

# Bacterial Colonization of Bone Allografts

## Establishment and Effects of Antibiotics

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Published online: 2 April 2010  
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### Abstract

**Background** Bone grafts are frequently used to supplement bone stock and to establish structural stability. However, graft-associated infection represents a challenging complication leading to increased patient morbidity and healthcare costs.

**Questions/purposes** We therefore designed this study to (1) determine if increasing initial *S. aureus* inoculation of bone allograft results in a proportionate increase in colonization; (2) assess if antibiotics decrease colonization and if antibiotic tethering to allograft alters its ability to prevent bacterial colonization; and (3) determine if covalent modification alters the allograft topography or its biological properties.

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One of more of the authors have received grants from the National Institutes of Health (grants DE-13319 [CSA], DE-10875 [CSA], and AR-051303 [CSA, NJH, JP]) and the Department of Defense (grant DAMD17-03-1-0713 [CSA, NJH, JP]), and Musculoskeletal Transplant Foundation for this study. The results presented are not the statement or policy of the funding agencies.

Each author certifies that his or her institution approved or waived approval for the use of human material for this investigation and that all investigations were conducted in conformity with ethical principles of research.

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**Methods** Allograft bone and vancomycin-modified bone (VAN-bone) was challenged with different doses of *S. aureus* for times out to 24 hours in the presence or absence of solution vancomycin. Bacterial colonization was assessed by fluorescence, scanning electron microscopy (SEM), and by direct colony counting. Cell density and distribution of osteoblast-like cells on control and modified allograft were then compared.

**Results** Bacterial attachment was apparent within 6 hours with colonization and biofilm formation increasing with time and dose. Solution vancomycin failed to prevent bacterial attachment whereas VAN-bone successfully resisted colonization. The allograft modification did not affect the attachment and distribution of osteoblast-like cells.

**Conclusions** Allograft bone was readily colonized by *S. aureus* and covered by a biofilm with especially florid growth in natural topographic niches. Using a novel covalent modification, allograft bone was able to resist colonization by organisms while retaining the ability to allow adhesion of osteoblastic cells.

**Clinical Relevance** Generation of allograft bone that can resist infection *in vivo* would be important in addressing one of the most challenging problems associated with the use of allograft, namely infection.

### Introduction

Surgeons are frequently faced with reconstruction challenges caused by bone loss [30]. Although autologous bone is the gold standard for bone restoration, donor site morbidity and limited bone volume [1, 6] have led to increased utilization of allograft bone. Approximately 800,000 bone allograft transplantations are performed yearly in the

United States, making bone the second most commonly transplanted tissue [7] (exceeded only by blood). Unfortunately, after more than 50 years of research into synthetic tissue substitutes, none of these bone substitutes yet match the unique fibrous and mineral composition of bone [13].

Although bone allograft generally restores bone mass [19], complications such as graft-host nonunion, fracture, and graft infection [5] are not infrequent. Allograft-associated infection often requires removal of infected bone and extensive débridement of the affected site [32], with substantial patient morbidity. Most of these allograft-associated infections occur early (within 4 months) [29, 37], and despite extended antibiotic prophylaxis [31], the reported incidence remains at 4% to 12% [29]. Like metallic implants, allografts act as highly porous, noncellular, and avascular foreign bodies that are prone to bacterial adhesion. Once bacteria attach, they secrete a thick glycocalyx matrix rendering them inaccessible to immune surveillance and local cellular defense mechanisms [39].

To better understand bacterial colonization of bone grafts, we determined whether (1) increasing initial *S. aureus* inoculation of bone allograft results in a proportionate increase in colonization; (2) addition of antibiotics to solution decreases allograft colonization; and (3) covalent tethering of antibiotic to allograft alters its ability to prevent bacterial colonization; (4) covalent modification altered the topography of the allograft or its biological properties in allowing osteoblast-like cell adhesion.

## Materials and Methods

The experimental design was performed three independent times (Fig. 1). Briefly, in order to characterize bacterial colonization of allograft, morselized bone was challenged with *S. aureus* ( $C_i = 10^2$ – $10^5$  cfu) for 6 hours, and sonicated to suspend adherent bacteria that were then plated and counted. We then asked if adding antibiotics to the solution would eradicate adherent *S. aureus* colonization. Morselized bone was challenged with *S. aureus* in (1) trypticase soy broth (TSB) alone; (2) TSB followed by addition of vancomycin (VAN) at 12 hours; or (3) TSB in the presence of VAN, and adherent bacteria were counted. The progression of bacterial attachment was also directly visualized on cortical bone stubs in the presence of TSB (control) or TSB + VAN. Control and vancomycin-modified bone (VAN-bone), were examined by SEM to allow assessment of any gross morphological changes in surface topography associated with the chemical modification process. The efficacy of VAN-bone to resist colonization was evaluated by challenging both control and VAN-bone

with *S. aureus* for 12 hours and visualization by confocal laser scanning microscopy after staining with the Live/Dead BacLight™ kit (Invitrogen, Carlsbad, CA); or by SEM following fixing. Finally, the distribution of human fetal osteoblastic cells (hFOBs) that had been cultured on control and VAN-bone cortical squares for 48 hours were examined by confocal microscopy as a preliminary indication of toxicity/biocompatibility of the surfaces.

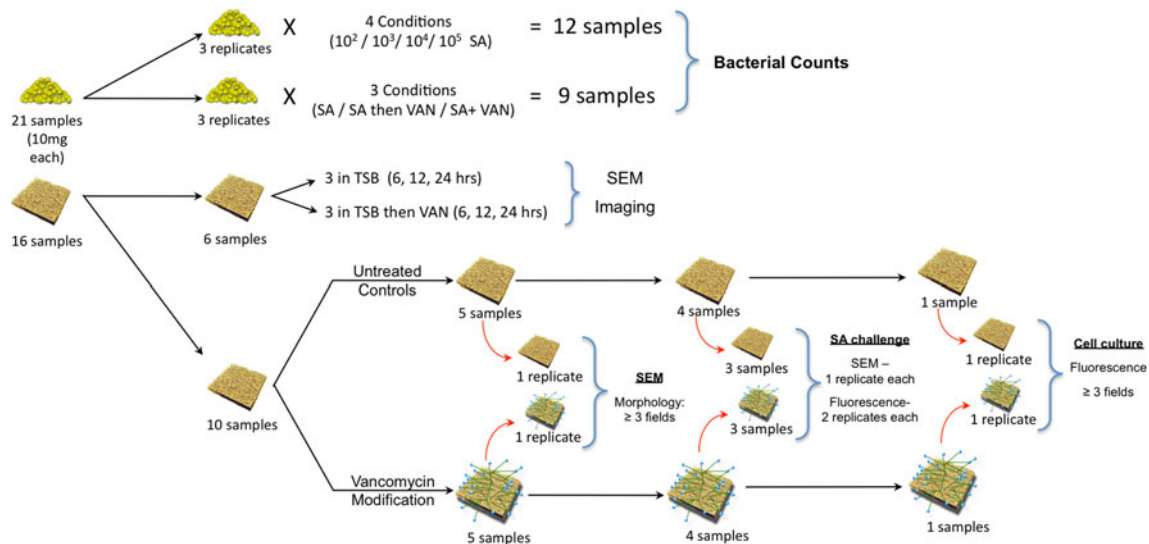
Three cortical stubs or morselized human allograft bone were obtained from the Musculoskeletal Transplant Foundation. Cortical bone was cut into 1 × 1-cm squares using a high-speed cutter (Dremel: Racine, WI), washed, and sonicated with dH<sub>2</sub>O until washings were clear. Samples were partially demineralized by incubation with 12.5% EDTA, pH 7, 37°C for 3 days with shaking; EDTA was replaced daily. Before synthesis, all samples were washed with dH<sub>2</sub>O and sonicated twice for 30 minutes in dimethylformamide (DMF; Acros Organics, Morris Plains, NJ).

Washed cortical bone stubs were coupled twice with 10 mg/mL Fmoc-[2-(2-amino-ethoxy)-ethoxy]-acetic acid (Fmoc-AEEA) followed by chemical coupling with 10 mg/mL clinical grade VAN (American Pharmaceutical Partners, Inc, Schaumburg, IL) as described previously for bone (Ketonis et al., manuscript under review) and metal alloys [3, 16, 25]. The modified bone was washed extensively with DMF and incubated in dH<sub>2</sub>O for at least 5 days before use. Presence of VAN was confirmed by reaction with a specific anti-VAN antibody (US Biologicals, Swampscott, MA).

Control or VAN-bone was sterilized with 70% ethanol for 15 minutes and washed three times with PBS and three times with TSB. *S. aureus* (Xen36 derived from ATCC 49525; Caliper Life Science, Hopkinton, MA) were cultured in TSB, 250 rpm, 37°C, 12 to 14 hours (overnight culture), followed by dilution using a 0.5 McFarland (a turbidity standard with approximately  $1 \times 10^8$  cfu/mL when  $A_{600} = 0.10$ ). Bacteria were incubated with the sterilized samples in TSB, 37°C, under static conditions for 6 to 24 hours.

To determine colonization as a function of bacterial dose, sterilized morselized bone (10 mg) was incubated with bacteria ( $C_i = 10^2, 10^3, 10^4$  or  $10^5$  cfu) for 6 hours in TSB, 37°C, under static conditions. Samples were washed three times with PBS, transferred to Eppendorf tubes, briefly vortexed, and washed three more times with PBS to remove nonadherent bacteria. To suspend the adherent bacteria, samples were sonicated in 0.3% Tween-80, 5 minutes, and after serial dilution, plated on 3 M® Petri-films (St. Paul, MN) and incubated overnight at 37°C. Films were digitally counted using a macro in Adobe Photoshop CS3 (San Jose, CA).

To test the efficacy of solution antibiotic in preventing bacterial colonization,  $1 \times 10^4$  cfu *S. aureus* were



**Fig. 1** The experimental flow diagram is shown. A total of 21 morselized bone samples were used to quantitatively assess bacterial growth on bone as it varies with initial bacterial dose (12 samples) and addition of solution antibiotics (nine samples). Sixteen (16) cortical bone samples were then used to qualitatively assess the temporal colonization of bone surfaces in the presence or absence of

solution antibiotics (six samples). Half of the remaining 10 samples were modified with vancomycin and half were used as controls for morphological assessment, visualization of SA colonization by SEM and fluorescence and toxicity determination by mammalian cell culture. All experiments were repeated at least three independent times. SA = Staphylococcus aureus.

incubated with (1) TSB, 12 hours, TSB 4 hours; (2) TSB, 12 hours, TSB + 10  $\mu\text{g}/\text{mL}$  VAN, 4 hours; (3) TSB + 10  $\mu\text{g}/\text{mL}$  VAN, 12 hours, TSB, 4 hours. Adherent bacteria were plated or imaged. Imaging of cortical stubs was performed on bone squares that had been challenged with *S. aureus* for 6, 12, or 24 hours in TSB, 37°C, washed thoroughly to remove nonadherent bacteria, and reincubated in a fresh plate containing either TSB (control) or TSB + VAN. After 3 hours, samples were thoroughly washed with PBS to remove nonadherent bacteria and were either stained with the Live/Dead BacLight™ Kit (Invitrogen, Carlsbad, CA; 20 minutes, room temperature) and visualized with confocal laser microscopy or prepared for visualization by SEM. Areas of surface colonization were determined from multiple fluorescent images analyzed using ImagePro (Media Cybernetics, Inc, Bethesda, MD).

Control and VAN-modified cortical bone squares (1 cm  $\times$  1 cm) were sterilized with 70% ethanol, rinsed three times with PBS, three times with DMEM/F-12 containing 10% FBS (full media), and exposed to ultraviolet radiation for 10 minutes. The sterilized samples were incubated with 1 mL of 5  $\times 10^4$  cells/mL hFOBs [22] in full media for 48 hours, stained with CellTracker (Invitrogen, Carlsbad, CA; 1  $\mu\text{M}$ , 30 minutes) and visualized using confocal laser microscopy.

Bacterially-colonized control or VAN-modified cortical bone squares (1 cm  $\times$  1 cm) were thoroughly washed with dH<sub>2</sub>O and fixed for 1 hour with 4% paraformaldehyde. Samples were sequentially dried with a graded ethanol

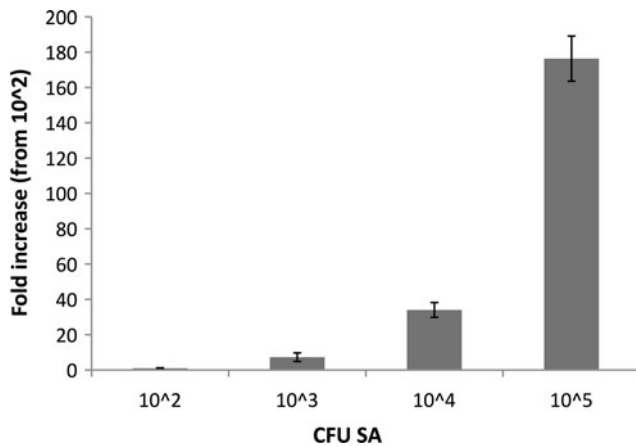
series, incubated in Freon, and vacuum-dried overnight. Samples were then affixed onto a metal plate, sputter-coated with gold, and visualized using a Hitachi TM-1000 SEM (Ibaraki, Japan).

All experiments (Fig. 1) were performed independently at least three times. Data are presented as means  $\pm$  standard errors. All statistical analyses were performed on normal equally variant data using a one or two-way analysis of variance (ANOVA) with a Tukey multiple comparison procedure.

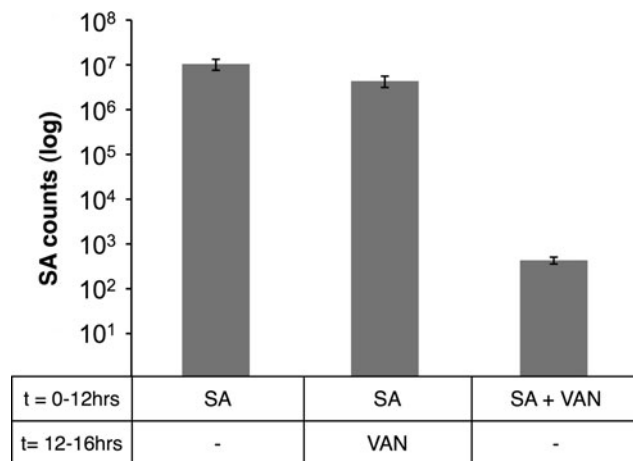
## Results

Increasing inocula resulted in increased colonization, with no apparent plateau under our study conditions. Bacteria added to solution proliferated over time so that an initial inoculate of 1  $\times 10^2$  cfu yielded approximately 4  $\times 10^4$  cfu after 6 hours incubation, whereas 1  $\times 10^5$  cfu resulted in yield of approximately 7.6  $\times 10^6$  cfu, an almost 200-fold increase (Fig. 2).

Addition of VAN to solution only partially prevented bacterial proliferation. Addition of VAN for 4 hours following bacterial attachment on the bone morsels, resulted in a marginal reduction in colonization as compared to control samples without VAN. Bacterial colonization, though reduced, still occurred even when VAN was added concurrently with the bacterial inoculum (Fig. 3). By microscopy, individual bacteria as well as biofilm



**Fig. 2** The colonization of allograft by *Staphylococcus aureus* is shown. Morselized bone squares were challenged with increasing numbers of *S. aureus* for 6 hours. Small increases in initial bacterial inoculates resulted in a much more robust colonization at the end of the incubation period. Numbers of colonizing bacteria are expressed as fold change relative to the 10<sup>2</sup> inoculum.



**Fig. 3** Effects of the addition of 10 µg/mL vancomycin (VAN) on bacterial colonization are illustrated. Morselized bone was colonized with trypticase soy broth (TSB) ± VAN using the schedule indicated under the bars showing that only a small reduction is achieved in colonization by solution antibiotics. Error bars = Standard error.

formation were evident on the surface of the cortical bone squares at 6 hours (Fig. 4A), which progressed to bacterial aggregates (Fig. 4B) consequently to mature biofilm with its characteristic reticulate honeycomb appearance (Fig. 4C). When incubated for an additional 3 hours in the presence of 10 µg/mL VAN (~5–10 times the MIC), bacterial colonization was still abundant on the bone surface at all time points (Fig. 4D–F: 6–24 hrs). By SEM, these VAN-treated, colonized surfaces showed individual grape-like clusters of bacteria (Fig. 4D–F, arrows) as well as mature biofilms (Fig. 4E–F, asterisks) that formed despite the presence of VAN in solution.

The endosteal surface of the bone pieces from the cortical stub squares was sanded until flat and VAN linked to the primary amines displayed on the ECM proteins of bone allograft (Fig. 5A–B). Covalent tethering of VAN to allograft did not alter the surface topography as seen by SEM (Fig. 5C–D). The microarchitecture of modified and control bone appeared similar by containing a dense collagen fiber meshwork, osteocytic lacunae with the Haversian and Volkmann's canals being preserved.

*S. aureus* readily colonized control bone ( $C_i = 10^4$  cfu, 12hrs), as evidenced by multiple green foci (Live/Dead stain, live bacteria fluoresce green), with patchy areas of abundant stain uptake indicative of biofilm. Using the same conditions, VAN-bone showed little evidence of microcolony formation; a few fluorescent green trails were apparent that are likely the result of stain trapping in the crevices of the bone surface (Fig. 6A). Morphometric analysis of multiple such images revealed that bacterial coverage on VAN-allograft surfaces was less ( $p < 0.001$ ) than that of controls (0.8% of controls) (Fig. 6B).

By SEM, control bone surfaces were covered with multiple colonies of *S. aureus* (Fig. 7A, control). At higher magnifications, these colonies organized into grape-like clusters (Fig. 7B–C). Planar surfaces were also covered with a slimy material characteristic of biofilm (Fig. 7D). Within this biofilm, multiple small spherical bacteria (diameter 0.3–1 µm) can be distinguished, representing entrenched *S. aureus*. At higher magnification, in areas where the biofilm was more mature, biofilm budding was seen as bright white features [20] (Fig. 7E–F). Natural topographic niches such as Haversian and Volkmann's canals seemed to be a nidus for bacterial aggregation, and examination of these structures at higher magnification showed that they were consistently populated with *S. aureus* colonies that extended into the canals (Fig. 7G–I). In contrast, the surface of the VAN-bone appeared free of bacterial colonies even within Haversian/Volkmann's canals (Fig. 7J–L).

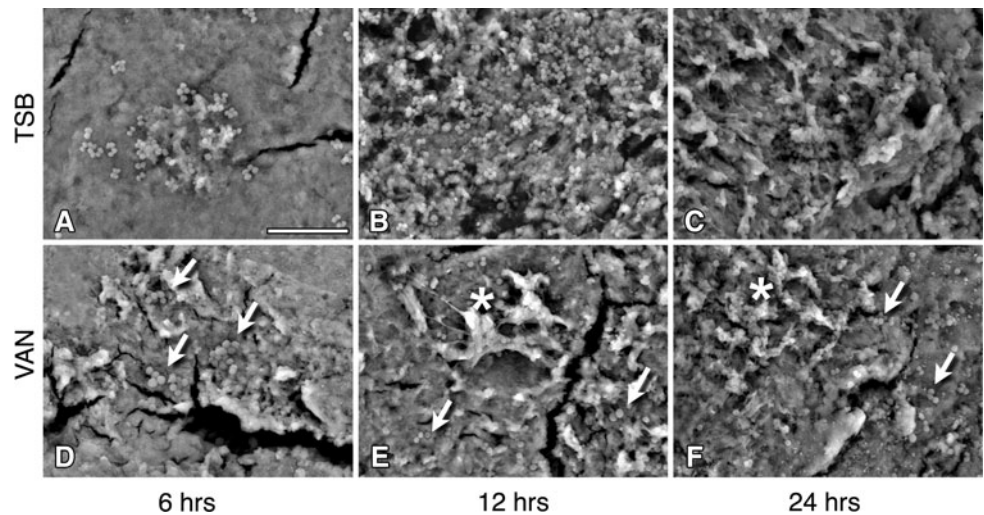
Human fetal osteoblast-like cell cultured on VAN-allograft (48 hrs) retained normal morphology and distribution. Cell shape and distribution were very similar between the control and VAN-modified allograft with cells appearing to align along the underlying collagenous matrix (Fig. 8). Cell density appeared similar on both the control and VAN-bone, suggesting the VAN-bone is sufficiently like the parent bone substrate to support bone ingrowth.

## Discussion

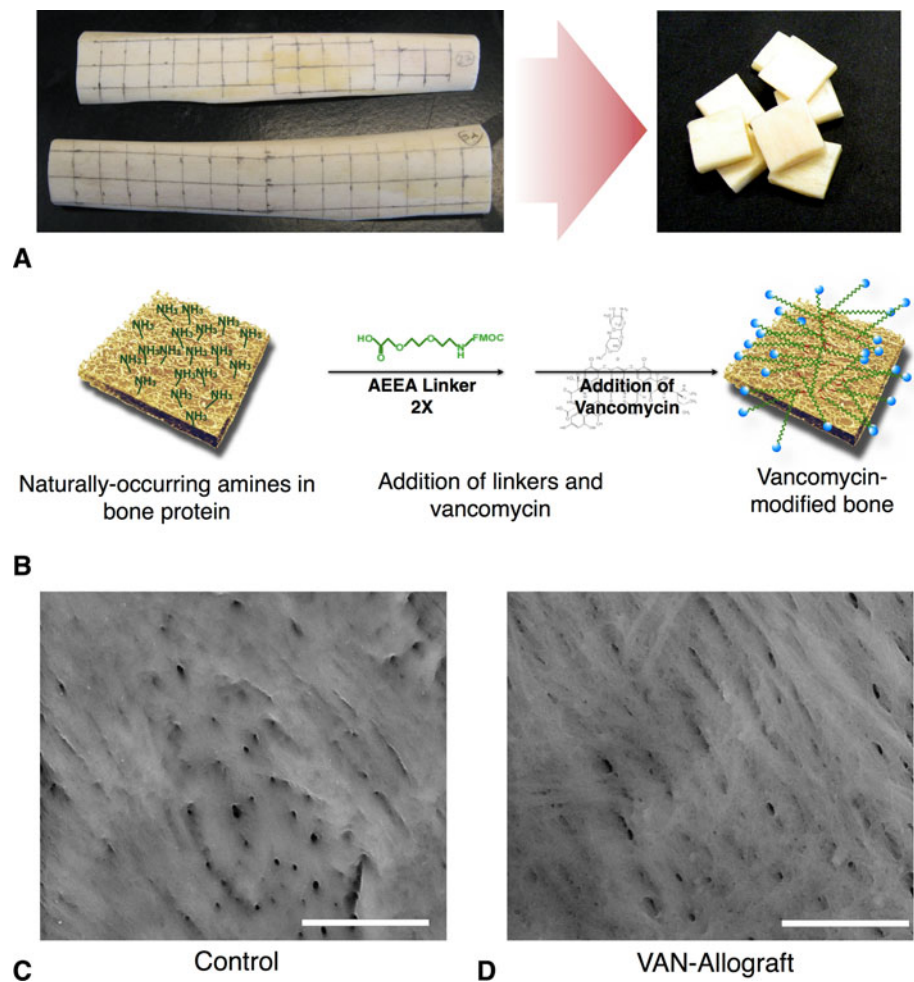
Allograft bone is used frequently to replenish bone loss that may be encountered during revision joint arthroplasty [30]. With the rise in the number of complex revision



**Fig. 4A–F** Surface colonization by *S. aureus* is shown. (A) Control cortical allograft was challenged for 6 to 24 hours with *S. aureus* and reincubated in TSB (A–C) or TSB in the presence of 10 µg/mL VAN (D–F) for an additional 3 hours. The micrographs show a gradual increase in biofilm generation and how it matures over time. Note the reticulate and characteristic honeycomb appearance entrenching most of the bacteria present and protecting them from solution antibiotics. Scale bar: 10 µm; arrows = bacterial clusters; asterisks = biofilm.



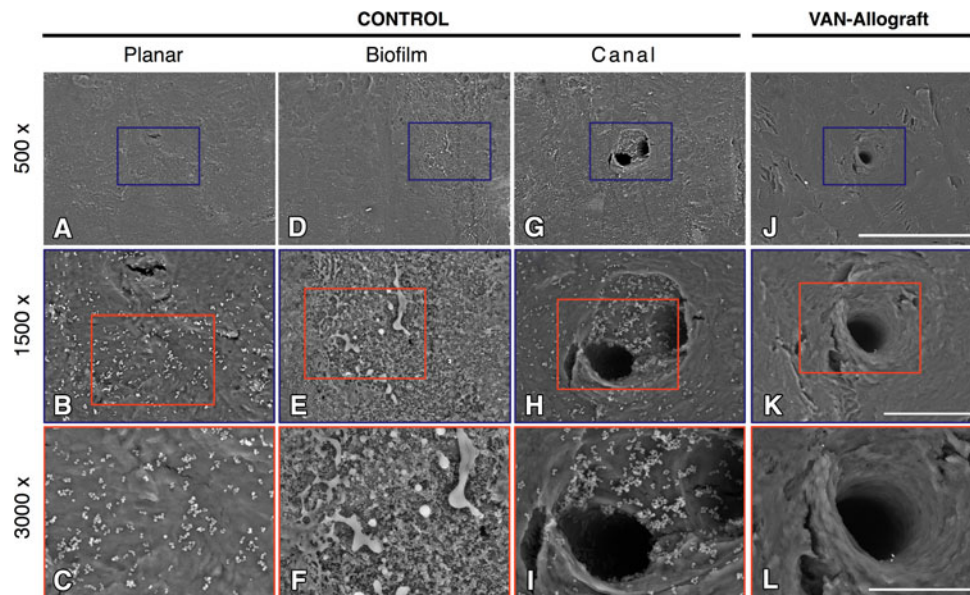
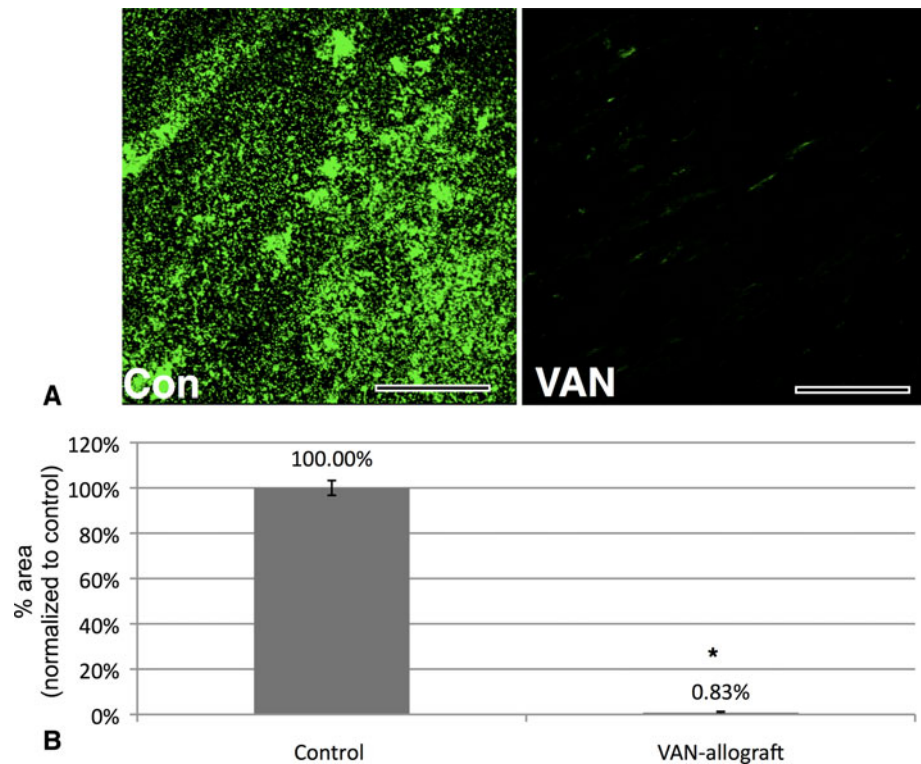
**Fig. 5A–D** Preparation of bone squares is illustrated. (A) Cortical stubs from human cadaveric tibias were supplied by the Musculoskeletal Transplant Foundation, washed, and marked into squares measuring 1 × 1 cm. Each cortical stub yielded between approximately 20 and 30 squares. (B) A high-speed cutter (Dremel) was used to cut the marked tibias into individual 1 × 1-cm squares that were further washed and processed. The endosteal surface of the bone pieces was sanded until flat making the thickness of each piece approximately 2 to 3 mm; a cartoon is shown of the synthetic scheme for attachment of vancomycin (VAN) (through two aminoethoxyethylacetate [AEEA] linkers) to the primary amines displayed on the ECM proteins of bone allograft. (C–D) Scanning electron microscopy analysis of bone following VAN coupling is shown. Note that the gross topography was unchanged between control (C) and modified bone (D) with preservation of the collagenous meshwork and the natural crevices and capillary canals. Scale bar: 10 µm.



arthroplasty cases and the increase of aging population, the demand for bone grafts will continue. Worldwide, bone grafts are used in approximately 2.2 million orthopaedic procedures annually, generating a \$2.5 billion per year industry [14]. Unfortunately, the prevalence of allograft-

related infection rates remains relatively high with a reported incidence of 4% to 12% compared to periprosthetic joint infection rates of 1% to 3% [11, 26, 41]. This study was designed to investigate the phenomenon of allograft infection by conducting a series of experiments.

**Fig. 6A–B** VAN-bone prevents bacterial colonization. (A) After 12 hours incubation with *S. aureus*, control bone (Con) shows green punctate staining (adherent bacteria), with larger areas of intense staining indicating biofilm presence. Note that minimal staining was seen on the VAN allograft with only occasional trails of stain trapped in the underlying crevices of the bone. Scale bar: 100  $\mu\text{m}$ . (B) Morphometric analysis shows that the total area covered on VAN-bone is smaller. Total colonized area is expressed as a percentage of controls. (\* =  $p < 0.001$ )



**Fig. 7A–L** SEM assessment of colonization is shown. Control surfaces were abundantly colonized with bacteria (CONTROL) after 12 hours. At low magnification on the planar surfaces (A), small white dots are evident that, at higher magnifications (B–C), resolve into multiple colonies of bacteria that populate the surface in grape-like clusters. On other areas, reticulated biofilm (D) is evident which at higher magnification (E–F) can be distinguished as a thick layer of slimy material with multiple small spherical bacteria (diameter 0.3–1

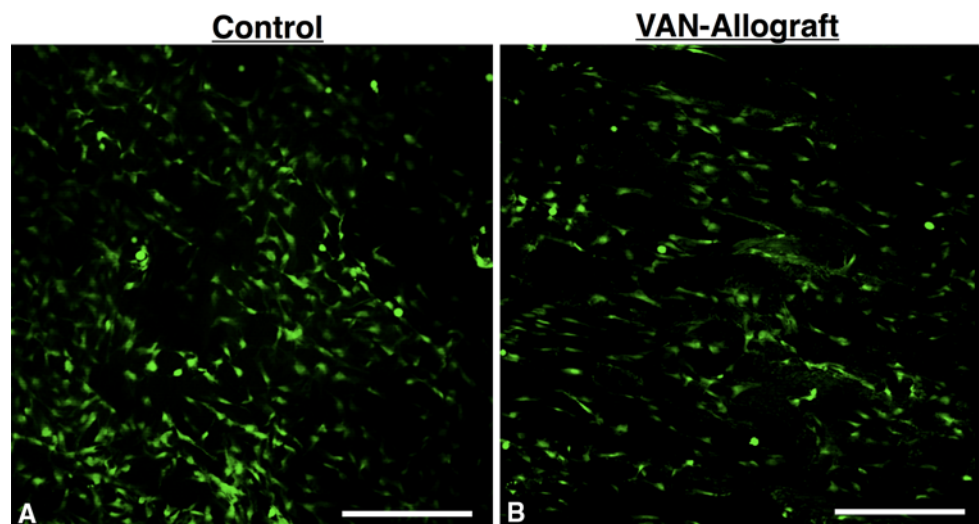
$\mu\text{m}$ ) representing biofilm entrenched *S. aureus* colonies. Natural topographic niches such as Haversian and Volkmann's canals (G) at low magnifications showed no apparent colonization. However, at higher magnifications, they were consistently filled with *S. aureus* (H) that at 3000x (I) were seen deep into these canals. The surface of the VAN-allograft appeared free of bacterial colonies on all surfaces at any magnification (J–L). Scale bars: A, D, G, J = 200  $\mu\text{m}$ ; B, E, H, K = 50  $\mu\text{m}$ ; C, F, I, L = 30  $\mu\text{m}$ .

We determined if (1) increasing initial *S. aureus* inoculation of bone allograft resulted in a proportionate increase in colonization; (2) addition of antibiotics to solution could

decrease allograft colonization; (3) covalent tethering of antibiotic to allograft altered its ability to prevent bacterial colonization; and (4) covalent modification altered the



**Fig. 8A–B** Cell morphology on control and vancomycin (VAN)-bone surfaces. Human fetal osteoblastic (hFOBs) cells were stained with CellTracker Green after culturing for 48 hours on control and VAN-bone. Abundant hFOBs attached to both control (A) and VAN-bone (B) surfaces showed normal morphology and exhibited a similar distribution and density. Scale bar: 400  $\mu\text{m}$ .



topography of the allograft or its biological properties in allowing osteoblast-like cell adhesion.

The most important limitation of this study is that it is an *in vitro* attempt to describe an *in vivo* phenomenon. As a result, it necessarily deals with the time frames and ideal environment associated with bacterial colonization under laboratory conditions. Second, much of the data that we present depends on visual assessment of bacterial colonization on surfaces. With the special properties of adherent/biofilm bacteria, detection of these bacteria using the stains and SEM, as we have described, are methods that circumvent the need for biofilm dissolution and bacterial detachment required for accurate counts and are thus, of necessity, observational. However, these methods can only sample limited areas on the surface and hence cannot offer the assurance that there are not pockets of allograft that appear different. Unfortunately, currently available more quantitative methods, ie, resuspension of adherent bacteria and subsequent plating are plagued by problems such as poor recovery of bacteria [34]. Third, we assessed colonization by one organism and one antibiotic construct. In a situation where infection is establishing, it may not be rare to find multiple microorganisms. We limited the experimental design to the most common infecting organism, namely *Staphylococcus aureus*, which we believe represents a “model organism” for allograft associated infections. However, we acknowledge other organisms may behave differently. Fourth, the concentrations of vancomycin used for addition to solution was based on our experience with these experiments over the past few years and appears to be  $\sim 10\times$  the MIC for the planktonic *S. aureus*. It was our aim to stay within clinically useful levels while avoiding concentrations that could become toxic to mammalian cells.

We found small increases in initial bacterial inoculate resulted in a disproportionately large increase in bacterial

colonization of allograft surfaces. The bacteria readily attached to, and colonized, cortical allografts *in vitro*. From our subsequent electromicrograph analysis, it appears that bacterial colonization was potentiated by the porous nature of bone that provides bacteria with topographically protected niches where they can attach, proliferate, and form a mature biofilm. Successful bacterial colonization can be achieved with very small inoculate sizes when foreign bodies are present [23]. For example, the initial inoculate of bacteria required to infect an incision site decreases by 4 logs when sutures are in place [17]. In our experiments, colonization was achieved on bone with the lowest inoculate tested (100 cfu) and the attached bacteria harvested dramatically increased for every subsequent 10-fold increase in dose. However, a much higher inoculum of  $10^4$  cfu was chosen to challenge the modified allograft in order to capture the clinical scenario when larger number of bacteria may be present.

Systemic or local antibiotics alone are unlikely to eradicate an established infection around a prosthesis or an allograft [12]. We attempted to recapitulate this situation through introduction of antibiotics after establishment of bacterial colonization on the allograft. As observed clinically, these bathing antibiotics, while clearing the nonadherent bacteria, were unable to affect the adherent bacteria, much of which remained encased in a biofilm slime. Importantly, bacteria were able to attach to bone surfaces even when inoculated in an antibiotic-rich medium. Electron microscopy demonstrated that *S. aureus* attached and initiated biofilm formation on cortical allografts within 6 hours. By 12 and 24 hours, the surface was covered with the thick biofilm glycocalyx, entrenching and protecting the underlying bacteria from environmental challenges including solution antibiotics [21, 33, 35]. We suggest *in vivo* colonization of allografts during establishment of infection can occur preferentially in protected

niches, although the timeframe of these events is likely to be longer than what we describe here. To prevent establishment of infection during the immediate postsurgical period, prophylactic antibiotic regimens have been adopted that involve the administration of antibiotics intravenously for 2 to 14 days and orally for up to 16 weeks [15, 24, 29]. Similarly, to prevent initial infection, physicians have empirically impregnated bone allografts with antibiotics before implantation, achieving high local concentrations of antibiotic during the initial elution [8]. Our *in vitro* data support these processes, and even though they are important means to prevent establishment of infection, they are imperfect. Unfortunately, as with supplementation of PMMA cement with antibiotics, elution kinetics from allograft are largely variable, in which high local antibiotic concentrations can have deleterious effects on host cells thereby retarding graft incorporation. Additionally, once antibiotic is depleted, the graft is again susceptible to bacterial colonization. Therefore, although use of allograft has yielded excellent results, its use in cases of infection has been controversial as a result of the possible increased risk of reinfection [8, 9, 18].

In an attempt to address these problems, we turned to an antibiotic-modified cortical allograft as an approach to providing an antibacterial surface that would effectively resist infection. Despite subjecting the modified allograft to bacterial inoculate three to four orders of magnitude higher than what one expects to encounter in a clinical scenario [4, 17], the allograft exhibited excellent efficacy in preventing colonization by *S. aureus*. The process of modification did not appear to affect the microarchitecture of bone or its biological activity, at least based on limited cellular adhesion studies that were performed here. The surface demineralization that we used is not uncommon in allograft preparations and reportedly enhances bone incorporation and ingrowth [27, 28]. The solvents used during the chemical modification also appeared to access the niches and allow coupling of allograft throughout.

The observation that osteoblast-like cells were able to adhere to the surface of the modified allograft as readily as the control allograft is encouraging. Previous experiments in our laboratory and those of others have shown antibiotics in higher concentrations can have deleterious effects on mammalian cells [2, 40]. Therefore, toxicity studies must be performed with the introduction of any novel bioactive construct or drug delivery system [10, 36, 38]. When the cells on our antibiotic-laden construct were visualized, careful observations failed to identify any differences among their density, morphology, distribution, and cell–cell associations on either control or VAN-modified allograft. Although a detailed assessment of biocompatibility, including measurements of osteoblastic maturation, is required to fully characterize the effect of the

VAN-surface on osteoblastic function, these initial findings are suggestive that the VAN-bone should be biocompatible. Furthermore, because the antibiotic is permanently bonded to the surface of the allograft, no systemic toxicity is expected *in vivo*.

**Acknowledgments** We thank the Musculoskeletal Transplant Foundation for providing samples for this work as well as for their generous support of these studies.

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