

Comparison of the effect of region‑of‑interest methods using gadoxetic acid‑enhanced MR imaging with diffusion‑weighted imaging on staging hepatic fibrosis

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Abstract

Objective To evaluate the utility of T1 mapping on gadoxetic acid-enhanced MRI and DWI for staging liver fibrosis and assess the influence of ROI positioning on interobserver variability, T1 relaxation time and ADC value.

Methods This retrospective study was approved by the institutional review board and included 150 patients (mean age 58 years old; 91 men and 59 women). Liver fibrosis stages (S) were histopathologically determined. T1 relaxation time and ADC value of liver were measured by three distinct ROI protocols (the whole left lobe liver, the whole right lobe liver and the individual ROIs). T1 relaxation time measurements were compared with ADC values according to S scores. Interobserver variability for the T1 relaxation times and ADC values by the three distinct ROI protocols was analyzed by calculating the ICC.

Results T1 relaxation time measurements by the three distinct ROI protocols on severe fibrosis stage were significantly higher than the relative values on mild fibrosis stage. The mean ADC values on severe fibrosis stage showed

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no significantly different when measured by means of the whole right lobe liver $(p = 0.057)$ and the individual ROIs $(p = 0.10)$, compared with the relative values on mild fibrosis stage. AUCs of T1 relaxation time and ADC value by the means of the three distinct ROI protocols were 0.614, 0.676, 0.677 and 0.656, 0.585, 0.575 for identification of severe fibrosis stage. The interobserver reproducibility was excellent for measuring the right lobe liver T1 relaxation time and the individual ROIs T1 relaxation time (ICC 0.814, 0.883, respectively).

Conclusions T1 relaxation time measurements by means of the three distinct ROI protocols on gadoxetic acidenhanced MR imaging were a potential biomarker in staging of hepatic fibrosis, which were more accuracy than DWI-ADC measurements. The more reproducible results were obtained when measuring T1 relaxation time of the whole right lobe liver and the individual ROIs.

Keywords Gadoxetic acid · T1 relaxation time · Magnetic resonance imaging · Apparent diffusion coefficient · Liver fibrosis · Observer variation

Introduction

Chronic liver diseases represent a major public health problem, accounting for significantly morbidity and mortality worldwide [\[1](#page-6-0)]. It can lead to hepatic fibrosis, cirrhosis, end-stage liver disease, and portal hypertension and to the development of hepatocellular carcinoma (HCC) [[2,](#page-6-1) [3](#page-6-2)]. The diagnosis of liver fibrosis staging remains an important issue in patients with chronic liver disease. The early detection of fibrosis is important for determining disease progression and postponing the evolution of chronic hepatitis into cirrhosis via the implementation of prompt and

specific treatment. Fibrosis is a part of the innate wound healing response, which occurs in injured tissues [\[4](#page-6-3)]. And within the liver, fibrosis is characterized by the deposition of extracellular matrix. Currently, histopathologic examination of a liver biopsy is still the "gold standard" for liver fibrosis diagnosis and staging [[5,](#page-6-4) [6\]](#page-6-5). However, liver biopsy is an invasive procedure with rarely but potentially lifethreatening complications and prone to sampling errors [\[7](#page-6-6), [8\]](#page-6-7). The patient, who should be monitored the treatment effect, will have liver biopsy repeatedly, and it will increase the rate on complications (haemorrhage in 0.3 % of patients and mortality in 0.01 %) [\[9](#page-6-8)]. Besides, due to sampling errors, liver biopsy is hindered by an approximately 24 % false negative rate for the diagnosis of cirrhosis [\[10](#page-6-9)]. Now the noninvasive methodologies for the assessment of fibrosis have developed, such as the indirect markers of liver injury, computed tomography (CT), transient elastography (TE) and magnetic resonance imaging (MRI) [\[11](#page-6-10), [12](#page-6-11)]. Among them, recent advances in MRI have led to a growing interest in optimizing and applying functional MRI to the assessment of liver disease [\[13](#page-6-12)]. Such MRI methods include diffusion-weighted imaging (DWI), perfusion weighted MRI, and MR spectroscopy. Of these methods, DWI particularly can be easily incorporated into a routine MRI protocol. DWI is based on the random Brownian motion of water molecules within the voxel. This motion can be quantified through the apparent diffusion coefficient (ADC) of protons, which depends on the tissue structure. Li H et al. [[14\]](#page-6-13) showed that hepatic MR-DWI played a key role in evaluating liver fibrosis following transcatheter arterial chemoembolization (TACE) with low doses of chemotherapy.

Gadoxetic acid (Primovist®; Bayer-Schering Pharma AG, Berlin, Germany) is a MR imaging contrast medium that is developed for evaluating the hepatobiliary system. Many studies have showed that it is useful for the detection and characterization of focal liver lesions, HCCs particularly [\[15](#page-6-14), [16\]](#page-6-15). After intravenous injection, gadoxetic acid is gradually taken up by hepatocytes and eventually excreted via the biliary pathway. Furthermore, hepatocyte-phase gadoxetic acid-enhanced MRI can measure hepatocyte function potentially. Previous studies showed that patients with liver dysfunction presented with reduction of liver parenchymal enhancement using gadoxetic acid-enhanced MR imaging on hepatobiliary phase (HBP) by the methods of direct measurement of liver parenchymal signal intensity or calculation of perfusion parameters [\[17](#page-6-16), [18](#page-6-17)].

An alternative approach to direct measurement of signal intensity and perfusion imaging would be to evaluate T1 relaxation time of liver parenchyma, which was directly correlated with the concentration of gadoxetic acid in theory, more reliable and less subjective. To our knowledge, evaluation of gadoxetic acid-enhanced MR imaging for hepatic fibrosis staging has been reported both in animal models and patients [\[19](#page-6-18), [20\]](#page-6-19). But, the methods of drawing region of interest (ROI) are inconformity. The progression of fibrosis to cirrhosis has a number of sequelae. Histological staging of fibrosis is a combinatorial assessment of amount of fibrosis and architectural disorganization. It is a continuous process and it maybe distributes unevenly in the whole liver.

Thus, the purpose of our study is to evaluate the potential biomarker for liver fibrosis staging, and compare the results of T1 relaxation time with DWI-ADC value and assess the influence of ROI positioning on interobserver variability, T1 relaxation time and DWI-ADC value on gadoxetic acid-enhanced MR imaging.

Materials and methods

Patients

This retrospective study was approved by Institutional Review Board of our hospital and the requirement for informed consent was waived. Between January 2013 and October 2015, 350 patients who were suspected of having focal hepatic lesions and underwent preoperative gadoxetic acid-enhanced MRI examination were included. Exclusion criteria consist of (a) non-availability of pre-treatment gadoxetic acid-enhanced MR imaging using T1 mapping; (b) difficulty to measure the ADC/T1 mapping values because of motion artifact; (c) diffuse hepatic lesions; (d) previous liver resection. *F* score was histopathologically determined with hepatectomy conducted to treat hepatic tumors. Finally, 150 patients were evaluated in the study. 91 of the 150 patients were men and 59 were women. Median age was 58 years old (range 25–78). The mean time interval between surgical resection and the MRI examination was 3 days (range 2–7 days).

MR imaging

MR imaging was carried out on a 1.5-T MR system (Magnetom Aera, Siemens Medical Solution, Erlangen, Germany) with phased-array coils. For T1 mapping with Syngo MapIt, a dual flip angle 3D gradient echo sequence with volumetric interpolated breath-hold examination (VIBE) was performed after injection of gadoxetic acid (Primovist®; Bayer-Schering Pharma AG, Berlin, Germany). The parameters were as follows: 4.38/1.93 (repetition time msec/echo time msec); flip angle, 2° and 12°; field of view (FOV), 380-400 \times 300-324 mm; matrix, 216×288 ; 200 cm slab thickness resulting in an interpolated 5-mm section thickness. A parallel imaging technique $(R = 2)$ was performed using generalized

autocalibrating partially parallel acquisition (GAPPA). In all patients, 0.025 mmol/kg body weight of gadoxetic acid was injected manually at about 1 ml/s, by one investigator through a 20-gange intravenous catheter placed in a cubical or cephalic vein. Immediately afterwards, a 20 ml saline flush was administered at the same injection rate. T1 mapping was obtained at 20 min after gadoxetic acid administration for HBP.

Three scan trace free-breath DW images were obtained prior to gadoxetic acid injection using a single-shot spinecho echo planar imaging sequence (TR/TE, 3200/56 ms; slice thickness, 5.5 mm; matrix size, 84×128 ; FOV, 380– $400 \times 300 - 324$ mm) with a b value of 0 and 500 s/mm². A parallel imaging technique $(R = 2)$ was performed using GAPPA.

Imaging evaluation

Quantitative T1 relaxation time maps and ADC maps were derived automatically on a voxel-by-voxel basis. The MR data sets were transferred to a workstation (Leonardo, Siemens, Erlangen, Germany) to measure the T1 relaxation time and ADC value of the liver parenchyma using operator-defined ROI. The MR images were independently analyzed by two radiologists (Cai-zhong Chen and Li Yang), who performed T1 relaxation times and ADC values. The readers were blinded to each other' results, the clinical patient data and pathology reports. They manually drew the ROIs on the T1-weighted images and high b value $(b = 500 \text{ s/mm}^2)$ DW images, except for the border of the liver (to avoid partial volume effects), any visible lesions, major hepatic veins and the inferior vena cava, then copied to corresponding T1 maps and ADC maps.

ROI protocols

The hepatic parenchyma T1 relaxation time and ADC value were measured according to three distinct ROI protocols: (a) the whole left lobe liver; (b) the whole right lobe liver; (c) four ROIs on the liver randomly and mean T1 relaxation time and ADC value for 4 ROIs being considered as the representative measurement for the liver (individual ROIs) (Fig. [1a](#page-3-0)–f).

Histopathology standard

All surgical specimens were evaluated by a senior hepatopathologist with 10 years of experience, having no knowledge of radiologic diagnoses. Fibrosis stages were determined semiquantitatively. Criteria for the fibrosis stages were as follows: F0, no fibrosis; F1, fibrous portal expansion; F2, bridging fibrosis; F3, bridging fibrosis with architectural distortion; and F4, cirrhosis [[18\]](#page-6-17).

Statistical analyses

Statistical analyses were performed using MedCalc (Med-Calc for Windows, version 11.5.0.0, www.medcalc.be). Interobserver variability for the T1 relaxation times and ADC values of the two readers for the right lobe liver and the left lobe liver and for the each individual ROI method were analyzed according to the method of Bland and Altman and by calculating the intraclass correlation coefficient (ICC) (0.00–0.20 poor, 0.21–0.40 fair, 0.41–0.60 moderate, 0.61–0.80 good and 0.81–1.00 excellent correlation). T1 relaxation times and ADC values were averaged between the two observers for further analyses. The correlations between MR measurements (T1 relaxation time and ADC value) and *F* scores were assessed using Spearman's rankcorrelation test. The T1 relaxation time and ADC value, respectively, were compared between F scores (≤ 2) and F scores (\geq 3) using a Student's *t* test when normally distributed or Mann–Whitney *U* test when not normally distributed. In addition, receiver operating characteristics (ROC) analyses were constructed to determine the potential diagnostic performance for differentiating F scores (≤ 2) from F scores (≥ 3) patients. Corresponding areas under the ROC curve (AUCs) and 95 % confidence intervals (95 %) CI) were calculated. Difference in diagnostic performance was analyzed by comparing the ROC curves. Difference in AUCs was analyzed by comparing the ROC curves according to the method of DeLong et al. [[19\]](#page-6-18). Difference with a *p* value smaller than 0.05 was considered statistically significant.

Results

Baseline patients' characteristics

A total of 150 patients, who underwent partial hepatectomy, were included finally. And the pathological results were as follows: hepatocellular carcinoma, $n = 89$; intrahepatic cholangiocarcinoma, *n* = 13; hemangioma, *n* = 15; cirrhosis, $n = 3$; focal nodular hyperplasia, $n = 9$; colorectal liver metastases, $n = 12$; inflammatory nodules, $n = 2$; degenerative nodule, $n = 2$; angiomyolipomas, $n = 3$; hepatocellular adenoma, $n = 2$. Patients were classified as mild fibrosis stage (*F* score \leq 2) and patients were classified as severe fibrosis stage (*F* score \geq 3).

Effect of ROI methods

The mean values of T1 relaxation time and DWI-ADC were displayed in Table [1](#page-4-0) for the mild fibrosis stage and severe fibrosis stage of each respective ROI protocol. The mean T1 relaxation time values on severe fibrosis stage

Fig. 1 a–**f** Examples of placement of regions of interest (ROI) in the liver parenchyma on T1 mapping to measure the T1 relaxation time by the whole left lobe liver (**a**), to measure the T1 relaxation time by the whole right lobe liver (**b**) and to measure the T1 relaxation time by individual ROIs (**c**). Examples of placement of regions of inter-

est (ROI) in the liver parenchyma on ADC map to measure the ADC value by the whole left lobe liver (**d**), to measure the ADC value by the whole right lobe liver (**e**) and to measure the ADC value by individual ROIs (**f**)

were significantly higher when measured by means of the whole left lobe liver ($p = 0.035$), the whole right lobe liver ($p = 0.002$) and the individual ROIs ($p = 0.0006$), compared with the relative values on mild fibrosis stage. The mean ADC values on severe fibrosis stage showed no significantly different when measured by means of the whole right lobe liver ($p = 0.057$) and the individual ROIs $(p = 0.10)$, compared with the relative values on mild fibrosis stage. Only by means of the whole left lobe liver, the mean value on severe fibrosis stage showed significantly lower than the value on mild fibrosis stage $(p = 0.003)$.

Table 1 Influence of choice of regions of interest (ROIs)

ADC apparent diffusion coefficient, values on T1 relaxation time and ADC were compared by means of a paired *t* test

Diagnostic performance for assessment of severe fibrosis stage

The ROC curves performed to compare the diagnostic performance of T1 relaxation time and ADC value by means of the three distinct ROI protocols for assessment of severe fibrosis stage were provided in Table [2.](#page-4-1) AUCs of T1 relaxation time value for identification of severe fibrosis stage were 0.614, 0.676 and 0.677, respectively. AUCs of ADC value for identification of severe fibrosis stage were 0.656, 0.585 and 0.575, respectively. The comparison of ROC analyses on severe fibrosis stage using T1 relaxation time and ADC value by the three distinct ROI protocols were showed in Table [3.](#page-5-0) The values of T1 relaxation time by means of three distinct ROI protocols (AUC 0.614, 0.676 and 0.677, respectively) were better than that of ADC by means of measuring the right lobe liver and the individual ROIs (AUC 0.585, 0.575, respectively) for identification of severe fibrosis stage. However, there was no significant difference among the each measuring methods on T1 relaxation time and ADC value.

Interobserver variability

ICCs between the two readers were provided in Table [4](#page-5-1) for the three distinct ROI protocols. The interobserver reproducibility was excellent for the measuring the right lobe liver T1 relaxation time and the individual ROIs T1 relaxation time (ICC 0.814, 0.883, respectively), and good for measuring the left lobe liver T1 relaxation time (ICC 0.768). For the measuring the ADC values by the three distinct ROI protocols, the ICCs ranged from 0.247 to 0.640.

Discussion

Our study results mainly revealed that T1 relaxation time measurement by the means of the three distinct ROI protocols on gadoxetic acid-enhanced MR imaging showed significantly different between mild fibrosis stage with severe fibrosis stage ($p = 0.035$, $p = 0.002$ and $p = 0.0006$, respectively) and had good accuracy for identification of severe fibrosis stage with AUCs of 0.614, 0.676 and 0.677. However, by means of measuring the whole right lobe liver and the individual ROIs, the mean ADC values on mild fibrosis stage showed no significantly different with the relative values on severe fibrosis stage. The results were in keeping with the previous study. Watanabe et al. [[21\]](#page-6-20) indicated that the contrast enhancement index with gadoxetic acid-enhanced MR imaging was an efficient biomarker in the staging of liver fibrosis and was more accurate than ADC values. It is clinically useful for the hepatologists to determine the stage of fibrosis to manage patients with chronic liver disease properly. The risks of various complications would increase dramatically if patients reached the stage of cirrhosis. Although, there are numerous ways of diagnosing and quantifying liver fibrosis with imaging tools, such as ultrasound methods. The gold standard on non-invasive methods for liver fibrosis detection is still not unanimous. However, a recently developed hepatobiliary contrast agent, gadoxetic acid, has been widely used to determine early-stage carcinogenesis of liver nodules;

Table 2 Diagnostic performance for T_1 relaxation time and ADC value by means of the three distinct receiver operating characteristics (ROC) protocols in assessing severe fibrosis stage

ADC apparent diffusion coefficient, *AUC* area under the ROC curve, 95 % *CI* 95 %confidence interval, *LL* the whole left lobe liver, *RL* the whole right lobe liver, *IN* the whole individual ROIs

Table 3 Comparison of receiver operating characteristics (ROC) analyses on severe fibrosis stage using T_1 relaxation time and ADC value by means of the three distinct ROI protocols

Compared groups	Severe fibrosis stage
	p
LL-T1 relaxation time versus RL-T1 relaxation 0.119 time	
LL-T1 relaxation time versus IN-T1 relaxation time	0.091
LL-T1 relaxation time versus LL-ADC	0.540
LL-T1 relaxation time versus RL-ADC	0.670
LL-T1 relaxation time versus IN-ADC	0.563
RL-T1 relaxation time versus IN-T1 relaxation time	0.984
RL-T1 relaxation time versus LL-ADC	0.768
RL-T1 relaxation time versus RL-ADC	0.195
RL-T1 relaxation time versus IN-ADC	0.144
IN-T1 relaxation time versus LL-ADC	0.746
IN-T1 relaxation time versus RL-ADC	0.179
IN-T1 relaxation time versus IN-ADC	0.129
LL-ADC versus RL-ADC	0.178
LL-ADC versus IN-ADC	0.165
RL-ADC versus IN-ADC	0.838

ADC apparent diffusion coefficient, *LL* the whole left lobe liver, *L* the whole right lobe liver, *IN* the individual ROIs

Table 4 Interobserver variability (measured as the intraclass correlation so efficient) for the different ROI protocols

	The whole left lobe liver	The whole right lobe liver	The individual ROIs
T1 relaxation time	0.768	0.814	0.883
ADC values	0.409	0.247	0.640

0.00–0.20 Poor, 0.21–0.40 fair, 0.41–0.60 moderate, 0.61–0.80 good and 0.81–1.00 excellent correlation

consequently, it has been used to identify early-stage liver fibrosis [\[22](#page-6-21)]. Therefore, we believed that T1 relaxation times could be differential from mild and severe fibrosis stage, which was very useful for the patients both on treatment in time and follow-up effectively. T1 relaxation time is an absolute value, which appears more reliable and less subjective than the direct hepatic signal intensity [\[23](#page-6-22)]. Syngo MapIt enables fast MRI sequencing using 3D-VIBE and has a high resolution [[24\]](#page-6-23). Therefore, we include this sequence in routine liver MR imaging in our department. The signal intensity on liver parenchyma would change during the stage of liver fibrosis with the hepatic architectural disruption. ADC value is significantly influenced by technical parameters, such as the *b* value. Thus, results of ADC values are the lack of a well cut-off value and it is

difficult to be used in clinical practice. Also, in our study, ADC values could not differentiate mild fibrosis stage from severe fibrosis stage and were relatively low for identification of severe fibrosis stage.

Until the end stage, the progression of fibrosis to cirrhosis has a number of sequelae. First it will distort hepatic architecture and vasculature, second it will have a deleterious effect on hepatic function and the third it will increase the propensity for neoplastic transformation. It is a continuous process. Therefore, histological staging of fibrosis maybe distributes unevenly in the whole liver. In our study we showed that T1 relaxation time measurements obtained by the three distinct ROI protocols could all differentiate mild fibrosis stage from severe mild fibrosis stage. But the AUCs of T1 relaxation time values obtained from the whole left lobe liver was relatively low for identification of severe fibrosis stage. We recommended that measuring T1 relaxation time used the ROI protocols of the whole right lobe liver and the individual ROIs.

Another interesting finding was that measuring T1 relaxation time in patients by means of the three distinct ROI protocols was more reproducible. T1 relaxation time measurements obtained from the whole right lobe liver and the individual ROIs were more reproducible than those obtained from the whole left lobe liver. They resulted in excellent interobserver reproducibility (ICC 0.814, 0.883). The main reason may be that the left lobe liver is near to the heart. The signal intensity is affected by the cardiac impulse easily. Besides, sometimes it is affected by the aorta beating artifacts. We also found that ADC values obtained by the means of the three distinct ROI protocols were less reproducible. ADC measurements by means of the three distinct ROI protocols resulted in lower interobserver agreement (ICC 0.247–0.640), compared with T1 relaxation time measurements (ICC $0.768-0.883$). The reasons are as follows: (I) ghosting artifacts; ② low spatial resolution using respiratory-triggered diffusion-weighted imaging.

There were some limitations in our study. Firstly, because of its retrospective nature and the relatively small patients, our study could not avoid sampling bias. Secondly, in our study we only used b value of 0 and 500 s/ mm² to calculate ADC. It might affect the accuracy of ADC values. Another new technique called intravoxel incoherent motion MR imaging (IVIM) has been used, which is a measurement of numerous points of ADC at different *b* values [\[25](#page-6-24)].

In conclusion, T1 relaxation time measurements by means of the three distinct ROI protocols on gadoxetic acid-enhanced MR imaging were a potential biomarker in staging of hepatic fibrosis, which were more accuracy than DWI-ADC measurement. The more reproducible results were obtained when measuring T1 relaxation time of the whole right lobe liver and the individual ROIs.

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Compliance with ethical standards

Conflict of interest There is no any conflict of interest information for all authors.

Ethical statement All procedures performed in studies involving human participants were in accordance with the ethical standards of the institutional. This retrospective study was approved by Institutional Review Board of our hospital and the requirement for informed consent was waived.

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