# CARDIAC RADIOLOGY



# The evaluation of non-ischemic dilated cardiomyopathy with T1 mapping and ECV methods using 3T cardiac MRI

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#### **Abstract**

Purpose The aim of this study was to examine the correlation between ventricular function and the extracellular volume fraction (ECV) in patients with non-ischemic dilated cardiomyopathy (NIDCM) using 3.0 T magnetic resonance imaging (MRI). We also hypothesized that native T1 and ECV values would be increased in patients with NIDCM, independent of the left ventricular ejection fraction (LVEF). The findings of our study could lead to further studies of the follow-up protocols.

☐ Cemile Ayşe Görmeli ayseyazici@yahoo.com

Zeynep Maraş Özdemir zynpmaras@yahoo.com

Ayşegül Sağır Kahraman mdasagir2003@hotmail.com

Jülide Yağmur julideyagmur@hotmail.com

Ramazan Özdemir ramazanozdemir@inonu.edu.tr

Cemil Çolak cemilcolak@yahoo.com

- Department of Radiology, Inonu University School of Medicine, İnönü Üniversitesi Turgut Özal Tıp Merkezi Radyoloji Ana Bilimdali, Elazığ yolu 15. km, Merkez, Malatya 44000, Turkey
- Department of Cardiology, Inonu University School of Medicine, İnönü Üniversitesi Turgut Özal Tıp Merkezi Kardiyoloji Ana Bilimdali, Elazığ yolu 15. km, Merkez, Malatya 44000, Turkey
- Department of Biostatistics, Inonu University School of Medicine, İnönü Üniversitesi Turgut Özal Tıp Merkezi Biyoistatistik Ana Bilimdali, Elazığ yolu 15. km, Merkez, Malatya 44000, Turkey

Materials and methods In total, 53 consecutive dilated cardiomyopathy patients who had undergone cardiac MRI were functionally evaluated and underwent tissue characterization.

Results The mean native T1 value was  $1235 \pm 10$  ms, and the mean ECV value was  $35.4 \pm 2.7\%$  in the myocardia. The LVEF values ranged from 29 to 44%. No significant correlations were observed between functional analysis measurements and native T1 or ECV values.

Conclusions Our results showed that myocardial fibrosis is unrelated to cardiac functional findings in NIDCM patients. Therefore, we propose that these patients should be evaluated using MRI and tissue characterization techniques, in addition to cardiac functional analysis.

**Keywords** Cardiac magnetic resonance imaging  $\cdot$  T1 mapping  $\cdot$  Extracellular volume fraction  $\cdot$  Nonischemic dilated cardiomyopathy  $\cdot$  Myocardial fibrosis  $\cdot$  Left ventricular ejection fraction

# Introduction

Non-ischemic dilated cardiomyopathy (NIDCM) can cause heart failure and sudden cardiac death (SCD) and is clinically defined as left ventricular (LV) or biventricular enlargement with decreased systolic function [1–3]. This clinical entity is responsible for a significant proportion of newly diagnosed heart failure cases and is the most frequent reason for heart transplantation in adults and children [1–3]. NIDCM predisposes individuals to ventricular arrhythmias and consequent SCD [4–6]. Moreover, although a reduced left ventricular ejection fraction (LVEF) is a criterion for inserting an implantable cardioverter-defibrillator (ICD) to prevent SCD [7–9], ICD candidates should not be



chosen solely on the basis of LVEF [6]. Myocardial fibrosis (MF) has been sufficiently defined as the main cause of arrhythmogenesis, which is a strong indicator of undesirable cardiac outcomes [5, 6, 10, 11]. MF changes and disrupts the myocardial structure, which results in mechanical and electrophysiological failure of the heart [12–15]. Therefore, assessment of MF has become important for the follow-up and recovery of patients with NIDCM.

Cardiac magnetic resonance (CMR) imaging is a powerful visualization method that provides the unique capability to not only detect the presence and position of MF but also quantitatively characterize examined tissue [16-22]. In contrast, although late gadolinium enhancement (LGE) imaging can successfully identify localized myocardial scar tissue, diffuse fibrosis may be overlooked, and quantitative assessment is not possible [23, 24]. In addition, McCrohon et al. showed that LGE is apparent in only 41% of NIDCM patients [25]. The native T1 mapping technique of CMR imaging, which does not require gadolinium enhancement, permits the detection of overall changes in myocardial tissue, such as fibrosis, edema, and the deposition of iron, lipids or proteins, that predict myocardial pathologies involving myocytes and interstitial spaces [26-28]. Furthermore, the extracellular volume fraction (ECV) technique of CMR imaging is a novel method that can differentiate the cellular and interstitial parts of the myocardium by measuring the extent of the extracellular space after administration of a contrast agent, thereby delineating MF. In addition, no approved treatment exists for reducing the duration of hospitalization or the mortality rate in heart failure patients who have sufficient systolic function. In these patients, reduced LVEF alone is not a sufficient assessment for predicting the prognosis of NIDCM [26, 29, 30].

The aim of this study was to examine the correlation between LV function and ECV values in NIDCM patients (with LVEF <45%) using 3.0-T CMR imaging. Our hypothesis was that native T1 and ECV values are increased in patients with NIDCM regardless of the LVEF. The findings of our study could lead to further studies of the follow-up protocols.

#### Methods

# Study population

Based on clinical and echocardiographic findings, 53 patients with dilated cardiomyopathy (DCM) who underwent CMR imaging in our radiology department were retrospectively evaluated for NIDCM between March 2015 and February 2016. Patients were excluded if they

exhibited the presence of ischemic DCM, an LVEF value >45%, a focal myocardial scar that was apparent via LGE imaging, and/or myocardial edema that could be observed via T2 mapping.

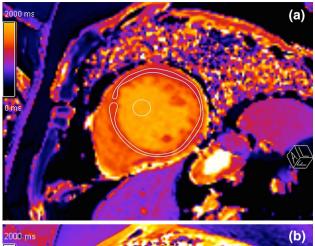
# Scanning protocol

Cardiac magnetic resonance imaging examinations were performed with a 3.0 T clinical scanner (Magnetom Skyra, Version E11, Siemens Healthcare, Erlangen, Germany) with an 18-channel cardiac coil and electrocardiography gating. Images were acquired according to a routine clinical protocol for volumes, tissue characterization, and LGE. For functional evaluation of the LV and assessment of the heart chambers, steady-state free-precession cine images in the short axis-view and 3 long-axis views (2, 3, and 4-chamber views) were obtained using the following parameters: TR, 41 ms; TE, 1.2 ms; flip angle, 47°. In all patients, the native and post-contrast T1 mapping data were acquired in a single mid-ventricular short-axis slice using the modified look-locker inversion recovery (MOLLI) sequence. The native T1 mapping parameters consisted of TR, 272.1 ms; TE, 1.2 ms; flip angle, 35°. T2 mapping was obtained in the same mid-ventricular short-axis level used for T1 mapping with the following imaging parameters: TR, 207.4 ms; TE, 1.32 ms; flip angle, 12°. LGE images were acquired 15 min after administration of a dose of 0.2 mmol/kg gadolinium using a phase-sensitive inversion recovery sequence (TR, 775 ms; TE, 2.67 ms; flip angle, 25°). The imaging procedure was concluded with post-contrast T1 mapping using the following parameters: TR, 361.6 ms; TE, 1.12 ms; flip angle, 35°. All data were stored in DICOM format. The scanning time for the entire CMR protocol with the T1 mapping technique was approximately 40 min for each patient.

# Image analysis

The acquired CMR images were analyzed on a Syngo Via workstation (Software Version VA30A, Siemens AG, Germany) by the same radiologist (CAG) who had 3 years of experience in cardiac imaging and was blinded to the patient age, patient gender, and echocardiographic results. T1 mapping images and findings from functional evaluations of the LV were analyzed in different readout sessions at three-day intervals to obtain objective and unbiased results. Endocardial and epicardial contours were semi-automatically traced at the end-diastolic phase and the end-systolic phase. The papillary muscles were included as part of the LV myocardial mass. Using the delineated endocardial and epicardial contours, the LVEF, left ventricular





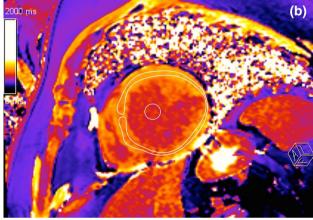


Fig. 1 Representative images of  $\boldsymbol{a}$  native and  $\boldsymbol{b}$  post-contrast T1 maps

end-diastolic volume (LV-EDV), and left ventricular end-systolic volume (LV-ESV) were measured and normalized to the body surface area (BSA).

Focal scar tissue was identified by myocardial LGE imaging and qualitatively characterized by myocardial post-contrast signal intensity. Pre- and post-contrast pixelwise T1 relaxation times were measured by manual region of interest (ROI) tracing to detect the LV myocardial circumference at the mid-ventricular level in short-axis images. Pre- and post-contrast blood T1 values were also calculated in a ROI traced in the blood pool (Fig. 1). In addition, pixelwise images of myocardial T2 mapping were analyzed for qualitative and quantitative assessments of the myocardium with the same technique used to map the T1 ROI.

ECV values were calculated according to the following formula:  $ECV = (1 - \text{hematocrit}) \times (1/\text{T1 myocardium})$  post-contrast - 1/T1 myocardium pre-contrast/(1/T1 blood post-contrast - 1/T1 blood pre-contrast) [29, 31].

The total time required to analyze CMR images was approximately 30 min for each patient.



The data were summarized as means  $\pm$  standard deviations (SDs) and as frequencies with percentages. Descriptive statistics were calculated for the variables. The correlations between the LVEF, LV-EDV, LV-ESV, native T1, and ECV variables were estimated using Pearson correlation coefficients. Intra-observer intraclass correlation coefficients (ICCs) were calculated to identify repeatability in the quantitative analyses, and the 95% confidence intervals (CIs) were also computed. For all quantitative values, measurements were obtained with intervals of at least 1 week between evaluation sessions for the ICC calculations. Values of P < 0.05 were considered statistically significant. IBM SPSS Statistics 23.0 (IBM Corp., Armok, NY, USA) and MedCalc 15.2 (MedCalc Software, Mariakerke, Belgium) were used for all statistical analyses.

## **Results**

Of the 53 patients, 14 patients indicated focal contrast enhancement after LGE imaging. Two of these 53 patients had increased T2 mapping values and were excluded from the study, resulting in a total of 37 NIDCM patients included in the analyses. The average age of the patients was  $43.5 \pm 10$  years (range 29–64 years); 54% (20/37) of the patients were women, and 46% (17/37) were men. The mean native T1 time was 1235 ms, and the mean ECV value in the myocardium was  $35.4 \pm 2.7\%$ . The LVEF values ranged from 29 to 44% (mean  $38 \pm 4.4\%$ ). The mean LV-EDV normalized to the BSA was  $90.1 \pm 12$  ml/m², and the mean LV-ESV was  $60.1 \pm 13.5$  ml/m². The CMR imaging findings are summarized in Table 1.

Statistically significant negative correlations were observed between the LVEF and LV-EDV values and between the LVEF and LV-ESV values (Pearson correlation coefficient = -0.959, P < 0.001; Pearson correlation coefficient = -0.971, P < 0.001, respectively). A statistically significant positive correlation was also found between native T1 values and ECV values (Pearson correlation coefficient = 0.932, P < 0.001). However, no significant correlations were observed between LVEF, LV-EDV, LV-ESV, and native T1 values or ECV values (Fig. 2).

The ICC for the LVEF calculations was 0.989 (95% CI 0.979–0.994), indicating excellent agreement. The ICC for the LV-EDV and LV-ESV measurements showed nearly perfect agreement (0.991, 95% CI 0.983–0.995; 0.996, 95% CI 0.993–0.998, respectively). In addition, the native T1 mapping values (ICC = 0.911, 95% CI 0.828–0.954) and ECV measurements (ICC = 0.997, 95% CI 0.995–0.998)

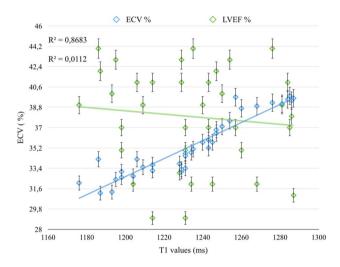


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Table 1 Demographic characteristics and CMR findings of NIDCM patients

|                             | All patients ( $n = 37$ ) (mean $\pm$ SD) |
|-----------------------------|---|
| Age (year)                  | $43.5 \pm 10$                             |
| Male gender (n, %)          | 17, 46%                                   |
| Native T1 (ms)              | $1235 \pm 10 \text{ ms}$                  |
| ECV (%)                     | $35.4 \pm 2.7$                            |
| LVEF %                      | $38 \pm 4.4$                              |
| LV-EDV (ml/m <sup>2</sup> ) | $90.1 \pm 12$                             |
| LV-ESV (ml/m <sup>2</sup> ) | $60.1 \pm 13.5$                           |
|                             |   |

ECV extracellular volume fraction, LV left ventricular ejection fraction, LV-EDV left ventricular end-diastolic volume, LV-ESV left ventricular end- systolic volume



**Fig. 2** Statistically significant positive correlation between native T1 values and ECV values, but neither had a significant relationship with the LVEF

indicated very good agreement. Therefore, we concluded that these data were reliable and reproducible.

## **Discussion**

In this study, to obtain a homogeneous cohort of NIDCM patients, we excluded patients who had edema on T2 mapping or positive LGE imaging findings. We observed several important results. First, we showed that the mean native T1 mapping values and ECV measurements in NIDCM patients could be obtained using 3.0 T magnetic resonance imaging (MRI); a limited number of previous studies in this area have been reported in the literature. More importantly, our study demonstrated that no significant correlations existed between metrics measuring LV function (LVEF, LV-EDV, and LV-ESV) and myocardial

tissue characterization values (native T1 mapping and ECV) in NIDCM patients.

CMR imaging has rapidly improved and is the gold standard for evaluating cardiac function due to its high spatial resolution. Rapid improvements in CMR imaging have allowed for the quantitative assessment of myocardial tissue. Moreover, relative to prior scanners, 3.0 T MRI scanners have higher magnetic field strength and provide better signal-to-noise ratio (SNR) and T1 imaging of the myocardium; thus, the use of such scanners has advantages in the context of cardiac perfusion, myocardial mapping and tagging [27, 32–36]. In addition, T1 mapping and ECV techniques have been demonstrated as effective methods for evaluating diffuse MF in NIDCM patients [37–39]. Dass et al. [17] indicated that native T1 values in 18 DCM patients (mean T1 value =  $1225 \pm 42$  ms) were significantly higher than in controls. A study of 27 DCM patients by Puntmann et al. [39] similarly showed increased T1 values (mean T1 value =  $1239 \pm 457$  ms). Consistent with those studies, we showed high native T1 times (mean T1 value =  $1235 \pm 10$  ms). In addition, Mordi et al. [40] (using 1.5 T MRI) and Puntmann et al. [39] (using 3.0 T MRI) found increased ECV values. Our study showed similar increased ECV values in NIDCM patients (mean  $ECV = 35.4 \pm 2.7\%$ ).

Several studies have shown that determining the ECV value is a useful technique for characterizing interstitial fibrosis and its consequential relationship with mortality [41–43] Furthermore, Dass et al. [17] showed that native T1 mapping could be a useful biomarker for the initial diagnosis and prognostic evaluation of cardiomyopathies. These findings suggest that high native T1 values or an increase in the ECV value could be helpful for risk stratification of patients with cardiomyopathies. In addition, because no proven treatment option exists for decreasing the mortality or the hospitalization time for NIDCM patients who have sufficient LVEF [29, 30], the identification of MF has become important. In this study, we have demonstrated for the first time that no relationship exists between metrics of LV function and myocardial tissue characterization in NIDCM patients. Our study showed that T1 mapping and ECV values could have high levels despite the fact that LVEF was relatively unchanged. Thus, we suggest that MF could be an independent predictor of risk factors, in addition to the ventricular functional findings. The use of T1 mapping and ECV methods are as important as cardiac functional assessments for evaluation of the prognostic stratification of NIDCM patients. Further investigations are needed to determine the cut-off values for ECV and T1 mapping to prevent SCD, arrhythmogenesis, and heart failure.

There are several limitations to our study. First, although to the best of our knowledge, this study examined the



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largest group of NIDCM patients assessed using the ECV technique, our study cohort was relatively small. Therefore, a larger cohort is needed to generalize the findings. Second, we did not correlate our CMR imaging findings with the results of histological methods. However, a previous study of the detection of MF using CMR imaging showed that ECV images were closely correlated with fibrosis that had been histologically verified [43].

In conclusion, the evaluation of cardiac function alone is inadequate for prognostic stratification. Based on this premise, we demonstrated that for NIDCM patients, MF is unrelated to cardiac functional findings obtained using 3.0 T MRI. Therefore, we propose that these patients should be evaluated with CMR imaging using tissue characterization techniques, in addition to cardiac functional analysis. Further research is needed to confirm our findings and evaluate MF in NIDCM patients.

## Compliance with ethical standards

Conflict of interest All authors declare that they have no conflicts of interest.

**Ethical approval** This study was performed at a single tertiary center and was approved by the local medical ethics committee.

**Informed consent** Informed consent was obtained from each participant included in this study.

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