



# Electrochemical synthesis of multilayered PEDOT/PEDOT-SH/Au nanocomposites for electrochemical sensing of nitrite

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## Abstract

A multilayered film of poly(3,4-ethylenedioxythiophene)/poly(thiomethyl 3,4- ethylenedioxythiophene)/gold nanoparticle (PEDOT/PEDOT-SH/Au) nanocomposites was successfully synthesized on indium tin oxide (ITO) and glassy carbon electrode (GCE) via an electrochemical technique. The structure and morphology of the composite was characterized by FT-IR, UV-vis, EDS, XPS, and SEM analyses. The prepared multilayered PEDOT/PEDOT-SH/Au nanocomposite was used for the electrochemical catalytic oxidation of nitrite by amperometry. The results showed that the microstructures of PEDOT/PEDOT-SH/Au nanocomposites are not strongly dependent on the substrate. Fibrous PEDOT as hard template absorbed EDOT-SH on it to form porous PEDOT/PEDOT-SH. Porous structure had the advantages of large specific surface area and high porosity for nitrite ion adsorption. The thiol group in PEDOT/PEDOT-SH stabilized Au nanoparticles (NPs) effectively through Au-S bond and allowed Au NPs to have high dispersion and excellent electrocatalytic activity. The PEDOT/PEDOT-SH/Au composite prepared on GCE had a good performance in its electrochemical response to nitrite ions. PEDOT/PEDOT-SH/Au/GCE displayed a low oxidation potential (0.74 V), a fast response time (< 3 s), a low detection limit (0.051  $\mu\text{M}$ ), two linear ranges (0.15–1 mM and 1–16 mM), good sensitivity (0.301  $\mu\text{A } \mu\text{M}^{-1} \text{ cm}^{-2}$  and 0.133  $\mu\text{A } \mu\text{M}^{-1} \text{ cm}^{-2}$ ) with good reproducibility, stability, and selectivity.

**Keywords** Layer-by-layer film · Thiol group functionalized PEDOT · Porous nanofiber · Gold nanoparticles · Electrochemical nitrite sensor

## Introduction

Nitrite is widely used in food additives and fertilizer industries. Large amounts of nitrite in the human body can cause serious harm to human health and may lead to cancer [1–3]. The World Health Organization has fixed the maximum limit at 3 mg/L for nitrite in drinking water [4]. Therefore, it is important to establish an accurate, rapid, simple, sensitive,

and selective method for the determination of nitrite in both physiological system and environmental.

Several common methods for the determination of nitrite include chemiluminescence [5], capillary electrophoresis [6], chromatography [7], fluorescence [8], and titration [9]. However, the high cost of equipment and the tedious and time-consuming testing procedures of these analytical methods hinder their wider application in practical. Electrochemical technology has the advantages of quick response, low cost, good real-time performance, low limit of detection (LOD), and excellent sensitivity and selectivity, so it is a promising method for nitrite determination [10–12]. However, the electrooxidation of nitrite on conventional electrode usually occurs at large overpotential, which would decrease the electrode accuracy and sensitivity. To overcome this problem, different kinds of chemically modified electrode were established with high sensitivity and selectivity [13–17]. Gold nanoparticles (Au NPs) are widely used as electrode modification materials due to their excellent catalytic performance [18]. However, their stability, reproducibility,

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and ability to assay nitrite at low concentrations are complicated due to their tendency to aggregate [19, 20]. Previous studies have shown that the composites consisting of Au NPs and conducting polymers possess not only the properties of each component, but also the new properties with a synergistic effect [10, 21–24]. Lin et al. [22] synthesized PEDOT/Au NP composite by electropolymerization of EDOT (3,4-diethoxythiophene) in a solution containing colloidal Au NPs showing good performance of detecting nitrite. Fan et al. [23] reported Au nanoclusters (Au NCs) stabilized by bovine serum albumin doped into PEDOT by electropolymerization for electrochemical sensing of nitrite.

Conductive polymers are ideal substrates for the uniform deposition of Au NPs, and the deposition of gold nanoparticles on conductive polymers can improve the electroactive surface area, promote electrodynamics, and improve the sensitivity and selectivity of electrodes. PEDOT and its derivatives are often used as substrates to stabilize Au NPs owing to the strong interaction between S atoms in thiophene rings and Au NPs [25, 26]. Researches have shown that thiol groups-functionalized PEDOT can effectively stabilize Au NPs by Au-S bonding. This allows Au NPs to have high dispersal, size-specific physical and chemical properties, and excellent electrocatalytic activity [27]. However, EDOT adducts may change the original bulk properties of a conducting polymer [15]. EDOT can be easily electropolymerized and form porous network at relatively low potentials [26, 28], while thiomethyl 3,4-ethylenedioxythiophene (EDOT-SH) can hardly electropolymerized at relatively high potential at 1.72 V [29]. Ouyang et al. found that electrochemically polymerized PEDOT-NH<sub>2</sub> had a higher impedance than PEDOT, and the formation of multilayered PEDOT/PEDOT-NH<sub>2</sub> films can overcome the deficiency of low conductivity of PEDOT-NH<sub>2</sub> effectively by the covalent bonds between the polymer and indium tin oxide (ITO) surface and PEDOT layer coated on PEDOT-NH<sub>2</sub> [30].

Herein, we reported a three-step approach to create a multilayered PEDOT/PEDOT-SH/Au nanocomposite on glassy carbon electrode (GCE) and ITO. First, PEDOT was selected for electropolymerization onto the substrate to form a porous network structure as a bottom layer. Then, using the PEDOT porous network as a hard template, the EDOT-SH monomer was electrochemically polymerized on the hard template to form a layer-by-layer structure of PEDOT/PEDOT-SH by the adsorption of EDOT-SH on the PEDOT layer by the  $\pi$ - $\pi$  staking between PEDOT polymer chains and EDOT-SH molecules. And, the porous networks have the advantages of large specific surface area and high porosity for ion adsorption. The Au NPs were then electrochemically deposited on PEDOT/PEDOT-SH by reducing HAuCl<sub>4</sub> to obtain multilayered PEDOT/PEDOT-SH/Au nanocomposites. The thiol group in PEDOT-SH can effectively stabilize Au NPs through Au-S

bond and allows Au NPs to have high dispersion and excellent electrocatalytic activity. Based on these considerations, the multilayered PEDOT/PEDOT-SH/Au nanocomposites were electrochemically deposited on GCE and ITO to find out the relations between structural properties and electrochemical performances of nanocomposites from GCE and ITO by applying the composite for the electrochemical sensing of nitrite. Furthermore, the effect of electrode materials on the electropolymerization process, morphology, and electrochemical response of multilayered nanocomposites to nitrite ions were also studied in this research.

## Experimental

### Chemicals

3,4-Ethylenedioxythiophene (EDOT, >99%), chloroauric acid hydrate (HAuCl<sub>4</sub>•4H<sub>2</sub>O, 99%), acetonitrile, lithium perchlorate (LiClO<sub>4</sub>, >99%), and sodium nitrite (NaNO<sub>2</sub>, 99%) were purchased from Shanghai Aladdin Reagent Company (<http://www.aladdin-reagent.com/>). All other chemicals were analytical grade, and all aqueous solutions were prepared with double distilled water. Phosphate buffer was prepared by mixing stock standard solutions of K<sub>2</sub>HPO<sub>4</sub> (>99%) and KH<sub>2</sub>PO<sub>4</sub> (>99%). All experiments were carried out at room temperature.

### Structure characterization

The FT-IR spectra of the samples were recorded on an FT-IR spectrometer (BRUKER-QEUNOX-55) using KBr disk at a resolution of 4 cm<sup>-1</sup>. The UV-vis spectra of the samples were recorded by a UV-visible spectrophotometer (UV4802, Unico, USA) to determine the absorbance of polymer films deposited on ITO (Ying kou you xuan Trade co., Ltd., square resistance <10 Ω) slides in situ directly. The morphological information of the samples was obtained by a scanning electron microscope (SEM, SO8010, Japan). Energy dispersive X-ray spectroscopy (EDS) of samples was performed with a scanning electron microscope (Hitachi, S-4800, operating voltage, 5 kV, Japan). X-ray photoelectron spectroscopy (XPS) of samples was obtained by an ESCALAB 250Xi spectrometer (Al K $\alpha$ ~1486.6 eV).

### Preparation of the PEDOT/PEDOT-SH/Au nanocomposite

The monomer of EDOT-SH was synthesized based on a literature report [31].

PEDOT/PEDOT-SH/Au nanocomposite was prepared in three steps as follows:

First, the electropolymerization of EDOT was carried out by the cyclic voltammetry (CV) method in acetonitrile containing 5 mM EDOT and 0.1 M LiClO<sub>4</sub> between 0 and 1.5 V at a scan rate of 50 mV s<sup>-1</sup> for five cycles. Then, the prepared PEDOT:ClO<sub>4</sub> film was labeled as PEDOT; PEDOT-modified glassy carbon electrode (PEDOT/GCE) was rinsed with acetonitrile.

Second, the PEDOT/GCE was employed as the working electrode for the electropolymerization of EDOT-SH by the CV method in acetonitrile containing 5 mM EDOT-SH and 0.1 M LiClO<sub>4</sub> between 0 and 1.5 V at a scan rate of 50 mV s<sup>-1</sup> for four cycles. Then, the prepared PEDOT:ClO<sub>4</sub>/PEDOT-SH:ClO<sub>4</sub> was labeled as PEDOT/PEDOT-SH; PEDOT/PEDOT-SH-modified GCE (PEDOT/PEDOT-SH/GCE) was rinsed with acetonitrile.

Finally, the electrodeposition of Au NPs was performed in a 1.0 mM HAuCl<sub>4</sub> solution with 0.1 M KCl by potentiostatic technique at the potential of -0.5 V for 100 s. After deposition, the prepared catalyst (PEDOT/PEDOT-SH/Au/GCE) was rinsed with deionized water for several times and then dried at room temperature.

The preparation method of pure PEDOT and PEDOT-SH was the same as the above, and the total number of cycles in this process was the same. The preparation process on ITO was the same as that on the GCE.

### Measurement of the electrocatalytic activity

Cyclic voltammogram experiments and amperometric measurements were performed using an electrochemical workstation CHI 660C (ChenHua Instruments Co., Shanghai, China). Electrochemical impedance tests were carried out using electrochemical workstation Zahner Zennium. A three-electrode system was employed to study the electrochemical performance of the composites. A saturated calomel electrode (SCE) was used as a reference electrode, a Pt electrode was used as a counter electrode, the PEDOT/PEDOT-SH/Au/GCE (diameter = 4 mm) and the PEDOT/PEDOT-SH/Au/ITO (length = 15 mm, width = 7 mm) were used as the working electrodes. CV measurement was performed in 0.1 M phosphate buffer (pH 6.86) containing 4 mM nitrite ion between 0 and 1 V at a scan rate of 50 mV s<sup>-1</sup>. Amperometric measurement techniques were used for the quantification of nitrite ion in 0.1 M phosphate buffer (pH 6.86). Electrochemical impedance spectroscopy (EIS) test was performed in 0.1 M KCl solution containing 5.0 mM Fe(CN)<sub>6</sub><sup>3-/4-</sup> at open circuit potential in the frequency range from 0.01 to 10<sup>5</sup> Hz with the amplitude of 5 mV.

## Results and discussion

### Preparation of the PEDOT/PEDOT-SH/Au nanocomposite on the GCE and ITO surfaces

Fig S1(a) shows the electrochemical deposition process of PEDOT-SH on a bare GCE from a solution of EDOT-SH in acetonitrile containing LiClO<sub>4</sub> as supporting electrolyte by scanning the potential between 0 and 1.5 V versus the SCE reference electrode. It is clear from the first voltammetric curve that a rapid increase in the anodic current started at ~ 1.30 V, which corresponded to the beginning of the EDOT-SH monomer oxidation. The current decreases with successive potential scanning, indicating that the electropolymerization of EDOT-SH to PEDOT-SH becomes increasingly difficult. The decrease in the anodic and cathodic peak current indicated an increase in the amount of polymer on the electrode surface and the poor conductivity of PEDOT-SH.

As shown in Fig. S1(b), in the first scan of the oxidation of the EDOT-SH monomer, the radical cation on the PEDOT film forms at approximately 1.0 V which is lower than that deposited on the bare GCE. The current increases with successive potential scanning, indicating the electropolymerization of EDOT-SH to PEDOT-SH. The increase in the anodic and cathodic peak current densities suggests an increase in the amount of polymer on the electrode surface, and that the electrochemical polymerization of EDOT-SH on PEDOT is easier than that on the bare GCE. In the case of ITO (Fig.S1(d, e)), the voltammetric curves show little difference in initial oxidation potential compared with the one recorded for the GCE. The initial oxidation potential of PEDOT-SH on ITO is slightly higher than that on the GCE which indicates that the electropolymerization process does not dependent on the electrode material.

Fig. S1(c, f) shows the I-T curves of the electrodeposition of Au NPs on the PEDOT-SH and PEDOT/PEDOT-SH films. In the first few seconds, the cathodic current decreases greatly, indicating the rapid formation of gold seeds on the PEDOT/PEDOT-SH film, while the cathodic current only decreases slightly on the PEDOT-SH film due to the poor conductivity of PEDOT-SH on the bare GCE and ITO. Over the next few hundred seconds, the intensity of cathodic current decreases slowly attributing to the gold seeds grow slowly into gold nanoparticles.

### Characterization of the PEDOT/PEDOT-SH/Au composite

The FT-IR spectra, UV-vis absorption spectra, and EDS of composites were shown in Fig.S2 and Fig.S3. XPS spectra were shown in Fig. 1. The wide-scan XPS spectra of PEDOT/PEDOT-SH/Au show sharp peaks at 86, 163, 284, and 532 eV corresponding to the signals of Au 4f, S 2p, C

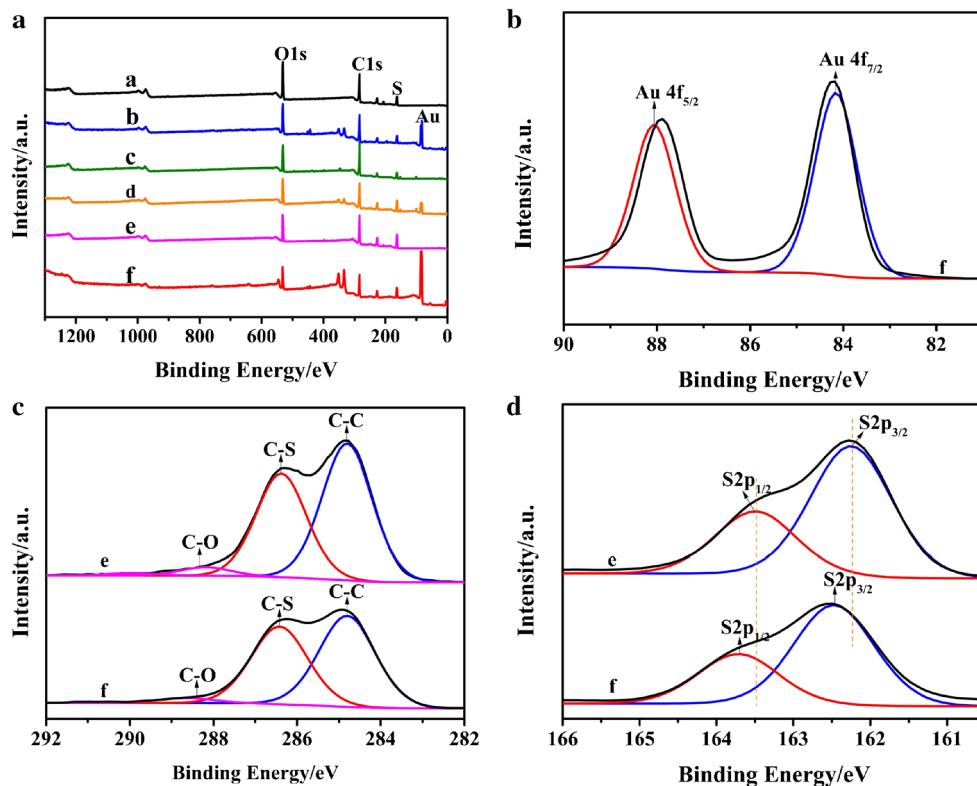
1s and O 1s, respectively. Figure 1b–d show the high-resolution XPS spectra of the PEDOT/PEDOT-SH/Au nanocomposite. For the PEDOT/PEDOT-SH/Au nanocomposite, the Au 4f<sub>7/2</sub> and Au 4f<sub>5/2</sub> peaks at 84.18 and 88.08 eV indicate the presence of Au<sub>0</sub> (Fig. 1b). As shown in Fig. 1c, the C 1s spectra of PEDOT/PEDOT-SH and the PEDOT/PEDOT-SH/Au nanocomposites display three peaks at 284.7, 286.3, and 288 eV corresponding to the C-C, C-S, and C-O bonds, respectively. The S 2p spectra of PEDOT/PEDOT-SH/Au possesses spin-split doublet peaks at 162.4 (S 2p<sub>3/2</sub>) and 163.7 eV (S 2p<sub>1/2</sub>). This is slightly lower than PEDOT/PEDOT-SH indicating the formation of Au-S bond in PEDOT/PEDOT-SH/Au (Fig. 1d).

Figure 2a displays the SEM images of polymers and composites films from GCE and ITO, respectively. As shown in Fig. 2a, the PEDOT-SH film on a GCE is composed of particles that are closely assembled to form a relatively rough surface morphology. However, after electrochemical reduction of HAuCl<sub>4</sub>, Au NPs are not clearly observed in PEDOT-SH/Au (Fig. 2d) due to the poor conductivity of PEDOT-SH on the GCE hindering the electrochemical reduction of HAuCl<sub>4</sub> to Au. This result is in accordance with the EDS results, which depicts that PEDOT-SH/Au from GCE shows low atomic percentage of Au. As shown in Fig. 2b, the PEDOT film on a GCE exhibits a porous network structure composed of nanofibers. This morphology is formed by rapid monomer initiation and polymer chain growth at a relatively high polymerization potential. This morphology of the PEDOT film is

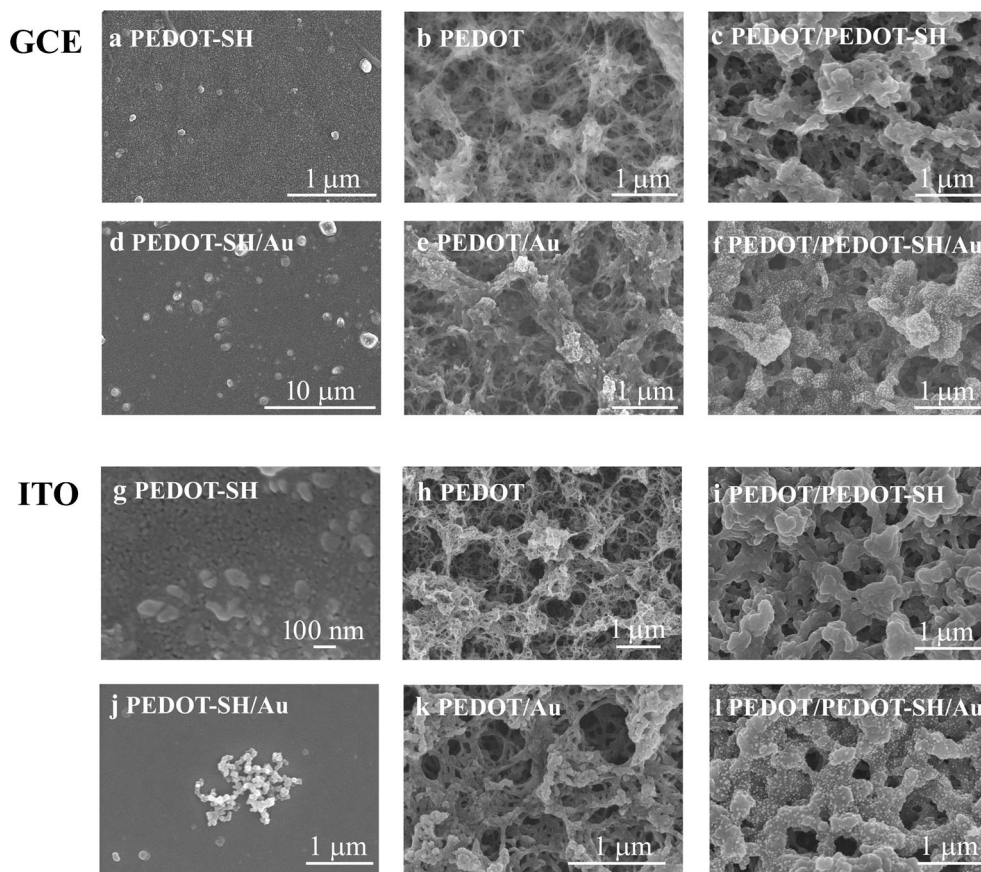
consistent with that reported for an electrochemically synthesized PEDOT film in 0.1 M TBAPC [16, 32]. After electrochemical deposition of Au on PEDOT film (Fig. 2b), the small amount of Au NPs and porous network structure PEDOT can be observed (Fig. 2e). As shown in Fig. 2e, the distribution of Au NPs on the PEDOT porous network is nonuniform and highly aggregated. As depicted in Fig. 2c, after electropolymerization of EDOT-SH on porous network structure PEDOT, the nanofibers become thick with some block structures, suggesting that the PEDOT-SH layer uniformly grows on the surface of the PEDOT layer to form a porous PEDOT/PEDOT-SH, and PEDOT/PEDOT-SH (Fig. 2f) displays more uniform distribution of Au NPs on the porous network of PEDOT/PEDOT-SH than that of PEDOT-SH/Au (Fig. 2d) and PEDOT/Au (Fig. 2e). Partial enlargement of PEDOT and PEDOT/PEDOT-SH was shown in Fig. S4.

A comparison implies that the films on GCE shows little difference from ITO indicating that the microstructures of PEDOT-SH, PEDOT, PEDOT/PEDOT-SH, and composites with Au NPs do not strongly depend on the substrate (GCE and ITO). And compared with the PEDOT-SH film on the GCE, there is massive accumulation of small particles on ITO. The morphology of PEDOT on ITO is similar to that on the GCE. After electrochemical deposition of Au on PEDOT film (Fig. 2k), nonuniform and highly aggregated Au NPs occurred in porous network of PEDOT. However, the morphology of the PEDOT/PEDOT-SH multilayer film on ITO (Fig. 2i) is different from GCE (Fig. 2c), and the

**Fig. 1** XPS spectra of (a) PEDOT/ITO, (b) PEDOT/Au/ITO, (c) PEDOT-SH/ITO, (d) PEDOT-SH/Au/ITO, (e) PEDOT/PEDOT-SH/ITO, and (f) PEDOT/PEDOT-SH/Au/ITO. High-resolution scans of (b) Au4f, (c) C1s, and (d) S2p



**Fig. 2** SEM images of (a) PEDOT-SH/GCE, (b) PEDOT/GCE, (c) PEDOT/PEDOT-SH/GCE, (d) PEDOT-SH/Au/GCE, (e) PEDOT/Au/GCE, (f) PEDOT/PEDOT-SH/Au/GCE, (g) PEDOT-SH/ITO, (h) PEDOT/ITO, (i) PEDOT/PEDOT-SH/ITO, (j) PEDOT-SH/Au/ITO, (k) PEDOT/Au/ITO, (l) PEDOT/PEDOT-SH/Au/ITO

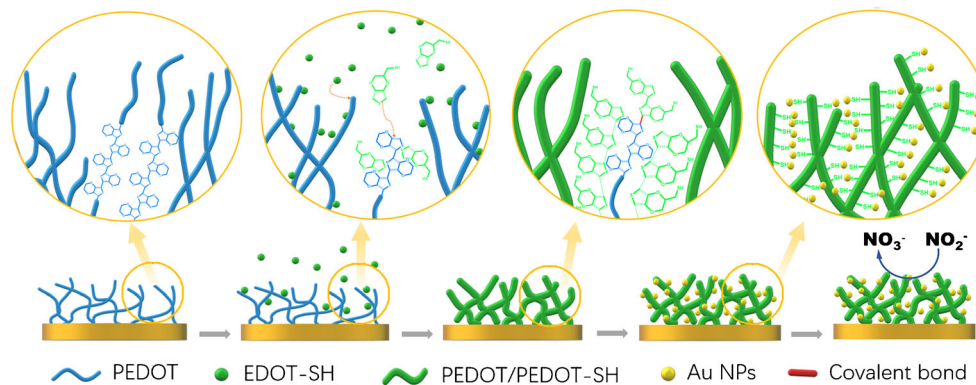


porous PEDOT/PEDOT-SH on ITO are thicker than those on the GCE. It is difficult to observe the fibrous structure inside the hole in the case of ITO, whereas the nanofiber can be observed clearly in the hole, in the case of the GCE. Another obvious difference is that the size of the gold obtained by electrochemical reduction on the polymer film surface on ITO is larger than that obtained on the GCE.

Scheme 1 indicates the possible formation mechanism of multilayered PEDOT/PEDOT-SH/Au. As a hard template for EDOT-SH polymerization, PEDOT first adsorbs EDOT-SH monomer on its surface by  $\pi$ - $\pi$  stacking, and the adsorbed EDOT-SH monomers polymerized with on the surface of

PEDOT, while some of them copolymerized with oligomers on the surface of PEDOT. PEDOT-SH grows uniformly on the surface of the PEDOT nanofibers and gradually results in an increase in the thickness of the fibers. When the redox reaction happens, Au nuclei will grow on the surface of the porous PEDOT/PEDOT-SH, and Au will attach to the thiol groups through Au-S bonding. Then, the Au nuclei will slowly grow into nanoparticles with low agglomeration of Au NPs because the coated PEDOT-SH layer on the PEDOT matrix reduces the conductivity of the polymer layer, while highly aggregated Au NPs occurred in porous network of PEDOT (Fig. 2e, k) resulting from its high conductivity. And the uniform

**Scheme 1** The growth process of PEDOT/PEDOT-SH/Au on electrode surface



distribution of Au NPs on the porous network of PEDOT/PEDOT-SH occurred in both of GCE and ITO, suggesting that the stabilization effect of thiol group in PEDOT-SH for Au NPs through Au-S bond, allowing Au NPs to have high dispersion.

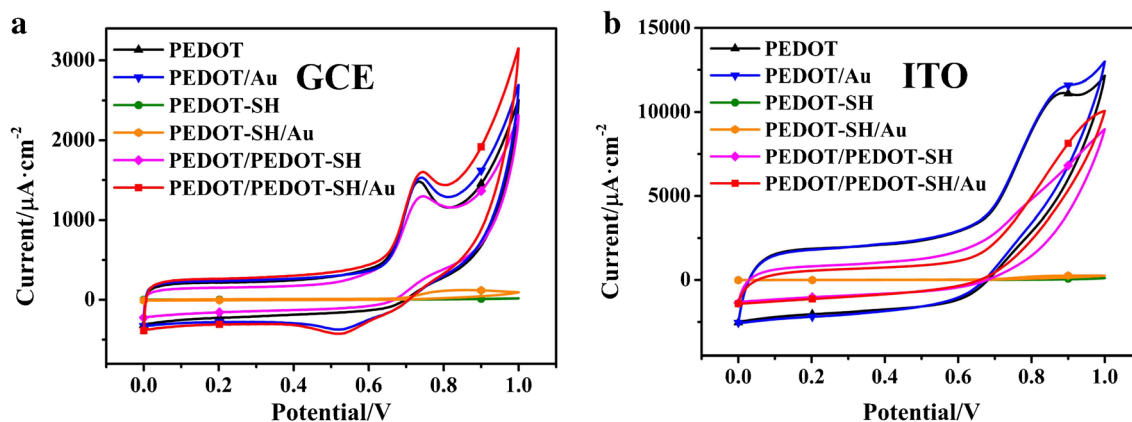
### Electrochemical impedance spectra

The impedance spectra of PEDOT, PEDOT-SH, PEDOT/PEDOT-SH, PEDOT/Au, PEDOT-SH/Au, and PEDOT/PEDOT-SH/Au on the GCE (A) and ITO (B) are shown in Fig. S4. As shown in Fig. S4(a), the PEDOT coatings decrease the impedance of the GCE over the entire frequency spectrum. At lower frequencies, a great decrease in the impedance amplitude is found. However, in the case of PEDOT-SH prepared under the same conditions, the impedance of the PEDOT-SH-modified electrode is two orders of magnitude greater than that of bare GCE electrode. This result indicates that the PEDOT-SH films are not electroactive, and the PEDOT-SH coating eventually hinders charge transport. The PEDOT-SH layer deposited on the PEDOT-modified electrodes can also decrease impedance, which is similar to the phenomenon observed for PEDOT. It should be noted that the impedance of PEDOT/Au, PEDOT-SH/Au, and PEDOT/PEDOT-SH/Au decreases significantly at lower frequencies with the presence of Au indicating that the Au NPs effectively promote charge transport. The impedance on ITO is similar to that on GCE (Fig. S4(b)).

### Electrocatalytic oxidation of nitrite with PEDOT/PEDOT-SH/Au/GCE and PEDOT/PEDOT-SH/Au/ITO

Figure 3a shows the CV curves of PEDOT, PEDOT/Au, PEDOT-SH, PEDOT-SH/Au, PEDOT/PEDOT-SH, and PEDOT/PEDOT-SH/Au-modified GCEs in the presence of 4 mM nitrite in 0.1 M phosphate buffer (pH 6.86) at a scan

rate of  $50 \text{ mV s}^{-1}$ . Figure 3a clearly shows that the PEDOT-SH/GCE does not show a significant anodic peak current for nitrite because of its low conductivity. However, the PEDOT-SH/Au-modified GCE exhibits a feeble broad oxidation peak current at 0.85 V due to the electrocatalytic capability of Au NPs for nitrite. In comparison with PEDOT-SH/GCE, the PEDOT and PEDOT/PEDOT-SH-modified GCEs exhibit well-defined oxidation peaks at 0.73 V and 0.74 V, with a prominent increase in the oxidation peak current. This enhancement in the peak current and oxidation peak potential can be attributed to the ideal electrocatalytic performance and high conductivity of PEDOT, which results from the deposition of PEDOT-SH on the PEDOT film enhancing its conductivity and electrocatalytic activity. After the deposition of Au nanoparticles on PEDOT and PEDOT/PEDOT-SH, the oxidation peak current significantly increases. The oxidation peak currents of the PEDOT/Au and PEDOT/PEDOT-SH/Au-modified GCEs are higher than those of the electrode without Au NPs deposition. The oxidation peak current of the PEDOT/PEDOT-SH/Au-modified GCE is higher than that of PEDOT/Au, which is attributed to the uniform distribution of Au NPs on PEDOT-SH. The electrochemical behavior of the same materials on ITO for the oxidation of nitrite is different from that on the GCE. As shown in Fig. 3b, the current response signals of these material-modified ITO electrodes with nitrite are stronger than those of the GCEs, and the oxidation potential is higher than that of the GCEs. The PEDOT-SH and PEDOT-SH/Au-modified ITO electrodes have the lowest current response among the polymers and composites on the GCEs and ITO electrodes. However, PEDOT/PEDOT-SH and PEDOT/PEDOT-SH/Au have a relatively small current response and lower oxidation potential than PEDOT and PEDOT/Au. This property should be due to the thicker PEDOT-SH layer coated on the PEDOT nanofiber, causing a decrease in the conductivity of the composite. The CV of the PEDOT/PEDOT-SH/Au in saturated nitrogen and saturated oxygen is shown in Fig. S6. The results showed that the



**Fig. 3** Cyclic voltammograms of PEDOT, PEDOT/Au, PEDOT-SH, PEDOT-SH/Au, PEDOT/PEDOT-SH, and PEDOT/PEDOT-SH/Au in 0.1 M phosphate buffer (pH 6.86) containing 4 mM  $\text{NaNO}_2$  on (a) GCE and (b) ITO at scan rate of  $50 \text{ mV s}^{-1}$

PEDOT/PEDOT-SH/Au/GCE did not respond to the oxygen dissolved in the solution, suggesting that the dissolved oxygen has no effect on the electrochemical detection of nitrite.

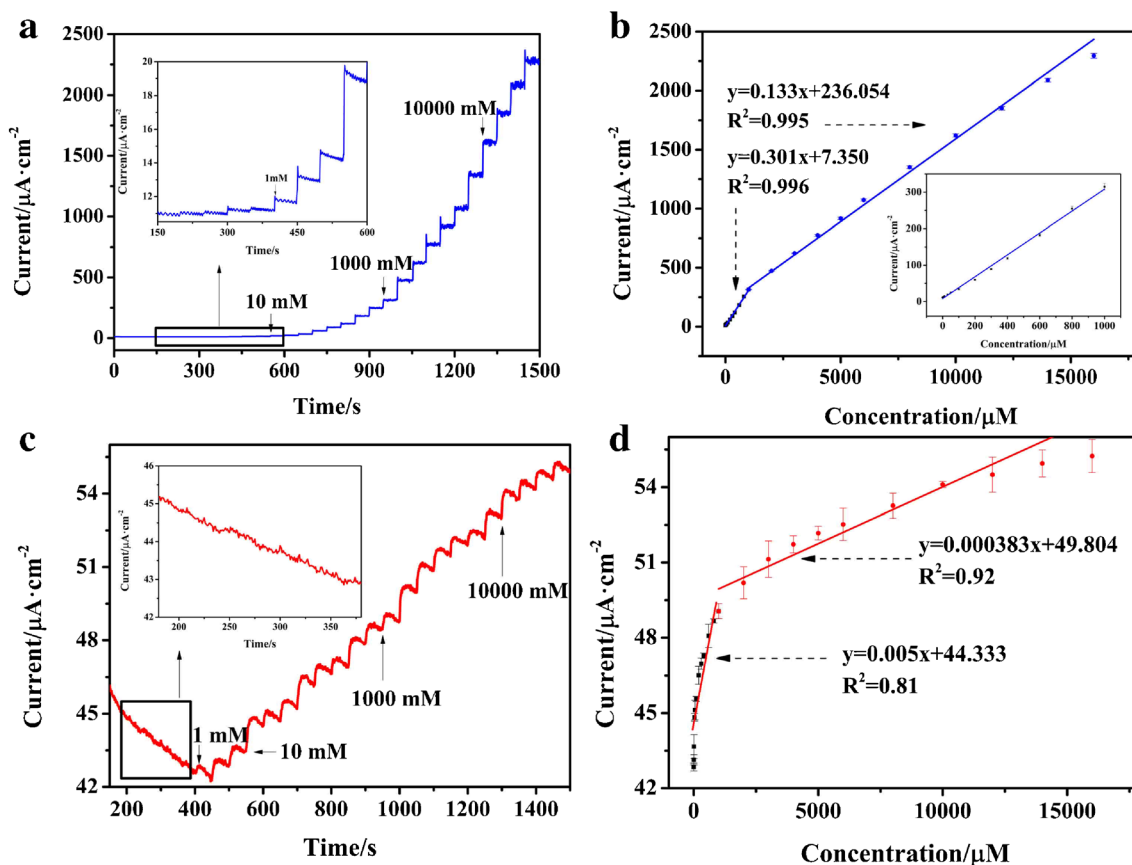
### Amperometric sensing of nitrite

The amperometry measurement was used on electrochemical oxidation of nitrite (Fig. 4) with the PEDOT/PEDOT-SH/Au-modified GCE and ITO for the successive addition of nitrite in 0.1 M phosphate buffer (pH 6.86) at potentials of 0.74 V and 0.95 V under stirring conditions. For the PEDOT/PEDOT-SH/Au-modified GCE, after adding nitrite, the current response of the PEDOT/PEDOT-SH/Au/GCE increases rapidly and reaches a stable state within 3 s (Fig. S7). Furthermore, this rapid increase in response to nitrite at the PEDOT/PEDOT-SH/Au-modified GCE is proportional to the concentration of nitrite. The corresponding calibration plot for the response of nitrite is presented in Fig. 4b. The amperometric response is linear with an increase in the peak current for the nitrite concentration over the ranges from 0.15 to 1 mM and 1 to 1.6 mM. The linear regression equation for the calibration plot can be expressed as  $j(\mu\text{A cm}^{-2}) = 0.301 C_{\text{nitrite}}(\mu\text{M}) + 7.350$  ( $R^2 = 0.996$ ) and  $j(\mu\text{A cm}^{-2}) = 0.133 C_{\text{nitrite}}(\mu\text{M}) + 236.054$

( $R^2 = 0.995$ ) with sensitivity of  $0.301 \mu\text{A } \mu\text{M}^{-1} \text{ cm}^{-2}$  and  $0.133 \mu\text{A } \mu\text{M}^{-1} \text{ cm}^{-2}$ , respectively. A detection limit of  $0.051 \mu\text{M}$  was calculated from  $3(S/N)$ , where  $S$  is the standard deviation of the blank signal, and  $N$  is the slope of the calibration plot. The standard error of slope and intercept of regression equations was shown in Table S1.

Compared with the PEDOT/PEDOT-SH/Au-modified GCE, the modified ITO electrode has a small current response for nitrite oxidation (Fig. 4c, d). After adding nitrite, the current response of the modified electrode increases slowly and hardly reaches a stable state. The amperometric response was found to be linear with an increase in the current for the nitrite concentration over the ranges from 40 to 1 mM and 1 to 1.6 mM, but the linear relationship is relatively poor. The linear regression equation for the calibration plot can be expressed as  $j(\mu\text{A cm}^{-2}) = 0.005 C_{\text{nitrite}}(\mu\text{M}) + 44.333$  ( $R^2 = 0.81$ ) and  $I(\mu\text{A}) = 0.000383 C_{\text{nitrite}}(\mu\text{M}) + 49.804$  ( $R^2 = 0.92$ ) with sensitivity of  $0.005 \mu\text{A } \mu\text{M}^{-1} \text{ cm}^{-2}$  and  $0.000383 \mu\text{A } \mu\text{M}^{-1} \text{ cm}^{-2}$ , respectively. Based on the above experimental results, the PEDOT/PEDOT-SH/Au/GCE with good performance was chosen for the following test.

The related data for the performance of the present sensor compared with the other previously reported sensors for the



**Fig. 4** Amperometric responses corresponding to consecutive additions of standard solutions of nitrite to a stirred 0.1 M phosphate buffer using the PEDOT/PEDOT-SH/Au-modified (a) GCE and (c) ITO biased at

0.74 V and 0.95 V, respectively. Calibration plot of current versus concentration of  $\text{NO}_2^-$  (b, d)

**Table 1** Comparison of the analytical performance of the various material-modified electrodes for nitrite detection

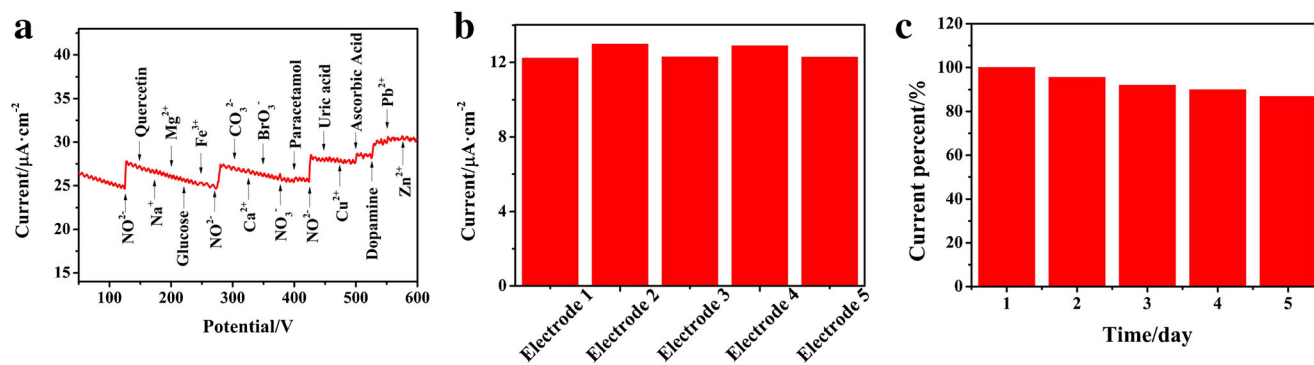
Modified electrode	Method	Potential (V)	Linear range ( $\mu\text{M}$ )	LOD ( $\mu\text{M}$ )	Sensitivity ( $\mu\text{A } \mu\text{M}^{-1} \text{ cm}^{-2}$ )	Ref.
AuNPS-PEDOT / $\text{PMo}_9\text{V}_3$ /GCE	CV	0.9	0.0025–1430	0.001	0.67	[10]
PEDOT/AuNP	AMP	0.8	0.2–1400	0.06	-	[22]
PEDOT/AuNCs	AMP	0.8	0.05–2600	0.017	-	[23]
PEDOT-Au	AMP	0.78	3–300	0.1	-	[24]
PANI/ABS/GCE	DPV	-	0.3–35 100–1000	0.48	23.04 0.8	[33]
Au/PANI/ $\text{SnO}_2$ /GCE	AMP	0.9	0.25–2400	0.08	0.00008314	[34]
CQD-PEDOT	AMP	0.8	0.50–1110	0.088	0.01436	[35]
GO-Ag	LSV	-	1–1000	0.24	-	[36]
Pt/CoO/GCE	AMP	0.9	0.2–3670 3670–2370	0.067	0.9014 0.4085	[37]
$\text{NiFe}_2\text{O}_4$ -CPE	AMP	0.85	0.1–1000	0.1236	7.9617	[38]
rGO- $\text{MoS}_2$ -PEDOT	DPV	-	1–1000	0.059	874.19	[39]
ZnS	AMP	0.85	0.02–1350	0.0085	-	[40]
PEDOT/PEDOT-SH/Au /GCE	AMP	0.74	0.15–1000 1000–16,000	0.051	0.301 0.133	This work

detection of nitrite are listed in Table 1. The LOD and linear range of present sensor is comparable with other sensor materials but not the best [10, 22–24, 33–40]. The performance of PEDOT/PEDOT-SH/Au/GCE in LOD is better than that of the electrode materials except AuNPS-PEDOT/ $\text{PMo}_9\text{V}_3$ /GCE [10], PEDOT/AuNCs [23], and ZnS [40]. However, it should be noted that the working potential of PEDOT/PEDOT-SH/Au/GCE is 0.74 V, which is lowest than that of electrode materials in Table 1. Furthermore, the best LOD in AuNPS-PEDOT/ $\text{PMo}_9\text{V}_3$ /GCE [10] compared with that of others may be affected when using in an alkaline condition, in which the acidic character of doping agent of heteropoly acid can decrease the electroactivity of composite material. This indicates the practical use of PEDOT/PEDOT-SH/Au/GCE in nitrite sensor. The linear range of detection is wide, and the LOD is lower than 3 mg/L of the World Health Organization fixed. This suggests that the modified GCE provided a good

platform for the effective recognition of nitrite in water samples at low concentration ranges. The sensitivity of present sensor are not very well compared with others reported.

### Reproducibility, stability, and selectivity of PEDOT/PEDOT-SH/Au/GCE

The interference experiments of nitrite detection were carried out in order to evaluate the selectivity of the prepared sensor. As shown in Fig. 5a, PEDOT/PEDOT-SH/Au/GCE shows an obvious response toward 10  $\mu\text{M}$   $\text{NaNO}_2$  and an unobvious current change toward 100  $\mu\text{M}$  various common ions (i.e.,  $\text{Na}^+$ ,  $\text{Ca}^+$ ,  $\text{Mg}^{2+}$ ,  $\text{Zn}^{2+}$ ,  $\text{CO}_3^{2-}$ ,  $\text{NO}_3^-$ , and  $\text{BrO}_3^-$ ), 100  $\mu\text{M}$  various metal ions (i.e.,  $\text{Fe}^{3+}$ ,  $\text{Cu}^{2+}$ , and  $\text{Pb}^{2+}$ ), 100  $\mu\text{M}$  physiological interference (i.e., glucose and uric acid), 100  $\mu\text{M}$  drug paracetamol, and 100  $\mu\text{M}$  flavonoid quercetin. But for 100  $\mu\text{M}$  dopamine and ascorbic acid, there are obviously



**Fig. 5** **a** Amperometric measurements performed with the PEDOT/PEDOT-SH/Au-modified GCE biased at 0.74 V during consecutive addition of 100  $\mu\text{M}$  different compounds tested as interferants and 10 mM nitrite to a stirred 0.1 M phosphate buffer. **b** Amperometric

responses for 50 mM nitrite recorded with 5 different PEDOT/PEDOT-SH/Au/GCE prepared by using the same electrodeposition conditions. **c** Amperometric response of the PEDOT/PEDOT-SH/Au/GCE in 0.1 M phosphate buffer with 50 mM nitrite in a period of 5 days



current response. Fortunately, the oxidation peak potentials of dopamine, ascorbic acid, and nitrite differ considerably, i.e., 0.15 V, 0.28 V, and 0.72 V (versus SCE), respectively, as shown in the differential pulse voltammetry (DPV) curve which can distinguish them very well (Fig. S8). The results demonstrate that the PEDOT/PEDOT-SH/Au/GCE sensing platform possesses good selectivity for the determination of nitrite.

The reproducibility of the PEDOT/PEDOT-SH/Au/GCE sensing platform was estimated by the analysis of the amperometric responses of 50  $\mu\text{M}$  nitrite for five independently prepared PEDOT/PEDOT-SH/Au/GCE. As shown in Fig. 5b, the relative standard deviation (RSD) of these current responses is 2.9%, indicating that the PEDOT/PEDOT-SH/Au/GCE sensing platform possesses good reproducibility for nitrite determination of nitrite.

Furthermore, the long-term stability of the PEDOT/PEDOT-SH/Au/GCE sensing platform was investigated (Fig. 5c). The stability of the sensor was tested by measuring the current response toward 50  $\mu\text{M}$  nitrite after long-term storage at room temperature. Nitrite ions were measured once a day, and the current remained at about 88% of the original value after 5 days. It is the evidence of the good long-term stability of the PEDOT/PEDOT-SH/Au/GCE sensor.

### Real sample analysis

In order to evaluate the usefulness of the PEDOT/PEDOT-SH/Au/GCE in practical applications, the performance of the sensor was tested with tap waters and milk samples. The standard addition method was used to determine the nitrite in tap water and milk samples; the Griess assay method was employed for the determination of nitrite ion present in the same samples and compared with the amperometric results (Table S2).

### Conclusions

In summary, a reliable electrochemical nitrite sensor of PEDOT/PEDOT-SH/Au/GCE was successfully prepared via an electrochemical technique. Systematical investigations revealed that microstructures of PEDOT/PEDOT-SH/Au nanocomposites are not strongly dependent on the substrate. Fibrous PEDOT as hard template can absorb EDOT-SH on it to form porous PEDOT/PEDOT-SH which had the advantages of large specific surface area and high porosity for nitrite ion adsorption. The thiol group in PEDOT/PEDOT-SH can effectively stabilize Au NPs through Au-S bond and allows Au NPs to have high dispersion and excellent electrocatalytic activity. The PEDOT/PEDOT-SH/Au/GCE has a good performance in its electrochemical response to nitrite ions with low oxidation potential, low detection limit, and two wide linear ranges. It also exhibited good reproducibility, stability,

selectivity, and detective performance of nitrite in tap water and milk samples. Nevertheless, the sensitivity of the current system needs to be further improved for trace detection.

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### Compliance with ethical standards

**Conflict of interest** The author(s) declare that they have no competing interests.

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