ORIGINAL ARTICLE



# **Anodal transcranial direct current stimulation over the primary motor cortex does not enhance the learning benefts of selfcontrolled feedback schedules**

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**Abstract** A distinct learning advantage has been shown when participants control their knowledge of results (KR) scheduling during practice compared to when the same KR schedule is imposed on the learner without choice (i.e., yoked schedules). Although the learning advantages of selfcontrolled KR schedules are well-documented, the brain regions contributing to these advantages remain unknown. Identifying key brain regions would not only advance our theoretical understanding of the mechanisms underlying self-controlled learning advantages, but would also highlight regions that could be targeted in more applied settings to boost the already benefcial efects of self-controlled KR schedules. Here, we investigated whether applying anodal transcranial direct current stimulation (tDCS) to the primary motor cortex (M1) would enhance the typically found benefts of learning a novel motor skill with a self-controlled KR schedule. Participants practiced a spatiotemporal task in one of four groups using a factorial combination of KR schedule (self-controlled vs. yoked) and tDCS (anodal vs. sham). Testing occurred on two consecutive days with spatial and temporal accuracy measured on both days and learning was assessed using 24-h retention and transfer tests without KR. All groups improved their performance in practice and a signifcant efect for

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practicing with a self-controlled KR schedule compared to a yoked schedule was found for temporal accuracy in transfer, but a similar advantage was not evident in retention. There were no signifcant diferences as a function of KR schedule or tDCS for spatial accuracy in retention or transfer. The lack of a signifcant tDCS efect suggests that M1 may not strongly contribute to self-controlled KR learning advantages; however, caution is advised with this interpretation as typical self-controlled learning benefts were not strongly replicated in the present experiment.

# **Introduction**

Knowledge of results (KR) refers to information provided to the learner following a motor response that indicates how successful the learner's outcome was relative to the task goal (Schmidt, & Lee [2011\)](#page-10-0). Although there are numerous ways to efectively schedule KR for motor skill learning (for a review see Magill, & Anderson [2013\)](#page-9-0), one technique that has shown distinct learning advantages is self-controlled KR schedules (for a review see Sanli, Patterson, Bray, & Lee, [2013](#page-10-1)). With this scheduling technique, one group of participants is given choice over their KR schedule during practice (i.e., self-controlled group), while another group is matched to a self-controlled participant and replicates the respective KR schedule without any choice (i.e., yoked group). Thus, both the frequency and timing of KR provision is identical between the selfcontrolled and yoked groups, while only the provision or withholding of choice over feedback schedule difers. This learning advantage of self-controlled KR over yoked KR is a robust fnding in the motor learning literature and it has been shown with discrete (e.g., Carter, Carlsen, & Ste-Marie, [2014\)](#page-8-0), serial (e.g., Patterson, & Carter [2010](#page-9-1)),

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as well as continuous (e.g., Huet, Camachon, Fernandez, Jacobs, & Montagne, [2009](#page-8-1)) motor skills.

The effectiveness of self-controlled practice conditions for motor learning are typically accounted for using a motivational infuences or an information-processing explanation (for a review see Sanli et al. [2013\)](#page-10-1). According to a motivational infuence, when learners are given the freedom to exercise choice during practice, this choice is intrinsically rewarding, autonomy-supportive, protects perceptions of competency, and increases self-efficacy; all which enhance intrinsic motivation and motor learning (Chiviacowsky [2014](#page-8-2); Chiviacowsky, Wulf, & Lewthwaite, [2012](#page-8-3); Lewthwaite, & Wulf [2012](#page-9-2)). However, there are many fndings in the extant self-controlled practice literature that are particularly difficult to reconcile from this motivational perspective (e.g., Carter et al. [2014;](#page-8-0) Carter, & Patterson [2012](#page-8-4); Carter, & Ste-Marie [2016](#page-8-5); Chiviacowsky, Wulf, de Medeiros, Kaefer, & Wally, [2008,](#page-8-6) [2012](#page-8-3); Chiviacowsky, & Wulf [2005;](#page-8-7) Fischman [2015](#page-8-8); Hansen, Pfeifer, & Patterson, [2011](#page-8-9); Patterson, Carter, & Sanli, [2011](#page-9-3); Patterson, & Lee [2008;](#page-9-4) Sanli, & Lee [2013](#page-9-5); Ste-Marie, Vertes, Law, & Rymal, [2013](#page-10-2)), and it has been shown that both intrinsic motivation and self-efficacy cannot account for the learning advantages of self-controlled feedback schedules compared to yoked schedules using causal modelling techniques (Ste-Marie, Carter, Law, Vertes, & Smith, [2015](#page-10-3)). In contrast, it has been proposed that the learning advantages associated with self-controlled practice conditions arise due to participants in the self-controlled group engaging in more effective and/or effortful information-processing activities during practice, which are not similarly engaged when practicing in a yoked group (Bund, & Wiemeyer [2004;](#page-7-0) Carter et al. [2014](#page-8-0); Janelle, Kim, & Singer, [1995;](#page-8-10) Janelle, Barba, Frehlich, Tennant, & Cauraugh, [1997](#page-8-11); Patterson et al. [2011](#page-9-3); Patterson, & Lee [2010\)](#page-9-6). Post, Fairbrother, and Barros [\(2011](#page-9-7)), for example, found that participants in the self-controlled group took signifcantly longer to initiate each trial (i.e., preparation time) than their yoked counterparts, which was interpreted as an indicator of more effortful processing activities under self-controlled relative to yoked practice conditions. This increase in response preparation time also suggests that these diferences in information-processing activities between self-controlled and yoked groups can be localized to non-movement periods between trials. In KR research, three important non-movement intervals can be defned in relation to the temporal placement of the KR presentation. These are the KR-delay interval, the post-KR interval, and the intertrial interval. The KR-delay interval represents the time between the end of a motor response and the presentation of KR for that trial (Swinnen [1988](#page-10-4)), whereas the post-KR interval refers to the period between the receipt of KR and the start of the next practice trial (Magill [1988\)](#page-9-8). Together, the KR-delay and the post-KR intervals make up the intertrial interval (Schmidt, & Lee [2011](#page-10-0)). Recent self-controlled KR research has revealed that the KR-delay (Carter, & Ste-Marie [2016\)](#page-8-5) and the post-KR (Grand et al. [2015](#page-8-12)) intervals are both critical time periods for the learning advantages associated with self-controlled KR schedules.

Carter and Ste-Marie [\(2016](#page-8-5)) demonstrated that the typical learning benefts of self-controlled KR schedules could be eliminated when the KR-delay interval was interposed with a number-solving task. As the KR-delay interval begins when a motor response ends, it is considered the period when participants engage in error detection processes (Sherwood [2010](#page-10-5); Swinnen [1988,](#page-10-4) [1996\)](#page-10-6) by comparing the actual and predicted sensory consequences of the motor response (Schmidt [1975;](#page-10-7) Wolpert, Diedrichsen, & Flanagan, [2011\)](#page-10-8). Carter and Ste-Marie concluded that these error detection processes were disrupted in the self-controlled group that engaged in the secondary number-solving task, and as a result, could not be used as the basis for the KR decision. In other words, because a reliable error signal between predicted and actual sensory consequences could not be generated, these participants were unable to selfschedule their limited KR requests in a way that maximized the informational value of the KR received (see Hansen et al. [2011](#page-8-9) for a similar discussion).

The importance of the post-KR interval for self-controlled KR learning advantages was revealed by Grand et al. ([2015\)](#page-8-12) who investigated feedback processing with event-related potentials (ERPs) time-locked to the receipt of KR. In particular, Grand et al. were interested in the feedback-related negativity (FRN) component of the ERPs waveform, which is a negative defection that peaks approximately 150–300 ms after feedback presentation (Luft [2014](#page-9-9)). The results indicated that the amplitude of the FRN component was signifcantly larger in the self-controlled group compared to the yoked group, which suggested that the self-controlled group was engaged in increased processing of the KR during the post-KR interval. Taken together, the work of Carter and Ste-Marie ([2016\)](#page-8-5) and Grand et al. [\(2015](#page-8-12)) make it reasonable to conclude that the efectiveness of self-controlled KR schedules is dependent on the information-processing activities engaged during the KR-delay and post-KR intervals.

The importance of processing activities during the KRdelay and post-KR intervals for motor learning is further underscored with data from experiments employing disruptive transcranial magnetic stimulation (TMS) protocols (e.g., Hadipour-Niktarash, Lee, Desmond, & Shadmehr, [2007;](#page-8-13) Lin, Fisher, Winstein, Wu, & Gordon, [2008](#page-9-10); Lin, Fisher, Wu, Ko, Lee, & Winstein, [2009;](#page-9-11) Lin, Winstein, Fisher, & Wu, [2010\)](#page-9-12). For example, applying disruptive single-pulse TMS over the primary motor cortex (M1) immediately upon movement completion during the KR-delay interval impaired retention of a visuomotor skill compared to when M1 was stimulated 700 ms after the end of a movement (Hadipour-Niktarash et al. [2007](#page-8-13)). Critically, this impaired retention (i.e., faster "washout") was not due to diferences in the acquisition of the visuomotor transformation as both TMS groups showed normal rates of adaptation. Hadipour-Niktarash et al. concluded that neural processing in M1 associated with movement error detection during the early portion of the KR-delay interval has a strong contribution to the retention of motor memories. Further support that the M1 is an important neural correlate of error-based information-processing activities during non-movement periods have been reported in a series of experiments by Lin et al. [\(2008](#page-9-10), [2009](#page-9-11), [2010\)](#page-9-12). In contrast to Hadipour-Niktarash et al., Lin et al. administered disruptive single-pulse TMS during the post-KR interval and found that the retention of three diferent spatiotemporal arm patterns was signifcantly reduced. Collectively, the results of Hadipour-Niktarash et al. and Lin et al. highlight that the retention of motor memories can be attributed to errorrelated processing in M1 that occurs immediately after a motor response (i.e., during the KR-delay interval) and following the provision of KR for a just completed motor response (i.e., during the post-KR interval).

Although the learning advantages of self-controlled KR schedules are well-documented, an outstanding question is what brain regions contribute to these benefcial processing activities. Based on the reviewed self-controlled research identifying the KR-delay and post-KR intervals as vital periods for self-controlled KR learning benefts (Carter, & Ste-Marie [2016](#page-8-5); Grand et al. [2015\)](#page-8-12) and the data revealing that neural processing in M1 during these nonmovement periods is essential for the retention of motor memories (Hadipour-Niktarash et al. [2007;](#page-8-13) Lin et al. [2008,](#page-9-10) [2009](#page-9-11), [2010\)](#page-9-12), it is reasonable to suggest that M1 may be a key neural correlate for self-controlled KR learning advantages. The purpose of the present experiment was to investigate whether combining a self-controlled KR schedule with anodal transcranial direct current stimulation (tDCS) applied over the M1 would have an additive beneft on motor learning. tDCS consists of passing a weak electrical current (e.g., 0.5–2 mA) between scalp-mounted electrodes that can infuence cortical excitability in a polarity-dependent manner (see Filmer, Dux, & Mattingley, [2014;](#page-8-14) Nitsche et al. [2008](#page-9-13) for respective reviews). Anodal stimulation has been shown to increase excitability, whereas cathodal stimulation can decrease excitability (Nitsche, & Paulus [2000,](#page-9-14) [2001](#page-9-15)). Depending on the duration of stimulation, these changes in excitability can outlast the actual stimulation period. Anodal-tDCS has been shown to enhance motor performance and learning on an isometric pinch force task (Marquez, Zhang, Swinnen, Meesen, & Wenderoth, [2013](#page-9-16); Reis et al. [2009](#page-9-17)), during sequence learning (Cuypers et al.

[2013](#page-8-15); Kantak, Mummidisetty, & Stinear, [2012](#page-8-16)), and on hand dexterity tests (Christova, Rafolt, & Gallasch, [2015](#page-8-17); Fregni et al. [2006](#page-8-18)). Although TMS in its repetitive application (rTMS) can produce similar efects (e.g., Baraduc, Lang, Rothwell, & Wolpert, [2004;](#page-7-1) Reis et al. [2008;](#page-9-18) Richardson et al. [2006\)](#page-9-19), tDCS is easier to administer and the required equipment is more portable and costs signifcantly less; thus, there is increased interest in the use of tDCS in clinical and rehabilitation contexts (Schulz, Gerlof, & Hummel,[2013\)](#page-10-9). Additionally, the application of tDCS does not produce similar physiological artifacts as those resulting from TMS (e.g., muscle twitches, clicking noise) and tDCS can also be administered while a person is physically performing a motor task (i.e., online) without unwanted interference. This is an advantage of tDCS considering there is evidence to suggest that anodal-tDCS applied over M1 is more efective for learning when it is applied concurrently with practice (Sriraman, Oishi, & Madhavan, [2014](#page-10-10); Stagg, Jayaram, Pastor, Kincses, Matthews, & Johansen-Berg, [2011](#page-10-11)).

Based on past tDCS research, we expected enhanced learning for the self-controlled group receiving anodaltDCS compared to the self-controlled group receiving sham-tDCS as measured using delayed retention and transfer tests (Kantak, & Winstein [2012](#page-9-20); Schmidt, & Bjork [1992](#page-10-12)). Independent of tDCS, it was expected that both selfcontrolled KR groups would demonstrate greater learning than their respective yoked groups (for a review see Sanli et al. [2013\)](#page-10-1).

## **Methods**

## **Participants**

Data were collected from 44 healthy individuals (*M*age = 20.73, SD 1.58; M/F=20/24) with no self-reported history of cognitive or motor dysfunction and were recruited from the undergraduate and graduate student population at the University of Ottawa. All participants were right-handed as verifed using the Edinburgh Handedness Inventory (Oldfeld [1971](#page-9-21)) and provided written informed consent.

#### **Task and apparatus**

The task goal was to use extension-fexion movements about the elbow of the non-dominant (left) arm to replicate a criterion waveform as accurately as possible (see Fig. [1\)](#page-3-0). The left arm was placed in a custom manipulandum that allowed measurement of movement about the elbow in the horizontal plane. The motor task consisted of two rapid elbow extension-fexion reversal movements



<span id="page-3-0"></span>**Fig. 1 a** Top-down view of participant setup and the goal waveform that participants had to match by performing two rapid elbow extension-fexion reversals. For tDCS, the anode (*rounded electrode*) was positioned over C4, whereas the cathode (*square electrode*) was placed over the contralateral supraorbital ridge. **b** The *black line* represents the goal waveform and the *gray line* represents a participant's

waveform. Spatial accuracy was quantifed by summing the absolute constant error at each reversal point which are represented by numbers 1 through 3 ( $\sum$ |CE|<sub>Amp</sub>). Temporal accuracy was quantified as the absolute constant error in movement time with respect to the goal time which is represented by number 4 ( $|CE|_{MT}$ )

with specific amplitude and temporal constraints, and an overall movement time goal of 900 ms (during the practice and retention phases). For the transfer test the same waveform trajectory was used, but the overall goal movement time was increased to 1150 ms. Variations of this task have been successfully used by motor learning researchers investigating the efects of non-invasive brain stimulation techniques (i.e., TMS) on motor memory encoding and consolidation processes (e.g., Kantak, Sullivan, Fisher, Knowlton, & Winstein, [2010](#page-8-19); Lin, Fisher, Wu, Ko, Lee, & Winstein, [2009](#page-9-11)).

Participants sat in a chair facing a 22-inch computer monitor with their left forearm resting semiprone in a padded armrest attached to the top of the manipulandum. The starting position required participants to have their elbow bent at approximately 90° in front of their torso with their hand grasping a handle that could be adjusted to ensure the central axis of rotation was collinear with the elbow joint, and vision of the arm and the manipulandum were occluded. A linear potentiometer powered by a 5 V direct current power supply attached to the central axis of the manipulandum provided position data which was sampled at 1000 Hz for the duration of each movement using analog-to-digital hardware (PCIe-6321, National Instruments Inc.). A customized LabVIEW (National Instruments Inc.) program controlled the timing of all experimental stimuli on each trial, and recorded and stored the data for ofine analysis.

#### **Procedure**

Upon arrival to the laboratory, participants completed a non-invasive brain stimulation screening questionnaire (Rossi et al. [2009\)](#page-9-22). The frst 22 participants were randomly assigned to one of the two self-controlled groups, while the last 22 participants were randomly assigned to one of the two yoked groups. This resulted in four experimental groups: self-controlled with anodal-tDCS (hereafter selfanodal), self-controlled with sham tDCS (hereafter selfsham), yoked with anodal-tDCS (hereafter yoked-anodal), and yoked with sham tDCS (hereafter yoked-sham). Sham tDCS groups were included to control for any possible efects due to the presence of the electrodes on the scalp and the initial tingling sensation that is felt during the ramping up phase at the onset of stimulation.

All participants completed 80 practice trials (8 blocks of 10 trials) of the waveform matching task on Day One. For the practice phase, the self-controlled groups were informed that they would have the opportunity to choose whether they wanted to receive KR after a trial, but with the restriction they would only have three KR opportunities per block of ten trials and that all three had to be used (Carter et al. [2014](#page-8-0); Chiviacowsky, & Wulf [2005](#page-8-7)). Once all three requests had been used in a block, the KR decision prompt was no longer displayed after a trial. This ensured all participants practiced with a relative KR frequency of 30%; thus, any learning diferences between groups could not be attributed to receiving diferent amounts of KR. The yoked groups were told that KR would be provided three times in each practice block based on a predetermined schedule.

Each trial began with the goal waveform displayed for 2 s, followed by a visual "Get Ready" and then an auditory "Go" signal (1 s apart). Participants were informed that they could start their movement when ready following the "Go" signal, but that it was not a reaction time task. No visual feedback was provided during the motor responses. For the self-controlled groups, a KR decision prompt (if KR trials remained unused in a block) was displayed 3 s following the end of movement (i.e., KR-delay interval), whereas the yoked groups experienced the same 3 s interval but with a blank screen. On KR trials, KR was displayed for 3 s and consisted of a graphic representation of the participant's displacement trace superimposed on the goal waveform. On no-KR trials, a blank screen was displayed for 3 s. Approximately 24-h after completing the practice phase, participants returned to the laboratory and performed delayed retention and transfer tests (both one block of ten trials) without KR.

# *tDCS protocol*

tDCS (1 mA, current density =  $0.128$  mA/cm<sup>2</sup> at the active electrode) was administered for 18 min using a Dupel iontophoresis constant current delivery device (Empi) connected to a pair of electrodes. Stimulation was administered while participants were performing the task in the practice phase, which lasted approximately 18 min. The active electrode (sponge electrode, 1.5 ml, 7.8 cm<sup>2</sup>; Ionto+) was saline-soaked (0.9% NaCl) to create a conducting medium between the electrode and the scalp. A large reference electrode (carbon foam, 39  $\text{cm}^2$ ; Ionto+) was used as the larger surface area allowed the current density to be sufficiently low such that it would have a negligible efect on underlying cortical areas (Nitsche et al. [2008\)](#page-9-13). The active electrode was centered over electrode site C4 of the International 10–20 EEG system using the procedures outlined by DaSilva and et al. ([2011\)](#page-8-20), wherein 20% of the auricular measurement was calculated and this value (~4 cm) was then measured from Cz through the auricular line. Neuroimaging studies have shown that C3/C4 correspond to the scalp locations directly over left and right M1, respectively (Okamoto et al. [2004](#page-9-23)). This spot has been used successfully in previous experiments to elicit behavioral changes following tDCS applied to the right M1 (e.g., Cogiamanian, Marceglia, Ardolino, Barbieri, & Priori, [2007](#page-8-21); Tecchio et al. [2010\)](#page-10-13). The reference electrode was positioned over the contralateral supraorbital ridge (Reis et al. [2009;](#page-9-17) Reis, & Fritsch [2011](#page-9-24)). Both electrodes were self-adhesive, but additional foam underwrap was used to hold the electrodes

in place, thereby ensuring optimal contact throughout stimulation. For anodal-tDCS groups, the active electrode was the relative positive terminal where positive current fowed into the body and the reference electrode was the relative negative terminal where the positive current then exited the body (DaSilva et al. [2011\)](#page-8-20). For the sham-tDCS groups, the stimulator was only powered on while ramping up to 1 mA  $(-15 s)$  and was then immediately shut off without the participant's awareness. Past research has shown that participants are unable to detect a diference between real and sham stimulation with this procedure (Gandiga, Hummel, & Cohen, [2006](#page-8-22)). All participants tolerated the tDCS very well and no adverse efects were reported.

#### **Dependent measures and statistical analyses**

Given that the goal waveform had specifc spatial and temporal requirements, separate measures for spatial and temporal accuracy were used. Using the procedures of Lin et al. ([2009\)](#page-9-11), temporal accuracy was quantifed using absolute constant error (|CE|) of movement time with respect to the goal time ( $|CE|_{MT}$ ; see Fig. [1\)](#page-3-0) and spatial accuracy was quantifed using the sum of |CE| in movement amplitude for each reversal point in the movement trajectory ( $\Sigma$ ICEI<sub>Amp</sub>; see Fig. [1](#page-3-0)). For the practice phase, mean  $|CE|_{MT}$  and  $\Sigma$ |CE|<sub>Amp</sub> were analyzed using separate 2 (KR schedule: self, yoked)  $\times$  2 (tDCS: anodal, sham)  $\times$  8 (block) mixedmodel analysis of variance (ANOVA) with repeated measures on Block. For the retention and transfer tests, mean  $\Sigma$ |CE|<sub>Amp</sub> and |CE|<sub>MT</sub> were analyzed using separate 2 (KR schedule)  $\times$  2 (tDCS) two-way ANOVAs. Differences with a probability of ≤0.05 were considered signifcant and partial eta squared  $(\eta^2$ <sup>p</sup>) is reported as an estimate of effect size. Post-hoc analyses were performed using Tukey's HSD and in cases where the assumption of sphericity was violated, Greenhouse–Geisser adjusted *P* values are reported.

# **Results**

## **Spatial accuracy**

#### *Practice*

 $\Sigma$ |CE|<sub>Amp</sub> decreased across practice blocks for all groups (Fig. [2\)](#page-5-0), which was supported by a signifcant main efect for Block,  $F(7, 280) = 25.58$ ,  $P < 0.001$ ,  $\eta_p^2 = 0.39$ . There was a trend for an advantage of anodal-tDCS versus sham-tDCS in the expected direction  $(P=0.08)$ ; however, this diference did not reach conventional levels of significance. The tDCS  $\times$  Block interaction,  $F(7, 280) = 4.95$ ,  $P < 0.001$ ,  $\eta^2$ <sub>p</sub> = 0.11, was significant and post-hoc analyses revealed for participants that received anodal-tDCS,



<span id="page-5-0"></span>**Fig. 2** Mean  $\sum$ ICEI<sub>Amp</sub> ( $\pm$ SE) for the practice phase (B1–B8) and the 24-h retention  $(B9)$  and transfer  $(B10)$  tests. Each block consisted of ten trials and KR was only available during Blocks 1 through 8

Block 1 was less accurate than Blocks 4, and 6–8. Similarly, the participants that received sham-tDCS were less accurate in Block 1 compared to Blocks 2–8 and Block 2 compared to Blocks 4–8. Importantly, in Block 1 participants that received sham-tDCS were not signifcantly less accurate than the anodal-tDCS participants. All other main effects and interactions were not statistically significant (*P* values  $> 0.05$ ).

#### *Retention*

There were no signifcant main efects or interactions as all comparisons for mean  $\Sigma$ ICEI<sub>Amp</sub> (Fig. [2](#page-5-0), middle) were not statistically significant (*P* values > 0.05).

#### *Transfer*

Similar to retention, there were no signifcant efects for any factors as all comparisons for transfer (Fig. [2](#page-5-0), right) failed to reach statistical significance ( $P$  values > 0.05).

#### **Temporal accuracy**

#### *Practice*

Mean  $|CE|_{MT}$  decreased across practice blocks for all groups (Fig.  $3$ , left), which was supported by a significant main efect for Block, *F*(7, 280)=17.15, *P*<0.001,  $\eta^2$ <sub>p</sub> = 0.30. Post-hoc analyses revealed that timing error was signifcantly greater in Block 1 compared to Blocks 2–8. All other main effects and interactions were not statistically significant ( $P$  values  $> 0.05$ ).



<span id="page-5-1"></span>**Fig. 3** Mean  $|CE|_{MT}$  ( $\pm SE$ ) for the practice phase (B1–B8) and the 24-h retention (B9) and transfer (B10) tests. Each block consisted of ten trials and KR was only available during Blocks 1 through 8. The *asterisk* (\*) denotes the significant main effect for KR schedule  $(P=0.001)$  where a self-controlled KR schedule (i.e., self-anodal and self-sham groups) resulted in signifcantly less timing error during transfer than a yoked KR schedule (i.e., yoked-anodal and yokedsham groups)

### *Retention*

There were no significant main effects or interactions as all analyses for mean  $|CE|_{MT}$  (Fig. [3](#page-5-1), middle) were not statistically significant ( $P$  values > 0.05).

#### *Transfer*

There was a signifcant main efect of KR schedule, *F*(1,  $(40) = 13.98$ ,  $P = 0.001$ ,  $\eta_{\text{p}}^2 = 0.26$ , whereby the self-controlled KR groups demonstrated less timing error compared to the yoked KR groups (Fig. [3](#page-5-1), right). All other main efects and interactions were not statistically signifcant (*P* values  $>0.05$ ).

#### **Discussion**

Although the efectiveness of self-controlled KR schedules compared to yoked KR schedules is well-documented in the motor learning literature, the brain regions contributing to these learning benefts remain unclear. In the present experiment, we examined whether applying anodal-tDCS over the M1 concurrently with practice would enhance the learning benefts of self-controlled KR schedules. Contrary to this prediction, the results showed that retention and transfer performance for both the self-anodal and the selfsham groups did not difer signifcantly in terms of either spatial or temporal accuracy. We also anticipated that practicing with a self-controlled KR schedule, independent of tDCS, would result in superior learning than practicing with a yoked KR schedule. This prediction was only partially supported as the self-controlled KR groups demonstrated less timing error in transfer, but not for retention, and no significant effect of KR schedule was found for spatial accuracy in either retention or transfer.

The main fnding from the current experiment is that a motor skill transfer advantage was found for participants that were provided the opportunity to self-schedule their KR (i.e., self-anodal and self-sham groups) throughout the practice phase. While we had expected that self-controlled KR learning advantages would have emerged during both retention and transfer, our fnding that the self-controlled KR groups were only signifcantly more accurate in generalizing their learning to a novel task variation than the yoked groups is not unprecedented in the self-controlled literature (e.g., Chiviacowsky, & Wulf [2002](#page-8-23); Fairbrother, Laughlin, & Nguyen, [2012;](#page-8-24) Grand et al. [2015](#page-8-12); Hansen et al. [2011](#page-8-9)). As such, some researchers have suggested that transfer tests may be a more sensitive measure of learning than retention of a previously practiced skill (e.g., Chiviacowsky, & Wulf [2002,](#page-8-23) [2005](#page-8-7)). Others, however, have suggested the transfer-specifc learning advantages of self-controlled practice conditions are the result of self-evaluation processes which strengthen the ability to efectively adapt or scale performance when confronted with novel task requirements (Fairbrother et al. [2012](#page-8-24); Grand et al. [2015](#page-8-12)). Indeed, previous research has provided evidence that suggests practicing with a self-controlled KR schedule increases one's sensitivity to detecting and correcting performance errors compared to yoked schedules (Carter et al. [2014](#page-8-0); Carter, & Patterson [2012](#page-8-4)).

In the current study, a transfer advantage was only noted for timing accuracy and not for spatial accuracy. One possible explanation to account for this unexpected result is that the task variation that was introduced during the transfer phase was a change in the overall movement time goal (from 900 to 1150 ms), while the spatial goals were held constant. In other words, the spatial goals were identical to those experienced during practice and retention and the data revealed no groups diferences at the end of practice or in retention. Based on these data, it is not entirely surprising that the transfer advantage was only seen in the temporal domain, as this was the only parameter for which participants had to scale their performance. In terms of the self-controlled literature, it remains an outstanding issue as to why self-controlled KR learning advantages only emerge in transfer in some experiments, whereas these learning benefts are apparent in both retention and transfer in other experiments.

To our knowledge, this experiment was the frst to incorporate a neurostimulation technique in a self-controlled KR experiment to determine whether M1 contributes to the well-known learning advantages of self-controlled KR schedules. We did not fnd a signifcant efect for tDCS in either retention or transfer, which suggests that M1 may not be strongly implicated in the learning benefts associated with self-controlled KR schedules. Our selection of targeting M1 was based on past research identifying M1 as an important neural correlate of the KR-delay and post-KR intervals for motor learning (Hadipour-Niktarash et al. [2007](#page-8-13); Lin et al. [2008,](#page-9-10) [2009,](#page-9-11) [2010](#page-9-12)), and that informationprocessing activities engaged during these intervals are essential for gaining self-controlled KR learning benefts (Carter, & Ste-Marie [2016](#page-8-5); Grand et al. [2015](#page-8-12)). The lack of a signifcant efect for tDCS is not consistent with past motor learning research where beneficial online (i.e., during practice) and/or ofine (i.e., consolidation) efects of anodal-tDCS applied over M1 concurrently with motor training have been reported (e.g., Christova et al. [2015](#page-8-17); Kantak et al. [2012;](#page-8-16) Nitsche et al. [2003;](#page-9-25) Reis et al. [2009](#page-9-17)). One reason for this inconsistency in fndings may relate to how motor performance and learning were quantifed in the present experiment compared to previous experiments. Specifcally, learning benefts of tDCS have typically been inferred based on pre- and post-tDCS diferences in reaction and/or movement time (Christova et al. [2015](#page-8-17); Kantak et al. [2012\)](#page-8-16). The fact that diferences are found using these two measures is not surprising from a neural activation perspective (Carlsen, Maslovat, & Franks, [2012](#page-7-2); Hanes, & Schall [1996](#page-8-25)) given that anodal-tDCS has been shown to increase cortical excitability (Nitsche, & Paulus [2001](#page-9-15)); thus, the time required to further raise activation over an initiation threshold would be reduced compared to shamtDCS. In contrast, motor learning was evaluated in the present experiment with respect to the memorial quality of matching specifc amplitude goals and an overall timing goal. As such, our fndings suggest that the efectiveness of tDCS for optimizing motor learning may, in part, depend on the measures used to quantify learning.

Additionally, the current density used in the present experiment  $(0.128 \text{ mA/cm}^2)$  was much higher than in most studies using a similar electrode montage (<0.1 mA/ cm<sup>2</sup>), and it is therefore possible that tDCS at this high current density is less efective. Indeed, some researchers have shown a reversal of intended stimulation efects at higher densities (see Batsikadze, Moliadze, Paulus, Kuo, & Nitsche, [2013](#page-7-3)). We, however, argue against the likelihood of these possibilities based on two recent fndings. First, other researchers have successfully used higher current densities  $(>0.12 \text{ mA/cm}^2)$  to elicit behavioral changes (e.g., Carlsen, Eagles, & MacKinnon, [2015](#page-7-4); Carter et al. [2015](#page-8-26), [2016;](#page-8-27) Kantak et al. [2012](#page-8-16)). Second, a recent metaanalysis by Hashemirad et al. [\(2016](#page-8-28)) showed the biggest efect size for a single session of anodal-tDCS was in Kantak et al.'s [\(2012](#page-8-16)) experimentation in which they also used

a small active electrode  $(8 \text{ cm}^2)$  and high current density  $(0.125 \text{ mA/cm}^2)$ . Another possible factor is that with the higher current density it was possible that participants were not adequately blinded to the stimulation (O'Connell et al. [2012](#page-9-26)) and this could have contributed to the lack of a tDCS efect. This seems unlikely, however, given that we used a between-groups rather than within-subjects design (see Russo, Wallace, Fitzgerald, & Cooper, [2013;](#page-9-27) Woods et al. [2016](#page-10-14)), and thus participants only experienced tDCS a single time and were never made aware that they may or may not receive real tDCS. As such, we are confdent that our lack of a tDCS effect is not attributable to either our high current density or an inadequate blinding of participants. However, some potential limitations of our tDCS protocol are that M1 excitability changes were not assessed, and thus we cannot rule out that the stimulation had a smaller than expected effect or those other brain regions were unaffected. Although our stimulation location was determined using procedures used by others (Cogiamanian et al. [2007](#page-8-21); DaSilva et al. [2011;](#page-8-20) Tecchio et al. [2010](#page-10-13)), this location was not confrmed using TMS for example and given our small active electrode it may not have sufficiently covered the movement representation for the motor task.

A fnal consideration relates to the brain region that was targeted in the present experiment. Although past research has shown that M1 is involved in the formation and retention of memory representations of recently acquired motor skills (Hadipour-Niktarash et al. [2007;](#page-8-13) Lin et al. [2008,](#page-9-10) [2009](#page-9-11), [2010;](#page-9-12) Muellbacher et al. [2002\)](#page-9-28), in the context of selfcontrolled KR schedules, M1 may not be a primary brain region contributing to the learning advantages. From a theoretical standpoint, a better understanding of the brain regions involved in these learning advantages would prove useful in characterizing the underlying mechanisms and may also provide an avenue for unifying components of the motivational infuences and information-processing per-spectives (Carter et al. [2014](#page-8-0); Wulf, & Lewthwaite [2016](#page-10-15)). While debate continues between these two perspectives (for a discussion see Sanli et al. [2013\)](#page-10-1), some researchers have highlighted the importance of KR processing and error detection capabilities (Carter et al. [2014](#page-8-0); Carter, & Ste-Marie [2016;](#page-8-5) Fairbrother et al. [2012;](#page-8-24) Grand et al. [2015](#page-8-12)). As such, it may be more appropriate for future studies to target brain areas that are more traditionally associated with the integration of sensory information for response evaluation and/or planning processes, such as the cerebellum (Criscimagna-Hemminger, Bastian, & Shadmehr, [2010](#page-8-29)), the posterior parietal cortex (Della-Maggiore, Malfait, Ostry, & Paus, [2004\)](#page-8-30), and/or the supplementary motor area (Stock, Wascher, & Beste, [2013\)](#page-10-16). For instance, the cerebellum may be a good candidate reason given its theoretical role in motor learning (i.e., internal forward models) (Miall, & Wolpert [1996;](#page-9-29) Wolpert et al. [1998,](#page-10-17) [2011](#page-10-8); Wolpert, & Flanagan [2001](#page-10-18)) and support for this role in error-driven motor learning paradigms (Bastian [2008](#page-7-5); Criscimagna-Hemminger et al. [2010](#page-8-29); McDougle, Ivry, & Taylor, [2016](#page-9-30)).

In conclusion, a signifcant role for M1 in the learning benefts of self-controlled KR schedules was not found in the present experiment using anodal-tDCS. Although continued investigation into uncovering the brain regions is highly encouraged in the self-controlled motor learning literature, it may be more fruitful for these future studies to use more focal forms of non-invasive brain stimulation, such as disruptive TMS protocols (e.g., Hadipour-Niktarash et al. [2007](#page-8-13)) or HD-tDCS (e.g., Kuo et al. [2013\)](#page-9-31). A better understanding of the relevant brain structures and their associated functions would prove valuable for our understanding of why self-controlled KR schedules enhance learning at a theoretical level.

#### **Compliance with ethical standards**

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#### **Confict of interest** None.

**Ethical standards** All participants gave written informed consent prior to inclusion in the studies and the studies were conducted in accordance with the ethical guidelines of the University, and hence with the ethical standards laid down in the 1964 Declaration of Helsinki and its later amendments.

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