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Cerebral and blood correlates of reduced functional connectivity in mild cognitive impairment

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Abstract Growing evidence suggests that decreased functional connectivity in cortical networks precedes clinical stages of Alzheimer's disease (AD), although our knowledge about cerebral and biological correlates of this phenomenon is limited. To shed light on this issue, we have investigated whether resting-state oscillatory connectivity patterns in healthy older (HO) and amnestic mild cognitive impairment (aMCI) subjects are related to anatomical grey matter (GM) and functional (2-[18F]fluoro-2-deoxy-Dglucose (FDG)-PET) changes of neuroelectric sources of alpha rhythms, and/or to changes in plasma amyloid-beta $(A\beta)$ and serum lipid levels, blood markers tied to AD pathogenesis and aging-related cognitive decline. We found that aMCI subjects showed decreased levels of cortical connectivity, reduced FDG-PET intake of the precuneus, and GM atrophy of the thalamus, together with higher levels of A β and apolipoprotein B (ApoB) compared to HO. Interestingly, levels of high-density lipoprotein (HDL) cholesterol were positively correlated with the strength of neural-phase coupling in aMCI subjects, and increased triglycerides accompanied bilateral GM loss in the precuneus of aMCI subjects. Together, these findings provide peripheral blood correlates of reduced resting-state cortical connectivity in aMCI, supported by anatomofunctional changes in cerebral sources of alpha rhythms.

D. Garcia-Solis Department of Nuclear Medicine, University Hospital Virgen del Rocio, Seville, Spain This framework constitutes an integrated approach to assess functional changes in cortical networks through neuroimaging and peripheral blood markers during early stages of neurodegeneration.

Keywords Functional connectivity · Resting-state cortical networks · Alpha rhythm · Grey matter · FDG-PET · Mild cognitive impairment · Plasma amyloid-beta · Lipid markers · Cholesterol

Introduction

Aging is characterized by morphological changes in neurons, synaptic loss, and alterations in neurotransmitter receptors (Masliah et al. 1993; Hof and Morrison 2004; Bishop et al. 2010). A β neuritic plaques and neurofibrillary tangles are also present in clinically intact older adults showing the same or different distribution as in Alzheimer's disease (AD) patients (Tomlinson et al. 1968; Katzman et al. 1988; Price et al. 1991), although agerelated tangle formation does not by itself represent a process that would inevitably progress to AD (Price and Morris 1999). Therefore, the different degree of resistance to AD neuropathology (Snowdon 2003) together with the heterogeneity of clinical outcomes in individuals with comparable degrees of pathologic brain lesions (Iacono et al. 2009) illustrate the complexity of the aging process and foresees major obstacles to establish biological boundaries between normal aging and incipient neurodegeneration.

Synaptic dysfunctions and neuronal loss are two major pathological hallmarks of AD (DeKosky and Scheff 1990; Terry et al. 1991). Mounting evidence has shown that increased brain levels of soluble A β oligomers are linked to

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synaptic damage in AD (Lambert et al. 1998; Mucke et al. 2000; Walsh et al. 2002; Lesné et al. 2006; Lacor et al. 2007), likely accounting for disruption of neural circuits (Hsia et al. 1999; Palop et al. 2007; Cao et al. 2012; Cheng et al. 2013) and aberrant connectivity patterns in distributed brain networks during disease progression (Babiloni et al. 2004; Greicius et al. 2004; Stam et al. 2006; Brier et al. 2012).

Alpha oscillations are intrinsically generated by pyramidal neurons of cortical layer 5 (Silva et al. 1991), which are affected by dense-core plaques in AD patients (Arnold et al. 1991). The thalamus, that also plays an important role in the generation of the alpha rhythm (Lopes da Silva 1991; Hughes et al. 2004), has shown modest A β deposits and neurofibrillary tangles in AD patients (Rudelli et al. 1984; Masliah et al. 1989; Braak and Braak 1991). However, it remains to be elucidated whether impaired functional connectivity of resting-state cortical networks is accompanied by anatomo-functional damage of cortical and thalamic sources of EEG-alpha rhythms in amnestic mild cognitive impairment (aMCI) subjects.

Up to now, neither A β nor lipid concentration in blood have been confirmed as reliable AD biomarkers. However, the plasma $A\beta_{1-42}/A\beta_{1-40}$ ratio predicts cognitive decline and AD progression (Koyama et al. 2012) as well as volume changes in the medial temporal lobe of healthy older (HO) subjects (Sun et al. 2011). Animal evidence also supports a link between alterations in lipid metabolism and AD pathogenesis (Pappolla et al. 2003; Shobab et al. 2005; Panza et al. 2006; Ghribi 2008; Martins et al. 2009; Di Paolo and Kim 2011), suggesting that elevated levels of cholesterol might contribute to accelerate AD progression (Simons et al. 1998; Grimm et al. 2008; Xiong et al. 2008) and to increase the risk for brain lesions and dementia (Leritz et al. 2011; Williams et al. 2013). However, no studies to date have investigated whether blood levels of A β and/or lipids are related to changes in the resting-state functional anatomy of the brain in aMCI subjects.

The purpose of the present study is therefore twofold: to investigate whether connectivity failures observed in aMCI are related to changes in grey matter (GM) and/or glucose consumption of the main neuroelectric sources of EEG-alpha rhythms; and to assess whether patterns of cortical connectivity are differently associated with changes in $A\beta$ and lipid levels in HO and aMCI subjects.

Materials and methods

Subjects

Twenty-nine older adults with aMCI (10 females, mean age: 70.1 ± 6.8 years) and 26 HO subjects (15 females, mean

age: 66.5 ± 4.9 years) were enrolled in the study. Participants were primarily recruited from older people's associations, normal community health screening, and hospital outpatient services. All of them gave written informed consent prior to experiments. Approval for the study was obtained from the Human Research Ethics Committee of the University Pablo de Olavide in accordance with the ethical standards of the Declaration of Helsinki.

Each participant underwent structured, uniform evaluation that included a medical history, neurological examination, and cognitive function testing. Only those who met established criteria (see below) were included in the study. Cerebral magnetic resonance imaging (MRI) was previously examined in all participants to rule out territorial cerebral infarctions, brain tumors, hippocampal sclerosis, and/or vascular malformations. Those subjects with large periventricular and/or deep white matter (WM) lesions, revealed by scores ≥ 2 on the Fazekas ischemic scale (Fazekas et al. 1987), were excluded from the study. Cardiovascular risk factors (hypertension, diabetes, overweight, family history of coronary heart disease or stroke) were also exclusion criteria.

aMCI subjects showed an idiopathic amnestic disorder with absence of impairment in cognitive areas other than memory, and they further met diagnostic criteria for aMCI (Petersen et al. 1999): (1) subjective memory complaints corroborated by the informant; (2) objective memory loss confirmed by the Spanish version of the Logical Memory subtest extracted from the Wechsler Memory Scale-Third Edition (WMS-III) (scorings 1.5 standard deviations below the age-appropriate mean); (3) global score of 0.5 (questionable dementia) in the clinical dementia rating (CDR); (4) normal independence function; and (5) no DSM-IV criteria for dementia. The global cognitive status was assessed with the Mini Mental State Examination (MMSE), adapted and validated for Spanish population (Blesa et al. 2001). A neurologist with long-standing experience in the diagnosis and treatment of dementia made the diagnosis of aMCI and ruled out any medical or neurological conditions in HO subjects. The diagnosis was further supported by results derived from a comprehensive neuropsychological battery: Boston Naming Test, Trail Making Test, Rey-Osterrieth Complex Figure Test, Visual Object and Space Perception Battery, verbal fluency and word list (Wechsler Memory Scale). The absence of secondary causes of cognitive deficits was confirmed by laboratory tests including complete blood count, vitamin B12/ folate, and thyroid function tests. Elderly depression was excluded using the shorter version of the Geriatric Depression Scale (Yesavage et al. 1983). None of the participants were taking cholinesterase inhibitors, and/or psychiatric medication at the time of recruiting or during the study.

Inclusion criteria for HO subjects were (1) absence of cognitive impairment (memory, language, attention, and

executive function) confirmed by neuropsychological assessment, (2) CDR global score of 0 (no dementia), and (3) normal independent function. HO subjects were tested following the same neuropsychological protocol as for aMCI subjects.

APOE genotyping

Genomic DNA was isolated from blood using a salting-out protocol (Miller et al. 1988), and ApoE polymorphisms were determined with pre-designed TaqMan SNP geno-typing assays (Applied Biosystem). The presence/absence of the ApoE ϵ 4 allele was not employed as an inclusion criterion during the recruiting process.

Blood A β and lipid levels

Venous blood samples were obtained after overnight fasting. Blood samples were collected in 10 mL K2-ethylenediaminetetraacetic acid (EDTA) coated tubes (BD Diagnostics), and further centrifuged (3,500 rpm) at 4 °C for 5 min. Supernatant plasma was collected and aliquoted into 250- μ L polypropylene tubes containing 8.32 μ L of a protease inhibitor cocktail (cOmplete Ultra Tablets mini, Roche). Plasma samples were stored at -80 °C and thawed immediately before assay.

Plasma A β levels were measured blind to cognitive status in duplicate samples (50 µL) according to manufacturer's instructions (Invitrogen). Averaged values (pg/ ml) were used for statistical analyses. Human A β_{1-40} and ultra sensitive A β_{1-42} specific enzyme-linked immunoassay (ELISA) kits were used for this purpose. The detection limit of these assays was 0.52 pg/ml for A β_{1-40} and 0.27 pg/ml for A β_{1-42} . Both inter-assay and intra-assay coefficients of variation were below 10 %. The A β_{1-42} / A β_{1-40} ratio was additionally computed for each subject given its ability to identify cognitively normal subjects who are at increased risk of developing MCI or AD (Graff-Radford et al. 2007), and its association with cognitive decline (Koyama et al. 2012) and with volume loss of the medial temporal lobe in HO adults (Sun et al. 2011).

Fasting serum levels of total cholesterol (TCh), lowdensity lipoprotein (LDL), high-density lipoprotein (HDL), triglycerides (TRIG), and apolipoprotein B (ApoB) were obtained in each participant with the automated A15 Random Access Analyzer[®] (Biosystems S.A., Barcelona, Spain) using Biosystems commercial test kits.

EEG recordings and signal preprocessing

EEG recordings were obtained from 59 scalp electrodes referenced to linked-mastoids, and positioned according to the extended International 10–10 system. Additional

electrodes were placed for monitoring vertical-horizontal eye movements and the muscular tone. Continuous EEG recordings were performed in resting state with eyes closed for 10 min between 9 and 10 AM. Electrophysiological measurements were amplified (BrainAmp MR, Brain Vision[®]), filtered (0.1–100 Hz bandpass), digitized (250 Hz, 16-bit resolution), and stored in digital format for subsequent analyses.

EEG epochs were transformed into the common average reference to partially avoid pernicious effects of reference on neural-phase synchrony results (Schiff 2005). Ocular and muscle artifacts were removed by applying Independent Component Analysis (Infomax algorithm), as implemented in the BrainVision Analyzer software v. 1.05 (Brain Products[®] GmbH). Epochs with noisy EEG channels were manually selected and excluded from further analysis to avoid artificial coupling patterns across electrodes. Quality of EEG recordings was apparently similar in HO and aMCI subjects precluding group effects in functional connectivity due to this factor.

Artifact-free EEG epochs from each participant were filtered within the alpha band (7.5–12.5 Hz), and the alpha peak frequency, defined as the maximum value of spectral power within the alpha band, was computed for each subject. Finally, artifact-free EEG epochs were bandpass filtered within the alpha peak frequency ± 0.5 Hz (Kaiser window, filter order: 1326th, frequency attenuation: 0.5 Hz).

Determining neural-phase coupling in resting-state cortical networks

We calculated instantaneous phases with the Hilbert transform. Neural-phase coupling between pair-wise combinations of scalp EEG signals was computed using the phase lag index (PLI, Stam et al. 2007):

PLI =
$$|\langle \operatorname{sign}[\Delta \varphi(t_k)] \rangle|$$

where $\Delta \varphi(t_k)$ represents the phase difference between the two EEG signals in the time sample t_k . The PLI quantifies how consistently one EEG signal is phase leading or lagging another EEG signal across time, disregarding zero-lag phase differences mainly due to volume conduction and/or active reference electrodes. PLI values range from 0 (no phase coupling) to 1 (perfect phase locking). The first 7 artifact-free EEG epochs of 8-s length were automatically selected in each participant. For each pair of scalp EEG electrodes and subject, we obtained a PLI value that resulted from averaging PLIs computed for each of the artifact-free EEG epochs. The same procedure was applied to surrogate data (see below).

To obtain functional connectivity patterns between EEG signals in each group, electrodes were previously grouped into four regions of interest (ROIs) for the left hemisphere

(frontal ROI: F7, F5, F3, F1, FC5, FC3, FC1; temporal ROI: FT7, T7, TP7; parietal ROI: Cp5, CP3, Cp1, P7, P5, P3, P1; and occipital ROI: PO7, PO3, O1) and their homologous ROIs for the right hemisphere. Electrodes placed in the midline were removed from further analyses together with other EEG locations commonly affected by muscular and oculomotor artifacts. PLIs were computed within each ROI as well as between ROIs, for the same hemisphere or between left and right hemispheres. Overall, we computed 780 PLIs for each subject: 380 PLIs within the same hemisphere and 400 PLIs between different hemispheres.

Cerebral MRI acquisition and image preprocessing

Structural cerebral images were acquired on a whole-body Philips Achieva 3T MRI scanner, using an 8-channel head array coil. A high-resolution MP-RAGE (magnetizationprepared rapid gradient echo) T1-weighted cerebral scan was obtained in each participant. Acquisition parameters were empirically optimized for GM/WM contrast (repetitiontime = 2,300 ms, echo-time = 4.5 ms, flip angle = 88, matrix dimensions 256×192 , 184 contiguous sagittal 1.2 mm thick slices, time per acquisition = 5.4 min).

Cerebral MRIs were visually inspected for artifacts (e.g., excessive blurring due to head motion, poor GM/WM contrast), and those brain scans with poor quality were repeated within the same week. Structural brain images were processed and analyzed with an optimized voxel-based morphometry (VBM) procedure implemented in SPM8 (www. fil.ion.ucl.ac.uk/spm). Briefly, T1 cerebral images on native space were partitioned into GM, WM and cerebrospinal fluid (CSF). GM and WM maps were then registered to the Montreal Neurological Institute canonical brain (MNI152) using DARTEL, a fast diffeomorphic image registration algorithm that minimizes anatomical variations among subjects preserving topology (Ashburner 2007). Resultant cerebral images were resampled to 1.5 mm³ isotropic voxel size. To maintain total GM within the normalized compartments, GM maps were multiplied by relative volumes of warped and unwarped structures derived from the non-linear step of spatial normalization (Jacobian determinants) (Ashburner and Friston 2000). Resultant non-linear modulated warped GM maps were finally smoothed with an isotropic Gaussian kernel of 16 mm.

FDG-PET acquisition and image preprocessing

FDG-PET cerebral images were acquired on a whole-body PET-TAC Siemens Biograph 16 HiREZ scanner (Siemens Medical Systems, Germany) with in-plane and axial resolution of 4.2 and 4.5 mm full-width at half maximum (FWHM), respectively. Subjects fasted for at least 8 h before PET examination. Intravenous lines were placed 10–15 min before tracer injection of a mean dose of 370 MBq of 2-[18F]fluoro-2-deoxy-D-glucose (FDG). Participants stayed in a dimly lit room with their eyes closed to minimize external stimuli during the FDG uptake period. PET scans lasted approximately 30 min. A transmission scan was used for attenuation correction, and FDG-PET cerebral images were reconstructed with $2.6 \times 2.6 \times 2$ mm voxel resolution using standard 2D back-projection filters. We applied partial volume correction (PVC) to cerebral FDG-PET cerebral images with the algorithm implemented in the PMOD software v3.17 (http://www.pmod.com) (Giovacchini et al. 2004).

Absolute values of PVC-FDG cerebral images were normalized to the mean cerebellar glucose consumption using the native brain space of each participant. Next, individual PVC-FDG images normalized to the cerebellum were registered with DARTEL to the MNI152 brain space by applying normalization parameters (deformation fields) previously obtained for cerebral MRI. Modulated warped maps of cerebral glucose consumption were finally smoothed with an isotropic Gaussian kernel of 16 mm.

Obtaining anatomical masks of cerebral sources of EEG-alpha rhythm

Evidence suggests that neuroelectric sources of the human alpha rhythm are located in the cuneus (occipital cortex), precuneus (superior parietal lobe) and thalamus (Cantero et al. 2009a, b). Therefore, all VBM analyses (MRI and FDG-PET) performed in the current study were limited to these ROIs.

Anatomical delimitation of EEG-alpha cerebral sources was obtained with the automated segmentation method implemented in Freesurfer v5.1 (https://surfer.nmr.mgh. harvard.edu/). First, manual edits were introduced in individual brain segmentations until the output was deemed acceptable upon visual inspection. Next, anatomical volume masks of EEG-alpha cerebral sources obtained from each subject were transformed into the same spherical coordinate system and further resampled to the spherical average surface of the study population (Fischl et al. 1999a, b). A transformation matrix was computed to convert average space coordinates of previously segmented alpha cerebral sources into the MNI152 brain space (resampled to 1.5 mm³ isotropic voxel size), allowing us to perform voxel-wise group analysis with anatomo-functional (GM and glucose consumption) masks of EEG-alpha cerebral sources in the same brain space.

Statistical analyses

We previously assessed the normality assumption of data distribution with the Kolmogorov-Smirnov test. All

demographics, cognitive, and plasma A β /serum lipid values were normally distributed, allowing us to apply parametric statistical tests.

Group differences in demographic and cognitive variables were assessed with unpaired t tests, whereas the influence of gender and ApoE ϵ 4 was tested with the Chisquare test due to the categorical nature of these variables. Group differences in blood A β (A β_{1-40} , A β_{1-42} , A β_{1-42} /A β_{1-40} ratio) and lipid levels (TCh, LDL, HDL, TRIG, ApoB) were assessed using different analyses of covariance (ANCOVA) adjusted for age and gender. All these analyses were performed with SPSS v. 15 (SPSS Inc. Chicago, IL).

A bootstrap method was employed to determine if PLI values were significantly above noise and, consequently, had physiological meaning (Lachaux et al. 1999). For each pair of scalp EEG signals, we generated 2,000 surrogate data by adding a temporal shift (a random lag between 4 and 8 s) in one of the two EEG signals originally used to compute the PLI. Surrogate data was then used to compute distribution of 2,000 PLI values for each pair of EEG signals. The PLI value corresponding to the 95th quantile of the surrogate distribution was chosen as the significance threshold. Original PLIs obtained in each group were compared to the thresholded surrogate-PLIs using the Wilcoxon-Mann-Whitney test (Pereda et al. 2005). Only those PLIs that reached statistical significance (p < 0.05) in at least one of the two groups (HO and/or aMCI; aMCI ɛ4 carriers and/or non-carriers) were selected for further analyses.

Next, we determined group differences for each significant PLI. To aim this goal, significant PLIs were permutated by randomly assigning a number of HO subjects to the aMCI group. We computed the T^2 statistic on each permutation (n = 2,000) using the maximum squared T statistic (max T^2) for each PLI, and the 95th quantile of this max T^2 distribution as statistical threshold. This procedure is aimed at controlling the family-wise error (FWE) rate for all pairs of electrodes jointly (Maris 2004). Only those PLI values that reached significant group differences (p < 0.05, FWE corrected) were reported in the current study, and they were next used for correlations with GM volume and glucose consumption of cerebral sources of alpha rhythms.

Group differences in GM volume/glucose consumption of alpha cerebral sources (cuneus, precuneus, and thalamus) were assessed using the modulated VBM approach implemented in SPM8 (ANCOVA with age, gender, and either GM volume or glucose consumption of alpha cerebral sources as covariates, p < 0.05 FWE corrected).

Voxel-wise linear regression analyses were performed to test for relationships between anatomical (GM)/functional (FDG-PET) changes in neural sources of EEG-alpha rhythms and patterns of resting-state EEG coupling. These analyses included group (HO versus aMCI; aMCI ε4 carriers versus non-carriers), age, gender, GM volume/ glucose consumption of alpha cerebral sources, and PLI as regressors. Regression analyses were separately performed for each significant PLI (Z-score transformed). PLIs were split into two groups to test for group differences (T-contrasts) in the way that PLI changes correlated with variations in GM volume/glucose consumption of alpha cerebral sources (p < 0.05, FWE corrected). Regression slopes were compared when correlations reached statistical significance in at least one of the two groups. A similar statistical approach was employed to study relationships between GM volume/glucose consumption of alpha cerebral sources and plasma Aβ/serum lipid levels.

Further regression analyses were performed to test for associations between plasma A β /serum lipid levels and patterns of resting-state cortical connectivity. If at least one of the two groups reached significance, differences between regression slopes were further assessed. These regression analyses were also adjusted for age and gender.

Results

Demographics, cognitive profile, and ApoE4 genotype

Table 1 includes demographic characteristics and cognitive profile for each group. As expected, subjects with aMCI showed significantly lower scores in MMSE (p < 0.01), immediate $(p < 10^{-6})$ and delayed verbal memory $(p < 10^{-10})$ than the HO individuals. The ApoE4 genotype was approximately fourfold higher in aMCI (48.3 %) than in HO subjects (11.5 %). The $\varepsilon 2/\varepsilon 4$ polymorphism was present in only one aMCI subject. aMCI ApoE4 carriers and non-carriers showed similar demographic and cognitive profiles, with the exception of impaired immediate memory (p < 0.03) and a trend toward significance in delayed recall of aMCI ApoE4 carriers (p < 0.07).

Group differences in $A\beta$ and lipid levels

Table 2 shows mean values of plasma A β and serum lipid levels for each group. Overall, A β levels significantly differed between the two groups ($F_{3,49} = 5.2$, p = 0.003). Post hoc analyses revealed that aMCI showed higher concentrations of A β_{1-40} (p = 0.01) and A β_{1-42} (p = 0.001) than HO subjects, whereas group differences in the A β_{1-42} /A β_{1-40} ratio did not reach significance.

The MANCOVA revealed that serum lipid levels were significantly different between the two groups ($F_{5,47} = 2.48$, p < 0.04), although only ApoB showed significant increased levels in aMCI compared to HO subjects (p = 0.05). aMCI ApoE4 carriers and non-carriers

Table 1 Demographics, cognitive profile, and ApoE ε4 distribution

Results are expressed as mean \pm standard deviation *CDR* clinical dementia rating, CDR = 0 no dementia, CDR = 0.5 questionable or very mild dementia. *MMSE* mini-mental state examination; *TMT* Trail Making Test, forms A and B; *VOSP* Visual object and space perception battery; *F/ M* female/male; $\epsilon 4^-$ ApoE $\epsilon 4$ non-carriers; $\epsilon 4^+$ ApoE $\epsilon 4$

carriers

	НО	aMCI	<i>p</i> <	aMCI ε4 ⁻	aMCI ε4 ⁺	Р
Age (years)	66.5 ± 4.9	70.2 ± 6.8	0.08	68.6 ± 7.1	71.8 ± 6.2	0.2
Gender (F/M)	15/11	10/19	0.09	3/12	7/7	0.09
Education (years)	8.6 ± 4.3	8.2 ± 5.4	0.8	7.7 ± 5.2	8.8 ± 5.7	0.6
CDR (sum of boxes)	0	0.5	N/A	0.5	0.5	N/A
MMSE	28.3 ± 1.3	26.8 ± 2.6	0.01*	27.5 ± 2.6	26.0 ± 2.5	0.1
Immediate recall	14.2 ± 3.1	9.2 ± 2.9	10^{-6}	10.3 ± 2.7	8.0 ± 2.7	0.03*
Delayed recall	13.2 ± 2.9	5.6 ± 3.7	10^{-10} *	6.8 ± 3.9	4.3 ± 3.2	0.07
TMT						
TMT-A (s)	49.7 ± 27	53.4 ± 33	0.7	50.1 ± 21	55.2 ± 30	0.7
TMT-B (s)	109 ± 46	125 ± 51.5	0.5	120 ± 11	129 ± 29	0.6
VOSP						
Screening	20	19.9 ± 0.2	0.9	19.6 ± 0.1	19.8 ± 0.4	0.9
Incomplete letters	19.4 ± 0.6	19.3 ± 0.9	0.9	19 ± 0.5	19.6 ± 0.6	0.7
Silhouettes	19.4 ± 0.6	17.5 ± 4.6	0.4	18.5 ± 1.3	19.5 ± 3.8	0.5
Object decision	15.5 ± 2.6	13.8 ± 6	0.5	14.8 ± 2.1	15.8 ± 2.5	0.3
Progress. silhouettes	11.71 ± 2.4	10.3 ± 8.1	0.8	10.9 ± 3.1	9.7 ± 2.8	0.4
Dot counting	9.9 ± 0.7	9.9 ± 0.2	0.9	9.7 ± 0.1	9.8 ± 0.1	0.8
Posit. discrimination	19.7 ± 1.8	18.6 ± 2	0.6	18.9 ± 0.5	18.3 ± 0.8	0.8
Number location	8.69 ± 1.6	8.3 ± 1.6	0.8	8.1 ± 2.1	8.5 ± 0.9	0.6
Cube analysis	8.6 ± 1.9	7.2 ± 2.7	0.2	7.6 ± 1.8	6.9 ± 2.3	0.4

Table 2 $A\beta$ and serum lipid levels

P exact *p* value. Significant *P* values were marked with an asterisk. N/A (not applicable)

Biological markers	НО	aMCI	Р
$A\beta_{1-40}$ (pg/ml)	60.5 ± 5.4	80.6 ± 6.1	0.01*
$A\beta_{1-42}$ (pg/ml)	3.8 ± 0.3	5.9 ± 0.5	0.001*
$A\beta_{1-42}/A\beta_{1-40}$	0.08 ± 0.01	0.07 ± 0.006	0.7
Total cholesterol (mg/dL)	202.3 ± 7.4	210.1 ± 7.5	0.5
LDL cholesterol (mg/dL)	112.3 ± 5.9	112.5 ± 5.7	0.9
HDL cholesterol (mg/dL)	49 ± 2.6	46.9 ± 2.4	0.9
Triglycerides (mg/dL)	121.9 ± 8.5	123 ± 8.2	0.9
ApoB (mg/dL)	110.3 ± 4.1	126 ± 7.8	0.050*

Results are expressed as mean \pm standard error of the mean

 $A\beta$ amyloid-beta, *LDL* low-density lipoprotein, *HDL* high-density lipoprotein, *ApoB* Apolipoprotein B

P exact p value of post hoc analysis, after significant MANCOVA. Significant P values were marked with an asterisk

did not show significant differences either in plasma $A\beta$ or serum lipid levels.

Group differences in resting-state alpha-phase coupling

Figure 1 illustrates differences in alpha-phase coupling between HO and aMCI subjects (left column), and between aMCI ApoE4 carriers and non-carriers (right column). The



Fig. 1 Group differences in alpha-phase coupling between HO and aMCI subjects (*left column*), and between aMCI ApoE4 carriers and non-carriers (*right column*). L left hemisphere; R right hemisphere

 Table 3 Group differences in GM and glucose consumption of EEGalpha generators

EEG-alpha source	CS	x	у	z	T_{49}	Р
GM (HO > aMCI)						
R thalamus	1,603	21	-16	-5	5.20	0.001
L thalamus	471	-23	-22	-5	5.31	0.001
FDG-PET (HO > al	MCI)					
R precuneus	4,321	9	-61	40	6.31	10^{-4}
L thalamus	154	-14	-16	3	4.27	0.02
R precuneus	45	-17	-45	67	4.24	0.02
L precuneus	24	-2	-39	34	4.42	0.01

GM grey matter, *FDG-PET* glucose consumption, *CS* cluster size (in mm³). *L* left, *R* right. Coordinates (x-y-z) are in the MNI152 brain anatomical space. *T* values (degrees of freedom in the subscript)

P exact *p* value corresponding to group comparison (FWE corrected, age and gender as covariates)

aMCI group showed decreased levels of neural synchrony (p < 0.05, FWE corrected) in 41 of 780 PLIs (5.25 %), no significant results were found in the opposite direction (i.e., aMCI > HO). More than half (51.2 %) of the above significant differences affected functional coupling between left and right hemispheres, whereas 29.2 and 19.5 % of significant differences were restricted to the left and right hemispheres, respectively (Fig. 1, left column). Significant group differences in neural-phase coupling mainly affected relationships between right parietal and left temporo-parietal regions, as well as functional connectivity within the right parietal lobe and between right parietal lobe, mainly from the right hemisphere, was the cortical region that accounted for most of the resting-state connectivity failures showed by aMCI subjects.

aMCI ApoE4 carriers also presented a significant reduction of neural-phase coupling in 16 of 780 PLIs (2 %) compared to aMCI ApoE4 non-carriers. As illustrated in Fig. 1 (right column), reduced connectivity in aMCI ApoE4 carriers mainly affected communication between regions of the frontal lobe, and regions of the right frontal and parieto-occipital cortex.

Group differences in GM and glucose consumption of cerebral sources of EEG-alpha rhythm

Table 3 summarizes group differences in GM and glucose consumption (FDG-PET) of cerebral sources involved in the generation of the alpha rhythm (p < 0.05, FWE corrected). Figure 2 displays these changes (top panel: GM; bottom panel: FDG-PET) on a volume rendering of cerebral MRI. Briefly, aMCI subjects showed volume reductions of the thalamus, those in the right hemisphere being more accentuated. We further found significant hypometabolism in bilateral regions of the precuneus, and the left



Fig. 2 Group differences in GM and glucose consumption of cerebral regions involved in the generation of alpha rhythms (p < 0.05; controlled for FWE). *Upper panel*: GM changes restricted to bilateral regions of the thalamus. *Bottom panel*: FDG-PET changes restricted to bilateral regions of the precuneus and left thalamus. *A* anterior, *P* posterior, *L* left; *R* right

thalamus. No significant differences in GM or glucose consumption were found when comparing aMCI ApoE4 carriers with non-carriers.

Relationship between changes in GM/glucose consumption of EEG-alpha sources and neural-phase coupling

We further investigated whether changes in resting-state alpha connectivity patterns were related to variations in GM/glucose consumption of EEG-alpha sources in HO and aMCI subjects, separately. These analyses revealed positive correlations between GM of the right thalamus and inter-hemispheric coupling of fronto-occipital regions restricted only in HO subjects (p < 0.02). Between-group

Electrode pair	EEG-alpha generator	CS	x	у	z	r	Р
GM							
$lF-rO HO^+ > aMCI^-$	R thalamus	18	26	-16	9	0.29	0.04
FDG-PET							
$rP-rP HO^+ > aMCI^-$	R precuneus	873	-5	-67	42	0.43	0.004
$lT-rP HO^+ > aMCI^-$	R precuneus	622	6	-49	25	0.39	0.01
$rP-rP HO^+ > aMCI^-$	R precuneus	208	0	-61	36	0.37	0.02

Table 4 Group differences in correlations between GM and FDG-PET changes in EEG-alpha sources and levels of alpha-phase coupling

GM grey matter, *FDG-PET* glucose consumption, *CS* cluster size (in mm³). *l/L* left, *r/R* right. *F* frontal, *P* parietal, *T* temporal, *O* occipital. Coordinates (x-y-z) are in the MNI152 brain space

 $^{+/-}$ Denotes the direction of correlations within each group, although only correlations for HO subjects reached significance. r Pearson correlation coefficient

P exact p value corresponding to between-group regression analyses (FWE-corrected, age and gender as covariates)



Fig. 3 Relationship between GM/glucose consumption of EEG-alpha cerebral sources and patterns of alpha-phase coupling (p < 0.05; controlled for FWE). a Cortico-cortical oscillatory coupling involved in significant correlations with GM and FDG-PET changes.

regression slopes also differed significantly (p < 0.04). Additionally, we found positive correlations between glucose consumption of right parietal lobe and alpha coupling of right parietal regions in HO subjects (0.02).Analysis yielded significant differences when comparedregression slopes of the two groups (<math>0.004).Further information on group differences in regressionslopes for correlations between neuroimaging changes andneuroelectric cortical coupling are shown in Table 4 andillustrated in Fig. 3. **b** Anatomical location of significant correlations. Correlations with GM are represented in *blue*, whereas correlations with FDG-PET are displayed in *red*. *L* left hemisphere, *R* right hemisphere

No significant relationship between GM/glucose consumption and cortical alpha-phase coupling was found either in aMCI ApoE4 carriers or in non-carriers.

Relationship between changes in A β -lipid levels and alpha-phase coupling

We examined whether changes in cortical connectivity patterns underlying alpha rhythms were associated with peripheral $A\beta$ -lipid levels in each group, separately.



Fig. 4 Relationship between Aβ-lipid levels and alpha-phase coupling in HO (*left panel*) and aMCI subjects (*right panel*). Each significant biological marker was displayed in different color. *Plus/minus* denotes the direction of significant correlations in each group. $A\beta_{1-42}$ amyloid-beta isoform 42, *TCh* total cholesterol, *LDL* low-density lipoprotein, *HDL* high-density lipoprotein. *L* left, *R* right

Results showed that decreased levels of $A\beta_{1-42}$ (r = -0.64, p < 0.001), TCh (r = -0.54, p < 0.005) and LDL (r = -0.57, p < 0.003; r = -0.47, p < 0.01) accompanied enhanced inter-hemispheric functional connectivity in HO subjects, although group differences in regression slopes did not reach significance between the two groups. In aMCI subjects, significant correlations were restricted to positive correlations between HDL levels and alpha-phase coupling (r values ranged from 0.41 to 0.47, p values ranged from 0.02 to 0.01) mostly involving the left hemisphere. Comparison of regression slopes revealed significant higher correlations in aMCI than in HO subjects (p < 0.01). Figure 4 illustrates significant relationships between A\beta-serum lipid levels and resting-state alpha connectivity patterns in HO (all negative correlations) and aMCI subjects (all positive correlations).

Relationship between $A\beta$ -lipid levels and GM/glucose consumption of EEG-alpha cerebral sources

Finally, we assessed whether A β and lipid levels were related to structural/functional changes in cerebral regions involved in the generation of the alpha rhythm. Regression analyses revealed a significant relationship between increased levels of triglycerides and decreased GM of precuneus only in aMCI (*r* values ranged from 0.5 to 0.57, *p* values ranged from 0.01 to 0.001). The analysis also yielded significant differences between the regression slopes of the two groups (Table 5; Fig. 5). No significant relationship was found between peripheral blood markers (A β or lipids) and glucose consumption either in HO or aMCI subjects. Neither did we find significant associations between A β -lipid levels and neuroimaging changes in either aMCI ApoE4 carriers or in non-carriers.

Discussion

In the present study, we have investigated whether changes in EEG-connectivity patterns underlying resting-state are accompanied by macroscopic changes (GM and glucose consumption) in cerebral sources of the alpha rhythm, as well as by changes in peripheral $A\beta$ and lipid levels in HO and aMCI subjects. Results revealed that individuals with aMCI showed hypometabolism in the precuneus, GM atrophy in the thalamus, and enhanced levels of $A\beta$ and ApoB. Contrary to the expected, most of these markers were significantly associated with the strength of neuralphase coupling observed in HO subjects, but not with impaired cortical synchronization proper of aMCI subjects, suggesting that synaptic destabilization associated with incipient neurodegeneration might lead to aberrant structural-functional relationships of alpha EEG sources.

Table 5 Group differences in correlations between triglycerides levels and FDG-PET changes in EEG-alpha sources

	EEG-alpha source	CS	x	у	z	r	Р
FDG-PET							
$\rm HO^{+} > aMCI^{-}$	R precuneus	669	14	-75	49	0.6	2×10^{-5}
$\rm HO^{+} > aMCI^{-}$	L precuneus	332	-9	-76	54	0.5	0.002
$\rm HO^+ > aMCI^-$	L precuneus	90	-17	-40	63	0.43	0.01

FDG-PET glucose consumption, CS cluster size (in mm³), L left, R right. Coordinates (x-y-z) are in the MNI152 brain anatomical space

 $+^{/-}$ Denotes the direction of correlations within each group, although only correlations for HO subjects reached significance. r Pearson correlation coefficient

P exact p value corresponding to between-group regression analyses (FWE-corrected, age and gender as covariates)



Fig. 5 Relationship between increased levels of triglycerides and decreased GM of precuneus in aMCI subjects (p < 0.05; controlled for FWE). *Plus/minus* denotes the direction of significant correlations in each group. *Upper panel*: anatomical location of significant correlations, restricted to bilateral regions of the precuneus. *Bottom panel*: *scatter plot* displaying relationships between GM loss of the right precuneus (*Z*-scored volume of the voxel reached maximum significance) and increased levels of triglycerides. Note that this relationship only reached significance in the aMCI group. *A* anterior, *L* left, *R* right

Interestingly, aMCI subjects showed a positive relationship between levels of HDL cholesterol and the strength of neural-phase coupling, leading to the hypothesis that high concentrations of HDL might have enhanced neuroprotector effects in aMCI. Together, these results provide the first evidence of cerebral and biological correlates of changes in neural oscillatory coupling in two different trajectories of aging.

Failures in resting-state cerebral networks reveal the unbalance between structure and function in aMCI

Synapse dysfunction, the major neurobiological correlate of cognitive impairment in AD (DeKosky and Scheff 1990; Terry et al. 1991), has shown to precede tangle formation and neuronal loss in MCI subjects (Masliah et al. 2001; Scheff et al. 2006). Most of the synaptic degeneration in neocortex affects large pyramidal neurons of layers III and V, largely connected through cortico-cortical association fibers (Terry et al. 1981; Rogers and Morrison 1985; Hof et al. 1990). Consequently, and given that oscillatory EEG activity results from summated excitatory and inhibitory postsynaptic potentials primarily generated by synaptic activity of large pyramidal neurons in the cerebral cortex (Lopes da Silva and Van Rotterdam 1993), synaptic dysfunction occurring in aMCI subjects may be reflected in abnormal patterns of EEG coupling. Accordingly, restingstate EEG alpha rhythms not only are significantly different in aMCI when compared with HO subjects (Babiloni et al. 2006a; Cantero et al. 2009a), but they are also able to predict progressive cognitive deterioration (Babiloni et al. 2014) and stability of MCI status over time (Babiloni et al. 2011). However, up to now only a few studies have established a link between abnormalities of EEG rhythms and cortical atrophy in aMCI subjects (Babiloni et al. 2006b, 2013). The present study gives a step further in evaluating the link between failures in resting-state largescale synchronization mechanisms and the anatomo-functional integrity of cerebral sources involved in the generation of alpha rhythms.

We showed structural and functional changes of the thalamus and precuneus in aMCI subjects, two regions considered canonical neuroelectric sources of EEG alpha rhythms (Cantero et al. 2009a, b). Accumulated evidence supports a complex relationship between the thalamus and neocortex during generation of alpha oscillations. For instance, increased glucose consumption of the thalamus is paralleled by increased amplitude of alpha oscillations over parieto-occipital regions (Goldman et al. 2002; Schreckenberger et al. 2004; Feige et al. 2005; De Munck et al. 2007). Furthermore, cortical and thalamic regions are highly coherent during generation of alpha waves (Lopes da Silva et al. 1973). Therefore, bilateral GM loss of thalamus characterizing our aMCI sample might account for impaired alpha connectivity between anterior and posterior regions of the brain, likely due to synaptic dysfunction or synaptic loss of thalamocortical neurons. This hypothesis is supported by studies showing amyloid deposits and neurofibrillary tangles in the thalamus of AD patients (Rudelli et al. 1984; Masliah et al. 1989; Braak and Braak 1991) together with significant GM loss (Karas et al. 2004) that further correlated with impaired cognitive functioning (de Jong et al. 2008), and by studies showing altered patterns of functional connectivity between thalamus and precuneus in aMCI subjects (Cantero et al. 2009a; Wang et al. 2012; Zhou et al. 2013).

The precuneus is a region of the superior parietal lobe also involved in EEG-alpha generation (Toth et al. 2007; Michels et al. 2008; Cantero et al. 2009a). An emerging body of evidence suggests that this area is extremely vulnerable to the accumulation of A β plaques during the progression of AD (Rowe et al. 2007; Driscoll et al. 2012), which might account for disrupted connectivity with other brain regions in amyloid-positive MCI subjects (Drzezga et al. 2011), as well as for cognitive decline in preclinical AD patients (Nickl-Jockschat et al. 2012; Yotter et al. 2013).

Contrary to our initial hypothesis, neither GM loss in the thalamus nor hypometabolism in the precuneus were correlated with the strength of alpha phase synchrony in aMCI subjects. This relationship only emerged in HO adults. Aging-related changes in synaptic loss likely accounted for coherent relationships between structure and function in normal aging, whereas synaptic dysfunctions in aMCI might lead to the lack of significant associations between damage of cerebral sources of alpha rhythm and failures in EEG alpha coupling.

Relationship between peripheral blood markers and patterns of resting-state cortical connectivity in HO and aMCI

Searching for reliable peripheral blood markers of incipient neurodegeneration is increasingly important, given the invasive nature, potential side effects, and problematic follow-up analysis based on CSF sample collections. However, results derived from cross-sectional studies using plasma Aβ in MCI patients are largely inconsistent (Sobów et al. 2005; Blasko et al. 2008; Storace et al. 2010; Pesini et al. 2012), likely due to the instability of A β peptides in plasma (Humpel 2011), the state of aggregation (Storace et al. 2010), and the heterogeneity of MCI populations across studies. In agreement with our results, only those studies that specifically included MCI of an amnestic type have found higher plasma levels of $A\beta_{1-42}$ compared to HO subjects (Storace et al. 2010; Sobów et al. 2005; Pesini et al. 2012). Although increased levels of plasma $A\beta_{1-42}$ observed in aMCI subjects might be signalling a central pathogenic process of AD, e.g., deregulation of β -APP metabolism followed by brain $A\beta$ accumulation, this hypothesis still requires experimental confirmation.

Interestingly, we found that elevated levels of $A\beta_{1-42}$ correlated with decreased parieto-occipital functional connectivity in HO, but not in aMCI subjects. This result suggests that plasma levels of $A\beta_{1-42}$ is a better marker of normal aging-related changes in alpha cortical networks than of aMCI-related changes, and, in turn, might be tentatively proposed as a surrogate marker of aging-related decline in cortical function. An alternative explanation for this result is that cognitively normal elderly with elevated concentrations of $A\beta_{1-42}$ might present a faster cognitive decline rate over time. This hypothesis is supported by

studies showing that an increased AB plaque burden. assessed with [(11)C]Pittsburgh compound B (PiB), is significantly associated with worsening of different cognitive domains (Wirth et al. 2013) and with cortical thinning in clinically normal elderly (Becker et al. 2011). Recent studies have also found significant associations between subjective cognitive complaints and PiB uptake in HO adults (Amariglio et al. 2012), mostly affecting medial prefrontal cortex, cingulate cortex, and precuneus (Perrotin et al. 2012). Subjective cognitive complaints might be related to increased plasma levels of $A\beta_{1-42}$ in HO subjects, accounting for failures in parieto-occipital functional connectivity observed in our study. Given that the presence of subjective cognitive complaints was not specifically assessed in HO subjects of our study, further investigation needs to be performed to clarify this hypothesis. Furthermore, the sample used in this study was relatively small and lacked in vivo markers of AD pathology (i.e., CSF Aβtau and/or amyloid-PET), impeding confirmation of preclinical AD in our aMCI sample. Therefore, further longitudinal research combining plasma AB and other biomarkers in non-demented older adults and preclinical AD, confirmed by CSF Aβ and/or amyloid-PET markers, is clearly needed to determine whether plasma AB has diagnostic value in combination with other biomarkers.

Lipid markers correlate with resting-state cortical connectivity patterns in HO and aMCI

Considerable evidence supports a pathogenic link between the deregulation of cholesterol homeostasis and AD (Roher et al. 1999; Wood et al. 1999). Early findings have shown that elevated cholesterol levels are an early risk factor for developing AD (Pappolla et al. 2003), sustaining the hypothesis that cholesterol plays a role in promoting amyloidogenesis (Bodovitz and Klein 1996; Simons et al. 1998; Refolo et al. 2000; Grösgen et al. 2010). However, our study is the first in assessing associations between serum lipid levels and oscillatory cortical connectivity in HO and aMCI subjects, and in establishing a link between these markers and macroscopic changes in cerebral regions involved in the generation of the human resting-state alpha rhythm.

We have shown that ApoB levels, the best estimate of circulating lipoproteins with atherogenic potential (Barter et al. 2006), were significantly elevated in aMCI subjects, confirming early findings reported in AD patients (Caramelli et al. 1999). Evidence has shown that high ApoB (Motta et al. 2009) and high LDL cholesterol levels (Lamarche et al. 1996) predict atherogenic alterations. Accordingly, cardiovascular risk factors have been found as predictive markers of faster conversion to AD through different pathophysiological mechanisms derived from

vascular pathology (Tabet et al. 2009; Peters and Beckett 2009). Although triglyceride levels did not differ in our study, their increase was associated with bilateral GM loss in precuneus of aMCI subjects. Evidence has shown significant associations between triglycerides and elevated peripheral A β levels in murine AD models (Burgess et al. 2006), although molecular mechanisms underlying this relationship remain to be fully defined.

Promoting successful cognitive aging is a topic of major importance to the field of public health. Different patterns of cognitive aging have been identified in the last two decades, and there is growing need to better understand what influences these trajectories. For instance, factors that impact cholesterol metabolism, such as dietary intake or physical activity, play an important role in late-life cognitive function and the risk of dementia. In our study, the strength of oscillatory cortical connectivity patterns (mostly in the left hemisphere) of aMCI subjects benefitted from increased levels of HDL, whereas inter-hemispheric connectivity loss in HO was associated with increased levels of total and LDL cholesterol. These results reveal, for the first time, that serum lipid levels in normal and pathological aging relate differently to resting-state functional networks and to macroscopic changes in cerebral sources of alpha rhythms. The relationship between altered lipid metabolism and cognitive function in aging and AD is likely indirect, due to the lack of positive effects of statins on cognitive performance in normal aging (Benito-Leon et al. 2010; Richardson et al. 2013) or their inability to prevent AD (Ancelin et al. 2012; Swiger et al. 2013). In summary, our findings provide a novel framework for establishing cerebral correlates of lipid levels in healthy aging and in older adults with aMCI. Major effort aimed at identifying modifiable cardiovascular risk factors will definitively promote successful cognitive aging and will lead to novel strategies to prevent dementia in the near future.

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