



# Enzymatic reaction modulated DNA assembly on graphitic carbon nitride nanosheets for sensitive fluorescence detection of acetylcholinesterase activity and inhibition

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## Abstract

A novel fluorescent strategy has been developed by using an enzymatic reaction modulated DNA assembly on graphitic carbon nitride nanosheets (CNNS) for the detection of acetylcholinesterase (AChE) activity and its inhibitors. The two-dimensional and ultrathin-layer CNNS-material was successfully synthesized through a chemical oxidation and ultrasound exfoliation method. Because of its excellent adsorption selectivity to ssDNA over dsDNA and superior quenching ability toward the fluorophore labels, CNNS were employed to construct a sensitive fluorescence sensing platform for the detection of AChE activity and inhibition. The detection was based on enzymatic reaction modulated DNA assembly on CNNS, which involved the specific AChE-catalyzed reaction-mediated DNA/Hg<sup>2+</sup> conformational change and subsequent signal transduction and amplification via hybridization chain reaction (HCR). Under the excitation at 485 nm, the fluorescence signal from 500 to 650 nm ( $\lambda_{\text{max}} = 518 \text{ nm}$ ) of the developed sensing system was gradually increased with increasing concentration of AChE. The quantitative determination range of AChE is from 0.02 to 1 mU/mL and the detection limit was 0.006 mU/mL. The developed strategy was successfully applied to the assay of AChE in human serum samples, and can also be used to effectively screen AChE inhibitors, showing great promise providing a robust and effective platform for AChE-related diagnosis, drug screening, and therapy.

**Keywords** Enzymatic reaction · DNA assembly · Graphitic carbon nitride nanosheets (CNNS) · Acetylcholinesterase · Inhibitor screening

## Introduction

Acetylcholinesterase (AChE) plays a pivotal role in maintaining the normal function of the cholinergic nerves in the central and peripheral nervous system [1–3]. Numerous

research have provided evidence that the abnormal content of acetylcholine caused by AChE is closely associated with the occurrence and development of neurodegenerative diseases such as Alzheimer's disease (AD), myasthenia gravis, depression, and Parkinson's disease [4, 5].

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Recently, AChE has been considered as an early biomarker and significant therapeutic target for the development of new drugs for the treatment of dementia [6]. For example, some AChE inhibitors that can affect AChE activity and enhance cholinergic neurotransmission were widely used in the AD therapies [7, 8]. Therefore, the development of efficient methods for specific detection of AChE activity and screening its potential inhibitors were not only very crucial for elucidating the function of AChE in complicated living systems but also for providing useful tools to AChE-related therapy and biomedical research.

Until now, considerable efforts have been made to develop efficient strategies to monitor the enzymatic activity of AChE and screen its potential inhibitors. The most widely used method for AChE activity is the colorimetric detection by using Ellman's reagent [9]. However, such methods may display some shortcomings such as low sensitivity, false-positive effects [10]. In recent years, various kinds of analytical techniques, including colorimetric methods [11–13], chemiluminescence [14], surface-enhanced Raman scattering (SERS) [15], fluorescence detection [16–19], and electrochemical analysis [20], have been developed for the sensing of AChE. In addition, advanced materials such as gold nanoparticles [21], quantum dots [22], single-walled carbon nanotubes (SWCNTs) [23], macromolecule polymers [24], and metal-organic frameworks (MOFs) [25] have also been utilized to construct novel strategies for AChE activity measurement. These approaches, however, still suffered from certain drawbacks, such as lack of sufficient sensitivity and specificity, the assistance of other enzymes for signal amplification and readout, and the requirement of expensive materials or instruments. Hence, the development of a new, sensitive, selective, and cost-effective method for the detection of AChE and its inhibitors is highly desirable.

Graphitic carbon nitride nanosheets (CNNS), a metal-free two-dimensional (2D) layered framework, belong to a type of rising star in the carbon-based nanomaterials family [26, 27]. The structure of CNNS is composed of *s*-triazine or tri-*s*-triazine formed by alternating C–N atoms instead of C–C atoms through  $sp^2$  hybridization, in which weak van der Waals' forces exists and the layer distance is about 3.3 nm [28]. In general, the CNNS can be easily prepared through the pyrolysis of low cost nitrogen-rich precursors, including melamine, cyanamide, dicyandiamide, urea, and thiourea, and then exfoliated into ultrathin nanosheets with various sizes. Excitingly, the CNNS were found to possess unique physicochemical properties, such as excellent stability and preferable biocompatibility, high surface-to-volume ratio, facily accessible functional sites on the basal planes, and inertness to environmental influences, which enable them suitable for biosensor, optoelectronic, and catalytic applications [29–33]. Moreover,

like other carbon-based nanomaterials, CNNS have been shown to selectively adsorb single-stranded DNA (ssDNA) but not double-stranded DNA (dsDNA), which can be used to design fluorescence sensors for nucleic acids by combining their ability to quench fluorophores [34, 35].

Herein, we report a novel fluorescent strategy for sensitive detection of AChE activity and for screening of its potential inhibitors. To the best of our knowledge, it is the first time that a highly effective enzymatic reaction modulated DNA assembly on CNNS has been developed for the assay of AChE activity and inhibition. Because of the ease of operation, satisfying sensitivity and specificity, this developed fluorescence sensing system will afford a useful platform for the detection of AChE activity and screening of its inhibitors.

## Experimental section

### Chemicals and materials

HPLC-purified oligonucleotides (Table S1) were synthesized by Shanghai Sangon Biotech Co., Ltd. (Shanghai, China). Acetylcholinesterase (AChE), acetylthiocholine chloride (ATCh), bovine albumin (BSA), glucose oxidase (GOX), lysozyme (Lys) ribonuclease (RNase), and horseradish peroxidase (HRP) were purchased from Sigma-Aldrich. 5,5'-dithiobis (2-nitro-benzoic acid) (DTNB), tacrine, dicyanamide, tris (hydroxymethyl) aminomethane (Tris), and magnesium sulfate ( $MgSO_4$ ) were gained from Aladdin Chemistry Co., Ltd. (Shanghai, China). All other reagents were of analytical grade. The human serum samples were obtained from the First Affiliated Hospital of Guangxi Medical University (Nanning, China). The double-distilled water, which was purified by a Milli-Q system (Millipore, Bedford, MA) with an electric resistance  $>18.25\text{ M}\Omega\text{-cm}$ , was used for preparing needed solutions.

### Apparatus and characterization

The fluorescence measurements were carried out on an FL-8500 fluorescence spectrometer (Perkin Elmer, USA). The transmission electron microscope (TEM) images were measured using a field-emission high-resolution 2100F TEM (JEOL, Japan). The morphology of the nanosheets was examined by field-emission scanning electron microscopy (SEM, S-4800, Hitachi, Japan). The atomic force microscopy (AFM) image was taken on means of Bruker Bioscope system (Bruker, USA). Zeta potential measurement was conducted using a Malvern Zetasizer 90 particle size and zeta potential analyzer (Malvern, UK). X-ray diffraction (XRD) patterns were recorded with a MiniFlex 600 X-ray diffractometer (Rigaku, Japan). The X-ray photoelectron spectroscopy (XPS) analysis was detected using an X-ray photoelectron spectroscope (Thermo Scientific, USA). Fourier-transform

infrared (FT-IR) experiments were performed on a Spectrum Two FT-IR Spectrometer (Perkin Elmer, USA).

## Preparation of two-dimensional (2D) CNNS

The CNNS were prepared according to our previously methods with some modification [34, 36]. Specific preparation procedure was described in the Electronic Supporting Material.

## Determination of AChE activity and inhibitor

For AChE activity detection, I-DNA and  $\text{Hg}^{2+}$  ions were first mixed with a molar ratio of 1:4 to obtain I-DNA/ $\text{Hg}^{2+}$  hairpin probe owing to the formation of T- $\text{Hg}^{2+}$ -T base pair in the stem region. Then, 2  $\mu\text{L}$  of 5  $\mu\text{M}$  ATCh, 2  $\mu\text{L}$  of different concentrations of AChE, and 26  $\mu\text{L}$  reaction buffer (5 mM Tris-HCl, 5 mM  $\text{MgSO}_4$ , pH 8.0) were incubated at 37 °C for 30 min. After that, 2  $\mu\text{L}$  of 1  $\mu\text{M}$  I-DNA/ $\text{Hg}^{2+}$  hairpin probe, 2  $\mu\text{L}$  of 5  $\mu\text{M}$  H1, and 2  $\mu\text{L}$  of 5  $\mu\text{M}$  H2 were added into the reaction system and incubated for 60 min at 37 °C. Thereafter, 6  $\mu\text{L}$  of 2 mg/mL CNNS solution was added into the above mixtures for 10 min at room temperature with a total volume of 200  $\mu\text{L}$ . Finally, the fluorescence analysis of the samples was carried out. The fluorescence emission spectra of samples were collected from 500 to 650 nm ( $\lambda_{\text{max}} = 518 \text{ nm}$ ) with a 485-nm excitation wavelength.

To study the inhibition of tacrine on AChE activity, 2  $\mu\text{L}$  of different concentrations of tacrine and 2  $\mu\text{L}$  of 0.1 U/mL AChE were mixed in reaction buffer at 37 °C for 30 min. Then, the following experimental procedures were the same as those used for the AChE activity assay.

## Detection of AChE activity in real samples

Human serum samples were chosen as actual samples to evaluate the practicability of the sensing strategy. First, the serum samples were obtained by centrifuging the whole blood samples at 3500 rpm for 5 min. Then, 20  $\mu\text{L}$  of the human serum samples was mixed with 20  $\mu\text{L}$  different concentrations of AChE and was diluted to 20 mL with 20 mM Tris-HCl buffer (pH 7.4). The final concentrations of added AChE were 0, 0.1, 0.2, 0.4, 0.8, and 1.0 mU/mL in the fluorescence analysis samples, respectively. Subsequently, the determination of AChE in the human serum samples was carried out using the procedure as described in the above.

## Results and discussion

### Characterization of two-dimensional (2D) CNNS

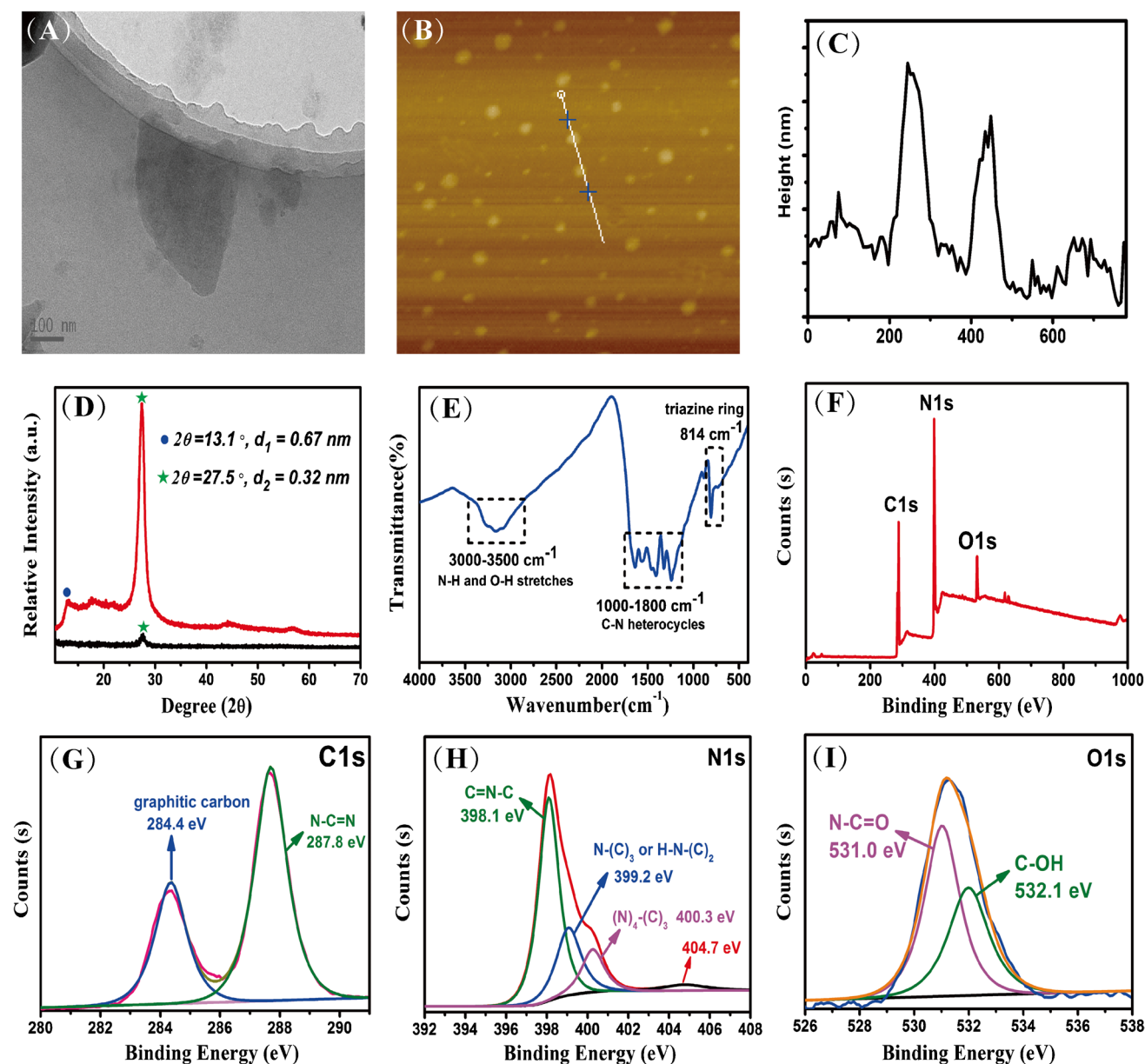
The main synthetic process of CNNS has already been described in our previous research works [34, 36]. Results

from TEM (Fig. 1A) and SEM (Fig. S1) revealed that the as-obtained CNNS showed a 2D planar sheet structure with a mean length of about 110 nm and width of 95 nm. Moreover, the as-prepared CNNS are positively charged, with a zeta potential up to +29.2 mV (Fig. S2). The high surface charge endows the CNNS with excellent stability and can stand still for several weeks without any aggregation, which is favorable for further biomedical and biosensing applications. The AFM image and section analysis for CNNS (Figs. 1B and 1C) disclosed that the thickness of these nanosheets is  $\sim 1.5$  nm, suggesting they mainly comprised of a single layer. The XRD pattern presented a strong diffraction peak located at 27.5° ( $d = 0.32 \text{ nm}$ ), corresponding to the typical graphitic interlayer stacking (002) peak of CNNS. The other weak peak is (100) phase at 13.1° ( $d = 0.67 \text{ nm}$ ), which can be ascribed to the periodic in-planar structure of the tri-s-triazine ring. Compared with bulk  $\text{g-C}_3\text{N}_4$ , the peak of CNNS located at 27.5° sharply decreased, and the peak located at 13.1° almost disappeared, implying that few-layered structure of CNNS after exfoliation (Fig. 1D) [37].

The surface structure and composition of the as-prepared CNNS were then investigated. The FT-IR spectrum (Fig. 1E) of the CNNS exhibits a distinct absorption peak at 814  $\text{cm}^{-1}$ , which was due to the vibration of the triazine ring. Furthermore, the absorption peaks around 1000 and 1800  $\text{cm}^{-1}$  are assigned to the characteristic stretching band of C-N heterocycles (C-N(-C)-C and C-NH-C) [38]. For a better insight, XPS measurement was performed. As shown in Fig. 1F, the CNNS contain C, N, O three elements, and that the atomic ratio of N/C was calculated to be 1.35, closing to the stoichiometric value of 1.33. The relatively high oxygen content within CNNS may be caused by chemical oxidation and ultrasonic exfoliation. XPS analysis of the C 1s spectrum reveals two peaks at 284.4 and 287.8 eV, which are identified as the  $\text{sp}^3$ -bonded carbon with oxygen (C-OH) and  $\text{sp}^2$ -bonded carbon (N-C=N), respectively (Fig. 1G). The high-resolution N 1s spectrum is shown in Fig. 1H. It can be deconvoluted into four peaks, mainly located at 398.1, 399.2, 400.3, and 404.7 eV, demonstrating the presence of  $\text{sp}^2$ -hybridized nitrogen (C=N-C), C-NH bond and  $\text{sp}^3$ -hybridized nitrogen (N-[C]<sub>3</sub>), quaternary N bonded to three C in the aromatic cycles and terminal nitrate groups in heterocycles. What's more, the peaks at around 531.0 and 532.1 eV in the XPS spectrum of O 1s belong to N-C=O and C-OH groups of CNNS, respectively (Fig. 1I) [39]. It can be seen that the surface components of the CNNS determined by the XPS were in good agreement with FT-IR results. Taken together, these results demonstrated that the CNNS has been successfully prepared.

### Design principle

As illustrated in Scheme 1A, CNNS were firstly obtained by directly using chemical oxidation and ultrasound method to handle the bulk graphitic carbon nitride ( $\text{g-C}_3\text{N}_4$ ) with



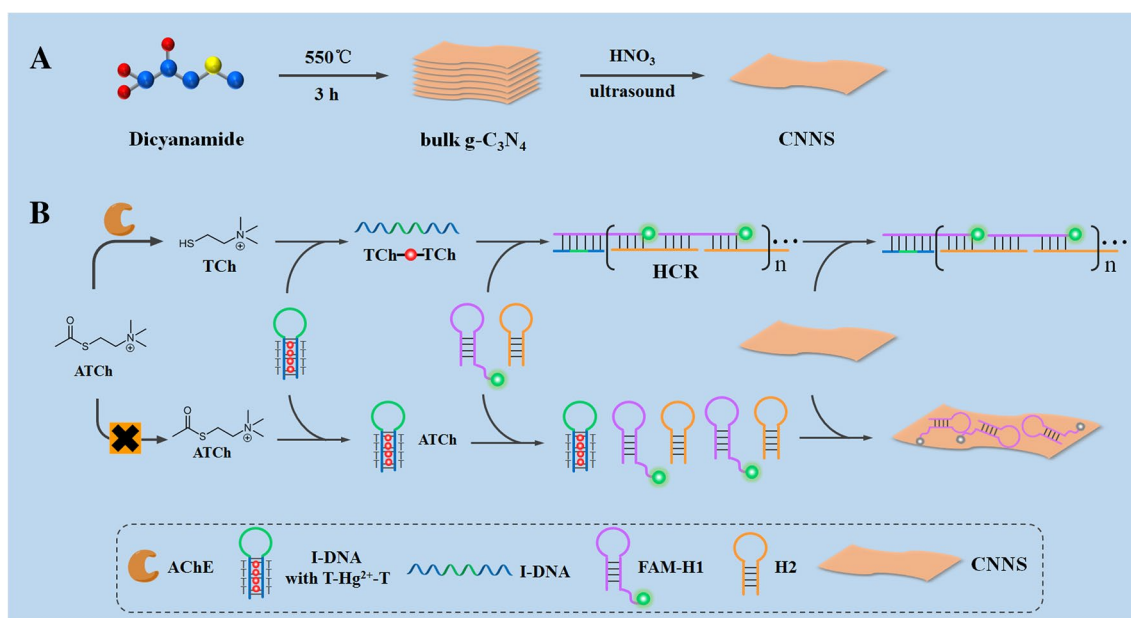
**Fig. 1** **A** TEM image of the CNNS. **B** AFM image of the CNNS. **C** The height profile of corresponding section of **B**. **D** XRD of bulk  $g\text{-C}_3\text{N}_4$  (red) and CNNS (black). **E** FT-IR of the CNNS. **F** Survey

XPS spectrum of the CNNS. **G** C 1s spectrum of the CNNS. **H** N 1s spectrum of the CNNS. **I** O 1s spectrum of the CNNS

pyrolysis of dicyanamide under high temperature. Then, the assay of AChE activity and its inhibitors were performed through enzymatic reaction modulated DNA assembly on CNNS (Scheme 1B).

In this rationally designed sensing system for AChE, three DNA probes (I-DNA, FAM-H1, and H2, Table S1),  $\text{Hg}^{2+}$ , acetylthiocholine (ATCh), and CNNS were mainly involved. The I-DNA probe that containing eight thymine (T) bases can hybridize with 4 equiv of  $\text{Hg}^{2+}$  to form a stem-loop hairpin structure (I-DNA with T- $\text{Hg}^{2+}$ -T) through  $\text{Hg}^{2+}$ -mediated T-T base pairing. When the analytical target AChE was

introduced, the analogue of acetylcholine—ATCh can be catalyzed and decomposed to thiocholine (TCh) that containing the chemically reactive group (-SH). The resulting thiol products can bind to with  $\text{Hg}^{2+}$  and effectively captures  $\text{Hg}^{2+}$  from the hairpin-shaped I-DNA, owing to the higher affinity interaction between TCh and  $\text{Hg}^{2+}$ . Accompanied by the release of  $\text{Hg}^{2+}$  triggered by AChE hydrolysis products, the hairpin I-DNA will be liberated into a single-stranded conformation, revealing its 3'-terminal, and thus generate a long dsDNA products via hybridization chain reaction (HCR) [40, 41], which was triggered by I-DNA



**Scheme 1** **A** Diagram of the synthesis of CNNS. **B** Schematic illustration of the fluorescence assay for AChE and its inhibitor based on the modulation of DNA assembly on CNNS

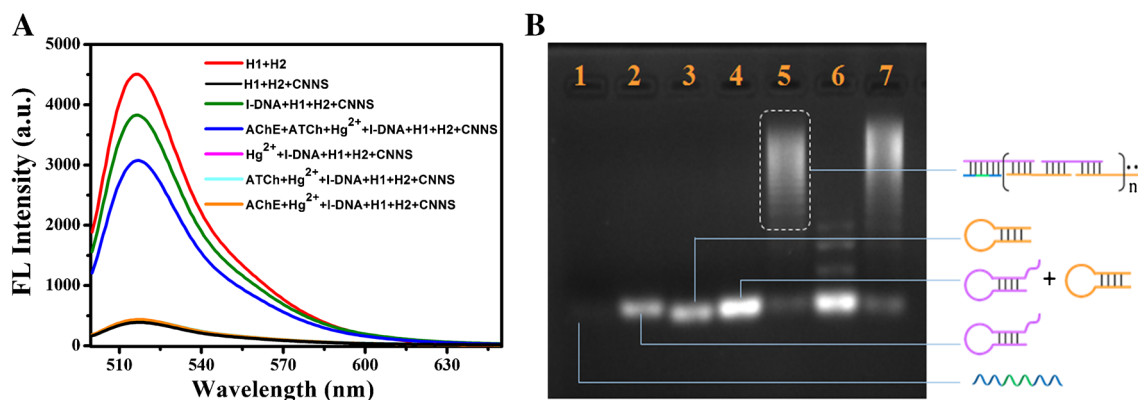
for alternating hybridization between FAM-H1 and H2. Notably, the FAM-labeled HCR product has a relative rigid conformation, which remains highly fluorescent upon addition of CNNS because of the weak assembly of dsDNA on CNNS. On the contrary, the catalytic hydrolysis of AChE is blocked in the presence of AChE inhibitor, and thus less TCh is generated, resulting in I-DNA with T-Hg<sup>2+</sup>-T maintained their initial hairpin configurations in the detection system. In this case, the hairpin structured I-DNA disables the assembly of the HCR product. As a result, the unreacted hairpin DNA probes, FAM-H1 and H2, can be adsorbed and assembled on the CNNS surface through their sticky ends and loops, delivering a very weak fluorescence signal due to the super quenching ability of CNNS toward the fluorescence of FAM labels. Therefore, the concentrations of AChE can be detected by the change of fluorescence signal.

### Feasibility study of AChE detection

With the as-prepared CNNS, we then test their feasibility as a fluorescent sensing platform for AChE detection. As illustrated in Fig. 2A, the mixture sample of H1 and H2 was found to exhibit a high fluorescence signal. After 60 µg/mL CNNS was introduced into the sample, a remarkable fluorescence decrease (> 92%) was obtained. This was ascribed to the fact that the strong adsorption of the hairpin DNA on the CNNS surfaces, which resulted in the proximity of fluorescein to CNNS and effective quenching of the fluorescence of the dye through photoexcited electrons transfer from the fluorophore to CNNS [34, 35]. In contrast, in the presence of 10 nM I-DNA, the response

signal recovered even after CNNS were added into the solution, testifying that I-DNA was able to initiate the hybridization chain amplification with H1 and H2. In addition, if Hg<sup>2+</sup> was further added, which could bind with I-DNA to form a hairpin structure, preventing the trigger of HCR, and thus the response signal remained almost unchanged. However, when reaction solution of AChE with its substrate ATCh was added to the mixture of Hg<sup>2+</sup>/I-DNA/H1/H2@CNNS, a significant fluorescence enhancement up to ~8-fold was obtained. Moreover, in the comparative experiment, after only incubation of AChE or ATCh with the mixture, no obvious fluorescence response can still be observed. These data indicated that the hydrolysis product of ATCh by AChE inhibited the binding of Hg<sup>2+</sup> with I-DNA, resulting in the trigger of HCR and providing a sensitive detection of AChE.

Further gel electrophoresis analysis was performed to investigate the AChE mediated hybridization chain assembly (Fig. 2B). Three clear bands were observed for I-DNA, H1, and H2, respectively (lanes 1, 2, and 3). The mixture of two metastable H1 and H2 hairpin probes did not show any new band (lane 4), verifying a low back-ground of the HCR amplification. When incubating H1 and H2 with I-DNA, a new ladder-like band with higher molecular weights appeared, implying the initiation of the hybridization chain assembly by I-DNA (lane 5). Furthermore, we found that only a negligible ladder-like band was obtained when the same system was further treated by Hg<sup>2+</sup> (lane 6), which indicated that Hg<sup>2+</sup> can efficiently inhibit the occurrence of HCR. However, upon addition of the reaction solution of AChE with its substrate ATCh to the mixture of Hg<sup>2+</sup>/I-DNA/H1/H2, an obvious ladder-like HCR band was



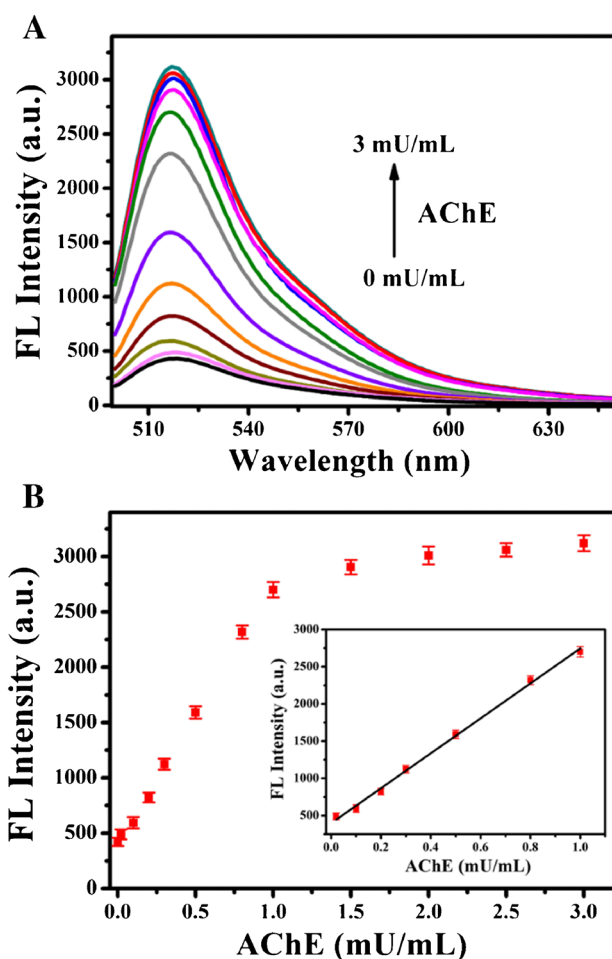
**Fig. 2** **A** The fluorescence spectral response obtained by incubating different probes. The concentrations of H1 and H2 were 50 nM, I-DNA was 10 nM, Hg<sup>2+</sup> was 40 nM, CNNS was 60 µg/mL, ATCh was 50 nM, and AChE was 3 mU/mL. **B** Agarose gel electrophoresis images. Lane 1, 0.2 µM I-DNA; lane 2, 1 µM H1; lane 3, 1 µM H2;

lane 4, 1 µM H1 + 1 µM H2; lane 5, 0.2 µM I-DNA + 1 µM H1 + 1 µM H2; lane 6, 0.2 µM I-DNA + 0.8 µM Hg<sup>2+</sup> + 1 µM H1 + 1 µM H2; lane 7, 0.5 µM ATCh + 30 mU/mL AChE + 0.2 µM I-DNA + 0.8 µM Hg<sup>2+</sup> + 1 µM H1 + 1 µM H2

observed (lane 7), which is similar with the direct incubation of I-DNA with H1 and H2 (lane 5). Collectively, these results demonstrated the great potential of the proposed biosensing strategy for AChE detection.

### Analytical performance of the fluorescence AChE assay

After verifying the feasibility, the analytical performance of developed fluorescence sensing system response to AChE was then evaluated. To achieve best performance for AChE, we first optimized several important parameters, including the concentration of CNNS, Hg<sup>2+</sup>, ATCh, and incubation time (Figs. S3 to S6). Accordingly, 60 µg/mL CNNS, 40 nM Hg<sup>2+</sup>, 0.05 µM ATCh, and 60 min reaction time were chosen as the optimal experimental conditions. Under the optimized experimental conditions, the fluorescence emission spectra of the sensing system in the presence of AChE at varying concentrations were measured. For the fluorescence measurement of AChE, after incubating different concentrations of AChE with its substrate ATCh, the resulting solution was then added to the mixture of Hg<sup>2+</sup>/I-DNA/H1/H2@CNNS and incubated at 37 °C for another 60 min. We found that the fluorescence signal was gradually increased with the increasing concentration of AChE (Fig. 3A). As can be seen in Fig 3B, there exhibited an excellent linear relationship between the fluorescence peak values at 518 nm and concentration of AChE ranging from 0.02 to 1.0 mU/mL ( $R^2 = 0.996$ , inset in Fig. 3B). The detection limit ( $3\sigma/\text{slope}$ ) was calculated to be as low as 0.006 mU/mL, which was comparable or better than most of existing assay methods especially those fluorescence assays for AChE detection (Table S2). Though the sensitivity is inferior to some methods, the CNNS adopted in this strategy has several advantages including cost-efficient, excellent stability, low biotoxicity, and outstanding



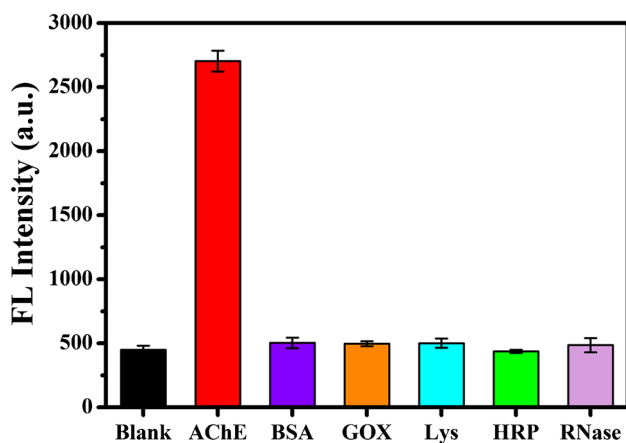
**Fig. 3** **A** Fluorescence spectral responses of CNNS-based sensing system to AChE with different concentrations. **B** Fluorescence peak intensity at 518 nm versus the concentration of AChE ( $E_x = 485$  nm). Inset: linear plot of the fluorescence peak intensity at 518 nm against the concentration of AChE in the range from 0.02 to 1.0 mU/mL. The error bars represent the standard deviation of three measurements

quenching capacity. Moreover, the construction of this sensing system is easy-to-operate.

In addition, to evaluate the selectivity of the developed sensing strategy, various potential interfering substances including glucose oxidase (GOX), lysozyme (Lys), bovine serum albumin (BSA), ribonuclease (RNase), and horseradish peroxidase (HRP) were tested under the same conditions. As shown in Fig. 4, compared with the target AChE, none of these proteins gave any noticeable fluorescence response, which clearly suggests that these proteins did not interfere with the assay, and developed sensing strategy has excellent selectivity for AChE detection. This excellent selectivity of our method can be attributed to the enzymatic reaction specificity of AChE and high affinity between the hydrolysis product of AChE and  $Hg^{2+}$ . More importantly, the high specificity of this sensing method also provided the potential for the detection of AChE activity in complex real samples.

### Detection of AChE in real samples

Next, we further explored the practical applicability of the developed fluorescence sensing system. The AChE in human serum samples were measured using proposed strategy



**Fig. 4** Selectivity of the strategy for AChE sensing. AChE is at a concentration of 1.0 mU/mL. The concentration of GOX, Lys, HRP, and RNase is 10 U/mL, respectively. The concentration of BSA is 20 mg/mL. Error bars are standard deviations of three repetitive experiments

through the standard addition method. Different concentrations of AChE were added in human serum sample to prepare the spiked samples. As shown in Table 1, the recoveries were in the range from 98.2 to 104.8% with an RSD of less than 4.0%. Besides, it is also clearly found that the detection results of AChE in human serum samples obtained by our sensing system were in accord with those data tested by standard Ellman's method. These observations disclosed that the established method is applicable for AChE detection in complex real samples with satisfactory reliability.

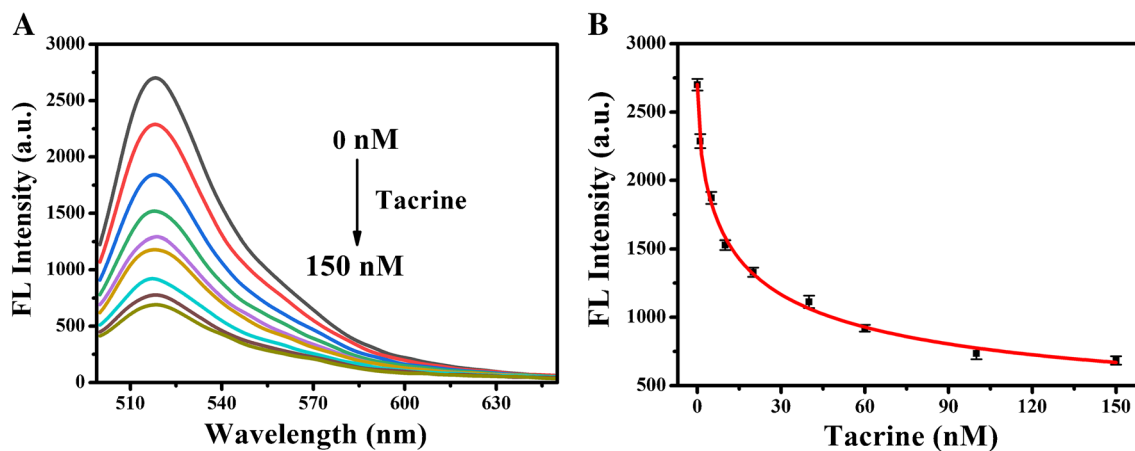
### AChE inhibitor assay

To demonstrate whether the developed sensing strategy could be also used for the screening of AChE inhibitors, a well-known AChE inhibitor tacrine that used for treatment of Alzheimer's disease [42] was chosen as the case of study. In this case, 2  $\mu$ L of tacrine at different concentrations was first mixed with 0.1 U/mL AChE for 30 min, and then incubated with the reaction solution of the sensing system. It was found that the fluorescence intensities decreased with the addition of increasing concentrations of the tacrine, clearly indicating the inhibitory capacity for AChE activity (Fig. 5). The corresponding  $IC_{50}$  value (the inhibitor concentration required for 50% inhibition of the enzyme activity) of tacrine was estimated to be 7.2 nM, which was comparable with those obtained by other AChE assays [43]. The above-mentioned results confirmed that our proposed sensing method possess great potential to screen AChE inhibitors and provides a broad prospect for AChE-based drug discovery.

Although this established method for sensing AChE activity and screening its inhibitors displays many remarkable features, it still had some limitations. One major disadvantage of the method was that strong oxidizing reagents were adopted for the synthesis of CNNS and the preparation procedure is time-consuming, which usually required chemical oxidation and ultrasound exfoliation for more than 10 h. Additionally, hybridization chain reaction (HCR) usually need a relatively long reaction time to generate a significantly amplified readout signal, which can be ascribed to its slow reaction kinetics [44].

**Table 1** Results of AChE activity assay in human serum samples

| Sample | Added (mU/mL) | Detected $\pm$ SD (mU/mL) | RSD (% , n=3) | Recovery (%) | Ellman's method $\pm$ SD (mU/mL) | RSD (% , n=3) |
|--------|---------------|---------------------------|---------------|--------------|----------------------------------|---------------|
| 1      | 0.100         | 0.097 $\pm$ 0.003         | 3.2           | 97.0         | ND                               | -             |
| 2      | 0.200         | 0.210 $\pm$ 0.004         | 2.1           | 104.8        | ND                               | -             |
| 3      | 0.400         | 0.407 $\pm$ 0.007         | 1.8           | 101.7        | ND                               | -             |
| 4      | 0.800         | 0.784 $\pm$ 0.031         | 3.9           | 98.2         | 0.792 $\pm$ 0.026                | 3.3           |
| 5      | 1.000         | 1.008 $\pm$ 0.027         | 2.7           | 100.6        | 0.995 $\pm$ 0.024                | 2.4           |



**Fig. 5** The inhibition analysis of tacrine on AChE activity. **A** Fluorescence spectra of the biosensing platform at various concentrations of tacrine. **B** Calibration curve corresponding to the fluorescence inten-

sity as a function of tacrine concentration. The error bars represent the standard deviation of three measurements

Therefore, our future research work will focus on the development of green and rapid methods for the preparation of CNNS. Moreover, the optimal sequences of DNA probes and the experimental conditions (such as reaction temperature, reaction buffer, and the concentration of metal ions) will further be investigated to circumvent the limitation.

## Conclusion

In this work, the ultrathin CNNS was successfully synthesized to demonstrate excellent selective recognition toward dsDNA over ssDNA and further utilized to establish a fluorescence sensing platform for the assay of AChE activity and inhibition. Combining the specific AChE-catalyzed reaction-mediated DNA/Hg<sup>2+</sup> conformational change and well-defined signal transduction and amplification via HCR, the constructed sensing platform enables sensitive and selective detection of AChE. Moreover, the developed strategy was successfully applied to the assay of AChE in real complex samples and could efficiently perform the screening of the AChE inhibitor. Given the method's merits including ease of operation, satisfying sensitivity and specificity, our proposed assay system will hold certain practicability and application potential in the clinical diagnosis of AChE-related disease and drug screening.

**Supplementary Information** The online version contains supplementary material available at <https://doi.org/10.1007/s00604-023-05850-8>.

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## Declarations

**Conflict of interest** The authors declare no competing interests.

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