ORIGINAL RESEARCH



# In vitro performance of prefilled  $CO_2$  absorbers with the Aisys®

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Abstract Low flow anesthesia increases the use of  $CO<sub>2</sub>$ absorbents, but independent data that compare canister life of the newest  $CO<sub>2</sub>$  absorbents are scarce. Seven different pre-packed  $CO<sub>2</sub>$  canisters were tested in vitro: Amsorb Plus, Spherasorb, LoFloSorb, Medisorb, Medisorb EF, LithoLyme, and SpiraLith.  $CO_2$  (160 mL min<sup>-1</sup>) flowed into the tip of a 2 L breathing bag that was ventilated with a tidal volume of 500 mL, a respiratory rate of 10/min, and an I:E ratio of 1:1 using the controlled mechanical ventilation mode of the Aisys® (GE, Madison, WI, USA). In part I, canister life of each brand (all of the same lot) was tested with 12 different fresh gas flows (FGF) ranging from  $0.25$  to  $4$  L min<sup>-1</sup>. In part II, canister life of six canisters each of two different lots of each brand were tested with a  $350$  mL min<sup>-1</sup> FGF. Canister life is presented as "FCU", fractional canister usage, the fraction of a canister used per hour, and is defined for the inspired  $CO<sub>2</sub>$  concentration  $(F<sub>I</sub>CO<sub>2</sub>)$  that denotes exhaustion. In part III, canister life per 100 g fresh granule content was calculated. FCU decreased linearly with increasing FGF. The relative position of the FCU–FGF curves of the different brands depends on the  $F_1CO_2$  threshold because the exhaustion rate (the rate of

 $\boxtimes$  Jan F. A. Hendrickx jcnwahendrickx@yahoo.com rise once  $F_1CO_2$  starts to increase) differs among the brands. Intra-lot variability was 18 % or less. The different prepacks can be ranked according their efficiency (least to most efficient) as follows: Amsorb Plus = Medisorb  $EF <$  LoFloSorb  $\lt$  Medisorb = Spherasorb = LithoLyme $\lt$ SpiraLith (all for an  $F_{I}CO_{2}$  threshold = 0.5 %). Canister life per 100 g fresh granule content is almost twice as long when LiOH is used as the primary absorbent. The most important factors that determine canister life of prepacks in a circle breathing system are the chemical composition of the canister, the absolute amount of absorbent present in the canister, and the  $F_1CO_2$  replacement threshold. The use of the fractional canister usage allows cost comparisons among different prepacks. Results should not be extrapolated to prepacks that fit onto other anesthesia machines.

**Keywords**  $CO<sub>2</sub>$  absorbers  $\cdot$  Low flow anesthesia  $\cdot$ Anesthesia machine

#### 1 Introduction

Conventional low flow anesthesia is increasingly used to decrease waste and thus cost of and pollution by anesthetic agents. In addition, already three anesthesia machines use automated low flow, target controlled agent and carrier gas delivery with minimal user intervention, making anesthesia with fresh gas flows (FGFs) well below 1  $L.min^{-1}$  the routine rather than the exception: the  $Aisys^{\omega}$  (GE, Madison, WI, USA) and FLOW-i (Maquet, Solna, Sweden) use a maintenance FGF of 500 and 300 mL  $min^{-1}$ , respectively, and the Zeus (Draeger, Lubeck, Germany) is fully closed. These low FGFs will increase  $CO<sub>2</sub>$  absorbent usage though, because more  $CO<sub>2</sub>$  will pass through them. The composition of the newest  $CO<sub>2</sub>$  absorbents has changed (e.g., KOH

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has been eliminated to reduce anesthetic degradation), and the canister life of these absorbents has been incompletely studied and compared. This paucity of data is reflected in the small number of references quoted in this manuscript [\[1](#page-9-0)].

The aim of this study was to determine canister life of prefilled, disposable canisters (''prepacks'') over a wide range of FGFs with the  $Aisys^{\circledR}$  under conditions that resemble in vivo conditions. Prepacks have a low volume to shorten the circle system's time constant, can be easily replaced without opening the circle system, and may ensure a more consistent humidity in the circle system [[2\]](#page-9-0). Prepacks with different chemical composition of different manufacturers readily available to the authors were studied under standardized conditions with the same anesthesia machine, with FGF ranging from  $0.25$  to  $5$  L.min<sup>-1</sup>. We examined the effect of canister brand, fresh gas flow (FGF), and  $F<sub>I</sub>CO<sub>2</sub>$  replacement threshold on canister life. In addition, we examined intra- and inter-lot variability. This study does not address the effects of granular size and shape, canister shape, void space and other factors that affect canister performance.

#### 2 Materials and methods

The patient's  $CO_2$  production (VCO<sub>2</sub>) was simulated by flowing  $CO<sub>2</sub>$  into the tip of a 2 L breathing bag that was attached to the Y-piece of a circle breathing system (Fig. [1](#page-2-0)). The breathing bag was ventilated with a tidal volume of 500 mL, a respiratory rate of 10/min, and an I:E ratio of 1:1 using the controlled mechanical ventilation mode of the Aisys® (GE, Madison, WI, USA). We used a  $CO<sub>2</sub>$  inflow of 160 mL min<sup>-1</sup>: endogenous  $CO<sub>2</sub>$  production during general anesthesia in adults is approximately 130 mL min<sup>-1</sup> [[3,](#page-9-0) [4\]](#page-9-0), and applying a  $CO<sub>2</sub>$  pneumoperitoneum increases alveolar  $CO<sub>2</sub>$  washout by approximately 30 mL min<sup>-1</sup> [\[5–7](#page-9-0)]. With a minute ventilation of 5 L.min<sup>-1</sup>, the in vitro end-expired  $CO<sub>2</sub>$  was approximately 4.5 %, resembling in vivo conditions. We avoided the use of higher  $CO<sub>2</sub>$  flows, so-called "accelerated'' testing because they cause higher temperature gradients within the canister, which may cause decreased  $CO<sub>2</sub>$ absorption by the formation of water deposits on the granules due to cooling by the colder temperature of the operating room [[8\]](#page-9-0).

A  $CO<sub>2</sub>$  flow rotameter (MEDEC<sup>®</sup>, Aalst, Belgium) was plugged into the  $CO<sub>2</sub>$  wall outlet of the operating room. Because the resolution of the flow meter  $(50 \text{ mL min}^{-1})$ was inadequate for the purpose of the study,  $CO<sub>2</sub>$  flow was derived from the line pressure in the line distal to the flow meter (Fig. [1](#page-2-0)). Four resistors between the  $CO<sub>2</sub>$  rotameter and the tip of the balloon attenuated the backpressure of

ventilation on the  $CO<sub>2</sub>$  flow. A pressure—flow calibration curve was constructed by dialing at least six different (arbitrary) rotameter settings, recording the corresponding line pressure, and measuring the corresponding  $CO<sub>2</sub>$  flow volumetrically. The line pressure was measured between the second and third resistor (Pressure Monitoring Set, Edwards Lifesciences<sup>TM</sup>, Irvine, CA); the corresponding  $CO<sub>2</sub>$  flow was measured volumetrically by measuring the time to fill a 250 mL glass syringe (Popper and Sons, Inc. New Hyde Park, NY, USA) after switching a three way stopcock placed between the last resistor and the tip of the balloon. The calibration procedure was repeated before testing each new canister. A 1 mm Hg pressure difference corresponded to a 3.4 mL min<sup>-1</sup> CO<sub>2</sub> flow difference (obtained from the linear regression curve).

The  $CO<sub>2</sub>$  flows used to test the different canisters were compared using ANOVA (followed by the Holm-Sidak to test for intergroup differences) to make sure that minor differences in  $CO<sub>2</sub>$  inflow could be ruled out as a factor contributing to any possible differences in canister life of the different prepacks.

Inspired and expired gases were sampled and analyzed by a M-CAiOV module (GE, Madison, WI), which was calibrated according to the manufacturer's specifications. Before each experiment, we ensured the  $CO<sub>2</sub>$  waveform had a consistent morphology, without any oscillations or other artifact. To eliminate artifacts on the capnogram from gas entrainment from the inspiratory limb of the breathing system during the expiratory phase, two heat and moisture exchangers (Ref 352/5877, Covidien™, Mansfield, MA) were placed in between the bag and the Y-piece. The gas was sampled from the filter closest to the breathing bag; sampled gases were redirected to the circuit via a connector between the expiratory limb and its connection to the Aisys $^{\circledR}$ .

# 2.1 Part I: canister life across a  $0.25-4.0$  L min<sup>-1</sup> FGF range with the same lot

The characteristics of the different prepacks that were tested can be found in Table [1.](#page-2-0) Twelve canisters of the same lot of each brand were tested with one of the 12 following O<sub>2</sub>/air fresh gas flows  $(L.min^{-1})$ : 0.25; 0.3; 0.35; 0.5; 0.65; 0.75; 1.0; 1.2; 1.5; 2.0; 3.0; and 4.0. The delivered  $O_2$  concentration was 55 %, except in those instances where the hypoxic guard imposed the delivery of higher  $O_2$ concentrations. The weight of fresh  $CO<sub>2</sub>$  absorbent was obtained by subtracting the weight of the plastic encasement from the initial total weight using a high precision weighing scale (XP10002, Mettler-Toledo, Columbus, Ohio).

Prior to inserting each canister into the breathing system, the  $CO<sub>2</sub>$  rotameter dial was adjusted to obtain a stable

<span id="page-2-0"></span>

 $\frac{1}{2}$  for  $\frac{1}{2}$  flow meter for CO2 flowmeter

Fig. 1 In vitro set-up. A 160 mL min<sup>-1</sup> CO<sub>2</sub> flow enters the tip of a 2 L breathing bag that is attached to the Y-piece of a circle breathing system. The bag is ventilated with a tidal volume of 500 mL, a respiratory rate of 10/min, and an I:E ratio of 1:1 using the controlled mechanical ventilation mode of the Aisys® (GE, Madison, WI, USA). Gases sampled by the gas analyzer (approximately  $200$  mL  $min^{-1}$ ) are redirected towards the expiratory limb of the circle breathing system. The experiment continues until the  $FICO<sub>2</sub>$  has reached at least 1.0 % (see text and Fig. [2](#page-3-0) for details).  $CO<sub>2</sub>$  from the wall outlet is titrated via a rotameter towards a line pressure distal to the flow meter that corresponds with a  $160 \text{ mL min}^{-1}$   $CO<sub>2</sub>$  flow. Four resistors between the  $CO<sub>2</sub>$  rotameter and the tip of the balloon attenuated the backpressure of ventilation on the  $CO<sub>2</sub>$  flow. A pressure-flow

calibration curve is constructed by dialing at least 6 different (arbitrary) rotameter settings, recording the corresponding line pressure, and measuring the corresponding  $CO<sub>2</sub>$  flow volumetrically. The line pressure was measured between the second and third resistor (Pressure Monitoring Set, Edwards Lifesciences<sup>TM</sup>, Irvine, CA); the corresponding  $CO<sub>2</sub>$  flow was measured volumetrically by measuring the time to fill a 250 mL glass syringe (Popper and Sons, Inc. New Hyde Park, NY, USA) after switching a three way stopcock placed between the last resistor and the tip of the balloon. The calibration procedure was repeated before testing each new canister. A 1 mm Hg pressure difference corresponded to a  $3.4 \text{ mL min}^{-1}$  CO<sub>2</sub> flow difference (obtained from the linear regression curve)

Table 1 Characteristics of the different prepacks

Brand name	Distributor	Primary absorbent	NaOH content $(vol\%)$	Net weight $(g)$ of lot used for part I
Amsorb Plus	Armstrong Medical	$Ca(OH)_{2}$	0	821 (7)
LoFloSorb	Intersurgical	$Ca(OH)_{2}$	0	915 (12)
Medisorb EF	GЕ	$Ca(OH)_{2}$	< 2.5	721 (4)
Medisorb	GЕ	$Ca(OH)_{2}$	2.5	796 (6)
Spherasorb	Intersurgical	$Ca(OH)_{2}$	2.5	1057(14)
LithoLyme	Allied Healthcare	$Ca(OH)_{2}$	$0(*)$	1010(17)
SpiraLith	Micropore	LiOH	0	569 (10)

Net refers to the weight of fresh product contained in the canister of the canisters tested in Part I of the study, all belonging to the same lot. The weight is expressed as average (SD)

(\*) Uses LiCl as a catalyst

line pressure that corresponded to a  $CO<sub>2</sub>$  inflow of 160 mL  $min^{-1}$  (derived from the calibration procedure described above). After the canister was inserted, inspired and expired  $CO<sub>2</sub>$  concentrations as well as line pressure were downloaded every 2 min into a spreadsheet. The canister was left in place until the inspired  $CO<sub>2</sub>$  fraction  $(F<sub>I</sub>CO<sub>2</sub>)$  had reached at least 1.0 %.

Canister life was expressed as the time (in hours) from canister insertion until  $F_{I}CO_{2}$  had reached 0.1 %  $F_{I}CO_{2}$ and each additional 0.1 % increment up to 1.0 % (Fig. [2](#page-3-0)).

<span id="page-3-0"></span>

Fig. 2 Expressing canister performance as fractional canister usage (FCU). Canister life was expressed as the time (in hours) from canister insertion until  $F_1CO_2$  had reached 0.1 %  $F_1CO_2$  and each additional 0.1 % increment up to 1.0 %. The upper left and right graph describe the  $F_1CO_2$  course (thick gray line) with a 0.35 and  $3$  L min<sup>-1</sup> FGF, respectively. The 0.1, 0.5, and 1.0 % thresholds are

represented by the blue, black, and orange line, respectively. In the blue shaded box, canister life for each  $F_1CO_2$  threshold is converted into fractional canister usage (FCU) as 100/hours till reaching threshold. The FCU values for the different FGF are then plotted, and a linear regression is applied to those values pertaining to one specific FICO2 threshold

	0.1	0.2	0.3	0.4	0.5	0.6	0.7	0.8	0.9	1
	Inspired $CO_2$ % at which canister is being replaced ( $F_1CO_2$ threshold)									
Slope										
Amsorb Plus	$-3.18$	$-2.44$	$-2.12$	$-1.96$	$-1.85$	$-1.78$	$-1.70$	$-1.65$	$-1.61$	$-1.58$
Medisorb EF	$-2.47$	$-2.29$	$-2.17$	$-2.08$	$-2.01$	$-1.94$	$-1.93$	$-1.85$	$-1.81$	$-1.78$
LithoLyme	$-1.51$	$-1.38$	$-1.30$	$-1.26$	$-1.22$	$-1.18$	$-1.16$	$-1.13$	$-1.11$	$-1.10$
LoFloSorb	$-2.57$	$-2.23$	$-1.99$	$-1.87$	$-1.78$	$-1.70$	$-1.63$	$-1.57$	$-1.54$	$-1.51$
Medisorb	$-2.22$	$-1.95$	$-1.81$	$-1.72$	$-1.65$	$-1.59$	$-1.54$	$-1.50$	$-1.46$	$-1.43$
Spherasorb	$-1.87$	$-1.64$	$-1.49$	$-1.40$	$-1.33$	$-1.27$	$-1.24$	$-1.21$	$-1.18$	$-1.17$
SpiraLith	$-1.24$	$-1.22$	$-1.20$	$-1.19$	$-1.18$	$-1.18$	$-1.17$	$-1.17$	$-1.16$	$-1.16$
Y-intercept										
Amsorb Plus	15.91	12.21	10.58	9.78	9.25	8.88	8.52	8.25	8.05	7.89
Medisorb EF	12.36	11.45	10.83	10.39	10.05	9.71	9.64	9.25	9.04	8.89
LithoLyme	7.57	6.90	6.52	6.31	6.10	5.91	5.78	5.66	5.57	5.52
LoFloSorb	12.86	11.12	9.93	9.37	8.89	8.51	8.16	7.83	7.69	7.53
Medisorb	11.11	9.76	9.07	8.59	8.23	7.93	7.69	7.50	7.32	7.16
Spherasorb	9.34	8.22	7.45	7.01	6.65	6.37	6.19	6.03	5.89	5.82
SpiraLith	6.20	6.09	6.01	5.97	5.91	5.88	5.85	5.83	5.80	5.78

The fraction of a canister  $(\%)$  used per hour (FCU) with a certain fresh gas flow (FGF, in L min<sup>-1</sup>) is calculated as:  $FCU = slope \times FGF + Y\text{-intercept. Note these values apply to the constraints defined in the$ Methods section. The same lot was used for each brand

$$
x\in\mathbb{R}^n\setminus\{0\}
$$

Table 2 Canister life and fractional canister usage (FCU)

<span id="page-4-0"></span>



Fig. 3 Canister life (in hours, left panes a, b) and fractional canister usage (FCU, right panes c, d) of the different prepacks for an  $F_1CO_2$ threshold of 0.1 % (upper panes  $\bf{a}, \bf{c}$ ) and 0.5 % (lower panes  $\bf{b}, \bf{d}$ ), respectively. Lines on the left panes are added for clarity, lines in the right panes are based on the fitting parameters from Table [2.](#page-3-0) Color

code: Amsorb Plus = *blue triangle*, Spherasorb = *red circle*, LoFlo- $Sorb = white$  circle/connecting black line, Medisorb = yellow diamond, Medisorb  $EF = grey \ square$ , LithoLyme = purple diamond, and SpiraLith  $=$  green circle

We will further refer to these 0.1 % increments as  $F_{I}CO_{2}$ thresholds" because they refer to the  $F_{I}CO_{2}$  concentration at which the anesthesia providers replace the canister.

The inverse of canister life, 1/(canister life in hours until a certain  $F_{I}CO_{2}$  threshold was reached), was defined as "fractional canister usage" (FCU), the fraction of the canister that is used in 1 h. A certain FCU pertains to the combination of 1 specific  $F<sub>I</sub>CO<sub>2</sub>$  threshold, canister brand, and FGF. The FCU with the 0.1, 0.2 …,1.0 % threshold to replace the canister is abbreviated as  $FCU_{0.1}$   $FCU_{0.2}$ ,...  $FCU_{1,0}$ , respectively. For example,  $FCU_{0,1}$  represents the fraction of the canister that is used in 1 h in the clinical situation where the canister is replaced once the  $F_1CO_2$ rises to 0.1 %. The higher the  $F_{I}CO_{2}$  threshold, the longer the canister life and thus the smaller the FCU will be. FCU can be presented as a fraction  $(0-1)$  or a percentage

(0–100 %). For example, a canister with a  $FCU_{0.5}$  of 0.125 or 12.5 % at 1 L min<sup>-1</sup> FGF means that when the canister is used with the Aisys with a 5 L.min<sup>-1</sup> ventilation, a  $CO<sub>2</sub>$ inflow of 160 mL  $min^{-1}$ , and a 1 L.min<sup>-1</sup> FGF, 1/8 of the canister will be used per hour (or the canister will last 8 h) when it is replaced once  $F_{I}CO_{2} = 0.5 \%$ .

Because visual inspection revealed the FGF-FCU relationship for each  $F_1CO_2$  threshold to be linear, a linear curve fit was applied to the FGF-FCU data (Fig. [2\)](#page-3-0). The intersection with the X-axis (=FGF) was forced through 5 L.min<sup>-1</sup> because there is no rebreathing and thus no  $CO<sub>2</sub>$ being absorbed (FCU  $= 0$ ) when FGF is equal or higher than minute ventilation  $(5 L.min<sup>-1</sup>)$ . Note that because the FGF-FCU fit was forced through  $5$  L.min<sup>-1</sup>, the slope and the Y-axis intercept of the linear fit provide the same information.

<span id="page-5-0"></span>The relative performance of the different type of canisters for each  $F_{I}CO_{2}$  threshold was determined by dividing the slope of a particular brand by that of the respective slope intercept of the most efficient canister (note: use of the Y-axis intercept would have given exactly the same results). The canister that was most efficient for an  $F_{I}CO_{2}$ threshold of 0.5 % was arbitrarily assigned the value " $100\%$ ".

### 2.2 Part II: intra-lot and inter-lot canister life variability  $(0.35 \text{ L min}^{-1} \text{ FGF})$

The canisters used to define the FGF-FCU relationship of the individual brands all had an identical lot number. To examine whether the results are more widely applicable, we tested intra-lot and inter-lot variability in two different lots. For each brand, intra-lot and inter-lot FCU variability was tested with an extra 12 canisters (6 each of a different lot) with a  $350$  mL min<sup>-1</sup> FGF. Initial fresh absorbent content,  $CO_2$  inflow, and FCU for a 0.5 %  $F_1CO_2$  threshold between the 2 lots were compared with a  $t$  test, with  $p<0.05$  denoting a statistically significant difference. Intra-lot variability was assessed with the coefficient of variation (standard deviation/mean, expressed in %). We also compared the different brands by combining the data of the 12 canisters of the 2 lots with regard to initial fresh absorbent content,  $CO_2$  inflow, and FCU for a 0.5 %  $F_1CO_2$ using ANOVA, with  $p < 0.05$  denoting statistical significance, followed by pairwise comparisons with the Holm-Sidak method.

To present intra-lot and inter-lot canister life variability in an intuitive, visual manner, we also plot the results with time (hours) time to 0.1 % on the X-axis, and rise time from 0.1 to 0.5 % on the Y-axis because the absolute and relative contribution of canister life until  $F_{I}CO_{2}$  reaches 0.5 % differs among the brands of canisters. If 0.5 %  $F<sub>I</sub>$ .  $CO<sub>2</sub>$  is used as the canister replacement threshold (see discussion), total canister life will be the sum of the time till  $F<sub>I</sub>CO<sub>2</sub>$  reaches 0.1 % plus the time it will take for  $F<sub>I</sub>$ .  $CO<sub>2</sub>$  to rise from 0.1 to 0.5 %.

The relative performance of the different type of canisters for each  $F_1CO_2$  threshold was determined by dividing canister life of the type of canister under consideration by that of the canister that was most efficient for an  $F_1CO_2$ threshold of 0.5 %, and expressed as %.

# 2.3 Part III: canister efficiency on a per product weight basis with a  $0.35$  L min<sup>-1</sup> FGF

To compare the efficiency of the canisters on a per product weight basis, canister life was normalized to fresh granule content by calculating how long 100 g of product lasts with each  $F<sub>I</sub>CO<sub>2</sub>$  threshold. Both absolute canister life (min/100 g of fresh  $CO<sub>2</sub>$  absorbent) and relative canister life (relative to that of the most efficient canister, which was assigned the value of 100 %) are presented for  $F_{I}CO_{2}$  thresholds ranging from 0.1 to 1.0 %. These data were calculated separately for the data for part I and II. For the data from part I, canister life for the  $0.35$  L min<sup>-1</sup> is derived from the fitted parameters of the FCU fit (see part I). The canister data of part

Table 3 Relative canister efficiency for each  $F_1CO_2$ threshold for canisters tested in part I (upper pane) and part II (lower pane)



The SpiraLith has been arbitrarily assigned the value "100 %". See text for details

II for the different brands were compared using ANOVA, with  $p < 0.05$  denoting statistical significance, followed by pairwise comparisons with the Holm-Sidak method.

# 3 Results

In part I, average  $CO<sub>2</sub>$  flow did not differ between any of the tests of the different canister brands. Canister life and FCU are presented in Table [2.](#page-3-0) While canister life (expressed in hours until a certain threshold was reached) increased with FGF in a non-linear manner (Fig. [3a](#page-4-0),c), FCU decreased linearly with FGF (Fig. [3](#page-4-0)b, d). The relative position of the FCU–FGF curves of the different brands depends on the  $F_{I}CO_{2}$  threshold. The efficiency relative to the most efficient canister for each  $F_1CO_2$  threshold is presented in Table [3](#page-5-0) (upper pane).

The results of part II, intra- and inter-lot variability, are pre-sented in Table [4](#page-7-0) and Fig. 4. Average  $CO<sub>2</sub>$  flow did statistically differ between lots for the Medisorb and Amsorb Plus, but this constitutes  $\langle 2.5 \, \%$  from the target 160 mL min<sup>-1</sup> FGF.

Also in part II, canister life (for a 0.5 %  $F_1CO_2$  replacement threshold) was found to differ significantly between the

different brands, except between Amsorb Plus and Medisorb EF, and between LithoLyme, Spherasorb, and Medisorb (Table [5\)](#page-7-0). The amount of fresh  $CO<sub>2</sub>$  absorbent differed between all brands, but  $CO<sub>2</sub>$  flow did not (Table [5\)](#page-7-0).

The efficiency relative to the most efficient canister for each  $F_{I}CO_{2}$  threshold is presented in Table [3](#page-5-0) (lower pane).

In part III, canister life per 100 g fresh granule content was found to be almost twice as long when LiOH is used as the primary absorbent instead of  $Ca(OH)_2$ , a consistent finding in canisters tested in part I and II (Table [6\)](#page-8-0).

#### 4 Discussion

Meaningful comparisons between different  $CO<sub>2</sub>$  absorbents require that the conditions in which they are being tested are standardized and represent real-life conditions. By standardizing the experimental set-up, we attempted to eliminate the variability of  $CO<sub>2</sub>$  production, degree of rebreathing, and rebreathing pattern (anesthesia machine configuration).

The relationship between FGF and canister life (hours) is curvilinear (Fig. [3](#page-4-0)). While absolute canister life may be

**Table 4** Inter-lot variability of amount of fresh CO<sub>2</sub> absorbent, CO<sub>2</sub> flow, and FCU<sub>0.5</sub>, and intra-lot variability of FCU<sub>0.5</sub>

	Net amount of absorbent		CO <sub>2</sub> load		Canisterlife			
	Weight (g)	Inter-lot variability significant? $(p$ value)	$CO2$ flow $\rm mL\,\,min^{-1}$	Inter-lot variability significant? $(p$ value)	FCU <sub>0.5</sub> (%)	Inter-lot variability significant? $(p$ value)	Intra-lot variability coeff var	
Medisorb								
Lot $1$	801(4)	0.00	163(1)	0.04	6.51(0.26)	0.47	4.0	
Lot 2	831 (14)		161(3)		7.01(1.37)		19.5	
Spherasorb								
Lot $1$	1057(7)	0.09	160(3)	0.70	6.45(0.44)	0.95	6.8	
Lot 2	1052(3)		159(3)		6.44(0.25)		3.9	
Medisorb EF								
Lot $1$	723 (6)	0.00	165(1)	0.09	9.86(0.31)	0.11	3.1	
Lot 2	699(5)		161(4)		10.5(0.58)		5.5	
LoFloSorb								
Lot $1$	916(6)	0.00	164(5)	0.14	7.64(0.58)	0.34	7.6	
Lot $2$	933(2)		159(2)		8.12 (0.54)		6.7	
<b>Amsorb Plus</b>								
Lot $1$	808 (12)	0.00	164(3)	0.01	10.03(0.87)	0.53	8.7	
Lot 2	751 (4)		156(2)		9.43 (0.93)		9.9	
LithoLyme								
Lot $1$	1000(12)	0.81	162(3)	0.46	6.94(0.43)	0.00	6.2	
Lot 2	1003(27)		161(3)		5.72(0.4)		0.7	
SpiraLith								
Lot $1$	564(6)	0.00	159(2)	0.16	5.69(0.13)	0.00	2.3	
Lot 2	594 (4)		161(3)		4.99(0.12)		2.4	

 $FCU_{0.5}$  = fractional canister usage when 0.5 % is used as the canister replacement threshold. Results are presented as mean (standard deviation)

<span id="page-7-0"></span>more intuitive to use, the use of FCU has the advantage to have a linear relationship with FGF (Fig. [3\)](#page-4-0). This facilitates comparisons among canisters as well as cost. Note



Fig. 4 Relationship between time until start of canister exhaustion  $(F<sub>I</sub>CO<sub>2</sub> = 0.1 \%)$  and rate of rise of  $F<sub>I</sub>CO<sub>2</sub>$  from 0.1 to 0.5 %. Small symbols denote individual canister data, with two different symbols denoting different lots of the same brand, with " $#1"$  = first lot and " $#2"$  = second lot. Large symbols denote average values of the two lots, with "Total av  $1 + 2$ " denoting the average of all canisters of both lots. Color code:  $AS = \overrightarrow{A}$ msorb Plus, *blue triangle*;  $SS = Spherasorb, red circle; LFS = LoFloSorb, white circle/con$ necting black line;  $MS =$  Medisorb, yellow diamond;  $EF =$  Medisorb EF, grey square;  $LL = LithoLyme$ , purple diamond; and  $SL =$  SpiraLith = green circle

this linear relationship may not hold for other anesthesia machines because the properties of the circle breathing system and the manner in which gases are handled during the different phases of the respiratory cycle will affect this relationship [[9\]](#page-9-0). This is corroborated by preliminary data comparing canister life of prepacks of different brands with the Aisys, the Zeus, and the FLOW-i (Maquet, Solna, Sweden). Therefore, our data for prepacks fitting on the Aisys should not be extrapolated to those fitting onto other anesthesia machines. In addition, the absolute and relative weight of fresh absorbent is different for canisters that fit onto different machines.

Because the anesthesia machine, ventilation, and  $CO<sub>2</sub>$ inflow were the same for all the tests, differences in canister life were only determined by the chemical composition of the  $CO<sub>2</sub>$  absorbent,  $F<sub>I</sub>CO<sub>2</sub>$  replacement threshold, and properties of the canister content. The latter include but are not limited to—the weight of fresh  $CO<sub>2</sub>$  absorbent, granular size and shape, canister shape, and void space. Let us consider some of these.

The effect of chemical composition was assessed by plotting total canister life of the different brands per 100 g of fresh canister content versus the  $F<sub>I</sub>CO<sub>2</sub>$ . CO<sub>2</sub> absorption capacity on a weight basis was higher with LiOH than with  $Ca(OH)_2$  as the primary absorbent. Within the  $Ca(OH)_2$ canister group, the presence of a catalyst (NaOH or LiCl)

	Net amount of absorbent	CO <sub>2</sub> load	Canister life	
	Weight $(g)$	$CO2$ flow $(mL min^{-1})$	$FCU_{0.5} (\%)$	
Medisorb				
Lot $1 + 2$	816 (18)	162(2)	6.76(0.97)	
Spherasorb				
Lot $1 + 2$	1055(6)	160(3)	6.44(0.34)	
Medisorb EF				
Lot $1 + 2$	712 (13)	163(4)	10.15(0.54)	
LoFloSorb				
Lot $1 + 2$	924 (10)	161 $(4)$	7.88(0.59)	
<b>Amsorb Plus</b>				
Lot $1 + 2$	777 (31)	159(5)	9.70(0.91)	
LithoLyme				
Lot $1 + 2$	1002(20)	161(3)	6.33(0.75)	
SpiraLith				
Lot $1 + 2$	579 (16)	160(3)	5.34(0.39)	
Differences between brands?	p < 0.001	0.074	p < 0.001	
Which brands differ?	All differ from one another		All differ from one another EXCEPT	
			$(1)$ Medisorb = Spherasorb = LithoLyme	
			$(2)$ Amsorb = Medisorb EF	

Table 5 Performance of different brands of prepacks tested in Part II (six canisters of two different lots each, tested with a 350 mL min<sup>-1</sup> FGF)

 $FCU_{0.5}$  = fractional canister usage when 0.5 % is used as the canister replacement threshold. Results are presented as mean (standard deviation). See text for details

<span id="page-8-0"></span>Table 6 Absolute and relative canister life per 100 g fresh granule content (for  $F<sub>I</sub>CO<sub>2</sub> = 0.5 %$  for the different brands with a  $350$  mL min<sup>-1</sup> fresh gas flow



Both absolute canister life (min/100 g of fresh  $CO<sub>2</sub>$  absorbent) and relative canister life (relative to that of the SpiraLith, which was assigned the value of 100 %) are presented for an  $F_1CO_2$  threshold of 0.5 % and a  $350$  mL min<sup>-1</sup> fresh gas flow. These data were calculated separately for the data for part I and II. See text for details

increased canister life for the lower  $F<sub>I</sub>CO<sub>2</sub>$  thresholds, an effect that faded if a higher  $F_1CO_2$  replacement threshold was accepted. Because the prepacks of the different brands contain different amounts of  $CO<sub>2</sub>$  absorbent, differences in efficiency on a per weight  $CO<sub>2</sub>$  absorbent basis cannot be directly translated into differences in canister life. From a clinical and economical point of view, canister life is what we are interested in if we use prepacks. Because of the many factors that affect  $CO<sub>2</sub>$  absorbent efficiency, care has to be taken to extrapolate the weight-based results to bulk CO2 absorbent for refillable canisters.

Because the rate of rise of  $F_{I}CO_{2}$  above 0.1 % differs among the prepack brands, the  $F_1CO_2$  threshold that the clinician uses to replace the canister has a profound impact on the absolute and relative performance of the different brands. The rise is slowest with the  $Ca(OH)_2$  based canisters that have no or little catalyst (Fig. [4](#page-7-0)), and thus most canister life can be gained by accepting a higher  $F_{I}CO_{2}$ threshold with these absorbents (Fig. [4\)](#page-7-0). On the contrary, less is gained by waiting for  $F_1CO_2$  to reach 0.5 % before replacing a SpiraLith canister. The  $F_1CO_2$  can be allowed to rise until it affects the end-expired  $CO<sub>2</sub>$  concentration  $(F_ACO_2)$  of the patient up to a point where it becomes clinically unacceptable:  $F_ACO_2$  is the physiologically important variable for the patient, *not*  $F_1CO_2$ . According to the alveolar gas equation, the effect of  $F_ACO_2$  on  $F_ICO_2$  is additive,  $F_ACO_2 = F_ICO_2 + (VCO_2/alveolar \; ventilation)$ . In most of our patients, the  $F_ACO_2$  (35 mmHg or 4.5 %) can be allowed to increase by 4 mmHg or 0.5 % without causing any harm. Therefore, the  $F_1CO_2$  can be allowed to rise to 4 mmHg or 0.5 % in most of our patients.

The use of "fractional canister usage" allows canister costs to be calculated by multiplying the FCU (expressed in fraction) with the cost of 1 canister, and this for any FGF. While the exact conditions in real life do differ from the in vitro conditions of this study, the ratios of the product of FCU and the cost of 1 canister of the different brands can be used to make fair cost comparisons among canisters.

The canisters used to define the FGF-FCU relationship all had an identical lot number. Are these results applicable to other lot numbers? Inter-lot differences were only statistically significant for the 2 longest lasting canisters, SpiraLith and LithoLyme-12 and 18 % respectively. Intra-lot variability was small, with the notable exception of the Medisorb canister. SpiraLith canisters have both the steepest  $F<sub>I</sub>CO<sub>2</sub>$  rise and the least intra-lot variability, a consistency we hypothesize is due to the preformed channels that leave little room for the more random channeling that is likely to occur with canisters containing the  $Ca(OH)$ <sub>2</sub> granules. If the results of the 2 lots are combined, the different prepacks can be ranked according their efficiency (least to most efficient) as follows: Amsorb Plus = Medisorb  $EF < L$ oFloSorb $\lt$  $Medisorb = Spherasorb = LithoLyme < SpiralLith$  (all for an  $F_{I}CO_{2}$  threshold = 0.5 %).

The use of a consistent, replicable model allows canisters to be compared and allows for external verification. Still, real life conditions may differ from in vitro conditions:  $CO<sub>2</sub>$  loads in real life vary, both in time and quantity. No canister is used for more than 24 h straight. It is unclear how—and whether—changing FGFs and  $CO<sub>2</sub>$  loading conditions with prolonged periods of non-use (at night, during the weekends) affect canister performance, both absolute and relative, from one brand to another. In addition,  $O_2$  was not removed from the system, while in real life patients do remove  $O_2$ . Therefore, in real life, the degree of rebreathing might be slightly different from that in the experimental setup. However, the effect on canister life is likely to be very small, and certainly will not affect relative canister life. Ongoing clinical studies will help address the issues raised in this paragraph.

To summarize, canister life of  $CO<sub>2</sub>$  absorber prepacks were determined over a wide range of FGFs with the Aisys<sup>®</sup> (GE, Helsinki, Finland) under identical  $CO<sub>2</sub>$  load conditions. The most important factors that determine canister life of prepacks in a circle breathing system are the chemical composition of the canister, the absolute

<span id="page-9-0"></span>absorbent content of the canister, and the  $F_1CO_2$  replacement threshold. The use of the fractional canister usage allows for cost comparisons among different prepacks. Results should not be extrapolated to prepacks that fit onto other anesthesia machines.

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Conflict of interest The authors declare that they have no conflict of interest.

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