RESEARCH PAPER



Use microfluidic chips to study the effects of ultraviolet lights on human fibroblasts

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Received: 9 January 2017 / Accepted: 7 April 2017 / Published online: 11 April 2017 © Springer-Verlag Berlin Heidelberg 2017

Abstract The ultraviolet (UV) radiation from sunlight exposure is highly related to skin damages such as photoaging and skin cancers. UVA radiation can cause altered expression of extracellular matrix proteins, and UVB is believed to be an apoptosis induction factor. In the past, many experiments have been conducted in vitro to investigate how UV lights are responsible for cell damages. However, most of these studies were done under static conditions such as culture dishes, which were quite different from the in vivo dynamic circulatory system. Also, in these studies, only one UV dose was applied at one time, limiting the experimental throughput. To best mimic the physiological condition as well as to increase the throughput, a microfluidic chip was designed and fabricated to create five different UV doses in one single experimental run. This biocompatible chip is used for seeding and culturing cells, together with observing cell morphology in a circulating condition. By using the "Christmas tree" structure, five different concentrations of blue dye solutions were generated within a microfluidic chip. And by illuminating this chip with the UV light, five different UV doses could be attained on cells cultured within this chip. The effects of UVB dose on NIH/3T3 fibroblasts, mainly in terms of morphology and fluorescence-based cell damage rate, were studied.

Keywords Microfluidic chips · Ultraviolet light · NIH/3T3 cells · Cell morphology · Cell damage

1 Introduction

The UV radiation from sunlight exposure has both positive and negative effects on human health. Adequate amounts of sunlight ensure normal production of Vitamin D by the body, which is essential in strengthening bones (Cranney et al. 2008; Hacker et al. 2011; Morris et al. 2010; Reid et al. 2014) and possibly inhibiting the growth of some cancers (Chakraborti 2011; Picotto et al. 2012). Also, UV exposure increases the amount of melanin in the skin. This brown pigment has an excellent photoprotective effect by absorbing UV radiation, dissipating the energy, and protecting the skin from DNA damages (Kvam and Dahle 2004; Miyamura et al. 2008; Wakamatsu and Ito 2006). On the other hand, excessive sun exposure is known to be associated with photoaging, skin cancers, immune suppression, and eye diseases such as cataracts. The World Health Organization (WHO) has classified the broad-spectrum UV radiation as a Group 1 carcinogen.

Depending on the wavelength, UV lights can be divided into UVA (315–400 nm), UVB (280–315 nm), and UVC (100–280 nm). While UVA, also referred to as the black light, cannot be absorbed by the ozone layer, UVB and UVC can be mostly and completely absorbed by the ozone shield, respectively. UVA has long been believed to play an important role in skin aging (Boisnic et al. 2005; Haywood et al. 2003; Kim et al. 2013; Krutmann 2003; Yin et al. 2001). Battie et al. (2014) reported that UVA radiation is a key role in pigmented changes occurring with age, the major sign of skin photoaging in Asians.

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Although UVB phototherapy is a common modality for psoriasis and other skin diseases, overexposure of UVB can cause direct DNA damage, leading to some forms of skin cancers such as basal cell carcinoma (BCC), squamous cell carcinoma (SCC), and melanoma (Green et al. 2007; Hearn et al. 2008; Lee et al. 2005; Saraiya et al. 2004). Situm et al. (2008) reported that a latency period of 20–50 years is typical between the time of UV damage and the clinical onset of BCC. Also, UV-induced mutations in the TP53 tumor suppressor gene have been found in about 50% of BCC patients. Jhappan et al. (2003) reviewed the correlation between UV radiation and cutaneous malignant melanoma and concluded that in vivo models in mice and human skin xenografts have contributed significantly toward the development of effective approaches to the prevention and treatment of melanoma.

Considering the effects of UVC, the eye is most sensitive to this wave band, and overexposure to this radiation can result in eye damages such as cataracts, pterygium, and pinguecula. By examining more than 100,000 Aborigines and non-Aborigines in rural Australia, a strong positive correlation between climatic UV radiation and pterygium prevalence was found (Moran and Hollows 1984). The impacts of UV radiation on eye diseases are reviewed in references (Behar-Cohen et al. 2014; Bergmanson and Soderberg 1995; Parisi et al. 2001).

To help people effectively protect themselves from UV radiation, an international standard UV index is designed to measure the strength of UV lights from sunlight exposure. This index is directly proportional to UV intensity, and it can be classified as follows: 0-2 (low, intensity = 0-20 W/m²); 3-5 (moderate, intensity = 21-35 W/m²); 6-7 (high, intensity = 36-45 W/m²); 8-10 (very high, intensity = 46-55 W/m²); and ≥ 11 (extreme, intensity ≥ 56 W/m²). Therefore, to quantitatively study the effects of UV radiation on cells, controllable UV intensity (in W/m²) and dose (in J/m²) are in demand.

Traditionally, experiments showing how UV lights could cause cell damages were conducted in static, onedose only conditions. This means that cells were cultured in petri dishes, microplates or glasses, and subjected to one UV dose at one time. For example, Kimura et al. (2010) investigated the cell-killing efficacy of UV light on fluorescent protein-expressing cancer cells in vitro and in vivo. Four types of cancer cells (human fibrosarcoma, human osteosarcoma, lung carcinoma, and human pancreas cancer) were cultured on cover glasses and irradiated with UV lights from the bottom of the substrate. It was shown that (1) most cells were viable after an UVA exposure of 200 J/m^2 , (2) cell death was observed with UVB irradiation at 50 J/m², and (3) 25 J/m² UVC irradiation killed almost 70% of the human osteosarcoma cells. Using NIH/3T3 fibroblasts and A431 epidermoid carcinoma cells grown in 12-well microplates as models, Tai et al. (2012) reported that UVC is a DNA damage inducer, and 20 J/m² of UVC irradiation caused cell growth inhibition as well as induced cell death after 24–36-h exposure. Bryant et al. (2000) studied the cytocompatibility of UV light photoinitiating system on NIH/3T3 fibroblasts cultured in 12- and 24-well microplates.

All above-mentioned and mostly other studies were performed in static conditions where cells didn't subject to fluidic flowing like they do in the in vivo microenvironment. Lo et al. (2013) found that lung cancer cells responded to an antioxidant, α -tocopherol, differently depending on circulating or static conditions they were cultured in. Also, in these studies, cells were irradiated with one UV intensity/ dose at one time, limiting the throughput of the experiment.

In order to systematically and quantitatively study how NIH/3T3 fibroblasts respond to UV lights, a microfluidic chip was designed and fabricated to mimic the physiologically circulating condition as well as to increase the experimental throughput. This chip is biocompatible for seeding and culturing cells, and it is transparent for observation of cell morphology and staining. Applying a "Christmas tree"shaped structure to mix and redistribute solutions, five relative concentrations of 0, 1/8, 1/2, 7/8, and 1 are achieved above the culture regions (Lo et al. 2013). A blue colorant, Brilliant Blue FCF, was used to shield off different amounts of UV lights in the five culture areas. The shielding ratio and therefore cell-exposed UV intensity can be well controlled by adjusting the concentration of the blue dye from the inlet. With the aid of this microfluidic chip, we were able to study the effects of UV dose on NIH/3T3 fibroblasts in a circulating condition and a high-throughput manner.

2 Materials and methods

2.1 Chip design and fabrication

The design of the microfluidic chip is shown in Fig. 1. The pattern was drawn in AutoCAD (Autodesk) and then loaded into a CO₂ laser scriber (ILS2, Laser Tools & Technics Corp.) to ablate desired patterns on polymethylmethacrylate (PMMA) substrates and double-sided tapes (8018, 3 M). As shown in Fig. 1a, five layers of PMMA substrates (thickness = 1 mm) and double-sided tapes (thickness = 260 and 70 μ m) were bound together to form the integrated chip, which was then attached to a petri dish (Nunc) for cell culture. The top PMMA layer had five small holes/adaptors serving as flow inlets and outlets. The next two double-sided tapes provided fluidic channels for the shielding area, having a width of 1 mm and a total thickness of 330 μ m (Fig. 1b left). The fourth PMMA layer connected the culture area with the topmost flow inlet/outlet. Fig. 1 Design of the microfluidic chip. *a* From *left* to *right*: 1-mm PMMA layer with adaptors, 260- μ m double-sided tape (shielding area), 70- μ m double-sided tape (shielding area), 1-mm PMMA layer, 260- μ m double-sided tape (culture area), and petri dish (culture area), and petri dish (culture area). **b** Fluidic channels of the shielding area (*left*) and the culture area (*right*)



The bottom double-sided tape (thickness = $260 \,\mu$ m) served as the culture area (Fig. 1b right). Cytotoxicity of PMMA substrates on cells was examined, and no significant change in cell viability was observed (Huang et al. 2009).

2.2 Calculation and simulation of concentrations and absorbance

As shown in Fig. 1b right, when two solutions with relative concentrations of 1 and 0 were injected from the two dye/water inlets, relative concentrations of 0, 0.125, 0.5, 0.875, and 1 could be achieved in the five rectangular areas near the waste outlet. Here, we assume that all liquids split-flowed smoothly and equally around the fork. Similar "Christmas tree" structures were reported for evaluating toxicity and teratogenicity of drugs on embryonic zebrafish developmental dynamics (Yang et al. 2011), for studying the effects of antioxidant concentrations on the production of reactive oxygen species (ROS) in lung cancer cells (Lo et al. 2013), and for investigating the migration of lung cancer cells under single or coexisting chemical/ electrical stimulation (Lo et al. 2016). In the present study, 0.5% (w/w in water) Brilliant Blue FCF (Sigma) was used as the UV blocker, creating concentrations of 0, 0.0625, 0.25, 0.4375, and 0.5% above five locations of the culture area. In addition, the numerical simulation of chemical concentrations inside the microfluidic chip was performed using the commercial software COMSOL Multiphysics (COMSOL, USA). The "Transport of Dilute Species" module was used with the following parameters and settings: medium = water; diffusion coefficient = 10^{-13} m²/s for Brilliant Blue FCF at room temperature (Gupta et al. 2006); inlet flow rate = $15 \,\mu$ L/h (set in each inlet).

The Beer's law was used to relate the attenuation of light to the properties of the material through which the light is traveling. The absorbance (*A*) of a material to a specific light band is proportional to the absorption coefficient of the material (α), the path length of the light (*x*), and the concentration of the material (*c*): $A = \alpha xc$. Also, the absorbance is related to the transmittance (*T*) of the light to the material as $A = -\log T$. Using these two equations, we can relate the absorbance (*A*) to the concentration (*c*) by measuring the light intensity underneath the shielding area and normalizing the transmittance to 1 for 0% Brilliant Blue FCF (i.e., the light was totally transmitted through the area without any UV blocker).

2.3 Cell preparation

The fibroblast cell line NIH/3T3 was purchased from the Bioresource Collection and Research Center (BCRC), Taiwan. A complete medium consisting of Dulbecco's modified Eagle medium (DMEM, Gibco) and 10% calf serum (CS, Invitrogen) was used for the cell culture. The cells were incubated in tissue culture polystyrene flasks (corning) in 5% CO_2 at 37 °C until 90% confluence before seeding into the microfluidic chip.

2.4 Experimental system and procedure

2.4.1 Chip assembly and cell preparation

The microfluidic chip was assembled inside the laminar flow hood. The medium/cell inlet and outlet were connected to two syringes driven by syringe pumps (NE-300, New Era). 1 \times phosphate-buffered saline (PBS) was flowed into the chip and kept within the channel overnight under 5% CO2 at 37 °C. Then, the syringes were pushed gently by hands to remove bubbles, and $1 \times PBS$ was replaced with DMEM. 4×10^5 cells suspended in 1 ml DMEM with 10% CS was loaded into the culture area by injecting the solution from the medium/cell inlet. The microfluidic chip with seeded cells was mounted on top of a transparent indium tin oxide (ITO) glass (Part No. 300739, Merck) which is connected to a proportional-integral-derivative (PID) controller (TTM-J4-R-AB, JETEC Electronics Co.) for maintaining the temperature at 37 \pm 0.5 °C via feedback from a thermal couple (TPK-02A, TECPEL) clamped tightly between the heater and the chip. Fresh medium (DMEM with 10% CS) was continuously pumped into the chip at a flow rate of 20 µL/h for 24 h before UVB treatments. The continuous flowing of fresh medium provides cells with enough nutrition as well as removes waste from cells. In vivo cells are subject to different flow rates in different body fluids such as urine, blood, saliva, and tears. In the present study, the flow rate is determined to be 20 µL/h based on our previous experience (Cheng et al. 2008; Lo et al. 2013; Sun et al. 2012; Wu et al. 2015). This rate should not be too high to affect the metabolism of cells. As reported, fluidic shear stresses of as low as 0.25-0.6 Pa could interface cell attachment, and even higher values of stresses (0.5-10 Pa) could remove adherent cells (Chisti 2001). Moreover, 0.8-1.5 Pa of laminar shear stresses could induce cell alignment in the direction of flow (Davies et al. 1986), and values of 0.1–1 Pa were shown to affect cellular morphology and permeability (Chisti 2001). A flow rate of 20 μ L/h corresponds to a shear stress of 0.0001 Pa (Sun 2016), which is considered harmless to cells. Also, this flow rate is high enough for providing cells with fresh medium since cells remain healthy inside the culture area for days (Cheng et al. 2008).

2.4.2 UV treatments

As indicated in our previous studies (Wu et al. 2016), UVC, compared to UVB, had a much lower transmittance to plastic materials such as petri dishes and microplates. Therefore, UVB was used as the UV light source in the present work. Before UV treatments, two syringes containing Brilliant Blue FCF of 0 and 0.5% were connected to the water/dye inlets of the microfluidic chip and driven by pumps at a flow rate of 15 µL/min (set in each inlet) for at least 30 min. Water and colorant solutions were kept flowing into and out of the chip during UV treatments to ensure uniform Brilliant Blue FCF concentrations in the shielding area. The UV lamp (3UV Lamps, UVP LLC) was mounted 3 cm above the chip and turned on for 22 min and 44 s, vielding UVB doses of 0.604, 0.423, 0.091, 0.035, and 0 J/ cm² underneath the five shielding areas. These doses were calculated by multiplying the power (in W/cm²), measured by a UV-specified power meter (UVX Radiometer, UVP LLC), by the total illumination time (in sec). Bright-field images of different field of views (FOVs) were captured using an inverted microscope (CKX41, Olympus) before UV treatments, right after UV treatments, 1, 2, 4, 10, and 24 h after UV treatments.

2.4.3 Cell staining

To quantify the effect of UVB dose on cell damage, cell staining with Hoechst and SYTOX Green was performed. Hoechst (H3570, Thermo), having excitation and emission wavelengths of around 350 and 461 nm, respectively, was used to stain double-stained DNAs in all cells. SYTOX Green (S7020, Thermo), having excitation and emission wavelengths of around 504 and 523 nm, respectively, was used to stain nucleic acids in damaged cells. 24 h after UV treatments, cultured cells inside the microfluidic chip were incubated with Hoechst (8 μ M in DMEM) and SYTOX Green (0.2 μ M in DMEM) for 20 min and then washed with fresh DMEM 3 times. Fluorescent images of different FOVs were captured using an inverted fluorescent microscope (TS-100, Nikon) equipped with a CCD camera (DSOi1, Nikon).

2.5 Data analysis

For each experimental condition, at least 120 cells were selected from at least three independent experiments for data analysis. The standard error of the mean (SEM) was also calculated. To quantify cell morphology, each cell was assumed to be elliptic, and its long axis (L_1) and short axis (L_2) were measured by ImageJ software (National Institute of Health), as shown in Fig. 2. Then, the long axis-to-short axis ratio, L_1/L_2 , was calculated.



Fig. 2 Long axes (L_1) and short axes (L_2) of NIH/3T3 cells before (left) and after (right) UVB exposure

To analyze cell-staining images, the numbers of all cells (those stained with Hoechst) and damaged cells (those stained with SYTOX Green) were counted in ImageJ software. The damage rate is defined as (the number of damaged cells)/(the number of all cells) \times 100%.

3 Results and discussion

3.1 Calculation and simulation of concentrations and absorbance

Figure 3a shows the model used in the simulation with the mesh distribution shown in Fig. 3b. There are 39,052

(b) (a) 66895 66995 20 20 10 10 0 0 -10 -10 -20 -20 -20 mm -20 mm 20 n 20 (c) (**d**) 0.5% 0.25% 10 mm 0% Intensity of brilliant blue FCF (e) 150 Mean Intensity 100 50 0 0.2 . 0.4 0.6 0.0 Blue FCF concentration(%, w/w)

Fig. 3 a Model used in the simulation. b Mesh distribution in the simulation. c Numerical simulation of Brilliant Blue FCF concentration inside the microfluidic chip. The concentrations in the two inlets are 0.5 and 0%, respectively. d Image of the microfluidic chip with 0.5 and 0% of Brilliant Blue FCF solutions continuously flowing into the two inlets. e Measured intensities plotted against calculated concentrations

prism elements, 25,712 tetrahedral elements, 19,960 triangular elements, 4872 edge elements, 774 vertex elements, 432 pyramid elements, and 84 quadrilateral elements. Figure 3c shows the numerical simulation of Brilliant Blue FCF concentration inside the microfluidic chip, where the concentrations in the two inlets are 0 and 0.5%, respectively. As indicated, the concentrations are close to calculated values, being 0, 0.0625, 0.25, 0.4375, and 0.5%. To experimentally verify the distribution of concentration, 0 and 0.5% Brilliant Blue FCF were continuously flowed into the two inlets of the chip for 1 h, and the whole chip was imaged using an inverted microscope, as shown in Fig. 3d. The absolute intensity in each shielding area was measured using ImageJ, and these values (the y-axis) were plotted against the calculated ones (the x-axis). A good linear correlation was obtained between calculation and measurement ($R^2 = 0.9962$) (see Fig. 3e).

The UVB intensity underneath each shielding area was measured as the light source passed through and blocked by the colorant. As shown in Fig. 4a, these values were around 443 ± 5.5 , 310 ± 4.4 , 67 ± 3.6 , 26 ± 0.0 , and $23 \pm 0.0 \,\mu$ W/cm² for colorant concentrations of 0, 0.0625, 0.25, 0.4375, and 0.5%, respectively (averaged over three measurements). After normalizing the transmittance to

1 for 0% Brilliant Blue FCF, the absorbance was calculated (Table 1) and plotted against the concentration, as shown in Fig. 4b. For example, for concentration (c) = 0.0625%, the normalized transmittance (*T*) was 310.3908/443.0049 = 0.7006487, and the absorbance (*A*) was $-\log 0.7006487 = 0.1545$. A good linear correlation of $R^2 = 0.9905$ indicated that within this concentration range Beer's law is valid and absorbance of other values can be achieved using interpolation.

3.2 Effects of UVB on cell morphology

After UVB treatments for 22 min and 44 s, cells cultured underneath five shielding areas were subject to UVB doses of 0.604, 0.423, 0.091, 0.035, and 0 J/cm², respectively. To quantify cell morphology, the long axis-to-short axis ratios of cells subject to different UVB doses at different time points were measured and calculated. These ratios served as an indicator to determine whether these cells were healthy or not: healthy NIH/3T3 cells appear spindlelike with higher L_1/L_2 ratios, while damaged NIH/3T3 cells look round with lower L_1/L_2 ratios ($L_1/L_2 = 1$ for a circle) (Coleman et al. 2000; Stacey et al. 1999; Sugita et al. 1992). For example, Coleman et al. reported that bFGF (a



Fig. 4 a UVB power densities measured underneath five shielding areas. b Relationship between Brilliant Blue FCF concentration and UVB absorbance

Brilliant Blue FCF concentration (c in %)	0	0.0625	0.25	0.4375	0.5
Power density (μ W/cm ²)	443.0049	310.3908	66.51232	25.8659	23.40248
Normalized transmittance (T)	1	0.7006487	0.150139	0.0583874	0.05282669
$A = -\log T$					
Absorbance (A)	0	0.1545	0.8235	1.2337	1.2771
Equation	A = 2.745c				
R^2	0.9905				

Table 1 Calculating theabsorbance of Brilliant Blue

FCF to UVB light

fibroblast growth factor)-treated NIH/3T3 cells tended to be smaller and rounder than the typical flat morphology of NIH/3T3 cells (Coleman et al. 2000). Other types of cells also appear round or oval during apoptosis (Elmore 2007; Imajoh et al. 2004; Miller et al. 1998). Therefore, the long axis-to-short axis ratio can be used to quantify the extent to which NIH/3T3 cells were damaged due to UVB treatments. The aspect ratio values for "before UV treatment" cells were 3.968, 4.574, 4.079, and 4.021 for UVB doses of 0.604, 0.423, 0.091, and 0.035 J/cm², respectively. Clearly, cells show a certain degree of deviation in the aspect ratio in these control cases. Such deviation is considered acceptable since cells cultured in different areas show certain randomness. We assume that cells start to become unhealthy/ damaged once the aspect ratio is smaller than around four.

Figure 5a shows these ratios for cells subject to 0.604 J/ cm² UVB radiation at different time points. The mean ratios were 3.968, 3.479, 2.948, 2.918, 2.913, 2.841, and 2.691 before UV treatment, right after UV treatment, 1, 2, 4, 10, and 24 h after UV treatments, respectively. Clearly, this ratio decreased after cells were subject to UVB radiation, and the value decreased even more with increasing post-treatment time. This result suggests that UVB of a 0.604 J/cm² dose did cause damage to NIH/3T3 cells, more or less in a post-treatment time-dependent manner. The longer the post-treatment time was, the more the cells were damaged (shown as a decreasing long axis-to-short axis ratio). A similar trend was observed for cells subject to 0.423 J/cm² UVB radiation, as indicated in Fig. 5b. The mean ratios were 4.574, 3.996, 3.737, 3.792, 3.52, 3.357, and 2.729 before UV treatment, right after UV treatment, 1, 2, 4, 10, and 24 h after UV treatments, respectively. Roughly speaking, this ratio decreased after cells were subject to UVB radiation, and the value decreased even more with increasing post-treatment time except at time points 1 and 2 h. For cells subject to UVB doses of 0.091 J/cm² or less, UVB treatments did not do significant damage to them at post-treatment time points 0, 1, 2, and 4 h. At time points 10 and 24 h, the long axis-to-short axis ratio started

to decrease, indicating clear damage to cells. For example, under a UVB dose of 0.091 J/cm², the mean ratios were 4.079, 4.312, 4.178, 4.288, 4.342, 3.909, and 3.271 before UV treatment, right after UV treatment, 1, 2, 4, 10, and 24 h after UV treatments, respectively. And under a UVB dose of 0.035 J/cm², the mean ratios were 4.021, 4.469, 4.307, 4.461, 4.256, 4.191, and 3.495 before UV treatment, right after UV treatment, 1, 2, 4, 10, and 24 h after UV treatments, respectively. These results indicate that the onset time point for UVB light (with a dose less than 0.091 J/cm^2) to do significant damage to NIH/3T3 cells is around 10 h after treatments. As a control group, under a UVB dose of 0 J/cm², the mean ratios were 4.387, 4.624, 4.412, 4.608, 4.750, 4.508, and 4.291 before UV treatment, right after UV treatment, 1, 2, 4, 10, and 24 h after UV treatments, respectively. Without UVB exposure, no clear damage to cells was observed.

Figure 6a shows the long axis-to-short axis ratios of NIH/3T3 cells 10 h after UVB treatments at different doses. This ratio was close to 4.2 before UV exposure, but decreased to 4.191, 3.909, 3.357, and 2.841 after subject to UVB doses of 0.035, 0.091, 0.423, and 0.604 J/ cm², respectively. As shown in Fig. 6b, a similar trend was observed for cells 24 h after UVB treatments at different doses. These ratios decreased to 3.495, 3.271, 2.729, and 2.691 after subject to UVB doses of 0.035, 0.091, 0.423, and 0.604 J/cm², respectively. These suggest that, after the onset time point of 10 h post-treatment, UVB did damage NIH/3T3 cells in a dose-dependent manner.

3.3 Effects of UVB on cell damage rate

Cell damage rates due to UVB treatments were measured and calculated by staining cells with Hoechst and SYTOX Green. Hoechst dyes are permeable to cell membrane and are commonly used to stain double-strained DNAs in cells. SYTOX Green dyes, on the contrary, are permeable only to damaged membrane, and are applied to stain nucleic acids in damaged cells. Figure 7 shows the images of

Fig. 5 Long axis-to-short axis ratios of NIH/3T3 cells under **a** 0.604 J/cm² and **b** 0.423 J/cm² UVB exposure at different time points







NIH/3T3 cells 24 h after UVB exposure at different doses. Cells in the bright-field images (Fig. 7 left column) can be mapped to those in the Hoechst images (Fig. 7 middle column, expressed in blue), and damaged cells were indicated in the SYTOX Green images (Fig. 7 right column, expressed in green). These images were further quantified by calculating the damaging rate, defined as the number of cells stained with SYTOX Green divided by the number of all cells (stained with Hoechst) in percentage. Figure 8a shows the damage rates 24 h after UVB treatments at different doses. These values were 3.1, 3.6, 3.9, 41.6, and 64.4% for UVB doses of 0, 0.035, 0.091, 0.423, and 0.604 J/cm², respectively. The damage rate increased with increasing UVB dose from 0.423 to 0.604 J/cm², and this value stayed almost constant for UVB doses below 0.091 J/cm^2 .

Figure 8b illustrates the correlation between the long axis-to-short axis ratio and the damage rate. As indicated, no linear correlation was observed, and significant damage rates (higher than 40%) were observed for ratios lower than 3. When subject to UVB radiation, cell morphology changed gradually from spindle-like (higher long axis-toshort axis ratios) to round (lower long axis-to-short axis ratios) in both dose- and post-treatment time-dependent manners. But in calculating the damage rate, cells were counted as either damaged or not by determining whether they lighted up or not after SYTOX Green staining. Therefore, the long axis-to-short axis ratio could be used to indicate the extent to which cells were damaged, yet the damage rate showed only the percentage of damaged cells. These results suggest that the threshold of the long axisto-short axis ratio to initiate observable SYTOX Green signals is around 3. UVB radiation was doing damage to cells gradually with ratios decreasing from 4.5 to 3, but these cells showed "not damaged" in staining. As the dose- or the post-treatment time increased, cells were damaged ever more with ratios further decreasing below 3, while these cells showed "damaged" in staining.

4 Conclusion

In this study, we developed a microfluidic chip for studying the effects of UVB radiation on NIH/3T3 cells. Five different concentrations of Brilliant Blue FCF were produced inside a single chip. Cells were subject to UVB treatments of different doses after the light source passed through the shielding area. By analyzing the cell morphology in terms of the long axis-to-short axis ratio, it was found that UVB radiation did damage to cells in both dose- and post-treatment time-dependent manners. And from cell staining, the damage rates were calculated at different UVB doses, indicating significant damage at UVB doses higher than 0.423 J/cm². To generate lights with different intensities, a graduated neutral density filter or a spatial light modulator can be used. Although these devices are commercially available and easily to be operated, the present microfluidic chip has the following advantages: (1) five different UV intensities could be attained simultaneously by using this device, highly increasing the experimental throughput, (2) by varying the concentration of the dye within this device, different UV intensities of a linear range could be attained following the calibration curve, and (3) it integrates a microenvironment where the intensity of the UV light is well controlled into a fluidic system where cells are subject to a physiologically circulating condition. In the future, by combining the current chip with other microfluidic designs, we are able to study cells' response to different chemical or physical stimuli (such as chemicals, lights, electric fields, shear stresses, and magnetic fields) in a high-throughput manner. This will definitely help in understanding the mechanisms of all aspects of cell metabolism.

Fig. 7 Images of NIH/3T3 cells 24 h after UVB exposure at different doses. Left column Bright-field; Middle column Hoechst staining; Right column SYTOX Green staining

(a)

Damage Rate(%)

100

80

60-

40 20.

0.

0,604 11002

Dose of UVB



Fig. 8 a Damage rates of NIH/3T3 cells 24 h after UVB exposure at different doses. b Correlation between the long axis-to-short axis ratio and the damage rate

Acknowledgements This work was financially supported by the Ministry of Science and Technology of Taiwan under Contract No. MOST 105-2112-M-030-002-MY2. The authors would like to thank Dr. Huai-Fang Chang for help in cell culturing.

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