direct thrombin inhibitor that is cleared by liver. Argatroban has rapid onset and elimination and appears to have a low risk of bleeding. Argatroban is an appropriate alternative in patients with HIT [52]. More studies are being done to look at the safety and efficacy of argatroban. Dosing range is 0.5–2 mcg/kg/min with goal of PTT 1–3 times normal range.

aPC

aPC inhibits and reduces the expression of tissue factor. Anecdotal reports and small studies in patients with sepsis who received aPC and CRRT suggest filter life was equivalent to other forms of anticoagulation [53].

Nafamostat

Nafamostat is a synthetic serine protease inhibitor and works as an anticoagulant by acting on factors IIa, Xa, XIIa and inhibiting TF–VIIa complex [54]. Disadvantages include agranulocytosis, hyperkalemia, and anaphylaxis. It is currently available only in Japan.

Regional Anticoagulation

Heparin–Protamine

In this form of anticoagulation, heparin is administered pre-filter and protamine given post-filter. Overall this has not proved to be an effective strategy [47]. Protamine also has risk of hypotension and anaphylaxis-type reactions.

Citrate-calcium

Regional anticoagulation with citrate is emerging as the most promising of all anticoagulation regimes [55]. Citrate chelates calcium, which decreases extracorporeal iCa^{++} . Citrate is partially removed by CRRT and partially enters the systemic circulation. In systemic circulation iCa^{++} levels rise due to liberation of calcium when citrate is metabolized and from replacement of calcium. Therefore, there is no net effect of systemic coagulation. Administration of citrate is usually based on titration of citrate based on post-filter iCa^{++} (with goal <0.35 mmol/l) or giving a fixed dose of citrate with no monitoring iCa^{++} in the circuit but titrating systemic calcium administration to a serum iCa^{++} of 1.0–1.1 mM [56].

Accumulation of citrate can occur when the ability to metabolize citrate is decreased (i.e., liver failure and decreased tissue perfusion). Clinical consequence includes decreased iCa^{++} , metabolic acidosis, increased anion gap and increased total/ iCa^{++} concentration [57]. It can also occur with unintended citrate over-infusion or decreased removal in case of a decline in membrane performance at constant citrate infusion. Clinical consequences include decreased iCa^{++} and metabolic alkalosis. Other complications of citrate include hypernatremia, hypo- or hypercalcemia, hypomagnesemia, alkalosis, and metabolic acidosis.

No Anticoagulation

CRRT can be successfully performed without the use of anticoagulation. Methods to reduce clotting without using anticoagulation include saline infusions and periodic saline flushes along with reduction in filtration fraction and pre-dilution fluid substitution [58]. Interventions that can

improve success of CRRT without anticoagulation include adequate access flow, minimization of machine stoppage and reduction in filtration fraction [59]. Performing CRRT without anticoagulation can be performed with good results in patients at high risk for bleeding [60].

Filter Technology

Dialysis membranes need to be efficient at clearing wastes, but must also be biocompatible with human blood. Compatibility means that exposure of blood to the dialysis membrane produces minimal adverse effects. Pore size, the number of pores and the thickness of the membrane influence filter permeability. Generally, high-flux membranes which have more or larger pores allow more solutes and ultrafiltrate to move across the membrane. Thinner membranes offer less resistance to solute movement by decreasing the distance the solute must travel across the membrane and also favors increased filtration [61].

Solutes are passed through the membrane according to solute size. Small and mid sized molecules pass across the membrane, without the loss of larger proteins. High-flux membranes that have a larger pore size increase clearance by allowing larger molecules to pass through the membrane, and by allowing more ultrafiltrate flow. The AN69 filter used with some CRRT circuits is a high-flux membrane.

Sieving properties of a membrane describe the membrane's permeability to solutes during ultrafiltration. Permeability of solutes decreases as the molecular size increases. The cut-off point for a membrane is defined by the molecular weight where only 10% of the solute is filtered. Sieving properties are usually expressed as sieving coefficients (S_c). The equation is shown in Fig. 4. Both the AN69 and the polysulfone filters have similar S_c [62].

Adsorption is the ability of larger solutes to adhere to the surface of the dialysis membrane [63]. AN69 filters have strong adsorptive properties including inflammatory mediators [64]. The greatest benefit appears to occur in the first few hours; once the filter becomes saturated with proteins, further removal from the serum is limited [65].

TMP is the pressure exerted on the dialysis membrane during operation and reflects the difference between blood and fluid compartments or essentially the hydrostatic pressure exerted from the blood interface within the filter. An increased TMP and the rate of TMP increase contribute to filter clotting. The greater the pressure drop the more likely there is filter clotting.

$$S = 2C_f/C_{bi} + C_{bo}$$

Fig. 4 The equation to calculate a sieving coefficient for any given substance. S sieving coefficient, C_f concentration in filtrate, C_{bi} concentration in blood inlet to filter, C_{bo} concentration in blood out of filter

Table 2 Listed are peer review article and books on various topics related to CRRT including debates on mode, prescription and other controversies

| Study | Authors | Journal/book |
|---|--|---|
| Intensity of continuous renal replacement therapy in critically ill patients | RENAL Replacement Therapy Study Investigators Bellomo R, Cass A, Cole L, Finfer S, Gallagher M, Lo S, McArthur C, McGuinness S, Myburgh J, Norton R, Scheinkestel C, Su S | N Engl J Med. 2009 Oct 22;361(17):1627–38 |
| Trends in dialysis modality for individuals with acute kidney injury | Afshinnia F, Straight A, Li Q, Slinin Y, Foley RN, Ishani A | Ren Fail. 2009;31(8):647–54 |
| Intermittent versus continuous renal replacement therapy for acute kidney injury patients admitted to the intensive care unit: results of a randomized clinical trial | SHARF investigators Lins RL, Elseviers MM, Van der Niepen P, Hoste E, Malbrain ML, Damas P, Devriendt J | Nephrol Dial Transplant. 2009 Feb;24(2):512–8 |
| Renal replacement therapy in acute kidney injury: intermittent versus continuous? How much is enough? | Bouchard J, Weidemann C, Mehta RL | Adv Chronic Kidney Dis. 2008 Jul;15(3):235–47 |
| A systematic review of continuous renal replacement therapy and intermittent hemodialysis in management of patients with acute renal failure | Ghahramani N, Shadrou S, Hollenbeak C | Nephrology. 2008 Oct;13(7):570–8 |
| Dose and efficiency of renal replacement therapy: continuous renal replacement therapy versus intermittent hemodialysis versus slow extended daily dialysis | Ricci Z, Ronco C | Crit Care Med. 2008 Apr; 36(4 Suppl):S229–37 |
| Intermittent versus continuous renal replacement therapy for acute renal failure in adults | Rabindranath K, Adams J, Macleod AM, Muirhead N | Cochrane Database Syst Rev. 2007 Jul 18;(3):CD003773 |
| Continuous versus intermittent renal replacement therapy in acute renal failure | Ronco C, Brendolan A, Bellomo R | Nephrol Dial Transplant. 1998;13 Suppl 6:79–85 |
| Continuous versus intermittent renal replacement therapy in the intensive care unit | Bellomo R, Ronco C | Kidney Int Suppl. 1998 May; 66:S125–8 |
| Principles of antibacterial dosing in continuous renal replacement therapy | Choi G, Gomersall CD, Tian Q, Joynt GM, Freebairn R, Lipman J | Crit Care Med. 2009 Jul;37(7):2268–82 |
| Metabolic and nutritional aspects of acute renal failure in critically ill patients requiring continuous renal replacement therapy | Wooley JA, Btaiche IF, Good KL | Nutr Clin Pract. 2005 Apr;20(2):176–91 |
| Amino acid requirements in critically ill patients with acute kidney injury treated with continuous renal replacement therapy | Btaiche IF, Mohammad RA, Alaniz C, Mueller BA | Pharmacotherapy. 2008 May;28(5):600–13 |
| Critical care nephrology, 2nd edition | Claudio Ronco, MD, Rinaldo Bellomo, MBBS(Hons), MD, FRACP, FCCP and John Kellum, MD | ISBN: 978-1-4160-4252-5 |
| Acute kidney injury | C Ronco, Rinaldo Bellomo, John Kellum | ISBN 10: 3805582714 ISBN 13: 9783805582711 |

References include discussions of medication dosing, nutrition, the debate over CRRT vs IHD, etc

Conclusion

This is a review of the technical aspects of CRRT. This is only a primer and not an exhaustive review. In Table 2 is a

list of references that explore this technology further and also discuss drug dosing and nutritional support during CRRT. Also, there are references that discuss and review debates that exist between CRRT and IHD.

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