



Energetics of sinusoidal exercise below and across critical power and the effects of fatigue

Marta Borrelli¹ · Sheida Shokohyar¹ · Susanna Rampichini¹ · Paolo Bruseghini² · Christian Doria¹ · Eloisa Guglielmina Limonta^{1,3} · Guido Ferretti² · Fabio Esposito^{1,3}

Received: 27 September 2023 / Accepted: 23 December 2023 / Published online: 19 January 2024
© The Author(s) 2024

Abstract

Purpose Previous studies investigating sinusoidal exercise were not devoted to an analysis of its energetics and of the effects of fatigue. We aimed to determine the contribution of aerobic and anaerobic lactic metabolism to the energy balance and investigate the fatigue effects on the cardiorespiratory and metabolic responses to sinusoidal protocols, across and below critical power (CP).

Methods Eight males (26.6 ± 6.2 years; 75.6 ± 8.7 kg; maximum oxygen uptake 52.8 ± 7.9 ml·min⁻¹·kg⁻¹; CP 218 ± 13 W) underwent exhausting sinusoidal cycloergometric exercises, with sinusoid midpoint (MP) at CP (CP_{ex}) and 50 W below CP (CP-50_{ex}). Sinusoid amplitude (AMP) and period were 50 W and 4 min, respectively. MP, AMP, and time-delay (t_D) between mechanical and metabolic signals of expiratory ventilation (\dot{V}_E), oxygen uptake (\dot{V}_{O_2}), and heart rate (f_H) were assessed sinusoid-by-sinusoid. Blood lactate ([La⁻]) and rate of perceived exertion (RPE) were determined at each sinusoid.

Results \dot{V}_{O_2} AMP was 304 ± 11 and 488 ± 36 ml·min⁻¹ in CP_{ex} and CP-50_{ex}, respectively. Asymmetries between rising and declining sinusoid phases occurred in CP_{ex} (36.1 ± 7.7 vs. 41.4 ± 9.7 s for \dot{V}_{O_2} $t_{D\text{ up}}$ and $t_{D\text{ down}}$, respectively; $P < 0.01$), with unchanged $t_{D\text{ s}}$. \dot{V}_{O_2} MP and RPE increased progressively during CP_{ex}. [La⁻] increased by 2.1 mM in CP_{ex} but remained stable during CP-50_{ex}. Anaerobic contribution was larger in CP_{ex} than CP-50_{ex}.

Conclusion The lower aerobic component during CP_{ex} than CP-50_{ex} associated with lactate accumulation explained lower \dot{V}_{O_2} AMP in CP_{ex}. The asymmetries in CP_{ex} suggest progressive decline of muscle phosphocreatine concentration, leading to fatigue, as witnessed by RPE.

Keywords Oxygen uptake · Oxygen debt · Blood lactate · Time delay · Sinusoid amplitude · Heart rate

Abbreviations

AMP Sinusoid amplitude
CP Critical power
CP-50_{ex} Sinusoidal protocol having the MP for power set 50 W below the CP

CP_{ex} Sinusoidal protocol having the MP for power set at the CP
 E_s Sinusoid energy consumption
 $E_{s,Al}$ Alactic oxygen deficit built during a sinusoid
 $E_{s,La}$ Anaerobic lactic metabolism during a sinusoid
 E_{s,O_2} Amount of energy from aerobic sources during a sinusoid
 f_H Heart rate
 f_R Respiratory rate
[La⁻] Blood lactate concentration
MLSS Maximal lactate steady state
MP Sinusoid midpoint
 P_{ACO_2} Alveolar carbon dioxide pressure
RPE_{GEN} Rate of general perceived exertion
RPE_{MUSC} Rate of muscular perceived exertion
RPE_{RESP} Rate of respiratory perceived exertion
T Sinusoid period
 t_D Time delay

Communicated by Michael I Lindinger.

✉ Susanna Rampichini
susanna.rampichini@unimi.it

¹ Department of Biomedical Sciences for Health, Università Degli Studi Di Milano, Via Giuseppe Colombo 71, 20133 Milan, Italy

² Department of Molecular and Translational Medicine, University of Brescia, Brescia, Italy

³ IRCCS Ospedale Galeazzi - Sant'Ambrogio, Via Cristina Belgioioso, 173, 20157 Milan, Italy

| | |
|----------------------|--|
| $t_{D\ down}$ | Time delay at downward midpoint crossing |
| $t_{D\ up}$ | Time delay at upward midpoint crossing |
| \dot{V}_{CO_2} | Pulmonary carbon dioxide output |
| \dot{V}_E | Expiratory ventilation |
| \dot{V}_{O_2} | Pulmonary oxygen uptake |
| $\dot{V}_{O_2\ max}$ | Maximum oxygen uptake |
| V_T | Tidal volume |
| \dot{W} | Mechanical power |
| $\dot{W}_{\ max}$ | Maximal mechanical aerobic power |

Introduction

The history of the energetics of muscular exercise concerns mostly the study of the cardiorespiratory and metabolic responses to square-wave, constant-power submaximal work (di Prampero 1981; Whipp and Ward 1982; Poole and Jones 2012; Ferretti 2015; Ferretti et al. 2022). In a square-wave transition from rest to light or moderate exercise, during which no lactate accumulation occurs, the time constant of the primary component of the bi-exponential pulmonary oxygen uptake (\dot{V}_{O_2}) kinetics (Poole and Jones 2012; Ferretti 2015) corresponds to that of phosphocreatine breakdown (Binzoni et al. 1992; Rossiter et al. 2002). In this type of exercise, the rest-to-exercise transition (on-phase) and exercise-to-rest transition upon exercise cessation (off-phase) show a symmetrical response (Özyener et al. 2001). In contrast, when a square-wave exercise is performed from rest to the heavy exercise domain, respiratory oxygen supply becomes too slow to match the increase in muscle metabolic rate, leading to lactate accumulation during the on-phase (Cerretelli et al. 1979). Due to anaerobic metabolism contribution to energy supply in this transient, asymmetries between the two phases appear, with a longer time constant in the on- than in the off-phase (Paterson and Whipp 1991; Özyener et al. 2001). In this scenario, the appearance of the so-called slow component, accompanied by a continuous increase in blood lactate accumulation, carries along a furtherly accentuated asymmetric pattern between the on- and off-phases of the \dot{V}_{O_2} kinetics (Poole et al. 1994; Jones et al. 2011; Ferretti 2015).

Despite being a convenient experimental model for laboratory studies, square-wave exercise is far away from actual exercise as performed in real life, wherein continuous oscillatory changes in workload occur. To simulate workload oscillations under controlled laboratory conditions, Wigertz (1970) proposed to study exercises in which the mechanical power varied continuously following a sinusoidal function. When we investigate sinusoidal exercise patterns with a sufficiently long sinusoid period (T), we should observe a sinusoidal \dot{V}_{O_2} response, with a time lag with respect to the mechanical sinusoidal pattern equal to the time constant of the primary phase of the \dot{V}_{O_2} kinetics (Casaburi et al. 1977; Girardi et al. 2021a; Ferretti 2023). In

spite of this, the number of studies so far devoted to an analysis of the cardiorespiratory and metabolic responses to sinusoidal exercise has been relatively small (Wigertz 1970; Casaburi et al. 1977; Bakker et al. 1980; Fukuoka and Ikegami 1990; Haouzi et al. 1993; Fukuoka et al. 1997; Nicolò et al. 2018; Girardi et al. 2021b). In particular, only two studies have investigated the \dot{V}_{O_2} response to sinusoid-wave work rates in two different exercise domains, one in healthy humans (Haouzi et al. 1993), the other in patients affected by chronic obstructive pulmonary disease (Porszasz et al. 2013). Some studies analyzed the effects of varying the T on the patterns followed by cardiorespiratory and metabolic variables during sinusoidal work rate in homogeneously aerobic exercise (light-moderate exercise domain) only, either by simulation (Girardi et al. 2021a) or experimentally (Casaburi et al. 1977; Bakker et al. 1980; Fukuoka and Ikegami 1990).

None of these authors attempted to investigate the energy balance of sinusoidal work rate in different exercise intensity domains. Moreover, all of them studied the cardiorespiratory and metabolic response to sinusoidal exercise work rate of relatively short duration only, without any exploration of the possible effects of peripheral fatigue during prolonged exercises under different intensity domains.

Hence, this study aims to: i) provide a comprehensive comparison of the cardiorespiratory and metabolic responses to two different sinusoidal exercises across and below the critical power (CP), taken as the uppermost limit of fully aerobic exercise (Poole et al. 2016); ii) analyze, from the obtained data, the contribution of aerobic metabolism to the energy balance and quantify blood lactate accumulation, across and below CP; and iii) investigate the effects of fatigue on the cardiorespiratory and metabolic responses to these two sinusoidal protocols up to exhaustion. We hypothesized that, at a given T , the sinusoidal exercise across CP may be characterized by a longer time delay between the mechanical and the cardiorespiratory sinusoids (t_{Ds}) compared to that below CP, especially in the up-phase. This difference in t_{Ds} may be associated with asymmetries introduced by lactate accumulation during the exercise transient in the former case. This would imply that the contribution of anaerobic metabolism to the energy balance of sinusoidal exercises of equal work rate sinusoid amplitude (AMP) should be larger across than below CP, due to the important role of anaerobic lactic metabolism. Lastly, during exhausting exercise, we expected a drift of the cardiorespiratory and metabolic responses to sinusoidal exercise across, but not below CP.

Materials and methods

Participants

Twenty participants were enlisted for inclusion in the experiments. Five of them dropped out for personal

reasons, seven were not able to complete the study for different reasons associated with the complexity of the protocol. Therefore, eight physically active male cyclists (age: 26.6 ± 6.2 years; body mass: 75.6 ± 8.7 kg; stature: 1.81 ± 0.04 m; maximum oxygen uptake, $\dot{V}_{O_{2,max}}$: 52.8 ± 7.9 ml·min⁻¹·kg⁻¹; mean \pm standard deviation) completed this protocol. None of them had any upper or lower limb disease nor cardiorespiratory pathologies. After being fully informed on the purpose of the investigation, the experimental design, and procedures, all the participants provided their written informed consent. The study was approved by the ethics committee of the University of Milan (#77/20) and was performed in accordance with the principles of the latest version of the Declaration of Helsinki.

Experimental design

Participants reported to the laboratory eight times, with at least 48-h in between. After a first visit for familiarization and anthropometric measurements, on a second occasion participants underwent incremental exercise testing on the cycle ergometer to determine their $\dot{V}_{O_{2,max}}$ and maximum mechanical aerobic power (\dot{W}_{max}) (Adami et al. 2013). During visits 3–6, they performed exhausting square-wave workloads to determine the CP. In visits 7–8, the volunteers performed randomly two sinusoidal tests of different exercise intensity domains until exhaustion, as detailed below.

Experimental procedures

All the experimental sessions were conducted in a climate-controlled laboratory, with constant temperature of 20 ± 1 °C and relative humidity $50 \pm 5\%$. Tests were performed approximately at the same time of the day to minimize any possible bias induced by circadian rhythms. On the day of the tests, participants were asked to abstain from caffeine and any other similar beverages for at least 12 h and to refrain from intense physical exercise for at least 24 h prior to testing. During the tests, participants were verbally encouraged and strongly motivated by operators to attain their best performance. In all tests, exercise cessation was established when the participant failed to maintain the cadence within the 5 rpm of imposed range for more than 5 s.

Familiarization and anthropometric assessment (visit 1)

In the first session, the participants were equipped with a face mask and wearable devices to familiarize with the equipment for cardiopulmonary testing. Moreover, saddle height, handlebar angle of inclination, and foot position over pedal were adjusted individually and maintained during all the subsequent tests.

Lastly, participant's body mass and stature were, respectively, measured to the nearest 0.1 kg and 1 cm, by a mechanical scale equipped with a stadiometer (Asimed, Samadell; Barcelona).

Incremental exercise test (visit 2)

On the second occasion, the $\dot{V}_{O_{2,max}}$ and its corresponding \dot{W}_{max} were determined through a step-wise incremental test (Adami et al. 2013). After 3 min of baseline recordings and 4 min of warm-up cycling at 100 W, work rate was increased by 25 W every 2 min until exhaustion.

Blood lactate concentration [La^-] was assessed at baseline, at the end of each work rate, and at minute 1, 3, and 5 of recovery. At the same time of blood sample collection, the rate of perceived exertion (RPE) was asked on a general (RPE_{GEN}; Borg 6–20), respiratory, and muscular (RPE_{MUSC} and RPE_{RESP}, respectively; CR-10) standpoints. During all tests, participants were asked to keep the cadence between 90 and 100 rpm, because spontaneously adopted in cyclists to minimize local muscle stress and improve effectiveness of the skeletal-muscle pump in facilitating venous return to the heart (Lucia et al. 2004).

Critical power assessment (visits 3–6)

On different days, to determine CP, four exhausting square-wave tasks at different intensities (90 – 115% \dot{W}_{max}) were administered (Hill 1993; Mattioni Maturana et al. 2018), so that the time-to-exhaustion was in the range between 2 and 20 min (Morton 2006; Vinetti et al. 2019).

Sinusoidal work rate tests (visits 7–8)

After CP assessment, volunteers randomly performed two exhausting sinusoidal tasks at different work rates. The protocols involved 3 min of baseline recordings, followed by a warm-up of 3 min at 50 W and 3 min at CP, after which the sinusoidal exercise began in its downward midpoint crossing toward the nadir. The warm-up at CP was chosen to standardize the starting point of both protocols.

The mechanical power, as a function of time (t), fluctuated in a sinusoidal fashion according to:

$$f(t) = MP + AMP \cdot \sin\left(\frac{2\pi}{T}t\right)$$

where, T is the period of the sinusoid, MP, the sinusoid midpoint, is the value around which the sinusoidal function oscillates, and AMP is the amplitude between MP and either the nadir or the zenith of the sinusoid.

Based on previous study trials, the sinusoidal protocols had the MP for power set at or 50 W below the CP (CP_{ex} and CP-50_{ex}, respectively). In both protocols, AMP and T were 50 W and 4 min, respectively (Fig. 1), so that the overall

power change between nadir and zenith was 100 W. The investigated AMP was selected as absolute power, to make the energy balance assessment possible. The 4-min T was chosen because it is long enough to accommodate the primary component and at the same time long enough to reveal any impacts of a slower component (Haouzi et al. 1993).

[La⁻] and RPE values (RPE_{GEN}, RPE_{MUSC} and RPE_{RESP}, respectively) were determined at baseline, at the end of CP warm-up, at the end of each cycle (corresponding to downward MP crossing), and at minute 1, 3, and 5 of recovery.

Measurements

Tests were performed on an electro-mechanically braked cycle ergometer (mod. 839E, Monark, Sweden). During the experiments, the work rate and cadence were continuously recorded. Expiratory ventilation (\dot{V}_E), \dot{V}_{O_2} , pulmonary carbon dioxide output (\dot{V}_{CO_2}), respiratory rate (f_R), tidal volume (V_T), alveolar carbon dioxide pressure (P_{ACO_2}), and respiratory exchange ratio were measured on a breath-by-breath basis by a metabolic unit consisting of a turbine flowmeter, a zirconium oxygen sensor, and an infrared CO₂ meter (Quark b², Cosmed, Rome, Italy). According to manufacturer's instructions, the turbine and gas analyzers were calibrated before each test by means of a 3-l syringe (mod. 5530, Hans-Rudolph, Shawnee, KS, USA) and a certified gas mixture of known concentration (16% O₂, 5% CO₂, balance N₂), respectively. \dot{V}_{O_2} and \dot{V}_{CO_2} were computed using the Auchincloss algorithm (Auchincloss et al. 1966). Heart rate (f_H) was continuously acquired (S810, Polar Electro Oy, Kempele, Finland). Lastly, 20 μ l arterialized blood samples were taken from the ear lobe and analyzed by an enzymatic-amperometric system (Labtrend, Bio Sensor Technology GmbH, Berlin, Germany) to determine [La⁻].

Data analysis

All the experimental data were analyzed offline. The respiratory and gas exchange responses were edited of spurious breaths that resulted from swallowing, coughing, sighing or premature ending of breath, by deleting values outside three standard deviation (SD) from the local mean (Lamarra et al. 1987).

From the incremental step-wise test, $\dot{V}_{O_2\max}$ was identified from the plateau in the relationship between \dot{V}_{O_2} , selected by averaging the last 30 s of each workload, and mechanical power (\dot{W}). Two subjects did not exhibit a \dot{V}_{O_2} plateau, therefore, the highest value of \dot{V}_{O_2} was considered as $\dot{V}_{O_2\max}$. The \dot{W}_{\max} was determined as the mechanical load corresponding to the intersection between the \dot{V}_{O_2} plateau and the linear relationship between \dot{V}_{O_2} and \dot{W} . The lactate accumulation point was estimated by D_{\max} -modified method (Bishop et al. 1998) as being correlated with maximal lactate steady state (MLSS) indicator (Van Schuylenbergh et al. 2004).

To provide an accurate measure of CP, tests shorter than 2 min were not considered in the analysis (Mattioli Maturana et al. 2018). The hyperbolic power–duration relationship was transformed into a linear formulation (Hill 1993), where the y-intercept of the regression line of \dot{W} vs. the inverse of exhaustion time was retained as CP.

The first 2 min of sinusoidal exercise were excluded from analysis to avoid any distortion in the physiological response induced by the transition of the workload intensity from CP (during the 3 min warm-up phase) to MP (sinusoidal phase). The cardiorespiratory and metabolic response was fitted by the sinewave function that minimized the least squared errors through a custom-built software (Matlab 2019b, MathWorks Inc., Natick, USA). AMP, MP, t_{DS} of all measured variables were calculated for each sinusoid. The average values of these three parameters from all the completed cycles were also determined. Moreover, the net amount of oxygen taken up within a cycle, reflecting the amount of energy derived

Fig. 1 Illustration of the two original sinusoidal work rates: CP_{ex} (red line) and CP-50_{ex} (blue line). CP critical power, MP midpoint, T period (color figure online)

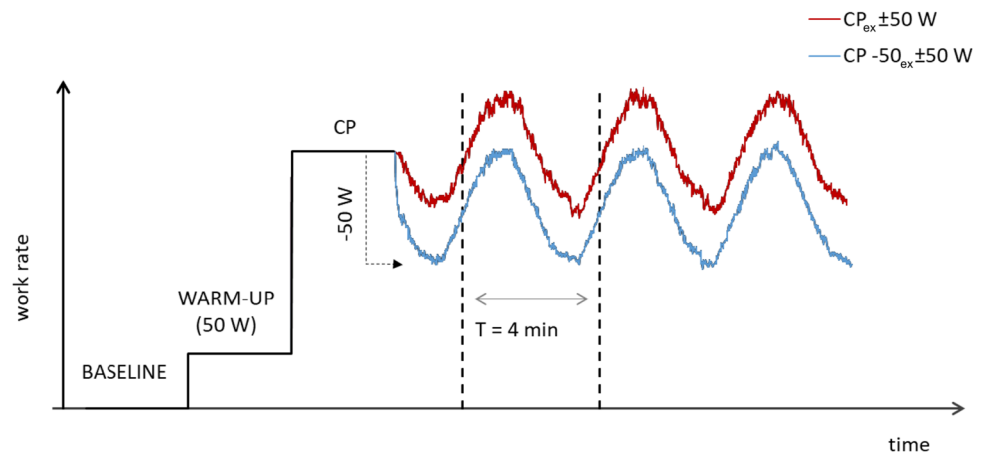
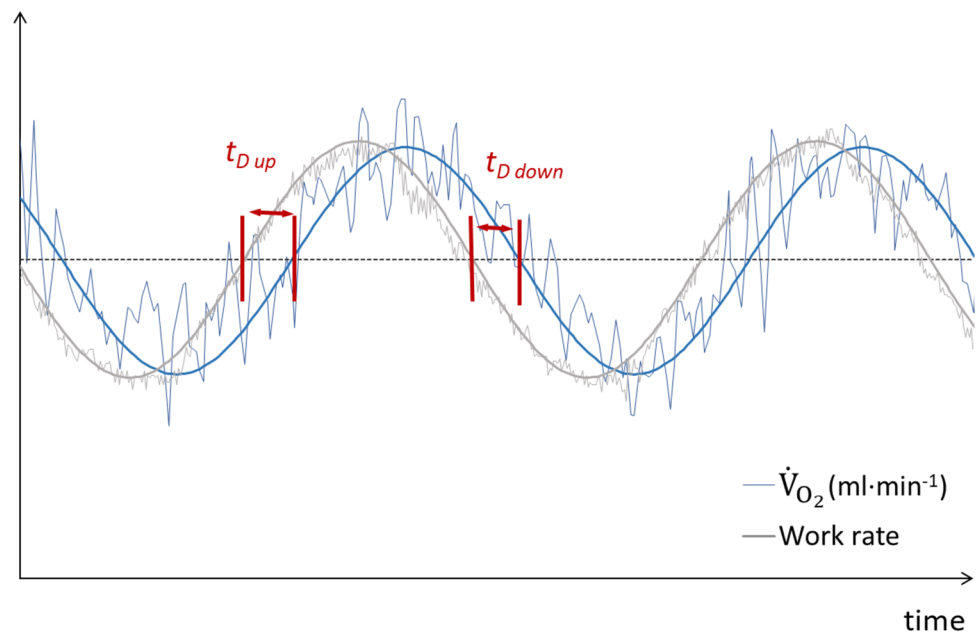


Fig. 2 Raw signals of a representative subject during two cycles of a sinusoidal protocol. Grey line: work rate; blue line: pulmonary oxygen uptake, \dot{V}_{O_2} . $t_{D\ up}$, delay at upward midpoint (MP) crossing; $t_{D\ down}$, delay at downward MP crossing (color figure online)



from aerobic sources only during a sinusoid (E_{s,O_2}), was computed as the time integral of the \dot{V}_{O_2} variation during the cycle itself. This latter was obtained by subtracting the \dot{V}_{O_2} at the nadir of the cycle from the overall \dot{V}_{O_2} of each breath.

t_D was determined as the time shift between the mechanical load and the physiological response. Two different t_D s were determined according to the following hallmarks: i) $t_{D\ up}$: upward MP crossing and ii) $t_{D\ down}$: downward MP crossing (Fukuoka et al. 1997) (Fig. 2). All these parameters were determined on a cycle-by-cycle basis for all the cardiorespiratory and metabolic variables. In addition, the average value of the investigated variables was also computed over all cycles.

Statistical analysis

Descriptive statistics were used to characterize the study sample. The Shapiro–Wilk test was applied to check the normal distribution. A two-way analysis of variance for repeated measures (two-way ANOVA RM) assessed the presence of differences in AMP, MP, and t_D s between the two work rates and among sinusoidal cycles. In the statistical analysis, the minimum number of cycles completed by all subjects, minus one, and the last completed cycle were included. For all pair-wise multiple comparisons, the Bonferroni's correction test was applied. A paired Student's t test determined the differences between average and all-cycle values and between the two sinusoidal protocols of cardiorespiratory and metabolic variables. Paired Student's t test also established the differences between the number of cycles completed during the two sinusoidal exercises and the difference between $t_{D\ up}$ and $t_{D\ down}$. The Hedge's g effect size

with $CI_{95\%}$ was also calculated and interpreted as follows: 0.00–0.19: trivial; 0.20–0.59: small; 0.60–1.19: moderate; 1.20–1.99: large; ≥ 2.00 : very large (Hopkins et al. 2009). All statistical analyses were performed using a statistical software (IBM SPSS Statistics v. 26, Armonk, NY, USA).

Table 1 Main outcomes of step-wise incremental test at peak of exercise

| | |
|--|-------------|
| \dot{W} (W) | 266 ± 16 |
| \dot{V}_{O_2} (ml·min ⁻¹) | 3971 ± 207 |
| \dot{V}_{CO_2} (ml·min ⁻¹) | 4391 ± 202 |
| RER | 1.11 ± 0.01 |
| f_H (beats·min ⁻¹) | 186 ± 2 |
| \dot{V}_E (l·min ⁻¹) | 176 ± 5 |
| f_R (breaths·min ⁻¹) | 48.8 ± 2.6 |
| V_T (l) | 3.19 ± 0.17 |
| [La ⁻] (mM) | 9.3 ± 0.8 |
| RPE _{GEN} (u.a.) | 18.0 ± 0.5 |
| RPE _{MUSC} (a.u.) | 8.6 ± 0.6 |
| RPE _{RESP} (a.u.) | 7.4 ± 0.5 |

Maximal mechanical aerobic power (\dot{W}), pulmonary oxygen uptake (\dot{V}_{O_2}), carbon dioxide production (\dot{V}_{CO_2}), respiratory exchange ratio (RER), heart rate (f_H), expiratory ventilation (\dot{V}_E), respiratory rate (f_R), tidal volume (V_T), blood lactate concentration ([La⁻]), rates of perceived exertion on a general (RPE_{GEN}; Borg 6–20), muscular and respiratory (RPE_{MUSC} and RPE_{RESP}; CR-10). Data are shown as mean ± standard error (SE)

The significance level was set at $\alpha < 0.05$. Unless, otherwise stated, results are presented as mean \pm standard error (SE).

Results

The main results obtained during the step-wise incremental exercise are shown in Table 1. The mean \dot{W} at the lactate accumulation point and at CP were 205 ± 13 and 218 ± 13 W, respectively. The latter was considered to set individually the sinusoidal exercises intensity.

Sinusoidal workloads

The main outcomes related to sinusoidal parameters are shown in Figs. 3, 4, 5, 6, 7. As expected, the number of cycles completed during CP-50_{ex} was higher than that completed during CP_{ex} (13.6 ± 3.9 and 5.5 ± 0.7 , respectively; $P = 0.029$; $g = 0.96$, $CI_{95\%}$: -0.34 to -76.69). The

details about the statistical analysis (the Hedge's g effect size and $CI_{95\%}$) are provided as Supplemental Material. The figures display group-mean responses for the sake of readability. Supplementary Materials include figures depicting also individual data obtained during the experiments.

Midpoint, MP

In CP-50_{ex}, MP of all cardiorespiratory and metabolic variables was lower compared to CP_{ex} in all the cycles and as average ($P < 0.001$). In CP_{ex}, \dot{V}_{O_2} MP of the second and the last cycles was higher compared to the first one ($P = 0.038$; $P = 0.050$, respectively), while in CP-50_{ex}, \dot{V}_{O_2} MP was invariant across the cycles. At both work rates, the \dot{V}_{O_2} MP of the first and the last sinusoid was different from the average of all cycles.

In CP_{ex}, an increment in \dot{V}_E MP was observed already from the second cycle ($P < 0.001$), while in CP-50_{ex},

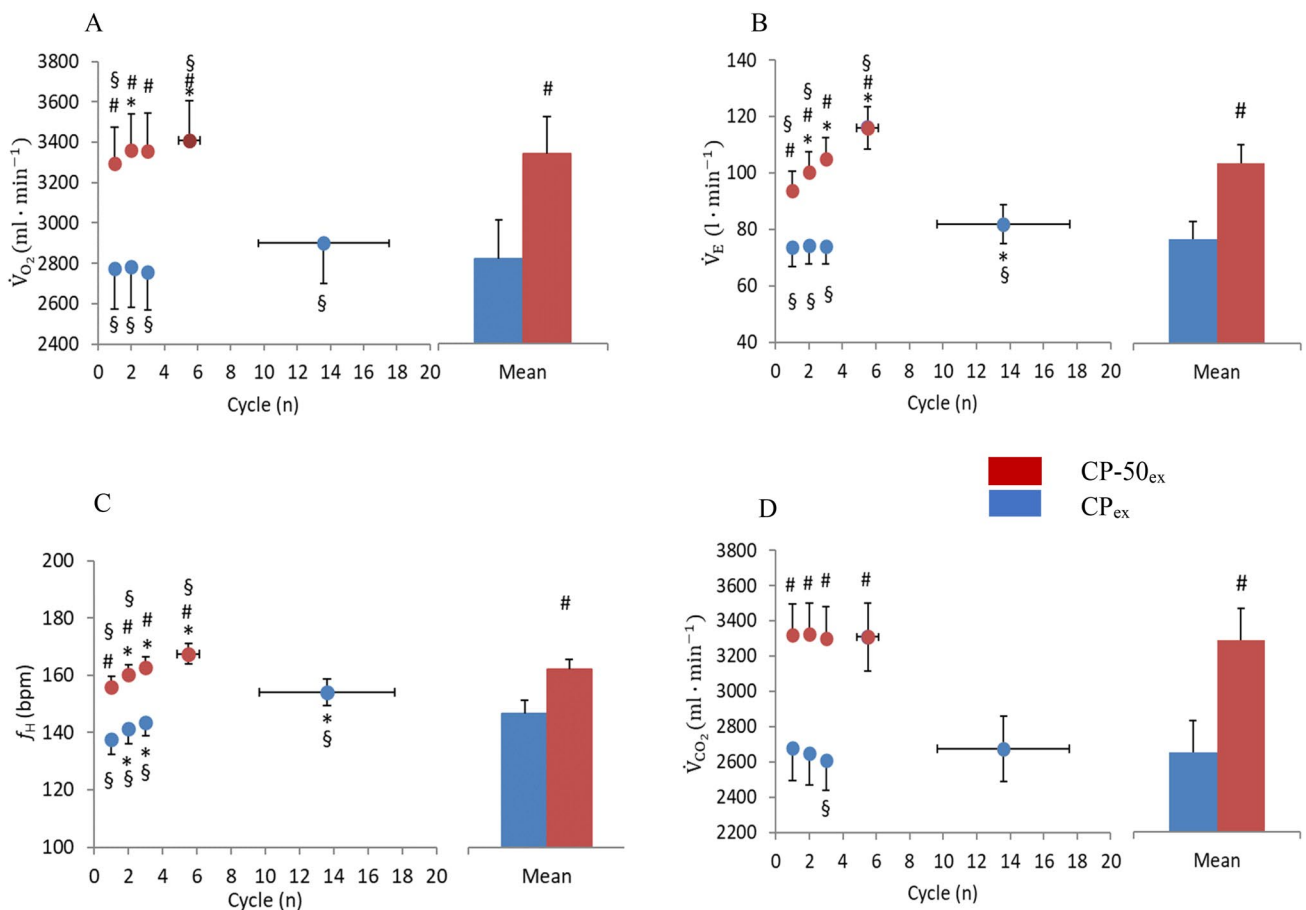


Fig. 3 Midpoint (MP) response of pulmonary oxygen uptake, \dot{V}_{O_2} (panel A), ventilation, \dot{V}_E (panel B), heart rate, f_H (panel C), carbon dioxide production, \dot{V}_{CO_2} (panel D) to each sinewave (Cycle) of CP_{ex} (red circles)

and CP-50_{ex} (blue circles). The column charts represent the average of all cycles during CP_{ex} (red bars) and CP-50_{ex} (blue bars). * $P < 0.05$ vs. Cycle 1; # $P < 0.05$ vs. CP_{ex}; § $P < 0.05$ vs. averaged cycles. Data are shown as mean \pm standard error (SE) (color figure online)

only the \dot{V}_E MP of the last cycle was higher than that of the first cycle ($P = 0.042$). In both protocols, the \dot{V}_E MP of most sinusoids turned out different from the overall average ($P < 0.05$). In both work rates, \dot{V}_{CO_2} MP remained unchanged. For f_H , in contrast, MP progressively increased in both work rates, to become higher than in the first sinusoid from the third sinusoid on ($P < 0.001$). In both protocols, the f_H MP of most sinusoids turned out different from the overall average ($P < 0.05$).

Amplitude, AMP

During CP_{ex}, lower values of \dot{V}_{O_2} AMP were observed than during CP-50_{ex} for both the single sinusoids ($P < 0.01$) and the average value ($P = 0.004$). In both the work rates, the \dot{V}_{O_2} AMP remained stable for the entire duration of the protocols.

Conversely, no differences in \dot{V}_E AMP were observed between CP_{ex} and CP-50_{ex} either in single cycles ($P = 0.92$) or in the average ($P = 0.74$). Coherently, within each protocol, we observed a progressive increase in \dot{V}_E AMP from the first to the last sinusoid (from 11.6 ± 1.1 to 15.3 ± 1.7 l·min⁻¹ in CP-50_{ex}, and from 11.7 ± 1.3 to 16.4 ± 1.5 l·min⁻¹ in CP_{ex}), despite contradictory statistic outcomes ($P = 0.040$ in the former case and $P = 0.46$ in the latter case). Yet, in CP_{ex}, differences were found between the last cycles with respect to the average value ($P = 0.050$).

\dot{V}_{CO_2} AMP reported lower values in CP_{ex} than in CP-50_{ex} for the second, third, and last cycles ($P < 0.05$), as well as for the average value ($P = 0.037$). In both work rates, \dot{V}_{CO_2} AMP remained stable for the entire duration of the protocol. Differences with average value were found in the first and the third sinusoids of CP-50_{ex} ($P = 0.006$ and $P = 0.050$, respectively).

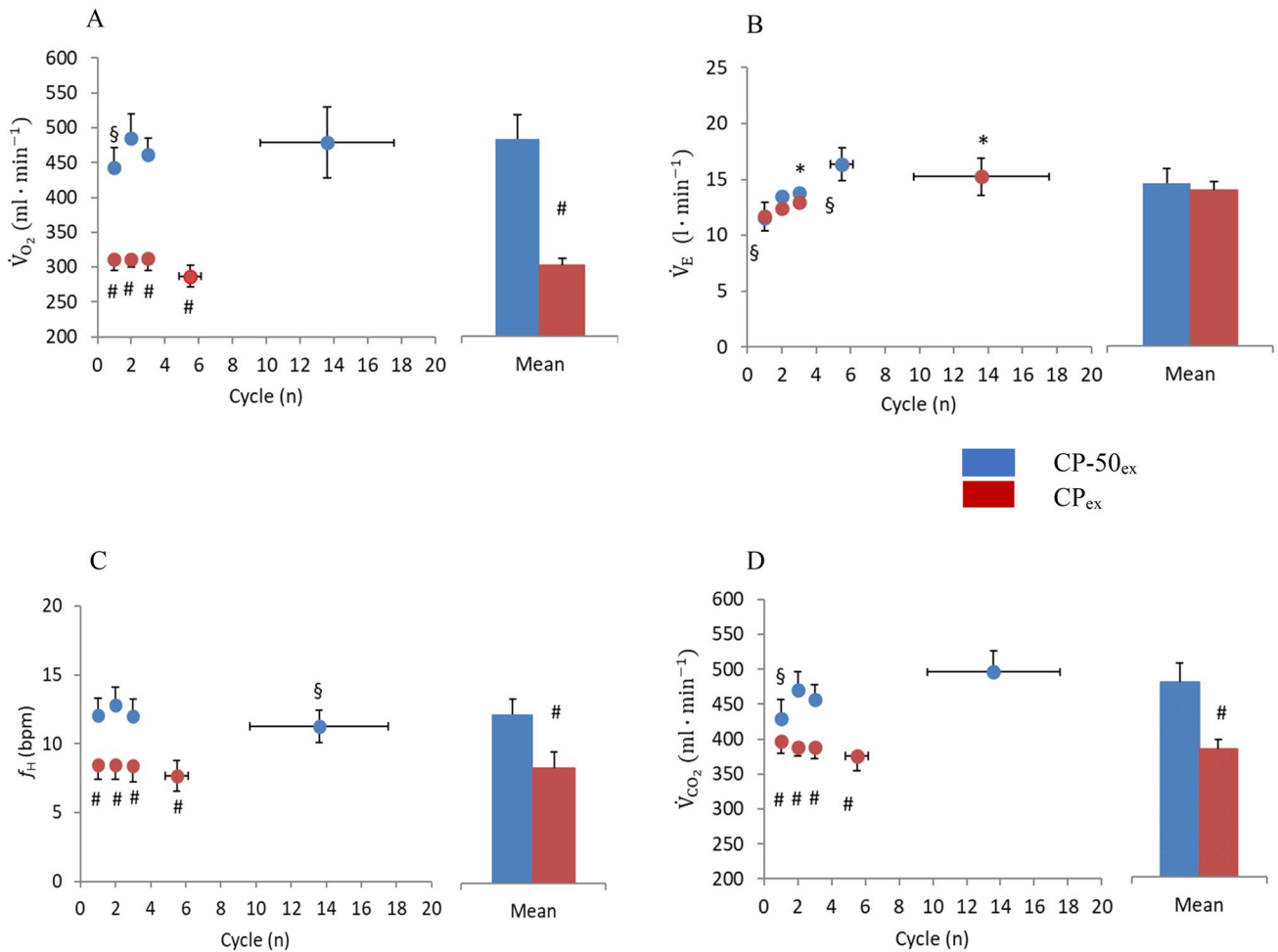


Fig. 4 Amplitude (AMP) response between midpoint and zenith of pulmonary oxygen uptake, \dot{V}_{O_2} (panel a), ventilation, \dot{V}_E (panel b), heart rate, f_H (panel c), carbon dioxide production, \dot{V}_{CO_2} (panel d) to each sinewave (Cycle) of CP_{ex} (red circles) and CP-50_{ex} (blue

circles). The column charts represent the average of all cycles during CP_{ex} (red bars) and CP-50_{ex} (blue bars). * $P < 0.05$ vs. Cycle 1; # $P < 0.05$ vs. CP_{ex}; § $P < 0.05$ vs. averaged cycles. Data are shown as mean \pm standard error (SE) (color figure online)

In comparison with CP-50_{ex}, CP_{ex} was characterized by a lower f_H AMP for all cycles ($P < 0.01$) and for the average ($P = 0.004$). In CP_{ex} and in CP-50_{ex} f_H AMP did not change for the entire duration of the protocol.

Aerobic energy sources, E_{s,O_2}

The E_{s,O_2} resulted equal to 2000 ± 125 and 1658 ± 126 ml, in CP-50_{ex} and CP_{ex}, respectively. Considering that the duration of a cycle was 4 min, this implies that the corresponding mean \dot{V}_{O_2} above the nadir during a cycle was 500 ± 32 and 415 ± 31 ml \cdot min⁻¹. Since the \dot{V}_{O_2} at the nadir was 2261 ± 200 and 2895 ± 185 ml \cdot min⁻¹ in CP-50_{ex} and CP_{ex}, respectively, the mean overall \dot{V}_{O_2} calculated this way (2761 ± 202 and 3310 ± 187 ml \cdot min⁻¹, respectively) did not differ significantly from the determined \dot{V}_{O_2} MP ($P = 0.64$ and 0.83 for CP-50_{ex} and CP_{ex}, respectively).

Time delays, t_D s

In CP_{ex}, \dot{V}_{O_2} $t_{D\ up}$ was longer than in CP-50_{ex} in the first cycle only ($P = 0.016$). A similar tendency appeared for \dot{V}_E $t_{D\ up}$ ($P = 0.059$). As a consequence, no differences between single cycles and average of all cycles appeared for both \dot{V}_{O_2} and \dot{V}_E , except for the last cycles of \dot{V}_E ($P = 0.042$). \dot{V}_{CO_2} $t_{D\ up}$ in CP_{ex} was longer than in CP-50_{ex} in the first cycle only ($P = 0.021$). Similarly, in CP_{ex}, f_H $t_{D\ up}$ was longer than during CP-50_{ex} in the first and in the second sinusoids ($P = 0.002$ and $P = 0.001$, respectively) and in the average ($P = 0.018$).

CP_{ex} was characterized by longer \dot{V}_{O_2} $t_{D\ down}$ compared to CP-50_{ex} in the first three cycles ($P < 0.01$) and the average ($P = 0.009$). Moreover, in CP_{ex}, \dot{V}_{O_2} $t_{D\ down}$ of the first cycle was longer than the average ($P = 0.006$). No differences between protocols and with the average values were

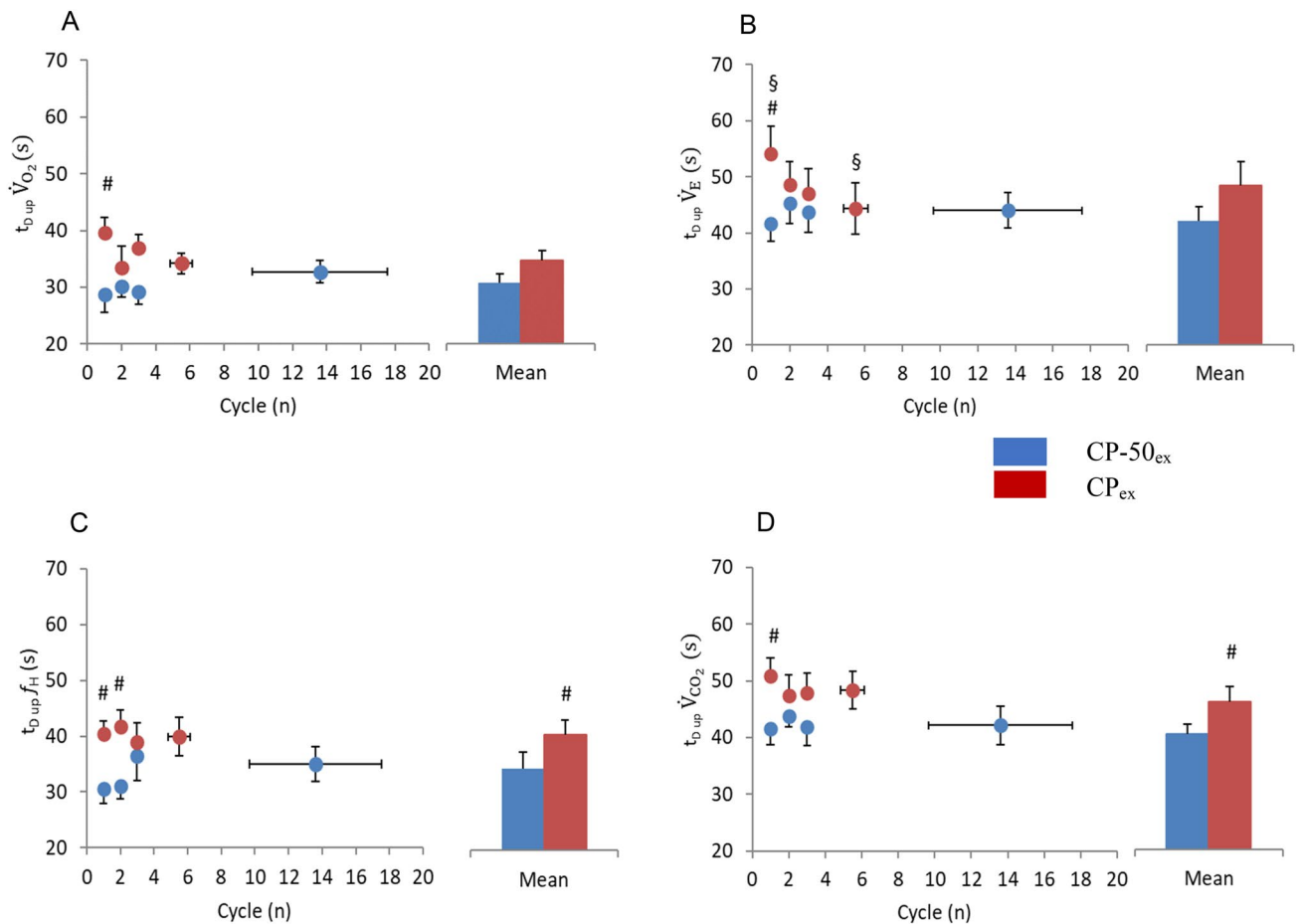


Fig. 5 Time delay upward MP crossing ($t_{D\ up}$) of pulmonary oxygen uptake, \dot{V}_{O_2} (panel A), ventilation, \dot{V}_E (panel B), heart rate, f_H (panel C), carbon dioxide production, \dot{V}_{CO_2} (panel D) to each sinuswave (Cycle) of CP_{ex} (red circles) and CP-50_{ex} (blue circles). The col-

umn charts represent the average of all cycles during CP_{ex} (red bars) and CP-50_{ex} (blue bars). * $P < 0.05$ vs. Cycle 1; # $P < 0.05$ vs. CP_{ex}; § $P < 0.05$ vs. averaged cycles. Data are shown as mean \pm standard error (SE) (color figure online)

observed in $\dot{V}_E t_{D\text{down}}$. In CP_{ex} $\dot{V}_{\text{CO}_2} t_{D\text{down}}$ was longer than in CP-50_{ex} in the first and last cycles ($P = 0.005$ and $P = 0.034$, respectively). Moreover, in CP_{ex} , a higher value of $\dot{V}_{\text{CO}_2} t_{D\text{down}}$ was found in the first cycle compared to the average ($P = 0.020$). Similar patterns were followed by $f_H t_{D\text{down}}$, except for the fact that the differences between the two protocols appeared for all the cycles ($P < 0.05$), and thus for the average ($P = 0.0001$).

In all cardiorespiratory and metabolic $t_{D\text{up}}$ and $t_{D\text{down}}$, no changes were revealed by the within protocol analysis; indeed, in both sinusoidal exercises, they remained unchanged.

Overall, $\dot{V}_{\text{O}_2} t_{D\text{up}}$ was 30.2 ± 6.6 s and $\dot{V}_{\text{O}_2} t_{D\text{down}}$ was 31.2 ± 6.3 s in CP-50_{ex} . This 1 s difference, despite being statistically significant ($P = 0.002$), due to the high number of observations, appears physiologically negligible and reveals remarkable symmetry between the up- and down-phases of the sinusoids. Conversely, in CP_{ex} , $\dot{V}_{\text{O}_2} t_{D\text{up}}$ was

36.1 ± 7.7 s and $t_{D\text{down}}$ was 41.4 ± 9.7 s ($P = 0.00001$). The 5-s difference reveals remarkable asymmetry between the up- and down-phases of the sinusoids. Moreover, $t_{D\text{up}}$ was 5.9 s longer in CP_{ex} than in CP-50_{ex} , although the difference was not significant ($P = 0.112$); nevertheless, $t_{D\text{down}}$ was 10.2 s and significantly ($P = 0.009$) longer in CP_{ex} than in CP-50_{ex} . The same was the case for f_H .

Blood lactate concentration, $[\text{La}^-]$, and rate of perceived exertion, RPE

As shown in Fig. 7, blood lactate concentration ($[\text{La}^-]$) differed between the two protocols in all cycles, being always higher in CP_{ex} ($P < 0.05$) than in CP-50_{ex} . In the former case, $[\text{La}^-]$ progressively increased with time, so that the third and the last cycle differed from the first ($P = 0.022$ and $P = 0.0001$, respectively). Conversely, in CP-50_{ex} , $[\text{La}^-]$ was not different among the cycles, resulting in an average

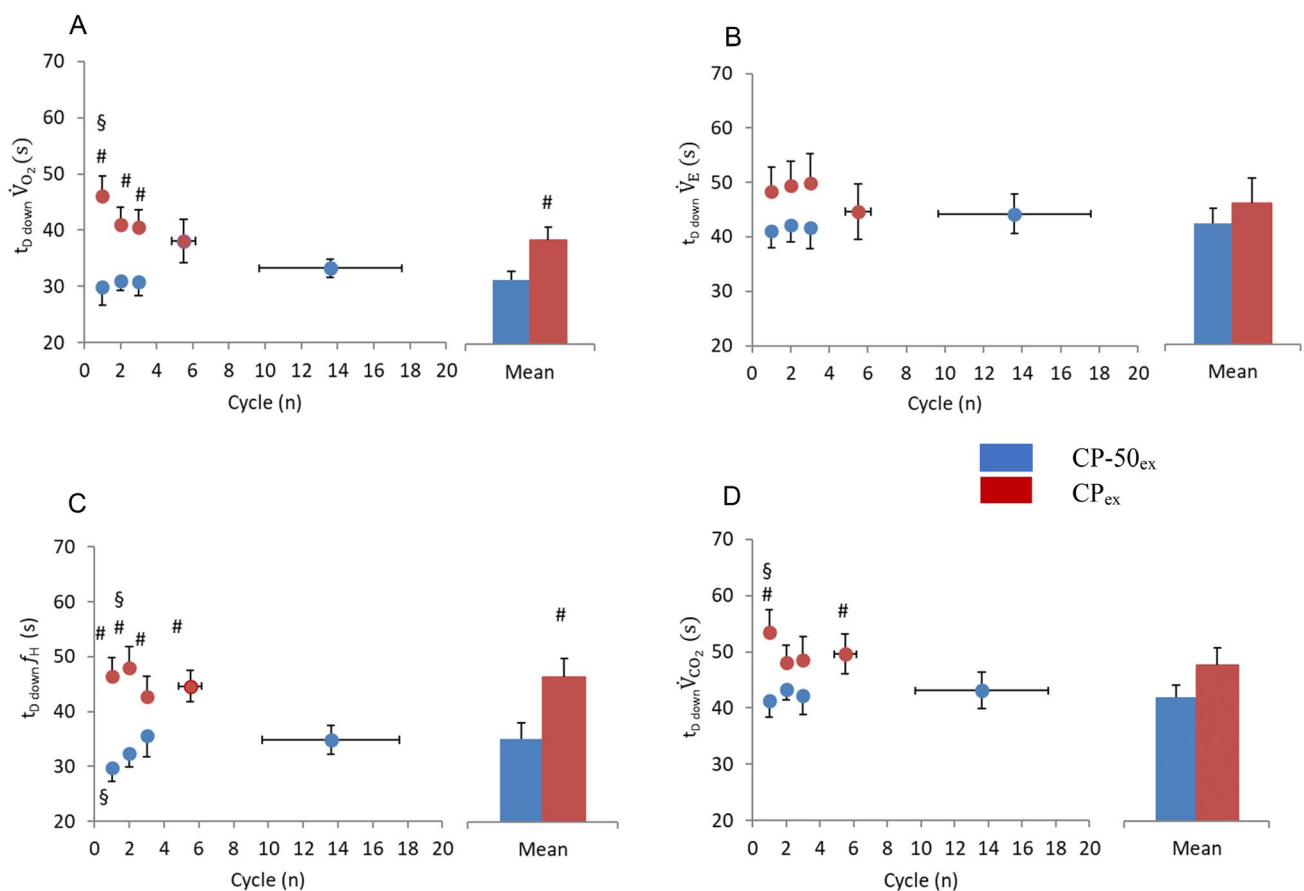


Fig. 6 Time delay downward MP crossing ($t_{D\text{down}}$) of pulmonary oxygen uptake, \dot{V}_{O_2} (panel A), ventilation, \dot{V}_E (panel B), heart rate, f_H (panel C), carbon dioxide production, \dot{V}_{CO_2} (panel D) to each sinuswave (Cycle) of CP_{ex} (red circles) and CP-50_{ex} (blue circles). The

column charts represent the average of all cycles during CP_{ex} (red bars) and CP-50_{ex} (blue bars). * $P < 0.05$ vs. Cycle 1; # $P < 0.05$ vs. CP_{ex} ; § $P < 0.05$ vs. averaged cycles. Data are shown as mean \pm standard error (SE) (color figure online)

of 2.9 ± 0.3 mM. In addition, P_{ACO_2} stayed stable (average: 38.9 ± 3.6 mmHg), independent of the cycle.

In almost all cycles, RPE_{GEN} , RPE_{MUSC} , and RPE_{RESP} were greater in CP_{ex} ($P < 0.05$) than in CP-50_{ex} . In both CP-50_{ex} and CP_{ex} , higher values of RPE_{GEN} (18.3 ± 0.3 and 18.4 ± 0.4 a.u., respectively), RPE_{MUSC} (8.3 ± 0.6 and 9.4 ± 0.4 a.u., respectively), and RPE_{RESP} (5.1 ± 0.4 and 6.6 ± 0.5 a.u., respectively) were registered in the last cycle compared to the first one ($P < 0.001$).

Discussion

This study reports an overall analysis of the energy balance of sinusoidal work rates in two exercise domains, below and across the CP, taken as the upper limit of purely aerobic exercise. The results showed that i) the AMP of the \dot{V}_{O_2} response to sinusoidal work was less than predicted from the corresponding expected difference in steady state \dot{V}_{O_2} , and the more so the higher the power at MP; ii) the sinusoids at CP_{ex} revealed asymmetries between the rising phase and the declining phase of the sinusoid, which was not the case for the sinusoids at CP-50_{ex} ; iii) the appearance of asymmetries is coherent with a greater role of anaerobic lactic metabolism to the energy balance; iv) no significant differences in $t_{\text{D}s}$ were observed between the protocols; v) contrary to CP-50_{ex} , there was a clear tendency toward a positive drift of the \dot{V}_{O_2} response during CP_{ex} , associated with a progressive $[\text{La}^-]$ and RPE increase.

These results are only partially in agreement with the tested hypotheses. In fact, the hypothesized longer $t_{\text{D}s}$ at CP_{ex} than at CP-50_{ex} were observed only in $t_{\text{D down}}$. As hypothesized, the tendency toward a drift in \dot{V}_{O_2} was demonstrated in CP_{ex} only; however, such a drift appeared for \dot{V}_{E} and f_{H} in both protocols. Further, and in agreement

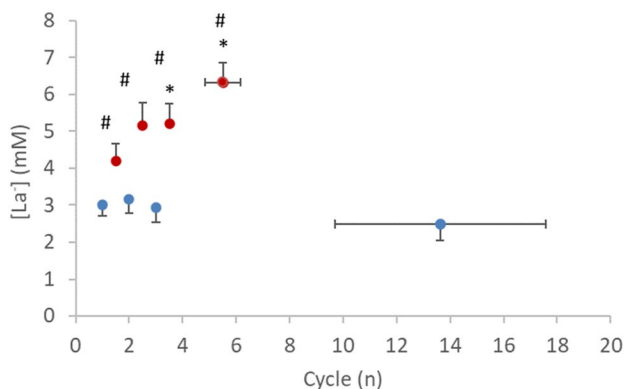


Fig. 7 Blood lactate concentration ($[\text{La}^-]$) to each cycle of CP_{ex} (red circles) and CP-50_{ex} (blue circles). * $P < 0.05$ vs. 1; # $P < 0.05$ vs. CP_{ex} . Data are shown as mean \pm standard error (SE) (color figure online)

with the tested hypothesis, a higher MP, lower AMP, and asymmetry between on- and off-phases of the sinusoids were observed during CP_{ex} with respect to CP-50_{ex} .

\dot{V}_{O_2} MP remained steady for the entire CP-50_{ex} duration, thus suggesting that exercise intensity was sustained primarily by the aerobic metabolism (Poole et al. 2016; Ferretti et al. 2017, 2022). Considering that no differences appeared either in \dot{V}_{CO_2} or in $[\text{La}^-]$ between the initial and the last cycles, the small rise in \dot{V}_{E} MP might be associated with thermoregulatory effects. Indeed, since the rise in body temperature may lead to increased stimulation of central and/or peripheral chemoreceptors by H^+ , and of muscle metaboreceptors (Hayashi et al. 2006), the increase in \dot{V}_{E} may contribute in keeping arterial blood pH and partial pressure of CO_2 unchanged. Nevertheless, the control mechanisms of \dot{V}_{E} during exercise are complex. There is still an open debate about three main mechanisms thought to be involved in the control of breathing during exercise (central command, chemoreceptor stimulation and muscle mechanical and metabolic afferences) (Haouzi 2006; Forster et al. 2012), preventing to attain clear-cut conclusions on this issue.

In CP_{ex} , other factors may have contributed to the increase in \dot{V}_{O_2} , \dot{V}_{E} , and f_{H} MP in addition to the mechanisms discussed here above. Indeed, the growth of the cardiorespiratory and metabolic response could also be an effect of the slow component of \dot{V}_{O_2} , which is known to occur above the CP and which is mainly related to the recruitment of fast-twitch fibers and to a progressive shift toward fatty acid utilization during a long-lasting exercise (Jones et al. 2011; Ferretti 2015; Burnley and Jones 2018). The higher $[\text{La}^-]$ observed in our study in CP_{ex} seems to support this statement.

Contrary to what we hypothesized, although there are differences between $t_{\text{D up}}$ and $t_{\text{D down}}$ in CP_{ex} , revealing asymmetries between up- and down-phase of the sinusoid, no significant differences in $t_{\text{D up}}$ were found between CP_{ex} and CP-50_{ex} (Figs. 5 and 6). When measuring $t_{\text{D up}}$ in CP-50_{ex} , the MP is preceded by 2 min of exercise below the CP level, and therefore the slow component unlikely affects the dynamics of the \dot{V}_{O_2} response, possibly leading to a shorter $t_{\text{D up}}$ in CP-50_{ex} than in CP_{ex} . Since, and likely for this reason, $t_{\text{D down}}$ was 10.2 s and significantly longer in CP_{ex} than in CP-50_{ex} , the lack of a significant differences in $t_{\text{D up}}$ between the two sinusoidal exercise level may appear as a statistical artifact.

In CP-50_{ex} , the entire sinusoid took place below the CP and below the MLSS (Beneke 2003; Jones et al. 2010; Leo et al. 2022; Ferretti et al. 2022). For a power AMP of 50 W, the mean \dot{V}_{O_2} AMP was 488 ± 36 $\text{ml}\cdot\text{min}^{-1}$ (see histogram of Fig. 4). During steady-state exercise on the cycle ergometer at 50 W, carried out at a pedalling frequency of 90–100 rpm (1.5–1.67 Hz), which we used as warm-up exercise, the net \dot{V}_{O_2} was 775 ± 35 $\text{ml}\cdot\text{min}^{-1}$. The

Table 2 Energy balance components

| | CP-50 _{ex} | CP _{ex} |
|--|---------------------|------------------|
| AMP \dot{V}_{O_2} (ml·min ⁻¹) | 488 ± 36 | 304 ± 31 |
| AMP* \dot{V}_{O_2} (ml·min ⁻¹) | 775 ± 35 | 775 ± 35 |
| E_s (ml·O ₂) | 2945 ± 149 | 2870 ± 170 |
| E_{s,O_2} (ml·O ₂) | 2000 ± 125 | 1658 ± 126 |
| $E_s - E_{s,O_2}$ (ml·O ₂) | 945 ± 187 | 1212 ± 246 |
| $E_{s,La}$ (ml·O ₂) | 0 | 392 ± 39 |
| $E_{s,Al}$ (ml·O ₂) | 945 ± 187 | 820 ± 260 |
| Rate of [La ⁻] accumulation in a sine (mM/cycle) | 0 | 1.93 ± 0.20 |

Measured sinusoid amplitude of pulmonary oxygen uptake (AMP \dot{V}_{O_2}), theoretical sinusoid amplitude of pulmonary oxygen uptake (AMP* \dot{V}_{O_2}), sine energy consumption (E_s), the amount of energy derived from aerobic source within the sine (E_{s,O_2}), the alactic oxygen deficit built during a sine ($E_{s,Al}$), anaerobic lactic metabolism ($E_{s,La}$), rate of blood lactate ([La⁻]) accumulation in a sine in CP-50_{ex} and CP_{ex}. Data are shown as mean ± standard error (SE). Note that $E_s - E_{s,O_2} = E_{s,Al} + E_{s,La}$. AMP* \dot{V}_{O_2} was calculated during steady state exercise on the cycle ergometer at 50 W, carried out at a pedalling frequency of 90–100 rpm (1.5–1.67 Hz), which we used as warm-up exercise

corresponding gas exchange ratio at 50 W was 0.83 ± 0.02 and the mechanical efficiency was 0.20 ± 0.01 , which is similar to the prediction made by di Prampero (2000).

The \dot{V}_{O_2} AMP observed in the present study was lower than the measured steady-state \dot{V}_{O_2} at 50 W ($P < 0.001$). This is another consequence of operating within a continuously oscillating exercise transient, as pointed out above, during which an oxygen deficit is built in the rising phase and an oxygen debt is paid in the declining phase of the sinusoid. Recently, Girardi et al. (2021a) conducted a theoretical analysis of the effects of T on \dot{V}_{O_2} AMP. For T equal to 4 min, they predicted \dot{V}_{O_2} AMP of some 70% of the \dot{V}_{O_2} that is necessary to sustain a power corresponding to the mechanical AMP. This prediction is substantially supported by the present results, showing that the \dot{V}_{O_2} AMP was 75% of the expected \dot{V}_{O_2} for an equivalent steady state exercise at 50 W (mechanical AMP in the present study).

[La⁻] did not change from the first sinusoid on, indicating [La⁻] steady state and no further net lactate accumulation at each sinusoid. Therefore, the postulated oxygen deficit would be only alactic. Coherently, the sinusoids appear to be symmetrical, as long as $t_{D\ up}$ was only 1 s lower than $t_{D\ down}$.

In CP_{ex}, the mechanical power MP was set at the CP, so that part of the cycle took place above it. A continuous rise in [La⁻] was found (Fig. 7), indicating a greater oxygen deficit than that incurring during CP-50_{ex}. This is suggested also by the fact that the \dot{V}_{O_2} AMP in CP_{ex} (304 ± 11 ml·min⁻¹) was less than in CP-50_{ex} (Fig. 4), even though T was the same. Since, in absence of [La⁻] accumulation during an

exercise transient, the time constant of the \dot{V}_{O_2} kinetics is invariant, power independent, and equal to that of phosphocreatine breakdown (di Prampero and Margaria 1968; Binzoni et al. 1997), and since the mechanical AMP was the same in CP_{ex} as in CP-50_{ex}, the postulated higher oxygen deficit in the former than in the latter case can only be attributed to its anaerobic lactic component (facultative component of the oxygen deficit due to early lactate accumulation) (di Prampero 1981; Ferretti 2015).

On these premises, to shed light on these energetic issues, we tried to perform an analysis of the energy balance of the sinusoids, along the following lines. An estimate of the mechanical work above the nadir was done by computing the time integral of net power during a sinusoid, after subtracting the power at the nadir. Assuming a mechanical efficiency equal to that reported above, which, however, may carry along a slight overestimate of the actual exercise efficiency in CP_{ex} (Gaesser and Brooks 1975; Whipp and Wasserman 1969; Hesser et al. 1977), the corresponding metabolic energy consumption (sinusoid energy consumption, E_s) was then computed. These values are reported in Table 2. Since we operate along a continuous sinusoidal change of power, implying continuous variations in oxygen deficit, E_s comprises energy deriving from aerobic and anaerobic energy sources. Thus, E_{s,O_2} must be less than E_s . E_{s,O_2} was computed as the time integral of \dot{V}_{O_2} during a sinusoid, after subtracting the \dot{V}_{O_2} at the nadir. E_{s,O_2} is also reported in Table 2.

Let us consider first CP-50_{ex}: the sinusoidal variations in power (50 W above and below the MP) occurred entirely below the CP and the MLSS, and in fact from the first sinusoid on, no changes in [La⁻] and P_{ACO_2} were observed. This means that no contributions from anaerobic lactic metabolism to the oxygen deficit occurred in this condition: thus, the difference between E_s and E_{s,O_2} , corresponding to the overall anaerobic energy contribution, turns equal to the alactic oxygen deficit built during a sinusoid ($E_{s,Al}$). This is also reported in Table 2. Considering that a sinusoid is made by a rising part, in which the oxygen deficit is contracted, and a declining part, in which the oxygen debt is paid, the $E_{s,Al}$ reported in Table 2 is a net oxygen deficit (deficit contraction minus debt payment). Were contraction and payment of the alactic oxygen deficit characterized by the same time constant, $E_{s,Al}$ should turn out nil. However, $E_{s,Al}$ has a positive value, because the oxygen debt payment during recovery has a longer time constant than the oxygen deficit contraction during an on-transient (di Prampero 1981). This state of things would imply a progressive decline of muscle phosphocreatine concentration during CP-50_{ex}, leading to exhaustion in a shorter time than during an equivalent constant-power exercise carried out at MP. This is coherent with progressive increase of RPE_{MUSC}, and thus RPE_{GEN}.

Let us now consider the CP_{ex} condition. In this case, part of the exercise would take place above CP, and thus above the MLSS. Therefore, a continuous increase in $[La^-]$ occurred. Thus, E_{s,O_2} must be less than in $CP-50_{ex}$, by an amount corresponding to the non-obligatory component of the oxygen deficit represented by anaerobic lactic metabolism during a sinusoid ($E_{s,La}$). This can be computed as follows: in CP_{ex} , the calculated net oxygen deficit is equal to $E_{s,AI} + E_{s,La}$, whereas in $CP-50_{ex}$, it is equal to $E_{s,AI}$ only. Since the time constant of the obligatory component of the oxygen deficit is invariant and independent of power, and AMP is the same in both experimental conditions, as already pointed out, $E_{s,La}$ is given by the difference in oxygen deficit between CP_{ex} and $CP-50_{ex}$. $E_{s,La}$ is also shown in Table 2. Assuming, from the first sinusoid on, a linear $[La^-]$ increase during CP_{ex} , we calculated and reported in Table 2 also the estimated rate of $[La^-]$ accumulation during a sinusoid. This allowed an estimate of the energy equivalent of $[La^-]$ accumulation within an average sinusoid, as the ratio between $E_{s,La}$ and the $[La^-]$ accumulation within that sinusoid. This estimated value turned out equal to $2.73 \text{ ml}\cdot\text{mM}^{-1}\cdot\text{kg}^{-1}$, which is inside the range of values generally reported in the literature (see di Prampero 1981; di Prampero and Ferretti 1999; Ferretti 2015). Considering the potential sources of error in these estimates, a remarkable result indeed, even though, due to possibly lower efficiency of exercise in CP_{ex} than in $CP-50_{ex}$, this value may turn out slightly overestimated.

In $CP-50_{ex}$, the MP for mechanical power was $168 \pm 13 \text{ W}$. If the phase I of the \dot{V}_{O_2} response upon exercise start is due to sudden vagal withdrawal (Lador et al. 2006; Fontolliet et al. 2021), one should expect no rapid phase I when the investigated power increase is imposed from the ongoing MP. This being the case, in $CP-50_{ex}$, we may assume that the metabolic response to exercise corresponds to that of a first-order system (Whipp et al. 1982; Haouzi et al. 1993; Ferretti 2023). This assumption has not been tested so far. However, the lack of $[La^-]$ accumulation, apart from early lactate accumulation (Cerretelli et al. 1979), and the stability of P_{ACO_2} demonstrate that the experiments were carried out entirely in the fully aerobic domain (Ferretti et al. 2017, 2022). Moreover, we found a substantial symmetry between the up- and down-phases of the sinusoids. Both these observations are in line with the assumption of a first-order system.

To detect the presence of fatigue, we investigated the cardiorespiratory and metabolic responses to sinusoidal exercises up to exhaustion. To this purpose, we had to apply a cycle-by-cycle analysis of the investigated variables. Previous studies chose to overlap all the cycles performed to strengthen the analysis of the physiological response to sinusoidal exercise (Wigertz 1970; Casaburi et al. 1977; Bakker et al. 1980; Fukuoka and Ikegami 1990; Haouzi

et al. 1993; Fukuoka et al. 1995, 1997; Wells et al. 2007; Nicolò et al. 2018; Girardi et al. 2021b). In those studies, the response to sinusoidal work rate was investigated only in protocols of relatively short duration. However, in the present protocols carried out up to exhaustion, significant differences among successive cycles were found for most of the investigated variables. This undermined the possible use of the overlapping procedure in this study.

The progressive increase in f_H MP, in accordance with Haouzi et al. (1993), during both protocols may be explained by a gradual hyper-activation of the sympathetic branch of the autonomic nervous system (Orizio et al. 1988; Rowell and O'Leary 1990), a rise in body's internal temperature (Rowell and O'Leary 1990; González-Alonso et al. 1997), an increase in blood catecholamine concentration (Orizio et al. 1988; Urhausen et al. 1994), and/or a gradual impairment of hydration status (González-Alonso et al. 1997). This last, together with skin vasodilation, might concur to a venous return reduction and, consequently, to a pre-load decrease that might have driven the progressive rise in f_H MP (Lonsdorfer-Wolf et al. 2003). However, if the stroke volume remains constant during both sinusoidal exercises, which might be the case indeed in the power range used in this study, the hypothesis of a reduction in cardiac pre-load might have to be rejected. The patterns of the stroke volume changes during sinusoidal exercise were not investigated so far, to the best of our knowledge, and should be the object of future studies.

Conclusion

This study represents an attempt at analyzing the energetics of sinusoidal exercise below and across CP and MLSS. A substantial energetic compatibility of the data with current theories of the energetics of muscular exercise appeared. The progressively lower aerobic component during CP_{ex} than during $CP-50_{ex}$ is associated with lactate accumulation in the former condition. This is coherent with the observed greater asymmetries and lower AMP for \dot{V}_{O_2} in the CP_{ex} sinusoids than in the $CP-50_{ex}$ sinusoids. The asymmetries observed in CP_{ex} suggest a progressive decline of muscle phosphocreatine concentration with time, implying the onset of fatigue. This may explain, at least in part, why, in athletic competitions, better performances are obtained when running at constant speed on flat terrain than when running at varying speed on undulating terrain.

Supplementary Information The online version contains supplementary material available at <https://doi.org/10.1007/s00421-023-05410-1>.

Acknowledgements The authors express their gratitude to the participants for their participation in the study. In addition, the authors extend their thanks to Stefano Longo and Emiliano Cè for their assistance with statistical analysis.

Author contributions GF and FE conceived and designed research, MB, SS SR PB, CD, and EL performed experiments, MB, SS, and SR analyzed data, MB, SR, and GF interpreted results of experiments. MB prepared figures. MB drafted manuscript. MB, GF, and FE edited and revised manuscript. All authors approved the final version of the manuscript.

Funding Open access funding provided by Università degli Studi di Milano within the CRUI-CARE Agreement. The present research project was supported by institutional grant provided by the Department of Biomedical Sciences for Health, University of Milan.

Data availability Data generated during and/or analyzed during the current study are available as Supporting Information.

Declarations

Conflict of interest The authors have no relevant financial or non-financial interests to disclose.

Ethical approval This study was performed in line with the principles of the Declaration of Helsinki. Approval was granted by the ethics committee of the University of Milan (#77/20).

Consent to participate Informed consent was obtained from all individual participants included in the study.

Consent to publish Participants signed informed consent regarding publishing their data and photographs.

Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>.

References

- Adami A, Sivieri A, Moia C et al (2013) Effects of step duration in incremental ramp protocols on peak power and maximal oxygen consumption. *Eur J Appl Physiol* 113:2647–2653. <https://doi.org/10.1007/s00421-013-2705-9>
- Auchincloss JH, Gilbert R, Baule GH (1966) Effect of ventilation on oxygen transfer during early exercise. *J Appl Physiol* 21:810–818. <https://doi.org/10.1152/jappl.1966.21.3.810>
- Bakker HK, Struikenkamp RS, De Vries GA (1980) Dynamics of ventilation, heart rate, and gas exchange: Sinusoidal and impulse work loads in man. *J Appl Physiol Respir Environ Exerc Physiol* 48:289–301. <https://doi.org/10.1152/jappl.1980.48.2.289>
- Beneke R (2003) Methodological aspects of maximal lactate steady state—implications for performance testing. *Eur J Appl Physiol* 89:95–99. <https://doi.org/10.1007/s00421-002-0783-1>
- Binzoni T, Ferretti G, Schenker K, Cerretelli P (1992) Phosphocreatine hydrolysis by ³¹P-NMR at the onset of constant-load exercise in humans. *J Appl Physiol* 73:1644–1649. <https://doi.org/10.1152/jappl.1992.73.4.1644>
- Binzoni T, Hiltbrand E, Yano T, Cerretelli P (1997) Step vs. progressive exercise: the kinetics of phosphocreatine hydrolysis in human muscle. *Acta Physiol Scand* 159:209–215. <https://doi.org/10.1046/j.1365-201X.1997.577354000.x>
- Bishop D, Jenkins DG, Howard A (1998) The critical power function is dependent on the duration of the predictive exercise tests chosen. *Int J Sports Med* 19:125–129. <https://doi.org/10.1055/s-2007-971894>
- Burnley M, Jones AM (2018) Power–duration relationship: physiology, fatigue, and the limits of human performance. *Eur J Sport Sci* 18:1–12. <https://doi.org/10.1080/17461391.2016.1249524>
- Casaburi R, Whipp BJ, Wasserman K et al (1977) Ventilatory and gas exchange dynamics in response to sinusoidal work. *J Appl Physiol Respir Environ Exerc Physiol* 42:300–311. <https://doi.org/10.1152/jappl.1977.42.2.300>
- Cerretelli P, Pendergast D, Paganelli WC, Rennie DW (1979) Effects of specific muscle training on VO₂ on-response and early blood lactate. *J Appl Physiol* 47:761–769. <https://doi.org/10.1152/jappl.1979.47.4.761>
- di Prampero PE (1981) Energetics of muscular exercise. *Rev Physiol Biochem Pharmacol* 89:143–222. <https://doi.org/10.1007/bfb0035266>
- di Prampero PE (2000) Cycling on earth, in space, on the Moon. *Eur J Appl Physiol* 82:345–360. <https://doi.org/10.1007/s004210000220>
- di Prampero PE, Ferretti G (1999) The energetics of anaerobic muscle metabolism: a reappraisal of older and recent concepts. *Respir Physiol* 118:103–115. [https://doi.org/10.1016/S0034-5687\(99\)00083-3](https://doi.org/10.1016/S0034-5687(99)00083-3)
- di Prampero PE, Margaria R (1968) Relationship between O₂ consumption, high energy phosphates and the kinetics of the O₂ debt in exercise. *Pflügers Arch* 304:11–19. <https://doi.org/10.1007/BF00586714>
- Ferretti G (2015) Energetics of muscular exercise. Springer International Publishing, Cham
- Ferretti G, Fagoni N, Taboni A et al (2017) The physiology of submaximal exercise: the steady state concept. *Respir Physiol Neurobiol* 246:76–85. <https://doi.org/10.1016/j.resp.2017.08.005>
- Ferretti G, Fagoni N, Taboni A et al (2022) A century of exercise physiology: key concepts on coupling respiratory oxygen flow to muscle energy demand during exercise. *Eur J Appl Physiol* 122:1317–1365. <https://doi.org/10.1007/s00421-022-04901-x>
- Ferretti G (2023) Exercise, respiratory and environmental physiology. In: Ferretti G (ed) Exercise, respiratory and environmental physiology. Springer, Cham
- Fontolliet T, Bringard A, Adami A et al (2021) Vagal blockade suppresses the phase I heart rate response but not the phase I cardiac output response at exercise onset in humans. *Eur J Appl Physiol* 121:3173–3187. <https://doi.org/10.1007/s00421-021-04769-3>
- Forster HV, Haouzi P, Dempsey JA (2012) Control of breathing during exercise. *Compr Physiol* 2:743–777. <https://doi.org/10.1002/cphy.c100045>
- Fukuoka Y, Ikegami H (1990) Respiratory response to sinusoidal work load in humans. *Ann Physiol Anthr* 9:175–183. <https://doi.org/10.2114/ahs1983.9.175>
- Fukuoka Y, Gwon O, Sone R, Ikegami H (1995) Characterization of sports by the VO₂ dynamics of athletes in response to sinusoidal work load. *Acta Physiol Scand* 153:117–124. <https://doi.org/10.1111/j.1748-1716.1995.tb09842.x>

- Fukuoka Y, Shigematsu M, Fukuba Y et al (1997) Dynamics of respiratory response to sinusoidal work load in humans. *Int J Sports Med* 18:264–269. <https://doi.org/10.1055/s-2007-972631>
- Gaesser GA, Brooks GA (1975) Muscular efficiency during steady-rate exercise: effects of speed and work rate. *J Appl Physiol* 38:1132–1139. <https://doi.org/10.1152/jappl.1975.38.6.1132>
- Girardi M, Gattoni C, Mauro L, Capelli C (2021a) The effects of sinusoidal linear drifts on the estimation of cardiorespiratory dynamic parameters during sinusoidal workload forcing: a simulation study. *Respir Physiol Neurobiol* 289:103652. <https://doi.org/10.1016/j.resp.2021.103652>
- Girardi M, Nicolò A, Bazzucchi I et al (2021b) The effect of pedalling cadence on respiratory frequency: passive vs. active exercise of different intensities. *Eur J Appl Physiol* 121:583–596. <https://doi.org/10.1007/s00421-020-04533-z>
- González-Alonso J, Mora-Rodríguez R, Below PR, Coyle EF (1997) Dehydration markedly impairs cardiovascular function in hyperthermic endurance athletes during exercise. *J Appl Physiol* 82:1229–1236. <https://doi.org/10.1152/jappl.1997.82.4.1229>
- Hauzi P (2006) Theories on the nature of the coupling between ventilation and gas exchange during exercise. *Respir Physiol Neurobiol* 151:267–279. <https://doi.org/10.1016/j.resp.2005.11.013>
- Hauzi P, Fukuba Y, Casaburi R et al (1993) O₂ uptake kinetics above and below the lactic acidosis threshold during sinusoidal exercise. *J Appl Physiol* 75:1683–1690. <https://doi.org/10.1152/jappl.1993.75.4.1683>
- Hayashi K, Honda Y, Ogawa T et al (2006) Relationship between ventilatory response and body temperature during prolonged submaximal exercise. *J Appl Physiol* 100:414–420. <https://doi.org/10.1152/japplphysiol.00541.2005>
- Hesser CM, Linnarsson D, Bjurstedt H (1977) Cardiorespiratory and metabolic responses to positive, negative and minimum-load dynamic leg exercise. *Respir Physiol* 30:51–67. [https://doi.org/10.1016/0034-5687\(77\)90021-4](https://doi.org/10.1016/0034-5687(77)90021-4)
- Hill DW (1993) The critical power concept: a review. *Sport Med an Int J Appl Med Sci Sport Exerc.* 16:237–254
- Hopkins WG, Marshall SW, Batterham AM, Hanin J (2009) Progressive statistics for exercise in sports medicine and exercise science. *Med Sci Sports Exerc* 41:3–12. <https://doi.org/10.1249/MSS.0b013e31818cb278>
- Jones AM, Vanhatalo A, Burnley M et al (2010) Critical power: Implications for determination of V_{O2}max and exercise tolerance. *Med Sci Sports Exerc* 42:1876–1890. <https://doi.org/10.1249/MSS.0b013e3181d9cf7f>
- Jones AM, Grassi B, Christensen PM et al (2011) Slow component of Vo₂ kinetics: mechanistic bases and practical applications. *Med Sci Sports Exerc* 43:2046–2062. <https://doi.org/10.1249/MSS.0b013e31821fcfc1>
- Lador F, Kenfack MA, Moia C et al (2006) Simultaneous determination of the kinetics of cardiac output, systemic O₂ delivery, and lung O₂ uptake at exercise onset in men. *Am J Physiol - Regul Integr Comp Physiol* 290:R1071–R1079. <https://doi.org/10.1152/ajpregu.00366.2005>
- Lamarra N, Whipp BJ, Ward SA, Wasserman K (1987) Effect of interbreath fluctuations on characterizing exercise gas exchange kinetics. *J Appl Physiol* 62:2003–2012. <https://doi.org/10.1152/jappl.1987.62.5.2003>
- Leo P, Spragg J, Podlogar T et al (2022) Power profiling and the power-duration relationship in cycling: a narrative review. *Eur J Appl Physiol* 122:301–316. <https://doi.org/10.1007/s00421-021-04833-y>
- Lonsdorfer-Wolf E, Richard R, Doutreleau S et al (2003) Pulmonary hemodynamics during a strenuous intermittent exercise in healthy subjects. *Med Sci Sports Exerc* 35:1866–1874. <https://doi.org/10.1249/01.MSS.0000094181.07571.72>
- Lucia A, San Juan AF, Montilla M et al (2004) In Professional road cyclists, low pedaling cadences are less efficient. *Med Sci Sport Exerc* 36:1048–1054. <https://doi.org/10.1249/01.MSS.0000128249.10305.8A>
- Mattioni Maturana F, Fontana FY, Pogliaghi S et al (2018) Critical power: how different protocols and models affect its determination. *J Sci Med Sport* 21:742–747. <https://doi.org/10.1016/j.jsams.2017.11.015>
- Morton RH (2006) The critical power and related whole-body bioenergetic models. *Eur J Appl Physiol* 96:339–354. <https://doi.org/10.1007/s00421-005-0088-2>
- Nicolò A, Girardi M, Bazzucchi I, et al (2018) Respiratory frequency and tidal volume during exercise: differential control and unbalanced interdependence. *Physiol Rep* 6:1–17. <https://doi.org/10.14814/phy2.13908>
- Orizio C, Perini R, Comandè A et al (1988) Plasma catecholamines and heart rate at the beginning of muscular exercise in man. *Eur J Appl Physiol Occup Physiol* 57:644–651. <https://doi.org/10.1007/BF00418477>
- Özyener F, Rossiter HB, Ward SA, Whipp BJ (2001) Influence of exercise intensity on the on- and off- transient kinetics of pulmonary oxygen uptake in humans. *J Physiol* 533:891–902. <https://doi.org/10.1111/j.1469-7793.2001.t01-1-00891.x>
- Paterson DH, Whipp BJ (1991) Asymmetries of oxygen uptake transients at the on- and offset of heavy exercise in humans. *J Physiol* 443:575–586. <https://doi.org/10.1113/jphysiol.1991.sp018852>
- Poole DC, Jones AM (2012) Oxygen Uptake Kinetics. *Compr Physiol* 2:933–996. <https://doi.org/10.1002/cphy.c100072>
- Poole DC, Barstow TJ, Gaesser GA et al (1994) VO₂ slow component: physiological and functional significance.pdf. *Med Sci Sport Exerc* 26:1354–1358
- Poole DC, Burnley M, Vanhatalo A et al (2016) Critical power: an important fatigue threshold in exercise physiology. *Med Sci Sports Exerc* 48:2320–2334. <https://doi.org/10.1249/MSS.0000000000939>
- Porszasz J, Rambod M, Van der Vaart H et al (2013) Sinusoidal high-intensity exercise does not elicit ventilatory limitation in chronic obstructive pulmonary disease. *Exp Physiol* 98:1102–1114. <https://doi.org/10.1113/expphysiol.2012.070375>
- Rossiter HB, Ward SA, Kowalchuk JM et al (2002) Dynamic asymmetry of phosphocreatine concentration and O₂ uptake between the on- and off-transients of moderate- and high-intensity exercise in humans. *J Physiol* 541:991–1002. <https://doi.org/10.1113/jphysiol.2001.012910>
- Rowell LB, O’Leary DS (1990) Reflex control of the circulation during exercise. *J Appl Physiol* 69:407–418. <https://doi.org/10.1111/sms.12600>
- Urhausen A, Weiler B, Coen B, Kindermann W (1994) Plasma catecholamines during endurance exercise of different intensities as related to the individual anaerobic threshold. *Eur J Appl Physiol Occup Physiol* 69:16–20. <https://doi.org/10.1007/BF00867921>
- Van Schuylenbergh R, Vanden Eynde B, Hespel P (2004) Correlations between lactate and ventilatory thresholds and the maximal lactate steady state in elite cyclists. *Int J Sports Med* 25:403–408. <https://doi.org/10.1055/s-2004-819942>
- Vinetti G, Taboni A, Bruseghini P et al (2019) Experimental validation of the 3-parameter critical power model in cycling. *Eur J Appl Physiol* 119:941–949. <https://doi.org/10.1007/s00421-019-04083-z>
- Wells GD, Diep T, Duffin J (2007) The ventilatory response to sine wave variation in exercise loads and limb movement frequency. *Respir Physiol Neurobiol* 158:45–50. <https://doi.org/10.1016/j.resp.2007.03.009>

- Whipp BJ, Ward SA (1982) Cardiopulmonary coupling during exercise. *J Exp Biol* 100:175–193. <https://doi.org/10.1242/jeb.100.1.175>
- Whipp BJ, Wasserman K (1969) Efficiency of muscular work. *J Appl Physiol* 26:644–648. <https://doi.org/10.1152/jappl.1969.26.5.644>
- Whipp BJ, Ward SA, Lamarra N et al (1982) Parameters of ventilatory and gas exchange dynamics during exercise. *J Appl Physiol* 52:1506–1513
- Wigertz O (1970) Dynamics of ventilation and heart rate in response to sinusoidal work load in man. *J Appl Physiol* 29:208–218. <https://doi.org/10.1152/jappl.1970.29.2.208>

Publisher's Note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.