

Ab initio investigation of the adsorption of zoledronic acid molecule on hydroxyapatite (001) surface: an atomistic insight of bone protection

Mun-Hyok Ri¹ · Chol-Jun Yu¹ · Yong-Man Jang² · Song-Un Kim²

Received: 22 September 2015 / Accepted: 25 November 2015 / Published online: 14 December 2015
© Springer Science+Business Media New York 2015

Abstract We report a computational study of the adsorption of zoledronic acid molecule on hydroxyapatite (001) surface within ab initio density functional theory. The systematic study has been performed, from hydroxyapatite bulk and surface, and zoledronic acid molecule to the adsorption of the molecule on the surface. The optimized bond lengths and bond angles were obtained and analyzed, giving an evidence of structural similarity between subjects under study. The formation energies of hydroxyapatite (001) surfaces with two kinds of terminations were calculated to be about 1.2 and 1.5 J/m² with detailed atomistic structural information. We determined the adsorption energies of zoledronic acid molecule on the surfaces, which are −260 kJ/mol at 0.25 ML and −400 kJ/mol at 0.5 ML. An atomistic insight of strong binding affinity of zoledronic acid to the hydroxyapatite surface was given and discussed.

Introduction

Bisphosphonates (BPs) are widely used as the most powerful drug for protecting bone and treating bone diseases such as osteoporosis and other metabolic bone disorders [1–5]. From the 1960s onward, a great number of extensive

studies on BPs with respect to the development and clinical treatment have been carried out, but the research field on BPs is still very active, being continued to evolve toward a better understanding of treatment mechanisms and a finding of more potent BP. In this context, zoledronic acid (or zoledronate, ZOD), whose chemical name is [1-hydroxy-2-(1H-imidazol-1-yl) ethylidene] bisphosphonic acid or 2-(imidazol-1-yl)-1-hydroxy-ethane-1,1-diphosphonic acid, was developed as a third-generation BP and was approved for the oral treatment of bone disease in 2012 in DPR Korea after the success of its synthesis in our own way by two of the authors (Yong-Man Jang and Song-Un Kim).

BPs are characterized by two phosphonate groups, central carbon atom in between, and two side groups R1 and R2, while human bone is composed of complex array of hydroxyapatite (HAP, Ca₅(PO₄)₃OH) crystallites with nano sizes ranging from 30 to 200 nm embedded within the collagen matrix [6–8]. It is well established that the function of BPs to inhibit bone resorption is originated with their ability of binding strongly to bone mineral, that is, HAP crystal, and stiff resistance to chemical and enzymatic hydrolysis [4]. In more detailed explanation, the P–C–P backbone of BPs made from two phosphonate groups and carbon atom has a high binding affinity for the compositions of HAP—tetrahedral PO₄ groups, OH groups and Ca ions—with an additional contribution from the R1 side group (in most cases including ZOD, it is –OH) [4, 9]. Moreover, the P–C–P group of BPs is considerably more resistant to the dissolution of HAP crystal than the P–O–P group of pyrophosphate, of which BPs are stable structural analogs [10–14].

Varying another side group R2 of BPs can result in differences in antiresorptive potency with several orders of magnitude. It was observed that more potent BPs possesses a primary, secondary, or tertiary nitrogen atom in the R2

✉ Chol-Jun Yu
ryongnam14@yahoo.com

¹ Department of Computational Materials Design (CMD), Faculty of Materials Science, Kim Il Sung University, Ryongnam-Dong, Taesong-District, Pyongyang, Democratic People's Republic of Korea

² Department of Organic Chemistry, Faculty of Chemistry, Kim Il Sung University, Ryongnam-Dong, Taesong-District, Pyongyang, Democratic People's Republic of Korea

side chain [15, 16]. At present, the most potent antiresorptive BPs include a heterocyclic R2 side chain containing a nitrogen atom like risedronate and zoledronate [17]. The structure–activity relationship analysis showed that the strong binding affinity of zoledronate for HAP is related to its 3D shape and atomic orientation, indicating an important role of 3D shape of nitrogen-containing BP and the orientation of its nitrogen in binding affinity for HAP [4].

Atomistic modeling and simulations are a powerful tool to describe the structural characteristics of BPs and bone mineral HAP and the interaction between them at atomic scale, as proved in materials science and molecular science through a vast number of applications. For instance, molecular dynamics (MD) simulations based on the well-constructed classical force field have provided the structural information and energetics of bone mineral, HAP crystal, and its surfaces [18–21]. Bhowmik et al. [18] obtained the structural parameters of monoclinic HAP crystal and its surface energetics using the consistent valence force field, presenting a valuable description of the interaction between polyacrylic acid and HAP. The surface energetics of HAP crystalline surfaces using ab initio density functional theory (DFT) calculations within the generalized gradient approximation (GGA) for the exchange–correlation functional has been studied by Zhu and Wu [19], testing the effects of slab thickness, vacuum width between slabs, and surface relaxation on surface energy. Barrios [21] has investigated the interaction between collagen protein and HAP surface by using a combination of computational techniques, DFT and classical MD methods. Duarte et al. [22] performed molecular mechanics simulations for molecular structures of 18 novel hydroxyl- and amino-BPs to examine the interaction between BPs and hydroxyapatite and to extract relating structural characteristics of BPs and their affinities for the mineral, which are in agreement with in vitro and in vivo studies for some of the studied BPs. Recently, there has been reported the experimental and DFT results showing a high sensitivity of HAP nanoparticles to the quality and quantity of some type of dopants [23–25]. To the best of our knowledge, however, investigation on surface adsorption of zoledronate on HAP surface with its detailed atomistic structure based on quantum mechanics is still scarce, in spite of such extensive theoretical studies of BPs and HAP surface, and we believe that ab initio study on this phenomenon should definitely contribute to a better understanding of the interaction of zoledronate with bone mineral at atomic and electronic scale.

In this paper, we carry out systematic ab initio DFT calculations for zoledronate molecule, hydroxyapatite bulk and surface, and surface adsorption of zoledronate molecule on hydroxyapatite surface. Our special focus is placed

on the adsorption of zoledronate molecule on hydroxyapatite surface, providing the adsorption energy and atomistic structures of surface complexes, and an insight how charge transferring is occurred in the event of adsorption. This is aimed to get a reliable insight for bone protection effect of zoledronate at electronic scale. In the following section, we describe a computational method, and present the results for structural parameters and electronic properties of hydroxyapatite bulk and surface, zoledronate molecule, and for binding of zoledronate to hydroxyapatite surface in “[Results and discussion](#)” section, and end the article with conclusions.

Computational method

For the DFT calculations in this work, we have employed SIESTA code [26] which solves numerically Kohn–Sham equation within DFT [27, 28] using a localized numerical basis set, namely pseudo atomic orbitals, and pseudopotentials for describing the interaction between ionic core (nucleus plus core electrons) and valence electrons. The BLYP GGA functional (the Becke exchange functional [29] in conjunction with the Lee–Yang–Parr correlation functional [30]) was used for exchange–correlation interaction between electrons. For all the atoms, Troullier–Martins [31] type norm-conserving pseudopotentials were generated within local density approximation (LDA) [32], and checked carefully. The basis sets used in this work were the DZP type (double ζ plus polarization). The mesh size of grid, which is controlled by energy cutoff to set the wavelength of the shortest plane wave represented on the grid, has taken a value of 200 Ry. Non-fixed atoms were allowed to relax until the forces converge less than 0.02 eV/Å.

We first determine the crystal lattice parameters of bulk HAP by performing structural optimization with atomic coordinate relaxation using the conjugate gradient scheme and appropriate Monkhorst–Pack k -points. Through a comparison of the lattice constants with the experimental values, we have a confidence of the above-mentioned selection for calculation parameters. Structural optimization for isolated ZOD molecule is performed as well, and this for several conformations to select the most stable one, of which total energy is the lowest among studied conformations.

We then select the interesting surface index as (001) on the basis of experimental evidence that this face provides binding sites for many ionic species [33, 34]. In order to simulate the surface within a three-dimensional simulation code, we use two-dimensional periodic slabs as discussed in the following section (“[Hydroxyapatite \(001\) surface](#)” section).

To check the stability of the surface, the surface formation energies are calculated approximately as the difference between the total energies of the slab and the corresponding bulk crystal:

$$\gamma = \left(E_{\text{slab}} - \frac{N_{\text{slab}}}{N_{\text{bulk}}} E_{\text{bulk}} \right) / 2A, \quad (1)$$

where N_{slab} and N_{bulk} are the numbers of atoms in the surface slab and in the bulk unit cell, A is the slab surface area, and E_{slab} and E_{bulk} are the total energies of the slab and bulk structures, respectively [35]. The sign of surface formation energy is a test of surface stability: positive (negative) means energy should be provided (released) in order to create a surface. We note that there might be several possible cutting planes for a particular Miller index while guaranteeing neutrality of the surface charge perpendicular to the surface [36].

Final step of the work is to simulate the adsorption of ZOD molecule on the relevant relaxed HAP (001) surfaces. In order to have the rough, initial surface adsorption structure, we use classical molecular mechanics (MM) method. In this MM simulation, general utility lattice program (GULP) [37] is utilized. For describing the interaction between atoms, we use the Dreiding force field, where the potential energy is described as the sum of the contributions resulting from the bonded interactions (bond stretching, bond bending, and torsions) and from the non-bonded interactions (e.g., electrostatic interaction, and van der Waals interaction) [38]. After making a guess for the initial state of the adsorption complex, we also carry out atomic relaxation for the surface complex—ZOD molecule and surface atoms in the slab—to obtain a stable final state. Then, the adsorption energy can be calculated as follows:

$$E_{\text{ads}} = \frac{1}{N_{\text{mol}}} [E_{\text{mol-slab}} - (E_{\text{slab}} + N_{\text{mol}}E_{\text{mol}})], \quad (2)$$

where N_{mol} is the number of adsorbed molecules, and $E_{\text{mol-slab}}$ and E_{mol} are the total energies of the adsorbed surface and of the isolated molecule, respectively. The adsorption energy can be either negative or positive: negative (positive) means energy should be released (provided) during the adsorption, indicating that the adsorption is (not) spontaneous exothermic (endothermic) process.

Results and discussion

Bulk hydroxyapatite

The crystal structure of hydroxyapatite is hexagonal with space group $P6_3/m$, which contains a formula unit $\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$. In fact, there must be four hydroxyl groups in the unit cell with the $P6_3/m$ space group, each oxygen atom

of hydroxyl group with 1/2 occupancy [21]. To make the DFT calculations enable, therefore, we have made a model with full occupancies for the hydroxyl groups, by assigning alternate 0 and 1 occupancies to these hydroxyl groups, which results in the change of the space group from $P6_3/m$ to $P6_3$. However, the modified model has a net electric polarization contrary to the experiment which shows zero polarization, because all the hydroxyl groups in the model are oriented in the same direction. To mimic the real structure where disorder exists in the relative orientation of the parallel OH channels, so that electric polarizations are compensated each other, we have created a supercell containing two unit cells in the [100] direction, and assigning opposite orientations to the two OH channels in the supercell. The crystal structure with antiparallel hydroxyl groups in a double unit cell compared to the original hexagonal structure is monoclinic with $P2_1$ space group. We have used this structure in this work, thus allowing a direct comparison of the simulation results with experimentally determined surfaces.

The full optimization of the structure was performed, allowing the cell shape and volume, and ionic positions to relax. We have checked the convergence with respect to the special k -points; increasing the k -points set from $(1 \times 2 \times 3)$ to $(2 \times 4 \times 6)$ leads to the change between the total energies as about 5 meV, thus indicating the safe use of $(1 \times 2 \times 3)$ set. Figure 1 depicts the fully optimized supercell of bulk HAP in this work. The calculated structural

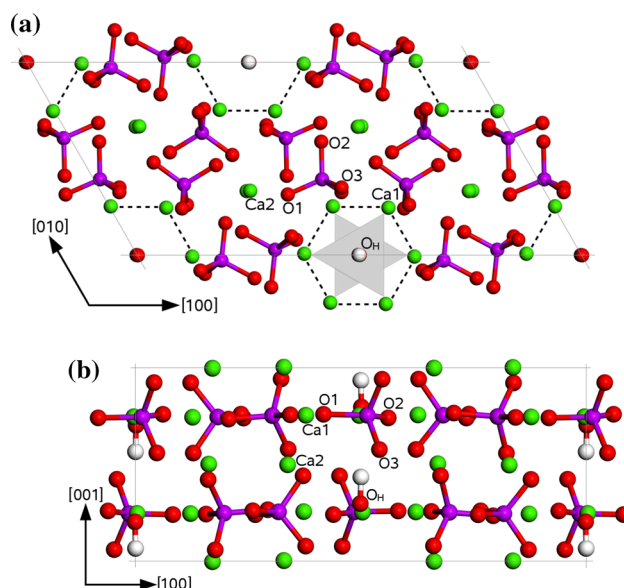


Fig. 1 (Color online) Top view (a) and side view (b) of supercell of bulk hydroxyapatite crystal with monoclinic $P2_1$ space group, which is doubled the unit cell in [100] direction so as to compensate the electric polarization by assigning opposite orientations to the two OH channels in hexagon surrounded by triangle of Ca1 ions. (Ca: green, P: purple, O: red, and H: white)

Table 1 Structural parameters of bulk hydroxyapatite crystal structure with monoclinic $P2_1$ space group, compared with experimental results

	Lattice parameters	
	This work	Experiment ^a
a, b, c (Å)	9.348, 9.352, 6.955	9.430, 9.430, 6.891
α, β, γ (°)	90, 90, 119.86	90, 90, 120
Average of bond lengths (Å)		
P–O	1.578	1.540
Ca1–O	2.423	2.478
Ca1–OH	2.339	2.354
Ca2–O	2.553	2.556
Average of bond angles (°)		
O–P–O	109.44	109.45
O–Ca1–O	98.62	
O–Ca2–O	99.40	

^a Ref. [39]

parameters and chemical bonding properties of bulk HAP are given in Table 1. The lattice constants ($a = 9.348$, $b = 9.352$, and $c = 6.955$ Å) of the fully optimized structure are in good agreement with the experimental values ($a = b = 9.43$, $c = 6.891$ Å) [39, 40] (<1.0 % error) as well as with the earlier DFT results [21, 41, 42]. Note that a is the half of lattice constant of the supercell.

As shown in Fig. 1, there are two different Ca sites (denoted as Ca1 and Ca2), four oxygen sites (O1, O2, and O3 of phosphate tetrahedron, and O_H of hydroxyl group), one P site, and one H site. The Ca1 atom is coordinated to seven oxygen ions, which are six oxygen ions of five different PO₄ groups, and one oxygen ion of OH group, while the Ca2 atom has a ninefold coordination with oxygen ions situated in six different PO₄ tetrahedra. The three Ca1 atoms also form a triangle at the same plane normal to the c axis, whose center is occupied by an OH group, and the two triangles form a hexagonal screw configuration. The calculations yield average bond lengths as 1.578 Å for P–O bond, 2.423 Å for Ca1–O, 2.339 Å for Ca1–O_H, and 2.553 Å for Ca2–O, compared to the corresponding experimental values of 1.54, 2.478, 2.354, and 2.556 Å, respectively. The similar agreement is obtained in the bond angles, as shown in Table 1. These comparisons confirm that our computational parameters are reasonably satisfactory for a good assessment of surface calculations.

Hydroxyapatite (001) surface

In this work, we have selected the Miller indices of HAP surface as (001), since there exists experimental evidence

that the (001) surface is the most stable among several surfaces with low indices and provides binding sites for many ionic species [33, 34, 43]. As we use the supercell doubled in the [100] direction as a unit cell for bulk HAP, the (001) surface unit cell is an oblique (2×1) surface cell and there might be two kinds of terminations; (1) $2\text{Ca}_2-(6\text{PO}_4 \cdot 6\text{Ca}_1 \cdot 2\text{OH})-2\text{Ca}_2$, denoted as Type (I), and (2) $(3\text{PO}_4 \cdot 3\text{Ca}_1 \cdot \text{OH})-4\text{Ca}_2-(3\text{PO}_4 \cdot 3\text{Ca}_1 \cdot \text{OH})$, denoted as Type (II). They are repeated in the [001] direction, assigned to building layer, and belong to the Tasker (II)-type surface [36] with no electric dipole moment perpendicular to the surface.

The HAP (001) surface has been modeled using three-dimensional periodic supercell (slab) with two equivalent surfaces at bottom and top side. To ensure no interaction between bottom surface of the above image slab and top surface of the present slab across the vacuum region, the vacuum region must be wide enough. And the atomic layer, which consists of surface layer allowed to be relaxed and crystal layer fixed at its crystalline position, should be thick enough so that the two surfaces of each slab do not interact through the crystal layer. To check the convergence according to the vacuum region, we tested 20, 30, 40, and 50 Å thicknesses, and confirmed that there is no distinct change between 20 and 50 Å thick vacuums (Table 2). Therefore, the vacuum region with a thickness of 30 Å will be used in the following calculations. The thickness of the slab is usually expressed in terms of number of building layers, where one layer contains 44 atoms. The four layers (two bulk unit cells, 176 atoms), six layers (three bulk unit cells, 264 atoms), and eight layers (four bulk unit cells, 352

Table 2 Surface energies (J/m^2) according to vacuum thickness and building layers of hydroxyapatite (001) surfaces with (2×1) surface unit cell

	Type (I); $2\text{Ca}_2-(6\text{PO}_4 \cdot 6\text{Ca}_1 \cdot 2\text{OH})-2\text{Ca}_2$			
	Size	Unrelaxed	Relaxed	Ref. ^a
Vacuum (Å)	20	1.460	1.208	
	30	1.461	1.205	
	40	1.448	1.197	
	50	1.449	1.205	
Layer	4 (176)	1.461	1.205	
	6 (264)	1.474	1.218	
	8 (352)	1.496		
Type (II); $(3\text{PO}_4 \cdot 3\text{Ca}_1 \cdot \text{OH})-4\text{Ca}_2-(3\text{PO}_4 \cdot 3\text{Ca}_1 \cdot \text{OH})$				
Layer	4 (176)	2.084	1.514	1.01
	6 (264)	2.057	1.506	
	8 (352)	2.078		

The values in parenthesis represent the number of atoms

^a Ref. [21]

atoms) were tested with a vacuum width of 30 Å, and the change of surface energies between 4 layers slab and 8 layers slab is only 0.05 J/m². Thus we will use the slab with 4 building layers in the study of surface adsorption.

As listed in Table 2, the surface energy of Type (II) surface is slightly higher than that of Type (I) surface, indicating the Type (I) terminated surface is more favorable than the Type (II) terminated surface. We see that the surface relaxation in the Type (I) surface is not really much compared to the Type (II) surface, since the difference between unrelaxed and relaxed surface energies in the former case is not remarkable contrary to the latter case. Since there are no data available in the literature for Type (I), we only compared the calculated Type (II) surface energy with the previous SIESTA work [21].

Figure 2 shows the fully relaxed atomistic structure of the HAP (001) surfaces modeled by a slab with vacuum thickness of 30 Å and four building layers. It is observed that the coordination number (CN) of Ca1 atom changes from 7 in bulk to 6, and CN of Ca2 from 9 to 6 in the

Type (I) termination, while in the Type (II) termination the CN of Ca1 atom changes from 7 to 6, and Ca2 atom from 9 to 5, and 6. The coordination environments around the surface oxygen atoms (O1, O2, O3, and O_H) are also changed from their bulk environment, while P atoms are still fully surrounded by four oxygen atoms like in bulk.

Table 3 shows the bond lengths of cation-oxygen and bond angles of oxygen-cation-oxygen at the top surface layer. In the case of Type (II) surface, we consider the two kinds of Ca1 and three kinds of Ca2 surface atoms. In both cases, the averages (1.583, 1.585 Å) of bond lengths of P–O are a bit expanded compared with the bulk (1.578 Å), and the averages of bond angles get smaller than in the bulk. The bond lengths of Ca2–O are clearly contracted at the surface; 2.434 in Type (I), and 2.325, 2.380, and 2.414 Å in Type (II), which are all smaller than the bulk value 2.553 Å. From these observations, it can be concluded that the undercoordinated surface Ca atoms and O atoms can be favorable adsorption sites.

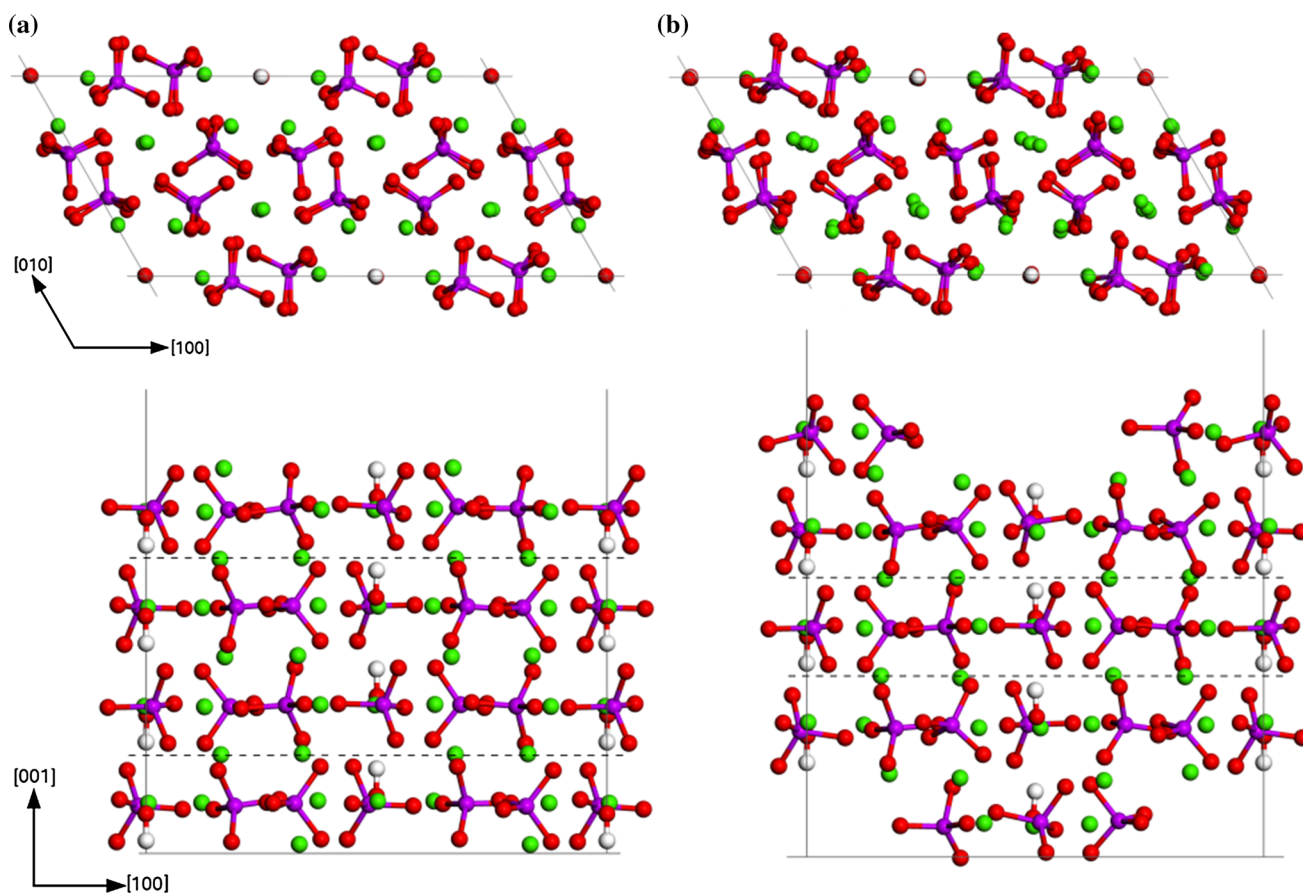


Fig. 2 (Color online) Top view (*upper panel*) and side view (*lower panel*) of optimized structure of hydroxyapatite (001) surface with (2 × 1) surface unit cell, vacuum thickness of 30 Å, 4 building layers, and termination 2Ca₂-(6PO₄-6Ca₁-2OH)-2Ca₂ (a) and

termination (3PO₄-3Ca₁-OH)-4Ca₂-(3PO₄-3Ca₁-OH) (b). The *top* and *bottom* layers are allowed to relax, while the layers between *dashed lines* are fixed at their crystalline positions. (Ca: green, P: purple, O: red, H: white)

Table 3 Bond lengths of cation-oxygen and bond angles of oxygen-oxygen at hydroxyapatite (001) surface with coordination numbers (CN) of cations

	Type (I); 2Ca ₂ –(6PO ₄ ·6Ca ₁ ·2OH)–2Ca ₂			CN
	Length (Å)	Angle (°)		
		Range	Average	
P	1.583	103.47–116.23	109.39	4
Ca ₁	2.352	64.54–155.26	101.50	6
Ca ₂	2.434	62.45–137.08	94.01	6
Type (II); (3PO ₄ ·3Ca ₁ ·OH)–4Ca ₂ –(3PO ₄ ·3Ca ₁ ·OH)				
P	1.585	102.07–117.07	109.22	4
Ca ₁	2.420	60.97–159.10	99.72	6
Ca ₁	2.343	64.73–160.44	102.36	6
Ca ₂	2.325	66.52–147.60	101.91	5
Ca ₂	2.414	60.91–170.66	98.61	6
Ca ₂	2.380	61.52–154.20	99.52	6

Zoledronic acid molecule

To simulate an isolated molecule, we have used a cubic supercell with lattice constants of $a = b = c = 50 \text{ \AA}$, which has been proved to be enough to prevent the artificial interaction between adjacent molecules. There might be four different conformations, as presented in Fig. 3. We can make a distinction between the conformations according to the directions of two pairs of OH groups attached to the two P atoms: (1) ZOD_{Bout} for the case where the directions of both OH pairs are outward against the nitrogen heterocyclic ring, (2) ZOD_{Bin} for the case of inward directions of both pairs, (3) ZOD_{Nin} for the case of inward direction of one pair in the same side of nitrogen atom, and (4) ZOD_{Nout} for the case of outward direction of one pair in the N side. After the total energy minimizations to get the optimized structure of molecule, we have compared the total energies of four conformations. The calculations tell us the most stable structure is just the third case, ZOD_{Nin}, which will be used in the following adsorption study.

The optimized bond lengths and bond angles related with P atoms in ZOD_{Nin} conformation are listed in Table 4. The averages of P–O bond lengths are 1.597 Å in P1 side and 1.586 Å in P2 side, which are similar to those of bulk HAP (1.578 Å) and of HAP (001) surface (1.583 Å). The averages of O–P–O bond angles (112.11° and 111.42°) are also close to those of bulk HAP (109.44°) and HAP surface (109.39°). It is found that those values of P2 side are slightly closer to the bulk and surface values than P1 side, so that P2 side is more favorable to binding with HAP due to the closer structural similarity. Since the P–O bond

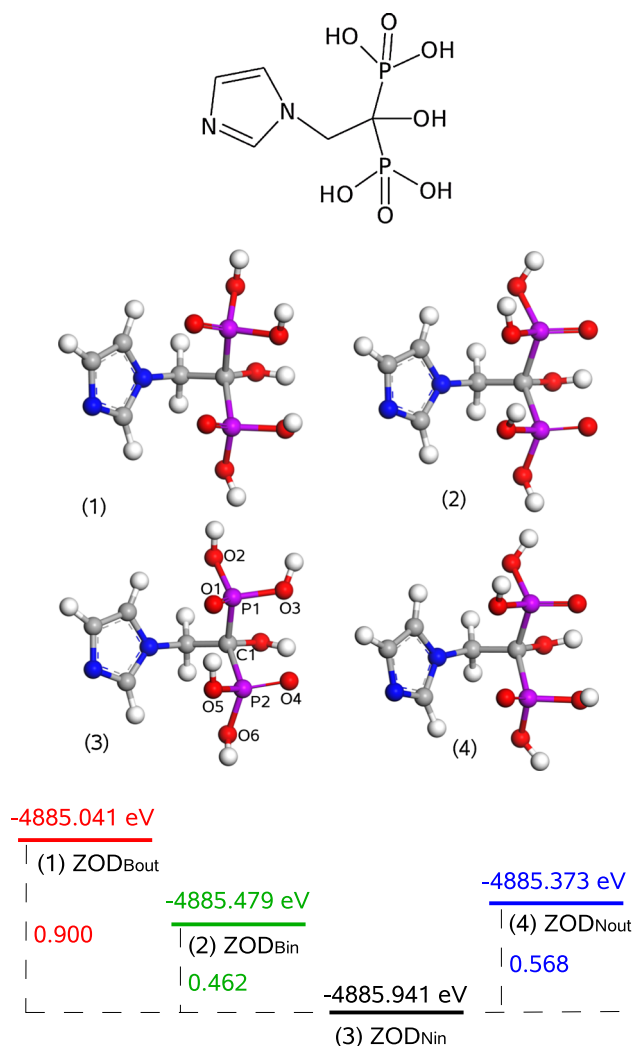


Fig. 3 (Color online) Optimized structures of zoledronic acid with four different conformations, (1) ZOD_{Bout}, (2) ZOD_{Bin}, (3) ZOD_{Nin}, and (4) ZOD_{Nout}. (C: gray, P: purple, N: blue, O: red, H: white)

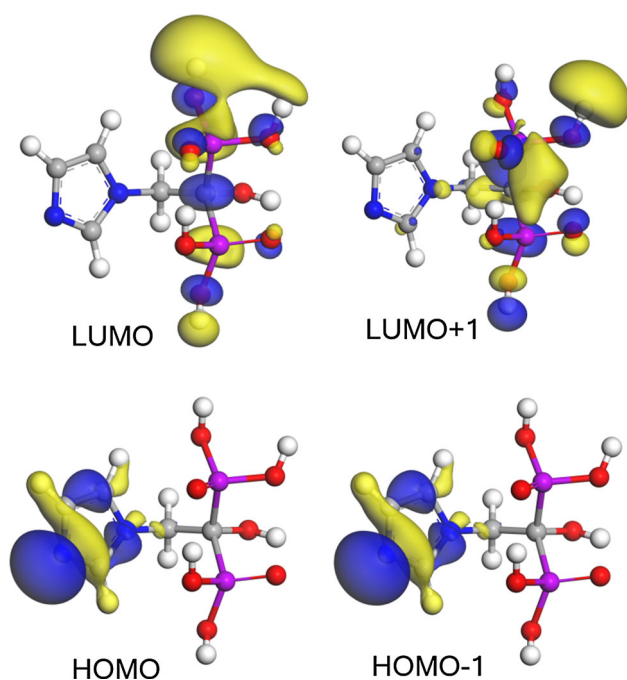
lengths and O–P–O bond angles of phosphonate group of ZOD molecule are similar to those of phosphate group of HAP surface, we can say with certainty that both P1 and P2 sides of ZOD molecule will bind to PO₄ groups of HAP surface and the strong P–C–P backbone of ZOD molecule adsorbed on HAP surface will protect the bone mineral against the attack of osteoclast.

Figure 4 shows the computed isodensity surfaces for the highest occupied molecular orbitals (HOMO) and lowest unoccupied molecular orbitals (LUMO) of ZOD (conformation ZOD_{Nin}). While the HOMO and HOMO–1 are localized on the heterocyclic ring containing nitrogen atom, LUMO and LUMO+1 are on the phosphonate groups. This leads to the intramolecular charge separation upon excitation. The change in electronic distribution between HOMO and LUMO indicates that two phosphonate groups can play a role of electron acceptor in the

Table 4 Optimized bond lengths and angles related with phosphorus atoms in zoledronic acid conformation, ZOD_{Nin}

P1 related			
Bond length (Å)		Bond angle (°)	
P1=O1	1.495	O1=P1-O2	117.26
P1-O2	1.654	O1=P1-O3	115.10
P1-O3	1.641	O1=P1-C1	115.22
P1-C1	1.902	O2-P1-O3	103.97
		O2-P1-C1	102.96
		O3-P1-C1	100.12
	Ave.	O-P1-O	112.11
	Ave.	O-P1-C1	106.10
P2 related			
P2=O4	1.495	O4=P2-O5	120.01
P2-O5	1.622	O4=P2-O6	117.35
P2-O6	1.641	O4=P2-C1	99.93
P2-C1	1.934	O5-P2-O6	96.91
		O5-P2-C1	112.73
		O6-P2-C1	110.40
	Ave.	O-P2-O	111.42
	Ave.	O-P2-C1	107.69
		P1-C1-P2	98.65

Ave. Average

**Fig. 4** (Color online) Molecular orbitals of zoledronic acid conformation, ZOD_{Nin}

chemical reaction, while the heterocyclic ring containing nitrogen atom could be a donor.

Adsorption of zoledronic acid on hydroxyapatite (001) surface

To begin with adsorption, we have utilized GULP to obtain rough structure of ZOD absorbed on HAP (001) surface, where Dreiding force field was adopted. Simulated annealing was performed, increasing the temperature from 300 to 10000 K and subsequently decreasing back to 300 K with the temperature interval of 50 K. Using the obtained rough structure as the starting structure, we then performed atomic relaxation with SIESTA code to get the final optimized structure of zoledronic acid-adsorbed HAP (001) surface.

In this work, we have tried to simulate the adsorption of ZOD molecule at 0.5 monolayer (ML) (one molecule on (2×1) surface cell) and at 0.25 ML coverages (one molecule on (2×2) surface cell). As mentioned above, there are two possible terminations in the HAP (001) surface and therefore four kinds of simulation tasks were carried out. We have used the slab model with 4 building layers and vacuum thickness of 30 Å, which guarantee to give reliable adsorption energy. To make a systematic error small, the pristine surface energies for (2×2) surface slabs were also calculated. In Table 5, the adsorption energies are listed. All the adsorption energies are negative, indicating that all the adsorptions are exothermic reactions. We see that the adsorption on Type (II) surface is slightly more favorable than on Type (I) at both 0.5 ML and 0.25 ML, although the Type (I) surface formation from the bulk needs more energy than the Type (II) surface.

Figure 5 shows the optimized atomistic structure of ZOD adsorption complexes on HAP (001) surfaces at 0.25 ML coverage. It is observed that in the Type (I) surface the hydrogen atom of ZOD's phosphonate group moved to oxygen atom of HAP surface's phosphate group, making formation of additional OH group on the surface, and thus indicating that the adsorption is a kind of chemisorption caused by proton exchange. There are several hydrogen bonds between ZOD's phosphonate OH

Table 5 Calculated adsorption energies (kJ/mol) of zoledronic acid on hydroxyapatite (001) surface

	Coverage	
	0.5 ML (2×1)	0.25 ML (2×2)
Type (I)	-388.44	-246.70
Type (II)	-439.49	-268.34

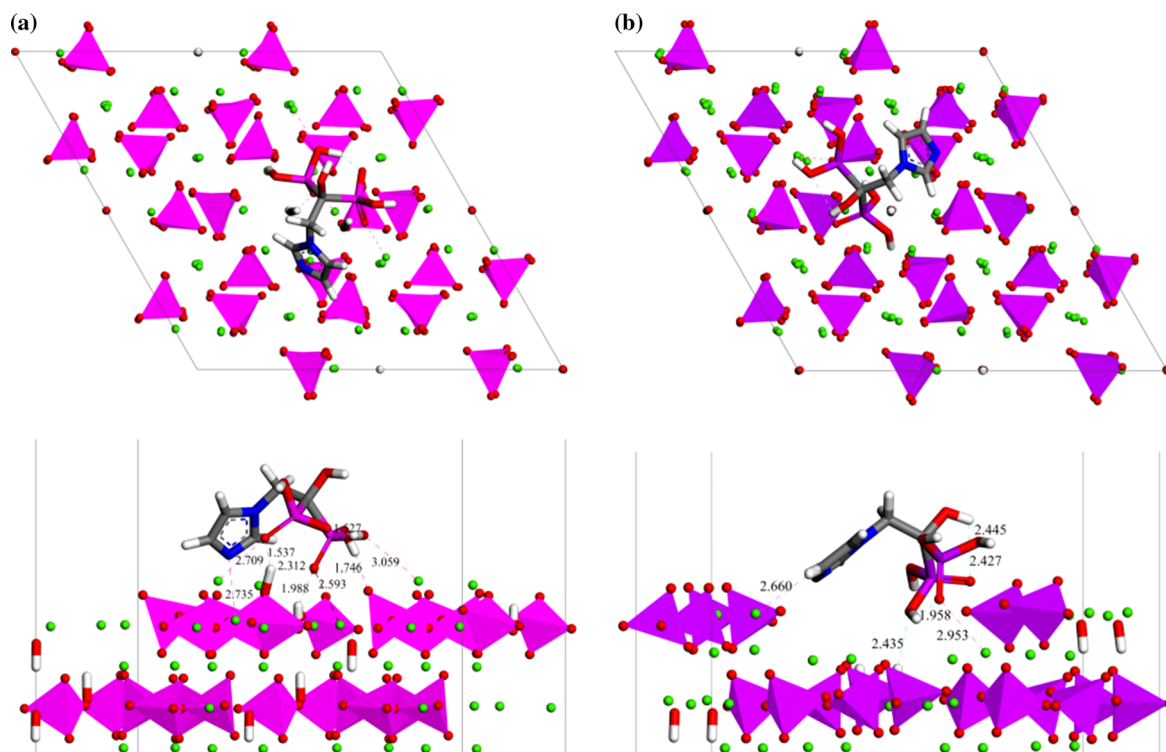


Fig. 5 (Color online) Top view (*upper panel*) and side view (*lower panel*) of optimized atomistic structure of zoledronic acid adsorption complexes on hydroxyapatite (001) surfaces with Type I (**a**) and

Type II (**b**) terminations at 0.25 ML coverage. (Ca: green, P: purple, O: red, N: blue, H: white)

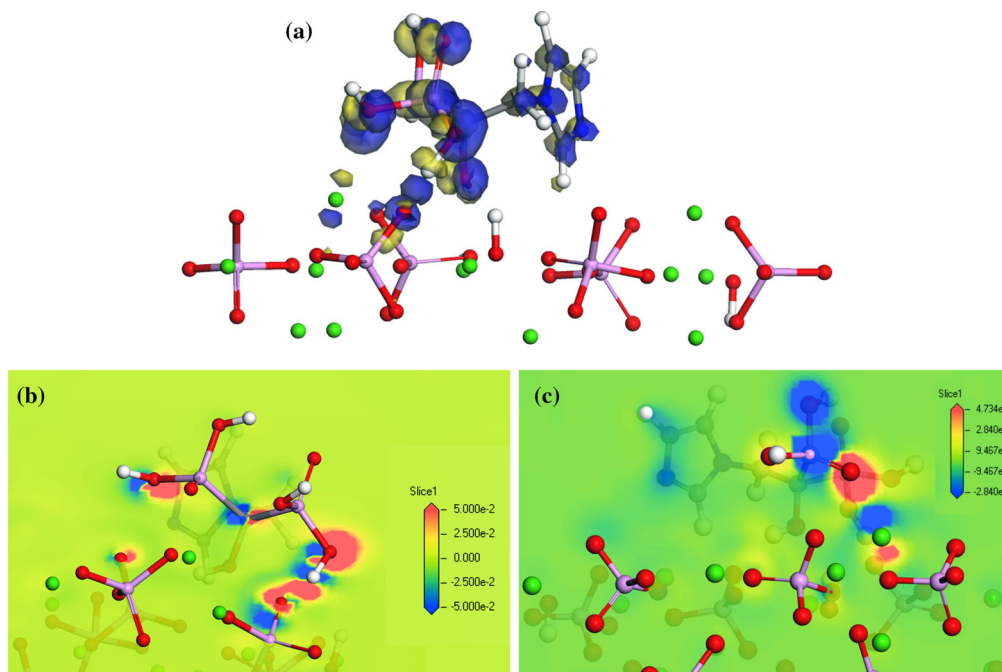


Fig. 6 (Color online) Electronic charge density difference of zoledronic acid adsorption complex on hydroxyapatite (001) surface. **a** Isosurface figure with the value of $\pm 0.04 \text{ eV}/\text{\AA}^3$ (yellow for + and blue for - value), **b** contour figure on the plane containing hydrogen

bond between O of phosphonate group of HAP surface and hydrogen of phosphate group, and **c** contour figure around Ca cation. (Ca: green, P: purple, O: red, N: blue, H: white)

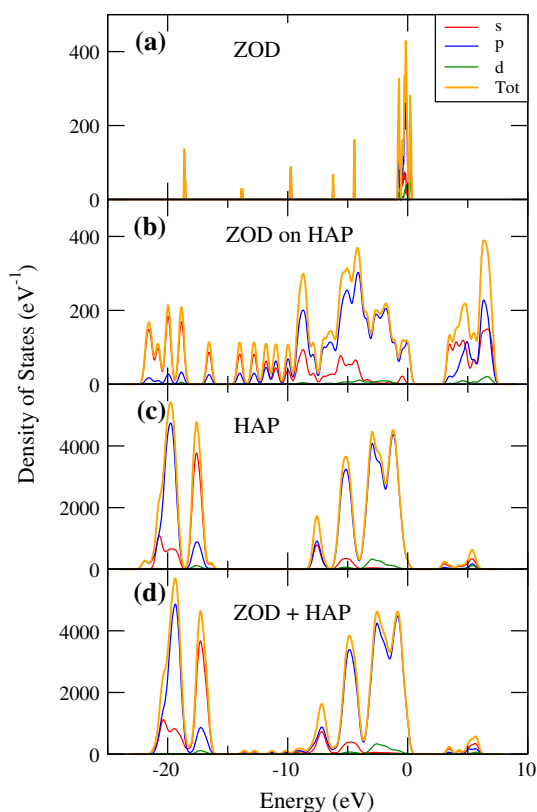


Fig. 7 (Color online) Total and partial density of states in isolated zoledronic acid (a), adsorbed zoledronic acid (b), hydroxyapatite (100) surface (c), and zoledronic acid adsorption complex on the surface (d)

group and oxygen atoms of the surface's phosphate groups, and vice versa. It is also found that Ca1 and Ca2 atoms with 6 coordination number (CN) make bonds with oxygen and nitrogen atoms of ZOD, respectively. Such bonding was expected based on the surface relaxation analysis and HOMO–LUMO distribution of isolated ZOD molecule. In the case of Type (II) surface, there are also hydrogen bonds between the surface and ZOD, but the move of hydrogen atom is not observed, which indicates that the adsorption is kind of physisorption. Nevertheless, the magnitude of adsorption energy on Type (II) surface is larger than that on Type (I) surface.

To make clear the charge transfer occurred during the adsorption, we show the electron density difference, $\rho_{\text{surf+mol}} - (\rho_{\text{surf}} + \rho_{\text{mol}})$, plots in Fig. 6, where (a) is for the isosurface figure with the value of $\pm 0.04 \text{ eV/\AA}^3$, and (b) and (c) are the contour plots on the planes around hydrogen bond and Ca cation, respectively. These figures clearly give the evidence of charge transferring at the event of adsorption, from hydrogen of phosphate group of ZOD molecule to oxygen of PO_4 group of HAP surface making formation of hydrogen bond, and from Ca of HAP surface to oxygen ions of phosphonate group forming the

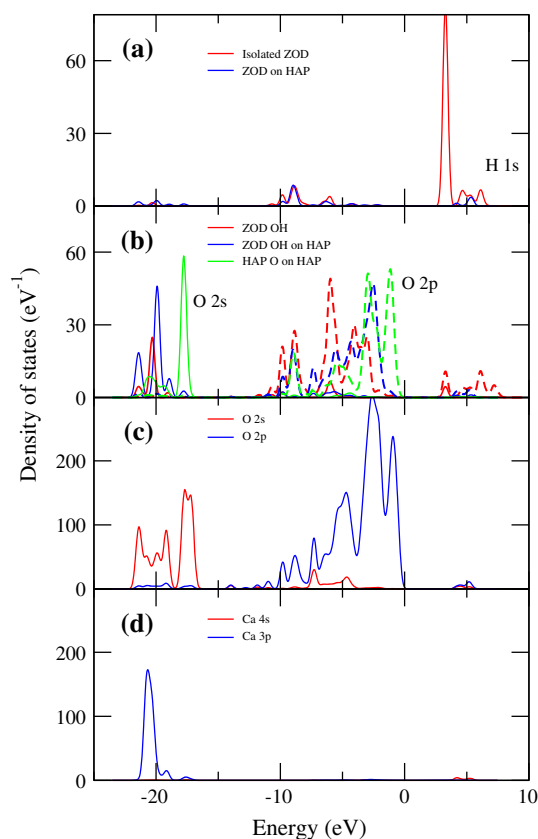


Fig. 8 (Color online) Atom projected partial density of states; a for 1s electrons of hydrogen in different situations, b for 2s and 2p electrons of oxygen atom in different situations, c for 2s and 2p states of oxygen atoms surrounding Ca cation in ZOD adsorbed HAP surface, and d for 4s and 3p of calcium forming the coordinate bond on HAP surface

coordinate bond. Therefore, the adsorption of ZOD on the HAP (100) surface is surely chemisorption.

We calculated the density of states (DOS) of electrons, total and partial DOS shown in Fig. 7 and atom projected and partial DOS in Fig. 8. In Fig. 7, we see the energy spectrum of isolated ZOD molecule (a), the DOS of ZOD molecule that was adsorbed on HAP surface (b), the DOS of HAP (100) surface (c), and the whole complex system comprising the adsorbed ZOD molecule and HAP (100) surface. Some hybridization between ZOD and HAP surface electrons is shown in the figures.

Which atoms cause the charge transferring in the event of adsorption? To give an answer to this question, we carefully investigate the atom-projected partial DOS. The 1s peak of hydrogen of isolated ZOD molecule placed over 0 eV (red line in Fig. 8a panel) is remarkably weakened after the adsorption (blue line in (a) panel), indicating the loss of electrons from hydrogen and the gain by oxygen, and thus the formation of hydrogen bond between hydrogen atom of ZOD and oxygen of HAP surface. We also see the hybridizations between hydrogen 1s state and oxygen

2p state in (a) and (b) panels, and between oxygen 2s state and calcium 3p state in (c) and (d) panels.

Conclusion

In conclusion, we have attempted to make a modeling of adsorption of zoledronic acid on hydroxyapatite (001) surface to get an atomistic insight of bone protection. The systematic study has been performed, from hydroxyapatite bulk and surface, and zoledronic acid to adsorption of the molecule on the (001) surface. We have carried out the structural optimizations and atomic relaxations of the bulk, molecule, surface, and adsorption complexes on the surfaces, and obtained the structural information and energetics.

Using the three-dimensional periodic supercell model, we determined the stable conformation of the molecule and calculated the molecular orbitals. It was concluded that two phosphonate groups can play a role of electron acceptor in the chemical reaction, while the heterocyclic ring containing nitrogen atom can be an electron donor. After verifying the validity of computational parameters of SIESTA work through the bulk hydroxyapatite calculation, surface modeling and relaxations were performed, and surface formation energies were calculated for two kinds of (001) surface terminations, which are about 1.2 and 1.5 J/m². Subsequently, the adsorption of zoledronic acid on the relaxed surface was studied, obtaining the surface binding structure and calculating the adsorption energies. We found that the surface Ca atoms and oxygen atoms of phosphate groups can form surface bond including hydrogen bond and coordinate bond with nitrogen, hydrogen, and oxygen atoms of zoledronic acid. The calculated adsorption energies are about −260 kJ/mol at 0.25 ML coverage and −400 kJ/mol at 0.5 ML coverage, indicating the strong binding affinity of zoledronic acid to hydroxyapatite surface.

We have made an interpretation of such strong binding affinity through the analysis of atomistic structures, electron density difference, and density of states. The results showed that bond lengths and bond angles of phosphonate group of zoledronic acid are similar to those of phosphate group of hydroxyapatite bulk and surface, indicating the strong binding affinity related to the structural similarity. It was also found that the charge transferring occurs mainly on the side of phosphonate group in one surface, while in another surface it occurs on both imidazol ring containing nitrogen atom and phosphonate group of zoledronic acid. Note that it is of importance to consider the effect of solvent, which should be treated in the further work.

Acknowledgements The simulations have been carried out on the HP Blade System c7000 (HP BL460c) that is owned and managed by Faculty of Materials Science, Kim Il Sung University. This work was supported from the Committee of Education (Grant No. 02-2014), DPR Korea.

Compliance with ethical standards

Conflict of interest The authors declare no competing financial interest.

References

- Ebetino FH, Hogan A-ML, Sun S, Tsoumpra MK, Duan X, Trift JT, Kwaasi AA, Dunford JE, Barnett BL, Oppermann U, Lundy MW, Boyde A, Kashemirov BA, McKenna CE, Russell RGG (2011) The relationship between the chemistry and biological activity of the bisphosphonates. *Bone* 49:20–33
- Bartl R, Frisch B, von Tresckow E, Bartl C (2007) Bisphosphonates in medical practice. Springer, Berlin
- Coxon FP, Thompson K, Rogers MJ (2006) Recent advances in understanding the mechanism of action of bisphosphonates. *Curr Opin Pharmacol* 6:307–312
- Russell RGG, Watts NB, Ebetino FH, Rogers MJ (2008) Mechanisms of action of bisphosphonates: similarities and differences and their potential influence on clinical efficacy. *Osteoporos Int* 19:733–759
- Russell RGG (2011) Bisphosphonates: the first 40 years. *Bone* 49:2–19
- Hassenkam T, Fantner GE, Cutroni JA, Weaver JC, Morse DE, Hansma PK (2004) High-resolution AFM imaging of intact and fractured trabecular bone. *Bone* 35:4–10
- Alberius-Henning P, Adolfsson E, Grins J (2001) Triclinic oxyhydroxyapatite. *J Mater Sci* 36:663–668. doi:10.1023/A:1004876622105
- Elliot JC (1994) Structure and chemistry of the apatites and other calcium orthophosphates. Elsevier Science, Amsterdam
- Russell RGG, Muhlbauer RC, Bisaz S, Williams DA, Fleisch H (1970) The influence of pyrophosphate, condensed phosphates, phosphonates and other phosphate compounds on the dissolution of hydroxyapatite in vitro and on bone resorption induced by parathyroid hormone in tissue culture and in thyroparathyroidectomised rats. *Calcif Tissue Res* 6:183–196
- Kontacka EG, Jezierska J, Lecouvey M, Leroux Y, Kozłowski H (2002) Bisphosphonate chelating agents. Coordination ability of 1-phenyl-1-hydroxymethylene bisphosphonate towards Cu(2+) ions. *J Inorg Biochem* 89:13–17
- Fleisch H (1998) Bisphosphonates: mechanisms of action. *Endocr Rev* 19:80–100
- Rogers MJ, Gordon S, Benford HL, Coxon FP, Luckman SP, Monkkonen J, Frith JC (2000) Cellular and molecular mechanisms of action of bisphosphonates. *Cancer* 88(12 Suppl):2961–2978
- Roelofs AJ, Thompson K, Gordon S, Rogers MJ (2006) Molecular mechanisms of action of bisphosphonates: current status. *Clin Cancer Res* 12:6222–6230
- Dunford JE, Thompson K, Coxon FP, Luckman SP, Hahn FM, Poulter CD, Ebetino FH, Rogers MJ (2001) Structure-activity relationships for inhibition of farnesyl diphosphate synthase in vitro and inhibition of bone resorption in vivo by nitrogen-containing bisphosphonates. *J Pharmacol Exp Ther* 296:235–242
- Nancollas GH, Tang R, Phipps RJ, Henneman Z, Gulde S, Wu W, Mangood A, Russell RGG, Ebetino FH (2006) Novel insights into

- actions of bisphosphonates on bone: differences in interactions with hydroxyapatite. *Bone* 38:617–627
16. Lawson MA, Xia Z, Barnett BL, Triffitt JT, Phipps RJ, Dunford JE, Locklin RM, Ebetino FH, Russell RGG (2010) Differences between bisphosphonates in binding affinities for hydroxyapatite. *J Biomed Mater Res B* 92B:149–155
 17. Green JR, Muller K, Jaeggi KA (1994) Preclinical pharmacology of CGP 42 446, a new, potent, heterocyclic bisphosphonate compound. *J Bone Miner Res* 9:745–751
 18. Bhowmik R, Katti KS, Katti D (2007) Molecular dynamics simulation of hydroxyapatite-polyacrylic acid interfaces. *Polymer* 48:664–674
 19. Zhu W, Wu P (2004) Surface energetics of hydroxyapatite: a DFT study. *Chem Phys Lett* 396:38–42
 20. Matsunaga K, Kuwabara A (2007) First-principles study of vacancy formation in hydroxyapatite. *Phys Rev B* 75:014102
 21. Barrios NA (2010) A computational investigation of the interaction of the collagen molecule with hydroxyapatite. Ph.D. thesis, Department of Chemistry, University College London
 22. Duarte LF, Teixeira FC, Fausto R (2010) Molecular modeling of the interaction of novel hydroxyl- and aminobisphosphonates with hydroxyapatite. *ARKIVOC* (v), pp 117–127
 23. Yavkin BV, Mamin GV, Orlinskii SB, Gafurov MR, Salakhov MK, Biktagirov TB, Klimashina ES, Putlayev VI, Tretyakov YD, Silkin NI (2012) Pb^{3+} radiation defects in $Ca_9Pb(PO_4)_6(OH)_2$ hydroxyapatite nanoparticles studied by high-field (w-band) EPR and ENDOR. *Phys Chem Chem Phys* 14:2246–2249
 24. Biktagirov TB, Gafurov MR, Mamin GV, Klimashina ES, Putlayev VI, Orlinskii SB (2014) Combination of EPR measurements and DFT calculations to study nitrate impurities in the carbonated nanohydroxyapatite. *J Phys Chem A* 118(8):1519–1526
 25. Gafurov MR, Biktagirov TB, Mamin GV, Klimashina ES, Putlayev VI, Kuznetsova L, Orlinskii SB (2015) The interplay of manganese and nitrate in hydroxyapatite nanoparticles as revealed by pulsed EPR and DFT. *Phys Chem Chem Phys* 17:20331–20337
 26. Soler JM, Artacho E, Gale JD, García A, Junquera J, Ordejón P, Sánchez-Portal D (2002) The Siesta method for ab initio order-N materials simulation. *J Phys Condens Matter* 14:2745
 27. Hohenberg P, Kohn W (1964) Inhomogeneous electron gas. *Phys Rev* 136:B864–B871
 28. Kohn W, Sham LJ (1965) Self-consistent equations including exchange and correlation effects. *Phys Rev* 140:A1133–A1138
 29. Becke AD (1988) Density-functional exchange-energy approximation with correct asymptotic behavior. *Phys Rev A* 38:3098–3100
 30. Lee C, Yang W, Parr RG (1988) Development of the Colle–Salvetti correlation-energy formula into a functional of the electron density. *Phys Rev B* 37:785–789
 31. Troullier N, Martins JL (1991) Efficient pseudopotentials for plane-wave calculations. *Phys Rev B* 43:1993–2006
 32. Perdew JP, Zunger A (1981) Self-interaction correction to density-functional approximations for many-electron systems. *Phys Rev B* 23:5048
 33. Almora-Barrios N, Austen K, de Leeuw N (2009) A density functional theory study of the binding of glycine, proline and hydroxyproline to the hydroxyapatite (0001) and (0110) surfaces. *Langmuir* 25:5018–5025
 34. Wierzbicki A, Cheung HS (2000) Molecular modeling of inhibition of hydroxyapatite by phosphocitrate. *J Mol Struct Theorchem* 529:73–82
 35. Yu C-J, Kundin J, Cottenier S, Emmerich H (2009) Ab initio modeling of glass corrosion: hydroxylation and chemisorption of oxalic acid at diopside and åkermanite surfaces. *Acta Mater* 57:5303–5313
 36. Tasker PW (1979) The stability of ionic crystal surfaces. *J Phys C* 12:4977–4984
 37. Gale JD, Rohl AL (2003) The general utility lattice program (GULP). *Mol Simul* 29:291–341
 38. Leach A (2001) Molecular modelling: principles and applications. Prentice Hall, Upper Saddle River
 39. Kim JY, Fenton RR, Hunter BA, Kennedy BJ (2000) Powder diffraction studies of synthetic calcium and lead apatites. *Aust J Chem* 53:679–686
 40. Posner AS, Perloff A, Diorio AF (1958) Refinement of the hydroxyapatite structure. *Acta Crystallogr* 11:308–309
 41. de Leeuw NH (2002) Density functional theory calculations of local ordering of hydroxy groups and fluoride ions in hydroxyapatite. *Phys Chem Chem Phys* 4:3865–3871
 42. Ellis DE, Terra J, Warschkow O, Jiang M, Gonzalez GB, Okasinski JS, Bedzyk MJ, Rossi AM, Eon JG (2006) A theoretical and experimental study of lead substitution in calcium hydroxyapatite. *Phys Chem Chem Phys* 8:967–976
 43. de Leeuw NH (2004) A computer modelling study of the uptake and segregation of fluoride ions at the hydrated hydroxyapatite (0001) surface: introducing a $Ca_{10}(PO_4)_6(OH)_2$ potential model. *Phys Chem Chem Phys* 6:1860–1866