**ORIGINAL PAPER**



# **Extended law of laplace for measurement of the cloverleaf anatomy of the aortic root**

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## **Abstract**

The cross-sectional shape of the aortic root is cloverleaf, not circular, raising controversy regarding how best to measure its radiographic "diameter" for aortic event prediction. We mathematically extended the law of Laplace to estimate aortic wall stress within this cloverleaf region, simultaneously identifying a new metric of aortic root dimension that can be applied to clinical measurement of the aortic root and sinuses of Valsalva on clinical computerized tomographic scans. Enforcing equilibrium between blood pressure and wall stress, fnite element computations were performed to evaluate the mathematical derivation. The resulting Laplace diameter was compared with existing methods of aortic root measurement across four patient groups: non-syndromic aneurysm, bicuspid aortic valve, Marfan syndrome, and non-dilated root patients (total 106 patients, 62 M, 44 F). (1) *Wall stress*: Mean wall stress at the depth of the sinuses followed this equation: Wall stress =  $BP \times$  Circumscribing circle diameter/(2 $\times$  Aortic wall thickness). Therefore, the diameter of the circle enclosing the root cloverleaf, that is, twice the distance between the center, where the sinus-to-commissure lines coincide, and the depth of the sinuses, may replace diameter in the Laplace relation for a cloverleaf cross-section (or any shaped cross-section with two or more planes of symmetry). This mathematically derived result was verifed by computational fnite element analyses. (2) *Diameters*: CT scan measurements showed a signifcant diference between this new metric, the Laplace diameter, and the sinus-to-commissure, mid-sinus-to-mid-sinus, and coronal measurements in all four groups (*p-value*<0.05). The average Laplace diameter measurements difered signifcantly from the other measurements in all patient groups. Among the various possible measurements within the aortic root, the diameter of the circumscribing circle, enclosing the cloverleaf, represents the diameter most closely related to wall stress. This diameter is larger than the other measurements, indicating an underestimation of wall stress by prior measurements, and otherwise provides an unbiased, convenient, consistent, physicsbased measurement for clinical use.

## **Graphical abstract**

"Diameter" applies to circles. Our mathematical derivation of an extension of the law of Laplace, from *circular* to *cloverleaf* cross-sectional geometries of the aortic root, has implications for measurement of aortic root "diameter." The suggested method is as follows: (1) the "center" of the aortic root is identifed by drawing three sinus-to-commissure lines. The intersection of these three lines identifes the "center" of the cloverleaf. (2) The largest radius from this center point to any of the sinuses is identifed as the "radius" of the aortic root. (3) This radius is doubled to give the "diameter" of the aortic root. We fnd that this diameter best corresponds to maximal wall stress in the aortic root. Please note that this diameter defnes the smallest circle that completely encloses the cloverleaf shape, touching the depths of all three sinuses.

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**Keywords** Aorta · Aortic root · Sinuses of Valsalva · Aortic diameter · Computerized tomography

## **Introduction**

The ultimate fate of a compromised thoracic aorta—dilatation, dissection, and rupture—depends on the imposed hemodynamic loads and mechanical properties of the wall, that is, on the mechanics. Of particular importance is a measure of the intensity of the force within the aortic wall, often calculated as a mechanical stress. Assessing and understanding values of wall stress are important clinically and scientifcally for two key reasons: the process of aneurysmal dilatation depends in part on mechanobiological responses of vascular cells to changes in wall stress, and dissection and rupture occur when wall stress exceeds wall strength [\[1](#page-11-0), [2](#page-11-1)]. Advances in medical imaging and computational methods now enable detailed calculations of wall stress in the aorta [\[3](#page-11-2)–[5\]](#page-11-3), but these calculations require knowledge of patientspecifc mechanical properties, which evolve as the disease progresses and vary from region-to-region even under normal conditions. Despite continued advances, it remains difficult to estimate the requisite (nonlinear, anisotropic) mechanical properties of the aorta.

For this reason, many rely on the classical law of Laplace, found prominently in engineering and medical textbooks alike. Although the simplicity of this relation, that wall stress is determined by blood pressure, inner diameter, and wall thickness, renders it attractive for use, this relation strictly holds only for an idealized cylindrical geometry. Another seldom appreciated advantage of this relation is its universality: it holds independently of the underlying mechanical properties of the material since it is derived from a force balance (equilibrium) alone. For this reason the law of Laplace always provides the correct mean (radially averaged) value of wall stress in the circumferential direction of a pressurized cylindrical tube [[6](#page-11-4)]. Yet, the complex, non-cylindrical cross-sectional



<span id="page-1-0"></span>**Fig. 1 A** Comparison of (lighter-colored line) "sinus-to-commissure" and (darker-colored line) "sinus-to-sinus" methods of measurement of "diameter" of the aortic root. Reproduced (modifed) with permission from Elefteriades JA, Mukherjee SK, Mojibian H. Discrepancies in measurement of the thoracic aorta. JACC. 76(2);2020:201–17. **B** Note that the imaging plane in this ECHO has visualized both sinuses

"full," not off-axis, misrepresented by a "flat" appearing sinus contour. Reproduced with permission from Goldstein SA, Evangelista A, Abbara S, et al. Multimodality imaging of diseases of the thoracic aorta in adults: from the American Society of Echocardiography and the European Association of Cardiovascular Imaging. J Am Soc Echocardiogr. 2015;28(2):119–82

geometry of the aortic root necessitated a search for an *extended* law of Laplace.

Currently, measurements of aortic diameter critically infuence decisions on surgical aortic intervention. There is, however, a "dirty little secret" in radiographic imaging and measurement of the aorta: it is unclear how best to measure this most anatomically complex site within the aorta, the aortic root [\[7](#page-11-5)]. Measuring the simple diameter of the aorta at diferent positions—ascending, arch, descending, and abdominal—is reasonable only because the lumen is circular in cross-section. By contrast, the aortic root has a 3-lobed cloverleaf cross-sectional shape. There is no defnition for the diameter of such a structure, hence rendering the classical law of Laplace inappropriate for use at the aortic root.

Absent societal guidelines, diferent imaging centers measure the aortic root diferently (Fig. [1](#page-1-0)A). Many centers measure a "diameter" from the depth of a sinus to the opposing commissure; other centers measure a "diameter" from the depth of one sinus to the depth of the opposing sinus. Furthermore, for each of these methods, there are three potential measurements, one for each sinus. If all three sinuses are indeed measured, most centers would likely choose the largest of the three measurements for the representative diameter. Clearly, then, there can be substantial diferences between measurements, with the sinus-to-sinus technique yielding larger measured dimensions. Without consistent techniques, accuracy of follow-up and precision of clinical care will suffer. Furthermore, without consistent techniques, research studies—especially those linking aortic size to adverse clinical outcomes—will also sufer.

One may wonder how echocardiography (ECHO) of the aortic root fts into this paradigm. As rightly taught by experts, the echocardiographer must ensure that both sinuses are full in the images selected for measurement. The plane of the image must be well selected to achieve this goal (Fig. [1B](#page-1-0)). Anatomically, this corresponds most closely to a sinus-to-sinus image on CT or MRI. Not achieving an ECHO image with full sinuses will underestimate the true sinus-tosinus dimension [\[8](#page-11-6)].

With these many considerations in mind, we sought to explore from a bioengineering standpoint the question of what method of measurement of aortic root diameter is more closely related to wall stress and thus preferred for clinical assessment. This paper presents the product of these efforts. It includes (i) a mathematical extension and validation of the law of Laplace from a circular to a cloverleaf cross-sectional shape, and (ii) careful assessment of patient imaging studies to determine which method of aortic root measurement best represents wall stress by the extended Laplace formula. In this way, we identifed a scientifcally motivated defnition for the diameter of the clover-leaf shaped cross-section of the aortic root.

#### **Methods**

This study was approved by the Human Investigations Committee of Yale University.

## **An extended Laplace relation for the clover leaf‑shaped sinuses of Valsalva**

We used a standard balance of forces (equilibrium) and the symmetrical properties of a prototypical aortic root to derive mathematically an extended law of Laplace for a cloverleaf shaped cross-section at the sinuses of Valsalva. Interpretation of this mathematical derivation is limited to the twodimensional oblique plane of the root.

If we defne the center of cloverleaf shaped cross-section as the point where the planes of symmetry, or the three depth-to-commissure lines, coincide (at Point *O* in Fig. [2](#page-3-0)), then the radially-averaged wall stress can be calculated as (see Supplementary Information for a description of the mathematical derivation)

<span id="page-2-0"></span>Wall stress 
$$
\cong
$$
 Pressure  $\times$  Distance from wall to center,  
Wall thickness (1)

which holds for any cross-sectional shape with two or more planes of refective symmetry. Equation [\(1](#page-2-0)) thus reveals that maximum wall tension occurs at the depth of a sinus independent of the specifc material properties. By considering the similarity of Eq. ([1\)](#page-2-0) to Laplace's law for a circular section, the equivalent diameter in a cloverleaf shaped crosssection is defned as twice the distance from sinus depth to cloverleaf center, which equals the diameter of a circle that circumscribes the cloverleaf. Note that these dimensions emerged naturally from the mathematical derivation; they were not selected based on prior experience or hypothesis.

The validity of this extended law of Laplace, derived from frst principles, was assessed by comparison to results from fnite element analyses using two diferent computational programs (commercially available and open source), two diferent material models (linear and nonlinear), and diferent cross-sectional geometries and distending pressures (see Supplementary Information). It can also be seen that this relationship reduces to the classical law of Laplace for circular cross-sections, with  $2 \times$  distance to the center equal to the circle's diameter, which provides additional validation.

#### **Patients**

We next considered clinical data with patients  $(n = 106)$ divided into four groups: those with non-dilated aortic roots (controls), non-syndromic root dilation, Marfan syndrome (MFS), and bicuspid aortic valve (BAV). We



<span id="page-3-0"></span>**Fig. 2** Derivation of an extended Laplace relation for shapes having multiple planes of refective symmetry. **A** The depth of a sinus, *D*, commissure *C*, and the center, *O*, where the planes of symmetry coincide, are used in the derivation of the extended law of Laplace,

Eq. ([1](#page-2-0)), as described in Supplemental Materials. **B** The free body diagram, including a portion of the wall and blood, used in deriving the extended law of Laplace



Values are listed, as appropriate, as the mean $\pm$ standard error

<span id="page-3-1"></span>**Table 1** Patient characteristics

sampled male and female patients by a 1 to 1 ratio, where possible. We used a root index [[11\]](#page-11-7), defined as mean depth to commissure measurement/patient height $2.7$ , to delineate patients in the non-dilated group from those in the non-syndromic dilated group, where patient height was in meters. A cut-off value of 8.5 mm/m<sup>2.7</sup> was used to categorize roots as non-dilated versus dilated. Patient characteristics are listed in Table [1](#page-3-1).

#### **Statistical tests**

Statistical tests were performed using GraphPad Prism (version 9, GraphPad Software Inc, San Diego, California). The Anderson–Darling test was performed to assess data normality. T-test and Mann–Whitney test were performed to compare two groups of measurements. One-way ANOVA test with Geisser-Greenhouse correction followed by Dunnett multiple comparisons test as well as Friedman tests with Dunn's multiple comparisons test were performed to compare multiple groups. Diferences with *p*-*values*<0.05 were considered signifcant.

#### **Area measurements**

The area of the cloverleaves was measured in the oblique plane using ImageJ (National Institutes of Health, Bethesda, Maryland; Ref. 12). An arbitrary measurement was marked on Visage (Visage Imaging, San Diego, California) that was then used for setting the image scale in ImageJ. The periphery of the cloverleaf shaped cross-section was subsequently marked by a polygonal selection, whose area was computed by ImageJ.

# **Results**

# **Validation of the mathematical derivation by fnite element computations**

The extended Laplace relation was derived mathematically using a force balance and a fuid–solid free body diagram. This derivation was validated by comparing results with those obtained using fnite element computational methods. The wall tension values, perpendicular to radii tracing outward from the center, computed by the fnite element model equaled those from the extended Laplace relation (Eq. [1\)](#page-2-0) with high precision in all tested cases (to within 0.01 of a percent), including that for an idealized epitrochoid shape of the aortic root (Fig. [3](#page-4-0)B). The agreement between the two methods, around the perimeter of the cross-section, was independent of the applied pressures over the range 80 to 150 mmHg. Moreover, the independence of the calculated wall stress from a material model and associated parameters in the fnite element computations confrmed the universality of the extended Laplace relation (Eq. [1\)](#page-2-0).

# **Comparison of diferent measurements in the four patient groups**

We quantifed the dimensions of aortic roots at the sinuses of Valsalva using previously employed metrics and the new proposed metric, the Laplace diameter (Fig. [4](#page-5-0)E). Measurements and associated comparisons across all patients are shown for each of the four groups (Fig. [5](#page-6-0)). Although the aortic roots were diferent in size across the four groups, the





<span id="page-4-0"></span>**Fig. 3** Validation of the extended Laplace relation for wall stress at the sinuses of Valsalva using fnite element computations. The fnite element numerical computations of maximum principal stress (open circles), calculated at multiple points around the perimeter of the

cross-section, agree with the mathematically derived (solid curves) extended Laplace relation, Eq. ([1](#page-2-0)). Computations using linear elastic and nonlinear material models produced the same result with high precision, confrming the universality of the extended law of Laplace



<span id="page-5-0"></span>**Fig. 4** Various measurements of aortic root size at the sinuses of Valsalva. **A** Schematic drawing of the aorta with the coronal and double-oblique planes marked at the sinuses of Valsalva. **B** Coronal measurement of aortic size within the coronal plane. **C** Mid-sinus-tomid-sinus (dashed line) and sinus-to-commissure (solid line) measurements within the oblique plane marked in panel (**A**). **D** Laplace

radius is the distance from the center (star) of the cloverleaf, where the three sinus-to-commissure lines coincide, to the depth of a sinus. **E** The Laplace diameter, twice the Laplace radius, is the diameter of the smallest circle enclosing the cloverleaf shape, the circumscribed circle, which touches the depths of the three sinuses

Laplace diameter was signifcantly diferent than each of the other metrics within each group (*p-value*<0.05). The Marfan group exhibited the largest measured Laplace diameters within this cohort, followed by the non-syndromic dilated and then bicuspid aortic valve groups.

# **Correlation of Laplace diameter with the area of the cloverleaf and patient height**

We next assessed possible correlations between the Laplace diameter and two readily measured patient-specifc metrics: the area of the cloverleaf shaped cross-section at the root and patient height. Cloverleaf area was found to scale with Laplace diameter via a power-law with an exponent between 1 and 2 (Fig. [6\)](#page-7-0). An exponent equal to 1 would indicate a linear correlation, whereas 2 would correspond to a uniform expansion of the cloverleaf with no change in shape. Observation of an exponent smaller than 2 agrees with the clinically observed change in shape of the cloverleaf shaped cross-section in more dilated roots. The linear correlations between the Laplace diameter and patient height

were stronger in the non-dilated group  $(R^2 = 0.62)$  than in the non-syndromic dilated, Marfan, and bicuspid groups  $(R^2=0.37, 0.21,$  and 0.23, respectively).

## **Efect of asymmetry of the sinuses in the bicuspid patients**

The derivation of the extended Laplace relation relies on the existence of two or more planes of symmetry within the cloverleaf shaped cross-section of the aortic root. These shapes were not all symmetric, however. For example, the symmetry condition was absent in roots where the cusps were not of the same size. Especially in the case of the bicuspid aortic valves, we visually observed a relatively larger number of asymmetrically dilated roots (Fig. [7](#page-8-0)). We thus quantifed the asymmetric dilatation of the roots via a twostep approach. First, we found the mean value of the three sinus-to-commissure dimensions in a single root; second, we found the relative deviation of each measurement from the mean. The calculated relative deviations were signifcantly higher in the bicuspid group compared with baseline, the



55 B Non-syndromic 50 Measurement (mm) dilated 45 40 35 30 25 Mid-sinus to Depth to Coronal Laplace mid-sinus commissure dimension diameter 55 D **Bicuspid** 50 Measurement (mm) 45 40 35 30 25 Depth to Mid-sinus to Coronal Laplace mid-sinus commissure dimension diameter

<span id="page-6-0"></span>**Fig. 5** Comparison of the Laplace diameter with other measurements across four diferent patient groups suggests that wall tension is generally underestimated in the cloverleaf shape of the aortic root. The coronal dimension was measured as in Fig. [4](#page-5-0). The error bars indi-

non-dilated group (*p-value*<0.05), as seen in Fig. [7](#page-8-0)E. We point out that the assessed roots were only mildly asymmetric, and in these cases we expect the extended law of Laplace to reasonably estimate wall stress. Moreover, in case of an asymmetrically dilated root, a conservative estimate may be made using twice the distance between the center of the cloverleaf and the depth of the most dilated sinus as the diameter.

## **Efect of the less protruded shape of the root in the Marfan syndrome patients**

The derivation of the extended law of Laplace suggested that the most dramatic diferences between the Laplace diameter and sinus-to-commissure measurements should emerge in aortic roots with more protruded sinuses. Various degrees of protrusion presented in the set of assessed roots. For instance, in the Marfan group, roots frequently exhibited more round / circle-like shapes, with less protruded sinuses, compared with the non-dilated group, which included more protruded sinuses (Fig. [8\)](#page-8-1). We quantifed the diferences in the protrusion of sinuses in these two groups by calculating acircularity of the cloverleaf

cate standard errors. The Laplace diameter difered signifcantly (\*) from each of the three other measurements in each of the four groups

shaped cross-sections at the root. Acircularity was measured by the relative diference in the diameters of the circles enclosed by and enclosing the cloverleaf shape (Fig. [8](#page-8-1)E, *inset*). A signifcant diference was observed in the relative acircularity of the non-dilated versus the Marfan roots ( $p$ -value < 0.05). That is to say, with the more severe deformity of the root in Marfan patients, the normal distinct sinus confguration (with normal, substantial protrusion of the sinuses) gave way to a more circular root shape.

## **Real world clinical application**

 $(p-value < 0.05)$ 

In order to assess clinical applicability and intra- and interobserver reliability, we applied the Laplace measurement technique to the most recent 24 consecutive, unselected patients seen in consultation (office of JAE) who had high quality CT scans available for analysis (official radiology reports with aortic root measurements were available for 18 of the 24 patients).



<span id="page-7-0"></span>**Fig. 6** Variation of the Laplace diameter with either area of the cloverleaf or patient height in each of the four patient groups. The correlation between Laplace diameter and patient height is stronger in the non-dilated group as compared with that in the other three groups. In panels **A**, **B**, **E**, and **F**, both axes are plotted logarithmically. A few patients from the four groups were not included in the correlation

analysis because the related data was unavailable at the time of this analysis. Note that the dashed lines are plotted to show power-law relations with exponents 1 (linear) and 2 (quadratic). The solid lines represent (**A**, **B**, **E**, and **F**) power-law and (**C**, **D**, **G**, and **H**) linear fts to the data



<span id="page-8-0"></span>**Fig. 7** The diference of the measurements in the diferent cusps increases in asymmetrically dilated roots. The cloverleaf shape of the root appears more asymmetric in the group of patients with bicuspid aortic valves (two bicuspid cases shown in panels **A**–**D**) compared

with the baseline, the non-dilated group. The non-coronary (NCS), left-coronary (LCS), and right-coronary sinuses (RCS) are marked in panels A and B



<span id="page-8-1"></span>**Fig. 8** Diferences between the Laplace diameter and the sinus-tocommissure measurements are smaller if the cloverleaf shape of the root appears more round and less protruded. A rounder shape is observed in the roots in Marfan syndrome. Snapshots of high acircularity versus circularity are shown in the cases of (**A** and **B**) nondilated and (**C** and **D**) Marfan syndrome groups. **E** Quantitative com-

parison of acircularity between the non-dilated and Marfan groups, which differed significantly (\*, *p-value* < 0.05). The *inset* displays the (dashed) circumscribed and (dotted) inscribed circles for an idealized root geometry. The diference in the diameters of the two circles was used in evaluating cloverleaf acircularity

#### **Comparative diameters by various techniques**

In this group of patients, aortic root diameter by the Laplace technique ranged from 30.4 mm to 59.5 mm, with a mean of 41.6 mm. These Laplace diameters were larger than the root diameters measured in the standard radiology reports (range 27 mm to 47 mm, mean 37.3 mm). The conventional coronal aortic root measurements were larger than root diameters

provided in radiology reports in 17 of the 18 patents (mean difference of 2.5 mm, range 0 to 4.1 mm). The Laplace diameters (above) were larger even than the coronal root diameters measured conventionally by our team (range 26.3 mm to 50.0 mm, mean 38.3 mm). Diameter of the aortic root in coronal views was measured by scrolling anteriorly and posteriorly and selecting the image with the largest diameter. Hence: Standard measurements<Coronal measurements<Laplace measurements.

Measurement types Radiology report measurements $(nm)(n=18)$	Mean		Range	
	37.3		$27.0 - 47.0$	
	Reader 1 (JAE)	Reader 2 (BAZ)	Reader 1 (JAE)	Reader 2 (BAZ)
Conventional Coronal Aortic Root Measurements (mm)	38.3	39.0	$26.3 - 50.0$	$29.3 - 49.6$
Laplace Aortic Root Measurements (diameter, mm)	41.6	44.4	$30.4 - 59.5$	$33.0 - 57.6$
Difference in Conventional Coronal Aortic Root Measure- ments between Reader 1 and Reader 2 (mm)	1.5		$0 - 6.7$	
Difference in Laplace Aortic Root Measurements (radius) between Reader 1 and Reader 2 (mm)	1.6		$0.2 - 2.9$	

<span id="page-9-0"></span>**Table 2** Quantifcation of inter-observer variability in measurements

#### **Intra‑observer variability**

Two observers (JAE and BAZ) independently measured the aortic roots by the Laplace technique on two separate occasions, one week apart. The absolute aortic root diameter diferences between the two measurement sessions ranged from 0.2 mm to 2.4 mm, mean 0.9 mm for one observer (JAE) and between 0 and 2.2 mm, mean 0.6 for the other observer. The intra-observer variability, analyzed by the Intra-class Correlation Coefficient (ICC)  $[13]$  $[13]$  $[13]$  was 0.96 (JAE) and 0.97 (BAZ).

#### **Inter‑observer variability**

A second experienced reader (BAZ) read the Laplace diameters independently (of JAE). The absolute aortic root radius diferences between the average of two measurements obtained by the two observers ranged from 0.2 to 2.9 mm (mean 1.6) (Table [2](#page-9-0)). The inter-observer variability ICC index was 0.89. Values of the Intra-class Correlation Coeffcient (used in this analysis for inter- and intra-observer variability calculations) between 0.75 and 0.9 show good reliability, and any value above 0.9 indicates excellent reliability [[13\]](#page-11-8).

#### **Discussion**

Thoracic aortic aneurysm and dissection (TAAD) is responsible for signifcant morbidity and mortality, with conservative estimates ranging up to 15,000 deaths/year in the USA alone [\[14\]](#page-11-9). Advances in genetics and medical screening continue to increase the number of TAADs diagnosed each year, which suggests that many prior dissection or rupture related deaths may have been falsely ascribed to other causes, including heart attack. In fact, among patients suffering outof-hospital cardiac arrest undergoing peri-mortem diagnostic CT scan, a staggering 8.07% had succumbed to undiagnosed aortic dissection [[15\]](#page-11-10). Even more troublesome is that thoracic aortic dissections are the cause of death in over 5%

of all young people suffering sudden cardiac death  $[16]$  $[16]$ ; that is, these lethal conditions afect young and old alike. There is clearly a pressing need for increased understanding.

Notwithstanding concerns with aortic diameter as a reliable metric of risk for acute aortic syndromes  $[17–19]$  $[17–19]$  $[17–19]$  $[17–19]$ , this easily measured quantity yet continues to play a critical role in clinical decisions [\[20\]](#page-11-14). Because the aorta dissects or ruptures only when the mechanical stress exceeds the strength of the wall, many authorities also continue to suggest a similar need to calculate and compare values of wall stress [\[21](#page-11-15)[–23](#page-11-16)]. For reasons noted above, however, there has been considerable variation in the measurement of aortic root diameter and no truly reliable method to estimate wall stress. We believe that in the future, with the advancement of methods for determining material stifness and strength properties, having fnite element computations in the decision loop will potentially provide a promising aid to clinical patient evaluation. However, in the absence of material parameters and image-based fnite element computations in everyday practice, the presented enhanced Laplace method addresses a pressing need for mechanistic tools that inform decisions related to the Sinuses of Valsalva.

Herein, we suggest an extended law of Laplace that provides a simple, universal estimate of wall stress in the aortic root that overcomes challenges with both the inappropriate use of the classical law of Laplace and insufficient information on patient-specifc material properties needed for image-based fnite element calculations. Moreover, this simple derivation revealed a reliable, easily measured, metric—the Laplace diameter—that promises to help delineate risk across diferent classes of aneurysms based on medical images of the aortic root. The intra-observer and interobserver variabilities for our Laplace technique of aortic root measurement fall well within the ranges usually found for traditional measurements of aortic diameter, where "Variations in AAA measurement of 0.5 cm or more are not uncommon…" [[24–](#page-11-17)[26](#page-11-18)].

As illustrative results, we found that this Laplace diameter was signifcantly larger than three other commonly used measures of aortic root dimensions, suggesting further that the prior measurements of diameter led to underestimating wall stress. Importantly, the Laplace diameter did not correlate strongly with patient height in the three aneurysmal groups considered–non-syndromic, bicuspid, and Marfan. Rather, the Laplace diameter correlated well with the cross-sectional area at the aortic root, consistent with it being primarily a measure of size ( $R^2$ =0.96, non-dilated group). As expected, the other measurements are also related to the size of the root and correlate rather well with cross-sectional area  $(R^2=0.95$  for depth-to-depth and depth-to-commissure measurements, and  $R^2$  = 0.93 for coronal measurements within the non-dilated group). With practice, determining the Laplace diameter becomes a simple method to quantify aortic size, providing an appropriate indicator of severity of wall stress (see accompanying video, demonstrating application of the Laplace measurement technique). These Laplace metrics, however, depend on the existence of certain symmetries within the aortic root. Of the cases considered, the aortic root in patients with bicuspid aortic valve exhibited a lack of root symmetry, thus necessitating careful evaluation of root shape, not just size, and warranting caution in the use of these metrics in these cases. In cases of symmetry, however, the extended law of Laplace and the Laplace diameter upon which it is based provides quick, straightforward assessments. It is suggested that these metrics can be added to others to increase risk stratifcation in regression-based predictive models [[27\]](#page-11-19). Finally, we hope that the proposed method would complement previous efforts in measurements of the aortic root structure [[28,](#page-11-20) [29\]](#page-11-21) and contribute to more uniform analysis of the root dimensions.

# **Conclusion**

In this study, we addressed head-on issues with discrepant methods of measurement of the aortic root—issues originating from its non-circular, cloverleaf shaped cross-section. Using fundamental mathematical calculations, we extended the classical law of Laplace specifc for the cloverleaf shaped cross-section at the aortic root. This work exploits basic force balances and particular symmetries in geometry; it was thus not an experimentally determined modifcation of the law of Laplace, but rather a purely mathematical derivation. Like the classical law of Laplace, this extended law is universal, thus determining radially-averaged circumferential wall stress in aortic roots having two or more planes of symmetry, independent of specifc material properties. We then confrmed the validity of the mathematical derivation using computational fnite element analyses with an idealized root geometry defned by an epitrochoid and other symmetric geometries such as ellipses, triangles, and diamonds and various values of material parameters for both linear and nonlinear material descriptions. The wall stresses calculated from the fnite element computations and the extended law

of Laplace (Eq. [1\)](#page-2-0) agreed with high precision. In the cloverleaf cross-sectional geometry of the Sinuses of Valsalva, the extended law of Laplace introduces the diameter of the circumscribed circle as the primary dimension related to wall stress. The Laplace diameter was larger than the sinusto-commissure, the mid-sinus-to-mid-sinus, and the diameter in the coronal plane, suggesting that the other measurements would underestimate the wall stress. Regardless, this Laplace diameter offers a new, theoretically motivated approach to measure and compare aortic root dimensions uniformly across centers.

#### **Perspectives/clinical competencies**

This manuscript analyzes in detail multiple factors involved in achieving well motivated and consistent measurements of the aortic root. The root portion of the aorta is anatomically complex and is quantifcation has been problematic in terms of intra- and inter-institutional methodology, subject to high variability and little uniformity. The geometric analyses herein should be of use to clinicians of all levels of experience. The derivation of an extended law of Laplace in this manuscript applies basic geometric and mechanical principles and more accurately represents maximal wall stress. This extension of Laplace has implications in terms of optimal methods of measuring the "diameter" of a cloverleaf shaped cross-section. We hope that this analysis and these recommendations may encourage standardization of measurements of the aortic root in a geometrically justifed fashion.

**Supplementary Information** The online version contains supplementary material available at<https://doi.org/10.1007/s10554-023-02847-5>.

**Author contributions** This study was approved by the Yale University Human Investigation Committee. All authors contributed substantially to this work. The concept was originated by JAE and JDH. The mathematical/engineering concepts were fashioned by EB, RK, ABR, and PDK. MAZ, HE, and BAZ analyzed clinical data. The Laplace CT scan reads were done by BAZ and JAE. The frst draft was written by EB (engineering) and JAE (clinical) and reviewed, edited, and revised by all authors.

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#### **Declarations**

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**Conflict of interest** Drs. Ban, Kalogerakos, Khosravi, Ziganshin, Ellauzi, Ramachandra, and Zafar have no disclosures. J.D. Humphrey: Member of the Scientifc Advisory Board who also receives consulting fees from HeartFlow, Inc., a company using computational modeling to assess coronary artery disease. J.A. Elefteriades: Principal, CoolSpine. CoolSpine has no clinical products.

**Ethical approval** This study was approved by the Yale University Human Investigation Committee.

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