#### REVIEW PAPER



# Pharmacodynamic model of slow reversible binding and its applications in pharmacokinetic/pharmacodynamic modeling: review and tutorial

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## Abstract

Therapeutic responses of most drugs are initiated by the rate and degree of binding to their receptors or targets. The law of mass action describes the rate of drug-receptor complex association ( $k_{on}$ ) and dissociation ( $k_{off}$ ) where the ratio  $k_{off}/k_{on}$  is the equilibrium dissociation constant  $(K_d)$ . Drugs with slow reversible binding (SRB) often demonstrate delayed onset and prolonged pharmacodynamic effects. This report reviews evidence for drugs with SRB features, describes previous pharmacokinetic/pharmacodynamic (PK/PD) modeling efforts of several such drugs, provides a tutorial on the mathematics and properties of SRB models, demonstrates applications of SRB models to additional compounds, and compares PK/PD fittings of SRB with other mechanistic models. We identified and summarized 52 drugs with in vitro-confirmed SRB from a PubMed literature search. Simulations with a SRB model and observed PK/PD profiles showed delayed and prolonged responses and that increasing doses/ $k_{on}$  or decreasing  $k_{off}$  led to greater expected maximum effects and a longer duration of effects. Recession slopes for return of responses to baseline after single doses were nearly linear with an inflection point that approaches a limiting value at larger doses. The SRB model newly captured literature data for the antihypertensive effects of candesartan and antiallergic effects of noberastine. Their PD profiles could also be fitted with indirect response and biophase models with minimal differences. The applicability of SRB models is probably commonplace, but underappreciated, owing to the need for in vitro confirmation of binding kinetics and the similarity of PK/PD profiles to models with other mechanistic determinants.

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#### Graphical abstract



Keywords Slow reversible binding · Pharmacodynamics · Mathematical modeling · Receptor binding kinetics · Indirect response models - Biophase models

# Introduction

The pharmacological responses of most drugs are initiated by binding to its receptor or target. To translate the receptor binding into clinical outcomes, many factors need to be considered: drug concentrations at the target site, type of drug-receptor interaction, and receptor activation and transduction processes [\[1](#page-14-0)]. The term receptor or target here represents any biological entity that interacts with a drug, including enzymes, ion channels, carrier transporters, DNA, and structures in the nucleus producing ensuing biological responses. Most of the time, binding events occur rapidly so that the receptor-bound drug complex is in constant equilibrium with the free drug at the effect site. In this case, drug-receptor interaction is quantified by receptor affinity and  $IC_{50}$ ,  $K_i$ , or  $K_d$  values determined from affinitybased measurements can be used to provide insight into the drug potency, which is also known as the drug thermodynamic selectivity [\[2](#page-14-0)]. However, when drug-receptor interaction does not equilibrate instantly, binding kinetics should be considered in accounting for the time-dependent changes in receptor engagement. Various conditions can cause the lack of and variability in equilibration, such as limited accessibility of the receptor binding site, limited conformational flexibility of the receptor, and hydrogen bonds for drug-receptor interaction being shielded by surrounding hydrophobic regions [\[3](#page-14-0)]. Under these circumstances, drug efficacy is influenced by the association rate constant  $(k_{on})$ , which primarily governes the time for drug to bind to the receptor, and the dissociation rate constant  $(k<sub>off</sub>)$ , which mainly determines the duration of receptor occupancy. Thus, even for drugs with similar  $IC_{50}$  values for their targets, if their  $k_{on}$  and  $k_{off}$  values differ, they may still have different response profiles, which is known as kinetic selectivity [[2\]](#page-14-0).

For drugs with Slow Reversible Binding (SRB), the duration of drug action can be determined by the dissociation half-life  $(0.693/k<sub>off</sub>)$  or residence time  $(1/k<sub>off</sub>)$  in addition to its pharmacokinetics. Drug dissociation halflives can vary from seconds to hours or even days. Long dissociation half-lives often result in prolonged drug action and maximized efficacy [\[4](#page-14-0), [5\]](#page-14-0). For example, tiotropium is an inhaled long-acting muscarinic acetylcholine receptor antagonist in the management of chronic obstructive pul-monary disease [\[6](#page-14-0)]. In a radioligand binding study, tiotropium showed slow dissociation kinetics to human muscarinic receptors with a dissociation half-life of 7.7 h, which is longer than the older antimuscarinic ipratropium

<span id="page-2-0"></span>(0.17 h) [\[7](#page-14-0)]. The SRB of tiotropium explains its long duration of action of 24 h, compared to less than 6 h for ipratropium [\[7](#page-14-0)]. This allows less frequent administration and higher trough efficacy for tiotropium than ipratropium [\[8](#page-14-0)]. Compared to fast kinetic drugs, drugs with SRB may be more vulnerable to target-based toxicity. This can be evidenced with antipsychotic agents with different  $k_{off}$ from  $D_2$  dopamine receptors. Typical antipsychotic agents, such as nemonapirde, spiperone, and haloperidol, have high affinities to  $D_2$  receptors with long dissociation halflives (5.92 h, 3.33 h, and 0.67 h, respectively), and are often associated with severe extrapyramidal motor side effects and prolactin elevation [[9\]](#page-14-0). Atypical antipsychotic agents such as clozapine and quetiapine, however, are free from these side effects and show less  $D_2$  receptor affinity with dissociation half-lives less than 0.5 min. This may be explained by the fact that when endogenous dopamine increases, drugs like clozapine can rapidly dissociate from the receptor to provide more access to the dopamine surge and thereby reduce the chance of extrapyramidal side effects and prolactin elevation [\[9](#page-14-0)]. Thus, drug binding kinetics, especially for those with slow dissociation, can shape the dose–response relationship by influencing the efficacy, duration of action, and safety [[1,](#page-14-0) [10](#page-14-0)].

The concept of SRB was noticed by Fuseau and Sheiner in 1984, where nonequilibrium between the drug concentration at the effect site and receptor was considered as a violation of the assumption of an effect compartment model [[11\]](#page-14-0). In 1996, Shimada et al. applied a SRB model to delineate the antihypertensive effects of eight calcium channel blockers [[12\]](#page-14-0). These drugs exhibited long-lasting antihypertensive effects compared to their short plasma elimination half-lives. The delay between plasma concentrations and effects usually produced counterclockwise hysteresis. The delayed effects were captured by incorporating drug association and dissociation rates in the ''ion-



Fig. 1 Structure of the SRB model with general PK compartments and receptor binding. Compartments and processes with broken lines are used when needed

channel binding model'' under the assumption that the pharmacological effect was directly proportional to the concentration of the drug-receptor complex. In addition to the model fitting, the estimated  $K_d$  values (ratio of  $k_{off}/k_{on}$ ) were well correlated with those obtained from in vitro binding studies.

The implications of binding kinetics in drug discovery and lead optimization have been partly reviewed previously [\[2](#page-14-0), [4](#page-14-0), [5](#page-14-0), [13,](#page-14-0) [14\]](#page-14-0). Copeland and Swinney both addressed the importance of obtaining these rate constants as they can provide additional insights on drug-target potency compared to traditional affinity parameters [\[5](#page-14-0), [13](#page-14-0)]. Drugs with different dissociation half-lives were pointed out to demonstrate the relation of dissociation rate and drug efficacy [\[4](#page-14-0), [5,](#page-14-0) [13](#page-14-0)]. Dahl et al. examined the combined effect of PK and binding kinetics on the duration of drug efficacy [\[14](#page-14-0)]. Most drugs have a longer elimination halflife than  $k_{off}$  half-life.

This report reviews and evaluates PK/PD models of SRB. We provide a review of the literature on drugs with SRB. Since drugs with target-mediated drug disposition (TMDD) demonstrate much more complex PK/PD, they were not included in the current review. A basic SRB model is provided with mathematical derivations of key graphical properties and simulations with signature profiles to describe the effects of dose,  $k_{on}$ ,  $k_{off}$ ,  $E_{max}$  and elimination rate constant  $(k_{el})$  values on response patterns. Additional demonstrations of model applications to two drugs and their effects illustrate principles of data analysis. Finally, a comparison of the SRB with other basic mechanistic models is provided.

#### **Theoretical**

The SRB model (Fig. 1) is based on the classical receptor occupancy theory and the law of mass action [\[15](#page-14-0)] with the assumption that the effect of drug  $(\Delta E)$  is proportional and directly linked to the concentration of the drug-receptor complex (RC). In addition, the model assumes that the delay of response is due to the rate of drug binding to  $(k_{on})$ or dissociating from  $(k_{off})$  the receptors. The total number of receptors  $(R_t)$  is assumed to remain constant. The model also assumes that drug concentration at the target site  $(C_t)$ is proportional to the plasma drug concentration  $(C_p)$  and is in excess compared to receptor concentration.

Accordingly, the rate of change of RC is:

$$
\frac{dRC}{dt} = k_{on} \cdot C_t \cdot (R_t - RC) - k_{off} \cdot RC \tag{1}
$$

with an initial condition of

$$
RC(0) = 0 \tag{2}
$$

<span id="page-3-0"></span>where  $R_t$  is the total receptor content,  $C_t$  is the free drug concentration at the target site,  $k_{on}$  is a second-order association constant, and  $k_{off}$  is a first-order dissociation constant. Free receptors  $(R)$  are equal to  $R_t$ –RC.

Since the pharmacological effect of drug is assumed to be proportional to the RC concentration,  $C_t$  is proportional to the plasma drug concentration  $(C_p)$ , and the maximum effect  $(E_{max})$  is obtained at  $RC = R_t$ . The relationship between drug effect and  $C_p$  can be defined as:

$$
\frac{d\Delta E}{dt} = k_{on} \cdot C_p \cdot (E_{max} - E) - k_{off} \cdot \Delta E \tag{3}
$$

with an initial condition of

$$
\Delta E(0) = 0 \tag{4}
$$

Thus drug effect as  $\Delta E/E_{max}$  corresponds to receptor occupancy  $(RC/R<sub>t</sub>)$ . This assumes that the drug is a full agonist. If the mechanism is for a partial agonist or a system with spare receptors, there may exist a more complex proportionality.

When the effect reaches its peak,  $\frac{dE}{dt} = 0$ , the observed maximum effect  $(\Delta E_m)$  can be expressed as:

$$
\Delta E_m = \frac{k_{on} \cdot E_{max}}{k_{on} + k_{off}/C_m} \tag{5}
$$

where  $C_m$  is the plasma concentration when  $\Delta E_m$  is reached  $(C_m > 0)$ . Since the equilibrium dissociation constant  $(K_d) = k_{off}/k_{on}$ , Eq. 5 can be rearranged as:

$$
\Delta E_m = \frac{E_{max}}{1 + K_d / C_m} \tag{6}
$$

Therefore, at a high dose level,  $C_m$  is high, which leads to  $\Delta E_m$  closer to  $E_{max}$ . If  $C_m >> K_d$ , then  $\Delta E_m = E_{max}$ .

#### Pharmacodynamic parameter estimations

The following study design is advisable to fully illustrate a PK/PD model of SRB for PD parameter estimation: (1) drug is administered at two or more dose levels; (2) one of the doses should lead to  $C_{max}$  much higher than  $K_d$  (around 10 times higher); (3) the baseline and/or placebo effects over time should be evident and constant.

Based on Eq. 6, the initial estimation of  $E_{max}$  can be obtained from the peak effect at the highest dose.

To obtain the initial estimation of  $k_{on}$ , the initial slope  $(S<sub>I</sub>)$  from the effect versus time curve can be obtained. Since at the initial phase,

$$
\frac{d\Delta E}{dt} \text{ or } S_1 \cdot \to k_{on} \cdot \cdot \cdot C \cdot \cdot \cdot E_{\text{max}} \cdot \cdot \cdot \cdot \cdot \text{ as } \cdot \Delta E \cdot \to \cdot 0 \tag{7}
$$

Using the concentration at the midpoint of the slope  $(C_{mid})$ ,  $k_{on}$  can be obtained as

$$
k_{on} \to \frac{S_I}{C_{mid} \cdot E_{max}} \text{ as } \Delta E \to 0 \tag{8}
$$

Based on Eq. 5, an initial estimation of  $k_{off}$  can be obtained from the  $\Delta E_m$  at a dose other than the highest dose, with  $C_m$  substituted by the maximum or initial plasma concentration ( $C_{max}$  or  $C_0$ ):

$$
k_{off} \rightarrow k_{on} \cdot C_{max/0} \cdot \left(\frac{E_{max}}{\Delta E_m} - 1\right) \tag{9}
$$

Due to the non-linearity and time-dependency of the SRB model, the final parameters should be obtained based on fitting the PK/PD model equations using nonlinear leastsquares regression analysis.

## Methods

#### Data

Data from the literature were used in the present report. A literature search was performed in PubMed using the keywords ''((slow binding kinetics) OR (slow dissociation)) AND (drug)''. In addition, references from published articles were traced. The mean values of PK/PD data from the publications were digitalized by WebPlotDigitizer (Version 4.5, <https://automeris.io/WebPlotDigitizer>). Thus, the estimated PK/PD parameters should be considered approximate.

## Data analysis

The PK and PK/PD data were analyzed sequentially. The mean values of the plasma concentrations were first fitted to an appropriate PK model. The PK parameters were then fixed to obtain the plasma concentrations that drive the PD. The PD data were then fitted with the SRB model (Eqs. 3) and 4) to obtain  $k_{\text{on}}$ ,  $k_{\text{off}}$ , and  $E_{\text{max}}$ . All data fitting and simulations were performed in NONMEM, version 7.4.1 (Sample model code is provided in Supplemental Materials). The proportional error model and the first-order conditional estimation method with interaction (FOCEI) were used. No interindividual variability was considered since mean values were used. The goodness-of-fit was assessed by the Akaike Information Criterion (AIC), residual error, precision (CV%) of the parameters, and visual check of the fitted curves.

<span id="page-4-0"></span>



#### Table 1 (continued)



\*Dissociation half-life ( $k_{off} t_{1/2}$ ) = 0.693/ $k_{off}$ 

## **Results**

# Literature review of drugs with slow binding kinetics

Literature search using PubMed resulted in 3443 articles (last accessed in April 2022). Although there is no clear demarcation between fast and slow binding kinetics, drugs with dissociation half-lives longer than 10 min (0.17 h) are considered SRB drugs in the current report and their in vitro binding kinetics, efficacy parameters, and plasma elimination half-lives are summarized in Table [1](#page-4-0). These drugs have a variety of therapeutic indications with many of them from sartans, antihistamines, and antivirals. Several drugs demonstrated extremely long dissociation halflives, such as darunavir (247 h) and dolutegravir (71 h), which explains their potent activities [[16,](#page-14-0) [17](#page-14-0)]. Many slow binding drugs have long elimination half-lives, which was observed by Dahl et al. [[14\]](#page-14-0).

#### Sources of binding parameters

The drug dissociation rates for these drugs are generally determined by preincubation of radiolabeled drugs with receptors followed by measuring the time-course of the receptor binding under wash-out conditions [\[18](#page-14-0)]. The wash-out medium is usually supplied with an excess of unlabeled competitive ligands to replace the binding of radiolabeled drugs to the receptors. The  $k_{off}$  can be obtained by fitting the percentage of receptor binding versus time  $(t)$ plot as:

$$
Receptor binding (\%) = e^{-k_{off} \cdot t}
$$
 (10)

Association rates of drugs can be directly measured by the time-course of binding of radiolabeled drugs to the receptors [[19\]](#page-14-0). The percentage receptor binding versus time curve can be first fitted by:

$$
Receptor binding (\%) = 1 - e^{-k_{obs} \cdot t}
$$
 (11)

to obtain the pseudo-first-order rate constant  $(k_{obs})$ . Then  $k_{on}$  can then be obtained based on:

$$
k_{obs} = k_{on} \cdot [D] + k_{off} \tag{12}
$$

where [D] is the radiolabeled drug concentration used for measuring receptor binding. The  $k_{on}$  can also be determined in competitive association experiments, where only unlabeled drugs are required to co-incubate with competitive radiolabeled ligands using the Motulsky–Mahan model [\[20](#page-14-0)]. Several antihistamines, muscarinic receptor

<span id="page-6-0"></span>





Fig. 2 Simulated PD effects (solid line) of a hypothetical drug with slow reversible binding following single bolus IV administration at doses of 0, 0.1, 0.2, 0.5, 1, and 2 mg. The corresponding PK profiles are shown as dashed lines. Values of  $CL = 20$  L/h,  $V = 80$  L, baseline  $E_{bl} = 20$ ,  $E_{max} = 10$ ,  $k_{on} = 0.125$  L/ $\mu$ g·h, and  $k_{off}$  = 0.125 /h were used for simulations. The observed effect =  $E_{bl} - \Delta E$ 



antagonists and antipsychotics were measured in this way [\[7](#page-14-0), [21,](#page-14-0) [22](#page-14-0)]. Biosensor-based studies or surface plasmon resonance (SPR) technology has been applied to analyze the binding kinetics of antivirals, such as darunavir and atazanavir [\[16](#page-14-0), [23](#page-14-0)]. It can measure the  $k_{on}$  and  $k_{off}$  and requires only a small amount of drug without radiolabeling. The drug affinity values  $(IC_{50}/K_i)$  summarized in Table [1](#page-4-0) are usually higher than  $K_d$ , suggesting the underprediction of drug affinity using  $IC_{50}/K_i$  values for SRB drugs. Lastly, the value of  $k_{on}$  can be determined from  $k_{on} = k_{off}/K_d$ , once the latter two have been assessed.

## Previous SRB modeling

Although many drugs with SRB have been reported, only few studies applied SRB models to describe the PK/PD (Table 2). Besides the application by Shimada et al. [\[12](#page-14-0)], the SRB model was applied to describe the inotropic response of digoxin in rats [[24\]](#page-14-0). The model well-captured the digoxin PD after bolus dose and in concentration clamp experiments. The SRB model was applied in analyzing the anti-secretory effects of several gastric acid pump inhibitors in dogs and humans [[25,](#page-14-0) [26\]](#page-14-0). One of these, H 335/25, showed rapid onset but delayed effects compared to its PK [\[25](#page-14-0)]. The delayed effects were captured by the SRB model and further compared with fittings using biophase and indirect response models. The SRB model was considered superior based on the Akaike Information Criterion. In addition, a SRB model was combined with a biophase model to describe the antinociceptive and respiratory depressant effects of buprenorphine in rats and humans [\[27–30](#page-15-0)]. In these studies, concentrations of buprenorphine at an effect site but not in plasma were assumed to form the drug-receptor complex to exert pharmacological effects.



Fig. 3 Simulated PD profiles of drug with indicated  $k_{on}$  or  $k_{off}$  values following a single bolus IV dose of 0.5 mg. The PK and other parameters used for simulations were the same and held constant as those in Fig. [2](#page-6-0). Note that the  $k_{el}$  was assumed to be 0.25 1/h

#### Model simulations

To evaluate the expected properties of the SRB model, the response profiles for a theoretical drug with mono-exponential kinetics and a range of doses were simulated as shown in Fig. [2](#page-6-0). The drug is assumed to have clearance  $(CL) = 20$  L/h and volume of distribution  $(V) = 80$  L after bolus intravenous  $(IV)$  doses of 0.1, 0.2, 0.5, 1, and 2 mg. The PD parameters of the drug were: baseline  $E_{bl} = 20$ ,  $E_{max} = 10$ ,  $k_{on} = 0.125$  L/ $\mu$ g·h, and  $k_{off} = 0.125$  /h. The observed effects  $E = E_{bl} - \Delta E$  were generated with no relative standard error.

As doses increased, the overall size of the response profile increased with a rapid initial decline, a plateau at the peak or nadir, and a return to baseline that was nearly linear and parallel at larger doses. The  $E_m$  and  $S_l$  increased with the time to reach  $E_m$  ( $t_{Em}$ ) shifting to earlier times (at 5.1, 4.8, 3.9, 2.9, and 2 h from low to high doses). Thus, at higher dose levels, a lesser delay in onset of effects is expected.

The explicit formula for area between the baseline and effect curve (ABEC) is:

$$
ABEC = \frac{E_{max}}{k_{el}} ln\left(1 + \frac{Dose/V}{K_d}\right)
$$
\n(13)

as shown by derivations in the Supplemental Materials.

Thus, ABEC is expected to increase in proportion to  $E_{max}$ ,  $1/k_{el}$ , and the log of the dose at higher value This has similar determinants as the ABEC of direct and indirect response models [[31,](#page-15-0) [32](#page-15-0)]. By substituting  $C_m$  with the initial concentration  $(C_0)$  of 1.25, 2.5, 6.2, 12.5, and 25 µg/ L from 5 doses in Eq. [6](#page-3-0), the resulting effects were 4.67, 6.51, 8.38, 9.17, and 9.59, which were close to the  $E_m$  of 2.57, 4.31, 7.02, 8.57, and 9.39. Thus,  $E_m$  can be obtained based on Eq. [6](#page-3-0) with either  $C_0$  or  $C_{max}$ .

Response profiles were also generated for a dose of 0.5 mg with changes in  $k_{on}$  (0.0125, 0.025, 0.125, 0.625,

and 1.25 L/ $\mu$ g-h) or  $k_{off}$  (0.0125, 0.025, 0.125, 0.625, and 1.25  $/h$ ) as demonstrated in Fig. 3. When  $k_{on}$  increased, the  $E_m$  and  $S_I$  increased with  $t_{Em}$  shifting to an earlier time. Decreasing  $k_{off}$  led to increase in  $E_m$  and a later  $t_{Em}$  but without change in  $S_I$ . The profiles for the SRB become particularly distinctive when  $k_{off}$  is much smaller than  $k_{el}$ producing, as expected, a prolonged duration of responses (also see Supplementary Fig. 2).

The effects of  $E_{max}$  and  $k_{el}$  on the PK/PD profiles for a dose of 0.5 mg were further evaluated. With increased  $E_{max}$ , the  $E_m$  and  $S_I$  increased with the  $t_{Em}$  remaining constant (Supplementary Fig. 1). The recession slopes  $(S_{fp})$ were directly proportional to  $E_{max}$  values. Decreasing  $k_{el}$ (2.5, 1.25, 0.5, 0.05, and 0.025 /h) by changing CL to 200, 100, 20, 4, and 2 L/h resulted in an increased  $E_m$  and a later  $t_{Em}$  and without changes in  $S_I$  values (Supplementary Fig. 2). The recession slopes increased with lower  $k_{el}$  but decreased at higher  $k_{el}$  values.

The pharmacodynamic profiles of the SRB model showed a single inflection point during the recession phase. The slope at the inflection point  $(S_{fp})$  was derived and is fully determined by the  $k_{on}$ ,  $k_{off}$ ,  $k_{el}$ ,  $E_{max}$ , concentration at the inflection point  $(C_{fp})$ , and effect at the inflection point  $(\Delta E_{fp})$  (Supplementary Materials). However, it was found that  $C_{fp}$  approaches a limiting value as the dose becomes very large. This results in a limiting value for  $S_{fp}$  so that the recession slopes are parallel at larger doses (Supplementary Fig. 3). In addition, it can be noted that the occurrence of  $C_{fp}$  becomes closer to  $K_d$  in the effect curve when  $k_{\text{off}} >> k_{el}$  (Supplementary Fig. 4).

When  $k_{off}$  becomes very large, the SRB model will behave like a simple direct effect model as drug-receptor binding essentially equilibrates instantly. The ratio of  $S_{fp}$  $k_{off}$  is an upper bound for the difference between these two models (derivation provided in Supplementary Materials). Thus, after normalizing with the effect, the quotient  $(S_{fp}/k_{off})/(E_0 - E_{max})$  can serve as a metric to examine the

<span id="page-8-0"></span>

placebo<br>1 mg<br>2 mg<br>4 mg<br>8 mg  $\ddot{\bullet}$ Increase of SBP after<br>angiotensin II challenge (mm Hg) 40 30 20  $\bullet$  $10$  $\pmb{0}$ ٦ 6  $12$  $\pmb{0}$ 18 24 Time (h)

Fig. 4 PK/PD profiles of candesartan on systolic blood pressure (SBP) after single oral administration of either candesartan cilexetil at the indicated doses or placebo in healthy volunteers. A onecompartment PK model with first-order absorption and elimination

and SRB model as shown in Fig. [1](#page-2-0) was applied. Symbols depict data calculated from Delacrétaz et al. [\[39\]](#page-15-0), and lines are fitted responses. Parameters are presented in Table 3

Parameters	Units	Definition	Estimate $(CV\%)$
PK.			
$k_a$	1/h	Absorption rate constant	0.54(6.1)
CL/F	L/h	Clearance	11.8(10.3)
V/F	L	Volume of distribution	84.3 (11.4)
<b>PD</b>			
$k_{on}$	$L/\mu g \cdot h$	Second-order association rate	0.0142(12.9)
$k_{off}$	1/h	First-order dissociation rate	0.277(62.5)
$E_{max}$	mm Hg	Maximum effect	33(25.8)
BASL	mm Hg	Baseline effect	$31.1$ (fixed)
<b>DREC</b>	mm Hg	Amplitude of placebo effect	$4.59$ (fixed)
$k_{ep}$	1/h	Rate of placebo effect	$0.0829$ (fixed)



Table 3 PK/PD parameters of candesartan effects on systolic blood pressure in humans



<span id="page-9-0"></span>

Fig. 5 PK/PD profiles of noberastine on histamine induced wheal diameter after single oral doses as indicated or placebo in healthy volunteers. A two-compartment PK model with zero-order absorption and first-order elimination and SRB model as shown in Fig. [1](#page-2-0) was

convergence of a SRB to a direct effect model (Supplementary Fig. 5). When  $k_{off}$  is larger than 4, corresponding to a dissociation half-life shorter than 10 min,  $(S_{\text{fp}}/k_{\text{off}})/(E_0 - E_{\text{max}})$  is close to zero, suggesting the convergence of the SRB to the direct effect model. Therefore, the SRB should be considered for drugs with a dissociation half-life longer than 10 min; otherwise, a simple direct effect model can be applied. A consequence of convergence of the SRB model to the simple direct model for large  $k_{off}$  is that  $C_{fp}$ ,  $\Delta E_{fp}$ , and  $S_{fp}$  are converging to the values reported for the latter model elsewhere [\[33](#page-15-0)]. Hence,  $C_{fp}$  becomes close to  $K_d$ ,  $\Delta E_{fp}$  close to  $E_{max}/2$  and  $S_{fp}$  close to  $k_{el}E_{max}/4$ .



Fig. 6 Model fittings for the effects of candesartan on systolic blood pressure in humans by the slow binding model (solid line), indirect response model I (broken line), and biophase model (dotted line). The data generated from Delacrétaz et al.  $[36]$  are shown as solid circles



applied. Symbols depict the observed data from Wood-Baker et al. [[48](#page-15-0)], and lines are fitted responses. Parameters are presented in Table [4](#page-8-0)



Fig. 7 Model fittings for the effects of noberastine on histamine induced wheal diameter in humans by the slow binding model (solid line), indirect response model I (broken line), and biophase model (dotted line). The observed data from Wood-Baker et al. [[44](#page-15-0)] are shown as solid circles

#### Clinical PK/PD examples of SRB applications

#### Sartans

Sartans are orally active angiotensin II receptor type 1 (AT1) antagonists used for the treatment of hypertension and related diseases [[34\]](#page-15-0). A number of sartans are frequently used in clinical therapy, including candesartan, olmesartan, telmisartan, valsartan, irbesartan, and losartan. Although they share a common binding site, their binding kinetics differ, which results in different binding potency and clinical effects. Losartan showed a surmountable antagonism phenomenon in an in vitro study, which is typical

Parameters	Units	Definition	Slow reversible binding model	Indirect response model I	Biophase model
AIC		Akaike Information Criterion	158.17	168.76	165.87
$k_{on}$	$L/\mu g \cdot h$	Second-order association rate	0.0142(12.9)		
$k_{off}$	1/h	First-order dissociation rate	0.277(62.5)		
$k_{out}$	1/h	First-order removal rate		0.606(42.1)	
$k_{eo}$	1/h	First-order distribution rate			0.544(79)
$IC_{50}$ or $K_d$	$\mu$ g/L	Concentration at half-maximal inhibition dissociation constant	19.5	12.9(6.4)	26.6(133.1)
$I_{max}$		Maximal inhibition		$1$ (fixed)	
$E_{max}$	mm Hg	Maximal effect	33(25.8)		44 (71.6)
BASL	mm Hg	Baseline effect	$31.1$ (fixed)	$31.1$ (fixed)	$31.1$ (fixed)
<b>DREC</b>	mm Hg	Amplitude of placebo effect	$4.59$ (fixed)	$4.59$ (fixed)	$4.59$ (fixed)
$k_{ep}$	1/h	Rate of placebo effect	$0.0829$ (fixed)	$0.0829$ (fixed)	$0.0829$ (fixed)
Prop. error		Proportional error	0.159(19.6)	0.182(19.2)	0.17(20.8)

<span id="page-10-0"></span>Table 5 Pharmacodynamic parameters of candesartan effects on systolic blood pressure in humans assessed by three models

Table 6 Pharmacodynamic parameters of noberastine effects on histamine-induced wheal diameter in humans assessed by three models

<b>Parameters</b>	Units	Definition	Slow reversible binding model	Indirect response model I	Biophase model
AIC		Akaike Information Criterion	$-27.4$	11.19	$-13.1$
$k_{on}$	$L/\mu g \cdot h$	Second-order association rate	0.134(7.3)		
$k_{off}$	1/h	First-order dissociation rate	0.203(6.9)		
$k_{out}$	1/h	First-order removal rate		1.17(15.6)	
$k_{eo}$	1/h	First-order distribution rate			0.458(12.6)
$IC_{50}$ or $K_d$	$\mu$ g/L	Concentration at half-maximal inhibition/ dissociation constant	1.51	0.906(11.8)	2.12(7.2)
$I_{max}$		Maximal inhibition		$1$ (fixed)	
$E_{max}$	cm	Maximal effect	7.61(1.9)		8.1(1.5)
BASL	cm	Baseline effect	6.9(2)	7.09(6.1)	6.76(0.9)
Prop error		Proportional error	0.159(19.6)	0.22(24.2)	0.154(11.4)

for fast-dissociating antagonists [[35\]](#page-15-0). Most sartans, such as candesartan, olmesartan, telmisartan, valsartan, and irbesartan, produced partial depression of the maximal response in the in vitro study, which is known as insurmountable antagonism [[19,](#page-14-0) [34](#page-15-0), [36](#page-15-0)]. Such behaviors are largely due to their slow dissociation from AT1 receptors, especially for candesartan with a dissociation half-life of 3.25 h in the radioligand binding study [[18\]](#page-14-0). Comparison of clinical studies showed that sartans with slow dissociation, such as valsartan, olmsartan and candesartan, had higher maximal effects on blood pressure than losaratan, which has a fast dissociation rate [[5\]](#page-14-0).

Candesartan cilexetil (TCV-116) is the esterified prodrug of candesartan and has been approved in many countries to treat hypertension [\[37](#page-15-0)]. Absorbed candesartan cilexetil is presumed to be completely metabolized to candesartan to exert pharmacological actions [[38\]](#page-15-0). Delacrétaz et al. evaluated the inhibitory effect of candesartan on blood pressure after oral administration of candesartan cilexetil at 1, 2, 4, and 8 mg in healthy volunteers [[39](#page-15-0)]. At 45 min before candesartan cilexetil or placebo administration, an IV bolus injection of angiotensin II at preestablished doses was given to increase the systolic blood pressure (SBP) by 31.1 mm Hg on average, which was considered as the baseline response. The plasma concentration of candesartan and change in SBP after drug intake were monitored. The plasma PK of candesartan following four oral doses were captured jointly by a one-compartment model with first-order absorption and elimination (Fig. [4](#page-8-0)). The PD of candesartan were assessed from the increase of SBP after angiotensin II challenge, which were back-calculated from the percent of baseline response in the published plot using the baseline response (BASL) of 31.1 mm Hg. The responses in the placebo group were described by a modified inverse Bateman function [\[40](#page-15-0), [41](#page-15-0)]:

$$
PLACEBO = BASIC - DREC \cdot k_{ep} \cdot t \cdot e^{-kept}
$$
 (14)

where *DREC* is the amplitude of placebo effect and kep is the rate constant for the associated placebo effect.

The PD effects of candesartan were obtained by:

$$
Effect = PLACEBO - \Delta E \tag{15}
$$

where  $\Delta E$  was based on the operation of SRB model (Eqs. [3](#page-3-0) and [4](#page-3-0)). The parameters for describing placebo effects were fixed during the model fitting of PD profiles of candesartan at four dose levels (Fig. [4\)](#page-8-0). The PK and PD parameters after model fitting are listed in Table [3.](#page-8-0) The estimated  $k_{on} = 0.0142$  L/µg·h (12.9% CV) and  $E_{max}$ = 33 mm Hg (25.8% CV) demonstrated reasonable precision. The estimated  $k_{off}$  was 0.277 1/h (62.5% CV), which translates to a dissociation half-life of around 2.5 h. This is close to the dissociation half-life of 3.25 h determined in the in vitro study  $[18]$  $[18]$ .

#### $H_1$ -Antihistamines

 $H_1$ -antihistamines are first-line treatments for allergic rhinoconjunctivitis and urticaria [\[42](#page-15-0)]. They target histamine, the major pathogenic mediator of allergic disorders, by binding to  $H_1$ -receptors to reduce the constitutive activity of the receptor and block the binding of histamine to the receptor [[43\]](#page-15-0). The first-generation antihistamines, such as chlorpheniramine, diphenhydramine, hydroxyzine, and ketotifen, demonstrated central nervous system (CNS) penetration that resulted in sedation and interference with the cognitive process [\[43](#page-15-0)]. The second-generation antihistamines overcome the CNS side effects with improved selectivity and tolerability. These include acrivastine, astemizole, cetirizine, ebastine, levocabastine, mizolastine, noberastine and terfenadine [\[44](#page-15-0)]. The in vitro receptor binding studies revealed the slow dissociation from the  $H_1$ receptor for several antihistamines, such as astemizole, cetirizine, fexofenadine, loratadine, levocetirizine, mequitazine, noberastine, and terfenadine [\[45](#page-15-0), [46\]](#page-15-0). This may contribute to the delayed onset and prolonged pharmacological actions of antihistamines observed in clinical studies [\[43](#page-15-0), [47](#page-15-0)].

Noberastine is a second-generation non-sedating antihistamine. The PK/PD profiles of noberastine at single oral doses of 10, 20, and 30 mg in healthy volunteers were published by Wood-Baker et al. [[48\]](#page-15-0). The plasma concentrations of noberastine were fitted using a two-compartment model with zero-order absorption and first-order elimination (Fig. [5](#page-9-0)). The PD responses of noberatine were assessed by the wheal diameters caused by histamine skin prick testing. One hour before drug administration, the baseline skin prick testing was performed to get the baseline wheal diameter. After drug administration, wheal diameters at designated intervals remained at similar levels to baseline in the placebo group and were inhibited in the noberastine treatment groups. Thus, the observed wheal diameters were described by

$$
Effect = BASIC - \Delta E \tag{16}
$$

where BASL was the baseline level and  $\Delta E$  was based on the operation of SRB model (Eqs. [3](#page-3-0) and [4\)](#page-3-0). The parameters after model fitting are listed in Table [4](#page-8-0). The zero-absorption rate was fixed to 30 mg/h since the data points in the absorption phase are limited. The PD profiles at all dose levels were well captured by the SRB model with good precision (1.9 to 7.3% CV) (Fig. [5\)](#page-9-0). The dissociation halflife calculated based on the estimated  $k_{off}$  of 0.203 1/h was 3.41 h, which is close to the dissociation half-life of 2.75 h measured in an in vitro study [\[45](#page-15-0)].

# Comparison of SRB model with indirect response and biophase models

In addition to the SRB model, we fitted the PD data of candesartan and noberastine with indirect response model I and the biophase model. The data can be captured by all three models with their fitted curves close to each other (Figs. [6](#page-9-0) and [7\)](#page-9-0). The very similar predictions from the three models were also observed for describing the effects of the gastric acid pump inhibitor, H  $335/25$ , by Abelö et al. [\[25](#page-14-0)]. However, one of the noticeable differences between the three models is that the peak or nadir effect is reached earlier with increasing doses for the SRB model; indirect response models exhibit peak or nadir effects later with increasing doses; and biophase models produce the time to peak or nadir effects that are constant for all doses. The PD plots of candesartan and noberastine both demonstrated an earlier nadir at higher doses, suggesting that the SRB model may be more appropriate. In addition, the SRB model showed the lowest AIC with acceptable variability for the two drugs (Tables [5](#page-10-0) and [6](#page-10-0)). The biophase model for candesartan showed the poorest precision of estimated parameters ( $CV > 71.6\%$ ). Therefore, the SRB model was superior to the other two models for the current PK/PD data for candesartan and noberastine. However, the differences between the three models are minimal. This may also result from the similar plasma elimination rates and dissociation rates for candesartan and noberastine, which will retain the return phase of the PD plots. Even when elimination rate is comparable or slower to the dissociation rate, the time to reach to peak or nadir effect are earlier at higher doses still hold true for SRB model. Thus, high quality data from a wide range of dose levels are required to differentiate the model type in performing fittings.

It is interesting to note that the 50% effective drug concentration values ( $EC_{50}$ ,  $IC_{50}$  and  $K_d$ ) are similar for each drug for the three models. This might be expected since it is the same PK profiles that are driving the same responses.

# **Discussion**

The responses of many drugs with SRB can be described by a simple model based on the law of mass action and classical receptor occupancy theory. This model connects the drug PK and effects by considering the kinetics of receptor association and dissociation. Distinctive signature profiles are produced as compared to some other PD models.

The model of SRB demonstrated delayed onset and prolonged responses as the result of slow binding of the drug to the receptor. Increased doses lead to larger effects with peak or nadir effects shifting to earlier times. The onset slope is related to dose,  $k_{on}$  and  $E_{max}$  while the recession slope exhibits more complex behavior and approaches to a limiting value determined by  $k_{el}$  and  $E_{max}$ for higher doses. In addition, the SRB model will behave like simple direct effect model when  $k_{off}$  becomes very large. Based on our simulations with  $k_{el}$  of 0.25 1/h, the SRB model is generally considered for a drug with dissociation half-life longer than 10 min. However, it is difficult to define a clear cutoff value of  $k_{off}$  or  $k_{on}$  for SRB drugs based on these simulations as they cannot reflect the universe of possible combinations of the independent variables. Dahl et al. observed that the duration of effect will be most prolonged when  $k_{off}$  is slower than kel [\[14](#page-14-0)], but most drugs have a faster  $k_{off}$  as we also show in Table [1](#page-4-0).

While ionotropic receptors might be most likely to produce SRB profiles, metabolotropic (G-protein mediated), kinase, and nuclear receptors might produce delayed responses owing to the signaling cascades that follow receptor binding. However, the drugs listed in Table [1](#page-4-0) and [2](#page-6-0) show interactions with diverse targets including receptors and protease and integrase enzymes.

Proper in vitro experimental conditions are essential to obtain accurate binding kinetic parameters for drugs with SRB. For measuring  $k_{off}$ , the wash-out conditions are discerned by whether the fresh medium is used to replace the radiolabeled drug-containing medium and whether an excess amount of unlabeled competitive ligand is supplied [\[4](#page-14-0)]. The former condition may not substantially influence  $k_{off}$  whereas the latter condition of adding unlabeled ligand can effectively prevent the rebinding of the dissociated drug to the receptor, a phenomenon pervasively found for drugs with slow dissociation that can further prolong the dissociation [[4](#page-14-0), [49](#page-15-0)]. In the in vitro dissociation study with candesartan, when unlabeled candesartan is supplied, the dissociation half-life of candesartan decreased from 11.6 h to around 2 h [\[50](#page-15-0)]. The acceleration in  $k_{off}$  positively correlated with the amount of unlabeled ligand added in the medium, so the addition of an excess amount of unlabeled ligand (usually 100-fold) is required. Alternatively, diluting the radiolabeled drug-containing medium before adding unlabeled ligand to ensure the accuracy of measuring  $k_{off}$  is needed [\[50](#page-15-0)]. The  $K_d$  is sometimes measured as a surrogate of binding kinetics and reflects the affinity of the drug to the receptor. However,  $K_d$  must be obtained at equilibrium condition, which may be difficult to achieve for drugs with long dissociation half-lives. Lack of equilibration may result in underpredicting the affinity, so a higher  $K_d$  value is obtained [\[51](#page-15-0)]. In a saturation binding assay of candesartan, increasing incubation times from 5 to 180 min resulted in decreased apparent  $K_d$  from 1 to 0.02 nM, suggesting a lack of equilibration with short incubation time [[50](#page-15-0)]. Similarly, geldanamycin demonstrated a 40-fold decrease in  $K_d$  over 24 h incubation time [\[52](#page-15-0)]. The  $K_d$  of maraviroc obtained in the saturation binding study (0.86 nM) was also higher than the  $K_d$  calculated from the ratio of  $k_{off}/k_{on}$  (0.071 nM) [\[53](#page-15-0)]. Thus, for drugs with SRB, it is better to obtain  $K_d$  either from the kinetic parameters  $k_{off}$  and  $k_{on}$  or from saturation binding studies with sufficient incubation times (5-times the dis-sociation half-life) [[51\]](#page-15-0). More advanced technology, such as resonance energy transfer (RET) based techniques with fluorescent or bioluminescent energy sources, enables high-throughput binding kinetic assays [[54\]](#page-15-0). Surface plasmon resonance methodology provides a rigorous mea-surement of binding kinetics [[16\]](#page-14-0).

Several assumptions were made in our operation of the SRB model. The most important one is that the drug effect is assumed to be directly linked and proportional to the RC concentration. Under this condition,  $RC$  and  $R_t$  concentrations in the classical receptor occupancy theory can be replaced by drug effect and  $E_{max}$ . This is more of a simplified scenario as the true relationship between receptor occupancy and response may be of sigmoid shape and other transduction and homeostatic feedback mechanisms may be involved [\[1](#page-14-0)]. More complex models with binding kinetics have been reviewed [\[10](#page-14-0)]. Another assumption is that the plasma concentration is proportional to the drug concentration at the target site and is much greater than the receptor concentration. This allows the fraction of drug bound to the receptor to be negligible in relation to the free drug concentration; thus the plasma concentration can be used as a surrogate for free drug concentration and drug PK is not influenced by drug receptor binding. If the concentrations of drug and receptor are comparable, free drug concentrations change during receptor binding, which is a more complex situation known as slow tight-binding [\[55](#page-15-0)]. Under this condition, receptor binding may influence the drug PK, which can be described by the TMDD model [\[56](#page-15-0)]. This review does not consider drugs and proteins with TMDD properties as both the PK and PD become far more complicated.

The current report showed the application of the SRB model to the antihypertension effects of candesartan and antiallergic effects of noberastine. Their PD effects were well-captured by the SRB model. The dissociation halflives of the two drugs from the model predictions were close to their in vitro dissociation half-lives [[18,](#page-14-0) [45](#page-15-0)]. This suggests an opportunity for using the SRB model with in vitro binding kinetic parameters to predict drug responses. However, the predicted  $K_d$  for candesartan (19.5) ug/L) is higher than the in vitro measured  $K_d$  (5.7 ng/L) [\[18](#page-14-0)]. This may be attributed to the extensive plasma protein binding of candesartan  $(> 99\%$  in humans) [[37\]](#page-15-0), which may lead to the true free drug concentrations for receptor binding being much lower than the total plasma concentration. Noberastine also showed an underpredicted  $K_d$  of 1.51 ug/L compared to its in vitro  $K_i$  of 47 ng/L [\[45](#page-15-0)]. Although no plasma protein binding information was found for noberastine, many secondary-generation antihistamines demonstrate high protein binding, which may contribute to in vitro/in vivo differences in affinity [[57\]](#page-15-0).

Besides the similarities in shapes and in fitting response profiles, the three basic PK/PD models (as well as direct effect models) share the properties of a ABEC that is proportional to log Dose at higher doses and recession slopes that are essentially linear, parallel for higher doses, and determined by the  $E_{max}$  (or equivalent) and terminal slope of the PK  $(k_{el})$  or biophase  $(k_{eo})$  constant. Further, the SRB model can be interpreted as an indirect response model with a linear effect on  $k_{out}$  when  $k_{off}E_{max} = k_{in}$ ,  $k_{off} = k_{in}$ , and  $E_{max} = R_o$ . This indicates the need for higher doses of drugs in order to discriminate between these models by fitting data. It can be noted that the SRB and biophase models only require fitting of 3 parameters, while full indirect response model models require 4 parameters.

A biophase can be added to the SRB model either for greater mechanistic relevance or to further capture delays between drug concentrations and responses. This was done in investigating the antinociceptive and respiratory depressant effects of buprenorphine in rats and humans by Yassen et al. [[27–30\]](#page-15-0), where they showed that adding an effect compartment significantly improved the modeling performance. The biophase delay likely reflects the slow distribution of buprenorphine into or from the brain [\[29](#page-15-0)]. Thus, biophase equilibration and receptor binding can both contribute to the delayed and prolonged effects of slow binding drugs. Of course, other pharmacologic complexities may also apply such as turnover of targets, receptor desensitization, more complicated receptor binding kinetics, and nonlinear- or time-dependent transduction processes. When multiple steps are involved in the pharmacological response, such as for some corticosteroid actions, receptor-binding events with  $k_{off}$  and  $k_{on}$  can be included as an early step in a mRNA/protein/biomarker cascade [[58\]](#page-16-0). In addition, free drug concentrations will often be the preferred substrate for many drugs and receptors. Further, when receptor mechanisms involve partial agonists, spare receptors, or nonlinear transduction the concepts from Black and Leff [[59\]](#page-16-0) should be invoked. In essence, our model is simply a basic starting point that can be expanded in many ways.

The SRB model has been introduced and used since 1990s but has been largely overlooked. One possible reason is that other PD models, like indirect response and biophase models, can produce similar profiles as SRB and produce similar  $K_{d}$ ,  $EC_{50}$  or  $IC_{50}$  values. Many slow binding drugs also have long elimination half-lives, which may mask their SRB nature and produce similar profiles as direct effect models. Another reason is the limited availability of the kinetic binding parameters as additional in vitro experiments are required. However, the SRB model should clearly be part of the ''toolbox'' of pharmacometricians as it is intrinsically mathematically and graphically different from other PD models and might fit data better than with other models. The SRB model illustrated in the present study is a simplified version when binding kinetics are considered as the rate-limiting step for PD effects, but works quite well for many drugs.

## Conclusions

The kinetics of SRB have significance in drug action and help shape the clinical outcomes and safety profiles of many drugs. For drugs with slow association or dissociation rates from targets, a simple SRB model can be used to describe delayed drug responses by incorporating drug binding kinetics. To apply the SRB model with better estimation, high quality data from a wide range of doses with rich sampling points and additional confirmation from in vitro experiments are required. However, if only based on drug PD responses, it may be difficult to discern the SRB from indirect response and biophase models. Thus,

<span id="page-14-0"></span>mechanistic studies are required to understand the ratelimiting step in affecting the drug responses and to ensure appropriate model selection and application.

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#### **Declarations**

Conflict of interest The authors declare no conflicts of interest.

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