

Temperature efect on the performance of a 1D grating‑based surface‑plasmon resonance sensors

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Abstract

We have theoretically studied the infuence of temperature on the performance of a 1D grating sensor based on surface plasmon resonance. Rigorous coupled wave analysis method has been utilized to study the effect of the temperature on the sensing performance. The performance of the sensor has been evaluated on the basis of detection accuracy (DA), the sensitivity (S) and the quality parameter (χ). The effect of temperature on the DA, χ and S of the sensor with two diferent metals (gold and silver) has been compared. Our analysis exhibits that increasing of temperature may lead to poor detection accuracy and quality of the sensor, but the sensitivity is very stable with the change of temperature. Further, the results confirm that the room temperature $T=300$ K provides a high DA and a high S, and a good quality.

Keywords Surface plasmon resonance (SPR) · Sensor performance · 1D grating · Temperature · RCWA

1 Introduction

Surface plasmons (SPs) are the collective oscillation of free electrons at the metal–dielectric interface and evanescently confned in the perpendicular direction (Ritchie [1957;](#page-14-0) Raether [1988;](#page-14-1) Maier [2007](#page-14-2)). The coupling of electromagnetic feld and propagation of coherent charge density oscillations along the boundary between metal and dielectric is a well-known physical efect, denoted as the surface plasmon resonance (SPR) (Homola [2006;](#page-13-0) Liedberg et al. [1983\)](#page-14-3). Due to this reason, various techniques of coupling are always the interest of researchers. The commonly used coupling techniques are prism coupling (Kretschmann and Raether [1968;](#page-13-1) Chen and Chen [1981](#page-13-2); Jha and Sharma [2009](#page-13-3)), grating coupling (Cai et al. [2008](#page-13-4); Dhibi et al. [2015,](#page-13-5) [2016a,](#page-13-6) [b\)](#page-13-7), tapered flm coupling (Tien and Martin [1971\)](#page-14-4) and fiber-optic coupling (Sharma and Gupta [2007](#page-14-5); Perrotton et al. [2011;](#page-14-6) Gentleman and Booksh [2006](#page-13-8); Kort and Bernhard [2015](#page-13-9)).

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The SPR phenomenon has many applications such as the sensors (Homola [2006;](#page-13-0) Liedberg et al. [1983](#page-14-3); Jha and Sharma [2009;](#page-13-3) Cai et al. [2008](#page-13-4); Dhibi et al. [2015](#page-13-5), [2016a;](#page-13-6) Sharma and Gupta [2007](#page-14-5); Perrotton et al. [2011;](#page-14-6) Gentleman and Booksh [2006;](#page-13-8) Kort and Bernhard [2015\)](#page-13-9). Since the frst application of SPR in gas sensing (Liedberg et al. [1983\)](#page-14-3), many research articles have been reported, for example, on chemical, biochemical and organic sensing, real-time detection of the concentration and variety of biological molecules, biomedicine and accurate and precise detection of other biomedical agents (Homola [1997;](#page-13-10) Salamon et al. [1997](#page-14-7); Jung et al. [1998;](#page-13-11) Homola et al. [1999](#page-13-12); Peng et al. [2013](#page-14-8); Hasan et al. [2018;](#page-13-13) Zhou et al. [2018;](#page-14-9) Islam et al. [2018](#page-13-14); Bijalwan and Rastogi [2018](#page-13-15)). Peng et al. proposed an SPR sensor consists of metallic nanowire grating deposited on a substrate positioned upside down above a conventional Kretschmann confguration at a certain distance. The proposed design found for chemical gas detection (Peng et al. [2013\)](#page-14-8). Recently, Hasan et al. ([2018\)](#page-13-13) employed a novel niobium nanoflm sensor. The proposed niobium nanoflm based sensor can be potentially implemented in biochemical and organic chemical sensing. Zhou et al. ([2018\)](#page-14-9) developed a photonic crystal fber (PCF) sensor based on SPR. This sensor can be used for real-time detection of the concentration and variety of biological molecules. Bijalwan and Rastogi ([2018\)](#page-13-15) proposed an SPR sensor based on a bimetallic diffraction grating for the detection of hemoglobin concentration in human blood. Moreover, it has been known from a large number of publications that many physical and chemical factors afect the SPR phenomenon. One signifcant factor is the temperature of the sensing environment. Hence, the efects from temperature variation may afect the performance of SPR sensor. However, Chiang et al. ([2001\)](#page-13-16) presented a self-contained model of the efect of temperature on the sensitivity of a prism-based SPR sensor. Hence, he used Drude model for making the modeling feasible on a purely theoretical basis. Here, only the temperature dependence of the metal properties was considered. Sharma and Gupta ([2006\)](#page-14-10) studied theoretically the efect of temperature on the sensitivity and signal-to-noise ratio (SNR) of a fber-optic-based SPR sensor. They used gold and silver fber-optic sensors. Thus, both the temperature dependences of the dielectric and metal properties were considered. These sensors show almost the same variation in SNR and sensitivity with temperature.

In this work, we have theoretically studied the effect of temperature on the performance of an SPR sensor. We used gold and silver grating sensors based on SPR. We have analyzed the efect of temperature on the sensitivity, the detection accuracy (DA) and quality parameter (χ) using numerical simulations based on rigorous coupled wave analysis (RCWA) (Moharam et al. [1995](#page-14-11)). Further, the sensitivity, DA and χ are compared is carried out for the two most commonly used metals (silver and gold).

2 Rigorous coupled‑wave analysis for one‑dimensional grating

Figure [1](#page-2-0) shows the schematic of grating-coupled surface plasmon resonance (GCSPR) sensors. The sensors consist of metal (gold or silver) grating of period d, depth h, width of the metal strip Λ and filling ratio $f = \frac{\Lambda}{d}$ deposited on metal film (gold or silver) and a analyte of refractive index n_a placed on the top of the grating. Grating parameters chosen for numerical simulations are grating period $d=0.5 \mu m$, grating depth h=0.03 μ m and filling ratio $f=0.5$. As is well known, the most effective way to model the reflectivity (R) of the GCSPR is to use the RCWA method. In this approach, we start by analyze the magnetic wave propagation in the first region for p polarization. So, the normalized incident magnetic feld in region I can be expressed as

Fig. 1 Illustration of SPR sensors based on metallic difraction grating

$$
H_{inc,y} = \exp(-jk_0 n_a (\sin(\theta)x + \cos(\theta)z), \tag{1}
$$

where $k_0 = \frac{2\pi}{\lambda_0}$ with λ_0 is the free-space wavelength, n_a is the refractive index of region I, θ is the incidence angle and $j = \sqrt{-1}$.

In both homogeneous regions I (z <0) and II (z >h), the normalized fields may be written as

$$
H_{I,y} = H_{inc,y} + \sum_{i} R_i \exp(-j(k_i^x x - k_i^{Iz} z)),
$$
 (2)

$$
H_{II,y} = \sum_{i} T_i \exp(-j(k_i^x x - k_i^{IIz}(z - h))), \tag{3}
$$

where the quantity k_i^x is the x component of the wave vectors. It is determined from the vector Floquet condition and is given by

$$
k_i^x = k_0 \left(n_a \sin(\theta) + i \left(\frac{\lambda_0}{d} \right) \right), \tag{4}
$$

and where the z components can be expressed as

$$
k_i^{Lz} = \sqrt{((k_0 n_L)^2 - (k_i^x)^2)}, \text{ with } L = I, II,
$$
 (5)

 (R_i) is the magnetic-field amplitude of the ith reflected (backward-diffracted) wave in region I, and (T_i) is the magnetic-field amplitude of the ith transmitted (forward-diffracted) wave in region II.

In the grating region $(0 < z < h)$ the periodic permittivity is represented in a Fourier series of the form

$$
\varepsilon(x) = \varepsilon(x + d) = \sum_{p} \varepsilon_{p} \exp\left(j\frac{2\pi px}{d}\right),\tag{6}
$$

where ε_p is the pth Fourier component of the relative permittivity in the grating region.

In the modulated region ($0 < z < h$) the tangential magnetic (H_y) and electric (E_x) fields may be written as

$$
H_{y} = \sum_{i} \Omega_{i}^{y}(z) \exp\left(-jk_{i}^{x}x\right),\tag{7}
$$

$$
E_x = j \left(\frac{\mu_0}{\varepsilon_0}\right)^{1/2} \sum_i \Psi_i^x(z) \exp\left(-jk_i^x x\right),\tag{8}
$$

where ϵ_0 and μ_0 are the permittivity and the permeability of free space. $\Omega_i^y(z)$ and $\Psi_i^y(z)$ are the normalized amplitudes of the ith space-harmonic felds.

Using Maxwell's equations, we fnd that the set of coupled wave equations for the electromagnetic felds, in matrix form, is

$$
\begin{bmatrix} \frac{\partial \Omega^{\mathcal{Y}}}{\partial \Psi^{\mathcal{X}}}_{\mathcal{O}}(\mathcal{Z}^{\prime}) \\ \frac{\partial \Psi^{\mathcal{X}}}{\partial \mathcal{G}}_{\mathcal{O}}(\mathcal{Z}^{\prime}) \end{bmatrix} = \begin{bmatrix} 0 & A \\ B & 0 \end{bmatrix} \begin{bmatrix} \Omega^{\mathcal{Y}} \\ \Psi^{\mathcal{X}} \end{bmatrix},\tag{9}
$$

where $z' = k_0 z$, *A* is the matrix formed by the permittivity harmonic components and *B* is the matrix given by

$$
B = K^x A^{-1} K^x - I,\t\t(10)
$$

where K^x is a diagonal matrix whose elements equal k_i^x/k_0 and *I* is the identity matrix. Noted that B, A, K^x , and I are $(n \times n)$ matrices, where n is the number of harmonics retained in the field expansion. By eliminating ψ^x , Eq. ([9](#page-3-0)) can be reduced to

$$
[\partial \Omega^{\gamma}/\partial (z')] = [AB] [\Omega^{\gamma}], \qquad (11)
$$

By diagonalizing AB, the decomposition of eigenvalues and the eigenvectors is able to be carried out more efficiently. Then the solution can be written as follows

$$
\Omega_i^y(z) = \sum_{m=1}^n w_{i,m} \{ C_m^+ \exp(-k_0 q_m z) + C_m^- \exp [k_0 q_m (z - h)] \},
$$
\n(12)

$$
\Psi_i^x(z) = \sum_{m=1}^n \nu_{i,m} \left\{ -C_m^+ \exp(-k_0 q_m z) + C_m^- \exp\left[k_0 q_m (z - h)\right] \right\}.
$$
 (13)

where $w_{i,m}$ is the (i, m)'th element of the eigenvector matrix W and q_m is the positive square root of the eigenvalues of the matrix AB. The quantities $v_{i,m}$ are the (i, m) 'th elements of the product matrix $V = A^{-1} W Q$, with Q being a diagonal matrix with the diagonal elements *q_m*. The quantities C_m^+ and C_m^- are unknown constants to be determined from the boundary conditions

The coupled-wave equations can be solved by setting up boundary value conditions of the tangential electric and magnetic feld components. With the normalized magnetic feld amplitudes of the refected wave, refectivity in each difraction order can be calculated.

3 Coupling of the incident feld and the SP

When the grating is illuminated by a p-polarized plane wave of a wavelength λ =632.8 nm, at some particular incident angle, the SP starts propagating at the metal–dielectric interface. It is due to the coupling of the incident feld and the coherent charge density oscillations at the interface. When, the wave vector of the SP is coincident with the wave vector of the incident electromagnetic radiation, a sharp dip in the refectance spectrum is shown Fig. [2](#page-4-0)a. This is an SPR condition. Therefore, the coupling condition is given by

$$
k_i^x = k_0 \left(n_a \sin \left(\theta_{res} \right) + i \left(\frac{\lambda_0}{d} \right) \right) = \pm \text{Re} \left(\sqrt{\frac{n_i^2 \epsilon_m}{n_i^2 + \epsilon_m}} \right),\tag{14}
$$

where ε_m is the metal permittivity, θ_{res} is the resonance angle at which coupling occurs and " $i = 0, \pm 1, \ldots$ " is the diffraction order."

From Eq. (14) (14) , the resonance angle is defined as

$$
\theta_{res} = \arcsin\left(\frac{\pm \text{Re}\left(\sqrt{\frac{n_a^2 \epsilon_m}{n_a^2 + \epsilon_m}}\right) - ik_0\left(\frac{\lambda_0}{d}\right)}{n_a k_0}\right).
$$
(15)

It is clear that θ_{res} changes with refractive index n_a , as shown in Fig. [2](#page-4-0)b.

4 Performance of grating‑based SPR sensors

The SPR sensor's performance is described by two very important features such as the sensitivity (S) and the detection accuracy (DA). Thus, if the resonance incidence angle is shifted by $\Delta\theta_{res}$ due to increase in refractive index by Δn_a (Temperature by ΔT), then the sensitivity is defned as (Roh et al. [2011\)](#page-14-12)

Fig. 2 a Illustration of the angular SPR response of the sensor for n_{a1} **b** for different analytes of refractive indices n_{a1} and n_{a2}

On the other hand, the detection accuracy (DA) as given by Brahmachari and Ray ([2014\)](#page-13-17) is

$$
DA = \frac{1}{FWHM},\tag{17}
$$

Besides the sensitivity and the detection-accuracy, the sensor performance is quantifed in other term such as the quality (χ) . It is defined as (Homola et al. [1999\)](#page-13-12)

$$
\chi = \frac{S_{\theta}}{FWHM}.\tag{18}
$$

5 Thermo‑optical metals properties

The frequency-dependent dielectric function of any metal is represented by the Drude formula, i.e.

$$
\varepsilon(\omega) = 1 - \frac{\omega_p^2}{\omega(\omega + i\omega_c)},\tag{19}
$$

where ω ^{*n*} is the plasma frequency given by

$$
\omega_p = \sqrt{\frac{4\pi Ne^2}{m^*}},\tag{20}
$$

with *N* and m^* are the density and effective mass of the electrons, respectively. Here, assuming that the variation of these two parameters with temperature can be neglected. However, the temperature dependence of plasma frequency can be described by (Sharma and Gupta [2006;](#page-14-10) Chiang et al. [1998](#page-13-18), [2000\)](#page-13-19)

$$
\omega_p = \omega_{p0} \left[1 + \gamma_e (T - T_0) \right]^{-1/2},\tag{21}
$$

where γ_e is the thermal linear expansion coefficient of the metal, T_0 is the room temperature acting as the reference temperature and ω_{p0} is the plasma frequency at T_0 .

On the other hand, ω_c is collision frequency that comes from two factors: phonon–electron scattering ω_{cp} and electron–electron scattering ω_{ce} . Hence, the combined effect of the two gives

$$
\omega_c = \omega_{cp} + \omega_{ce},\tag{22}
$$

The temperature dependence of phonon-electron scattering is accounted by the following Holstein's model (Chiang et al. [1998](#page-13-18), [2000;](#page-13-19) Holstein [1954](#page-13-20)):

$$
\omega_{cp}(T) = \omega_0 \left[\frac{2}{5} + 4 \left(\frac{T}{T_D} \right)^5 \int_0^{T_D/T} \frac{z^4 dz}{e^z - 1} \right],
$$
\n(23)

where ω_0 is a constant that must be calculated with care and T_D is the Debye temperature.

In addition, the Lawrence's model provides the temperature dependence of electron–electron scattering given by (Lawrence [1976\)](#page-13-21)

	Gold	Silver
Parameters		
Thermal expansion coefficient γ_e	1.42×10^{-5} per K	1.89×10^{-5} per K
Room temperature T_0	300 K	300 K
Plasma frequency at room temperature ω_{n0}	1.3754×10^{16} rad/s	1.3724×10^{16} rad/s
ω_0	2.0477×10^{13} rad/s	2.0347×10^{13} rad/s
Debye temperature T_D	170 K	215 K
Fermi energy E_F	5.53 eV	5.48 eV
Fermi constant h	$4.13566733 \times 10^{-15}$ eV	$4.13566733 \times 10^{-15}$ eV
Г	0.55	0.55
Δ	0.77	0.73
Boltzmann constant k_R	8.617343×10^{-5} eV	8.617343×10^{-5} eV

Table 1 Gold and silver parameters used for the numerical simulation

$$
\omega_{ce}(T) = \frac{1}{6}\pi^4 \frac{\Gamma \Delta}{hE_F} \left[\left(k_B T\right)^2 + \left(\frac{h\omega}{4\pi^2}\right)^2 \right].\tag{24}
$$

where E_F is the Fermi energy, *h* is the Fermi constant, Γ is a constant giving the average over the Fermi surface of the scattering probability, Δ is the fractional scattering and k_B is

Fig. 3 Variation of refectivity with incidence angle at room temperature $T=300$ K. Here, the refractive index of analyte $n_a = 1.35$

Table 2 The real part and the imaginary part of the metal–dielectric function with temperature for gold and silver

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Fig. 4 Efect of temperature on the surface plasmon resonance (SPR) phenomenon: **a** gold and **b** silver

the Boltzmann constant. For gold and silver, the values of these parameters are summarized in Table [1](#page-6-0) (Sharma and Gupta [2006](#page-14-10); Chiang et al. [1998,](#page-13-18) [2000\)](#page-13-19). The values of the real part and the imaginary part of the metal–dielectric function with temperature for gold and silver are given in Table [2](#page-6-1).

6 Results and discussion

Figure [3](#page-6-2) gives the SPR curves of refectivity depending on the incident angle at room temperature $T=300$ K. Two very important key features may be noted from these curves. The resonance angle and the full width at half maximum (FWHM) of the SPR curves. These

Fig. 5 aFWHM and **b** detection accuracy versus diferent temperature of gold and silver

two features are more susceptible to the value of the complex dielectric constant of the metal given by Eq. ([19](#page-5-0)). The real part of the dielectric constant determines the SPR position and the imaginary part determines the bandwidth (Jha and Sharma [2009;](#page-13-3) Su et al. [2012;](#page-14-13) Yuk et al. [2014\)](#page-14-14). We observe refectance dips with close resonance angles. This is due to the similar values of the real part of Au and Ag at the room temperature. In the other hand, an important observation is that there is not much diference between the FWHM of SPR curves corresponding to Au and Ag. This is due to the small diference in the imaginary part of the dielectric constant of pure metals.

Figure [4](#page-7-0)a, b, respectively, show how the SPR curve between refectivity and incident angle varies with temperature. Two main factors may be noted from these curves. First,

Fig. 6 Angular SPR curves of gold with six diferent refractive indices of analyte

Fig. 7 Angular SPR curves of silver with six diferent refractive indices of analyte

with an increase in temperature the resonance angle shifts to the higher side. The results are shown in Table [3](#page-7-1). Second, the SPR curve broadens with the increase in temperature. This can be understood from the increase in plasma frequency and increase in collision frequency in the Drude model as the temperature increases (Sharma and Gupta [2006\)](#page-14-10). The variations of these two parameters cause a variation of the metal–dielectric function with temperature according to Eq. [\(19](#page-5-0)). Hence, the combined efect of the above two factors on the real part and the imaginary part of the metal–dielectric function appears in the shifting of the resonance condition and the broadening of the SPR curve. For a good sensor, this shift should be large and FWHM should be small.

In Fig. [4](#page-7-0), we see that the SPR spectra with bigger temperature have larger FWHM. For discussion, we have plotted the variation of FWHM with temperature for two diferent

metal sensors: silver and gold as shown in Fig. [5a](#page-7-2). We observe that FWHM increases with increasing temperature. This efect of temperature on FWHM can be explained in terms of the permittivity. Indeed, when we vary the temperature, the real part of the permittivity changes. This temperature dependent permittivity is the reason for increasing FWHM.

The broadening of the SPR curve is very important feature within the context of detection accuracy (DA) of the SPR sensor. Figure [5](#page-7-2)b shows the variation of DA with temperature. It is very clear that the silver has a larger DA than gold. Also, the variation in DA with temperature is more evident in silver. As the temperature T varies from 300 to 800 K, DA decreases from 1.169 to 0.710 deg⁻¹ in the case of gold grating-based SPR sensor, whereas for silver grating-based SPR sensor the DA decreases from 1.385 to 0.809 deg⁻¹. This result allows one to understand that the increase of temperature can further deteriorate the detection accuracy of the sensor.

Figures [6](#page-8-0) and [7](#page-9-0) provide the refectance spectra of the gold and silver grating-based SPR sensor for analyte refractive indexes between 1.35 and 1.40 with diferent temperature. The results show that the position of the resonant angle is afected by the varying of analyte RI. The resonance dips shift to the longer angles with the analyte RI increase. But the FWHM is unchanged when varying the analyte RI. Tables [4](#page-10-0) and [5](#page-10-1) describes the changes in the resonance peak positions ($\Delta\theta_{res}$) and variations of the analyte refractive indexes (Δn_a) for diferent temperature. As temperature increases, but the changes in the resonance peak positions does not change. Therefore $\Delta\theta_{res}$ is independent of the temperature. This is due to the well-established fact that ε_{mr} varies relatively insignificantly with T compared to the imaginary part of the dielectric function for metals (Leung et al. [1996](#page-14-15)).

Besides the detection-accuracy (DA), the sensor performance is quantifed in other terms; the sensitivity (S) and the quality (γ) . Mathematically, the sensitivity is calculated by Eq. ([16](#page-4-2)). From Eq. ([16](#page-4-2)), and Figs. [6](#page-8-0) and [7,](#page-9-0) the variation of sensitivity with temperature is listed in Tables [6](#page-10-2) and [7.](#page-11-0) As is clear from the results, we fnd that the sensitivity of gold and silver grating-based SPR sensors is very stable with the change of temperature. It may be

noted that the theoretical results are in reasonable agreement with the literature one (Chiang et al. [2001](#page-13-16); Sharma and Gupta [2006](#page-14-10)). Further, increases of the temperature decreases the quality of proposed sensors, as expected from Eq. ([18](#page-5-1)). It decreases to 37.55 RIU⁻¹ and 43.04 RIU−1 for the case of gold grating-based SPR sensor and silver grating-based SPR sensor, respectively. So we cannot improve the sensitivity and the quality of grating-based

Fig. 8 Linear regression analysis between resonance angle and refractive index of analyte for gold

Fig. 9 Linear regression analysis between resonance angle and refractive index of analyte for silver

SPR sensor by increases the temperature. On the other hand, the resonant angles were plotted as a function of the sensing refractive index for diferent temperature in Figs. [8](#page-11-1) and [9.](#page-12-0) It could be observed from that the resonance angle increases linearly as analyte index increases. This is show a good linearity and stability of the gold and silver grating- based SPR sensors response, respectively.

7 Conclusions

In this paper, we have analyzed in detail the temperature dependence of the performance of a 1D grating sensor based on surface plasmon resonance. The sensor performance has been presented in terms of the detection accuracy (DA), the sensitivity S and the quality parameter (χ) . We have used two sensors with different metals, namely gold and silver. Silver provides large values of DA, S and γ compared to gold. As far as the temperature dependence is concerned, there is not much diference in the sensor's performance. Both metals show almost the same variation in DA, S and χ with temperature. However, best performance has been obtained for sensor consists of Ag at the room temperature $T = 300$ K.

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