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Poly (rhodamine B) sensor for norepinephrine and paracetamol: a voltammetric study

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Abstract

A voltammetric study of norepinephrine (NE) in the presence of paracetamol (PA) was carried out using a poly (rhodamine B)modified carbon paste electrode (CPE). The poly (rhodamine B) electrode was fabricated by potential cyclic voltammetry using a rhodamine B monomer. The modified electrode exhibited a good affirmative response towards the electrooxidation of NE and PA in physiological pH 7.4 phosphate buffer solution (PBS). The influence of sweep rates and pH (6.2 to 7.8) was studied. The simultaneous electroanalysis of NE and PA and the interference study were investigated by CV and DPV. The modified electrode showed good selectivity and sensitivity with a detection limit of NE of 1.8 μ M and PA of 2.2 μ M. The real sample analysis of the proposed method is studied by determining the NE in the injection sample and PA in a commercial tablet sample with good recovery results obtained.

Keywords Norepinephrine · Paracetamol · Rhodamine B · Electropolymerization · Voltammetry

Introduction

Electrochemical determination of biomolecules has been intensively studied over the past two decades. Among the family of catecholamines, norepinephrine (NE) is a kind of catecholamine neurotransmitter that mediates chemical communication in the central nerves system. It acts as a dual character of neurotransmitter as a stress hormone and fulfils many significant physiological functions. Decrease in the concentration level of NE may lead to the incidence of some neurological disorders such as Parkinson disease, paraganglioma, ganglion neurons, and ganglia neuroblastoma, respectively [1]. Recent reports have indicated that NE enhances adhesion of human immunodeficiency virus-1-infected leukocytes to cardiac

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microvascular endothelial cells and also accelerates HIV replication via protein kinase [2, 3]. In view of this, it is essential to develop sensitive, fast, and accurate methods for the investigation of trace of NE which is of great importance to diagnostic information for the above mentioned disorder. Generally, the determination of NE is carried out by different methods, including spectrophotometry, capillary electrophoresis, and high-performance liquid chromatography which have been employed to the investigation of NE. Because NE is an electroactive compound, its electrochemical detection has been the focus of research for electroanalytical researchers and neurochemists and some modified electrodes have been used to determine NE [4–10].

In addition, drug investigation plays an important role in the quality control of drug formulation which has great impact on public health. Paracetamol is a well-known drug and extensively used as a pain reliever (analgesic) and fever reducer (antipyretics) [11, 12]. It is a weak acid with a pKa value of 9.5. Paracetamol quickly gets adsorbed and circulated after oral administration and is easily eliminated in the urine in normal therapeutic dose. However, overdose of PA accumulates toxic metabolites that cause damages to the kidney and liver. In general, paracetamol does not show any harmful side effects on human health [13]. So far, many analytical techniques have been used for the investigation of PA such as spectrophotometry [14], high-performance liquid

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chromatography [15], electrophoresis [16], and flow injection [17]. The above methods have some drawbacks with several disadvantages like high cast, long analysis time, and requirement of sample preparation. Comparatively, electrochemical techniques are convenient, are reliable, have less time consumption, and are the cheapest [18]. PA administration is known to increase brain serotonin (5-HT) levels as a result of liver tryptophan-2,3-dioxygenase (TDO) inhibition, and 5-HT is known to play a role in NE release in the brain [3, 10]. Therefore, simultaneous determination of NE and PA is very essential. Moreover, oxidation peaks of NE and PA are similar potentials at the bare CPE. This results in overlap and fouling during the investigation of these compounds. Therefore, fabrication of an economically viable electrochemical sensor with simultaneous determination of NE and PA (Scheme 1a) with higher selectivity, stability, and sensitivity is still one of the challenging tasks for electrochemists. However, the shape of the peak and the electrochemical reaction are not good for conventional electrodes. Therefore, to solve this problem, a number of modified electrodes have been used for the investigation of NE and PA [19, 20]. Some forms of carbon and conducting polymers are the most accepted materials that are used as modified electrodes. This is mainly because of their electrochemical stability and relatively high resistance against electrode fouling in physiological environments.



Rhodamine B

 $\mbox{Scheme 1}\ a$ Oxidation mechanism of NE and PA. b Structure of rhodamine B

Sensing-based electrochemical methods on conductive polymers are of great importance in the cutting edge field due to their distinctive properties of simple functionality and biocompatibility. In several fields, conducting polymers have emerged as one of the interesting materials and have an expensive potential application for electrochemical sensors which covers biosensors and chemical sensors. Mainly in the area of biosensors, the covalent bond formation with biomolecules is used perfectly to get stable and more sensitive sensor methods. There are few proposed methods using conductive polymers as they contain active groups like -COOH and -NH2 groups to detect various biomolecules, DNA, and heavy metal ions [21-23]. Shim et al. and their recent review clearly discussed the importance of some conducting polymers and applications [24-26]. By using electropolymerization techniques, the electropolymer films coated with dyes have attracted extensive attention in the investigation of analytes because of their advantages like fast electron transfer, large surface area, high sensitivity, selectivity, good stability, homogeneity, and strong adsorption. Rhodamine B is a triphenylmethane dye and also belongs to a family of fluorone dyes which are used extensively in biotechnology applications such as fluorescence microscopy flow cytometry fluorescence correlation spectroscopy ELISA. Recently, electropolymerization of rhodamine B-based polymer films is reported as redox mediators for developing electrochemical sensors [27–29].

In the present work, the focus is on the poly (rhodamine B) layer that was fabricated on the CPE surface by using cyclic voltammetry. These modified electrodes displayed improved selectivity and sensitivity for the investigation of NE and PA. The poly (rhodamine B)-modified CPE offers several distinct advantages including high electron transfer, rate constant, and low detection limit. The electrocatalytic activities of NE and PA were disscussed in detail. The electrochemical sensing interference exhibits good performance towards the determination of NE and PA, which is of great significance in the chemical and biological fields. The practical application of the current method was confirmed by investigation of the concentration of NE in injection samples and PA in commercial tablets.

Experimental part

Materials and methods

An electrochemical experiment was conducted on a CH660c electrochemical work station (CH Instrument). The cyclic and differential voltammetric measurement was performed in a standard three-electrode cell system. The bare carbon paste electrode or carbon paste electrode was modified with rhodamine B and was used as a working electrode. The platinum wire and saturated calomel electrode were used as counter and

reference electrodes, respectively. Oxidation potentials of all the analytes were recorded versus SCE at an ambient temperature of 25 °C.

Chemicals and reagents

Norepinephrine (NE) was purchased from Himedia (molecular weight = 169.2, purity 99%), Paracetamol (PA) was purchased from Himedia (molecular weight = 151.64, purity 99%), and rhodamine B was collected from Sigma-Aldrich (molecular weight = 479.02, 90% dye content). The graphite fine powder (particle size 50 mm) was collected from Lobo Chemie and silicon oil from Himedia, and they were used to prepare the modified electrode. The stock solution of NE $(25 \times 10^{-4} \text{ M})$ was prepared in 0.1 M perchloric acid (HClO₄), and PA (25×10^{-4} M) and rhodamine B ($25 \times$ 10⁻⁴ M) were prepared in double-distilled water. Different pH's of PBS were produced as per literature with 0.2 M NaH₂PO₄ and 0.2 M Na₂HPO₄ solution with doubledistilled water. The above mentioned chemicals were of analytical grade and no needed further purification. All the experiments were performed at an ambient temperature.

Results and discussion

Fabrication of poly (rhodamine B)-modified CPE

The carbon paste electrode was fabricated according to our previous report [30]. The poly (rhodamine B) modified carbon paste electrode (MCPE) was successfully fabricated by electropolymerization of 1 mM aqueous rhodamine B monomer containing 0.1 M NaOH as supporting electrolyte. As shown in Fig. 1 (A), an anodic peak was observed at the first cycle which is corresponding to the oxidation of the rhodamine B monomer. The continuous electrochemical polymerization for the cyclic voltammograms of poly (rhodamine B) in the potential cycles is between -0.4 and 1.2 V at a sweep rate of 100 mV/s for 20 successive cycles. During the process of multiple cycles, the voltammogram has decreased gradually with further increase in potential cycling. The phenomenon implies that the poly (rhodamine B) membrane was formed and deposited on the surface of the CPE by an electropolymerization process [31]. After completion of the electropolymerization, the obtained modified electrode was dipped in demineralized water to eliminate the physically adsorbed material. The structure of rhodamine B is presented in Scheme 1b.

Based on the above observation, the polymer thickness of the film shows a significant effect on the electrochemical response of poly (rhodamine B)-modified CPE. The film thickness can be effectively controlled by changing the number of cycles (from 5 to 30 multiple cycles)



Fig. 1 *A* Electropolymerization of 1 mM of rhodamine B at 0.1 M NaOH solution as supporting electrolyte for 20 cycles with a sweep rate of 100 mV/s. Inset, *B*, graph of the anodic peak current versus number of cycles

during the polymerization process. The effect of thickness, determined by the number of electropolymerization sweeps, was studied on the response of NE (0.1 mM) in physiological pH (7.4) PBS. The graph of I_{pa} versus number of cycles was plotted from 5 to 20 cycles; I_{pa} increased linearly. Hence, at 20 cycles, the current response was maximum and after that it gradually decreases by increasing the number of cycles as shown in the inset in Fig. 1 (B). However, after 20 cycles, the poly (rhodamine B) monomer covers the electrode surface completely and did not show any significant change in the active area as well as the background current of voltammogram that slightly increases [32]. The maximum current signal for poly (rhodamine B) was observed at 20 cycles; thus, the same potential cycles were chosen as the optimum



Fig. 2 CVs of 1 mM potassium ferrocyanide at bare CPE (dashed line) and poly (rhodamine B)-modified CPE (solid line) at a sweep rate of 50 mV/s





condition to prepare poly (rhodamine B)-modified CPE for subsequent experiments.

Characterization of bare CPE and poly (rhodamine B) -modified CPE

Figure 2 illustrates the electrochemical response from freshly prepared potassium ferrocyanide at unmodified CPE (dashed) and poly (rhodamine B)-modified CPE in 1 M KCL as supporting electrolyte at a sweep rate of 50 mV/s. The redox peaks were observed due to the Fe⁺ $^{2}/Fe^{+3}$ for bare CPE and poly (rhodamine B)-modified CPE. The peak-to-peak separation (Δ Ep) at the developed electrode was significantly condensed to 53 mV than at unmodified CPE (110 mV). The result indicated that the surface property of modified CPE was drastically changed as well as the outcome at poly (rhodamine B)-modified CPE. The total active surface area was calculated by our previous reports [30] and found to be of higher value for poly (rhodamine B)-modified CPE (0.046 cm²) compared with unmodified CPE (0.0291 cm²).

Scanning electron microscope (SEM) images were used to study the electrode surface (Fig. 3). The SEM image of unmodified CPE shows the irregularly shaped micrometer-sized flakes of graphite. However, the poly (rhodamine B) filmcoated carbon paste electrode has the typical uniform arrangement of poly (rhodamine B) molecules on the surface of the carbon paste electrode. This confirms that the carbon paste electrode was coated with the poly (rhodamine B) film [33]. The proposed equation (1) was given to estimate the surface coverage concentration [32].

$$I_{\rm p} = n^2 F^2 A \Gamma \upsilon / 4 R T \tag{1}$$

Here, Γ (M/cm²) is the surface coverage concentration, v is the scan rate, A is the geometric surface area of the electrode, n is the number of electrons involved in the reaction, and R, F, and T have their scientific significance. The surface

concentration of poly (rhodamine B) was determined to be 0.073×10^{-10} M/cm².

Electrochemical analysis of NE and PA at poly (rhodamine B) MCPE

The electrochemical behavior of NE (0.1 mM) in physiological pH (7.4) PBS, with the sweep rate of 50 mV/s at bare CPE



Fig. 4 a CVs of 0.1 mM NE in 0.2 M PBS solution of pH 7.4 at bare CPE (dashed line) and poly (rhodamine B)-modified CPE (solid line) at a sweep rate of 50 mV/s. **b** CVs of 0.1 mM PA in 0.2 M PBS solution of pH 7.4 at bare CPE (dashed line) and poly (rhodamine B)-modified CPE (solid line) at a sweep rate of 50 mV/s

and poly (rhodamine B)-modified CPE, is illustrated in Fig. 4a. In bare CPE, NE shows that the oxidation peak current response was less sensible and low in current signal. The oxidation peak potential appeared at 192 mV. At the same time, poly (rhodamine B)-modified CPE showed that the oxidation peak current was significantly enhanced when compared to bare CPE and the oxidation peak potential which appeared at 162 mV. This reduces the overpotential and enhancement in peak currents, which reveals the electrocatalytic activity of poly (rhodamine B)-modified CPE towards the electrochemical oxidation of NE. Figure 4b illustrates the



Fig. 5 *A* CVs of 0.1 mM NE in 0.2 M PBS solution of pH 7.4 at poly (rhodamine B)-modified CPE at different sweep rates. (a–h, 50 to 400 mV/s). Inset, *B*, graph of the anodic peak current versus sweep rate. Inset, *C*, graph of the log of the anodic peak current versus log of sweep rate. *D* CVs of 0.1 mM PA in 0.2 M PBS solution of pH 7.4 at poly (rhodamine B)-modified CPE at different sweep rates. (a–h, 50 to 400 mV/s). Inset, *E*, graph of the anodic peak current versus sweep rate. Inset, *F*, graph of log of the anodic peak current versus log of sweep rate

CVs of PA (0.1 mM) in physiological pH (7.4) PBS, with a sweep rate of 50 mV/s using bare CPE and poly (rhodamine B)-modified CPE. On the bare CPE (dashed line), PA shows an irreversible behavior with relatively weak redox peak current and high potential difference. However, poly (rhodamine B)-modified CPE shows strong improvement of the well-defined redox peak current with E_{pa} and E_{pc} at 332 and 222 mV, respectively. This better activity is mainly due to the poly (rhodamine B)-modified CPE that accelerates the electrochemical reaction, and the peak potential difference of PA becomes lower than that on the bare CPE and the oxidation peak shifts slightly towards the negative side. It is clear that this polymer film-coated electrode shows very good electrocatalytic activity by reducing the overpotential and also by improving the current signal.

The sweep rate effect on the peak current of NE and PA

The sweep rate effect of NE (0.1 mM) at the surface of poly (rhodamine B)-modified CPE in physiological pH (7.4) PBS was studied in the range of from 50 to 400 mV/s in order to investigate whether the redox behavior of NE on the modified CPE was either adsorption or diffusion controlled. Figure 5 (A) depicts that the CVs of NE at different sweep rates show an increase in the redox peak current with increases in the sweep rate; the plot of I_{pa} versus sweep rate (υ) (inset, Fig. 5 (B)) and log of I_{pa} versus log of sweep rate (V/s) (inset, Fig. 5 (C)) exhibit good linearity, and the linear regression equations for both graphs were found to be I_{pa} (μA) = 0.0149 v(mV/s) + 1.112 (μ A) ($R^2 = 0.9988$) and log I_{pa} (μ A) = 0.626 log $v(V/s) + 1.068 (\mu A) (R^2 = 0.9848)$. The slope (0.626) obtained from the graph of the log sweep rate (v) versus the log of the anodic peak current (log I_{pa}) is closer to the theoretically obtained value of 0.5 for a diffusion-controlled elctrode

 Table 1
 Variation of the voltammetric parameters gathered from the plots shown in Fig. 5 as a function of the potential sweep rate

Sweep rate (mV/s)	$\Delta Ep/mV$		k°/s			
	Norepinephrine (NE)	Paracetamol (PA)	Norepinephrine (NE)	Paracetamol (PA)		
50	46	100	0.939	0.504		
100	42	122	1.963	0.787		
150	39	137	3.047	0.995		
200	40	149	4.008	1.156		
250	40	157	5.011	1.315		
300	41	165	5.956	1.445		
350	42	177	7.464	1.468		
400	42	181	7.673	1.603		

process [34]. Similarly, the effect of the sweep rate for PA was studied by CV at poly (rhodamine B)-modified CPE. Poly (rhodamine B)-modified CPE showed an increase in the redox peak current with an increase in sweep rates, over the range from 50 to 400 mV/s as shown in Fig. 5 (D). In order to investigate the nature of the electrode process, the plot of I_{pa} versus the sweep rate (v) (inset, Fig. 5 (E)) and log of I_{na} versus log of sweep rate (V/s) (inset, Fig. 5 (F)) exhibit good linearity, and the linear regression equations for the graphs were found to be as follows: I_{na} (μ A) = 0.049 v(mV/s) + 6.993 (μ A) ($R^2 = 0.9961$) and log I_{pa} (μ A) = 0.534 log $v(V/s) + 1.617 (\mu A) (R^2 = 0.9989)$. The slope from the graph of the log sweep rate (v) versus the log of the anodic peak current (log I_{pa}) is 0.534 which is closer to the theoretically obtained value of 0.5 for the diffusion-controlled electrode process [34]. From Fig. 5, the obtained ΔEp values were used to find the heterogeneous rate constant (k°) using Eq. (2) and was a valid approximation of such a curve intended for ΔEp > 10 mV; the k° values for NE and PA oxidation were obtained and recorded in Table 1 with a range of 50-400 mV/s.

$$\Delta Ep = 201.39 \log (\nu/k^{\circ}) - 301.78$$
⁽²⁾

Concentration effect of NE and PA at poly (rhodamine B) MCPE

In order to express, the NE detection with the prepared poly (rhodamine B)-modified CPE, the electrochemical response of the modified electrode at different concentrations of NE was examined in physiological pH (7.4) PBS at the sweep rate of 50 mV/s. Figure 6 (A) shows the CVs of various concentrations (20 to 90 µM) of NE at poly (rhodamine B)modified CPE. From the observation, Ipa and Ipc increase with the addition of NE from 20 to 90 μ M. The inset graph in Fig. 6 (B) is the plot of I_{pa} versus the concentration of NE at poly (rhodamine B)-modified CPE and corresponding linear regression equations I_{pa} (μA) = 0.0273 (C₀, $\mu M/L$) + 1.374, and their correlation co-efficient was found to be 0.9991. The limit of detection (LOD) and limit of quantification (LOQ) calculated in the lower concentration range for NE were found to be 1.8 and 6.1 μ M, respectively. At the same time, the electrochemical response of poly (rhodamine B)-modified CPE at different concentrations of PA was examined in physiological pH (7.4) at the sweep rate of 50 mV/s. Figure 6 (C) illustrates CVs of various concentrations of PA (20 to 90 μ M). There was a dramatic enhancement of I_{pa} . The graph of I_{pa} versus concentrations of PA was plotted (inset, Fig. 6 (D)). Ipa was propositional to the concentration of PA, but a better linearity occurred in the range 20 to 90 μ M and the linear regression equation can be written as I_{pa} (µA) = 0.0345 (C₀, µM/L) + 1.252 (R^2 =



Fig. 6 *A* CVs of NE in 0.2 M PBS solution of pH 7.4 at poly (rhodamine B)-modified CPE at a sweep rate of 50 mV/s with different concentrations (a–h, 20, 30, 40, 50, 60, 70, 80, and 90 μ M). Inset, *B*, graph of the anodic peak current versus different concentrations of NE. *C* CVs of PA in 0.2 M PBS solution of pH 7.4 at poly (rhodamine B)-modified CPE at a sweep rate of 50 mV/s with different concentrations (a–h, 20, 30, 40, 50, 60, 70, 80, and 90 μ M). Inset, *D*, graph of the anodic peak current versus different concentrations (a–h, 20, 30, 40, 50, 60, 70, 80, and 90 μ M). Inset, *D*, graph of the anodic peak current versus different concentrations of PA

0.9979). The limit of detection for PA in the lower concentration range was 2.2 μ M, and the quantification limit was 7.4 μ M. The limit of detection (LOD) and limit of quantification (LOQ) was calculated by using Formulas (3) and (4), respectively [30]. Here, M is the slope of the calibration graph and S is the standard deviation. The comparison of the detection limit of poly (Rhodamine B)-modified CPE for NE and PA with other reported modified electrodes are presented in Tables 2 and 3 [35–48].

$$LOD = 3S/M \tag{3}$$

$$LOQ = 10S/M$$
(4)

Sl. no.	Electrode	Modifier	pН	Limit of detection (LOD)	Techniques	Reference
1	Carbon paste	5ADMBCNPE	7.0	$8.0 imes 10^{-6}$	SWV	35
2	Gold	ME/Au SAMs	5.5	$0.7 imes 10^{-6}$	SWV	36
3	Gold	Thiolactic	5.9	$2.0 imes 10^{-6}$	CV	37
4	Carbon paste	TX-100/CPE	7.0	$5.0 imes 10^{-6}$	CV	38
5	Glassy carbon	SWNT-modified electrode	5.7	6.0×10^{-6}	CV	39
6	Gold	C_{60} -[dimethyl-(β cyclodextrin)] ₂ /Nafion	6.0	$8.0 imes 10^{-6}$	CV	40
7	Glassy carbon	Poly(2,4,6-trimethylpyridine)	7.4	$8.0 imes 10^{-6}$	CV	41
8	Carbon paste	Poly (rhodamine B)-modified CPE	7.4	1.8×10^{-6}	CV	This work

Table 2 Comparison of the detection limit of poly (rhodamine B)-modified CPE for NE with other reported modified electrodes

Effect of buffer of pH on NE and PA at poly (rhodamine B)-modified CPE

The effect of pH on the oxidation of NE (0.1 mM) at the sweep rate of 50 mV/s in poly (rhodamine B)-modified CPE was examined over a pH range of 6.2 to 7.8 (Fig. 7A). The Fig. 7B shows the graph of E_{pa} versus the pH obtained from the voltammograms of NE recorded at different pH's of phosphate buffer solution by the CV method. From the graph, the equation can be written as E_{pa} (mV) = 0.625 - 0.061 (mV/pH), for poly (rhodamine B)-modified CPE. The graph illustrated linearity with a slope of 61 mV/pH, and the obtained slope value is almost following the Nernst equation for an equal number of electron and proton transfer reaction [49]. At the same time, the effect of solution of pH on the redox reaction of PA at the poly (rhodamine B)-modified CPE was investigated in the range of pH 6.2-7.8. The CVs of PA (0.1 mM) was recorded at 0.2 M PBS of different pH's as shown in Fig. 7 (C). The plot of E_{pa} versus pH of the supporting electrolyte (inset, Fig. 7 (D)) has shown that E_{pa} linearly depends on the pH and a linear regression equation can be written as E_{pa} (mV) = 48.50 (mV/pH) + 68.8 ($R^2 = 0.9911$). This shows the uptake of an electron accompanied by an equal number of electron and proton transfer reaction [49].

Simultaneous electroanalysis of NE and PA

The electrochemical behavior of NE and PA at the bare CPE and poly (rhodamine B)-modified CPE has been investigated. The corresponding CVs of NE and PA in physiological pH (7.4) PBS is shown in Fig. 8 (A). As seen, NE and PA showed a poor oxidation peak at the bare CPE (dashed line) with oxidation peak potentials appeared at 222 and 382 mV, respectively. A poly (rhodamine B)-modified CPE (solid line) shows two well-defined anodic peaks of NE and PA with anodic peak potentials that appeared at 154 and 320 mV, respectively. ΔEp was found to be 166 mV, and this outcome was sufficient for the simultaneous investigation of NE and PA. The interference method was carried out in the samples containing both NE and PA in DPV experiments. This work was carried out by changing the concentration of NE and PA. The concentration of one species was varied, and the other remained constant. In the first step, the NE concentration was changed from 20 to 70 µM, while the concentration of PA was kept constant at $20 \ \mu M$ (Fig. 8 (B)). There was no change in the peak current and peak potential for PA. Similarly in the second step, the concentration of PA was increased from 20 to 70 µM when 20 µM NE was kept constant (inset, Fig. 8 (C)). However, PA does not have any effect on the peak potential and peak

Table 3 Comparison of the detection limit of poly (rhodamine B)-modified CPE for PA with other reported modified electrodes

Sl. no.	Electrodes	Modifier	pН	Limit of detection (LOD)	Techniques	Reference
1	GCE	C ₆₀ /GCE	7.2	50×10^{-6}	DPV	42
2	CPE	<i>N</i> -(3,4-Dihydroxyphenethyl)-3,5- dinitrobenzamide-modified MWCNT	7.0	10×10^{-6}	DPV	43
3	Palladized aluminum surface	Aluminum electrode modified by Thin layer of palladium	6.0	5×10^{-6}	DPV	44
4	GCE	Polyphenol oxidase-modified electrode	7.4	2.1×10^{-5}	DPV	45
5	CPE	BH and TiO ₂ nanoparticles	8.0	2.6×10^{-6}	DPV	46
6	GCE	Cu-poly-TTCA	7.0	5×10^{-6}	CV	47
7	GCE	BDD electrode	8.0	10×10^{-6}	CV	48
8	CPE	Poly (rhodamine B)-modified CPE	7.4	2.2×10^{-6}	CV	This work



Fig. 7 *A* CVs of the poly (rhodamine B) MCPE in 0.2 M PBS solution containing 0.1 mM NE at different pH values (a–e, 6.2 to 7.8) at a sweep rate of 50 mV/s. Inset, *B*, Graph of the anodic peak potential versus different pH's of NE. *C* CVs of the poly (rhodamine B) MCPE in 0.2 M PBS solution containing 0.1 mM PA at different pH values (a–e, 6.2 to 7.8) at a sweep rate of 50 mV/s. Inset, *D*, graph of the anodic peak potential versus different pH's of PA

current. This result shows that NE and PA existed independently in their mixture of samples.

Analysis of real samples

The poly (rhodamine B)-modified CPE was used for the investigation of NE and PA in noradrenaline bitartrate injection and paracetamol tablets, respectively. The NE injection sample was purchased from Troikaa Pharmaceuticals Ltd., with the specified amount of NE, i.e., 2.0 mg/mL, and the injection sample was used after suitable dilution in 0.2 M PBS [50]. The obtained results are presented in Table 4. From the experimental results, the recovery result was obtained which was



Fig. 8 A CVs for simultaneous determination of 0.2 mM NE, 0.1 mM PA at bare CPE (dashed line), and poly (rhodamine B)-modified CPE (solid line) at a sweep rate of 50 mV/s. *B* DPVs of a 20 μ M, b 30 μ M, c 40 μ M, d 50 μ M, e 60 μ M, and f 70 μ M NE in 0.2 M PBS of pH 7.4 in the presence of 20 μ M PA at poly (rhodamine B)-modified CPE and (dashed line) blank solution of PBS. Inset, *C*, DPVs of a 20 μ M b 30 μ M, c 40 μ M, d 50 μ M, e 60 μ M, and f 70 μ M PA in 0.2 M PBS of pH 7.4 in the presence of 20 μ M NE at poly (rhodamine B)-modified CPE and (dashed line) blank solution of PBS.

between 95.06 and 98.97%. This method shows promising results for NE in injection samples. Furthermore, a commercial tablet (Dolo 500, Micro Labs Limited [specified content

Table 4	Detection	of NE a	nd PA in	real	sample	(n =	3)
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Samples	Added (µM)	Found (µM)	Recovery (%)
NE injection	10	9.5	95.06
sample	20	19.5	97.74
	30	29.69	98.97
Paracetamol tablet	10	10.12	101.21
(Dolo 500 mg)	20	21.78	108.91
	30	30.79	102.64

of PA is 500 mg]) was used for the investigation of paracetamol. The obtained results are shown in Table 4. The recovery results showing the proposed methods could be efficiently used for the detection of PA in the commercial tablet with recovery in the range between 101.21 and 108.91%. All the experiments were carried out for three times using poly (rhodamine B)-modified CPE.

Conclusion

In the present work, the modified poly (rhodamine B) was used for the determination of NE and PA. The higher oxidation and reduction peak currents were observed at poly (rhodamine B)-modified CPE. The modified carbon paste electrode showed good sensitivity, selectivity, and electrocatalytic activity towards the oxidation of NE in the presence of PA. The detection limits of NE and PA were found to be 1.8 and 2.2 μ M, respectively. The potential difference between NE and PA was 160 mV, and it was large enough to determine the NE and PA simultaneously. From these observations, poly (rhodamine B)-modified CPE could be used as a promising sensor probe for the simultaneous detection of NE and PA in various medically important samples.

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