

# **Design, optimization and critical analysis of graphene based surface plasmon resonance sensor for DNA hybridization**

**Yagyesh Kumar1 · Rishi Mishra1 · Ekta Panwar2 · Jaswinder Kaur3 · Ravi Panwar[1](http://orcid.org/0000-0002-9015-0891)**

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### **Abstract**

In this paper, the design, optimization and critical analysis of Surface Plasmon Resonance sensor is presented, which works on angular interrogation method. It comprises of fve layers which are "Prism–Copper–Germanium–Graphene–Sensing medium". The infuence of the chemical potential  $(\mu_c)$  of graphene on the sensor performance has been studied in detail. Thickness of all the layers has been optimized. Remarkable results are achieved for the optimal thickness of copper and germanium layers as 50 nm and 6 nm respectively, while two layers of graphene having  $\mu_c$  of 0.5 eV are introduced to boost-up the performance. Best results in terms of detection accuracy, sensitivity and quality factor have been achieved that fulfll the necessary requirements for good sensing applications.

**Keywords** Surface plasmon resonance · Graphene · Plasmons · Chemical potential · Sensitivity

# **1 Introduction**

SPR sensor has attracted great attention in the feld of medical diagnosis, food safety and air quality monitoring (Tamersit and Djeffal [2016\)](#page-11-0). Generally, SPR sensors have three major components viz. optical system, transducing medium and electronic system. Optical system provides a light wave of the desired wavelength while transducing medium introduces it to the bio-chemical reactants. The electronic system converts the optical signal into the electrical signal using optoelectronic transducers. Kretschmann and Raether [\(1968](#page-10-0)) confguration of the sensor working with angular interrogation method is used for detection of Deoxyribo-Nucleic-Acid (DNA) hybridization (Zeng et al. [2014](#page-11-1)). It has played a keen role in the domain of molecular biology like DNA hybridization.

 $\boxtimes$  Ravi Panwar rpanwar.iitr@gmail.com; rpanwar@iiitdmj.ac.in

<sup>&</sup>lt;sup>1</sup> Discipline of Electronics and Communication Engineering, Indian Institute of Information Technology, Design and Manufacturing Jabalpur, Jabalpur, India

<sup>&</sup>lt;sup>2</sup> Department of Biotechnology, Indian Institute of Technology Roorkee (IIT Roorkee), Roorkee, India

<sup>&</sup>lt;sup>3</sup> Department of Electronics and Communication Engineering, Thapar Institute of Engineering and Technology, Patiala, India

DNA hybridization is a biological event that evaluates the level of dissimilarity between two samples of DNA to obtain the genetic diference between two organisms. The identifcation of a specifc orientation or muted sequence of thymine 'T' and adenine 'A' or cytosine 'C' and guanine 'G', between nucleotide bonds is involved in the DNA hybridization sensing. Surface Plasmons are the oscillation of free electrons at the interface of metal and dielectric having a dielectric constant of opposite sign which are produced when electromagnetic (EM) wave which is Transverse Magnetic (TM) polarized falls on it (Homola et al. [1999](#page-10-1)). These free electron oscillations lead to the generation of Surface Plasmon Wave (SPW), which is p-polarized EM wave and uses the energy of light to propagate. Angular interrogation based SPR sensor uses the SPW waves generated at the junction of prism and metal to examine the changes in the RI of sensing medium.

The concentration of SPW wave is much more in the dielectric than in the metal (Homola et al. [1999\)](#page-10-1), it is highly susceptible to the changes in the optical properties of sensing medium. SPR angle is an important parameter in the angular interrogation system, this method provides better control on the light beam and is quite easy to implement in small sensors (Ronald [2013](#page-11-2)). Monochromatic light source has been used, whose wavelength belongs to near-infrared region (NIR). The light of this wavelength insures minimum damage to biomolecules and other efects like optical non-linearity, Kerr efect, birefringence is also less in the NIR region (Rahman et al. [2018](#page-11-3)). A detailed discussion regarding such conventional SPR sensor has been presented by (Pandey and Sharma [2018](#page-10-2)). The metal layer was coated on the base of the prism by the sputtering technique (Biednov et al. [2015](#page-10-3)). Copper provides a very high degree of accuracy as compared to gold and silver, because of the large SPR ratio (a ratio of real over imaginary part of dielectric constant). Gold has been found to have a poor adsorption property while silver is found to be highly sensitive to oxidation (Verma et al. [2015](#page-11-4); Fu et al. [2015\)](#page-10-4). But at the same time sensitivity obtained by using copper metal is very less and hence polished germanium semiconductor with high refractive index (RI) has been used to increase the sensitivity of the sensor (Li [1980\)](#page-10-5). Various researchers have reported that use of dielectric increases the light trapping capability due to which number of free electrons participating in oscillations increases (Xu et al. [2013](#page-11-5)). An increase in the oscillations increases the concentration of SPW waves and therefore sensitivity increases. Dielectrics also have additional features which are benefcial for SPR sensor like low optical dispersion and transparency in the NIR region. Metal or dielectric are not good adsorbers of biomolecules, therefore a binding material is required for proper detection.

Graphene has high affinity for bio-molecules and serves as a good binding agent due to the large surface area ([Mishra et al. 2016\)](#page-10-6). The binding of biomolecules on graphene is strong and stable, due to interaction between aromatic rings of graphene's hexagonal cells and carbon rings in biomolecules. It has several other useful properties like high carrier mobility, good fexibility and mechanical strength (Pumera [2011](#page-11-6)). Recently, various optoelectronic devices like ultra-fast lasers, solar cells and polarizers are also incorporating graphene (Geim and Konstantin [2010;](#page-10-7) Bonnacorso et al. [2010;](#page-10-8) Muller et al. [2010;](#page-10-9) Xia et al. [2009;](#page-11-7) Zheng et al. [1992](#page-11-8)). Various researchers have also reported its use as Frequency Selective Surface (FSS) (Mishra et al. [2018;](#page-10-10) Mishra et al. [2019](#page-10-11)). But graphene layer causes damping of SPW due to large negative part of RI (Maharana and Jha [2012](#page-10-12)). Thus germanium can serve as a good candidate to overcome it due to its high light absorption property. Graphene chemical potential  $(\mu_c)$  is crucial in deciding the performance of SPR sensor, because it has significant impact on RI of graphene (Bludov et al. [2010](#page-10-13); Kim et al. [2016](#page-10-14)). Further, the impact of  $\mu_c$  on the charge carriers can be explored (Falkovsky [2008](#page-10-15); Chu and Gan [2013](#page-10-16)).

This paper presents a theoretical and mathematical modeling of copper-germanium based, highly sensitive sensor for DNA hybridization. Germanium layer is sandwiched between copper and graphene to enhance the performance. This paper is organized as follows: in Sect. [2](#page-2-0), a theoretical model of structure is developed which consists of optimized layers of diferent materials and then mathematical modeling is done. Section [3](#page-5-0) discusses about the results obtained and at last conclusion is made in Sect. [4](#page-9-0). Necessary references are included at the end of the article.

## <span id="page-2-0"></span>**2 Theoretical modeling of sensor**

Schematic layout of all the three proposed device confgurations is shown in Fig. [1](#page-2-1)a–c. Confguration-I comprises of three media which are "Prism–Copper–Sensing medium". Confguration-II incorporates a germanium layer in between the copper and sensing medium. Further, graphene is included in the confguration-III. The material specifcations (RI and thickness)



<span id="page-2-1"></span>**Fig. 1** SPR sensor device confgurations **a** confguration-I **b** confguration-II, and **c** confguration-III

are given as follows: prism (SF11) has RI of 1.7786 (Maurya et al. [2015](#page-10-17)). Copper has RI ( $n_{\text{Cu}}$ ) of 0.01838+j2.223 [\(Mishra et al. 2016](#page-10-18)) and thickness  $d_{Cu} = 50$  nm which has been optimized in the paper. Third is germanium layer, having RI of 5.31 (Li [1980\)](#page-10-5) and optimized thickness  $(d_{Ge})$  of 6 nm. Next is graphene layer having a RI  $(n_G)$  of 3+j1.1487 and thickness  $(d_G)$  of  $N \times 0.34$  nm (Verma et al. [2011\)](#page-11-9) where N is the number of layers. At last, fifth layer is sensing medium whose refractive index is considered as 1.33 before the adsorption of molecules. Operating wavelength of light is taken to be 633 nm, which lies in the NIR region.

#### **2.1 Operating principle**

The working of SPR sensor can be explained by the angular interrogation method (Ronald [2013](#page-11-2)). Either monochromatic optical system or sensor which is kept on base is rotated slowly while keeping other one fxed. The intensity of refected light is monitored continuously. When a particular angle called as resonance angle  $(\theta_{SPR})$  is reached, the intensity of reflected light decreases sharply to almost zero. This resonance angle depends on the materials used in the structure, wavelength of light and optical properties of sensing medium. The sudden decrease in intensity of refected light is due to the formation of Surface Plasmon Waves (SPW) which absorbs the energy from light to propagate. This resonance angle is extremely sensitive to the changes in the concentration of bio-molecules in sensing medium. The change in resonance angle provides very important information to detect DNA hybridization of the sample.

#### **2.2 Mathematical modeling of sensor**

Calculation of the refection intensity has been carried out using N-Layer matrix method (Bao et al. [2011](#page-10-19)) implemented on the MATLAB platform. According to it the tangential feld components of EM wave at frst and last boundary are related by Eq. [\(1\)](#page-3-0) below.

<span id="page-3-0"></span>
$$
\begin{bmatrix} U_1 \\ V_1 \end{bmatrix} = M \begin{bmatrix} U_{n-1} \\ V_{n-1} \end{bmatrix}
$$
 (1)

 $U_1$  and  $V_1$  represents the field at the first boundary, whereas  $U_{n-1}$  and  $V_{n-1}$  represents the feld at the last boundary. The characteristic matrix M of the sensor structure is defned as

$$
M_{ij} = \left(\prod_{k=2}^{n-1} M_k\right)_{ij} = \left[\begin{array}{cc} M_{11} & M_{12} \\ M_{21} & M_{22} \end{array}\right] \tag{2}
$$

$$
M_k = \begin{bmatrix} \cos \beta_k & (-i \sin \beta_k) / q_k \\ -i q_k \sin \beta_k & \cos \beta_k \end{bmatrix}
$$
 (3)

Where

$$
q_k = \left(\frac{\mu_k}{\epsilon_k}\right)^{1/2} \cos \theta_k = \frac{\left(\epsilon_k - n_1^2 \sin^2 \theta_1\right)^{1/2}}{\epsilon_k} \tag{4}
$$

$$
\beta_k = \frac{2\pi}{\lambda} n_k \cos \theta_k (z_k - z_{k-1}) = \frac{2\pi d_k}{\lambda} \left( \varepsilon_k - n_1^2 \sin^2 \theta_1 \right)^{1/2} \tag{5}
$$

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In the above two equations,  $d_k$  denotes the thickness of kth layer, RI and dielectric constant of the kth layer are designated as  $n_k$  and  $\varepsilon_k$ . The incident angle of light at first layer is given by  $θ_1$  and wavelength of the light is given by  $λ$ . The reflection coefficient of the p-polarized can be written as:

$$
r_p = \frac{(M_{11} + M_{12}q_N)q_1 - (M_{21} + M_{22}q_N)}{(M_{11} + M_{12}q_N)q_1 + (M_{21} + M_{22}q_N)}
$$
(6)

The refectivity of the device can be expressed as:

$$
R_p = \left| r_p \right|^2 \tag{7}
$$

#### **2.3 Performance evaluation of the sensor**

The performance of the SPR sensor has been judged upon sensitivity (S), minimum refection intensity  $(R_{min})$ , detection accuracy (DA), quality factor (Q), and full width at half maximum (FWHM). All of these terms are quantifed as follows:

$$
S = \Delta \theta_{res} / \Delta n_s \tag{8}
$$

$$
DA = \frac{\Delta \theta_{SPR}}{FWHM} \tag{9}
$$

$$
Q.F = \frac{S}{FWHM(RIU^{-1})}
$$
(10)

FWHM is the width of the refectance curve in degrees at the point on the refectance curve where refection intensity is half of its maximum value.

#### **2.4 Refractive index and chemical potential of graphene**

RI of graphene is highly dependent upon the chemical potential of the graphene. This dependency is expressed by the Kubo formula and the Drude model (Sharma and Dominic [2018\)](#page-11-10), it considers both inter-band and intra-band efect as given below.

$$
\sigma_{\text{intra}}(\omega) = \frac{je^2\mu}{\pi h^2(\omega + j\tau^{-1})}
$$
\n(11)

$$
\sigma_{\text{intra}}(\omega) = \frac{je^2}{4\pi h} \ln \left( \frac{2|\mu| - (\omega + j\tau^{-1})h}{2|\mu| + (\omega + j\tau^{-1})h} \right) \tag{12}
$$

In the above two equations, e is the electronic charge,  $\omega$  is the angular frequency of the light wave, h is the reduced Planck's constant and  $\tau$  is the electron relaxation time. RI of gra-phene is derived from its conductivity by (Bao et al. [2011\)](#page-10-19).

$$
\varepsilon_{xx} = \varepsilon_{yy} = \frac{1 + i\sigma(\omega)}{\omega \varepsilon_0 dG_r} \tag{13}
$$

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where  $dG_r$  is the thickness of graphene layer,  $\varepsilon_0$  is the free space permittivity,  $\sigma$  is the conductivity of graphene, n is the complex RI and ε is the dielectric constant.

#### <span id="page-5-0"></span>**3 Results and discussions**

The basic principle behind the optical wave absorption is the generation of the surface plasmon wave (SPW), which is highly sensitive to the dielectric constant of the material (Homola et al. [1999\)](#page-10-1). It has been observed that the generation of SPW maximizes, when the surface formed by two diferent kinds of materials have real and complex dielectric constants (DC), respectively (Homola et al. [1999\)](#page-10-1). This phenomenon has been kept in consideration, while designing the SPR-sensor. Moreover, an ideal SPR sensor should have high sensitivity with minimum refection intensity. It has been observed that the minimum refection intensity increases with the sensitivity and there is a trade-of between sensitivity and refection intensity. Hence, the maximum adaptable value (MAV) of refection intensity has been fxed as 0.1 and maximum sensitivity has been observed in the range of 0.0–0.1 of refection intensity only.

First, a simple structure (configuration-I), as shown in Fig. [1](#page-2-1)a, has been considered. The confguration comprises of a prism with real DC, and a thin copper layer (in order of nm) with complex DC, which has two surfaces to produce SPW wave. Figure [2a](#page-5-1)–c depicts the performance of the proposed confguration. Figure [2](#page-5-1)a shows the



<span id="page-5-1"></span>**Fig. 2** Performance of confguration-I: **a** refection intensity v/s incident angle **b** variation in minimum refection intensity v/s copper layer thickness (**b**) variation in sensitivity v/s copper layer thickness

variation of reflection intensity with angle of incidence for two RI values (i.e.,  $n=1.33$ ) and  $n = 1.40$ ), where Fig. [2b](#page-5-1), c presents the variation of reflection intensity and sensitivity over the thickness of the copper layer  $(t_{cu})$ , respectively. It can be observed that the sensitivity has zig-zag variation between two values (62.57 and 62.72 approx) with the increment of  $t_{cu}$ . While the reflection intensity first decreases and becomes zero at  $t_{cg}$ =53 nm and then increases with a further increment of  $t_{cg}$ . After considering a trade-off between the reflection intensity and sensitivity and applying the design rule, a sensitivity of 62.71 deg/RIU has been achieved with a minimum refection intensity of 0.0865. Quite good results have been achieved, but it cannot fulfl the requirements and still there is a possibility to enhance the performance of the device. Hence, in this way, a dielectric layer has been introduced, and the sensitivity and refection intensity of the device have been analyzed by varying its DC value in the range of 1-6 (i.e., RI from 1 to 6) as depicted in Fig. [3](#page-6-0)a, b, respectively. The sensitivity increases up to  $RI = 5.6$ and then decreases while the refection intensity remains below the MAV for the entire range of RI. It can be noticed that the maximum absorption has been achieved at a RI value of 5.6, which is close to the RI of germanium, hence it has been considered as a newly inserted dielectric layer. Figure [4](#page-7-0)a fgures the incidence angle dependent refection intensity of the device (confguration-II). The sensitivity, and refection intensity spectra's of the configuration-II over the newly inserted germanium layer thickness  $(t_{Ge})$ are shown in Fig. [4](#page-7-0) b, c, respectively. It is found that the sensitivity increases with an increment of  $t_{Ge}$ , but after 6 nm the reflection intensity exceeds the MAV. Hence,  $t_{Ge}$  is restricted to 6 nm, which results 132.00 deg/RIU of sensitivity with minimum refection intensity of 0.0925 after optimizing all the design parameters.

Since, the DC criteria of the SPW generation have not fulflled at all the surfaces, there is a chance to further enhance the performance of the device. Hence, a graphene layer (having complex DC value) has been incorporated just after the germanium layer. Graphene is a carbonic material which is bio-friendly and hence, it can be used directly in contact of SM (Sensing Medium). As graphene has a complex DC value, it can fulfl the DC-criteria of the SPW generation. Now, the confguration (confguration-III) has four SPW generating surfaces, which are able to dramatically enhance the device performance. These surfaces are: prism-copper surface, copper-germanium surface, germanium-graphene surface, and graphene-SM surface, as fgured in Fig. [1c](#page-2-1). An excellent performance has been achieved with this confguration. After optimizing all design parameters, a sensitivity of 160.71 deg./RIU has been achieved with the minimum



<span id="page-6-0"></span>**Fig. 3** Efect of refractive index of dielectric layer on **a** sensitivity and **b** refection intensity of sensor



<span id="page-7-0"></span>**Fig. 4** Performance of confguration II **a** refection intensity versus incident angle, **b** refection intensity versus Ge layer thickness, and **c** sensitivity versus Ge layer thickness

refection intensity of 0.0615. The results are well presented in Fig. [5](#page-7-1). Table [1](#page-8-0) provides a better comparison of all the confgurations carried out in the research work.

Graphene has some unique electrical and optical properties like other carbon-based structures (Knapek et al. [2017\)](#page-10-20), which varies with its layer thickness and  $\mu_c$  (Mishra et al. [2018;](#page-10-10) Mishra et al. [2019](#page-10-11)). Hence, a critical analysis of these parameters has been carried out to analyze the behavior of the graphene layer. Figure  $6$  a, b depicts the variation of sensitivity, and refection intensity with an increase in the number of graphene layers, respectively. It can be observed that both sensitivity and refection intensity increases linearly

<span id="page-7-1"></span>**Fig. 5** Performance of confguration III: refection intensity versus incident angle



<span id="page-8-0"></span>

with an increment of graphene-layer (from 1 to 3). After two graphene layers, the refection intensity exceeds MAV, which is not desirable. Hence, the corresponding optimal number of layers can be concluded as 2. Further, the effect of  $\mu_c$  on the performance of SPR sensor has been explored.

Figure [7](#page-8-2) depicts the variation of refractive index of the graphene layer with its chemical potential. It can be observed that real part of refractive index increases from 3 to 4.5, when  $\mu_c$  varies from 0.2 to 0.4, and then sharply tends to zero at 0.5 eV and then stays almost constant on a further increase in  $\mu_c$ , whereas the imaginary part follows an opposite trend. It decreases from 2.8 to nearly about 0.1 with increase of  $\mu_c$  from 0.1 to 0.42 eV and then increases rapidly to 4.5 at 1 eV. Further, the effect of chemical potential on the sensitivity of the sensor and refection intensity has been studied by drawing a curve between them as shown in Fig. [8a](#page-9-1), b, respectively.



<span id="page-8-1"></span>**Fig. 6** Plots of sensitivity versus number of graphene layer and minimum refection intensity versus number of graphene layer

<span id="page-8-2"></span>





<span id="page-9-1"></span>**Fig. 8** Effect of graphene chemical potential: **a** sensitivity (deg/RIU) versus chemical potential ' $\mu$ ,' (eV), **b** Minimum reflectance versus chemical potential ' $\mu_c$ ' (eV)

It is observed that sensitivity frst increases, then remains constant for a small period and then rapidly decreases with peak sensitivity of 149.57 at 0.4 eV, while the value of minimum refectance follows decreasing staircase type of trend and is greater than 0.1 for a chemical potential of less than 0.5 eV. It is because of the decrease in imaginary RI value of graphene, which can be observed in Fig. [7](#page-8-2), and when RI of the graphene becomes pure imaginary, the refection intensity saturates at 0.08, but the sensitivity goes down simultaneously. Thus, from both the above successive fgures, it can be concluded that the optimum result is obtained for  $\mu_c$  at 0.5 eV. All optimized design variables are well presented in Table [2.](#page-9-2)

### <span id="page-9-0"></span>**4 Conclusions**

In the progressive designing and analysis presented, a highly sensitive and accurate SPR sensor using germanium and copper layer has been developed with minimum possible thickness. An increase in the detection accuracy, sensitivity, and quality factor has been obtained as 100.48%, 165.94% and 166.02% more than conventional sensor, respectively. Further, it has been found that the chemical potential of graphene has signifcant impact on the sensitivity of the sensor. SPR sensor proposed here can be used for DNA hybridization with better sensitivity and accuracy.



<span id="page-9-2"></span>**Table 2** Optimal design parameters of each confi **Funding** Dr. Ravi Panwar would like to acknowledge the Faculty Initiation Grant (FIG) provided by the Indian Institute of Information Technology, Design and Manufacturing to support this work.

#### **References**

- <span id="page-10-19"></span>Bao, Q., et al.: Broadband graphene polarizer. Nat. Photonics **5**(7), 411–415 (2011). [https://doi.org/10.1038/](https://doi.org/10.1038/NPHOTON.2011.102) [NPHOTON.2011.102](https://doi.org/10.1038/NPHOTON.2011.102)
- <span id="page-10-3"></span>Biednov, M., Lebyedyeva, T., Shpylovyy, P.: Gold and aluminum based surface plasmon resonance biosensors: sensitivity enhancement. Optical Sens. **9506**, 95061P (2015).<https://doi.org/10.1117/12.2177992>
- <span id="page-10-13"></span>Bludov, Y.V., Vasilevskiy, M.I., Peres, N.M.R.: Mechanisum for graphene-based optoelectronic switches by tuning surface plasmon polaritons in monolayer graphene. EPL Europhys. Lett. **92**(6), 161–166 (2010). <https://doi.org/10.1209/0295-5075/92/68001>
- <span id="page-10-8"></span>Bonnacorso, F., Sun, Z., Hasan, T., Ferrari, A.C.: Graphene photonics and optoelectronics. Nat. Photonics **4**(9), 611–622 (2010).<https://doi.org/10.1038/nphoton.2010.186>
- <span id="page-10-16"></span>Chu, H.S., Gan, C.H.: Active plasmonmic switching at mid-infrared wavelengths with graphene ribbon arrays. Appl. Phys. Lett. **102**(23), 231107 (2013). <https://doi.org/10.1063/1.4810003>
- <span id="page-10-15"></span>Falkovsky, L.A.: Optical properties of graphene. J. Phys: Conf. Ser. **120**(1), 012004 (2008). [https://doi.](https://doi.org/10.1063/1.3525940) [org/10.1063/1.3525940](https://doi.org/10.1063/1.3525940)
- <span id="page-10-4"></span>Fu, H., Zhang, S., Chen, H., Weng, J.: Graphene enhances the sensitivity of fber optic surface plasmon resonance biosensor. IEEE Sens. J. **15**(10), 5478–5482 (2015). [https://doi.org/10.1109/](https://doi.org/10.1109/JSEN.2015.2442276) [JSEN.2015.2442276](https://doi.org/10.1109/JSEN.2015.2442276)
- <span id="page-10-7"></span>Geim, A.K., Konstantin, S.N.: The rise of graphene. In: Rodgers, P. (ed.) Nanoscience and Technology: A Collection of Reviews from Nature Journals, pp. 11–19. World Scientifc, Singapore (2010). [https://doi.org/10.1142/9789814287005\\_0002](https://doi.org/10.1142/9789814287005_0002)
- <span id="page-10-1"></span>Homola, J., Yee, S.S., Gauglitz, G.: Surface plasmon resonance sensors. Sens. Actuators B Chem. **54**, 3–15 (1999). [https://doi.org/10.1016/s0925-4005\(98\)00321-9](https://doi.org/10.1016/s0925-4005(98)00321-9)
- <span id="page-10-14"></span>Kim, S.J., et al.: Charachterization of chemical doping of graphene by in situ Raman spectroscopy. Appl. Phys. Lett. **108**(20), 203111 (2016). <https://doi.org/10.1063/1.4950969>
- <span id="page-10-20"></span>Knapek, A., Sobola, D., Tománek, P., Pokorna, Z., Urbanek, M.: Field emission from the surface of highly ordered pyrolytic graphite. Appl. Surf. Sci. **395**, 157–161 (2017). [https://doi.org/10.1016/j.](https://doi.org/10.1016/j.apsusc.2016) [apsusc.2016](https://doi.org/10.1016/j.apsusc.2016)
- <span id="page-10-0"></span>Kretschmann, E., Raether, H.: Radiative decay of non radiative surface plasmons excited by light. Zeitschrift für Naturforschung A **23**(12), 2135–2136 (1968). <https://doi.org/10.1515/zna-1968-1247>
- <span id="page-10-5"></span>Li, H.H.: Refractive index of silicon and germanium and its wavelength and temperature derivatives. J. Phys. Chem. Ref. Data **9**(3), 561–658 (1980).<https://doi.org/10.1063/1.555624>
- <span id="page-10-12"></span>Maharana, P.K., Jha, R.: Chalcogenide prism and graphene multilayer based surface plasmon resonance afnity biosensor for high performance. Sens. Actuators, B **169**, 161–166 (2012). [https://doi.](https://doi.org/10.1016/j.snb.2012.04.051) [org/10.1016/j.snb.2012.04.051](https://doi.org/10.1016/j.snb.2012.04.051)
- <span id="page-10-17"></span>Maurya, J.B., Prajapati, Y.K., Singh, V., Saini, S.P.: Sensitivity enhancement of surface plasmon resonance sensor based on graphene—MoS2 hybrid structure with TiO2-SiO2 composite layer. Appl. Phys. (2015). <https://doi.org/10.1007/s00339-015-9442-3>
- <span id="page-10-6"></span>Mishra, A.K., Mishra, S.K., Verma, R.K.: Graphene and beyond graphene MoS2: a new window in surface-plasmon-resonance-based fber optic sensing. J. Phys. Chem. C **120**(5), 2893–2900 (2016a). <https://doi.org/10.1021/acs.jpcc.5b08955>
- <span id="page-10-18"></span>Mishra, A.K., Mishra, S.K., Verma, R.K.: Graphene and Beyond graphene MoS2: a ewindow in surface-plasmon-resonance- based fber optic sensing. The Journal of Physical Chemistry. **120**(5), 12 (2016b).<https://doi.org/10.1021/acs.jpcc.5b08955>
- <span id="page-10-10"></span>Mishra, R., Panwar, R., Singh, D.: Equivalent circuit model for the design of frequency-selective, terahertz-band, graphene-based metamaterial absorbers. IEEE Magn. Lett. **9**, 1–5 (2018). [https://doi.](https://doi.org/10.1109/LMAG.2018.2878946) [org/10.1109/LMAG.2018.2878946](https://doi.org/10.1109/LMAG.2018.2878946)
- <span id="page-10-11"></span>Mishra, R., Sahu, A., Panwar, R.: Cascaded graphene frequency selective surface integrated tunable broadband terahert metamaterial absorber. IEEE Photonics J. **11**(2), 1–10 (2019).. [https://doi.](https://doi.org/10.1109/jphot.2019.2900402) [org/10.1109/jphot.2019.2900402](https://doi.org/10.1109/jphot.2019.2900402)
- <span id="page-10-9"></span>Muller, T., Xia, F., Avouris, P.: Graphene photodetectors for high speed optical communications. Nat. Photonics **4**(5), 297–301 (2010). <https://doi.org/10.1109/JPROC.2013.2250892>
- <span id="page-10-2"></span>Pandey, A.K., Sharma, A.K.: Simulation and analysis of plasmonic sensor in NIR with fuoride glass and graphene layer. Photonics Nanostructures Fundam. Appl. **28**, 94–99 (2018). [https://doi.](https://doi.org/10.1016/j.photonics.2017.12.003) [org/10.1016/j.photonics.2017.12.003](https://doi.org/10.1016/j.photonics.2017.12.003)
- <span id="page-11-6"></span>Pumera, M.: Graphene in biosensing. Mater. Today **14**(7–8), 308–315 (2011). [https://doi.org/10.1016/](https://doi.org/10.1016/S1369-7021(11)70160-2) [S1369-7021\(11\)70160-2](https://doi.org/10.1016/S1369-7021(11)70160-2)
- <span id="page-11-3"></span>Rahman, M.S., Hasan, M.R., Rikta, K.A., Anower, M.S.: A novel graphene coated surface plasmon resonance biosensor with tungsten disulfde (WS2) for sensing DNA hybridization. Optical Mater. **75**, 567–573 (2018). <https://doi.org/10.1016/j.optmat.2017.11.013>
- <span id="page-11-2"></span>Ronald Jr., L.E: Multiwavelength Surface Plasmon Resonance Sensor Designs for Chemical and Biochemical Detection. Ph. D thesis, Dept. of Chemistry, Virginia Polytechnic Institute and State University, Ontario, Canada, (2013)
- <span id="page-11-10"></span>Sharma, A.K., Dominic, A.: Infuence of chemical potential on graphene-based SPR sensor's performance. IEEE Photonics Technol. Lett. (2018).<https://doi.org/10.1109/LPT.2017.2776945>
- <span id="page-11-0"></span>Tamersit, K., Djefal, F.: Double-gate graphene nanoribbon feld efect transistor for DNA and gas sensing applications: simulation study and sensitivity analysis. IEEE Sens. J. **16**(11), 4180–4191 (2016). [https](https://doi.org/10.1109/JSEN.2016.2550492) [://doi.org/10.1109/JSEN.2016.2550492](https://doi.org/10.1109/JSEN.2016.2550492)
- <span id="page-11-9"></span>Verma, R., Gupta, B.D., Jha, R.: Sensitivity enhancement of a surface plasmon resonance based biomolecules sensor using graphene and silicon layers. Sens. Actuators, B **160**(1), 623–631 (2011). [https://](https://doi.org/10.1016/j.snb.2011.08.039) [doi.org/10.1016/j.snb.2011.08.039](https://doi.org/10.1016/j.snb.2011.08.039)
- <span id="page-11-4"></span>Verma, A., Prakash, A., Tripathi, R.: Sensitivity enhancement of surface plasmon resonance biosensor using graphene and air gap. Optics Commun. **357**, 106–112 (2015). [https://doi.org/10.1016/j.optco](https://doi.org/10.1016/j.optcom.2015.08.076) [m.2015.08.076](https://doi.org/10.1016/j.optcom.2015.08.076)
- <span id="page-11-7"></span>Xia, F., Muller, T., Lin, Y.M., Sun, F.B.Z., Hasan, T., Ferrari, A.C.: Ultra fast graphene photodetector. Nat. Nanotechnol. **4**(12), 839–843 (2009). <https://doi.org/10.1038/nnano.2009.292>
- <span id="page-11-5"></span>Xu, J., Xiao, X., Stepanov, A.L., Ren, F., Wu, W., Cai, G., Zhang, S., Dai, Z., Jiang, C.: Efciency enhancements in Ag nanoparticles-SiO2–TiO2 sandwiched structure via plasmonic efect enhanced light capturing. Nanoscale Res Lett. 8 **73**(1), 73 (2013). <https://doi.org/10.1186/1556-276X-8-73>
- <span id="page-11-1"></span>Zeng, S., Baillargeat, D., Ho, H.P., Yong, K.T.: Nanomaterials enhanced surface plasmon resonance for biological and chemical sensing applications. Chem. Soc. Rev. **43**(10), 3426–3452 (2014). [https://doi.](https://doi.org/10.1039/c3cs60479a) [org/10.1039/c3cs60479a](https://doi.org/10.1039/c3cs60479a)
- <span id="page-11-8"></span>Zheng, J.P., Jiao, K.L., Shen, W.P., Anderson, W.A., Kwok, Sing, H.: Highly sensitive photodetector using porous silicon. Appl. Phys. Lett. **61**(4), 459–461 (1992). <https://doi.org/10.1063/1.107884>

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