ORIGINAL ARTICLE



# Low-level laser irradiation induces in vitro proliferation of stem cells from human exfoliated deciduous teeth

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Abstract The aim of this study was to evaluate the effect of low-level laser irradiation (LLLI) on the proliferation and viability of stem cells from human exfoliated deciduous teeth (SHED). Cells were irradiated or not (control) with an InGaAlP laser diode (660 nm, 30 mW, continuous action mode) using two different energy densities  $(0.5 \text{ J/cm}^2 - 16 \text{ s})$ ; 1.0 J/cm<sup>2</sup>-33 s). Irradiation was performed at 0 and 48 h. with the laser probe fixed at a distance of 0.5 cm from the cells. Cell proliferation was analyzed at 0, 24, 48, and 72 h by the Trypan blue exclusion method and MTT assay. Cell cycle and Ki67 expression were analyzed by flow cytometry. Apoptosis-related events were evaluated by expression of annexin V/PI and nuclear morphological changes by staining with DAPI. Differences between groups at each time were analyzed by the Kruskal-Wallis and Mann-Whitney tests, adopting a level of significance of 5% (p < 0.05). The results showed that an energy density of 1.0 J/cm<sup>2</sup> promoted an increase in cell proliferation at 48 and 72 h compared to the control and 0.5 J/cm<sup>2</sup> groups. Cell cycle analysis revealed a predominance of cells in the S and G2/M phases in the

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irradiated groups. This finding was confirmed by the increased expression of Ki67. Low positive staining for annexin V and PI was observed in all groups, and no nuclear changes were detected, indicating that cell viability was not affected by the energy densities tested. It can be concluded that the LLLI parameters used (660 nm, 30 mW, 1.0 J/cm<sup>2</sup>) promote the proliferation of SHEDs and the maintenance of cell viability.

Keywords Deciduous teeth  $\cdot$  Dental pulp  $\cdot$  Stem cells  $\cdot$  Laser therapy  $\cdot$  Cell proliferation

## Introduction

Stem cells from human exfoliated deciduous teeth (SHEDs) were isolated by Miura et al. [1] as a population of clonogenic cells with proliferative capacity that are able to differentiate into a variety of cell types. Experiments using these cells have shown significant differences in the biology of stem cells obtained from deciduous and permanent teeth. When compared to stem cells isolated from the pulp of permanent teeth, SHEDs exhibited a higher proliferation rate [2] and a larger number of cell divisions—which could facilitate their in vitro expansion, as well as greater colony formation, in vivo osteoinductive capacity, and formation of different tissues of the dentin pulp complex [1].

The isolation of SHEDs is a simple and convenient process that causes little or no trauma considering that every child loses deciduous teeth, thus representing the perfect opportunity of recovering and storing stem cells to treat diseases or injuries in the future [3]. However, these cells need to be stored for subsequent clinical use, and their yield in culture is usually low. Thus, stimulation of in vitro proliferation is fundamental to obtain an adequate number of cells [4]. Low-level laser irradiation (LLLI) could be an effective strategy for promoting significant expansion of the number of cells in vitro and their subsequent differentiation and may therefore be a useful tool in in vivo regenerative processes and tissue engineering protocols. The important physiological effect of LLLI has been related to its capacity to stimulate the proliferation of different cell types [5]. Studies have shown that stimulation with LLLI increases the proliferation rate of different cells such as fibroblasts [6, 7], endothelial cells [8], and osteoblasts [9].

Few of the various sources of stem cells have been submitted to laser irradiation [10–12], a fact highlighting the need for further studies to better understand the effect of laser therapy on the proliferation of these cells. With respect to laser therapy applied to stem cells of dental origin, most studies have used stem cells derived from the pulp of permanent teeth, while investigations using other dental or periodontal sources of stem cells are sparse in the literature [12, 13]. Therefore, we tested the hypothesis that LLLI promotes proliferation of SHEDs. For this purpose, we performed in vitro cell proliferation and viability assays and evaluated cell cycle, apoptosis, and nuclear morphology in order to assess the influence of LLLI on the biological activity of SHEDs.

#### Materials and methods

The study was approved by the Ethics Committee of the Federal University of Rio Grande do Norte (Approval No. 34913314.4.0000.5537). Three human deciduous teeth exhibiting at least one third of physiological root resorption were used for the isolation of SHEDs.

#### **Cell culture**

After extraction, each tooth was immediately transferred to a Falcon tube (TPP, Trasadingen, Switzerland) containing 5 mL alpha-MEM medium (Gibco, Carlsbad, CA, USA) and stored at 4 °C. In a laminar flow chamber, the teeth were submitted to the protocol described by Vasconcelos et al. [14] to prevent possible contamination with microorganisms: three washes of 10 min each with a solution containing alpha-MEM medium supplemented with 10,000 IU/mL penicillin, 10 mg/mL streptomycin, 100 mg/mL gentamicin, and 250  $\mu$ g/mL amphotericin B (all reagents from Gibco, Carlsbad, CA, USA).

SHEDs were obtained according to the protocol of Ginani et al. [15]. The pulp tissue was carefully removed by curettage using an endodontic excavator (Dentsply Maillefer, Ballaigues, Switzerland), and the extract was digested with 3 mg/mL collagenase I (Gibco, Carlsbad, CA, USA) and 4 mg/mL dispase (Gibco, Carlsbad, CA, USA) for 1 h at 37 °C. The cultures were incubated in alpha-MEM medium supplemented with 15% fetal bovine serum (Gibco, Carlsbad, CA, USA) at 37 °C in a 5% CO<sub>2</sub> atmosphere until they reached 70–90% confluence. The medium was changed every 3 days.

In the first passage (P1), the cells were analyzed to confirm their stem cell nature according to the criteria proposed by Dominici et al. [16]. Briefly, an aliquot of cells was evaluated by flow cytometry using the Human MSC Analysis Kit (BD Stemflow<sup>™</sup>, BD Biosciences, San Jose, CA, USA), which permits to identify mesenchymal stem cells by detecting positive (CD105 PerCP-Cy5.5, CD73 APC, CD90 FITC) and negative (CD45, CD34, CD11b, CD19, HLA-DR PE) expression of cell surface markers. In addition, the cells were cultured in osteogenic and adipogenic differentiation medium (StemPro® Differentiation Kits, Invitrogen, Carlsbad, CA, USA) for up to 21 days, and the multipotent nature of SHEDs was confirmed by von Kossa (Abcam, Cambridge, UK) and Oil Red (Sigma-Aldrich, St. Louis, MO, USA) staining.

#### **Experimental design**

Figure 1 illustrates the steps performed in this study. After characterization, SHEDs were expanded and divided into three groups according to treatment: (1) control: no irradiation, (2) Laser 0.5: cells irradiated with a dose of 0.5 J/cm<sup>2</sup>, and (3) Laser 1.0: cells irradiated with a dose of 1.0 J/cm<sup>2</sup>. Next, assays were conducted for evaluating cell viability and proliferative capacity in all groups and to identify apoptosis-related and cell cycle events.

## Laser irradiation

Cells of groups 2 and 3 in the third and fourth passage (P3 and P4) were irradiated with an InGaAlP laser diode (Bio Wave LLLT Dual, Kondortech, São Carlos, SP, Brazil) in the continuous action mode using the following parameters: power of

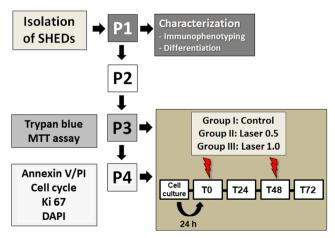


Fig. 1 Study design. P passage, T time of analysis after the first irradiation (in hours)

30 mW, wavelength of 660 nm, doses of 0.5 and 1.0 J/cm<sup>2</sup>, irradiation time of 16 s  $(0.5 \text{ J/cm}^2)$  and 33 s  $(1.0 \text{ J/cm}^2)$ , and tip diameter of 0.01 cm<sup>2</sup>. The irradiation probe was applied perpendicular to the plate at a distance of 0.5 cm from the cells. The power of the laser was measured with a LaserCheck Power Meter (Coherent Inc., Santa Clara, CA, USA) before each application.

The cells were irradiated at 0 and 48 h, and the analyses were carried out at 0, 24, 48, and 72 h after the first laser application. For the Trypan blue exclusion test and MTT assay, the cells were cultured in 24 and 96-well plates, respectively. Irradiation was applied to the center of each well. For the cell cycle, Ki67 expression, and apoptosis assays, the cells were cultured in 6-well plates and the laser was applied at five fixed and distinct points in each well. The cells were plated in such a way that there was an empty well between seeded wells to prevent the unintentional spread of light between wells during laser application.

#### Analysis of cell proliferation

Cell proliferation was analyzed by the Trypan blue exclusion method and by the MTT assay at 0, 24, 48, and 72 h after the first irradiation. All assays were carried out in quadruplicate (n = 4). For Trypan blue staining (Gibco, Carlsbad, CA, USA), the cells were cultured in 24-well plates at a density of 2 × 10<sup>4</sup> cells/well. The number of Trypan blue-stained cells in each well was counted in a Neubauer chamber (Optik Labor, Lancing, UK) at the time points analyzed. For the MTT assay (Invitrogen, Carlsbad, CA, USA), the cells were cultured in 96-well plates at a density of 5 × 10<sup>3</sup> cells/well and absorbance was measured in a microplate reader (Epoch, BioTek Instruments, Winooski, VT, USA) at 570 nm.

#### Cell cycle analysis

To evaluate the effects of laser therapy on the cell cycle, cells of each group were cultured in triplicate (n = 3) in 6-well plates at a density of  $2 \times 10^5$  cells/well. The cells were processed after the intervals studied (0, 24, 48, and 72 h), and 5 µL propidium iodide (PI, 25 mg/mL; Invitrogen, Carlsbad, CA, USA) in 200 µL ice-cold PBS (Gibco, Carlsbad, CA, USA) was added for analysis in a FACS Canto II flow cytometer (BD Biosciences, San Jose, CA, USA).

## Analysis of Ki67 expression

The expression of nuclear protein Ki67 was analyzed by flow cytometry. For this purpose, the cells were cultured in triplicate (n = 3) in 6-well plates at a density of  $2 \times 10^5$  cells/well. After 72 h (T72), the cells were processed and incubated with 10 µL of FITC-conjugated anti-Ki67 monoclonal antibody (Clone 7B11, Invitrogen, Carlsbad, CA, USA) for 20 min in

the dark and analyzed in a flow cytometer (FACS Canto II, BD Biosciences, San Jose, CA, USA).

#### Analysis of apoptosis

The effects of laser therapy on apoptosis were analyzed using the FITC/Annexin V Dead Cell Apoptosis Kit with FITC annexin and PI for flow cytometry (Invitrogen, Carlsbad, CA, USA). The cells were cultured in triplicate in 6-well plates at a density of  $2 \times 10^5$  cells/well. After the last interval analyzed (T72), the cells were processed and incubated with 3 µL FITC annexin V and 1 µL PI (100 µg/mL) for 15 min at room temperature in the dark. After incubation, the cells were analyzed by flow cytometry (FACS Canto II, BD Biosciences, San Jose, CA, USA), measuring fluorescence emission at 530 and 575 nm.

### Analysis of nuclear morphology

To evaluate the presence of nuclear damage in the cells submitted to laser therapy, the cells were cultured in 24-well plates at a density of  $2 \times 10^4$  cells/well. After 72 h, the cells were incubated with 4'-6-diamidino-2-phenylindole (DAPI; Molecular Probes, Carlsbad, CA, USA) diluted 1:1000 for 20 min in a dark chamber. The cells were examined under a fluorescence microscope (Eclipse Ti-U, Nikon Instruments Inc., Melville, NY, USA) to identify the presence of pyknotic nuclei and nuclear fragmentation in cells of the three groups.

## Statistical analysis

Statistical analyses were carried out using GraphPad Prism 6.0 software (GraphPad, San Diego, CA, USA). Since data did not show normal distribution (Shapiro–Wilk test, p < 0.05), non-parametric analyses were performed. Differences between groups at each time point (0, 24, 48, and 72 h) were analyzed by the Kruskal–Wallis and Mann–Whitney tests, adopting a level of significance of 5% (p < 0.05; beta 0.2; power 0.8).

## Results

Pulp cells were positive for the surface markers CD90 (98.8%), CD73 (99.9%), and CD105 (97.4%), while less than 1% of cells were positive for CD45, CD34, CD11b, CD19, and HLA-DR. Light microscopy revealed the deposition of mineralized matrix stained with von Kossa stain and the presence of lipid vesicles stained with Oil Red O, indicating the differentiation of cells into osteoblasts and adipose cells, respectively (Fig. 2).

Analysis of the number of viable cells by the Trypan blue exclusion method revealed that the dose of  $1.0 \text{ J/cm}^2$ 

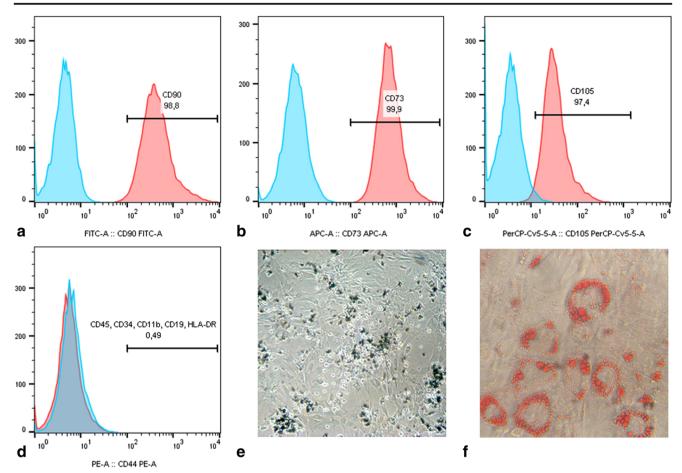


Fig. 2 a-d Expression of stem cell markers in SHEDs: a CD90, b CD73, c CD105, and d negative cocktail. e-f Photomicrographs of SHEDs subjected to osteogenic (e; von Kossa stain, original magnification ×40) and adipogenic differentiation (f; Oil Red, original magnification ×100)

promoted an increase in cell proliferation at 48 and 72 h when compared to the control and Laser 0.5 groups (p < 0.05). Cell proliferation was lower in the control group compared to the irradiated groups (Laser 0.5 and Laser 1.0), with a statistically significant difference (p < 0.05) between the irradiated groups at 72 h (Fig. 3).

The results of mitochondrial activity measured by the MTT assay were similar to the Trypan blue counts. In this respect, a significantly greater reduction of MTT was observed in the group irradiated with the dose of 1.0 J/cm<sup>2</sup> at 24, 48, and 72 h when compared to the non-irradiated group. A significant difference between the irradiated groups was only observed at 48 h (Table 1).

The distribution of cells across the different cell cycle phases was consistent with proliferating cells throughout the experiment, with a predominance of cells in the S and G2/M phases in the group irradiated with 1.0 J/cm<sup>2</sup> at T48 and T72 (Fig. 4a–d). At 72 h after the first irradiation, expression of nuclear protein Ki67 was higher in cells of the irradiated groups compared to the control, with the dose of 1.0 J/cm<sup>2</sup> promoting the highest expression of Ki67 (Fig. 4e). This result corroborates the findings of cell cycle analysis, showing that cells of the Laser 1.0 group were in the proliferative phase.

Regarding the evaluation of apoptosis, the cells exhibited low levels of fluorescence for annexin V and PI by flow cytometry—which is compatible with viable cells—at 72 h, demonstrating the absence of significant alterations throughout the experiment (Fig. 5a–c). This finding indicates that the doses studied did not cause cell damage in SHEDs. Cells

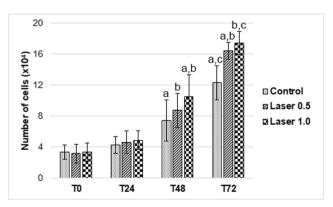


Fig. 3 Number of SHEDs at the different time points studied. The same lowercase letters indicate a statistically significant difference (p < 0.05; Mann–Whitney test)

**Table 1** Absorbance values ofSHEDs at each time point in thedifferent groups studied

	Control	Laser 0.5	Laser 1.0	$p^{\mathrm{a}}$		
				C vs. 0.5	C vs. 1.0	0.5 vs. 1.0
T0	$0.306 \pm 0.080$	$0.334 \pm 0.061$	$0.358 \pm 0.070$	0.3624	0.0524	0.2152
T24	$0.387\pm0.077$	$0.469\pm0.060$	$0.454\pm0.055$	0.0038	0.0077	0.6619
T48	$0.593 \pm 0.095$	$0.608\pm0.088$	$0.695\pm0.088$	0.9430	0.0127	0.0184
T72	$0.696\pm0.095$	$0.773\pm0.095$	$0.813\pm0.076$	0.1067	0.0183	0.4965

Values are the mean  $\pm$  standard deviation. The numbers in italics indicate a statistically significant difference (p < 0.05)

<sup>a</sup> Mann-Whitney test

submitted to laser therapy exhibited no significant morphological nuclear damage such as nuclear fragmentation or pyknotic nuclei over the period studied (Fig. 5d–f).

## Discussion

Dental stem cells are isolated from dental alveolar tissues [17, 18] and are characterized by high proliferative capacity and plasticity. These cells can be used for the regeneration of dental facial structures (e.g., alveolar bone, dentin pulp complex) or other tissues such as neural tissue [19]. Human deciduous teeth have been reported as a promising source of mesenchymal stem cells, which can be used in different clinical applications such as dental tissue engineering [1], repair of bone defects [20], and even the treatment of neural tissue damage and degenerative diseases [21, 22].

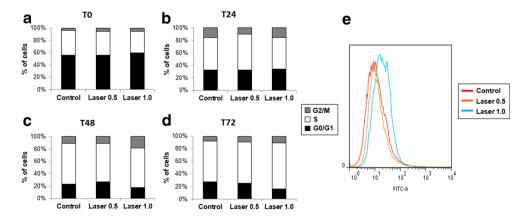
The simple and convenient isolation of SHEDs and nonsignificant immunogenicity, which permits their use in allogenic transplants without the need for immunosuppressors [21, 23, 24], confer important clinical utility, including the creation of cell banks. However, the proliferation of these cells is a time-consuming process, and the development of methods that increase the number of available cells within a short period of time is fundamental. Within this context, one possible approach suggested in the literature is LLLI [25–27]. The biostimulating effect of LLLI has been reported for more than four decades. Since its first description, researchers in this field have tried to develop the best laser therapy protocol that would promote positive biostimulating effects attributed to low-level lasers [28]. Few of the various sources of stem cells have been submitted to laser irradiation [11–13], especially stem cells of dental origin. Thus, further studies using stems cells obtained from other sources are needed to better understand the effect of laser therapy on the proliferation of these cells. The present study evaluated the effect of LLLI on SHEDs, a source of dental stem cells that has been poorly studied, with only three published reports [28–30].

Regarding the effect of LLLI on pulp stem cells, positive effects of laser therapy on stem cells derived from the pulp of permanent teeth have been reported [27, 31, 32]. Investigation of the treatment of SHEDs with LLLI has shown positive effects on the survival of these cells under stress conditions [30] and on dental osteogenic differentiation [29]. However, this is the first study that investigated, in addition to cell viability and proliferation, the effects of laser therapy on cell cycle, apoptosis, and nuclear morphology, and favorable results regarding these biological events were obtained.

The choice of parameters of LLLI such as wavelength, power, and energy density influences the desirable proliferation results [26]. In this respect, both visible (red) and infrared lights exert biological effects on irradiated cells, and better results in terms of cellular biostimulation have been reported

Fig. 4 a–d Distribution of SHEDs across the phases of the cell cycle in the different groups at the time points analyzed. The percentage of each phase represents the mean of triplicate experiments. e

Immunoexpression of Ki67 in the groups studied. FlowJo (USA)



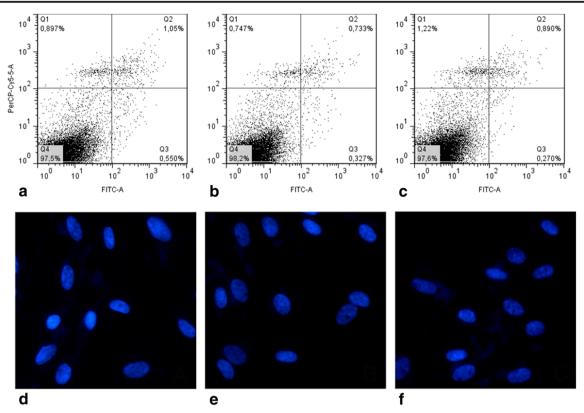


Fig. 5 a–c Immunostaining of SHEDs with annexin V/PI at 72 h. Annexin V negative/PI positive (Q1), annexin V/PI positive (Q2), annexin V positive/PI negative (Q3), and annexin V/PI negative (Q4). a

Non-irradiated control group. **b** Laser 0.5 group. **c** Laser 1.0 group. **d**–**f** Photomicrographs of SHEDs stained with DAPI after 72 h of culture. **d** Control. **e** Laser 0.5. **f** Laser 1.0 (DAPI staining, ×400)

for the wavelength of 600 to 700 nm [33-35]. We therefore chose the wavelength of 660 nm, which promoted positive effects similar to those reported by Soares et al. [26], Zaccara et al. [27], and Eduardo et al. [31], confirming the biostimulating effect of the red light spectrum. In addition to the wavelength, the dose (energy density) is another parameter that needs to be considered when cellular biostimulation is desired. Doses ranging from 0.5 to 10 J/cm<sup>2</sup> are used to induce cell proliferation, while doses higher than 10 J/cm<sup>2</sup> exert antiproliferative effects [35]. Energy densities ranging from 0.5 to 4 J/cm<sup>2</sup> have been more effective in stimulating the growth of stem cells [25–27, 36, 37], but the effect of varying energy density while maintaining the laser power constant is unknown for SHEDs.

According to Karu [38], an increase in energy density can damage photoreceptors, which reduces the biomodulatory effect of the laser. Lower doses therefore reduce the risk of cell damage and, in the case of stem cells, contribute to an increase in the population of these cells, maintaining their initial characteristics intact [26]. Using lower doses (0.5 and 1.0 J/cm<sup>2</sup>), laser therapy employed in the present study promoted biostimulation without causing damage to nuclear morphology or the loss of viability. This fact was confirmed by DAPI staining of the nuclei of irradiated cells, which demonstrated intact nuclei and the absence of nuclear fragmentation or pyknotic nuclei. In addition, analysis of apoptosis-related markers (annexin V/PI) showed that most of the cells subjected to laser therapy remained viable, supporting that LLLI does not affect the viability of the cells studied.

Our results corroborate the findings of Fernandes et al. [28] regarding the successful stimulation of proliferation of stem cells derived from the pulp of deciduous teeth using a wavelength of 660 nm and a low dose ( $1.2 \text{ J/cm}^2$ ). However, the authors evaluated different combinations of dose and power ( $1.2 \text{ J/cm}^2$ –0.5 mW,  $2.5 \text{ J/cm}^2$ –10 mW,  $3.7 \text{ J/cm}^2$ –15 mW,  $5.0 \text{ J/cm}^2$ –20 mW, and  $6.2 \text{ J/cm}^2$ –25 mW), and cell proliferation was assessed after very short intervals (6 and 24 h). In fact, variations in the parameters of laser therapy have been one of the main obstacles to the comparison of studies on photobiomodulation [39].

Doses of 0.5 and 1.0 J/cm<sup>2</sup> have been tested in studies on stem cells derived from the human periodontal ligament [26] and from the pulp of permanent teeth [27], with the other parameters of laser therapy being the same as those employed in the present study. Pulp stem cells from permanent teeth exhibited higher proliferation at the last time points studied (72 and 96 h after irradiation) when irradiated with the dose of 1.0 J/cm<sup>2</sup> compared to the non-irradiated control group [27]. A similar behavior has been demonstrated for stem cells derived from human periodontal ligament, which exhibited a

significantly higher proliferation rate when irradiated with a dose of  $1.0 \text{ J/cm}^2$  compared to the non-irradiated group at the last time points evaluated (48 and 72 h after irradiation) [26]. These results and the present findings suggest that the dose of  $1.0 \text{ J/cm}^2$  is effective in increasing the proliferation of other sources of stem cells. Furthermore, this dose resulted in a more marked proliferative response of SHEDs when compared to the dose of  $0.5 \text{ J/cm}^2$ , as demonstrated by the expression of Ki67 and cell cycle distribution of cells.

Cell cycle analysis demonstrated the distribution of cells in the phases consistent with cell proliferation (S and G2/M), corroborating previous findings obtained for dental pulp stem cells [27]. Although the exact molecular mechanism whereby LLLI exerts its effects on cell proliferation is not fully understood, experimental data show that irradiation is followed by an increase in the synthesis of growth factors, nitric oxide, reactive oxygen species, ATP, RNA, and DNA [40]. In the MTT assay, the group irradiated with the dose of  $1.0 \text{ J/cm}^2$ exhibited better results at 24, 48, and 72 h after the first irradiation compared to the non-irradiated (control) group and performed significantly better than the group irradiated with the dose of 0.5 J/cm<sup>2</sup> at 48 h. These results agree with Barboza et al. [25] who irradiated bone marrow and adipose tissue stem cells and Stein et al. [41] who irradiated human osteoblasts. Both studies reported increased cell proliferation when a wavelength of 660 nm and a dose of 1.0 J/cm<sup>2</sup> were used.

Returning to the hypothesis posed at the beginning of this paper, it is now possible to state that LLLI under the conditions used in this study (power of 30 mW, wavelength of 660 nm, and energy density of 1.0 J/cm<sup>2</sup>) stimulates the proliferation of SHEDs without affecting cell viability. These data have potential clinical relevance since LLLI represents a therapeutic opportunity, especially in the field of cell therapy and tissue engineering. Considering the limited number of experiments and heterogeneity of the methods employed, further studies are needed to establish the ideal parameters of laser therapy for stimulating the differentiation of this type of cells.

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#### Compliance with ethical standards

**Conflict of interest** The authors declare that they have no conflict of interest.

**Ethical approval** All procedures performed in the study were in accordance with the Ethics Committee of the Federal University of Rio Grande do Norte (Approval No. 34913314.4.0000.5537) and with the 1964 Declaration of Helsinki and its later amendments or comparable ethical standards.

**Informed consent** Informed consent was obtained from all individual participants included in the study.

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