## **SI: PACIFIC RIM 2020**



# **Longitudinal changes of focal cortical glucose hypometabolism in adults with chronic drug resistant temporal lobe epilepsy**

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Accepted: 29 September 2021 / Published online: 20 October 2021 © The Author(s), under exclusive licence to Springer Science+Business Media, LLC, part of Springer Nature 2021

## **Abstract**

A high proportion of patients with drug-resistant temporal lobe epilepsy (TLE) show focal relative hypometabolism in the region of the epileptogenic zone on [<sup>18</sup>F]-Fluorodeoxyglucose positron emission tomography (FDG PET). However, whether focal (hypo)metabolism changes over time has not been well studied. We analysed repeated [<sup>18</sup>F]-FDG PET scans of patients with TLE to determine longitudinal changes in glucose metabolism. Adults  $(n=16; 9$  female, 7 male) diagnosed with drug resistant chronic TLE were assessed. Each patient had two [<sup>18</sup>F]-FDG PET scans that were 2–95 months apart. Region-ofinterest analysis was performed on MR images onto which PET scans were coregistered to determine the relative [<sup>18</sup>F]-FDG uptake (normalised to pons) in the bilateral hippocampi and temporal lobes. Statistical Parametric Mapping analysis investigated global voxel-wise changes in relative metabolism between timepoints. Normalised [<sup>18</sup>F]-FDG uptake did not change with time in the ipsilateral (baseline  $1.14 \pm 0.03$ , follow-up  $1.19 \pm 0.04$ ) or contralateral hippocampus (baseline  $1.18 \pm 0.03$ , follow-up  $1.19\pm0.03$ ). Uptake in the temporal neocortex also remained stable (ipsilateral baseline  $1.35\pm0.03$ , follow-up  $1.30\pm0.04$ ; contralateral baseline  $1.38\pm0.04$ , follow-up  $1.33\pm0.03$ ). The was no relationship between change in uptake on the repeated scans and the time between the scans. SPM analysis showed increases in metabolism in the ipsilateral temporal lobe in 2/16 patients. No areas of decreased metabolism concordant to the epileptogenic zone were identified. [<sup>18</sup>F]-FDG uptake showed no signifcant changes over time in patients with drug-resistant TLE. This suggests that repeating FDG-PET scans in patients with subtle or no hypometabolism is of low clinical yield.

**Keywords** Temporal lobe epilepsy · Glucose hypometabolism · [<sup>18</sup>]fluorodeoxyglucose · FDG · Positron emission tomography

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## **Introduction**

Temporal lobe epilepsy (TLE) is the most common form of focal epilepsy in adults and is estimated to account for the highest proportion of drug-resistant cases (Stephen et al., [2001\)](#page-8-0). 70–89% of patients with drug-resistant TLE have focal glucose hypometabolism in the region of the epileptogenic zone detected on  $[{}^{18}F]$ -fluorodeoxyglucose (FDG) positron emission tomography (PET) (Benedek et al., [2006](#page-7-0); Gaillard et al., [1995](#page-8-1); O'Brien et al., [2001,](#page-8-2) [2008](#page-8-3); Spencer, [1994](#page-8-4)). [ 18F]-FDG PET is particularly useful in cases of MRI negative focal epilepsy, and depending on the sensitivity and scanner resolution this method can detect focal and regional hypometabolism in 80% of patients (Carne et al., [2004](#page-7-1); Engel, [1984](#page-8-5); Engel et al., [1990;](#page-8-6) Gaillard et al., [1995](#page-8-1); O'Brien et al., [2001](#page-8-2), [2008;](#page-8-3) Theodore et al., [1983](#page-8-7)), which is predictive of a good outcome following resective epilepsy

surgery (Carne et al., [2004;](#page-7-1) O'Brien et al., [2001](#page-8-2), [2008](#page-8-3)), thus reducing the need for invasive intracranial EEG recording (Theodore et al.,  $1983$ ). The extent of  $[^{18}F]$ -FDG-PET hypometabolism can also be used to predict surgical outcome (Vinton et al.,  $2007$ ). Despite the central role  $[{}^{18}F]$ -FDG PET imaging plays in the diagnosis and the pre-surgical evaluation of focal epilepsy, there are limited data regarding the progression of these metabolic abnormalities over time.

It has been shown that increasing epilepsy duration is strongly associated with a reduction in the volumes of temporal lobe structures (Goncalves Pereira et al., [2005](#page-8-9)), a trend that can be augmented in patients with familial mesial TLE (Conz et al., [2011\)](#page-8-10). Conficting evidence exists for whether these changes are dependent on seizure frequency (Conz et al., [2011;](#page-8-10) Theodore, [2003\)](#page-8-11)**.** Although the serial MRI fndings indicate progressive structural atrophy, few studies have investigated whether similar evolution of brain metabolism can be observed in patients with chronic TLE. The reasons for this are manifold, and include limited access to PET, risks associated with radiation exposure and fnancial considerations, and patients proceeding to resective epilepsy surgery following the initial pre-surgical PET scan.

Several studies have suggested that metabolic abnormalities observed in epilepsy are associated with repeated seizures. Jokeit and colleagues demonstrated a positive correlation between epilepsy onset, duration and hypometabolism (Jokeit et al., [1999\)](#page-8-12). Furthermore, only a small number of patients with newly diagnosed focal epilepsy had glucose metabolism abnormalities (Gaillard et al., [2002](#page-8-13)) and greater hypometabolism in the ipsilateral temporal lobe is associated with longer epilepsy duration in unilateral TLE (Vivash et al., [2013](#page-8-14)). A longitudinal PET study in children with non-lesional focal epilepsy demonstrated progressive cortical glucose hypometabolism, which was moderately related to seizure frequency (Benedek et al., [2006](#page-7-0)). However, to our knowledge there are no longitudinal studies of PET in adult epilepsy. Therefore, this study aimed to investigate glucose metabolism longitudinally in adults with chronic drug resistant TLE, to ascertain whether repeating an FDG-PET scan at a later time point yields additional information upon reinvestigation.

## **Methods**

### **Subjects**

Retrospective data were collected from patients who were admitted to the Comprehensive Epilepsy Program Video EEG Monitoring (VEM) Unit at Royal Melbourne Hospital between 2004 and 2014. Inclusion criteria were patients with chronic drug resistant TLE that had undergone two [ 18F]-FDG scans and at least one epilepsy protocol MRI as

part of their evaluation for potential epilepsy surgery. Localisation of the epileptogenic zone was determined in accordance with International League Against Epilepsy guidelines by the consensus of the consultant epileptologists on the basis of the ictal and interictal VEM fndings, unequivocal patient history, and without any psychogenic events captured (Nightscales et al., [2020\)](#page-8-15). In cases of bilateral TLE the hemisphere with the greater proportion of seizures was considered ipsilateral. The study was approved by the Melbourne Health Human Ethics Research Committee (QA2012044).

# **[ 18F]‑FDG PET acquisition**

Interictal [ 18F]-FDG PET scans were acquired at the Peter MacCallum Cancer Centre on the Discovery STE PET/CT scanner (GE healthcare) or PENN PET 300H Tomograph scanner, and image acquisition was conducted as previously described (O'Brien et al., [2001,](#page-8-2) [2008](#page-8-3)). Patients were scanned on the same scanner in all but two cases (those with the longest inter-scan intervals). Patients fasted for 4 h prior to the scan and rested for 15–20 min in a darkened and quiet room. Subsequently,  $[$ <sup>18</sup>F]-FDG (250 MBq) was administered intravenously and scanning was undertaken 1 h after radiotracer administration. The patient was in a single bed position for at least 20 min and tape was used to immobilise the head. Voxel size was  $2.73 \times 2.73 \times 3.27$  mm, FOV 350 mm and matrix size  $128 \times 128 \times 47$ .

## **MRI acquisition**

MR imaging was conducted using a 3 T clinical wholebody scanner (Sigma Horizon SE120, GE Healthcare). A standardised TLE protocol was undertaken, including volumetric T1, FLAIR and high resolution T2 through the temporal lobes (Vivash et al., [2013](#page-8-14)). The T1-weighted volumetric MPRAGE  $(1.5 \text{mm}^3, \text{FOV } 22 \times 22 \text{ cm}, \text{ matrix size})$ 128\*128\*208) was used for image analysis.

### **ROI Analysis**

An operator blinded to all clinical variables and demographics conducted all image processing. Manual region of interest (ROI) tracing was performed on volumetric MPRAGE images using Analyze v10.0 (Mayo Clinic, MO), delineating the hippocampi, temporal lobes and pons. Hippocampal delineation was conducted in the coronal plane, followed by corrections in the sagittal plane. The temporal lobes, including the hippocampal, limbic, and neocortical structures, were delineated as previously described (Vinton et al., [2007](#page-8-8)). The pons was traced manually, where the tracing reached the edge of the pons, in the sagittal plane and corrected in the coronal plane. Intracranial volume was estimated using the tissue segmentation tool within SPM12 (Matlab 2017b).

PET scans were coregistered to their corresponding MRI using the 3D voxel registration tool in Analyze, and the ROIs applied producing values of uptake for all ROIs. Uptake in the hippocampi and temporal lobes were normalised to uptake in the pons.

### **SPM analysis**

In addition to the ROI analysis, whole-brain voxel-wise changes in hypometabolism were investigated individually in each patient using SPM12 (Matlab 2017b). The second PET scan was realigned to the frst PET scan using linear registration. These scans were masked with SPM's MNI intracranial volume (ICV) mask as follows: the two aligned PET scans were averaged and the average image registered to the inbuilt SPM PET template, followed by inversion of the MNI intracranial volume (ICV) and grey matter (GM) masks back into subject space. The PET images were proportionally scaled to their global mean, to account for between subject uptake variability. The mean activity in each scan within the ICV mask was calculated and voxels with activity  $< 0.125$  of the mean discounted and the mean recalculated. All remaining voxels were then divided by the global mean and multiplied by 50, giving a mean signal of 50. Images of percentage change were then created: % change =  $((T2-T1)/T1)*100$ .

These % change images were then masked using the GM mask (threshold  $> 0.1$ ). This image contains the relative change from T1 to T2 in each voxel independently. To measure meaningful change over time the percentage change was initially set at 20%, which resulted in two reductions in hypometabolism at T2, but no increases in hypometabolism. The percentage change was then adjusted to 10%, which was too noisy, detecting multiple areas of increased and decreased hypometabolism in each patient that were neither observable on visual inspection of the image pairs, nor pathologically or clinically meaningful. Thus 15% threshold was selected, considerably reducing the false detection of noise, without missing potentially pathological alterations. Images were extent thresholded, with clusters smaller than 300mm<sup>3</sup> removed. The resulting thresholded difference images were visually inspected overlaid on the realigned, normalised PET images to ensure fndings were real and not due to a processing error.

## **Statistical analysis**

The normalised  $[$ <sup>18</sup>]F-FDG uptake values were compared between the two scans using Jamovi (version 1.1.9.0). Median and SEM per group are reported within the text and a two-tailed Wilcoxon Signed Rank test was used to assess diferences between regions, and Spearman's correlation

was used to assess relationship with time. Mixed models were also used to investigate whether covarying for seizure frequency afected the association with time. Statistical analyses were re-run excluding the two bilateral TLE cases, this did not change the signifcance of any of the results described.  $p < 0.05$  was considered significant.

## **Results**

## **Patient characteristics**

Sixteen patients with chronic drug resistant TLE (9 females and 7 males) were included in this study. Median age was 35 years (range 18–64 years), and median age of epilepsy onset 27 years (range 4–58 years). Median epilepsy duration at scan 1 was 4.5 years, (range 0–41 years), and at scan 2 was 7 years (range 1–52 years). Six patients had MRI lesions  $(n=3$  hippocampal or mesial temporal sclerosis,  $n=1$  focal cortical dysplasia, *n*=1 tuberous sclerosis, and *n*=1 cavernoma), ten patients had non-lesional TLE. Clinical characteristics are detailed in Table [1.](#page-3-0)

#### **ROI analysis—MRI**

Hippocampal and temporal lobe volumes are shown in Fig. [1.](#page-3-1) Ipsilateral hippocampal volume  $(0.207 \pm 0.015 \, \text{\%ICV})$ ,  $2792 \pm 200.1$  mm<sup>3</sup>) was less than contralateral  $(0.225 \pm 0.01 \text{ %ICV}, 3051 \pm 130.2 \text{ mm}^3)$  hippocampal volume  $(p=0.01, Fig. 1A)$  $(p=0.01, Fig. 1A)$ . Temporal lobe volumes were similar between the ipsilateral  $(6.474 \pm 0.268 \sqrt{\frac{20 \text{ C V}}{90,856 \pm 3370}})$ mm<sup>3</sup>) and contralateral  $(6.72 \pm 0.233 \, \text{\%ICV}, 91,258 \pm 3033 \, \text{\%ICV})$ mm<sup>3</sup>) regions ( $p = 0.89$ ) (Fig. [1B](#page-3-1)). Exclusion of the two bilateral TLE cases does not afect the hippocampal asymmetry  $(0.207 \pm 0.015 \text{ %ICV vs } 0.225 \pm 0.01 \text{ %ICV, } p = 0.01)$ , nor the similarity of temporal lobe volumes observed  $(6.528 \pm 0.289 \text{ %ICV vs } 6.860 \pm 0.251 \text{ %ICV, } p = 0.95).$ 

#### **ROI analysis – FDG‑PET**

Figure  $1C$  shows  $[$ <sup>18</sup>F]-FDG uptake in the hippocampal ROIs on the serial scans, and Fig. [1D](#page-3-1) temporal lobe ROIs. Normalised FDG uptake was lower in the ipsilateral than contralateral hippocampus at baseline  $(1.14 \pm 0.03 \text{ vs } 1.18 \pm 0.03,$  $p=0.04$ ), but interestingly not at follow-up  $(1.19 \pm 0.04 \text{ vs } 1.19 \pm 0.04 \text{ vs } 1.1$  $1.19 \pm 0.03$ ,  $p > 0.19$ ). Normalised FDG uptake did not differ between ipsilateral and contralateral temporal lobes at baseline or follow-up  $(p > 0.16)$ . No change in normalised FDG uptake over time was observed in the ipsilateral (baseline  $1.14 \pm 0.03$ , follow-up  $1.19 \pm 0.04$ ,  $p = 0.25$ ; Fig. [1C](#page-3-1)) or contralateral (baseline  $1.18 \pm 0.03$ , follow-up  $1.19 \pm 0.03$ ,  $p = 0.94$ ) hippocampi. Similarly, normalised FDG uptake in the temporal lobes did not change over time (ipsilateral

<span id="page-3-0"></span>**Table 1** Clinical data of patient cohort, including age and age at diagnosis (years), time interval between [ 18F]-FDG PET scans (months), location of epileptogenic zone (Bilat TL -bilateral temporal lobe, LTL – left temporal lobe, RTL – right temporal lobe) and lesion type on MRI (NL – non-lesional, MTS – mesial temporal sclerosis, FCD – focal cortical dysplasia, HS – hippocampal sclerosis and TS—tuberous sclerosis), seizure frequency (per month). ? indicates pathology is uncertain



<span id="page-3-1"></span>**Fig. 1** Volumes and normalised FDG uptake in the hippocampi and temporal lobes. (**A**) Hippocampal and (**B**) temporal lobe volumes (expressed as %ICV). Blue squares represent the regions ipsilateral to the epileptogenic temporal lobe, and red squares the contralateral hemisphere. (**C**) Hippocampal and (**D**) temporal lobe FDG uptake (normalised to the pons). Closed circles represent baseline measurements, and open circles follow-up measurements. Error bars show median and inter-quartile range. \* *p*<0.05



baseline  $1.35 \pm 0.03$ , follow-up  $1.30 \pm 0.04$ ,  $p = 0.63$ ; contralateral baseline  $1.38 \pm 0.04$ , follow-up  $1.33 \pm 0.03$ ,  $p = 0.82$ ; Fig. [1D\)](#page-3-1). Exclusion of the two bilateral cases did not afect the overall results of the normalised FDG uptake (baseline hippocampal FDG uptake  $1.15 \pm 0.04$  vs  $1.18 \pm 0.04$ ,  $p = 0.04$ , all other comparisons non-significant).

Median change in normalised FDG uptake between baseline and follow-up was  $0.056 \pm 0.031$  in the ipsilateral hippocampus,  $0.014 \pm 0.035$  in the contralateral hippocampus and  $-0.002 \pm 0.032$  and  $-0.003 \pm 0.037$  in the ipsilateral and contralateral temporal lobes respectively. No diferences were detected between regions and none of these were different from 0 ( $p > 0.53$ ). Given the wide range of time between scans, and annualised rates of change were also calculated which were  $0.013 \pm 0.040$ ,  $0.003 \pm 0.041$  for the ipsilateral and contralateral hippocampus, and  $-0.001 \pm 0.039$ ,  $0.001 \pm 0.057$  for the ipsilateral and contralateral temporal lobes. No diferences

were detected between regions and none of these were different from  $0 (p > 0.3)$ .

## **Correlation with clinical characteristics**

Figure [2](#page-4-0) shows change in FDG uptake plotted against time. No correlations were found between time between scans and change in FDG uptake in any of the regions (Spearman's rho  $< 0.37$ ,  $p > 0.16$ ). Including seizure frequency as a covariate in mixed models showed no efect of time on uptake in any region.

The relationship between FDG uptake and epilepsy duration was also investigated. No correlation was found in the ipsilateral hippocampus or temporal lobes bilaterally (Spearman's rho  $< 0.13$ ,  $p > 0.49$ ), however a positive correlation was observed in the contralateral hippocampus (Spearman's rho=0.41,  $p=0.02$ ). Covarying for seizure frequency did not change these results.

The change in FDG uptake was also investigated relative to the inter-scan duration as a proportion of total epilepsy duration (Fig. [3\)](#page-5-0). Positive correlations were observed between change in FDG uptake and proportion of total epilepsy duration for the ipsilateral hippocampus (Spearman's rho=0.67,  $p < 0.01$ , Fig. [3A\)](#page-5-0) and bilateral temporal lobes (Spearman's rho $> 0.53$ ,  $p < 0.04$ , Fig. [3B\)](#page-5-0), the contralateral hippocampus was approaching signifcance (Spearman's  $rho=0.48$ ,  $p=0.06$ ). The data shows that for patients where this proportion is low (i.e. their epilepsy was long-standing at the time of the frst PET scan) FDG uptake tended to decrease, suggesting disease progression, whereas for patients where the proportion was at or approaching 1 (i.e. they were newly diagnosed at the time of the frst PET scan) FDG uptake did not change or increased marginally.

#### **SPM analysis**

Of the 16 subjects, 4 had supra-threshold increases in FDG-PET signal, and 3 had supra-threshold decreases. The most common locations of signal increases were the cerebellum and temporal lobes, and areas of decrease the frontal lobes. Figure [4](#page-6-0) shows example images of areas of increased and decreased metabolism between scans. 3/4 patients showed increases in the cerebellum, and 2/4 showed increases in the ipsilateral temporal lobe (and 1/4 in the contralateral temporal lobe). 2/3 patients had decreases in the frontal lobe, one contralateral and one bilateral, the other patient had a



<span id="page-4-0"></span>**Fig. 2** Change in FDG uptake between baseline and follow-up scans plotted against inter-scan duration. Change in hippocampal ROI (**A**) and temporal lobe ROI (**B**) relative FDG uptake between scans plotted against time between scans in the ipsilateral (blue) and contralateral (red) hemispheres

<span id="page-5-0"></span>**Fig. 3** Change in FDG uptake between baseline and follow-up scans plotted against inter-scan duration as a proportion of epilepsy duration. Change in hippocampal ROI (**A**) and temporal lobe ROI (**B**) relative FDG uptake between scans plotted against inter-scan duration as a proportion of epilepsy duration in the ipsilateral (blue) and contralateral (red) hemispheres



**Inter-scan duration as a proportion of epilepsy duration**

**-0.4**

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<span id="page-6-0"></span>**Fig. 4** Example SPM images showing increases (top row) and decreases (bottom row) in FDG uptake between scans. The left panel show baseline images, the middle panel the followup images and the right panel the specifc region of changed signal between the two images. The increased metabolism in both temporal lobes between baseline and follow-up suggests a resolution of hypometabolism (top row, patient 15), whereas the decreased metabolism in the left frontal lobe is suggestive of a misalignment during processing, and not a real change (bottom row, patient 4)



decrease in the cerebellum. No areas of decreased metabolism colocalised with the epileptogenic zone.

## FDG-PET repeated, and thus the fndings may not necessarily be generalisable to the wider TLE population.

**Discussion**

This study investigated whether brain glucose metabolism, as measured on  $[$ <sup>18</sup>F]-FDG PET imaging, changes over time in adults with chronic drug resistant TLE. The main fnding was that there was no evidence that  $[{}^{18}F]$ -FDG uptake evolved over time in this cohort of patients studied. This is therefore of signifcance in the clinical setting, suggesting repeating an FDG-PET scan in a patient who has previously had a negative or equivocal scan, will not yield diferent information.

Previous studies in an animal model of epilepsy showed acute hypometabolism early after an epileptogenic insult, with an increase in the severity of hypometabolism during chronic epileptogenesis and the development of spontaneous recurrent seizures (Jupp et al., [2012](#page-8-16)). In traumatic brain injury, hypometabolism occurred acutely following injury, which remained stable at later time points (Y. R. Liu et al., [2010](#page-8-17)). However, both these animal studies focused on the epileptogenic period, rather than chronic epilepsy.

We expected an increase in the hypometabolism to be observed on the FDG-PET scan over time in our patients, which was not the case. Patients included in the current study showed either subtle hypometabolism, or no hypometabolism, rather than the typical severe ipsilateral hypometabolism seen in the majority of TLE cases, which is the reason for repeating the PET scan and thus inclusion in the current study. This suggests the patients included in this study may be considered "complex" or "atypical" cases, which is why they had not proceeded to epilepsy surgery, but rather had an

Clinical studies of longitudinal imaging are scarce in patients with epilepsy, one study reported progressive volume loss in the ipsilateral hippocampus in TLE patients with ongoing seizures, which was not seen in those who were seizure free (Fuerst et al., [2003\)](#page-8-18). However, another study found early volume loss does not evolve over time, even with recurrent seizures (R. S. Liu et al., [2002](#page-8-19)). More recent studies report progressive atrophy in focal epilepsies (most commonly TLE). Temporal and extratemporal atrophy are observed in non-lesional TLE and TLE with hippocampal sclerosis both independent of, and associated with, seizures (Alvim et al., [2016](#page-7-2); Bernhardt et al., [2009,](#page-7-3) [2013](#page-7-4)). Additionally, widespread cortical thinning is reported in focal epilepsies (TLE and extra-TLE) in both the ipsilateral and contralateral hemispheres (Galovic et al., [2019](#page-8-20)).

The only previously published studies investigating longitudinal FDG PET have been in paediatric epilepsy populations. One study reported a signifcant reduction in the spatial extent of cortical glucose hypometabolism ipsilateral to the epileptic zone over time in paediatric patients with "intractable" non-lesional focal epilepsy. Another study investigated patients with West syndrome, an infantile epileptic encephalopathy that can be associated with focal cortical dysplasia in some patients. Of four patients, two had hypometabolism at baseline which had resolved on repeated imaging, one had hypermetabolism which resolved on repeated imaging, and one had normal metabolism at baseline which evolved to hypometabolism at follow-up (Sakaguchi et al., [2018](#page-8-21)). These, however, may not be suitable comparators for several reasons. Firstly, the aetiology of adult TLE and paediatric nonlesional focal epilepsy are diferent (Shukla & Prasad, [2012](#page-8-22)). Additionally, paediatric epilepsy will also be infuenced by higher cortical glucose metabolism, a trait which occurs during early development of the brain and may have underlying consequences on epilepsy related glucose hypometabolism (Chugani et al., [1987](#page-7-5)).

This study did observe a positive correlation between contralateral hippocampal FDG uptake and epilepsy duration. This fnding is contrary to our expectations, as previous work by our group has shown epilepsy duration negatively correlated with ipsilateral but not contralateral hippocampal FDG uptake in patients with TLE (Vivash et al., [2013](#page-8-14)). Further, this change in FDG uptake on ROI analysis is not supported by the SPM analysis and should therefore be interpreted with caution.

An interesting finding was the relationship between changes in FDG uptake as related to total epilepsy duration. Here, the results demonstrate that for patients whose epilepsy was long-standing at the time of their frst FDG-PET scan, the hypometabolism increased on the scan. However, for those who were newly diagnosed at the time of their frst FDG-PET scan there was no change in hypometabolism over the repeat scans. This suggests that hypometabolism may worsen after many years of chronic TLE, but may not evolve in the frst few years after a diagnosis of TLE.

This study has several limitations. Firstly, due to the reticence to rescan patients without a strong clinical justifcation, and the fact that a proportion of patients proceed to resective epilepsy surgery following their FDG-PET, the sample size is relatively small, and heterogenous with respect to epilepsy duration, MRI lesions, seizure frequency and interscan interval. Secondly, none of the patients included in this study had a typical pattern of severe unilateral hypometabolism often seen in TLE. For this reason they may be considered complex or atypical TLE cases. Lastly, changes in PET acquisition and reconstruction parameters may have impacted image quality and SUV quantifcation through improvements in signal to noise, which have the potential to impact diferences in measures for the cases of long inter-scan intervals who were scanned on two diferent scanners.

## **Conclusions**

This study indicates that  $[$ <sup>18</sup>F]-FDG PET does not significantly change in patients with chronic drug resistant TLE who had subtle or normal focal temporal hypometabolism on the frst scan. Therefore, rescanning these patients is unlikely to provide clinically useful new information. While a larger cohort study is required to confrm these fndings, the results could impact clinical care by reducing radiation exposure and lessening economic burden on the health care system of repeating FDG-PET scans in these patients.

**Author contributions** CS drafted the manuscript. CS and BS were responsible for data collection, analysis and interpretation. RH supervised the FDG-PET image acquisitions and contributed to data interpretation. PK and TOB contributed to data analysis and interpretation. LV conceived the study and contributed to data analysis and interpretation. All authors edited the manuscript and approved the fnal submitted version.

**Funding** This project was not supported by any specifc grant or other external party. PK is supported by a Medical Research Future Fund Fellowship (MRF1136427).

**Data availability** Data included in this study is patients' clinical data and is therefore not publicly available.

**Code availability** Not applicable.

#### **Declarations**

**Ethics approval** This study was approved by the Melbourne Health Human Research Ethics Committee (QA2012044). The study was conducted in accordance with this approval and ICH GCP.

**Consent to participate** In accordance with the HREC approval, specifc consent to participate was not sought from patients.

**Consent for publication** Not applicable.

**Conflict of interest** The authors have no conficts to declare.

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