



# Myco-engineered gold nanoparticles from *Jahnula aquatica* coated with ampicillin/amoxicillin and their antibacterial and anticancer activity against cancer cells

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## Abstract

**Introduction** Antibiotics play an important role in medical treatments. However, the multidrug resistance (MDR) bacteria impairs their functionality. Therefore, drug delivery represents the solution for this problem. Many techniques and methods are used in drug delivery, however nanoparticles conjugated drug is one of the most effective and promising techniques. The current work investigates a one-step method of extracellular biosynthesis of gold nanoparticles (AuNPs) and their biocompatibility in antibiotic delivery, where the synthesized AuNPs were loaded with Ampicillin/Amoxicillin.

**Results** Both ampicillin and amoxicillin antibiotics are successfully conjugated with the Au NPs surface (the potential efficiency), especially, at the smaller particle size. Where, the Au NPs with particle size of 8 m size reveals a promising activity against cancer cells with 48 µg/mL inhibitory concentration (IC<sub>50</sub>) after 24 h of their exposure to HeLa cells, and

induction of apoptosis was also noticed on HeLa treated cells.

**Conclusions** The bio-synthesised Au NPs using *Jahnula aquatica* fungi show a promising nanocarrier biocompatibility drug delivery system in cancer clinical treatments, in particular for antibiotics delivery antibiotics in pharmaceutical applications with large-scale commercial production. To the best of our knowledge, freshwater fungi have never been exploited for AuNPs synthesis.

**Keywords** Gold nanoparticles · Antibiotics · Antibacterial and anticancer · Drug delivery

## Introduction

Antibiotics play an important role in curing almost of infection problems (Delcaru et al. 2017). However, the excessive usage have impaired their function that appears as a resistance by bacteria against the curing drug or what is know as multi-drug resistance (MDR), which is real global threat and one of the greatest challenges for healthcare practitioners (Lien et al. 2017). The β-lactam antibiotics represent a wide potential base against different resistant drug bacteria (Sotgiu et al. 2016), however, the level of antibiotic bacterial resistance is increasing contentiously, decreasing the antibiotic efficiency (Baroud et al. 2013). According to the global antibiotic free curing plan, new alternative strategies have been proposed

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overcome the continued outgrowth of antibiotic bacterial resistance (Tang et al. 2016). Antibiotics synergism with the same/different mechanism is widely common and leads to a clinical delay of antibiotic resistance if utilized wisely (Miliani et al. 2011; Sun et al. 2014; Yang et al. 2016; Paczkowska et al. 2016). Another promising solution is to insert an antibiotic molecules inside a complex agent from in vivo hydrolysis in the human body. However, more efforts are required to confirm the degree of safety and stability of these complexes. Recently, different nanocarriers are available for constructing unique types of drug delivery systems at the nanoscale including liposomes, dendrimers, polymers, carbon materials, silicon, and magnetic nanoparticles (NPs) (Brown et al. 2012; Rastogi et al. 2012; Thomas et al. 2014; Gannimani et al. 2016; Kandimalla et al. 2016; Roy et al. 2018). Consequently, extensive researches are still ongoing in the delivery system area to address the most reliable and effective methods to fix the above mentioned problem.

Nanoparticles conjugated drug is one of the most effective and promising techniques in intracellular delivering antibiotics. Among all nanomaterials, gold nanoparticles (Au NPs) have attracted the attention due to their cytotoxic effect on cancer cells without a damage of the normal cells, which introduce these NPs in cancer clinical treatment (Cui et al. 2012; Patil et al. 2017). Their wide usage refers to the high safety profile, biocompatibility with the human body, unique covalent binding and electrostatic adsorption of their surface (Kandimalla et al. 2016; Mori and Hegmann 2016; Foo et al. 2017; Kim et al. 2017; Maity et al. 2018). Au NPs are synthesized using in several physical and chemical methods, and almost of these methods are energy intensive (Dhamecha et al. 2016; Yuan et al. 2017a, b). However, many synthesis methods involves toxic chemicals that precluding their use in numerous pharmaceutical and medical areas (Yuan et al. 2017a, b). Recently, biological synthesis of gold nanoparticles has become more attractive than physical and chemical methods due to safety, low cost and various shape (size, and morphology) (Kasthuri et al. 2009; Balasooriya et al. 2017). Fungi are good option in comparison with other biological methods such as bacteria and plants. This is because of fungi contains high amount of proteins, enzymes, and other biomolecules that have the ability of redox capacity, increasing the productivity during the nanomaterials synthesis (Kasthuri et al.

2009). Till now, there are more than six hundred fungal species of ascomycetes and anamorphic that have been discovered from freshwater ecosystems. However, few studies that have focused on the chemical/biological properties (Hernández-Carlos and Gamboa-Angulo 2011). Therefore, not much information are available about their metabolites potential and its properties that may be wisely used and exploited in different applications including nanotechnology.

In this work we investigate the extracellular synthesis and drug delivery functionality of mycogenic gold nanoparticles using the *Jahnula aquatica* fungus. This is achieved via uploading Ampicillin/Amoxicillin antibiotics on top of different sizes of gold NPs. This is in addition to the evaluation of the anticancer effect against human cancer cell lines with fundamental molecular techniques to understand the cytotoxicity mechanism against HeLa cancer cells in vitro. As far of author's knowledge, there is no reported results in the exploitation of the freshwater fungi generally in nanomaterials synthesis.

## Materials and methods

### Chemicals

Gold chloride hydrate (analytical grade) was purchased from Sigma-Aldrich. The Au NPs were loaded with Ampicillin (Amp.) and Amoxicillin (Amox) purchased from Astra-Zeneca (Boston, Massachusetts, USA) in a Pharmaceutical analytical grade. Human cervical carcinoma cell lines (HeLa) were obtained from the American Type Culture Collection (ATCC, MD, USA).

### The freshwater fungus

The freshwater fungus *Jahnula aquatica* was isolated according to the single-spore isolation technique (Choi 1999) from submerged woody debris collected from Ju car River in Spain 2015, and morphologically identified following the corresponding keys and the relevant literatures (Goh and Hyde 1999). However, species identification under genus *Jahnula*, based only on morphological criteria, may not prove absolutely accurate. Thus, molecular identification was applied for additional confirmation. Thus, the genomic DNA of the fungal isolate was purified as reported by (Abdel-Hafez

et al. 2016). The ITS was amplified and sequenced. Alignment with *Jahnula aquatica* rDNA in NCBI GenBank (JN942348.1) resulted in a 100% identity match.

#### Biosynthesis of gold nanoparticles (AuNPs)

Au NPs were biologically synthesized using the freshwater fungus *Jahnula aquatica* aqueous extract as reducing/capping agent. The synthesis process was conducted with varied reaction conditions to obtain different Au NPs sizes of 8 nm, 20 nm and 60 nm, the details are reported elsewhere with some modification (Poojary et al. 2016).

#### Au NPs- antibiotics conjugation

The conjugation of Au NPs and antibiotics were prepared by adding 4 ml of the antibiotics under study in (1 mg/ml in PBS, pH 7.4) concentration drop wise to 10 ml from the Au NPs in different sizes of 8 nm, 20 nm and 60 nm with continuing magnetic stirring for two hours at room temperature. The change in the surface plasmon resonance (SPR) of the conjugated Au NPs was measured using UV–visible spectroscopic analyse in the range of 200–800 nm. The extra unloaded antibiotic molecules were collected by centrifugation the Au NPs mixture solution at 20,000 rpm for 20 min. The percentage (%) of loading efficiency in percentage of antibiotic content attached on the Au NPs surface were evaluated by measuring the unloaded antibiotics content in the residual supernatant of the mixture solution by UV measurements in the range of 300 and 295 nm for Ampicillin and Amoxicillin, using Eqs. 1 and 2, respectively (Rohman et al. 2015).

#### Drug loading efficiency (%)

$$= \frac{[(\text{Total antibiotic} - \text{antibiotic in supernatant}) / \text{total amount of the antibiotics}] \times 100}{(1)}$$

#### Drug content (%)

$$= \frac{[(\text{Total antibiotic} - \text{antibiotic in supernatant}) / \text{amount of AuNPs} + (\text{Total antibiotic} - \text{antibiotic in supernatant})] \times 100}{(2)}$$

Moreover, we measured the possibility of adsorbed antibiotics in the inner surface of the centrifugation tube by centrifuging 3 ml mixture solution from both Ampicillin and Amoxicillin (1 mg/ml) at 30,000 rpm for 20 min. The results show the same antibiotic content the produced supernatant, which excludes the possibility of Amp./Amox. adsorption in the centrifuge wall. And the results of UV spectroscopic analysis of supernatant excludes the interfering possibility of the Au NPs supernatant with Ampicillin/Amoxicillin as well. The scanning spectra indicated the lacking of any interfering absorption at the measurement range of wavelengths. The abbreviations AuNPs, Amp-AuNPs and Amox-AuNPs were used to refer the formed gold nanoparticles, Ampicillin conjugated AuNPs and Amoxicillin conjugated gold nanoparticles, respectively, while the subscripted number adjacent to the proposed abbreviation refers to nanometer size of the formed gold nanoparticles.

#### Au NPs characterization

##### *UV–visible spectrometric analysis*

The gold solution was sampled for different times to monitor the bio-reduction of Au NPs and also to evaluate their stability over 1 month. The UV–visible spectrum of the sampled solution was measured using a UV–visible spectrophotometer (Shimadzu UV-1800) at wavelengths ranged in the 200–800 nm.

##### *High resolution transmission electron microscopy (HR-TEM)*

The Au NPs shape and size characteristics were measured using a JEOL 3010 instrument operated at an accelerating voltage of 300 kV. Briefly, the HR-TEM samples were prepared by drop coating Au NPs solution onto carbon coated copper TEM grids. The prepared films on the TEM grids were allowed to stand for 5 min for dryness, while the extra solution was erased using a blotting paper.

### *The dynamic light scattering (DLS) and zeta potential analysis*

The NPs size and Zeta value of Au NPs in aqueous phase potential were evaluated using particle size analyser (ELSZ-1000, Otsuka, Japan).

### *X-ray diffraction (XRD) analysis*

The XRD technique was examine crystallinity of Amp/Amox before and after the conjugation with the Au NPs using a Bruker AXS D8 Advance X-ray diffractometer with Cu K radiation of wavelength 1.541 Å and scanning angle 2  $\theta$  in (10°–90°) range.

### *Fourier transform infrared (FT-IR) analysis*

FT-IR analysis was performed to confirm the conjugation of Amp/Amox with the Au NPs. 10 mg of the Amp/Amox conjugated Au NPs powder mixed with a pinch of potassium bromide (Himedia FT-IR graded) in a crucible were used for FT-IR measurement. The mixture was pelletized by hydraulic press and the pellet was analysed in Jasco FT/IR-6300 equipped with JASCO IRT-7000 Intron Infrared Microscope with transmittance at range a 4 cm<sup>-1</sup> resolution (JASCO, Tokyo, Japan).

### *Drug release*

The degree of antibiotics release was investigated via the membrane dialysis technique in vitro as reported in (Harsha 2012; Onuigbo et al. 2016; Yuan et al. 2017a, b). 5 ml of antibiotic was loaded on AuNPs (3 mg/ml in PBS, pH 7.4) and left over-night soaked dialysis bags, (MWCO 3500 Daltons). The inoculated bags were slowly transferred to a sterilized closed bottles containing 50 ml of the same buffer and maintained at 37 °C with shaking at 100 rpm. A small amount (5 ml) from the released media were taken over a course of time and replaced by fresh phosphate buffer solution (PBS) medium. The amount of Ampicillin and Amoxicillin released in the media was analyzed by UV–visible spectrophotometer (Shimadzu UV-1800) at 318 nm and 295 nm, respectively.

### *Au NPs antibacterial activity*

#### *Bacterial Antibiotic susceptibility*

Different infectious bacterial isolates were collected with a permission from the clinical laboratories of Kasr El-Ainy Hospitals, University of Cairo, Egypt. The Gram negative bacteria were purified and maintained following the standard protocols and confirmed to specific species according to Bergey's manual (Boone et al. 2001). The antibiotic susceptibility against each bacterial isolate was evaluated following disk diffusion assay method under the Clinical and Laboratory Standards Institute guidelines (CCLS) in 2015. The bacterial isolates: *Pseudomonas aeruginosa*, *Staphylococcus aureus* (MRSA), and *Enterobacter aerogenes* were selected as a result of their high resistant activity against both antibiotics (Amp and Amox). Identification of MRSA was confirmed according to the recommendations of the National Committee for Clinical Laboratory Standards. Thus, they were selected for the present study.

#### *The minimum inhibitory concentrations (MICs)*

The MICs of Amp, Amox and their conjugation with the AuNPs were determined for the used bacteria using the micro titre assay method. Each bacterial strain was firstly inoculated on a fresh Muller-Hinton (MH) growth medium and incubated for 12 h at 37 °C. Then, 2- fold serial dilutions from Amp and their equivalent amounts from Amp-AuNPs and from Amox-AuNPs respectively were prepared in a concentration of (640–1.25 µg/ml) in MH broth medium. The cultivated bacterial plates were diluted to 1 × 10<sup>6</sup> CFU/ml concentration and then inoculated with the antibiotic dilutions. All the inoculated bacterial plates were placed for incubation at 37 °C for 24 h. All the practical experiments were repeated three times and the free AuNPs were served as a negative control. The MIC values for all treatments were considered as the least concentration of used agent that is completely impair the bacterial colony growth.

#### *Antibiotic's loaded AuNPs time kill test*

The rate of antibiotic's loaded AuNPs in killing the resistant bacteria under the study was carried out by

performing a time kill assay experiments for both antibiotics individually (Amp, Amox) and also in loading form (Amp-AuNPs8, Amox-AuNPs8) against *Pseudomonas aeruginosa* and *Staphylococcus aureus* and compare them with untreated ones. Briefly, the bacterial strains were cultured in Luria–bertani (LB) medium reaching  $1 \times 10^6$  CFU/ml. Then, the bacterial suspension for each strain was challenged with the treatments: Amp, Amp-AuNPs8, Amox and Amox-AuNPs8 till final concentration 2.5 µg/ml for *S. aureus* and 1.25 µg/ml for *P. aeruginosa* and incubated at 37 °C. At different time intervals (0, 1, 2, 4, 8, 12, and 24 h), the samples were withdrawn and diluted 10 folds to count the number of viable bacterial colonies using the surface drop method (Shameli et al. 2012).

#### Cytotoxicity analysis of AuNPs

The cytotoxicity of the 8 nm Au NPs on the proliferation of HeLa cells was analyzed by the MTT (3-(4, 5-dimethylthiazol-2-yl)-2, 5-di phenyl tetra-zolium bromide) assay. Firstly, the, HeLa cancer cells were cultivated in DMEM supplemented with antibiotic agents (penicillin 120 IU/mL and streptomycin 100 IU/mL) and 10% (v/v), fetal bovine serum (FBS) and non-essential amino acids. Then, the cultivated cells were maintained in a humidified atmosphere of 5% Carbon dioxide (CO<sub>2</sub>) at 37 °C. Briefly, the cells were grown to  $1 \times 10^5$  cells/well in 96 well plates and then incubated with various different AuNPs concentrations (15, 30, 60, 125, 250 and 500 µg/mL) at 37 °C with 5% CO<sub>2</sub> for 24 h. After treatment with varied AuNPs concentrations, the treated Hela cells were extensively washed with PBS with changing the medium to remove the dead cells. The cytotoxicity and the inhibitory concentration (IC<sub>50</sub>) was calculated by incubating the treated HeLa cells with 300 µL (1 mg/mL) of MTT for 3 h in 5% CO<sub>2</sub> incubator. The mitochondrial dehydrogenases reduce the MTT medium with the yellow tetrazole characteristic color into purple formazan in the living cells. Higher number of living cells resulted in increasing optical intensity of the purple color. Micro-plate Reader (Bio Rad, M-680) was used to analyze the measurement of MTT assay by color development using a spectrophotometer at 540 nm after the removal MTT solution and cell lysis in

DMSO (600 µL). The cytotoxicity level was evaluated following the equation:

$$\% \text{ Cell viability} = \frac{\text{(Optical density (OD) in sample well)}}{\text{Optical density (OD) in control well}} \times 100$$

#### Apoptotic Effects

##### *Acridine orange (AO) and ethidium bromide (EtBr) stain*

The acridine orange/ethidium bromide staining technique was used firstly to measure the apoptosis effect of AuNPs on Hela cells and also to differentiate between active and non active proliferating cells. Briefly, 10 µl of AO/EtBr were gently added to the treated cells on a clean glass slide. The stained slide was then incubated for 5–7 min at 22 °C. The treated cells showing apoptotic characters with and deformed condensed chromatin with fragmented nuclei were observed by the appearance of their red fluorescence in contrast to the normal cells that appear by their shin green fluorescence. This was counted by using epifluorescence microscopy (Eclipse 80i, Nikon, Japan) at  $\times 40$  magnification with excitation filter centered at 510–590 nm.

##### *DAPI Staining*

The nuclear apoptosis of AuNPs was also tested by preparing two equal concentrations ( $1 \times 10^5$ ) from untreated and treated HeLa cells. The treated cells were washed several times with the phosphate solution and fixed with 3.7% paraformaldehyde in PBS for 1 h under normal temperature, and finally stained with DAPI solution for 15 min at 37 °C. Finally, the epifluorescence microscopy (Eclipse 80i, Nikon, Japan) at  $\times 40$  magnification with excitation filter at 510–590 nm was used to investigate the treated cells.

##### *Ultra-thin sections*

Ultra-thin sections from the AuNPs treated cancer cells were prepared in order to study the localization of AuNPs inside those cells. HeLa cells were firstly washed with PBS, detached by trypsinization and

centrifuged at 12,000–14,000 rpm for 10–12 min after 24 h incubation with 4 µg/mL AuNPs, and untreated cells were served as control. The medium without nanoparticles was used as control in the experiment. The treated cells were then fixed with 2.5% glutaraldehyde for 24 h, followed by post-fixation in 1% osmium tetroxide for 2 h and dehydrated with different ethyl alcohol concentrations (10%, 20%, 40%, 60%, 70%, and 80%). The dehydrated cells were then treated with 2% Uranyl-acetate in 95% for 1 h followed by 100% ethanol for the same time. Then, the cells were subjected two times to propylene oxide for 15–20 min each, followed by 1:1 propylene-oxide: araldite resin overnight, and infiltration with fresh araldite resin. Finally, the HeLa cells were embedded for 2 days in araldite resin at 60 °C. The ultra-thin sections were then prepared using an ultra-microtome (Leica EM UC6, Netherlands) instrument. The prepared sections were finally stained with 1% uranyl acetate and 0.2% aqueous lead citrate and mounted on a carbon-coated copper grid (carbon type-B, 300 mesh, Ted Pella, Inc., Redding, CA, USA). The prepared stained sections were finally scanned under a Hitachi H-7500 HR-TEM microscope at 100 kV for ultra-structural observations.

#### DNA fragmentation analysis

The effect of AuNPs on the DNA of HeLa cancer cells was performed following the method presented in (Barbosa et al. 1995). Briefly, the HeLa cells were firstly plated on DMEM medium contained 10% FBS in 6 well plates with a concentration ( $1 \times 10^6$  cells/mL) per well. The plates were incubated under 5% CO<sub>2</sub> at 37 °C for 24 h, followed by removing the DMEM medium and extensively washing the plated cells with the Phosphate buffer. Fresh serum free medium was then added and incubated under carbon dioxide at 37 °C for 1 h. The cells were then treated with the IC<sub>50</sub> conc. of the formed AuNPs and incubated again for 24 h. The DNA was then extracted from the treated cells as follows: The cells were properly washed with PBS three times; 0.5 ml of lysis buffer was then added followed by incubation for the mixture solution at 37 °C for 1 h. Small aliquots (4 µL) from proteinase K was added with raising the incubation temperature for 50 °C for 3–4 h. Then, About 0.75 mL of phenol:chloroform:isoamyl alcohol (25:24:1) was added, mixed and centrifuged at

12,000–14,000 rpm for 30 min under cooled conditions. Then two equals volumes from sodium acetate (3 M) and ethanol (iced) solutions were slowly poured and the mixture then was incubated for 1 h on ice to precipitate the nucleic acid (DNA). The DNA was then centrifuged at 14,000 rpm for 10–15 min under cooled conditions 4 °C. The supernatant was discarded and the nuclei acid pellets were properly washed with 1.0 mL of 70% ethanol. The genetic (DNA) pellet was then dried and re-suspended in 50 µl of TE buffer. Finally, 10 µg/mL of the treated DNA samples were separated by electrophoresis using a 1% agarose gel at 75 V for 45 min. The gel was stained with ethidium bromide and then subjected to UV irradiation to photograph the nucleic acid (DNA) bands.

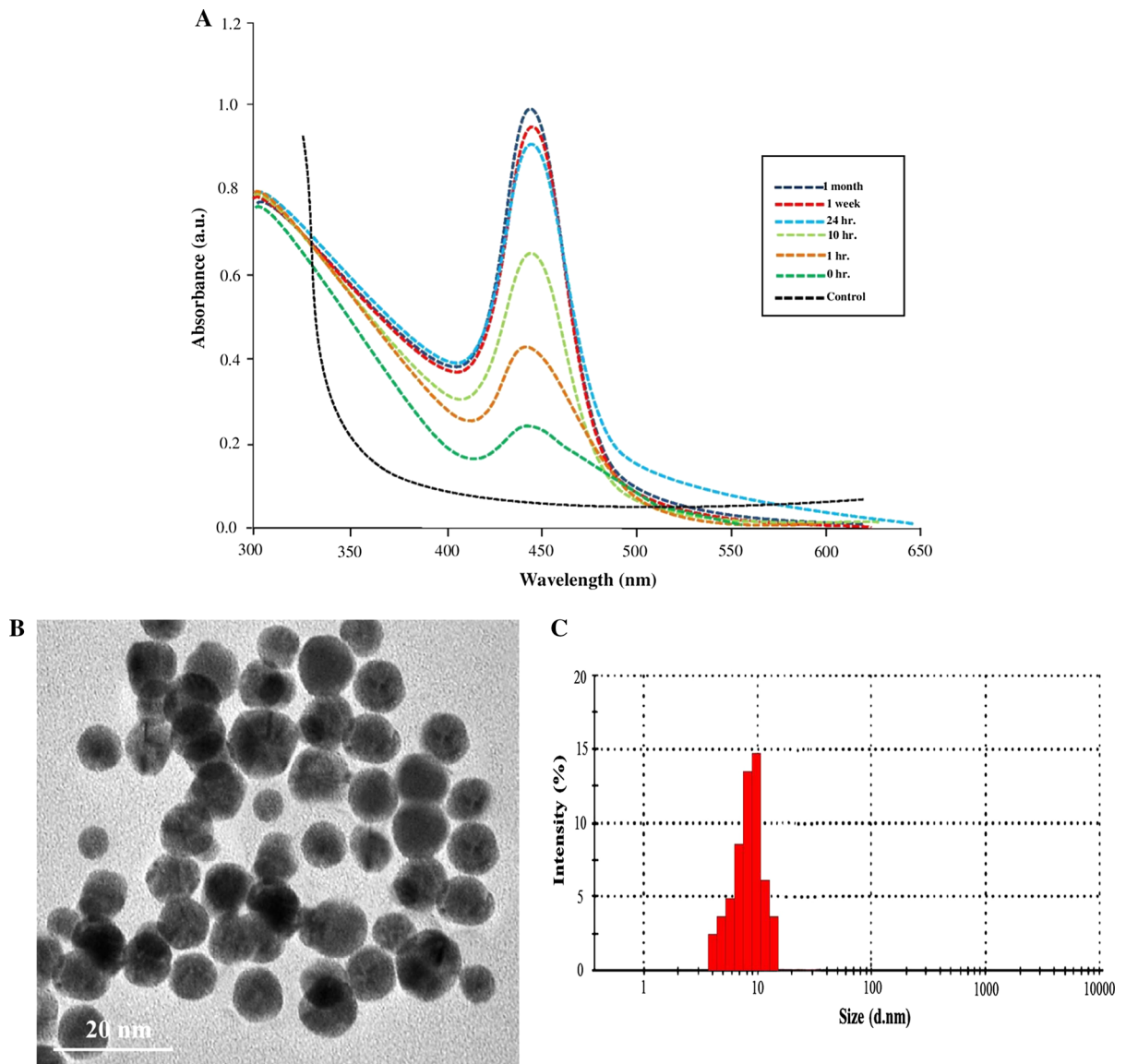
#### Statistical analysis

All the obtained data were statistically analysed using Origin 8.0 version. Three replicates of each experiment were used and the differences between data values were only significant if the p value was < 0.05.

## Results and discussion

#### Au NPs synthesis

The change in color of the gold salt solution from dark yellow to dark wine red (~ 5 min) after challenging with *J. aquatica*, fungal extract suggests the formation of spherical shaped AuNPs. The UV–vis absorption spectra indicate the appearance of strong absorption peak centered at 540 nm, revealing the formation of gold nanoparticles (Fig. 1a), and confirms the formation of mono-dispersed Au NPs (Shameli et al. 2012). It is worth to mention that the intensity of the absorbance peak and broadness decrease with time progress as shown in (Fig. 1a), which indicates long time stability of the formed Au NPs (Chen and Li 2007). Consequently, the maximum peak intensity is accomplished after 48 h of reaction, meaning that a complete reduction of the AuCl<sub>4</sub>—ions. These findings indicate that the freshwater fungal extracted *J. aquatica* is a promising natural reducing agent for synthesizing high concentrations of Au NPs at room temperature (26 °C), without any waste products. On the other hand, the obtained results show the formation



**Fig. 1** Mycosynthesis of the formed gold nanoparticles: **a** UV-vis spectra of the formed AuNPs (60 nm) at different times as indicated during the synthesis and after 1 month of storage,

of spherical shaped nanoparticles with particle size of  $60.4 \pm 1.2$  nm size and  $-43.5 \pm 0.5$  mV zeta value, indicating an ideal surface charge (Fig. 2a). Furthermore, the zeta potential absolute value indicates a high electrical charge on the Au NPs surface (Fig. 1a), causing a strong repulsive force between the particles to avoid agglomeration and therefore might be liable for their elevated stability and does not change the pink color solution even after 1 month storage at room temperature. Interestingly, the UV-spectra of the

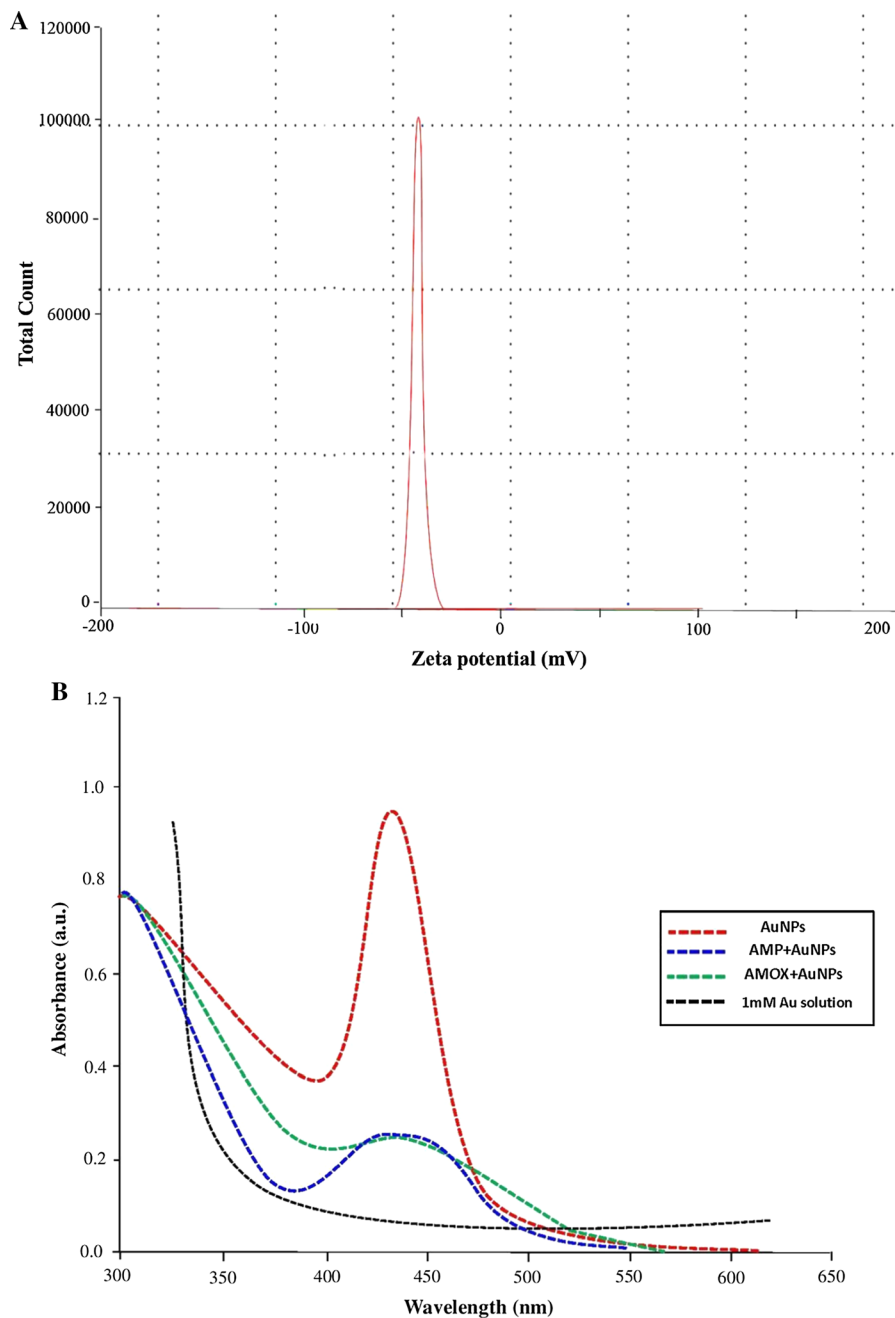
**b** HR-TEM image of the mycosynthesized AuNPs at 60 nm scale, and **c** Particle size distribution

conjugated Au NPs with antibiotics do not show any red/blue shift when in comparison with the spectra of the pure Au NPs. This illustrates the stability of the conjugated AuNPs without aggregation (Fig. 2b).

#### Characterization of the AuNPs

Raising the reaction temperature to 70 and 90 °C leads to a smaller size of the resultant Au NPs with  $20 \pm 2.6$  and  $8 \pm 0.9$  nm sizes, respectively (Fig. 1b–c, 3a, b).

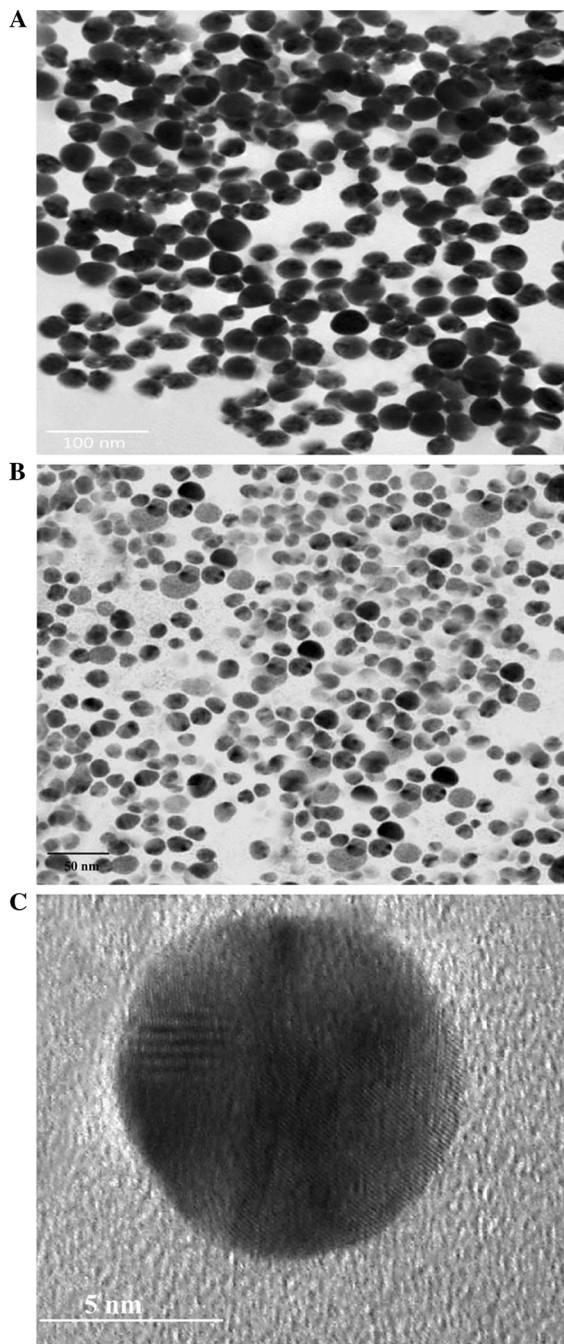
**Fig. 2** Characterization of the formed AuNPs: **a** Zeta potential measurements of the formed AuNPs  
**b** conjugation of gold nanoparticles (8 nm) with Ampicillin (Amp-AuNPs) and Amoxicillin (Amox-AuNPs)



These findings are in agreement with the fact that the reactants consumption is directly proportional with the reaction temperature (Baghizadeh et al. 2015). Data analysis of zeta potential of the free Au NPs indicates the negative surface charge for the particles with 60 nm, 20 nm and 8 nm ( $-43.5 \pm 0.5$ ,  $42 \pm 1.2$ ,  $39.1 \pm 0.2$ ) mV, respectively, revealing the high stability during storage. The slight decrease in zeta

value with AuNPs size may be attributed to the increase in the *J. aquatica* concentration that works as a reducing agent during the synthesis process and the process can be accelerated with raising up the reaction temperature. In contrast, the antibiotics conjugated Au NPs show lower zeta potential values, this refers to the positive charges of the loaded antibiotics on the Au NPs surfaces. Thus, uncovers the ramifications of





**Fig. 3** Optimization and tuning the AuNPs size: **a, b** HR-TEM images of the mycosynthesized AuNPs at 20 and 8 nm sizes respectively. **c** Ampicillin loaded gold nanoparticles (8 nm)

intermolecular electrostatic attraction in the Ampicillin/Amoxicillin molecules and the nano gold particles conjugation (Fig. 3c) (Dhar et al. 2008). The XRD patterns for the Ampicillin/Amoxicillin molecules and

their conjugation with the Au NPs with particle size of 8 nm are shown in (Fig. 4a). The figure shows multiple peaks, revealing the stability and polycrystalline nature of both antibiotic molecules. These peaks are in correspondence with (111), (200), (220), and (311) crystalline planes of the face-centered cubic structure of the metallic gold (space group  $Fm\bar{3}m$ , JCPDS File NO. 89-3697), respectively. This is in agreement with the reported results of (Kandimalla et al. 2016). Figure 4b, c shows the FTIR for the Amp, Amox, free Au NPs, AuNPs- Amp-and Amox-AuNPs. The spectra for both Amp and Amp-conjugated Au NPs show broad absorption bands at  $3350\text{ cm}^{-1}$  and  $3270\text{ cm}^{-1}$  that refers to the stretching vibrations of the ( $-\text{OH}$ ) group in Amp. The observed broadness in these bands may be attributed to the intermolecular existence of the hydrogen bonds in these molecules. The absorption peaks at  $2956\text{ cm}^{-1}$  and  $2870\text{ cm}^{-1}$  refers to the stretching of  $\text{N}-\text{H}$  and  $\text{C}-\text{H}$  bonds in Amp, respectively. Similarly, the IR spectra for pure Amox and Amox-AuNPs show bands at  $3490\text{ cm}^{-1}$  and  $3390\text{ cm}^{-1}$  that may be attributed to the stretching vibrations of the ( $-\text{OH}$ ) functional group in Amox. Also, the peaks at  $3035\text{ cm}^{-1}$ , and  $2870\text{ cm}^{-1}$  may be attributed to the stretching of the amide  $\text{N}-\text{H}$  and the aliphatic  $\text{C}-\text{H}$  bonds, respectively, in contrast with the absorption peak at  $3576\text{ cm}^{-1}$ , which coming up due to the stretching of amide ( $\text{N}-\text{H}$ ) bond of the pyrrolidine ring and peaks at  $2989\text{ cm}^{-1}$  and  $2935\text{ cm}^{-1}$  are for the stretching of the aliphatic  $\text{C}-\text{H}$  in the dimethyl carbanoyl moiety of Amox. Also, the spectra of the Amp and its conjugation with AuNPs also demonstrate the peaks centered at  $1779\text{ cm}^{-1}$ ,  $1740\text{ cm}^{-1}$ ,  $1657\text{ cm}^{-1}$  and  $1585\text{ cm}^{-1}$  refers to stretching vibration of the carbonyl functional group ( $\text{C}=\text{O}$ ) found in the  $\beta$ -lactam ring,  $\text{C}=\text{O}$  of the ( $\text{COO}^-$ ) functional group, amide I and II bands, of Amp respectively. Furthermore, the peaks at  $1464/1447\text{ cm}^{-1}$ ,  $1390/1235\text{ cm}^{-1}$ ,  $1075/1035\text{ cm}^{-1}$ ,  $995/957\text{ cm}^{-1}$ ,  $897/802\text{ cm}^{-1}$  refer to the stretching of  $\text{C}=\text{N}$ ,  $\text{C}=\text{C}$ ,  $\text{N}-\text{C}-\text{S}$  moiety containing plane vibration,  $\text{C}=\text{C}$  bending and  $\text{C}-\text{C}$  of the Amp, respectively. Similarly, the peaks at  $724\text{ cm}^{-1}$  and  $692\text{ cm}^{-1}$  refer to the bending of  $\text{C}-\text{N}-\text{H}$  and  $\text{C}-\text{O}-\text{H}$  bonds of the Amp, respectively. Likewise, the spectra of the Amox and its conjugation with Au NPs (Amox-Au NPs) illustrate that the peaks at  $1759\text{ cm}^{-1}$ ,  $1705\text{ cm}^{-1}$ ,  $1657\text{ cm}^{-1}$  and  $1509\text{ cm}^{-1}$ , which are due to the stretching of carbonyl ( $\text{C}=\text{O}$ ) in the ( $\text{COO}^-$ ) group, in beta lactam

ring vibration, in amide group, and in amide group (N–H) bending of the Amox respectively. Furthermore, the dual peaks at  $1609/1545\text{ cm}^{-1}$ ,  $1456/1390\text{ cm}^{-1}$ ,  $989/946\text{ cm}^{-1}$ ,  $888/817\text{ cm}^{-1}$ ,  $779/715\text{ cm}^{-1}$  and  $554/527\text{ cm}^{-1}$  are attributed to C=C stretching, the aliphatic C–H, CH<sub>3</sub>, C–C stretching, C–N–H bending and C–C–C bending, of the Amox respectively. Similarly, the peaks centered at  $1335\text{ cm}^{-1}$ ,  $844\text{ cm}^{-1}$  and  $617\text{ cm}^{-1}$  are suggested to be attributed to the aliphatic C–H stretching in pyrroline, C–H and C–O–H bending, of the Amox respectively. Meantime, the symmetric/asymmetric stretching of C–S absorption peaks for both the Amp and the Amox appear at  $662\text{ cm}^{-1}$  and  $567\text{ cm}^{-1}$  wave length. Most importantly, the IR spectra also shows that a noticeable decrease was recorded in the first peak intensity occurred after the surface conjugation with AuNPs (Amp-AuNPs and Amox-AuNPs) and shifted to a lower wave number by  $36\text{--}40\text{ cm}^{-1}$ . This significantly reveals that the thio-ether functional group chemisorbed on the AuNPs surface by bonding the sulphur atom (S) with the metallic gold surface. Assignment of the above produced peaks either in the free formed gold nanoparticles or those conjugated with Amp and Amox also confirms their association on the formed AuNPs surface. Additionally, the intensity decrease for the C–S peak, this also reveals that sulphur atom in the thio-ether moiety is full incorporate in the antibiotic self-assembled monolayer on the gold nanoparticles surface.

#### Cytotoxicity of AuNPs and their intracellular localization inside viable cells

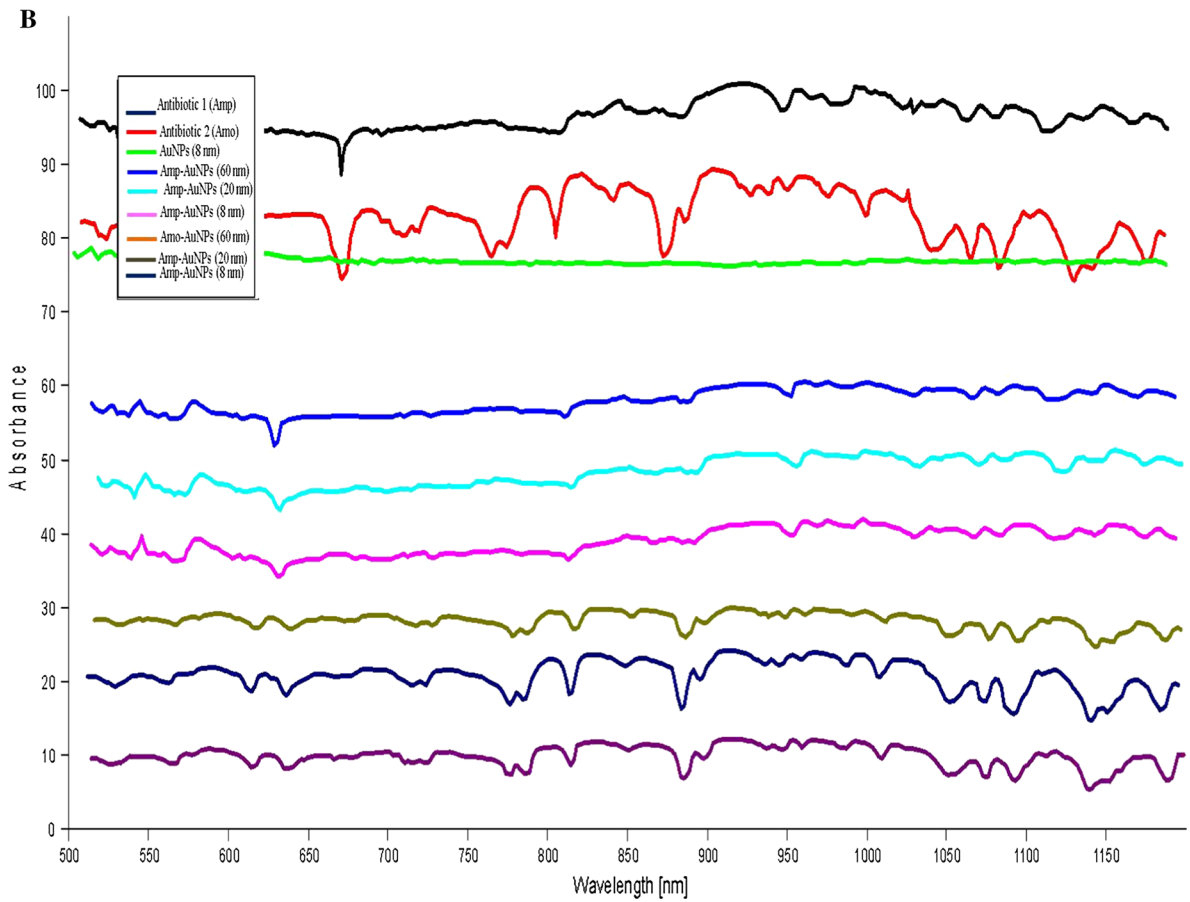
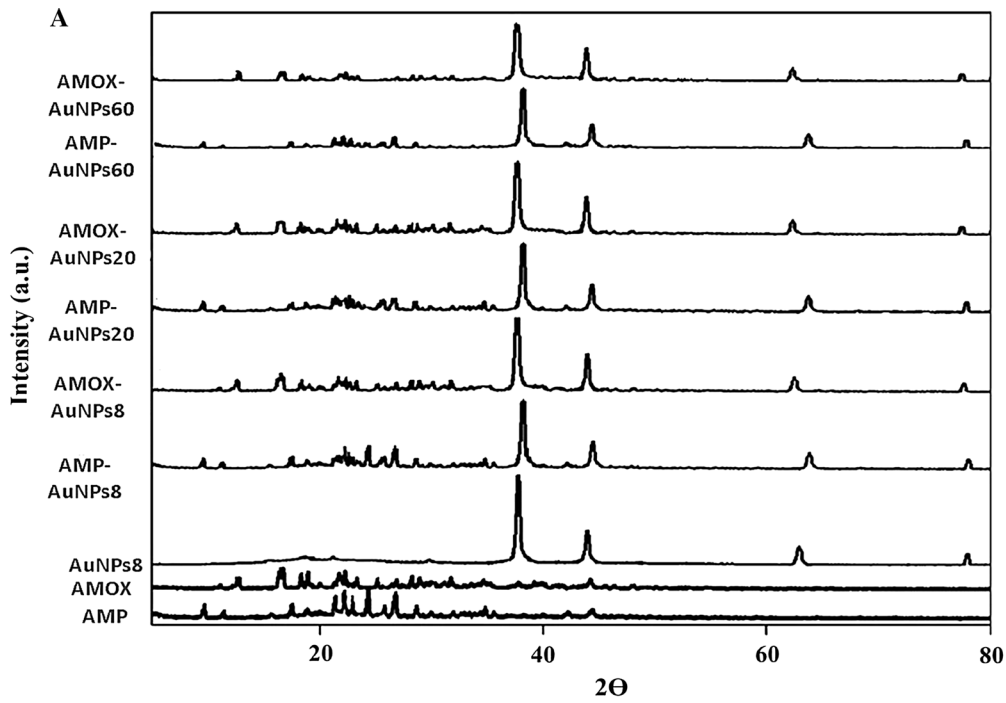
The toxicity of the 8 nm AuNPs and their cellular uptake inside the living cells is a key factor for evaluation their safety and also utility in biomedical and drug delivery applications (Guo et al. 2014). In this regard, the cytotoxicity of the AuNPs was evaluated in vitro against the cell lines in terms of their effect in various concentrations viz., 15.0, 30.0, 60.0, 125, 250 and 500  $\mu\text{g/ml}$  on cell proliferation by the MTT assay. The results show that the dependent toxicity and the IC<sub>50</sub> of AuNPs on HeLa cells is 48  $\mu\text{g/mL}$  after 24 h of their exposure on HeLa cells. In reality, the metallic nanoparticles may fortify the reactive oxygen species (ROS) and effect in damage cellular components that ultimately lead to cell death (Vivek et al. 2012). On the other hand, the TEM

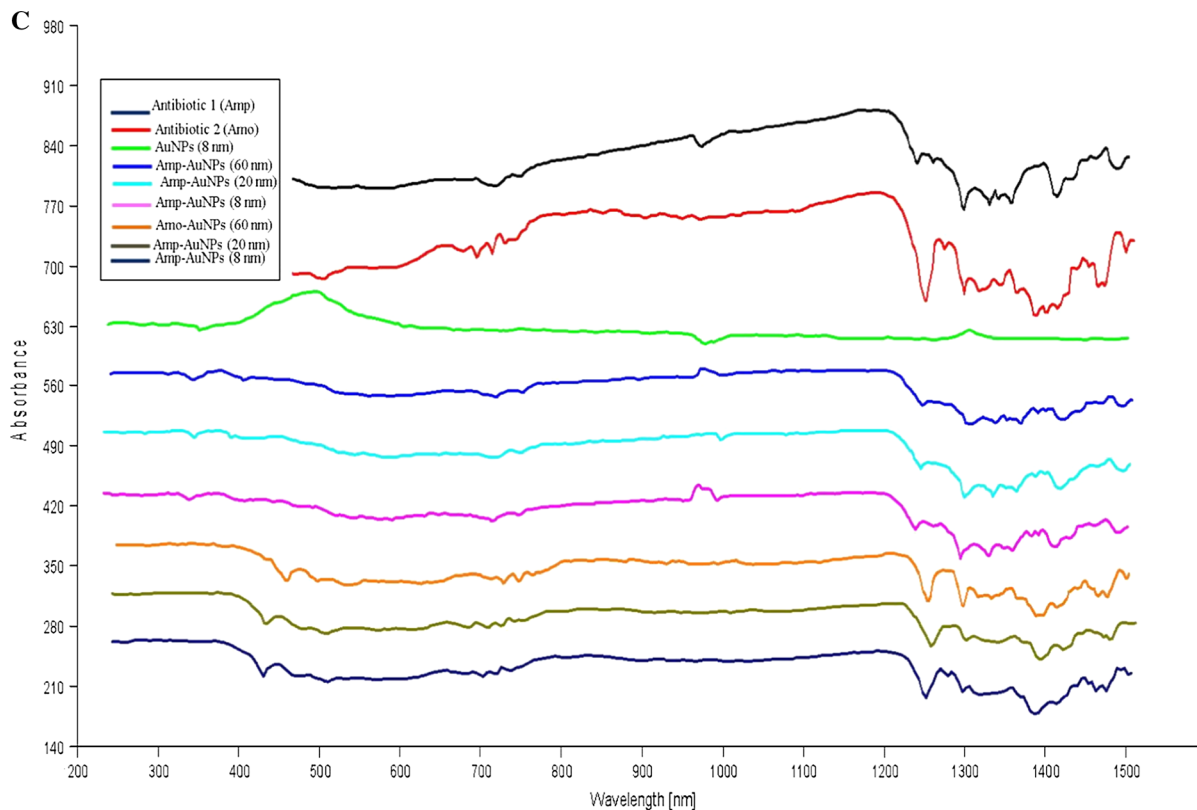
**Fig. 4** Characterization of the AuNPs and their conjugation with Amp, Amox. **a** X-ray diffraction pattern of Ampicillin (Amp), Amoxicillin (Amox), 8 nm diameter gold nanoparticles (AuNPs), Ampicillin loaded gold nanoparticles, Amoxicillin loaded gold nanoparticles, **b** FT-IR spectra of Ampicillin, Amoxicillin, gold nanoparticles, Ampicillin conjugated gold nanoparticles, and Amoxicillin conjugated gold nanoparticles) in the range of  $1200\text{--}500\text{ cm}^{-1}$  **c** FT-IR in the range of  $4000\text{--}1200\text{ cm}^{-1}$

analysis proves the successful entry of the Au NPs into the treated HeLa cells in comparison to the untreated cells (Fig. 5a). These nanoparticles were founded agglomerated inside the treated cells and localized inside the endosomes (Fig. 5b, c), revealing their internalization were through endocytosis, however further studies are needed to fully understand and elucidate their uptake mechanism inside the living cells.

#### Effect of Au NPs on HeLa cells nucleic acid

The results show an induced cytotoxic effect by the Au NPs, including different apoptotic changes and nuclear condensation with fragmented/marginated chromatin structure as demonstrated by the AO/EtBr and DAPI staining methods. Furthermore, a complete nuclear damage with clear chromatin fragmentation was observed in the fluorescence images of the treated cells, without any evidence of nuclei breaking in the untreated Hela cells (Fig. 6). Based on the AO/EtBr stain observation, it is clear that the mechanism of cell death induced by AuNPs occurs via apoptosis. Where the orange color of the apoptotic/necrotic cells appears in red color in contrast with untreated controlled cells that appear healthy with green color (Fig. 6a, b). The results are in agreement with the nuclear degradation/fragmentation behavior in AuNPs treated cells that was reported by (Patra et al. 2007; Guo and Lu 2010; Khelifi et al. 2013; Alnasser et al. 2016). However, the confirmation of AuNPs penetration into cell membrane is still in progress. Those findings also were revealed by gel electrophoresis analysis, which showed clear intact DNA bands without any fragmentation or smearing with the untreated DNA (control), where there was no significant damage occurred. In contrast, the DNA of cells treated with IC<sub>50</sub> concentration of AuNPs show the induction of apoptosis in interspersing smears in the lanes and substantial alter





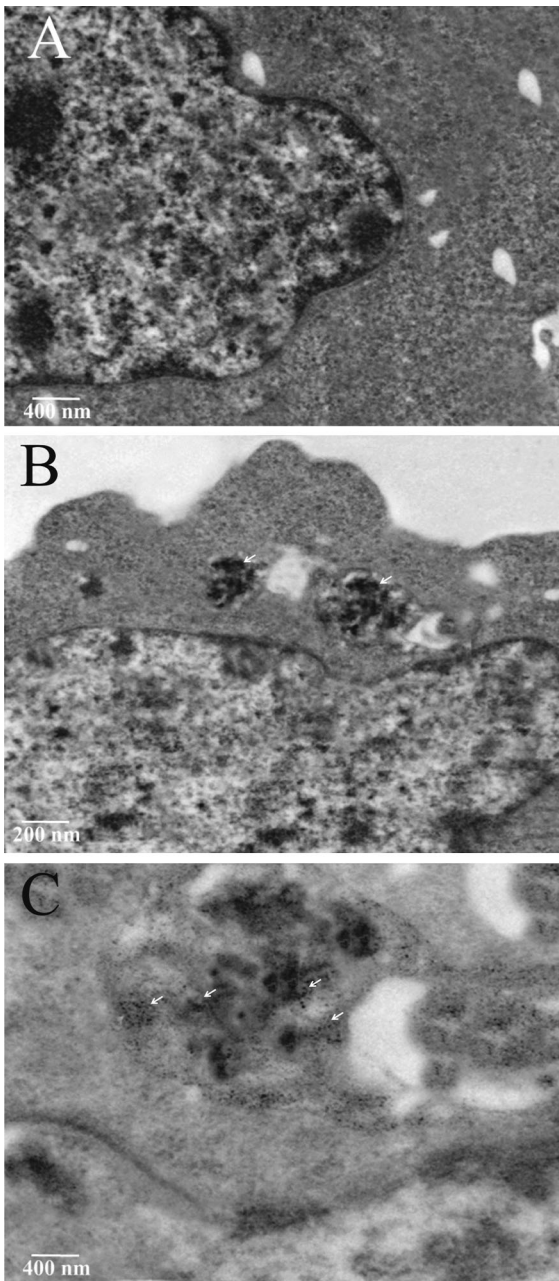
**Fig. 4** continued

the electrophoretic migration within a time period of 24 h (Fig. 7). The smearing of DNA could occur due to some post-apoptotic HeLa cell necrosis. The results suggest that the decrement in the cell survival is caused by induction of DNA fragmentation and its direct chemical damage (Sriram et al. 2010). In this regard, the effect of Au NPs cytotoxicity on the HeLa cells is attributed to the potentiality of the mitochondrial dehydrogenase enzyme in the viable cells to cleave the tetrazolium rings of the pale yellow MTT and produce formazan crystals with blue color, which is hard to pass through the cell membranes (Konwarh et al. 2011). The NPs size and dose play a key role in toxicity due to the presence of protein/enzyme on their surfaces (Bellman 2015). While, the variability in cellular responses to the Au NPs may support the distinctive surface reactivity modulated by the presence of cytotoxic enzymes/proteins, contaminants, other poly-morphs and surface imperfections (Shi et al. 2015; Patil et al. 2018). The obtained results

reveal the toxicity effect of Au NPs on cancer cells by inducing apoptosis in HeLa cells.

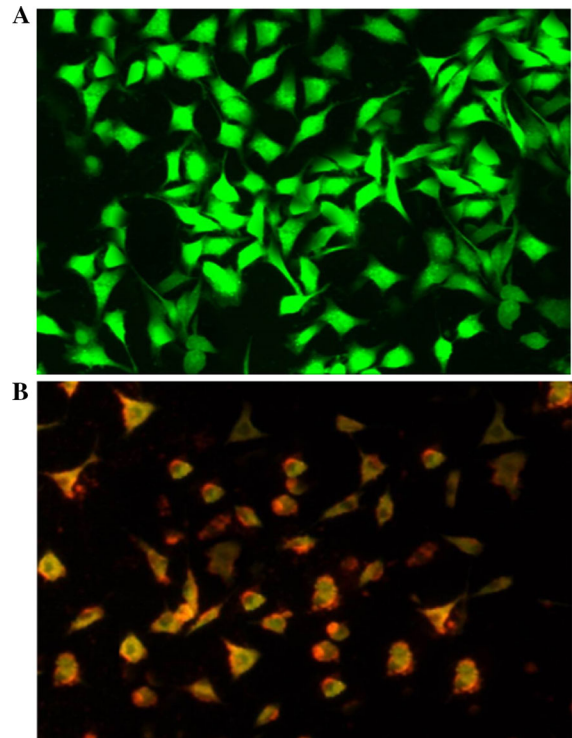
#### Ampicillin/Amoxicillin drug release (In-vitro)

Figure 8a, b shows the kinetics of drug release rate of Au NPs conjugated Ampicillin and Amoxicillin for different Au NPs sizes. The figure indicates a controlled release for ampicillin and Amoxicillin from the conjugated AuNPs surfaces. Interestingly, two biphasic release profiles are observed for both Ampicillin and Amoxicillin. The first short term and rapid release rate take about 6 h followed by a relatively slow steady and long term drug release, which is extended to a complete release for all the drug loaded on the AuNPs's surface. It is worth to mention that the drug release rate depends on the size of the Nano-carrier system exploited in the loading process (Table 1). Where, the smaller AuNPs (8 nm) the faster drug release rate (92%) after 24 h and archives

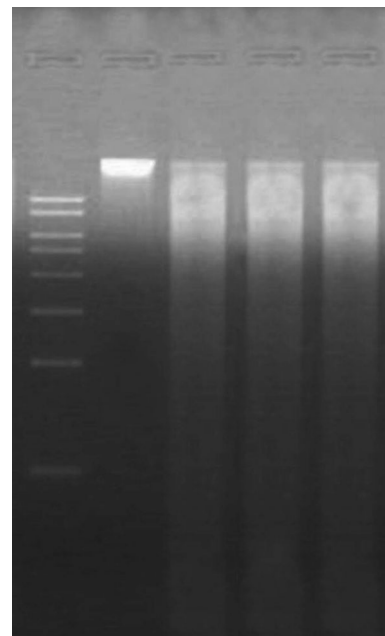


**Fig. 5** Uptake and localization of AuNPs in HeLa cells: **a** control (untreated cells), **b** AuNPs-treated HeLa cells for 24 h showing AuNPs aggregates in the endosomes as black and electron dense spots (indicated by arrows). **c** Showing a cluster of individual nanoparticles inside treated cells

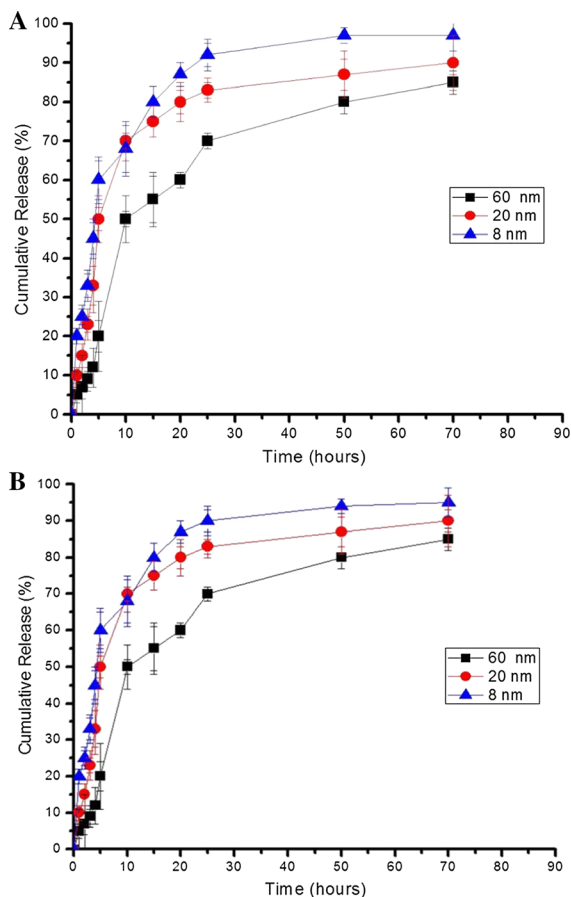
96% after 48 h, in contrast to the larger AuNPs of 60 nm that shows a release rate of 70%, 80% after 24 and 48 h, respectively. Similar results are also recorded for Amoxicillin. This significant behavior



**Fig. 6** Cytotoxic activity of the formed AuNPs: **a** fluorescence microscopic study of DAPI staining of control HeLa cells **b** gold nanoparticles treated HeLa cells



**Fig. 7** DNA fragmentation of HeLa cells treated with biosynthesized AuNPs at 24 h: Lane 1: 1 kb DNA ladder, Lane 2: HeLa control DNA, Lane 3, 4 and 5: AuNPs treated (48 µg/mL)



**Fig. 8** Cumulative percentage of released Ampicillin: **a** and Amoxicillin (**b**), from the loaded gold nanoparticles of different particle sizes (8, 20 and 60 nm) in PBS (pH 7.4) as a release media at 37 °C

is correlated to the larger surface area-to-volume ratio of the smaller AuNPs they obtained compared to the larger NPs. Thus, higher amount of the loaded drug with the same volume of NPs giving a higher

probability of the drug molecules repulsion, leading to faster diffusion through the dialysis membrane. On the other hand, the AuNPs show a larger cores volume as the amount of the loading drug (Ampicillin/Amoxicillin) decreases, this means less repulsion force between the drug molecules and leads to slower release rate. Consequently, smaller tuned AuNPs size smaller, higher ampicillin/amoxicillin releasing rates.

On the other hand, the drug content for Ampicillin and Amoxicillin conjugated gold nano-particles was about  $88.2 \pm 4.8\%$  and  $82.4 \pm 9.4\%$ , respectively in case of the smallest AuNPs (8 nm). So, each milligram of Amp-AuNPs<sub>8</sub> and Amox-AuNPs<sub>8</sub> contains 0.88 and 0.82 mg of Ampicillin and Amoxicillin, respectively. The 20 nm nanoparticles showed  $70.5 \pm 6.2\%$  and  $72.8 \pm 5.6\%$ , loading for Ampicillin and amoxicillin, respectively. As well, the 60 nm nanoparticles showed a  $74.2 \pm 10.2\%$  and  $67.6 \pm 7.5\%$ , loading for Ampicillin and Amoxicillin, respectively. It should be mentioned that the measured Amp/Amox content in the supernatant was found to be the same to exclude the possibility of adsorption on the wall of the centrifuge tube. Meanwhile, the possibility of interfering of the supernatant of AuNPs with Ampicillin/Amoxicillin measurement was also excluded by the UV scanning of supernatant obtained after centrifugation of the prepared nanoparticles at 20,000 rpm for 30 min.

#### Antibacterial activity

Fifty-five Gram-negative bacterial isolates belong to *Pseudomonas aeruginosa*, *Enterobacter aerogenes*, and *Staphylococcus aureus* were assessed in vitro to study their susceptibility to Ampicillin (Amp) and Amoxicillin (Amox). The lowest susceptible bacterial

**Table 1** Drug loading efficiency in relation to different sizes (8, 20, 60) nm of the biosynthesized gold nanoparticles (AuNPs)

Gold nanoparticles form	Loading efficiency (%)	Drug loading (%)
AuNPs <sub>8</sub> (alone)	–	–
AuNPs <sub>40</sub> (alone)	–	–
AuNPs <sub>80</sub> (alone)	–	–
Amp-AuNPs <sub>8</sub> (conjugated)	$78 \pm 2.1$	$88.2 \pm 4.8$
Amp-AuNPs <sub>20</sub> (conjugated)	$59 \pm 1.0$	$70.5 \pm 6.2$
Amp-AuNPs <sub>60</sub> (conjugated)	$45 \pm 2.7$	$74.2 \pm 10.2$
Amox-AuNPs <sub>8</sub> (conjugated)	$71 \pm 2.5$	$82.4 \pm 9.4$
Amox-AuNPs <sub>20</sub> (conjugated)	$57 \pm 1.5$	$72.8 \pm 5.6$
Amox-AuNPs <sub>60</sub> (conjugated)	$47 \pm 2.3$	$67.6 \pm 7.5$

isolates to Amp and Amox were selected to evaluate the antibacterial activity of Amp, Amox, and their conjugated formulations with the AuNPs (Amp-AuNPs and Amox-AuNPs). According to data presented in Table 2, the incubation of the unloaded Au NPs with either *Pseudomonas aeruginosa*, *Staphylococcus aureus* and *Enterobacter aerogenes* at 37 °C for 24 h did not show any suppression in the pathogenic bacterial growth. While, the bacterial growth suppression is observed with both free Ampicillin, Amoxicillin and with conjugated Au NPs. Interestingly, the results clearly prove that both conjugated Au NPs show higher antibacterial activity in comparison with the pure Au NPs. The antibacterial activity of conjugated Amp AuNPs are in the order of Amp -AuNPs8 > Amp -AuNPs20 > Amp -AuNPs60 > Amp. Similarly, for Amox, it is in the order of Mem-AuNPs8 > Amox -AuNPs20 = Amox -AuNPs60 > Amox. Meaning, that as the Amp/Amox formulated AuNPs size decrease as their antibacterial activity increase. This is also supported by the 3–4 folds decrease in the MIC value for the Amp -AuNPs versus *P. aeruginosa*, respectively. While, the Amp -AuNPs20 and Amp -AuNPs60 reduce the MICs values only by 2-fold, respectively. On the same way, Amox loaded AuNPs8 significantly decreases the MICs of the Amox versus *S. aureus* and *E. aerogenes* by more than 2–3 folds, respectively. Hence, it can be concluded that the Amp-AuNPs8 and Amox -AuNPs8 versus Gram negative Antibiotic-resistant isolates introduce a superior activity in comparison with to

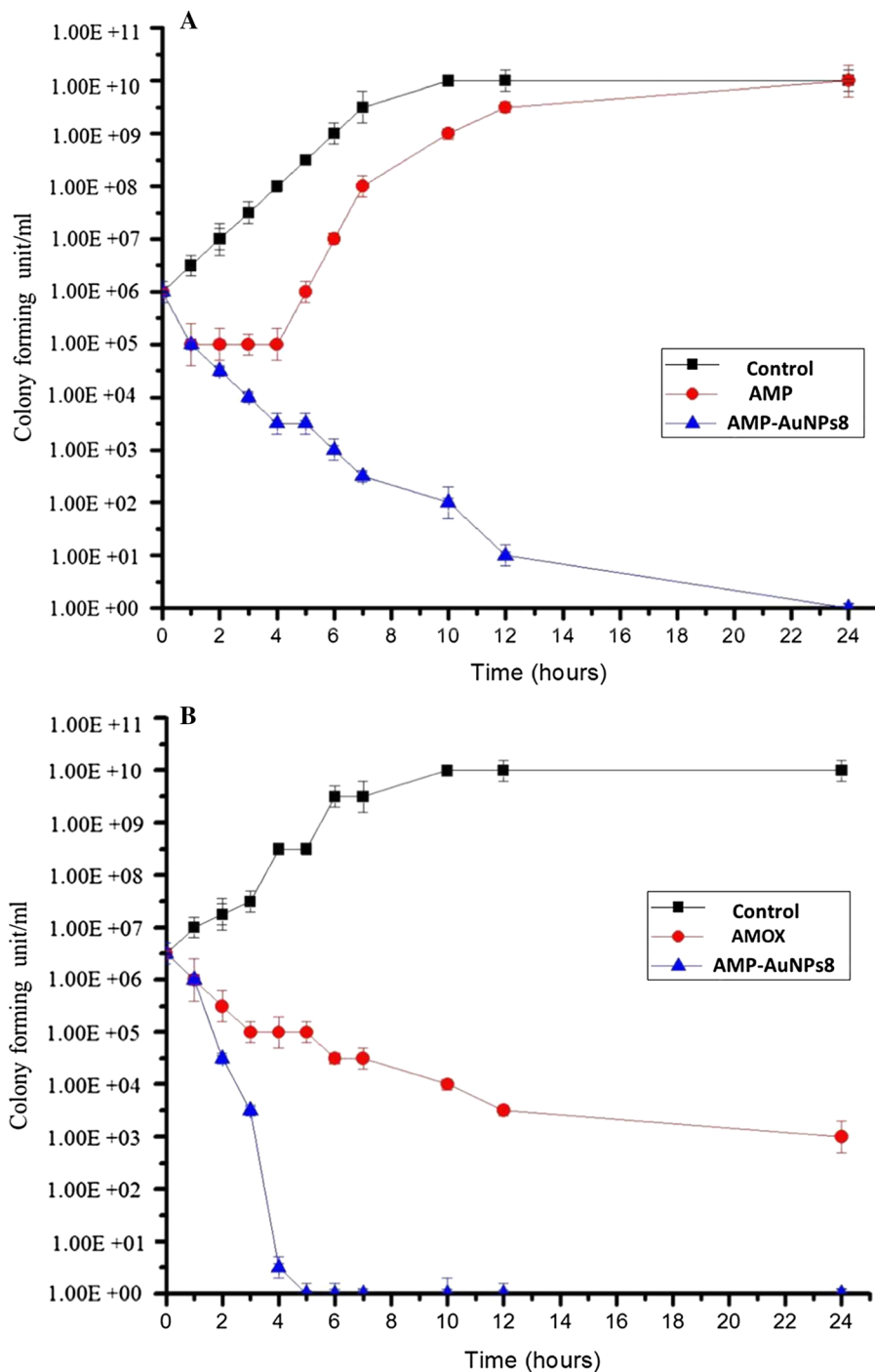
the free antibiotics (Table 2). formulation as AuNPs8 reduced the MICs below the CLSI breakpoint for Amp and Amox according to CLSI guidelines, 2015. In this regards, the data prove that the antibacterial action can be introduced by loading these drugs on the AuNPs surface, therefore it shows high restore potentiality for their actions against bacteria and using also a small size nanomaterials to gain a successful and better results. Furthermore, the killing rate of both Amp/Amox loaded AuNPs against Antibiotic resistant bacteria was also evaluated for *S. aureus* and *P. aeruginosa* isolates after their incubation with Amp-AuNPs8 and Amox-AuNPs8 and count the lining bacteria at different time intervals. The results indicate that the Amp-AuNPs8 formulation is able to kill the *S. aureus* rapidly. The bacterial count data reveals that after 1 h of incubation with Ipm-AuNPs8, the *S. aureus* shows a drastic drop in the living bacterial cells from  $1.6 \times 10^6$  colony forming unit (CFU)/ml to  $1.6 \times 10^4$  CFU/ml with complete bacterial death after 24 h (Fig. 9a). Similarly, Mem-AuNPs8 rapidly killed Ks1.0 (Fig. 9b) after only 2 h of incubation and completely killed all viable bacteria after only 5 h of incubation. We can conclude that the formulation of conjugated Au NPs enhances the antibacterial action of the two studied antibiotics against antibiotic resistant bacteria. The antibacterial action of the amoxicillin conjugated AuNPs is greater than the ampicillin conjugated AuNPs (Table 2), (Amp: Ampicillin; Amox: Amoxicillin; AuNPs8, AuNPs20 and AuNPs60: are gold nanoparticles size 8, 20 and 60 nm

**Table 2** The minimum inhibitory concentration (MIC) of Ampicillin and Amoxicillin compared to their conjugated gold nanoparticles in different sizes against different infectious G -Ve bacteria (n = 3)

Amp Ampicillin; Amox Amoxicillin; AuNPs<sub>8</sub>, AuNPs<sub>20</sub> and AuNPs<sub>60</sub> are gold nanoparticles size 8, 20 and 60 nm respectively and NE no antibacterial effect

	The minimal inhibitory concentration (MIC-µg/ml)					
	<i>Pseudomonas aeruginosa</i>		<i>Staphylococcus aureus</i>		<i>Enterobacter aerogenes</i>	
	St.1.0	St.2.0	St.1.0	St.2.0	St.1.0	St2.0
Amp	27	29	35	42	49	52
Amp-AuNPs <sub>8</sub>	1	1.5	3	4.5	3	2
Amp-AuNPs <sub>20</sub>	4	4	8	10	5	7
Amp-AuNPs <sub>60</sub>	7	6.5	12	14	11	14
Amox	12	14	26	22	27	24
Amox-AuNPs <sub>8</sub>	0.5	0.5	2.5	2	4	3
Amox-AuNPs <sub>20</sub>	1.5	1.5	5	3	8	7
Amox-AuNPs <sub>60</sub>	2	4	8	6	12	15
AuNPs <sub>8</sub>	NE		NE		NE	
AuNPs <sub>20</sub>	NE		NE		NE	
AuNPs <sub>60</sub>	NE		NE		NE	

**Fig. 9** Time kill assay of *Staphylococcus aureus* treated with: **a** free Ampicillin (Amp) and 8 nm diameter Ampicillin loaded gold nanoparticles (Amp-AuNPs8); **b** free Amoxicillin (Amox) and 8 nm diameter Amoxicillin loaded gold nanoparticles (Mem-AuNPs8), compared to control antibiotic free culture



respectively and NE: no antibacterial effect). This refers to the superiority of the amoxicillin molecules over ampicillin ones in suppressing the bacterial cell wall synthesis (Nicolau 2008). Different reports reveal that amoxicillin has more affinity to PBPs

compared to the ampicillin (Bax et al. 1989; Kuo et al. 2016). The amoxicillin molecules show more functionality more than the ampicillin molecules, where it interacts strongly and diffuses through the outer bacteria membrane, which refers to its better reactivity



against Gram -Ve bacilli in comparison with the amoxicillin. However, the Amp-AuNPs and Amox-AuNPs are valuable antibacterial agents due to their great killing effect of different multi-resistance bacteria. The decrease in the Au NPs size increases the adsorption area to carry more antibiotics on the surface and improves the suppression rate in bacterial growth. The results are in agreements with (Brown et al. 2012; Rastogi et al. 2012; Kuo et al. 2016; Payne et al. 2016). It worth to mention that only few works that investigate the antimicrobial effect of AuNPs against microbial pathogens (Zhou et al. 2012; Lima et al. 2013), which increases/synergizes the action of these conjugated NPs, as a result of the direct interaction between the free antibiotics and the loaded AuNPs from one side and the bacterial cells from the other one (Kuo et al. 2016). However, in the presented work all the Au NPs don't show any bactericidal effect on all the tested bacterial growth (Tables 2), whereas antibiotics retained their antibacterial action proficiency upon conjugation on the surface of the AuNPs. However, the mechanistic antibacterial effect of the conjugated AuNPs is less understood till now. The observed improve in the antimicrobial activity of a drug conjugated AuNPs refers to two different reasons (Gupta et al. 2016). The first reason refers to the large AuNPs surface area that permits a better chance for loading large amount of antibiotics that have the potential to interact and bind to the PBP receptor site as a single molecule, leading to better attachment of the antibiotic molecules on the outer bacterial cell membrane in comparison with the free antibiotic (Gu et al. 2003; Gupta et al. 2016). As a result, the accumulation of antibiotic with this high concentration it allows to disturb the osmotic bacterial membrane balance and also inhibit or reduce the cell wall synthesis of the bacterial cell pathogen (Grace and Pandian 2007). The second reason is the high possibility offered to the loaded drug to target multiple sites on the bacteria cell surface and penetrate their cell wall. Consequently block the sulphur containing proteins as well as the phosphorous in the nucleic acid (i.e. DNA) (Cui et al. 2012; Khan et al. 2013; Kandimalla et al. 2016). In spite of these findings, more comprehensive biocompatible studies are needed as a prerequisite to qualify the formulated gold nano-carriers as a clinically accepted delivery transporter before considering this protocol for clinical application (Khan et al. 2013). This may be due to

the lack of complete understanding of these unique nanomaterials regarding their toxicity, accumulation and elimination inside the human body. In the past few years, several reports showed a great bio-distribution after IV administration in the different organs/tissues of liver (Balasubramanian et al. 2010; Morais et al. 2012), however few reports indicated the sequential hepato-biliary track for their excretion (Zhang et al. 2016). In conclusion, a better understanding of biocompatibility of those smart pharmaceutical nano-carriers (showing interesting anticancer and antibacterial activity) is really required to reinforce their implementations in clinical therapy.

## Conclusions

In the present work, we report a one step, safe and rapid method (5 min) for the AuNPs synthesis using aqueous extract of the freshwater fungus *J. aquatica* that is developed for the first time. To the best of our knowledge, freshwater fungi are never exploited in nanomaterials synthesis. The potentiality of different sizes of the produced AuNPs to working as antibiotic delivery system was evaluated for the therapy of multi-resistant human pathogenic bacteria. The results indicated the successful conjugation of both ampicillin and amoxicillin antibiotics with the gold nanoparticles surface, suggesting the presence of a promising chance with unique antibacterial effect for antibiotic -loaded AuNPs over free drug. The potential efficiency of the AuNPs loading is improved with the smaller AuNPs size than the larger sizes. Moreover, the produced AuNPs showed a dose-dependent cytotoxicity against Hela cancer cells provided with appearance of apoptosis observation, suggesting their possible use as a reliable tumor-targeted drug carrier system. A possible mode of effective cytotoxic action of the mycosynthesized AuNPs has been clarified through molecular studies. However, more studies are required in vivo clinical application for authenticating the application of the above mentioned material. Undoubtedly, this simple procedure for the biosynthesis of AuNPs with its unique merits has several advantages including cost effectiveness, simplicity, possibility for cancer treatment as well as improvement and delivering either antibiotic or any other drug in biomedical and pharmaceutical applications with large-scale commercial production. Most importantly, the commercial

production of a dry powdered functionalized antibiotic conjugated AuNPs formula to be used as new intravenous infusion is a promising study that will be the core of interest in the future.

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**Author contributions** MAM designed the study. He wrote, revised and approved the final version of the manuscript before submission.

#### Compliance with ethical standards

**Conflicts of interest** The authors declare no conflict of interest and no competing financial interests.

**Research involving human and animal participants** This article does not contain any studies with human participants or animals performed by any of the authors.

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