ORIGINAL RESEARCH



In vitro performance of prefilled CO₂ absorbers with the Aisys[®]

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Abstract Low flow anesthesia increases the use of CO_2 absorbents, but independent data that compare canister life of the newest CO₂ absorbents are scarce. Seven different pre-packed CO₂ canisters were tested in vitro: Amsorb Plus, Spherasorb, LoFloSorb, Medisorb, Medisorb EF, LithoLyme, and SpiraLith. CO_2 (160 mL min⁻¹) flowed into the tip of a 2 L breathing bag that was ventilated with a tidal volume of 500 mL, a respiratory rate of 10/min, and an I:E ratio of 1:1 using the controlled mechanical ventilation mode of the Aisys® (GE, Madison, WI, USA). In part I, canister life of each brand (all of the same lot) was tested with 12 different fresh gas flows (FGF) ranging from 0.25 to 4 L min⁻¹. In part II, canister life of six canisters each of two different lots of each brand were tested with a 350 mL min⁻¹ FGF. Canister life is presented as "FCU", fractional canister usage, the fraction of a canister used per hour, and is defined for the inspired CO₂ concentration (F₁CO₂) that denotes exhaustion. In part III, canister life per 100 g fresh granule content was calculated. FCU decreased linearly with increasing FGF. The relative position of the FCU-FGF curves of the different brands depends on the F₁CO₂ threshold because the exhaustion rate (the rate of

Jan F. A. Hendrickx jcnwahendrickx@yahoo.com rise once F_1CO_2 starts to increase) differs among the brands. Intra-lot variability was 18 % or less. The different prepacks can be ranked according their efficiency (least to most efficient) as follows: Amsorb Plus = Medisorb EF < LoFloSorb < Medisorb = Spherasorb = LithoLyme <SpiraLith (all for an F_1CO_2 threshold = 0.5 %). Canister life per 100 g fresh granule content is almost twice as long when LiOH is used as the primary absorbent. The most important factors that determine canister life of prepacks in a circle breathing system are the chemical composition of the canister, the absolute amount of absorbent present in the canister, and the F_1CO_2 replacement threshold. The use of the fractional canister usage allows cost comparisons among different prepacks. Results should not be extrapolated to prepacks that fit onto other anesthesia machines.

Keywords CO_2 absorbers \cdot Low flow anesthesia \cdot Anesthesia machine

1 Introduction

Conventional low flow anesthesia is increasingly used to decrease waste and thus cost of and pollution by anesthetic agents. In addition, already three anesthesia machines use automated low flow, target controlled agent and carrier gas delivery with minimal user intervention, making anesthesia with fresh gas flows (FGFs) well below 1 L.min⁻¹ the routine rather than the exception: the Aisys[®] (GE, Madison, WI, USA) and FLOW-i (Maquet, Solna, Sweden) use a maintenance FGF of 500 and 300 mL min⁻¹, respectively, and the Zeus (Draeger, Lubeck, Germany) is fully closed. These low FGFs will increase CO₂ absorbent usage though, because more CO₂ will pass through them. The composition of the newest CO₂ absorbents has changed (e.g., KOH

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has been eliminated to reduce anesthetic degradation), and the canister life of these absorbents has been incompletely studied and compared. This paucity of data is reflected in the small number of references quoted in this manuscript [1].

The aim of this study was to determine canister life of prefilled, disposable canisters ("prepacks") over a wide range of FGFs with the Aisys[®] under conditions that resemble in vivo conditions. Prepacks have a low volume to shorten the circle system's time constant, can be easily replaced without opening the circle system, and may ensure a more consistent humidity in the circle system [2]. Prepacks with different chemical composition of different manufacturers readily available to the authors were studied under standardized conditions with the same anesthesia machine, with FGF ranging from 0.25 to 5 L.min⁻¹. We examined the effect of canister brand, fresh gas flow (FGF), and F₁CO₂ replacement threshold on canister life. In addition, we examined intra- and inter-lot variability. This study does not address the effects of granular size and shape, canister shape, void space and other factors that affect canister performance.

2 Materials and methods

The patient's CO₂ production (VCO₂) was simulated by flowing CO₂ into the tip of a 2 L breathing bag that was attached to the Y-piece of a circle breathing system (Fig. 1). The breathing bag was ventilated with a tidal volume of 500 mL, a respiratory rate of 10/min, and an I:E ratio of 1:1 using the controlled mechanical ventilation mode of the Aisys[®] (GE, Madison, WI, USA). We used a CO_2 inflow of 160 mL min⁻¹: endogenous CO_2 production during general anesthesia in adults is approximately 130 mL min⁻¹ [3, 4], and applying a CO₂ pneumoperitoneum increases alveolar CO2 washout by approximately 30 mL min^{-1} [5–7]. With a minute ventilation of 5 L.min⁻¹, the in vitro end-expired CO₂ was approximately 4.5 %, resembling in vivo conditions. We avoided the use of higher CO₂ flows, so-called "accelerated" testing because they cause higher temperature gradients within the canister, which may cause decreased CO₂ absorption by the formation of water deposits on the granules due to cooling by the colder temperature of the operating room [8].

A CO₂ flow rotameter (MEDEC[®], Aalst, Belgium) was plugged into the CO₂ wall outlet of the operating room. Because the resolution of the flow meter (50 mL min⁻¹) was inadequate for the purpose of the study, CO₂ flow was derived from the line pressure in the line distal to the flow meter (Fig. 1). Four resistors between the CO₂ rotameter and the tip of the balloon attenuated the backpressure of ventilation on the CO₂ flow. A pressure—flow calibration curve was constructed by dialing at least six different (arbitrary) rotameter settings, recording the corresponding line pressure, and measuring the corresponding CO₂ flow volumetrically. The line pressure was measured between the second and third resistor (Pressure Monitoring Set, Edwards LifesciencesTM, Irvine, CA); the corresponding CO₂ flow was measured volumetrically by measuring the time to fill a 250 mL glass syringe (Popper and Sons, Inc. New Hyde Park, NY, USA) after switching a three way stopcock placed between the last resistor and the tip of the balloon. The calibration procedure was repeated before testing each new canister. A 1 mm Hg pressure difference corresponded to a 3.4 mL min⁻¹ CO₂ flow difference (obtained from the linear regression curve).

The CO_2 flows used to test the different canisters were compared using ANOVA (followed by the Holm-Sidak to test for intergroup differences) to make sure that minor differences in CO_2 inflow could be ruled out as a factor contributing to any possible differences in canister life of the different prepacks.

Inspired and expired gases were sampled and analyzed by a M-CAiOV module (GE, Madison, WI), which was calibrated according to the manufacturer's specifications. Before each experiment, we ensured the CO₂ waveform had a consistent morphology, without any oscillations or other artifact. To eliminate artifacts on the capnogram from gas entrainment from the inspiratory limb of the breathing system during the expiratory phase, two heat and moisture exchangers (Ref 352/5877, CovidienTM, Mansfield, MA) were placed in between the bag and the Y-piece. The gas was sampled from the filter closest to the breathing bag; sampled gases were redirected to the circuit via a connector between the expiratory limb and its connection to the Aisys[®].

2.1 Part I: canister life across a 0.25–4.0 L min⁻¹ FGF range with the same lot

The characteristics of the different prepacks that were tested can be found in Table 1. Twelve canisters of the same lot of each brand were tested with one of the 12 following O_2/air fresh gas flows (L.min⁻¹): 0.25; 0.3; 0.35; 0.5; 0.65; 0.75; 1.0; 1.2; 1.5; 2.0; 3.0; and 4.0. The delivered O_2 concentration was 55 %, except in those instances where the hypoxic guard imposed the delivery of higher O_2 concentrations. The weight of fresh CO₂ absorbent was obtained by subtracting the weight of the plastic encasement from the initial total weight using a high precision weighing scale (XP10002, Mettler-Toledo, Columbus, Ohio).

Prior to inserting each canister into the breathing system, the CO₂ rotameter dial was adjusted to obtain a stable



for CO₂ flowmeter

Fig. 1 In vitro set-up. A 160 mL min⁻¹ CO₂ flow enters the tip of a 2 L breathing bag that is attached to the Y-piece of a circle breathing system. The bag is ventilated with a tidal volume of 500 mL, a respiratory rate of 10/min, and an I:E ratio of 1:1 using the controlled mechanical ventilation mode of the Aisys[®] (GE, Madison, WI, USA). Gases sampled by the gas analyzer (approximately 200 mL min⁻¹) are redirected towards the expiratory limb of the circle breathing system. The experiment continues until the FICO₂ has reached at least 1.0 % (see text and Fig. 2 for details). CO₂ from the wall outlet is titrated via a rotameter towards a line pressure distal to the flow meter that corresponds with a 160 mL min⁻¹ CO₂ flow. Four resistors between the CO₂ rotameter and the tip of the balloon attenuated the backpressure of ventilation on the CO₂ flow. A pressure-flow

calibration curve is constructed by dialing at least 6 different (arbitrary) rotameter settings, recording the corresponding line pressure, and measuring the corresponding CO_2 flow volumetrically. The line pressure was measured between the second and third resistor (Pressure Monitoring Set, Edwards LifesciencesTM, Irvine, CA); the corresponding CO_2 flow was measured volumetrically by measuring the time to fill a 250 mL glass syringe (Popper and Sons, Inc. New Hyde Park, NY, USA) after switching a three way stopcock placed between the last resistor and the tip of the balloon. The calibration procedure was repeated before testing each new canister. A 1 mm Hg pressure difference corresponded to a 3.4 mL min⁻¹ CO₂ flow difference (obtained from the linear regression curve)

 Table 1
 Characteristics of the different prepacks

Brand name	Distributor	Primary absorbent	NaOH content (vol%)	Net weight (g) of lot used for part I 821 (7)	
Amsorb Plus	Armstrong Medical	Ca(OH) ₂	0		
LoFloSorb	Intersurgical	Ca(OH) ₂	0	915 (12)	
Medisorb EF	GE	Ca(OH) ₂	<2.5	721 (4	
Medisorb	GE	Ca(OH) ₂	2.5	796 (6)	
Spherasorb	Intersurgical	Ca(OH) ₂	2.5	1057 (14)	
LithoLyme	Allied Healthcare	Ca(OH) ₂	0 (*)	1010 (17)	
SpiraLith	Micropore	LiOH	0	569 (10)	

Net refers to the weight of fresh product contained in the canister of the canisters tested in Part I of the study, all belonging to the same lot. The weight is expressed as average (SD)

(*) Uses LiCl as a catalyst

line pressure that corresponded to a CO_2 inflow of 160 mL min⁻¹ (derived from the calibration procedure described above). After the canister was inserted, inspired and expired CO_2 concentrations as well as line pressure were downloaded every 2 min into a *spreadsheet*. The

canister was left in place until the inspired CO_2 fraction (F_ICO₂) had reached at least 1.0 %.

Canister life was expressed as the time (in hours) from canister insertion until F_1CO_2 had reached 0.1 % F_1CO_2 and each additional 0.1 % increment up to 1.0 % (Fig. 2).



Fig. 2 Expressing canister performance as fractional canister usage (FCU). Canister life was expressed as the time (in hours) from canister insertion until F_1CO_2 had reached 0.1 % F_1CO_2 and each additional 0.1 % increment up to 1.0 %. The upper left and right graph describe the F_1CO_2 course (*thick gray line*) with a 0.35 and 3 L min⁻¹ FGF, respectively. The 0.1, 0.5, and 1.0 % thresholds are

represented by the blue, black, and orange line, respectively. In the blue shaded box, canister life for each F_1CO_2 threshold is converted into fractional canister usage (FCU) as 100/hours till reaching threshold. The FCU values for the different FGF are then plotted, and a linear regression is applied to those values pertaining to one specific F_1CO_2 threshold

	0.1	0.2	0.3	0.4	0.5	0.6	0.7	0.8	0.9	1
Inspired CO ₂ %	% at whic	h canister	r is being	replaced	(F _I CO ₂ t	hreshold))			
Slope										
Amsorb Plus	-3.18	-2.44	-2.12	-1.96	-1.85	-1.78	-1.70	-1.65	-1.61	-1.58
Medisorb EF	-2.47	-2.29	-2.17	-2.08	-2.01	-1.94	-1.93	-1.85	-1.81	-1.78
LithoLyme	-1.51	-1.38	-1.30	-1.26	-1.22	-1.18	-1.16	-1.13	-1.11	-1.10
LoFloSorb	-2.57	-2.23	-1.99	-1.87	-1.78	-1.70	-1.63	-1.57	-1.54	-1.51
Medisorb	-2.22	-1.95	-1.81	-1.72	-1.65	-1.59	-1.54	-1.50	-1.46	-1.43
Spherasorb	-1.87	-1.64	-1.49	-1.40	-1.33	-1.27	-1.24	-1.21	-1.18	-1.17
SpiraLith	-1.24	-1.22	-1.20	-1.19	-1.18	-1.18	-1.17	-1.17	-1.16	-1.16
Y-intercept										
Amsorb Plus	15.91	12.21	10.58	9.78	9.25	8.88	8.52	8.25	8.05	7.89
Medisorb EF	12.36	11.45	10.83	10.39	10.05	9.71	9.64	9.25	9.04	8.89
LithoLyme	7.57	6.90	6.52	6.31	6.10	5.91	5.78	5.66	5.57	5.52
LoFloSorb	12.86	11.12	9.93	9.37	8.89	8.51	8.16	7.83	7.69	7.53
Medisorb	11.11	9.76	9.07	8.59	8.23	7.93	7.69	7.50	7.32	7.16
Spherasorb	9.34	8.22	7.45	7.01	6.65	6.37	6.19	6.03	5.89	5.82
SpiraLith	6.20	6.09	6.01	5.97	5.91	5.88	5.85	5.83	5.80	5.78

The fraction of a canister (%) used per hour (FCU) with a certain fresh gas flow (FGF, in L min⁻¹) is calculated as: $FCU = slope \times FGF + Y$ -intercept. Note these values apply to the constraints defined in the Methods section. The same lot was used for each brand

Table 2	Canister	life an	d
fractional	canister	usage	(FCU)

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Fig. 3 Canister life (in hours, *left panes* **a**, **b**) and fractional canister usage (FCU, *right panes* \mathbf{c} , \mathbf{d}) of the different prepacks for an F₁CO₂ threshold of 0.1 % (upper panes **a**, **c**) and 0.5 % (lower panes **b**, **d**), respectively. Lines on the left panes are added for clarity, lines in the right panes are based on the fitting parameters from Table 2. Color

code: Amsorb Plus = blue triangle, Spherasorb = red circle, LoFlo-Sorb = white circle/connecting black line, Medisorb = yellow diamond, Medisorb $EF = grey \ square$, LithoLyme = purple diamond, and SpiraLith = green circle

We will further refer to these 0.1 % increments as " F_1CO_2 thresholds" because they refer to the F_ICO₂ concentration at which the anesthesia providers replace the canister.

The inverse of canister life, 1/(canister life in hours until a certain F_ICO₂ threshold was reached), was defined as "fractional canister usage" (FCU), the fraction of the canister that is used in 1 h. A certain FCU pertains to the combination of 1 specific F_1CO_2 threshold, canister brand, and FGF. The FCU with the 0.1, 0.2 ..., 1.0 % threshold to replace the canister is abbreviated as $FCU_{0,1}$ $FCU_{0,2}$,..., $FCU_{1,0}$, respectively. For example, $FCU_{0,1}$ represents the fraction of the canister that is used in 1 h in the clinical situation where the canister is replaced once the F_ICO₂ rises to 0.1 %. The higher the F_1CO_2 threshold, the longer the canister life and thus the smaller the FCU will be. FCU can be presented as a fraction (0-1) or a percentage

(0-100 %). For example, a canister with a FCU_{0.5} of 0.125 or 12.5 % at 1 L min⁻¹ FGF means that when the canister is used with the Aisys with a 5 $L.min^{-1}$ ventilation, a CO₂ inflow of 160 mL min⁻¹, and a 1 L.min⁻¹ FGF, 1/8 of the canister will be used per hour (or the canister will last 8 h) when it is replaced once $F_1CO_2 = 0.5$ %.

Because visual inspection revealed the FGF-FCU relationship for each F₁CO₂ threshold to be linear, a linear curve fit was applied to the FGF-FCU data (Fig. 2). The intersection with the X-axis (=FGF) was forced through 5 L.min⁻¹ because there is no rebreathing and thus no CO₂ being absorbed (FCU = 0) when FGF is equal or higher than minute ventilation (5 $L.min^{-1}$). Note that because the FGF-FCU fit was forced through 5 L.min⁻¹, the slope and the Y-axis intercept of the linear fit provide the same information.

The relative performance of the different type of canisters for each F_1CO_2 threshold was determined by dividing the slope of a particular brand by that of the respective slope intercept of the most efficient canister (note: use of the Y-axis intercept would have given exactly the same results). The canister that was most efficient for an F_1CO_2 threshold of 0.5 % was arbitrarily assigned the value "100 %".

2.2 Part II: intra-lot and inter-lot canister life variability (0.35 L min⁻¹ FGF)

The canisters used to define the FGF-FCU relationship of the individual brands all had an identical lot number. To examine whether the results are more widely applicable, we tested intra-lot and inter-lot variability in two different lots. For each brand, intra-lot and inter-lot FCU variability was tested with an extra 12 canisters (6 each of a different lot) with a 350 mL min⁻¹ FGF. Initial fresh absorbent content, CO2 inflow, and FCU for a 0.5 % F_ICO2 threshold between the 2 lots were compared with a t test, with p < 0.05 denoting a statistically significant difference. Intra-lot variability was assessed with the coefficient of variation (standard deviation/mean, expressed in %). We also compared the different brands by combining the data of the 12 canisters of the 2 lots with regard to initial fresh absorbent content, CO₂ inflow, and FCU for a 0.5 % F_ICO₂ using ANOVA, with p < 0.05 denoting statistical significance, followed by pairwise comparisons with the Holm-Sidak method.

To present intra-lot and inter-lot canister life variability in an intuitive, visual manner, we also plot the results with time (hours) time to 0.1 % on the X-axis, and rise time from 0.1 to 0.5 % on the Y-axis because the absolute and relative contribution of canister life until F_1CO_2 reaches 0.5 % differs among the brands of canisters. If 0.5 % F_{I-} CO_2 is used as the canister replacement threshold (see discussion), total canister life will be the sum of the time till F_1CO_2 reaches 0.1 % plus the time it will take for F_{I-} CO_2 to rise from 0.1 to 0.5 %.

The relative performance of the different type of canisters for each F_1CO_2 threshold was determined by dividing canister life of the type of canister under consideration by that of the canister that was most efficient for an F_1CO_2 threshold of 0.5 %, and expressed as %.

2.3 Part III: canister efficiency on a per product weight basis with a $0.35 \text{ Lmin}^{-1} \text{ FGF}$

To compare the efficiency of the canisters on a per product weight basis, canister life was normalized to fresh granule content by calculating how long 100 g of product lasts with each F_1CO_2 threshold. Both absolute canister life (min/100 g of fresh CO_2 absorbent) and relative canister life (relative to that of the most efficient canister, which was assigned the value of 100 %) are presented for F_1CO_2 thresholds ranging from 0.1 to 1.0 %. These data were calculated separately for the data for part I and II. For the data from part I, canister life for the 0.35 L min⁻¹ is derived from the fitted parameters of the FCU fit (see part I). The canister data of part

Table 3 Relative canisterefficiency for each F_1CO_2 threshold for canisters tested inpart I (upper pane) and part II(lower pane)

	0.1	0.2	0.3	0.4	0.5	0.6	0.7	0.8	0.9	1
F _I CO ₂ threshold	d (%)									
Part I										
Medisorb EF	50	53	56	57	59	61	61	63	64	65
Amsorb Plus	39	50	57	61	64	66	69	71	72	73
LoFloSorb	48	55	61	64	66	69	72	74	75	77
Medisorb	56	62	66	69	72	74	76	78	79	81
Spherasorb	66	74	81	85	89	92	95	97	98	99
LithoLyme	82	88	92	95	97	99	101	103	104	105
SpiraLith	100	100	100	100	100	100	100	100	100	100
Part II										
Medisorb EF	43	46	49	51	53	54	55	57	57	58
Amsorb Plus	34	43	48	52	55	58	60	61	63	65
LoFloSorb	50	57	61	65	68	70	72	74	75	77
Medisorb	69	73	75	77	79	80	82	83	83	84
Spherasorb	64	70	76	80	83	86	88	90	91	92
LithoLyme	68	75	79	82	84	87	89	90	91	93
SpiraLith	100	100	100	100	100	100	100	100	100	100

The SpiraLith has been arbitrarily assigned the value "100 %". See text for details

II for the different brands were compared using ANOVA, with p < 0.05 denoting statistical significance, followed by pairwise comparisons with the Holm-Sidak method.

3 Results

In part I, average CO_2 flow did not differ between any of the tests of the different canister brands. Canister life and FCU are presented in Table 2. While canister life (expressed in hours until a certain threshold was reached) increased with FGF in a non-linear manner (Fig. 3a,c), FCU decreased linearly with FGF (Fig. 3b, d). The relative position of the FCU–FGF curves of the different brands depends on the F₁CO₂ threshold. The efficiency relative to the most efficient canister for each F₁CO₂ threshold is presented in Table 3 (upper pane).

The results of part II, intra- and inter-lot variability, are presented in Table 4 and Fig. 4. Average CO_2 flow did statistically differ between lots for the Medisorb and Amsorb Plus, but this constitutes <2.5 % from the target 160 mL min⁻¹ FGF.

Also in part II, canister life (for a $0.5 \ \% F_1CO_2$ replacement threshold) was found to differ significantly between the

different brands, except between Amsorb Plus and Medisorb EF, and between LithoLyme, Spherasorb, and Medisorb (Table 5). The amount of fresh CO_2 absorbent differed between all brands, but CO_2 flow did not (Table 5).

The efficiency relative to the most efficient canister for each F_1CO_2 threshold is presented in Table 3 (lower pane).

In part III, canister life per 100 g fresh granule content was found to be almost twice as long when LiOH is used as the primary absorbent instead of $Ca(OH)_2$, a consistent finding in canisters tested in part I and II (Table 6).

4 Discussion

Meaningful comparisons between different CO_2 absorbents require that the conditions in which they are being tested are standardized and represent real-life conditions. By standardizing the experimental set-up, we attempted to eliminate the variability of CO_2 production, degree of rebreathing, and rebreathing pattern (anesthesia machine configuration).

The relationship between FGF and canister life (hours) is curvilinear (Fig. 3). While absolute canister life may be

Table 4 Inter-lot variability of amount of fresh CO₂ absorbent, CO₂ flow, and FCU_{0.5}, and intra-lot variability of FCU_{0.5}

	Net amount of absorbent		CO ₂ load		Canisterlife		
	Weight (g)	Inter-lot variability significant? (p value)	CO ₂ flow mL min ⁻¹	Inter-lot variability significant? (p value)	FCU _{0.5} (%)	Inter-lot variability significant? (p value)	Intra-lot variability coeff var
Medisor	b						
Lot 1	801 (4)	0.00	163 (1)	0.04	6.51 (0.26)	0.47	4.0
Lot 2	831 (14)		161 (3)		7.01 (1.37)		19.5
Spheras	orb						
Lot 1	1057 (7)	0.09	160 (3)	0.70	6.45 (0.44)	0.95	6.8
Lot 2	1052 (3)		159 (3)		6.44 (0.25)		3.9
Medisor	b EF						
Lot 1	723 (6)	0.00	165 (1)	0.09	9.86 (0.31)	0.11	3.1
Lot 2	699 (5)		161 (4)		10.5 (0.58)		5.5
LoFloSc	orb						
Lot 1	916 (6)	0.00	164 (5)	0.14	7.64 (0.58)	0.34	7.6
Lot 2	933 (2)		159 (2)		8.12 (0.54)		6.7
Amsorb	Plus						
Lot 1	808 (12)	0.00	164 (3)	0.01	10.03 (0.87)	0.53	8.7
Lot 2	751 (4)		156 (2)		9.43 (0.93)		9.9
LithoLy	ne						
Lot 1	1000 (12)	0.81	162 (3)	0.46	6.94 (0.43)	0.00	6.2
Lot 2	1003 (27)		161 (3)		5.72 (0.4)		0.7
SpiraLit	h						
Lot 1	564 (6)	0.00	159 (2)	0.16	5.69 (0.13)	0.00	2.3
Lot 2	594 (4)		161 (3)		4.99 (0.12)		2.4

 $FCU_{0.5}$ = fractional canister usage when 0.5 % is used as the canister replacement threshold. Results are presented as mean (standard deviation)

more intuitive to use, the use of FCU has the advantage to have a linear relationship with FGF (Fig. 3). This facilitates comparisons among canisters as well as cost. Note



Fig. 4 Relationship between time until start of canister exhaustion $(F_1CO_2 = 0.1 \%)$ and rate of rise of F_1CO_2 from 0.1 to 0.5 %. Small symbols denote individual canister data, with two different symbols denoting different lots of the same brand, with "#1" = first lot and "#2" = second lot. Large symbols denote average values of the two lots, with "Total av 1 + 2" denoting the average of all canisters of both lots. Color code: AS = Amsorb Plus, *blue triangle*; SS = Spherasorb, *red circle*; LFS = LoFloSorb, *white circle/connecting black line*; MS = Medisorb, *yellow diamond*; EF = Medisorb EF, *grey square*; LL = LithoLyme, *purple diamond*; and SL = SpiraLith = *green circle*

this linear relationship may not hold for other anesthesia machines because the properties of the circle breathing system and the manner in which gases are handled during the different phases of the respiratory cycle will affect this relationship [9]. This is corroborated by preliminary data comparing canister life of prepacks of different brands with the Aisys, the Zeus, and the FLOW-i (Maquet, Solna, Sweden). Therefore, our data for prepacks fitting on the Aisys should not be extrapolated to those fitting onto other anesthesia machines. In addition, the absolute and relative weight of fresh absorbent is different for canisters that fit onto different machines.

Because the anesthesia machine, ventilation, and CO_2 inflow were the same for all the tests, differences in canister life were only determined by the chemical composition of the CO_2 absorbent, F_1CO_2 replacement threshold, and properties of the canister content. The latter include but are not limited to—the weight of fresh CO_2 absorbent, granular size and shape, canister shape, and void space. Let us consider some of these.

The effect of chemical composition was assessed by plotting total canister life of the different brands per 100 g of fresh canister content versus the F_1CO_2 . CO_2 absorption capacity on a weight basis was higher with LiOH than with $Ca(OH)_2$ as the primary absorbent. Within the $Ca(OH)_2$ canister group, the presence of a catalyst (NaOH or LiCl)

	Net amount of absorbent	CO ₂ load	Canister life
	Weight (g)	CO_2 flow (mL min ⁻¹)	FCU _{0.5} (%)
Medisorb			
Lot $1 + 2$	816 (18)	162 (2)	6.76 (0.97)
Spherasorb			
Lot $1 + 2$	1055 (6)	160 (3)	6.44 (0.34)
Medisorb EF			
Lot $1 + 2$	712 (13)	163 (4)	10.15 (0.54)
LoFloSorb			
Lot $1 + 2$	924 (10)	161 (4)	7.88 (0.59)
Amsorb Plus			
Lot $1 + 2$	777 (31)	159 (5)	9.70 (0.91)
LithoLyme			
Lot $1 + 2$	1002 (20)	161 (3)	6.33 (0.75)
SpiraLith			
Lot $1 + 2$	579 (16)	160 (3)	5.34 (0.39)
Differences between brands?	p < 0.001	0.074	p < 0.001
Which brands differ?	All differ from one another		All differ from one another EXCEPT
			(1) Medisorb = Spherasorb = LithoLyme
			(2) $Amsorb = Medisorb EF$

Table 5 Performance of different brands of prepacks tested in Part II (six canisters of two different lots each, tested with a 350 mL min⁻¹ FGF)

 $FCU_{0.5}$ = fractional canister usage when 0.5 % is used as the canister replacement threshold. Results are presented as mean (standard deviation). See text for details

Table 6Absolute and relativecanister life per 100 g freshgranule content (for $F_1CO_2 = 0.5$ %) for thedifferent brands with a350 mL min⁻¹ fresh gas flow

	Part I		Part II		
	Absolute min/100 g	Relative (%)	Absolute min/100 g	% Relative	
Amsorb Plus	85	44	81	41	
LoFloSorb	79	41	83	42	
Medisorb EF	89	46	83	43	
Spherasorb	92	48	89	45	
LithoLyme	105	55	96	49	
Medisorb	98	51	111	57	
SpiraLith	192	100	195	100	

Both absolute canister life (min/100 g of fresh CO_2 absorbent) and relative canister life (relative to that of the SpiraLith, which was assigned the value of 100 %) are presented for an F_ICO_2 threshold of 0.5 % and a 350 mL min⁻¹ fresh gas flow. These data were calculated separately for the data for part I and II. See text for details

increased canister life for the lower F_1CO_2 thresholds, an effect that faded if a higher F_1CO_2 replacement threshold was accepted. Because the prepacks of the different brands contain different amounts of CO_2 absorbent, differences in efficiency on a per weight CO_2 absorbent basis cannot be directly translated into differences in canister life. From a clinical and economical point of view, canister life is what we are interested in if we use prepacks. Because of the many factors that affect CO_2 absorbent efficiency, care has to be taken to extrapolate the weight-based results to bulk CO_2 absorbent for refillable canisters.

Because the rate of rise of F_ICO₂ above 0.1 % differs among the prepack brands, the F_1CO_2 threshold that the clinician uses to replace the canister has a profound impact on the absolute and relative performance of the different brands. The rise is slowest with the Ca(OH)₂ based canisters that have no or little catalyst (Fig. 4), and thus most canister life can be gained by accepting a higher F_1CO_2 threshold with these absorbents (Fig. 4). On the contrary, less is gained by waiting for F₁CO₂ to reach 0.5 % before replacing a SpiraLith canister. The F_ICO₂ can be allowed to rise until it affects the end-expired CO₂ concentration (F_ACO_2) of the patient up to a point where it becomes clinically unacceptable: FACO2 is the physiologically important variable for the patient, not F₁CO₂. According to the alveolar gas equation, the effect of F_ACO_2 on F_ICO_2 is additive, $F_ACO_2 = F_ICO_2 + (VCO_2/alveolar ventilation)$. In most of our patients, the F_ACO_2 (35 mmHg or 4.5 %) can be allowed to increase by 4 mmHg or 0.5 % without causing any harm. Therefore, the F_ICO₂ can be allowed to rise to 4 mmHg or 0.5 % in most of our patients.

The use of "fractional canister usage" allows canister costs to be calculated by multiplying the FCU (expressed in fraction) with the cost of 1 canister, and this for any FGF. While the exact conditions in real life do differ from the in vitro conditions of this study, the ratios of the product of FCU and the cost of 1 canister of the different brands can be used to make fair cost comparisons among canisters.

The canisters used to define the FGF-FCU relationship all had an identical lot number. Are these results applicable to other lot numbers? Inter-lot differences were only statistically significant for the 2 longest lasting canisters, SpiraLith and LithoLyme-12 and 18 % respectively. Intra-lot variability was small, with the notable exception of the Medisorb canister. SpiraLith canisters have both the steepest F_1CO_2 rise and the least intra-lot variability, a consistency we hypothesize is due to the preformed channels that leave little room for the more random channeling that is likely to occur with canisters containing the Ca(OH)₂ granules. If the results of the 2 lots are combined, the different prepacks can be ranked according their efficiency (least to most efficient) as follows: Amsorb Plus = Medisorb EF < LoFloSorb < Medisorb = Spherasorb = LithoLyme < SpiraLith (all for an F_1CO_2 threshold = 0.5 %).

The use of a consistent, replicable model allows canisters to be compared and allows for external verification. Still, real life conditions may differ from in vitro conditions: CO_2 loads in real life vary, both in time and quantity. No canister is used for more than 24 h straight. It is unclear how-and whether-changing FGFs and CO₂ loading conditions with prolonged periods of non-use (at night, during the weekends) affect canister performance, both absolute and relative, from one brand to another. In addition, O₂ was not removed from the system, while in real life patients do remove O₂. Therefore, in real life, the degree of rebreathing might be slightly different from that in the experimental setup. However, the effect on canister life is likely to be very small, and certainly will not affect relative canister life. Ongoing clinical studies will help address the issues raised in this paragraph.

To summarize, canister life of CO_2 absorber prepacks were determined over a wide range of FGFs with the Aisys[®] (GE, Helsinki, Finland) under identical CO_2 load conditions. The most important factors that determine canister life of prepacks in a circle breathing system are the chemical composition of the canister, the absolute absorbent content of the canister, and the F_1CO_2 replacement threshold. The use of the fractional canister usage allows for cost comparisons among different prepacks. Results should not be extrapolated to prepacks that fit onto other anesthesia machines.

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Conflict of interest The authors declare that they have no conflict of interest.

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