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# Advanced experimental methods toward understanding biophysicochemical interactions of interfacial biomolecules by using sum frequency generation vibrational spectroscopy

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Sum frequency generation vibrational spectroscopy (SFG-VS) has been demonstrated to be a powerful technique to study the interfacial structures and interactions of biomolecules at the molecular level. Yet most previous studies mainly collected the SFG spectra in the frequency range of  $1500-4000 \text{ cm}^{-1}$ , which is not always sufficient to describe the detailed interactions at surface and interface. Thorough knowledge of the complex biophysicochemical interactions between biomolecules and surface requires new ideas and advanced experimental methods for collecting SFG vibrational spectra. We introduced some advanced methods recently exploited by our group and others, including (1) detection of vibration modes in the fingerprint region; (2) combination of chiral and achiral polarization measurements; (3) SFG coupled with surface plasmon polaritons (SPPs); (4) imaging and microscopy approaches; and (5) ultrafast time-resolved SFG measurements. The technique that we integrated with these advanced methods may help to give a detailed and high-spatial-resolution 3D picture of interfacial biomolecules.

protein, cholesterol, 3D interfacial structures, fingerprint region, amide III, chiral polarization, surface plasmon polaritons, time-resolved

# 1 Introduction

The interface between biomolecules (e.g., amino acids, lipid, peptides, proteins, DNA, RNA, antibodies) and a surface is one of the most ubiquitous environments on earth and in the human body. One important example of such an interface is biological membranes, which are vital components that constitute the barrier between the inside and the outside of a living cell [1]. The interactions between biomolecules and natural surfaces are essential to human well-being. These interactions are not only critical for many cellular processes such as ion transport and cell signaling in a controlled

manner [2, 3], but also play a crucial role in many technological processes including bioseparation, biosensing, biofouling, biomedical implants, and medicine/drug delivery [4–6]. Aside from the natural surfaces that already exist, a number of new artificial surfaces are being developed by combination of science and technology. The rapid growth in nanotechnology greatly enhances the probability of interaction among engineered nanomaterials, humans and the environment, which may result in a series of nanoparticle/biological interfaces [7]. These interactions between nanoparticles and biomolecules (proteins, membranes, cells, DNA, and organelles) lead to the formation of particle wrapping, protein coronas, intracellular uptake and bio-catalytic processes that are directly related to biocompatibility and biodiversity [7]. It is urgent for the emerging

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discipline of bio-interface science to achieve a better understanding of the interactions between biomolecules and surfaces. However, such interactions are still poorly understood due to their complexity as well as the lack of surface-sensitive and label-free techniques. Consequently, solutions to many scientific problems associated with the characterization of such interactions and biomolecular structures at the interface remain elusive. For instance, conceptual structural models for cholesterol-lipid interactions have been the subject of a long lasting debate even though it is well known that the organization and transport of the cholesterol within cell membrane are critical for human health and many cellular functions [8-10]. Furthermore, accurate determination of protein structures and dynamics at interface [11] and knowledge of interactions at the nano-bio interface are two of the most challenging areas within biology and chemistry today [7].

Addressing the complex interactions at bio-interfaces demands new ideas and in situ, real-time and label-free surface methodologies. Techniques such as spectroscopic methods including nuclear magnetic resonance (NMR) and X-ray diffraction have been used to probe the structures of bulk biomolecules. However, most of the current bioanalytical methods that are used to characterize bulk molecules are not sensitive enough to map the inherently small number of molecules bound to a surface. Techniques such as X-ray photo-electron spectroscopy (XPS), secondary ion mass spectrometry (SIMS), scanning electron microscopy (SEM), and scanning tunneling microscopy (STM) are powerful surface-sensitive analytical tools [12], but they require high vacuum to operate or suffer from interference from the surrounding environment, or need exogenous labels. Therefore, they are difficult to be applied to the study of liquid surfaces/ interfaces or buried solid interfaces where most interfacial biomolecules are located. In contrast to the methods mentioned above, sum frequency generation vibrational spectroscopy (SFG-VS) has been demonstrated to be a label-free and highly surface-sensitive method that allows study of molecular structures at interface in different conditions [13-17]. It has several advantages over other analytical techniques: it is intrinsically surface-sensitive, requires small amounts of samples, and can probe surfaces and interfaces in situ in real time [18]. SFG-VS has been applied to the structure and orientation of various molecules in interfacial environments [4, 11, 13-18] in studies that have been summarized in more than 250 review papers. Yet most of these studies have focused on collecting the spectra in the frequency range of  $1500-4000 \text{ cm}^{-1}$ .

As mentioned above, the interactions between biomolecules and surfaces are very complicated. The biomolecules themselves are also complex. For example, the membrane of a biological cell is actually a diverse system that is composed of lipids, proteins, carbohydrates and other molecules such as cholesterol [1, 2]. Because all of the compositions are made up of the elements of C, H, O, and N, different molecules may have similar functional groups. Accordingly, only measuring SFG vibrational spectra in the frequency range of 1500–4000 cm<sup>-1</sup> may not be enough to unambiguously differentiate interfacial biomolecules' structures and interactions. New ideas and advanced experimental methods are therefore indispensable to get more information from the SFG vibrational spectra. In this paper, we introduce some advanced experimental methods for collecting SFG vibrational spectra that our group and others have recently developed. These methods include: (1) detection of vibration modes in the fingerprint region; (2) combination of chiral and achiral polarization measurements; (3) SFG coupled with surface plasmon polaritons (SPPs); (4) imaging and microscopy approaches; and (5) ultrafast time-resolved SFG measurement. It is evident that these advanced methods can determine structures more accurately and give a clearer picture of the interactions of biomolecules at surfaces or interfaces.

### 2 Brief introduction of SFG-VS

SFG-VS is a second-order polarized nonlinear laser technique that involves two pulsed polarized laser beams that are overlapped spatially and temporally on the sample surface (Figure 1). One is a pulsed visible beam (with a fixed frequency in the visible frequency range  $(\omega_{Vis})$  and the other is an infrared beam (with a tunable or broad-band frequency in the infrared frequency range ( $\omega_{IR}$ )). These two overlapped input beams generate a coherent SFG signal at the sum frequency of the two input beams ( $\omega_{SFG} = \omega_{IR}$  +  $\omega_{Vis}$ ). As described elsewhere [13–17], under dipolar approximation, bulk materials that possess inversion symmetry do not generate a sum frequency signal; however, surfaces and interfaces where the symmetry is broken do generate a sum frequency signal. The intensity of the SFG light is linear to the intensity of the two input fields  $I_1(\omega_{\text{Vis}})$ and  $I_2(\omega_{\rm IR})$  and the square of the sample's second-order nonlinear susceptibility ( $\chi_{eff}^{(2)}$ ), as shown in Eq. (1).



Figure 1 Schematics of SFG experimental geometry.

$$I(\omega_{\rm SFG}) = \frac{8\pi^3 \omega_{\rm SFG}^2 \sec^2 \beta}{c^3 n_1(\omega_{\rm SFG}) n_1(\omega_{\rm Vis}) n_1(\omega_{\rm IR})} \times \left| \chi_{\rm eff}^{(2)} \right|^2 I_1(\omega_{\rm Vis}) I_2(\omega_{\rm IR})$$
(1)

where *c* is the speed of light;  $n_i(\omega_j)$  is the refractive index of medium *i* at frequency  $\omega_j$ ;  $\beta$  is the incident angle of the SFG beam (Figure 1); and  $\chi_{\text{eff}}^{(2)}$  is the effective nonlinear susceptibility corrected by the respective Fresnel factors.

As the IR beam frequency is tuned over the vibrational resonance of interfacial molecules, the effective surface nonlinear susceptibility  $\chi^{(2)}_{\text{R,}ijk}$  is enhanced. The subindices *ijk* are the Cartesian coordinates *x*, *y*, and *z*. The frequency dependence of  $\chi^{(2)}_{\text{eff}}$  is described by Eq. (2).

$$\chi_{\rm eff}^{(2)}(\omega) = \chi_{\rm NR}^{(2)} + \chi_{\rm R, ijk}^{(2)} = \chi_{\rm NR}^{(2)} + \sum_{\nu} \frac{A_{\nu}}{\omega - \omega_{\nu} + i\Gamma_{\nu}}$$
(2)

where  $A_{\nu}$ ,  $\omega_{\nu}$ , and  $\Gamma_{\nu}$  are the strength, resonant frequency, and damping coefficient of the vibrational mode ( $\nu$ ), respectively.  $A_{\nu}$  could be either positive or negative, depending on the phase of the vibrational mode. A plot of SFG signal versus IR input frequency shows a polarized vibrational spectrum of the interfacial molecules.  $A_{\nu}$ ,  $\omega_{\nu}$ , and  $\Gamma_{\nu}$  can be extracted by fitting the spectrum.

In terms of polarization of the electromagnetic wave of a polarized light, the light is split into p and s polarizations. The polarized component that is parallel to the plane of incidence is called p polarization, and the component that is polarized perpendicularly to the plane of incidence is called s polarization. Under the SFG experimental geometry shown in Figure 1, the p-polarized light may be resolved into surface electric fields at both the *x* axis and *z* axis at the surface, whereas the s-polarized light has a component solely in the *y* direction [13–17]. Because the SFG light, visible, and IR beams all can be p or s polarization, there are 8 polarization combinations, resulting in 27 elements of  $\chi_{iik}^{(2)}$  (Table 1).

# **3** Overall view of SFG-VS application on interfacial biomolecules

Since the first SFG study was reported by Shen *et al.* [19, 20] in 1987, SFG-VS has been used by many research groups to investigate molecular structures and interactions at surfaces and interfaces. SFG-VS has also been applied to study the molecular structures and interactions of various biomolecules at surfaces and interfaces. Overall, in terms of biomolecules, the applications include lipid [21–32], vesicle [33], cell [34–37], cellulose [38, 39], starch [40], cholesterol [41–45], amino acids [46–48], peptide and protein [11, 18,

**Table 1** Polarization combinations and the elements of  $\chi_{ijk}^{(2)}$  that contribute to the SFG spectra

Polarization combinations <sup>a)</sup>	Elements of $\chi_{ijk}^{(2)}$				
SSP	${\mathcal X}^{(2)}_{yyz}$ , ${\mathcal X}^{(2)}_{yyx}$				
SPS	$oldsymbol{\chi}_{y ext{zy}}^{(2)}$ , $oldsymbol{\mathcal{X}}_{y ext{xy}}^{(2)}$				
PPP	$\chi^{(2)}_{_{XXX}}$ , $\chi^{(2)}_{_{ZZZ}}$ , $\chi^{(2)}_{_{XXZ}}$ , $\chi^{(2)}_{_{ZXX}}$ , $\chi^{(2)}_{_{XXX}}$ , $\chi^{(2)}_{_{ZXZ}}$ , $\chi^{(2)}_{_{ZXZ}}$ , $\chi^{(2)}_{_{ZZX}}$ , $\chi^{(2)}_{_{ZZZ}}$				
PSS	${\mathcal X}^{(2)}_{zyy}$ , ${\mathcal X}^{(2)}_{xyy}$				
PSP	$\chi^{(2)}_{_{XYX}} ,  \chi^{(2)}_{_{XYZ}} ,  \chi^{(2)}_{_{ZYX}} ,  \chi^{(2)}_{_{ZYZ}}$				
SPP	$oldsymbol{\chi}_{yzz}^{(2)}$ , $oldsymbol{\chi}_{yzx}^{(2)}$ , $oldsymbol{\chi}_{yxz}^{(2)}$ , $oldsymbol{\chi}_{yxx}^{(2)}$				
PPS	$oldsymbol{\chi}_{\scriptscriptstyle ZZY}^{(2)}$ , $oldsymbol{\chi}_{\scriptscriptstyle ZXY}^{(2)}$ , $oldsymbol{\chi}_{\scriptscriptstyle XZY}^{(2)}$ , $oldsymbol{\chi}_{\scriptscriptstyle XXY}^{(2)}$				
SSS	${\cal X}^{(2)}_{_{yyy}}$				

a) The polarizations are given in this order: SFG output, visible input, infrared input.

49-56], lipase [57, 58], and DNA [59, 60]. In terms of scientific questions, the applications include bacterial adhesion [61], peptide absorption [62, 63], peptide immobilization [64-66], lipid-membrane interaction [11, 18, 49-56], ligand-protein recognition [67], lipase activity [57, 58], ion-channel formation [68], ionic effects on biointerfaces [69, 70], hydrophobic mismatching [71, 72], nanomaterials and lipid interactions [73], lipid phase kinetics [29], and lipid flip-flop [74]. Numerous reviews have summarized these applications [51-55, 75-88]. For example, Hore et al. [51] recently published an excellent review paper to introduce the study on biomolecular structure at solid-liquid interfaces using SFG-VS. We wrote a book chapter to introduce how to use SFG-VS to determine the structure and orientation of interfacial proteins [52]. Table 2 contained a list of the review papers published since 1994 [51-55, 75-88]. Summarily, SFG vibrational spectra can provide the following information about surfaces and interfaces: (1) the kinds of molecular species (or chemical groups); (2) the ordered or disordered degree of the molecules; (3) change in molecular structure; (4) molecular absorption and the orientation of functional groups; (5) interfacial hydrogen-bond networks; (6) assignment of vibrational modes; and (7) surface chirality.

# 4 Advanced experimental methods for SFG study

It is not easy to understand the biophysicochemical interactions of interfacial biomolecules. It requires employing new ideas and developing advanced experimental methods to accurately determine the interfacial molecular structures and dynamics. According to recent SFG-VS studies, the advanced experimental methods mentioned in the introduction section have greatly expanded the possibility of obtaining a

Table 2 Review papers on the SFG-VS applications for biomolecules at surfaces and interfaces [51–55, 75–88]

Year	Title	Biomolecules	Interface	Signals	Ref.
2014	Biomolecular structure at solid-liquid interfaces as revealed by nonlinear optical spectroscopy	Amino acids, peptides and proteins, carbohydrates, DNA, lipids, cells	Solid/liquid	OH, CH <sub>2</sub> , CH <sub>3</sub> , amide I, N–H	[51]
2014	Sum frequency generation vibrational spectroscopy: a sensitive technique for the study of biological molecules at interfaces	Peptides, proteins, lipid bilayer, nucleic acids	Solid/liquid	CH <sub>2</sub> , CH <sub>3</sub> , amide I, N–H	[75]
2013	Elucidation of molecular structures at buried polymer interfaces and biological interfaces using sum frequency generation vibrational spectroscopy	polymer materials, protein, model cell membranes, DNA	Air/liquid, air/solid, solid/liquid	OH, CH <sub>2</sub> , CH <sub>3</sub> , OCH <sub>3</sub> , amide I	[76]
2013	Sum-frequency vibrational spectroscopic studies of Langmuir monolayers	Lipid monolayer, membrane-bound water	Air/water	OH, CH <sub>2</sub> , CH <sub>3</sub> , OD, CD <sub>2</sub> , CD <sub>3</sub> , PO <sub>2</sub> <sup>-</sup>	[77]
2013	Structure and orientation of interfacial proteins deter- mined by sum frequency generation vibrational spectros- copy: method and application	Peptides, proteins	Solid/liquid, air/liquid	Amide I	[52]
2013	Characterization of crystalline cellulose in biomass: basic principles, applications, and limitations of XRD, NMR, IR, Raman, and SFG	Cellulose	Air/solid	OH, CH <sub>2</sub> , CH <sub>3</sub> , OD, amide I	[78]
2013	Nano-bio interfaces probed by advanced optical spec- troscopy: from model system studies to optical biosensors	Peptides and proteins, nano-bio interface	Solid/liquid Air/solid	CH <sub>2</sub> , CH <sub>3</sub> , amide I	[79]
2012	Molecular interactions of proteins and peptides at inter- faces studied by sum frequency generation vibrational spectroscopy	Proteins, peptides	Solid/liquid	CH <sub>2</sub> , CH <sub>3</sub> , CD <sub>2</sub> , CD <sub>3</sub> , amide I	[53]
2012	Molecular structures of buried polymer interfaces and biological interfaces detected by sum frequency genera- tion vibrational spectroscopy.	Polymers, peptides	Solid/liquid	OH, CH <sub>2</sub> , CH <sub>3</sub> , SiCH <sub>3</sub> , amide I	[80]
2011	Chiral vibrational structures of proteins at interfaces probed by sum frequency generation spectroscopy	Peptides and proteins	Air/liquid	CH <sub>2</sub> , CH <sub>3</sub> , amide I, N–H	[54]
2011	Nonlinear spectroscopy of bio-interface	Polysugars, proteins, biopolymer, SDS surfactant	Air/solid, metal surface,	CH <sub>2</sub> , CH <sub>3</sub> , OSO <sub>3</sub> <sup>2–</sup> , fingerprint modes	[81]
2009	<i>In situ</i> molecular level studies on membrane related pep- tides and proteins in real time using sum frequency gen- eration vibrational spectroscopy	Lipids, peptides, proteins	Solid/liquid, air/liquid	CH <sub>2</sub> , CH <sub>3</sub> , CD <sub>2</sub> , CD <sub>3</sub> , amide I	[55]
2009	Nonlinear optical spectroscopy of soft matter interfaces	Phospholipid monolayer, colloidal surface	Air/water Solid/liquid, air/solid	CH <sub>2</sub> , CH <sub>3</sub>	[82]
2009	Optical methods for the study of dynamics in biological membrane models	Lipid monolayer	Air/liquid	OH, CH <sub>2</sub> , CH <sub>3</sub>	[83]
2009	Sum frequency generation studies on bioadhesion: eluci- dating the molecular structure of proteins at interfaces	Fibrinogen, factor XII, mefp-3	Solid/liquid	CH <sub>2</sub> , CH <sub>3</sub> , amide I,	[84]
2006	New insights into lung surfactant monolayers using vibrational sum frequency generation spectroscopy	Lipid monolayer, surfactant monolayer	Air/water	CH <sub>2</sub> , CH <sub>3</sub> , CD <sub>2</sub> , CD <sub>3</sub> , PO <sub>2</sub> <sup>-</sup>	[85]
2006	SFG studies on interactions between antimicrobial pep- tides and supported lipid bilayers	Antimicrobial peptides, lipid bilayer	Solid/liquid	OH, CH <sub>2</sub> , CH <sub>3</sub> , CD <sub>2</sub> , CD <sub>3</sub> , amide I	[86]
2005	Sum frequency generation vibrational spectroscopy stud- ies on molecular conformation and orientation of biolog- ical molecules at interfaces	Proteins, peptides, amino acids, lipid monolayers, lipid bilayers,	Solid/liquid, air/liquid	CH <sub>2</sub> , CH <sub>3</sub> , amide I, amide A,	[87]
1996	What do nonlinear optical techniques have to offer the biosciences?	Amine monolayer, lipid	Air/water	OH, CH <sub>2</sub> , CH <sub>3</sub>	[88]

thorough knowledge of interfacial biomolecules. Our discussion here begins with the SFG studies on the detection of fingerprint-region vibrational modes.

### 4.1 Detection of vibrational modes in fingerprint region

Molecular vibrational spectra have been proven to be a highly sensitive way to probe molecular structures and interactions [89, 90]. The vibrational frequencies are split into two regions: functional-group region  $(4000-1500 \text{ cm}^{-1})$  and fingerprint region  $(1500-400 \text{ cm}^{-1})$  [22, 91]. The vibrational

peaks in the functional-group region are characteristic of specific kinds of bonds. But the molecules with the same functional groups have similar spectra. The peaks in the fingerprint region are contributed by the skeletal vibrations of the molecule or some particular bond stretching (C–O [92],  $CF_2/CF_3$  [93], surfactant sulphate group [94–96], phospholipid phosphate group [22], carboxylate [93], azo group [97], and flavin aromatic ring [98]). In general, the bands associated with skeletal vibrations are likely to conform to a unique fingerprint of the entire molecule or large fragments of the molecule, rather than a specific group within the molecule [91]. In short, the functional group

region can be used to identify which kind of functional group is present, whereas the fingerprint region can be used to positively identify the molecule when its information is used with information indicated by the functional-group region.

As shown in Table 2, SFG-VS is extensively utilized to probe the vibrational modes in the functional group region, yet studies in the fingerprint region are quite rare because of the limited tunability of IR light sources [51–55, 75–88]. With the recent and continuing development of more powerful and reliable pulsed-infrared laser sources (picosecond and femtosecond), it has become possible to detect the vibrational modes in the fingerprint region. Currently, the studies of interfacial biomolecules in the fingerprint region can be classified into three main subjects: head-group motions of surfactant or phospholipid molecules, skeletal vibrations of biopolymers, and amide III signals of proteins.

# Head group motions of the surfactant and phospholipid molecules

Amphipathic molecules such as phospholipid are important components of cell membranes. These molecules consist of hydrophobic tailed alkyl chains and hydrophilic head groups. Although the tailed alkyl chains have been well studied by probing the  $CH_2$  and  $CH_3$  functional groups, few reports have been submitted on the head groups whose vibrational frequencies are typically in the fingerprint region. Richmond *et al.* [95, 96] reported the first SFG measurement of the molecular structure and orientation of the head group of a charged alkyl surfactant. They used sodium dodecyl sulfate (SDS) as a prototype system and demonstrated how to use polarization experiments to determine the interfacial orientation of sulfate modes (SO<sub>3</sub> symmetric stretch) in the 1100 cm<sup>-1</sup> region [95, 96]. Subsequently, the Allen group studied the hydration behavior of the phosphate group of a DPPC lipid monolayer by measuring the frequency in the fingerprint region [22]. They observed the peak position of the  $PO_2^-$  symmetric stretch in the liquid-expanded (LE) phase at about 1094 cm<sup>-1</sup> and that it shifted to higher frequency at 1104 cm<sup>-1</sup> upon compression to the liquidcondensed (LC) phase (Figure 2). They were able to well explain the change in hydration state of the DPPC monolayer using a water-squeeze-out process model because the strong hydrogen-bonding network between water molecules and the phosphate group in the LE phase weakened the  $PO_2^{-}$  bonds and then led to peak-shift at a lower frequency  $(1094 \text{ cm}^{-1})$  than the LC phase  $(1104 \text{ cm}^{-1})$ . They finally concluded that lipid head-group hydration is a crucial factor regulating lung-surfactant interfacial behavior during inhalation and exhalation [22].

#### The skeletal vibrations of biopolymers

In principle, the structure and orientation of a small molecule can be determined by detecting its functional groups. However, biomolecules such as polymers, peptides, and proteins are usually very large and have quite complicated structures. They can form structures at different-level (i.e., primary, secondary, and tertiary). Because the differentlevel structures have the same functional groups, it is impossible to access the details of secondary and tertiary structures by analyzing the functional groups alone. By contrast, the skeletal vibrations in the fingerprint region often arise from the movement of several chemical groups



Figure 2 (a) SSP BBSFG spectra of the DPPC- $d_{62}$  monolayer in the fingerprint region at two different surface pressures; (b) illustration of the watersqueeze-out process (blue dots representing water molecules) [22].

or an entire molecule, rather than a localized vibration of single chemical bond. These delocalized modes are extremely sensitive to the backbone conformation and tertiary 3D structure changes in a molecule. Therefore, it is feasible to deduce complicated 3D structures by probing the vibrational modes in the fingerprint region combined with the modes in functional group region. In order to get highpower pulsed-infrared energy for SFG experiments in the fingerprint region, Roke et al. [99] developed a modified Ti:Sapphire laser based on a three-stage chirped-pulse amplification scheme. Using the pulses from that system, they measured the fingerprint-region delocalized modes of a biopolymer (poly(lactic acid) (PLA)) with different crystalline states and successfully determined its 3D surface structure as amorphous L-PLA (L-A), crystalline L-PLA (L-C), and racemic D/L-PLA (R) (Figure 3) [100]. By probing the delocalized vibrational modes, they observed dramatic changes in the 3D arrangement of the surface molecular backbones (Figure 3(a)). This type of information could not be obtained from probing only localized group modes (Figure 3(b)).

### Amide III signal of proteins and peptides

Proteins (peptides) are essential for humans and are especially important molecules of cell membranes. The studies on interfacial structures of proteins and peptides at interfaces are extremely important because they can provide vital understanding in many important fundamental research projects and real applications. It has recently been demonstrated that SFG-VS is a unique and powerful technique for probing structures of peptides and proteins at interfaces. The backbone vibrations of proteins are known as the amide vibrations in three different energy regions, known as amide I, II, and III. Because the signals of amide II and amide III bands are too feeble to be detected, previous research has mainly focused on the side-chain signals and amide I signals in SFG-VS studies. It is evident that  $\alpha$ -helical and β-sheet structures can be identified by probing the backbone amide I vibration. However, the amide I vibrations (which arise mainly from the C=O stretching vibration with minor contributions from the out-of-phase C-N stretching vibration) have at least three weaknesses. The first weakness is that the amide I signals are seriously overlapped with the signal from water bending modes at ~1645  $\text{cm}^{-1}$ . Therefore, infrared (IR) energy loss due to the absorption in atmosphere by water vapor can often introduce some errors and uncertainties in interpretation of SFG-VS results. The second weakness is that the characteristic amide I bands of various secondary structures are clustered in the spectral region of 1600–1700 cm<sup>-1</sup>. The third weakness is that the center frequency of  $\alpha$ -helical and random-coil structures overlap in the frequency of ~1655 cm<sup>-1</sup> [101, 102]. Consequently, it becomes extremely difficult, if not impossible, to accurately differentiate the random-coil and  $\alpha$ -helical structures at the interface. Conversely, the so-called amide III<sub>3</sub> bands (denoted as amide III below) comprise the spectral range between about 1200 and 1400 cm<sup>-1</sup> and no water interference occurs in this region [103]. Amide III bands are predominated by the in-phase combination of C-N stretching and N-H in-plane bending. For various secondary structures of proteins, amide III bands are more resolved and better defined than amide I bands. Because the amide III frequency is known to be particularly sensitive to the polypeptide backbone conformation and tertiary structure, consideration of the amide III bands can, at least in principle, resolve the difficulties in determining interfacial protein structures using amide I bands. Accordingly, it is important



**Figure 3** (a) SFG spectra of L-crystalline (L-C), L-amorphous (L-A), and racemic (R) PLA films in the fingerprint region (taken with three different IR pulses, which are displayed at the bottom); (b) SFG spectra of the same structures in the functional-group region. The right insert of (b) shows the Crossed-polarized microscopy images of the L-C and L-A films which reflect the difference in the state of the films. SFG-VS experimental geometry and Chemical repeat unit of L-PLA are illustrated in the left insert of (a) [100].

to extend SFG-VS studies to the fingerprint region to get more useful information with which to elucidate the molecular structure of peptides and proteins at interfaces. Certainly, it is impossible to determine interfacial protein structure using amide III bands alone. To address this measurement gap in the structural characterization of interfacial proteins, we recently demonstrated for the first time that SFG-VS can unambiguously differentiate interfacial protein secondary structures by combining surface-sensitive amide I and amide III spectral signals [11]. In order to obtain the hardly-measureable SFG signals in the amide III region, we recently employed several newly developed technical procedures: (1) a near-total-internal-reflection geometry; (2) assigning higher voltage to the detector of PMT; and (3) equipping a new and longer difference-frequency generation (DFG) crystal to generate a stable IR pulse with energy > 20  $\mu$ J. With these improvements, we have successfully probed the very weak amide III signals of several antimicrobial peptides (AMPs) in negatively charged lipid bilayers (Figure 4) [11]. These AMPs include LKα14, mastoparan X (MP-X), cecropin P1 (CP-1), pardaxin, and melittin. Although NMR and CD results suggested that these peptides have different helicities [11], the SSP spectra in the amide I region (Figure 4(B)) are all dominated by a single resonance peak centered at 1655  $\rm cm^{-1}$ , which does not permit us to distinguish the random-coil structure from the  $\alpha$ -helical structure. In contrast to a single peak observed in the amide I region, the amide III spectra (Figure 4(C)) show two peaks with the frequencies below (Peak 1, Figure 4(C-e)) and above (Peak 2, Figure 4(C-a)) 1260 cm<sup>-1</sup>. A linear correlation is also clearly observed between the peak amplitude ratio of  $\chi^{(2)}_{Peak1} / \chi^{(2)}_{Peak2}$  and the content ratio of the disordered structure [11]. As indicated in Figure 4, the method that combines surface-sensitive amide I and amide III spectral signals can unambiguously

identify the  $\alpha$ -helical and random-coil structures for interfacial proteins, which resolves one of the most important long-standing problems in interfacial protein science [11].

By monitoring an amide III signal, we can also get an indepth insight into how the lipid-charge status and the solution ions affect the interfacial interaction between peptides and model cell membranes. Figure 5(A) shows the SSP amide III spectra of pardaxin in fully negatively charged DMPG and partly negatively charged DMPC/DMPG (molecular ratio = 3:1) bilayer. The intensity ratio between the peak at ~1230 cm<sup>-1</sup> (Peak 1) and the peak at ~1280 cm<sup>-1</sup> (Peak 2)  $(\chi^{(2)}_{Peak1} / \chi^{(2)}_{Peak2})$  increased from 0.34 to 0.73 when the negative charge of the membrane decreased from 100% to 25%. This result indicates that pardaxin undergoes a conformational change from the random-coil structure to the  $\alpha$ -helical structure with the increase of the fraction of the negatively charged lipids. Figure 5(B) presents the timedependent spectra in the amide III region after a certain amount of phosphate buffer solution was injected into the melittin-DPPG bilayer system. Following the addition of the salt solution, we observed that the signals of the peaks at ~1230 and ~1280 cm<sup>-1</sup> both gradually increased, whereas the ~1115 cm<sup>-1</sup> peak from symmetric mode of PO<sub>2</sub> decreased and finally disappeared. This information deduced from the signals in the amide III region may suggest that the interaction between melittin and DPPG bilayer in the phosphate buffer solution follows a toroidal model. The phosphate ions may also change the helicity of melittin.

# 4.2 Combination of chiral and achiral polarization measurements

Chiral molecules are the molecules that can not be superimposed by translation and rotation on their mirror images [104, 105]. Accordingly, chiral molecules do not have



**Figure 4** The SSP amide spectra of the peptides in lipid bilayers [11]. (A) Schematics of secondary structures with red helix and blue random coil given by NMR studies; (B) the amide I spectra; (C) the amide III spectra. (a)  $LK\alpha 14$ ; (b) MP-X; (c) CP-1; (d) pardaxin; (e) melittin.



**Figure 5** (A) The amide III SSP spectra of pardaxin in mixed DMPC/DMPG (3/1) bilayer (a) and pure d-DMPG lipid bilayer (b); (B) time-dependent spectra in amide III region after a certain amount of phosphate buffer solution was injected into the melittin-DPPG bilayer system [11].

symmetry planes, inversion centers, or improper rotation axes. Because of the lack of inversion symmetry in chiral molecules, SFG is a specifically powerful and effective method for probing molecular chirality [106–108]. In terms of the features of a chiral molecule, the 3D characteristics of chirality require the three subindices *ijk* of  $\chi_{R,ijk}^{(2)}$  to be different ( $i \neq j \neq k$ ) [104, 105]. In other words, the polarization combinations of PSP, SPP, and PPS in Table 1 are termed as chiral polarizations while others are achiral polarizations. Thus surface chirality can be probed by using the PSP, SPP, and PPS polarizations. In this case, the interference from the backgrounds of achiral solute and solvent molecules at the interface can be eliminated because the SFG signals from the achiral molecules are all silent in PSP (or SPP or PPS) spectra [104, 105].

In nature, most molecules in natural biological systems are chiral, from amino acids to sugars, nucleic acids, proteins, and hormones [106–110]. For example, except for glycine, all amino acids have a chiral carbon center. Chiral molecules have been considered to be the backbones of all life forms. Therefore, SFG measurements that combine chiral and achiral polarization will be indispensable for the characterization of the molecular structures and interactions of biomolecules at surfaces and interfaces. However, chiral SFG studies are unusual compared to the thousands of SFG reports in web of science. Only biomolecules such as amino acids [47, 111], peptides and proteins [112–121], 6-keto-cholestanol [122], and DNA [123, 124] have been examined using chiral SFG-VS.

#### The study of peptides and proteins

Peptides and proteins may form different secondary structures (e.g.,  $\alpha$ -helix,  $3_{10}$ -helix, anti-parallel  $\beta$ -sheet, and parallel  $\beta$ -sheet) [52]. The repeat units of these secondary structures have symmetries of  $C_{18/5}$ ,  $C_{3\nu}$ ,  $D_2$ , and  $C_2$ , respectively. As a consequence,  $\beta$ -sheet structures generate chiral signals but the real helical structures do not (Table 3), which allows us to distinguish the  $\beta$ -sheet structures from the helical structures. The Chen group [117] first developed chiral SFG to probe interfacial protein structures using PSP and SPP polarization combinations. They detected chiral amide I signals from a peptide of tachyplesin I, which forms an anti-parallel  $\beta$ -sheet structure on a polystyrene surface. Later, they developed a method for quantifying the orientation of the interfacial  $\beta$ -sheet structure by analyzing both achiral SSP and chiral PSP SFG spectra in the amide I region, as well as combining attenuated total reflectance Fourier transformation infrared spectroscopic measurements (ATR-FTIR) [118]. Recently, Yan's group not only applied the chiral SFG to identify secondary structures of proteins at interfaces through measuring the chiral and achiral signals in amide I and amide A (N-H) regions [119] but also probed the kinetics of conformational changes of amyloid proteins at lipid monolayer surfaces by using an amide I signal [120]. They also monitored the proton exchange rate in interfacial antiparallel β-sheet proteins using chiral signals in the N-H/N-D regions [121] and examined the self-assembly of an amphiphilic peptide (LK7B) into macromolecular chiral structures by using chiral signals from the C-H stretch [113].

It is worth mentioning that the Yan's group claimed that the chiral N–H signal can be used as a vibrational optical marker to distinguish protein secondary structure at interfaces based on the unique spectral features for the observed random coils,  $\alpha$ -helices, and  $\beta$ -sheets at interfaces. They claimed that the  $\alpha$ -helix structures show chiral N–H stretch signals but are silent in the amide I chiral spectra, while the  $\beta$ -sheet structures show the amide I chiral spectra, but do not have chiral N–H stretch signals [119]. These conclusions

Secondary structure	Repeating residues	Symmetry	SFG active modes	Peak center (cm <sup>-1</sup> )	Chiral
α-Helix	3.6	$C_{18/5}$	A, $E_1$	~1655	No
3 <sub>10</sub> -Helix	3	$C_{3v}$	A, $E_1$	~1635	No
Anti-parallel β-sheet	4	$D_2$	$B_1$	~1685	Yes
			$B_2$	~1630	Yes
			$B_3$	~1720	Yes
Parallel β-sheet	2	$C_2$	А	~1625	Yes
			В	~1670	Yes

Table 3 Properties of different types of secondary structures of proteins [52]

contradict not only our recent study of prion protein [125] but also their own results on proton exchange in antiparallel  $\beta$ -sheets at interfaces [121]. Recently, we used a prion protein fragment (PrP118-135) as a model and investigated the influence of the concentration of the protein fragment on interactions between PrP118-135 and a POPG lipid bilayer [125]. We found that the fragment adopted mostly in α-helices at low concentrations. As the PrP118-135 concentration increased, the SSP signals from the peak at 1657  $cm^{-1}$  at the concentration of > 0.03 mg/mL, which is characteristic of an  $\alpha$ -helical structure and are much weaker than those at the concentration of  $\leq 0.03$  mg/mL. Conversely, the intensity of PSP signals at 1625 and 3300 cm<sup>-1</sup> increased with the increasing concentration (Figure 6). By analyzing the SFG spectra at different polarization combinations, we can conclude that the molecular number ratio of parallel β-sheet structures on a POPG bilayer increases with prion concentration and reaches 44% at the prion concentration of 0.10 mg/mL. The  $\alpha$ -helical structures were oriented close to perpendicular to the surface normal, while the  $\beta$ -sheet structures were oriented parallel to the lipid bilayer. In addition, our results suggested that the chiral N–H stretch signals (the PSP N-H signals) mainly arise from the α-helical structure due to the leakage of SSP and PPP spectra at low PrP concentrations and from the  $\beta$ -sheet structure

at high PrP concentrations. Therefore, the chiral N–H signal cannot be used to distinguish protein secondary structures at interfaces.

#### Organization and transport of cholesterol

Currently, combination of chiral and achiral polarization measurements is mainly applied to the studies on interfacial peptides/proteins. Recently, we reported the first application of chiral SFG-VS on the organization and transport of cholesterol in a model cell membrane [122]. Cholesterol is a ubiquitous component of mammalian plasma membrane. The organization and transport of the cholesterol within cell membranes are known to be critical for human health and many cellular functions [8, 126]. However, a precise molecular description of cholesterol behavior within a membrane remains elusive due to the lack of surface-sensitive and label-free techniques [8-10]. Cholesterol is a molecule that comprises a near-planar tetracyclic-fused chiral steroid ring and a flexible achiral isooctyl hydrocarbon tail. The chiral sterol ring has two sides: one side is flat and smooth with no substituent ( $\alpha$  face), and the other is rough with chiral methyl substitutions ( $\beta$  face). Hence, a combination of achiral-sensitive SSP and chiral-sensitive PSP polarization measurements can permit the explicit differentiation of structural change of cholesterol isooctyl tail and methyl substitutions of cholesterol sterol rings. In this case, the



Figure 6 SFG spectra of PrP118–135 in POPG/POPG bilayer at different concentrations in amide I region [125]. (a) SSP in amide I region; (b) PSP in amide I region; (c) PSP in amide A region. Solid line represents the fitting profile.

structural change of chiral methyl substitutions can be monitored using the PSP spectra without interference from lipid, cholesterol hydrocarbon tail, or membrane-bound water molecules. To materialize this idea, we used cholesterol analog 6-ketocholestanol (6-KC) as a model to investigate the interactions between cholesterol and neutral lipid bilayer in situ and in real time. 6-KC has a similar structure to cholesterol except with a keto moiety at the position of the B ring (Figure 7(A)) [122]. For such a molecule, there are three possible forms of side-by-side organization on one leaflet:  $\alpha$ - $\alpha$ ,  $\beta$ - $\beta$ , and  $\alpha$ - $\beta$  (Figure 7(B)). When a flip-flop of 6-KC occurs, tail-to-tail structure will be organized on both leaflets (Figure 7(C)). This different organization will result in a distinct dependence of SSP and PSP intensities upon the 6-KC concentration. According to the SFG symmetry constraints, the formation of tail-to-tail organization on both leaflets (Figure 7(C)) can effectively cancel the SSP signal. Similarly, the formation of  $\alpha$ - $\alpha$  and  $\beta$ - $\beta$  structures (Figure 7(B-a, b)) can effectively eliminate chiral signal but an  $\alpha$ - $\beta$ structure (Figure 7(B-c)) cannot. We investigated the influence of 6-KC concentration on the SSP and PSP intensities. We observed that the SSP intensity (achiral SFG) follows

an almost linear dependence upon the bulk concentration of 6-KC whereas the PSP intensity (chiral SFG) reached a plateau after a certain concentration (Figure 8). Because chiral SFG signals depend mostly on the chiral arrangement of the chiral centers rather than their absolute number, we can conclude that the tail methyl groups of different 6-KC molecules adopt the same orientation direction while the chiral methyl substitutions organize with  $\alpha$ - $\beta$  structure at low 6-KC concentration and  $\alpha$ - $\alpha$  or  $\beta$ - $\beta$  structure at high 6-KC concentration. In addition, we found that the longanticipated flip-flop motion of the cholesterol does not take place in a lipid bilayer at room temperature. Our results favor the so-called umbrella model with the formation of cholesterol clusters [122].

#### 4.3 SFG coupled with surface plasmon polaritons (SPPs)

High signal-to-noise (S/N) ratio and better spectral resolution are goals that a wide range of scientists continues to pursue. High S/N ratio and better spectral resolution can greatly decrease acquisition times. Because plasmon oscillations in metallic nanostructures can cause large amplification



**Figure 7** (A) Molecular structure and defined molecular axis of 6-KC; (B) possible forms of side-by-side organization of 6-KC on one leaflet of lipid bilayer ((a)  $\alpha$ - $\alpha$  structure; (b)  $\beta$ - $\beta$  structure; (c)  $\alpha$ - $\beta$  structure; (c) possible forms of 6-KC organizing on both leaflets [122].



**Figure 8** (A) The SSP intensity; (B) PSP intensity change with the 6-KC amount; (C) the maximum SSP intensity at 2865 cm<sup>-1</sup>; (D) PSP intensity at 2935 cm<sup>-1</sup> as a function of the 6-KC amount [122].

of the local electric field, surface plasmon polaritons (SPPs) have attracted great attention for their potential applications through spectroscopy [127]. Here, SPPs are electromagnetic waves trapped at the conductor/dielectric interface and evanescently confined in the perpendicular direction [128]. These electromagnetic waves arise via the coupling of the electromagnetic fields to oscillations of the conductor's electron plasma [128]. The coupling of optics with SPPs can largely increase the yield of nonlinear optical processes because the light energy is condensed into subwavelength volumes and can thereby reach higher spectroscopic sensitivity [128-130]. One of the most well- known examples of this effect is surface-enhanced Raman spectroscopy (SERS) [131]. Therefore, coupling of SFG-VS with SPPs may provide a major solution to the problem of accessing high S/N ratio. In fact, SPPs have been proved to be compatible with SFG-VS. To date, several SPPsenhanced SFG phenomena have been explored. It is evident that the total SFG intensity is enhanced from several tens to ten thousands times. For example, Yakovlev et al. [132, 133] first observed that the SFG signals of the thin organic films and fullerene films on silver could be enhanced by excitation of a surface plasmon on silver. Baldelli et al. [134] reported that the SFG signal of CO adsorbed on platinum particles of 45 nm diameter was  $\sim 10^4$  times larger than that from CO on smooth Pt films. Chou et al. [135] examined the SFG signals of an octadecanethiol self-assembled monolayer on an AgFON surface and found that the SSP SFG signals were enhanced by up to 730 times. Busson et al. [136] showed that an enhancement factor of 21 could be deduced for the SFG signal of thiophenol adsorbed on gold nanoparticles with an average diameter of 17 nm. Lis et al. [129] investigated the enhancement of SFG signals from molecules adsorbed on metallic nanopillars excited at a resonance frequency that matched their localized surface plasmons. This nanostructured platform increased the molecular SFG signal of a monolayer by two orders of magnitude (Figure 9) [129]. Most recently, Liu and Shen [137] successfully demonstrated the feasibility of measuring in situ and real-time vibrational spectra during electrochemical (EC) reactions at noble metal gold electrodes by using SP-enhanced SFG-VS carried out with Kretschmann geometry (Figure 10). Unfortunately, the application of SFG-VS coupled with SPPs to the research of interfacial biomolecules remains unexplored. Nevertheless, SPPs-enhanced SFG can largely improve spectral sensitivity and specific spatial selectivity, which will make it a promising platform in the development of analytical biomolecular devices.

#### 4.4 Imaging and microscopy approaches

Imaging and microscopy are the best language that physicists, chemists, materials scientists, and biologists can use to communicate with each other easily and directly. Because SFG vibrational imaging and microscopy (SFG-VI, SFG-



**Figure 9** SFG spectra of dodecanethiol molecules chemisorbed on platinum in SSP polarization (a), gold in SSP polarization (b) [129]. Open circles are the SFG intensities from the gold nanopillar zones on the aforementioned surfaces; open squares are the SFG intensities on the bare flat surfaces. The insets sketch the experimental conditions in which the spectra were recorded.



Figure 10 Schematic of an experimental arrangement for an SP-SFVS setup [137].

VM) provide a natural choice to achieve a chemically selective contrast for the interfacial endogenous biomolecules without interference from other off-target molecules, these methods have become important tools for obtaining spatial information about the dynamic process of biological samples, specifically cellular biology at surface and interface [138, 139]. Several groups have modified their SFG-VS systems to SFG-VI (SFG-VM) and have exploited their new systems to study the biomolecules of proteins, lipids and cells. For example, Raghunathan *et al.* [140] developed a rapid vibrational SFG imaging using a tunable picosecond pulse from a high-repetition-rate (76 MHz) optical parametric oscillator and demonstrated that the vibrationally selective imaging of collagen fibers is achieved with submicrometer lateral resolution. Sakai *et al.* [141] used a homemade SFG-VM with the detected IR wavelength of 6-9 µm to measure the IR super-resolution images of cross sections of a human hair and obtained a submicrometer spatial resolution. Conboy et al. [142] built a simplified SFG-VI setup to characterize lipid bilayer arrays asymmetrically prepared by 1,2-distearoyl-sn-glycero-3-phosphocholine (DSPC):1,2distearoyl (d70)-sn-glycero-3-phosphocholine (DSPC-d70). They successfully exploited this SFG-VI to probe the transition temperature of a patterned DSPC:DSPC-d70 lipid bilayer array and the phase behavior in a multi-component micro-patterned lipid bilayer array (MLBA) prepared using three different binary lipid mixtures (1,2-dioleoyl-sn-glycero-3-phosphocholine (DOPC):DSPC, DOPC:1,2-dipalmitoylsn-glycero-3-phosphocholine (DPPC), and 1,2-dimyristoylsn-glycero-3-phosphocholine (DMPC):DSPC [142]. Fujii et al. [141, 143] used SFG-VI to record the single-cell infrared (IR) imaging of onion (Allium cepa) root cells. As for the applications of SFG-VI and SFG-VM on interfacial biomolecules, in 2013 Chung et al. [139] gave a detailed introduction to biomolecular imaging with coherent nonlinear vibrational microscopy. It is worth mentioning that most of the previous SFG microscopy studies collect the SFG signals in the CH-stretching vibrational range and had a limited spatial resolution (up to a few hundred nanometers) due to the diffraction of light or the wavelength of visible light. In order to improve the spatial resolution, a combination of different methods is required. Because the light can be confined to a nanometer region by the excitation of localized surface plasmons at the apex of sharp metal or metal-coated tips [127-131], SPPs-enhanced SFG-VI (SFG-VM) will be feasible to achieve a resolution in tens of nanometers and to improve the S/N ratio for high-speed imaging. In addition, collecting SFG signals in the fingerprint region and using chiral polarization combinations may give a wealth of 3D chemical information [144]. Therefore, the image and microscopy technique integrated with SPPs enhancement, fingerprint region and chiral polarization may help to give a detailed and high-spatial- resolution 3D picture of interfacial molecules.

#### 4.5 Ultrafast time-resolved SFG measurement

Insights into the interfacial molecular structures at static states are necessary but not always sufficient to describe their interaction at surfaces and interfaces. For instance, a complete understanding of the relevant interfacial chemical reactivity and biological processes requires knowledge of interfacial structural dynamics such as the formation of equilibrium surface structures, occurrence of the chemical transformations on surfaces, the coupling between substrate and biomolecules, and the energy transfer or mass transport at the interface, etc. [145–147]. A timescale of these dynamic processes is typically from hundreds femtosecond (fs) to picosecond (ps). Advances in time-resolved SFG-VS experiments may help to provide important information that

cannot be obtained from static experiments. In a timeresolved SFG-VS experiment, an intense fs or ps laser pulse in the visible, near-infrared, infrared region is used to pump the sample to cause electronic, vibrational, and thermal excitation of the molecules and substrates. Next, SFG-VS is used to monitor these transient changes in real time at high temporal resolutions to provide direct information about the structural changes induced by the pump-laser pulse [145–147]; these studies are shedding new light on the translational and vibrational dynamics of interfacial molecule [146-151]. For example, Bonn et al. [146, 147] used this technique to probe the energy-flow dynamics in model membranes and demonstrated the potential of using time-resolved SFG measurement to elucidate biomolecular dynamics at membrane surfaces. Their studies revealed that an incoherent energy transfer occurs from the excited CH<sub>2</sub> groups to the terminal CH<sub>3</sub> groups in the lipid alkyl chains. It takes less than 1 picosecond for the heat to be transferred from the polar head-group region of the lipid to the end of the alkyl chain. However, applications of these timeresolved SFG experiments are not being widely explored at this time. Instead, studies are mainly focused on small molecules such as water. In addition, although two different kinds of SFG systems, a narrow-band frequency scanning system (FSSFG) [145] or a broad-band IR laser system (BBSFG) [146–151], have been exploited for the time-resolved experiments, only a few groups have constructed time-resolved systems: a near-infrared (1064 nm) pump-FSSFG probe system by the Domen group [145], and an fs UV (visible or infrared beam) pump-BBSFG probe by the Shen [149], Bonn [146–148], Borguet [151], Eisenthal [152], and Tahara groups [153]. Because numerous important biological processes at surface and interface depend on rapid dynamic processes such as fast energy-transfer processes, we believe that time-resolved SFG measurements will play a vital role in the deep understanding of the biophysicochemical interactions of biomolecules at surfaces and interfaces.

## 5 Conclusions

Herein, we have summarized the advanced experimental methods on collecting SFG vibrational spectra recently developed by our group and others. These methods include: (1) detection of fingerprint-region vibration modes; (2) combination of chiral and achiral polarization measurements; (3) SFG coupled with surface plasmon polaritons; (4) imaging and microscopy approaches; (5) ultrafast time-resolved SFG measurement. It is evident that application of these advanced methods may help to determine structures more accurately and give a clearer picture of the interaction of biomolecules at surfaces or interfaces. Although we focused these methods on interfacial biomolecules, they will be directly feasible for other interfacial molecules as well.

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