**RESEARCH ARTICLE** 



# Evaluation of normal-appearing white matter with perfusion and diffusion MRI in patients with treated glioblastoma

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#### Abstract

**Objective** We tried to reveal how the normal appearing white matter (NAWM) was affected in patients with glioblastoma treated with chemo-radiotherapy (CRT) in the period following the treatment, by multiparametric MRI.

**Materials and methods** 43 multiparametric MRI examinations of 17 patients with glioblastoma treated with CRT were examined. A total of six different series or maps were analyzed in the examinations: Apparent Diffusion Coefficient (ADC) and Fractional Anisotropy (FA) maps, Gradient Echo (GRE) sequence, Dynamic susceptibility contrast (DSC) and Arterial spin labeling (ASL) perfusion sequences. Each sequence in each examination was examined in detail with 14 Region of Interest (ROI) measurements. The obtained values were proportioned to the contralateral NAWM values and the results were recorded as normalized values. Time dependent changes of normalized values were statistically analyzed.

**Results** The most prominent changes in follow-up imaging occurred in the perilesional region. In perilesional NAWM, we found a decrease in normalized FA (nFA), rCBV (nrCBV), rCBF (nrCBF), ASL (nASL)values (p < 0.005) in the first 3 months after treatment, followed by a plateau and an increase approaching pretreatment values, although it did not reach. Similar but milder findings were present in other NAWM areas. In perilesional NAWM, nrCBV values were found to be positively high correlated with nrCBF and nASL, and negatively high correlated with nADC values (r: 0.963, 0.736, -0.973, respectively). We also found high correlations between the mean values of nrCBV, nrCBF, nASL in other NAWM areas (r: 0.891, 0.864, respectively).

**Discussion** We showed that both DSC and ASL perfusion values decreased correlatively in the first 3 months and showed a plateau after 1 year in patients with glioblastoma treated with CRT, unlike the literature. Although it was not as evident as perfusion MRI, it was observed that the ADC values also showed a plateau pattern following the increase in the first 3 months. Further studies are needed to explain late pathophysiological changes. Because of the high correlation, our results support ASL perfusion instead of contrast enhanced perfusion methods.

Keywords Glioblastoma · Radiotherapy · Diffusion MRI · DSC perfusion MRI · ASL perfusion MRI

# Introduction

Chemo-radiotherapy (CRT) is a widely used treatment modality for patients with primary or metastatic brain tumors. The standard treatment protocol of glioblastoma includes the use of radiotherapy (RT) with temozolomide chemotherapy for the first month. The aim of RT planning is to minimize the possibility of complications in normal tissues and to ensure tumor cell death at the highest level.

Ersen Ertekin drersen@hotmail.com Although advances allow for more precise identification of treated areas, large amounts of healthy tissue are inevitably exposed to significant doses of radiation [1, 2]. Radiation-induced changes in brain tissue can be divided into acute effects, early delayed effects, and late effects [3–6]. Even if late radiation damage is irreversible, understanding its development and quantifying the damage is still unclear [7, 8]. It is known that RT disrupts tissue perfusion by causing vascular damage. It is manifested by dilatation and wall thickening in the vessels, endothelial cell damage, and disruption of the blood–brain barrier in normal-appearing brain tissue [3, 5, 6, 9]. Studies evaluating radiation damage show that white matter is more sensitive than gray matter [10, 11]. Magnetic Resonance Imaging (MRI) is the most effective

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method for imaging brain damage caused by radiation. However, pathological signal changes observed in conventional sequences (T2W series) are not specific and can be seen in processes such as edema, demyelination, and necrosis. In addition, central nervous system damage can be found in areas that appear normal on MRI after RT [8, 12]. For this reason, advanced MRI techniques such as Perfusion MRI and Diffusion Weighted MRI have become frequently used.

There are not many studies evaluating the changes in normal-appearing brain tissue after fractionated radiotherapy (FRT) or stereotactic radiosurgery with perfusion MRI [13–24]. Although there are incompatible findings in these studies, both cerebral blood volume (CBV) and cerebral blood flow (CBF) decreases have been shown in general after FRT or single-fraction stereotactic radiosurgery. Although CBV and CBF data can be calculated with Dynamic Susceptibility Contrast (DSC) MRI, which is widely used in the clinic, it has limitations such as reproducibility and quantification of data acquisition and post-processing [25–31]. Another important method used to evaluate CBF is arterial spin labeling (ASL). There are some studies examining RTrelated changes with ASL perfusion [14, 17, 32, 33]. They are advantageous over contrast-enhanced perfusion imaging because they do not require contrast material and are easily reproducible.

Diffusion-Weighted Imaging (DWI) is important in defining the response to RT [34–37] and normal tissue involvement [38–40]. Quantitative Diffusion Tensor Imaging (DTI) measurements are the most sensitive method for identifying white matter abnormalities [41] and vary before any other imaging modality [39, 40]. Generally, DTI changes are progressive and occur after some threshold or in a dose-sensitive manner [40, 42, 43].

In this study, we wanted to evaluate the treatmentrelated changes over time in normal-appearing white matter (NAWM) with multiparametric MRI in patients with glioblastoma treated with CRT. For this purpose, we analyzed the images of patients who underwent perfusion examination in addition to standard MRI protocols in follow-up imaging. We aimed to evaluate the changes in MRI parameters such as DSC perfusion, ASL perfusion, GRE, DWI, and FA over time and their relationships with each other.

### Methods

This retrospective study was approved by the local ethics committee of our institution.

298 patients who underwent MRI between January 2011 and December 2019 were found to have intracranial masses were scanned. Of these patients, 69 patients with unsatisfactory image quality, 17 patients under the age of 18, 160 patients with a diagnosis of non-glioblastoma (78 had benign, 29 had metastasis, and 53 had non-glioblastoma diagnosis), and 35 patients with missing any of MRI sequences on follow-up imaging were excluded from the study. MRI images of 17 patients with pathologically confirmed diagnosis of glioblastoma and treated with the standard CRT regimen were evaluated.

Surgical resection was performed in all patients. Following the healing of the wound, almost 60 Gy was administered in 30 fractions, together with 4–6 weeks of adjuvant chemotherapy, 5 days a week. No patient using chemotherapeutics other than TMZ or receiving RT with a protocol other than the standard treatment protocol before imaging was present in our study.

#### **MRI** investigation

MRI investigations were performed using the 1.5 T MR device (Philips Achieva, Philips Medical Systems Nederland B.V.). In addition, tumor perfusion protocol was used in at least one cranial MRI during follow-up in all patients. Initially, conventional cranial MRI, diffusion MRI, and ASL perfusion MRI were performed, respectively without administering any contrast medium. In conventional cranial MRI investigation, axial T1 and T2 weighted (W) sequences, axial FLAIR sequence, sagittal T2W, and axial gradient echo sequences were obtained. Diffusion weighted gradient code was applied in seven directions with a diffusion weight factor of b = 1000 s/mm<sup>2</sup> for each axial section, and a set of blank images with b = 0 s/mm<sup>2</sup> was obtained. ADC and FA maps were created from the diffusion tensor.

For perfusion MRI, single-phase ASL involving the entire supratentorial region was obtained without administering any contrast material. The Pulsed ASL (PASL) labeling method available in our system was used. Using single saturation pulses, the post-labeling delay was set to 300 ms and bolus duration was set to 600 ms. Then, DSC perfusion images were obtained with a bolus contrast injection (0.1 mmol/kg) using an automated syringe. For DSC perfusion mapping, the arterial input function (AIF) was defined in the middle cerebral artery, and its proximity, as suggested by Scholdei et al. [44]. Contrast plateaus were marked on the obtained signal intensity-time curves depending on changing sensitivity with the contrast material passing through the cerebral tissues. Then, colour maps (CBV, CBF, and MTT) were created.

The patients' non-contrast and contrast enhanced conventional cranial MRI images, ASL and DSC perfusion images were evaluated via (Picture Archiving Communication Systems) PACS.

#### **Imaging analysis**

Two radiologists with 4 and 20 years of experience performed all assessments by consensus. Firstly, T2, FLAIR, and contrast-enhanced images were evaluated, and areas of probable tumor spread, compression, edema effect, and radiation necrosis were excluded.

The areas with no signal alteration, not enhanced after contrast-enhanced imaging in T2W, and FLAIR series were defined as the normal appearing white matter (NAWM). Measurements were made in 14 areas of NAWM in total, seven of which were bilateral in the patient's last investigation included in the study. These areas were as follows:

1-2: perilesional ipsilateral-contralateral.

- 3–4: frontal lobe ipsilateral-contralateral.
- 5–6: parietal lobe ipsilateral-contralateral.
- 7–8: occipital lobe ipsilateral-contralateral.

9-10: corona radiata ipsilateral-contralateral.

11–12: anterior limb of the internal capsule ipsilateral-contralateral.

13–14: posterior limb of the internal capsule ipsilateral-contralateral.

Bilateral measurements were made at the same level and similar dimensions ( $\pm 3$  voxel), creating circular ROIs. Care was taken to keep the standard deviation at a minimum. In follow-up investigations, an effort was made to maintain a similar positioning of ROIs. Initially, the areas were defined in conventional T2w or FLAIR images on PACS, the ROIs were transferred to the FA, ADC, GRE, and single-phase ASL maps at the same levels. Then, measurements were made, and mean values were recorded. Since they represented the gray matter, ROI areas with values under the threshold value of FA=0.2 were recreated, as described by Chapman et al. [45]. Thus, the areas involving other than the white matter were excluded. Besides, at the Workstation, similar section levels were aligned on the raw images. Measurements were made on a minimum of three similar-sized ROIs drawn, paying attention to positioning, and the highest rCBF and rCBV values were selected (Fig. 1).

The measurements were normalized. The contralateral, same axial level, mirror-symmetrical, and normal-appearing white matter was used as the reference tissue [22, 43]. Thus, the normalized ADC (nADC), FA (nFA), GRE (nGRE), ASL (nASL), and the normalized relative CBV (nrCBV), normalized relative CBF (nrCBF) values were recorded and used in statistical analysis.

The measurements were divided into seven groups regarding month-based time points as the pretreatment values and the posttreatment values of 1-3, 4-6, 7-9, 10-12, 13-18, and > 18 months. In addition, normalized values of ipsilateral NAWMs were recorded for each time point. Except for perilesional NAWM, the values of other NAWM areas were averaged (frontal, parietal, occipital lobe, corona radiata, anterior and posterior limbs of the internal capsule). Consequently, the averages and standard deviations (SD) of two different values ('perilesional' and 'other NAWM' areas) for the time points they belonged to were calculated and recorded.

#### **Statistical analysis**

The statistical analysis of the data was made with SPSS (Statistical Package for Social Sciences, version 20.0; SPSS Inc., Chicago, IL, USA) and MedCalc (MedCalc version 18; Ostend, Belgium) software [61].

Student *T*-test was used to compare two time-point groups. Normality tests (Kolmogorov–Smirnov) determined the distributions of continuous variables. Pearson



Fig. 1 Placement of sample ROI-Corona Radiata-NAWM- ADC/FA/sfASL/GRE/DSC

Correlation Analysis assessed correlations of changes in different parameters' values over time. The correlation coefficient is expressed by the lowercase 'r,' which is between -1 and +1. Values above 0.7 were considered a strong correlation. A *p*-value < 0.05 was considered statistically significant.

## Results

Seventeen patients who met the criteria were included in the study. A total of 43 MRI investigations of 17 patients were evaluated. Among 17 patients, 11 (64.7%) were male, 6 (35.3%) were female, and the mean age was 54.35 (SD: 12.48) years. At the time of data collection, 13 (76.5%) patients died, and treatment and follow-up continued in 4 (23.5%) patients. The mean life duration was 29.3 (SD: 16.67) months in the patients who died. The mass was located in the frontal lobe in seven (41.2%) patients, the parietal lobe in seven (41.2%) patients, and the temporal lobe in three (17.6%) patients. The mean follow-up duration of patients was 13.04 (SD: 11.6) months.

The mean normalized values were recorded after grouping in seven different pre-treatment and post-treatment time points. The values of two different regions were plotted according to their time points, and the significance of changes over time was evaluated. The changes of perilesional mean values and their 'p' values were presented in Table 1. Figure 2 shows the changes of mean perilesional NAWMs over time.

In perilesional NAWM, even though an almost 20% increase was determined in the 1–3 months group compared to the pre-treatment group, the difference was not statistically significant. This increase was limited to some extent in the 13–18 months and > 18 months groups (~ 16%), but it was present in all time-point groups at similar rates. In nFA, following RT, a significant reduction of ~ 19% was

Table 1 The changes of perilesional mean values over time



Fig. 2 The changes of mean perilesional NAWM areas over time

determined in the 1–3-month group (p: 0.0027), and significant reduction continued in the >18 months group (20%) (p: 0.0194). No significant changes in mean nGRE values with time were determined.

Regarding nrCBV among perfusion values, the mean values of the 1-3 months and 4-6 months time-point groups were ~ 40% lower than the preRT value (p: 0.0090 and p: 0.0087, respectively). This value significantly increased in post-RT 10–12 months, 13-18 months, and > 18 months (p: 0.0300, p: 0.0070, and p: 0.0069, respectively), but never returned to its pretreatment levels. Similarly, regarding nrCBF, the mean value of the 1-3 months was~35 lower in the 1–3 months group,  $\sim 30\%$  lower in the 4–6 months and 7-9 months groups, compared to its preRT value, and these reductions were statistically significant (p: 0.0053, p: 0.0004, and p: 0.0317, respectively). This value significantly increased in the groups of 13-18 months and > 18 months compared to its value in the 1-3 months group (p: 0.0002, and p: 0.0002, respectively), but never returned to its pretreatment levels. For nASL, similar to the other perfusion measurements, significant reductions are present in the 1–3 months group ( $\sim 20\%$ ) and the 4–6 months group  $(\sim 30\%)$  compared to the preRT value (p: 0.0020 and p: 0.0051, respectively). On the other hand, significant increases were determined in the > 18 months group (~40%, p: 0.0047), and values similar to the pretreatment values were reached.

| Perilesional | Pre-treatment | 1-3 months                 | 4-6 months                  | 7–9 months                 | 10-12 months              | 13-18 months                | >18 months                   |
|--------------|---------------|----------------------------|-----------------------------|----------------------------|---------------------------|-----------------------------|------------------------------|
| nADC         | 0.91          | 1.09                       | 1.12                        | 1.09                       | 1.07                      | 1.05                        | 1.06                         |
| nFA          | 1.03          | 0.84 ↓<br><i>p</i> : 0.002 | 0.87                        | 0.85                       | 0.84                      | 0.94                        | $0.82 \downarrow p: 0.0194$  |
| nGRE         | 0.97          | 1.03                       | 1.01                        | 1.00                       | 1.00                      | 1.02                        | 1.05                         |
| nrCBV        | 0.93          | 0.56↓<br><i>p</i> : 0.009  | 0.56                        | 0.73                       | 0.74 ↑<br><i>p</i> : 0.03 | 0.92 ↑<br><i>p</i> : 0.007  | $0.91 \uparrow p: 0.006$     |
| nrCBF        | 0.96          | 0.63 ↓<br><i>p</i> : 0.005 | 0.69 ↓<br><i>p</i> : 0.004  | 0.69↓<br><i>p</i> : 0.0317 | 0.75                      | 0.96 ↑<br><i>p</i> : 0.0002 | 0.93 ↑<br><i>p</i> : 0.0002  |
| nASL         | 0.79          | 0.64 ↓<br><i>p</i> : 0.007 | 0.55 ↓<br><i>p</i> : 0.0009 | 0.51                       | 0.64                      | 0.78                        | 0.82 ↑*<br><i>p</i> : 0.0347 |

↓ Significant decrease compared to pretreatment period

↑ Significant increase compared to 1–3 months (\*compared to 4–6 months) period

| Та | b | е | 2 | ſ | The | corre | lated | peri | les | ional | va | lues |
|----|---|---|---|---|-----|-------|-------|------|-----|-------|----|------|
|----|---|---|---|---|-----|-------|-------|------|-----|-------|----|------|

| Perilesional | nADC    | nrCBV   | nrCBF   | nASL    |
|--------------|---------|---------|---------|---------|
| nADC         |         |         |         |         |
| r            | 1       | - 0.973 | - 0.908 | - 0.809 |
| р            |         | 0       | 0.005   | 0.028   |
| nrCBV        |         |         |         |         |
| r            | - 0.973 | 1       | 0.963   | 0.736   |
| р            | 0       |         | 0       | 0.049   |
| nrCBF        |         |         |         |         |
| r            | - 0.908 | 0.963   | 1       | 0.716   |
| р            | 0.005   | 0       |         | 0.041   |
| nASL         |         |         |         |         |
| r            | - 0.809 | 0.736   | 0.716   | 1       |
| р            | 0.028   | 0.049   | 0.041   |         |

Statistically significant data are indicated in bold



Fig. 3 The changes in mean values of the other NAWM areas over time

The alterations over time were assessed using Pearson's correlation test. In perilesional NAWM, strong correlations were determined among the mean values of nADC, nrCBV, nrCBF, and nASL. The strongest was the negative correlation between nrCBV and nADC (r: -0.973,  $p \le 0.001$ ). The other strong correlations were nrCBV-nrCBF (r: 0.963), nrCBF-nADC (r: -0.908), respectively. Moreover, strong correlations of nASL were present with nADC (r: -0.809), nrCBV (r: 0.736), and nrCBF (r: 0.716).

The mean normalized values of ipsilateral frontal, parietal, occipital lobe deep white matter and corona radiata, anterior and posterior limbs of the internal capsule, and the changes of the calculated values over time were presented in Table 2, and the significance of such changes was evaluated. Figure 3 shows the changes in mean values of the other NAWM areas over time.

In the other NAWM areas, no significant changes were determined in nADC and nGRE values over time. In nFA values, when compared to the pretreatment value, a mild but progressive increase was present (~ 6% in the 1–3 months time-point group, and ~ 10% in the > 18 months time-point group); however, the differences were not statistically significant.

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The 1-3 months nrCBV values were determined to be significantly reduced (~ 25%) compared to the preRT values (p: 0.0178). In addition, the values were significantly increased in the final time-point group (the > 18 months group) when compared to the posttreatment 1-3 months group (p: 0.0176); however, the value did not reach the pretreatment level. Similarly, ~ 20% significant reduction was determined in the 1–3 months group in nrCBF values (p: 0.0178), and a significant increase was observed in the > 18 months group compared to the 1-3 months group (p: 0.0026), not reaching the pretreatment values. A similar change was determined in the nASL values; when compared to the pretreatment group, a significant reduction of ~ 30%(p: 0.0480) was determined in the 1–3 months group, ~ 25% (p: 0.0020) in the 4–6 months group, and ~ 30% (p: 0.0199)in the 7–9 months group. Even though ~ 20% increases were determined in the 13-18 months and > 18 months groups compared to the first posttreatment period (p: 0.0265 and p: 0.0434), the significant decrease in the > 18 months group compared to the pretreatment period continued (p: 0.0041).

The changes of calculated mean values of other NAWM areas in Table3 over time were evaluated with Pearson's correlation test. Regarding the alterations over time in other NAWM areas, strong correlations of nASL with nrCBV and nrCBF were determined (*r*: 0.891, and *r*: 0.864, respectively). Besides, there was a strong correlation between nrCBV and nrCBF (*r*: 0.882) (Table 4).

### Discussion

Our study extended the literature findings that after CRT treatment in patients with glioblastoma, perfusion of white matter areas that appear normal in conventional sequences show a significant decrease and this change is more pronounced than in diffusion sequences. In addition, our study determined that ASL perfusion is at least as sensitive as contrast-enhanced perfusion MRI in showing these changes, in addition to previous studies. The convergence of the defined perfusion and ADC findings with time in follow-up imaging suggests that the damage is partially reversible.

To the best of our knowledge, our study is the first study to evaluate time-dependent changes in NAWM after RT by using PASL and DSC perfusion MRI and DAG parameters such as FA and ADC and to examine the correlation between these methods. We showed significant changes in perfusion measurements in each perfusion method, and a strong correlation between perfusion methods and ADC measurements. In addition, our results make an important contribution to the fact that the ASL perfusion method, which does not require external contrast agent administration, can be used instead of contrast perfusion methods, as the use of contrast

| Other NAWM | Pre-treatment | 1–3 months                  | 4–6 months                  | 7–9 months         | 10–12 months | 13–18 months                | >18 months                  |
|------------|---------------|-----------------------------|-----------------------------|--------------------|--------------|-----------------------------|-----------------------------|
| nADC       | 1.03          | 1.03                        | 1.02                        | 1.02               | 1.05         | 1.01                        | 1.01                        |
| nFA        | 1.03          | 0.97                        | 0.97                        | 0.96               | 0.88         | 0.97                        | 0.93                        |
| nGRE       | 1.01          | 1.02                        | 1.02                        | 1.00               | 0.99         | 1.00                        | 1.01                        |
| nrCBV      | 1.12          | 0.83↓<br><i>p</i> : 0.0178  | 0.87                        | 0.88               | 0.87         | 1.02                        | 0.98 ↑<br>p: 0.0176         |
| nrCBF      | 1.07          | 0.86↓<br>p: 0.0178          | 0.90                        | 0.87               | 0.86         | 1.06                        | 0.97 ↑<br><i>p</i> : 0.0026 |
| nASL       | 1.12          | 0.78 ↓<br><i>p</i> : 0.0480 | 0.84 ↓<br><i>p</i> : 0.0020 | 0.79↓<br>p: 0.0199 | 0.84         | 0.94 ↑<br><i>p</i> : 0.0265 | 0.96 ↑*<br>p: 0.0434        |

Table 3 The changes in mean values of the other NAWM areas over time

Statistically significant data are indicated in bold

↓ Significant decrease compared to pretreatment period

↑ Significant increase compared to 1–3 months (\*compared to 4–6 months) period

Table 4 Correlated 'Other NAWM' values

| Other NAWM | nrCBV | nrCBF | nASL  |
|------------|-------|-------|-------|
| nrCBV      |       |       |       |
| r          | 1     | 0.882 | 0.891 |
| р          |       | 0.009 | 0.007 |
| nrCBF      |       |       |       |
| r          | 0.882 | 1     | 0.864 |
| р          | 0.009 |       | 0.012 |
| nASL       |       |       |       |
| r          | 0.891 | 0.864 | 1     |
| р          | 0.007 | 0.012 |       |

Statistically significant data are indicated in bold

material is increasingly questioned due to its potential side effects.

In this study, we used DSC and PASL perfusion methods to examine vascular damage secondary to CRT, and we found a reduction of up to 40% in nrCBV, 35% in nrCBF, and 30% in nASL in perilesional NAWM with expected high radiation exposure, in 1-3 months and 4-6 months time-point groups. In the other ipsilateral NAWM, we calculated this decrease as approximately 25%, 20%, and 30%, respectively. Our findings show that there is a significant decrease in perfusion over time due to radiation in WM, which does not show any change in conventional MRI series. The decrease in nrCBV, nrCBF, and nASL observed in perilesional and other NAWM areas in the 1-3th month time group, first reach a peak value and draw a plateau in the follow-up images, and then increases, although it does not reach pre-treatment values, after 1 year. This finding indicates that perfusion reduction is largely reversible and transient. Fahlstrom et al. [22] showed a reduction of an average of 5% in nCBV and 4% in nCBF in their study with a shorter follow-up period (3.5 months) using only DSC perfusion MRI, although the use of the overall measurement means from both hemispheres explains the lesser reduction. Also, similar to our study, they reported a plateau and reversal in the nCBV and nCBF reduction curves, although not statistically significant, after 2 months. In a few similar studies, decreased rCBV and rCBF values returned to pre-treatment or close values in the following periods [18, 20, 23, 24]. All these findings are consistent with the theory that acute and early delayed effects are reversible [3, 5].

In the literature, there are few studies using the ASL perfusion MRI for evaluating the perfusion changes in normal brain tissue after RT, and in these studies, the gray matter was evaluated in general. Petr et al. [17] used the pCASL method in the group of patients older than 18 years of age with a diagnosis of glioblastoma and found a 10% decrease in global CBF values in the contralateral normal appearing gray matter. They reported that similar to our study, the decrease in perfusion varied according to the dose regions (2-16%) and this decrease was stabilized in the late time group. In our study, on the contrary, it was observed that the decrease in perfusion was reversed more significantly, although not reaching pre-treatment values, in later periods, with longer follow-up periods. Similarly, Matthew et al. [45] showed a decrease in perfusion in normal appearing gray matter (NAGM) after RT with the pCASL in patients diagnosed with Medulloblastoma and Pilocytic Astrocytoma, while Taki et al. [15] showed a decrease in NAGM perfusion after RT with gamma rays.

Unlike our study, there are also studies reporting increased perfusion in normal appearing brain tissue after RT, in the literature. Jabukovic et al. [19] reported a 20% increase in rCBV and rCBF values with DSC perfusion MRI, which they evaluated only in the first month. On the other hand, Hu et al. [32] found 9–17% increased perfusion in different regions in the brain tissue that appeared normal in the acute period after RT in patients with nasopharyngeal carcinoma, without distinguishing between gray and white matter. They commented that vasodilatation and increased blood flow, which occurs as a response of normal brain tissue to radiation in the acute period, can be seen as the cause of increased perfusion.

In this study, we showed that normalized measurements on ADC and FA maps can detect white matter damage and time-dependent changes not seen in conventional series, in NAWM in patients with glioblastoma treated with standard CRT. It is known that RT-induced white matter injury is dose-dependent, and therefore it is inevitable that the WM areas closest to the lesion are more affected [46, 47]. As we move away from the lesion, it is expected that the effect of WM will gradually decrease due to the decrease in the radiation dose exposed. The fact that nADC increase in perilesional NAWM is higher than other NAWM areas in our study supports this information. A similar situation also explains why the decrease in perilesional FA values is higher than in other WM areas. A 20% increase in nADC values and a 19% decrease in nFA values were observed in perilesional NAWM at 1-3 months after RT, indicating loss of axonal integrity in irradiated NAWM areas. A progressive decrease of 10% in mean nFA values in ipsilateral outside of the perilesional (other) NAWM area, although less than in the perilesional area, may suggest the presence of axonal damage. However, we did not detect any significant difference in mean nADC values in other NAWM areas. Similar to our study, Connor et al. [48] using multiple 'b' values, reported a 10-35% increase in mean diffusivity (MD) and a 7-22% decrease in FA values compared to dose sites. In our study with a longer follow-up period, we found that the increase in ADC values was limited and showed a plateau in the late periods. This finding suggests that disruption of axonal integrity is limited by various injury repair mechanisms. Consistent with this finding, Haris et al. [43] in their study on a limited number of patients reported that the early increase in MD and the decrease in FA detected in high-dose regions were limited in the late periods. In addition, many studies have reported an increase in ADC values and a progressive decrease in FA values in different NAWM areas in patients who received radiotherapy for various reasons [23, 45, 49–52].

In the normalized measurements we performed with T2-FFE, which is a T2-weighted GRE sequence, we did not detect any difference over time both in the perilesional area and in the other ipsilateral NAWM areas. This finding means that there are no significant changes such as calcifications or microbleeds that could cause susceptibility artifacts. There are few studies in the literature evaluating microbleed-ing after radiation, and most of them used SWI [53–55]. Although SWI is superior in detecting microbleeds [56], in one study using GRE sequences, up to  $\sim 26\%$  microbleed-ing was detected in the white matter later in T2\*A images [57], and in another study up to 4% reduction in T2\* signal has been reported [58]. The reason why no difference

was observed in our study may be due to the GRE imaging parameters we used and the limited number of patients.

There are very few studies evaluating the radiation-related effects of NAWM with both diffusion and perfusion parameters [23, 24, 33]. Nilsen et al. [23] investigated the changes in diffusion and vascular function over time in NAWM after Stereotactic Radiosurgery in patients with brain metastases and evaluated radiation dose regions using DSC Perfusion MRI and diffusion MRI. In their study that included a heterogeneous group with 15-25 GY radiation dose exposure in patients, they found that after reaching the peak value of 5% in the low-dose region and 9% in the high-dose region, it decreased to 2.5% and 3%, respectively. They stated that the reduction in nCBV and nCBV was also partially reversible, similar to ADC. When compared with the reported nCBV and nCBF values, the perfusion improvement that did not return to the pre-treatment values we found in our study is consistent. Naturally, we find more pronounced changes due to the homogeneous patient group and chemotherapy regimen and exposure to a higher amount of standard radiation dose.

In this study, we found a strong correlation between perfusion measurements and nADC measurements in perilesional NAWM exposed to high-dose radiation. The strongest correlation was found between nADC and nrCBV, then between nrCBV and nrCBF. In the other NAWM, a strong correlation was found only between perfusion measurements, and the strongest correlation was between nASL and nrCBV averages. Weber et al. [14] found a strong correlation between the PASL method and DSC perfusion methods, similar to our study, in their study evaluating the contralateral hemisphere with DSC perfusion and two different PASL perfusion methods (ITS-FAIR, Q2TIPS).

In our study, the nASL values, which show a high correlation with the perfusion parameters obtained by the contrastenhanced DSC MRI method, are remarkable. The use of gadolinium-containing MR contrast agents has become an increasingly questionable subject due to the risk of Nephrogenic Systemic Fibrosis (NSF), which is an accumulation disease that can result in death, restricted use in pregnant women, lactation period and newborns, and possible side effects. For these reasons, the importance of advanced MRI methods without contrast material, such as ASL perfusion, is increasing. In recent years, many studies using the ASL perfusion method have been reported as an alternative to the DSC perfusion imaging method. There are publications reporting that the ASL perfusion imaging is less sensitive to susceptibility artifacts than DSC perfusion [59, 60]. Due to the bolus contrast agent required in DSC perfusion, the advantage of reproducibility in ASL perfusion imaging becomes prominent. Apart from this, providing absolute quantification in ASL-based perfusion examinations and limited exposure due to disruption of the blood-brain barrier (leaked contrast agent in DSC perfusion examinations causes residual signal loss) are other advantages. For all these reasons and due to the high correlation with contrast-enhanced perfusion MRI in our study, we think that the ASL perfusion method can also be performed for the perfusion studies on the normal appearing brain parenchyma.

### Limitations

Due to the retrospective design of the study, the probability of recording errors is high. Although the number of our patients was relatively low, this limitation was attempted by the unity of histopathological diagnosis, homogeneity of the CRT regimen (60 Gy/30 Fr), the lack of use of other known treatment agents, and the high number of analyses. Multivariate analysis was not possible because the number of patients differed between time groups and each patient was not included in each time group. We could not examine dose-dependent changes because the planned dose information before RT could not be included in the examinations. However, we tried to avoid this limitation by grouping perilesional NAWM representing high radiation exposure and ipsilateral other NAWM areas representing average radiation dose exposure. Although circular ROI areas are considered to be a limitation compared to voxel-based measurements, this effect was tried to be avoided by keeping their size  $(\pm 3)$ pixels) similar and the SD value minimal. While selecting the ROI, values less than 0.2, which is suggesting gray matter contamination, in FA measurements were avoided. Another limitation is that it is impossible to differentiate completely from surgical effect and wound healing in the perilesional area. We tried to limit this effect by excluding the enhanced perilesional tissue from the ROI area and evaluating other conventional MR studies such as GRE. In addition, the absence of a significant change in the T2-weighted GRE (T2 FFE) sequence obtained with ROIs in similar areas indicates that areas such as microbleeds that may cause sensitivity artifacts are avoided and that measurements are made from areas that appear normal with conventional series. And finally, ASL perfusion examinations were performed on a 1.5 T MR device using the PASL method, and relatively newer methods such as pCASL with higher Signal-to-Noise-Ratio (SNR) could not be used.

# Conclusion

In our current study, we found a perfusion reduction and increased diffusion in NAWM in patients with glioblastoma treated with CRT. We also observed that these findings were more common in the perilesional region due to high radiation exposure. However, we determined that these changings were reversible over time. These findings show that the brain parenchyma, which appears normal in conventional sequences, is also affected by treatment, and this damage can be demonstrated by perfusion and diffusion MR imaging.

We showed that the power of detecting perfusion changes of the ASL perfusion method is similar to that of the contrast perfusion methods. For this reason, we think that ASL and DCE perfusion methods can be used as biomarkers for the evaluation of CRT-related damage in NAWM, however, ASL perfusion methods should be preferred instead of contrastenhanced methods due to their high correlation and usage advantages.

Our findings need to be supported by new studies with a larger patient group and standardized follow-up protocol investigating the effects of CRT on normal brain tissue. In addition, studies involving neurocognitive tests and perfusion and diffusion changes in NAWM and the effects of pathophysiological changes on the cognitive status of patients should be evaluated. Thus, the quality of life of the patients can be increased with treatment and post-treatment follow-up arrangements.

## Declarations

Conflict of interest The authors declare no conflict of interest.

**Ethical statement** This retrospective study was approved by the local ethics committee of our institution.

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