ORIGINAL ARTICLE

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A CO₂ removal system using extracorporeal lung and renal assist device with an acid and alkaline infusion

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Abstract

The patients with respiratory failure need high tidal volume by mechanical ventilation, which lead to the ventilator-induced lung injury. We developed an extracorporeal lung and renal assist device (ELRAD), comprising acid infusion, membrane lung, continuous hemodiafiltration and alkaline infusion. To evaluate this system, we conducted in vivo studies using experimental swine which were connected to the new system. In vivo experiments consist of four protocols; baseline = hemodiafiltration only (no O_2 gas flow to membrane lung); membrane lung = "Baseline" plus O_2 gas flow to membrane lung; "Acid infusion" = "Membrane lung" plus continuous acid infusion; ELRAD = "Acid infusion" plus continuous alkaline infusion. We changed the ventilatory rate of the mechanical ventilation to maintain PCO_2 at 50-55 mmHg during the four protocols. The results showed that there was statistically no significant difference in the levels of pH, HCO_3^- , and base excess when each study protocol was initiated. The amount of CO_2 eliminated by the membrane lung significantly increased by 1.6 times in the acid infusion protocol and the ELRAD protocol compared to the conventional membrane lung protocol. Minute ventilation in the ELRAD protocol significantly decreased by 0.5 times compared with the hemodiafiltration only protocol (P<0.0001), the membrane lung (P=0.0006) and acid infusion protocol (P=0.0017), respectively. In conclusion, a developed CO_2 removal system efficiently removed CO_2 at low blood flow and reduced minute ventilation, while maintaining acid—base balance within the normal range.

 $\textbf{Keywords} \ \ \text{Extracorporeal circulation} \cdot \text{Renal replacement therapy} \cdot \text{Respiratory insufficiency} \cdot \text{Lung injury} \cdot \text{Hemodiafiltration}$

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Abbreviations

CHDF Continuous hemodiafiltration
ECCO2R system Extracorporeal carbon dioxide removal

system

ELRAD Extracorporeal lung and renal assist

device

PEEP Positive end expiratory pressure VCO₂ML The amount of CO₂ eliminated by the

membrane lung

Introduction

Patients with respiratory failure including acute respiratory distress syndrome often require a high minute volume of the mechanical ventilation to prevent not only hypoxia but also hypercapnia [1–5]. The high minute volume results in high driving pressure, which can potentially cause lung injury;



recent guidelines recommend a low tidal volume of 4–8 ml/kg/predicted body weight [6, 7]. Because additional lung injury due to mechanical ventilation is obviously harmful to patients with respiratory failure, the development of alternative methods for CO₂ removal which can avoid lung injury is a crucial research topic, and may contribute to improved clinical outcomes [8–11].

An extracorporeal carbon dioxide removal system (ECCO2R system), which is a system for CO2 removal from blood using extracorporeal circulation and an artificial membrane lung, was considered to be a practical method for clinical application [8, 12–15]. However, a conventional ECCO2R system requires high blood flow to achieve sufficient CO₂ removal, which potentially limits the clinical application. To overcome this limitation, numerous CO₂ removal approaches have been investigated [16, 17]. The initially reported techniques involved the addition of acid (e.g., lactic acid) to blood upstream to the ECCO2R system, which increased CO₂ removal by changing bicarbonate ion to CO_2 (H⁺+HCO₃⁻ \leftrightarrow H₂CO₃ \leftrightarrow CO₂+H₂O) [18–20]. However, these trials resulted in a high level of accumulated molecules such as lactic acid. Since the blood lactate level is an important marker for critically ill patients, hyperlactatemia due to the infusion of lactic acid reduces the utility of blood lactate levels as a marker [21]. Furthermore, lactic acid causes vasodilation which may be harmful for critically ill patients [22]. More recent studies have reported on another CO₂ removal system in which acid is added to the blood using an "electrolyte bath." In these reports, the acid was generated by oxidation-reduction reaction instead of direct H⁺ addition [23, 24]. However, the system required a complex circuitry including several hemodialysis systems and multiple pumps, which would potentially result in the limitation of clinical use.

We have developed an ECCO2R system, which has a high efficiency of CO₂ removal based on a simple and easy-to-setup to permit clinical application. The system comprises an acid infusion, membrane lung, continuous hemodiafiltration (CHDF) for pH adjustment and removal of accumulated molecules, and alkaline infusion. To evaluate this system, we conducted in vivo study using experimental swine, taking potential application for humans into consideration. Since this system has the ability to remove CO₂ and provide renal support through continuous hemodiafiltration, we coined it as the Extracorporeal Lung and Renal Assist Device (ELRAD).

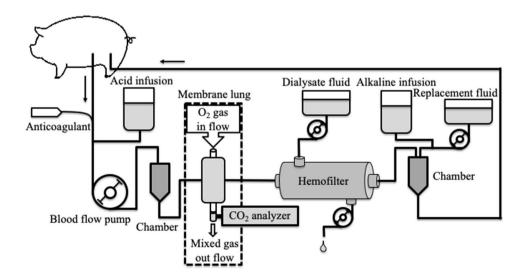
Materials and methods

Extracorporeal circulation system

The ELRAD system was created by combining devices which are commonly used in clinical practice including vascular access catheter (12Fr, GentleCath®, Nippon Sherwood, Tokyo, Japan), bedside console and extracorporeal circuit for CHDF (TR-525®, TORAY Medical, Tokyo, Japan), hemofilter (FB-150Uβeco® [membrane surface 1.5 m²], NIPRO, Osaka, Japan), dialysate fluid (Sublood BSG® [HCO₃⁻ 35 mEq/L, Cl⁻ 111.5 mEq/L], Fuso Pharmaceutical Industries, Osaka, Japan), replacement fluid (Bicarbon® [HCO₃⁻ 25 mEq/L, Cl⁻ 113 mEq/L], AY Pharmaceuticals, Tokyo, Japan) and a membrane lung (Capiox RX05 Baby RX Oxygenator® [membrane surface 0.5 m²], TERUMO, Ann Arbor, MI, USA). The membrane lung was interposed between the blood pump and hemofilter (Fig. 1).

Hydrochloric acid (Wako Pure Chemical Industries, Osaka, Japan) was titrated with distilled water to produce a 0.5 mol/L acid solution [25], and trometamol (concentration 0.3 mol/L) (THAM®, Otsuka, Tokushima, Japan) was used as an alkaline solution for adjustment of the bicarbonate ion. The acid infusion port was set upstream to the membrane

Fig. 1 Experimental circuit





lung, and the alkaline infusion port was set downstream to the hemofilter. Unfractionated heparin (Heparin Sodium, Mochida Pharmaceutical Co., Ltd. Tokyo, Japan.) was used as an anticoagulant for extracorporeal circulation.

Swine model

Six healthy female crossbred pigs (age, 3–4 months; body weight, 38 ± 2 kg) were studied at Fujita Health University, Japan. Propofol and rocuronium bromide were used through an ear vein as their respiration was synchronized for mechanical ventilation after intubation [see Appendix (Supplemental Digital content)].

Mechanical ventilator and ELRAD setting

Oral endotracheal intubation and pressure-controlled mechanical ventilation (EvitaXL®, Dräger Medical, Lübeck, Germany) were performed under anesthesia. The inspired oxygen fraction was fixed at 0.4, the positive end expiratory pressure (PEEP) at 5 cm $\rm H_2O$, and tidal volume at 8 mL/kg, respectively.

The double lumen vascular access catheter, which was inserted into the right jugular vein, was connected to the ELRAD circuit. The blood flow in the ELRAD circuit was 200 mL/min, O₂ gas flow of the membrane lung was 10 L/min, dialysate flow was 1000 mL/h, filtration flow 1500 mL/h and replacement flow 500 mL/h. The acid and alkaline infusion rate was 480 mL/h.

Experimental protocols

The in vivo experiment consisted of four protocols; each protocol took 1 h. To align the initial condition of each protocol, an interval period of 1 h was utilized between protocols (Fig. 2).

Baseline hemodiafiltration only (no O_2 gas flow to

membrane lung)

Membrane lung "Baseline" plus O₂ gas flow to membrane

lung

Acid infusion "Membrane lung" plus continuous acid

infusion

ELRAD "Acid infusion" plus continuous alkaline

infusion

To evaluate the efficiency of CO_2 removal using the extracorporeal system for the four protocols, we changed the ventilatory rate of the mechanical ventilation to maintain PCO_2 at 50–55 mmHg during the each of the protocols. The ventilator setting in the interval period was the same as during the preparation period and replacement flow was set to 20 mL/h in the acid infusion and ELRAD protocol.

Sample collection and measurement

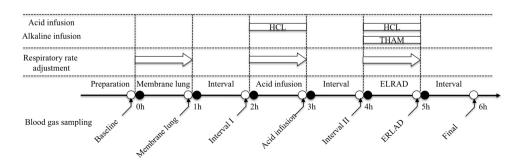
Blood was collected from the artery line at the end of each protocol and interval, and immediately measured using the blood gas analyzer (iSTAT[®], Abbott Point of Care Inc., Abbott Park, Illinois, USA). Blood cell counts (white, red blood cells, and platelet) and blood chemistry were determined using blood collected before the implementation of the membrane lung protocol and after the ELRAD protocol (Bio Majesty JCA-BM6050[®]; JEOL Ltd., Tokyo, Japan). Previously reported normal ranges for swine blood data were used as Ref. [26].

The amount of CO_2 eliminated by the membrane lung (VCO₂ML) was measured using a CO_2 analyzer (CGP-31[®]; TOA-DKK Co. Ltd., Tokyo, Japan) which was connected to the gas-out port of membrane lung. Vital signs (blood pressure, heart rate, and body temperature) and SpO_2 were continuously recorded in all experiments.

Tidal volume, ventilatory rate, minute ventilation (tidal volume × ventilatory rate), peak pressure and plateau pressure were recorded at the point of the blood gas analysis and the beginning and end of each protocol.

This study was approved by the Institutional Animal Care and Use Committee of Fujita Health University. All experiments were performed with strict adherence to the Guidelines for proper conduct of animal experiments proposed by Science Council of Japan.

Fig. 2 Timeline of the experiment





Statistical analysis

The primary outcome variables were VCO₂ML and minute ventilation to maintain PCO₂ at 50–55 mmHg. The secondary outcome variables were measurement parameters of the blood cell counts and blood chemistry. The variables were compared using a paired t test based on an initial baseline and the preceding baseline of each protocol, and Tukey's multiple comparisons test for mechanical ventilator variables and VCO₂ML. Any differences were considered to be statistically significant using a two-tailed value of P < 0.05. Data were presented as mean values with standard errors. Analyses were performed using R version 3.3.3 (R Foundation for Statistical Computing, Vienna, Austria, http://www.R-roject.org/) and PRISM version 7 (GraphPad Software, Inc., La Jolla, California, USA).

Results

All the experiments were successfully conducted as planned in the six healthy swine. The levels of PCO_2 were tightly maintained within a target range of 50–55 mmHg and did not significantly differ throughout the entire period of the experiment (P=0.22) (Table 1). There was no statistically significant difference in the levels of pH, HCO_3^- and the base excess between baseline, interval I and II (pH, P=0.44; HCO_3^- , P=0.31; base excess, P=0.30).

In the analysis of VCO₂ML which is a primary outcome variable, this parameter significantly increased by 1.6 times in the acid infusion protocol and ELRAD protocol compared to the membrane lung protocol (acid infusion, P < 0.0001;

ELRAD, P=0.0003) (Fig. 3). There was no statistically significant difference between the acid infusion protocol and the ELRAD protocol (P=0.55).

In the analysis of minute ventilation which is co-primary outcome variable, this parameter significantly decreased in the ELRAD protocol by 0.5 times compared to the baseline protocol (P < 0.001), and also significantly decreased compared to the membrane lung and acid infusion protocol (membrane lung, P = 0.0006; acid infusion, P = 0.0017) (Table 2).

In the secondary analysis of the study on the blood tests, there was a decrease in the sodium level for the blood gas analysis (Table 1), the white blood cells, and levels of total protein, albumin, ALT, and magnesium (Table 3). An increase in the AST levels was observed at the end of the experiment compared to the initial baseline protocol, while

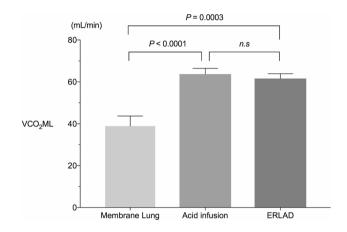


Fig. 3 Amount of CO₂ eliminated by membrane lung

Table 1 Changes in arterial blood gas and physiological data

Variables	Baseline	Membrane lung	Interval I	Acid infusion	Interval II	ELRAD	Final
MAP (mmHg)	100±4	98±6	98±4	94±7	98±6	89±6 [‡]	94±5
Heart rate (/min)	124 ± 10	$115 \pm 8*$	$114\pm7*$	119 ± 5	117 ± 5	$106 \pm 5^{\ddagger}$	110 ± 7
Oxygen saturation (%)	100 ± 0	100 ± 0	100 ± 0	99 ± 0	99 ± 1	99 ± 1	99 ± 1
Body temperature (°C)	38.0 ± 0.1	37.8 ± 0.1	$37.6 \pm 0.1*$	37.5 ± 0.2	$37.6 \pm 0.1*$	$37.7 \pm 0.1*$	$37.6 \pm 0.1*$
Blood gas analysis							
pН	7.43 ± 0.01	7.42 ± 0.01	7.42 ± 0.01	$7.36 \pm 0.02*^{\dagger}$	7.43 ± 0.01	7.42 ± 0.01	7.44 ± 0.01
PCO_2 (mmHg)	52.1 ± 0.5	52.8 ± 0.5	52.7 ± 0.7	53.2 ± 0.4	52 ± 0.7	52.2 ± 0.8	50.5 ± 1.4
HCO ₃ ⁻ (mmol/L)	34.8 ± 0.6	33.9 ± 0.4	34.1 ± 0.4	$30 \pm 1.1^{*\dagger}$	34.1 ± 0.5	34.2 ± 0.7	34.6 ± 1
Base excess	11 ± 1	10 ± 0	10 ± 1	$5 \pm 1^{*\dagger}$	10 ± 1	10 ± 1	11 ± 1
Hemoglobin (mg/dl)	8.4 ± 0.5	8.4 ± 0.3	8.6 ± 0.3	8.6 ± 0.2	7.7 ± 0.2	$7.1 \pm 0.2^{*\ddagger}$	7.5 ± 0.2
Na (mmol/L)	142 ± 1	143 ± 0	142 ± 0	$140 \pm 0^{*\dagger}$	142 ± 1	$139 \pm 0*^{\ddagger}$	$139 \pm 0^{*\ddagger}$
K (mmol/L)	4 ± 0.1	3.9 ± 0.1	4.2 ± 0.1	4.2 ± 0.1	4.3 ± 0.1	4.4 ± 0.2	4.2 ± 0.1
Cl (mmol/L)	98 ± 1	99 ± 1	99 ± 0	$101 \pm 1^{*\dagger}$	99 ± 1	101 ± 1	99 ± 0

Data are mean \pm standard deviation. P values were calculated with the use of the paired t test

MAP mean arterial pressure



^{*}P < 0.05 vs baseline, $^{\dagger}P < 0.05$ vs interval I, $^{\ddagger}P < 0.05$ vs interval II

Table 2 Changes in respiratory data

Variables	Baseline	Membrane lung	Acid infusion	ELRAD
Minute ventilation (L/min)	5.53 ± 0.33	3.98 ± 0.21*	4.10±0.28*	$2.87 \pm 0.21^{*\dagger\ddagger}$
Respiration rate (/min)	19 ± 1	$14 \pm 1*$	$15 \pm 1*$	$10 \pm 1^{*^{\dagger \ddagger}}$
Tidal volume (mL)	301 ± 5	302 ± 5	302 ± 5	302 ± 5
Peak pressure (cmH ₂ O)	17 ± 0	17 ± 0	17 ± 0	17 ± 0
Plateau pressure (cmH ₂ O)	16 ± 0	16 ± 0	16 ± 0	16 ± 0

Data are mean \pm standard deviation. P values were calculated with the use of the paired t test

Table 3 Changes in blood cell counts and chemistry data

Variables	Baseline	Final	P
Blood cell counts			
White blood cells ($\times 10^2/\mu L$)	212 ± 18	$160\pm10^*$	0.0045
Red blood cells ($\times 10^4/\mu L$)	558 ± 23	524 ± 15	0.18
Platelet ($\times 10^4/\mu L$)	22.4 ± 3.5	17.2 ± 4.0	0.15
Blood chemistry			
Total protein (g/dL)	4.8 ± 0.1	$4.3 \pm 0.1*$	0.00089
Albumin (g/dL)	2.8 ± 0.1	$2.6 \pm 0.1*$	0.0015
AST (U/L)	21 ± 2	$33 \pm 2*$	0.00011
ALT (U/L)	27 ± 2	$20\pm2*$	0.0036
LDH (U/L)	525 ± 38	459 ± 36	0.12
Creatinine (mg/dL)	0.7 ± 0.0	0.8 ± 0.0	0.47
Ureanitrogen (mg/dL)	4 ± 0	4 ± 1	0.33
Total bilirubin (mg/dL)	0.1 ± 0.0	0.1 ± 0.0	0.61
Mg (mg/dL)	1.6 ± 0.0	$1.5 \pm 0.0*$	0.025
Ca (mg/dL)	10.2 ± 0.3	10 ± 0.4	0.41

Reference interval; AST, 8-76 U/L; ALT, 18-54 U/L; LDH 217-1105 U/L.

Data are mean \pm standard error. P values were calculated with the use of paired t test

all these values were within the normal range for the experimental swine (Table 3).

Discussion

The ELRAD, which comprised an acid infusion system, a membrane lung, hemodiafiltration and an alkaline infusion, significantly increased CO_2 removal compared to the control condition of the membrane lung. The ELRAD significantly reduced the minute ventilation by half compared to the baseline protocol.

The investigation of efficient CO₂ elimination by regional acidification has been reported [19, 20]. A previous study on the addition of 0.5 mEq/L lactic acid upstream of the membrane lung was shown to remove 70% more CO₂ compared to the baseline condition without acid infusion [18]. In accord with this result, our ELRAD system using

hydrochloric acid as an acid solution could remove 60% more blood CO₂ content compared to the conventional method using a membrane lung.

In another previous study, regional blood acidification using lactic acid in an ECCO2R system increased VCO₂ML, but failed to reduce minute ventilation [27]. In accord with this result, the acid infusion protocol of our experiment was not able to reduce the minute ventilation. Investigators have speculated that the decreased pH [28, 29] or caloric intake effect of lactic acid which decreases glycolysis [30, 31], might contribute to the failure. Since the hydrochloric acid chosen in the current study has no effect on the caloric intake, the unchanged minute ventilation in the acid infusion protocol may be associated with a decreased pH. In the ELRAD protocol, we used trometamol to correct the acid state due to loss of CO2 buffer, other than the sodium bicarbonate which potentially generates CO₂ [32, 33]. Trometamol, which has low toxicity and short half-life (1.2 h), is used as an alkaline agent as a pure proton acceptor in metabolic acidosis according to the following formula; $(CH₂OH)₃C-NH₂+HA \leftrightarrow (CH₂OH)₃C-NH₃⁺+A⁻ (HA:$ acid) [34]. A pharmaceutical product of trometamol approved for intravenous administration was chosen in the study. In addition, it has been reported that trometamol might preserve myocardial contractility and hemodynamic stability in patients with acute respiratory distress syndrome. It may also attenuate ventilator-induced lung injury by decreasing intracellular CO₂ content that impairs the pH-dependent protecting system against cellular injury and plasma membrane injury [35, 36].

Recently, another ECCO2R system using a new acidification method called "respiratory electrodialysis" was reported [23, 24]. In respiratory electrodialysis, electrons are used for blood acidification instead of the addition of H⁺ ions. These electrons are generated by oxidation–reduction reactions with a 14 Fr double lumen catheter, three hemodialysis systems, and four blood pumps, and the system was shown to reduce the minute ventilation from 6.66 ± 1.2 to 3.36 ± 0.8 L per minute in experiments using swine of similar size. In the current study, ELRAD had a similar efficiency of CO_2 removal (minute ventilation reduced from 5.53 ± 0.33 to 2.87 ± 0.21 L per minute) compared to the



^{*}P<0.05 vs baseline, †P<0.05 vs membrane lung, †P<0.05 vs acid infusion

respiratory electrodialysis system. Since the ELRAD system is constructed by incorporating the membrane lung into the circuit of a conventional continuous hemodiafiltration, it is more simple and easy-to-setup. ECCO2R system connected with continuous renal replacement therapy console without regional acidification and alkaline infusion was also reported [37]. An existing lung and renal replacement system reduced tidal volume from 6 to 4 ml/kg at blood flow rate of 420 mL/min but increased PaCO₂ from 43 to 53 mmHg and decreased pH from 7.39 to 7.32. Compared to this existing lung and renal replacement system, our system had higher CO₂ removal efficiency and halved minute ventilation at lower blood flow rate (200 mL/min) within normal range of PaCO₂ and pH, which highlighted the clinical advantage of ELRAD.

The ELRAD system does not only play the role of respiratory assist, but also plays the role of renal assist, which may help to mitigate against several undesired outcomes that were highlighted in previous studies. First, respiratory electrodialysis and several ECCO2R studies using lactic acid have shown a significant increase of the creatinine level [20, 23], while the creatinine level remained within the normal range in the current ELRAD study. Second, acid infusion can possibly increase the levels of accumulated molecules. In a previous study on acid infusion using lactic acid, the blood level of lactate increased from 4.2 at the baseline time point to 15.1 mmol/L at the 15 min time point. However, in our study, there was no significant increase of the blood chlorine ion. Thus, regional acidification by hydrochloric acid with hemodiafiltration can maintain normal levels of blood chlorine ions.

In previous studies based on lactic acid infusion, there was no hemolysis observed when the pH of the blood reached 6.9–7.0 [18, 20]. In accord with these results, no signs of hemolysis were observed in the laboratory test of the blood cell counts and blood chemistry, in the present study. Since inhalation anesthetic had an effect on the $\rm CO_2$ exchange at the swine lung, we chose intravenous anesthetic for this study [38]. This resulted in the requirement of a large amount of fluid due to the vasodilation effect of anesthetic. A positive fluid balance may contribute to a slight decrease in the levels of hemoglobin, total protein, and albumin.

The present experimental study has several limitations. First, the ELRAD system requires a high administration rate of the acid solution. In addition, the safety use of acid infusion to human blood is not established. However, in a previous study using up to 1 mol/L of hydrochloric acid for the treatment of metabolic alkalosis, no hemolysis was observed [25, 39–41]. We decided to use 0.5 mol/L hydrochloric acid as a safe concentration and an administration rate of 480 ml/h, in reference to another blood acidification study which reported 5 mEq/min infusion of 0.5 mol/L lactic acid to 500 mL/min blood flow and obtained more than

130 mmHg CO₂. A safety mechanism which checks the pH upstream to the reinfusion will be considered for clinical application. Second, we did not evaluate the oxygenation of the ELRAD system, while the oxygen saturation was kept in the range of 99-100% during all experiments. The oxygenation ability of the membrane lung we used at a blood flow rate of 200 mL/min could only maintain 15 mL/min oxygen [42], which is far less than the 3.5 mL/kg/min oxygen consumption of humans [43]. The ELRAD system is inadequate for oxygenation, therefore, we did not evaluate the oxygenation capability. Finally, we fixed the dialysate flow rate of 1000 mL/h and filtration flow rate of 500 mL/h in all protocol to evaluate whether hydrochloric acid infusion would alter serum levels of chlorine ion or not. We maintained the fluid balance by adjusting replacement flow rate from 500 to 20 mL/h in the acid infusion protocol, while we did not add further adjustment of the hemodiafiltration settings in ELRAD protocol in which the fluid balance increased. This positive fluid balance may contribute to temporarily decreased hemoglobin level in the ELRAD protocol. In further study, the fluid balance should be controlled by adjustment of dialysate flow.

Conclusions

We developed an efficient CO₂ removal system, ELRAD using acid and alkaline infusion, with a membrane lung incorporated into a CHDF console at low blood flow. This novel system removed 1.6 times the volume of CO₂ compared to a conventional method and reduced minute ventilation to about a half compared to the control model while maintaining the acid–base equilibrium within normal range. Further studies are needed prior to the clinical application of this easy setup system comprising of materials that are typically found in a clinical setting.

Author contributions NT and TN contributed to the study's conceptualization and design, the acquisition of data, analysis, and interpretation of data, statistical analysis, and drafting and critical revision of the manuscript for intellectual content. TS, YK, and KM contributed to the acquisition of data, interpretation of data, and critical revision of the manuscript for intellectual content. ON and SO contributed to the study's conceptualization and design and critical revision of the manuscript for intellectual content. All authors read and approved the manuscript.

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Compliance with ethical standards

Conflict of interest The authors have no conflicts of interest to declare. This work was supported by JSPS KAKENHI Grant Number 17K17042 and Yoshimi Memorial TMP Grant from the Japanese So-



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