BASIC SCIENCE



Mesenchymal cells and fluid flow stimulation synergistically regulate the kinetics of corneal epithelial cells at the air–liquid interface

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Abstract

Purpose In vivo microenvironments are critical to tissue homeostasis and wound healing, and the cornea is regulated by a specific microenvironment complex that consists of cell–cell interactions, air–liquid interfaces, and fluid flow stimulation. In this study, we aimed to clarify the effects of and the correlations among these three component factors on the cell kinetics of corneal epithelial cells.

Methods Human corneal epithelial–transformed (HCE–T) cells were cocultured with either primary rat corneal fibroblasts or NIH 3T3 fibroblasts. We employed a double-dish culture method to create an air–liquid interface and a gyratory shaker to create fluid flow stimulation. Morphometric and protein expression analyses were performed for the HCE–T cells.

Results Both the primary rat fibroblasts and the NIH 3T3 cells promoted HCE–T cell proliferation, and the presence of fluid flow synergistically enhanced this effect and inhibited the apoptosis of HCE–T cells. Moreover, fluid flow enhanced the emergence of myofibroblasts when cocultured with primary rat fibroblasts or NIH 3T3 cells. Extracellular signal-regulated kinase and p38 signaling were regulated either synergistically or independently by both fluid flow and cellular interaction between the HCE–T and NIH 3T3 cells.

Conclusion The cell–cell interaction and fluid flow stimulation in the air–liquid interface synergistically or independently regulated the behavior of HCE–T cells. Fluid flow accelerated the phenotypic change from corneal fibroblasts and NIH 3T3 cells to myofibroblasts. Elucidation of the multicomponent interplay in this microenvironment will be critical to the homeostasis and regeneration of the cornea and other ocular tissues.

Keywords Corneal microenvironment · Shear stress · Cell-cell interaction · Wound healing

Introduction

The cornea is a transparent tissue and is composed of five layers: the multilayered corneal epithelium, Bowman's membrane, the corneal stroma, Descemet's membrane, and the corneal endothelial layer (Fig. 1a) [1]. Both corneal epithelial cells and stromal keratocytes possess the paracrine loop and regulate the homeostasis and wound healing process of the cornea [2]. The cornea exists in the air–liquid interface, which

Shigehisa Aoki aokis@cc.saga-u.ac.jp is composed of lacrima (the covering watery fluid) and the surrounding atmosphere [3]. In addition, corneal stromal cells are exposed to interstitial fluid flow produced by the aqueous humor from the anterior chamber [4].

In vivo microenvironments are critical for tissue homeostasis and the wound healing process [5, 6]. The paracrine loop that originates during cell–cell interaction is a cellular factor of the microenvironment [7]. Physical stimulation such as fluid shear is in turn a location-specific factor of the microenvironment of a given tissue [8]. In cornea, lacrima is stirred by palpebration and eye movement, and corneal epithelial cells are constantly exposed to fluid flow stimulation. In addition, these corneal epithelial cells are in the air–liquid interface composed of lacrima and air at the surface of the eye. We hypothesized that there may be a connection, in the cornea, among interactions between epithelial and stromal cells, fluid flow stimulation, and the air–liquid interface and that each of these three factors may

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Fig. 1 Corneal microenvironment and experimental design. **a** Corneal physical and cellular microenvironment. The cornea exists with an airliquid interface composed of the covering watery lacrimal fluid and the surrounding air. The cornea itself consists of three cellular layers: the epithelial layer, the corneal stroma, and the endothelial layer. The interaction between the epithelial and stromal layers constitutes a specific cellular microenvironment of the cornea. **b** Histologic features of corneal ulcers. In this illustration, alpha-smooth muscle actin (α SMA)–positive myofibroblasts are located beneath the epithelial layer and the surface of the eroded corneal stroma (arrowhead). Cytokeratin (CK) AE1/AE3

have an important role to play in the homeostasis of corneal tissue as a specific constituent of the microenvironment. No culture models that can simultaneously reconstruct cell–cell interaction, fluid flow stimulation, and air–liquid interface are available. To the best of our knowledge, we overcame this issue by establishing a simple culture model that could concurrently replicate the cellular and physical microenvironments in the cornea.

This study aimed to clarify the effect of both the cellular and physical microenvironments on the homeostasis and wound healing in corneal tissue. immunostaining shows epithelial cell invagination into the corneal stroma (arrow). **c** Coculture models of human corneal epithelium–transformed (HCE–T) cells seeded on collagen gel discs embedded with corneal fibroblasts or NIH 3T3 cells. As a control, HCE–T cells were seeded on collagen gel discs without stromal cells. **d** Double-dish air–liquid interface (ALI) culture method. To replicate the air–liquid interface, the culture fluid level of outer dish was adjusted to the height of collagen gel of the inner dish. **e** Continuous fluid flow–generating system. To generate fluid flow, culture dishes were placed on a gyratory shaker in a CO₂ incubator

Methods

Cell lines and tissue samples

Human corneal epithelial-transformed (HCE–T) cell lines were obtained from the RIKEN Cell Bank (Ibaraki, Japan) and maintained in Roswell Park Memorial Institute (RPMI) 1640 medium supplemented with 10% fetal bovine serum (FBS), 0.5% dimethyl sulfoxide, 100 μ /mL streptomycin, and 100 μ /mL penicillin. NIH 3T3 mouse fibroblasts were obtained from the Japanese Cancer Research Bank, Osaka. NIH 3T3 cell lines were maintained in RPMI 1640 medium supplemented with 10% FBS, 100 μ /mL streptomycin, and 100 μ /mL penicillin. Primary corneal fibroblasts were isolated from the corneal tissue of 4- to 6-week-old Wistar rats. To isolate cells, the corneas were incubated in a 3-mg/mL collagenase A solution for 1 h at 37 °C with a stirring device. The digest was then immediately placed in a monolayer culture and maintained in RPMI 1640 medium supplemented with 10% FBS, 100 μ /mL streptomycin, and 100 μ /mL penicillin. Under the culture condition, isolated keratocytes lost their phenotype and differentiated into fibroblasts in the presence of FBS [9]. All cell lines were incubated in a humidified atmosphere of 5% CO₂ and 20% O₂ at 37 °C in a CO₂ incubator.

Air-liquid interface cell culture system

To analyze the cell-cell interaction and kinetics of HCE-T cells, we developed a double-dish culture system (Fig. 1c) [10, 11]. First, corneal fibroblasts or NIH 3T3 cells were mixed with a collagen gel solution (Cellmatrix, type I-A; Nitta Gelatin Co. Ltd., Osaka). Next, 1 mL of the mixture (including 5×10^5 keratocytes or NIH 3T3 cells) was poured into 30-mm-diameter Millicell-CM dishes (Millipore, Bedford, Massachusetts, USA). After the gel was solidified at 37 °C for 30 min, 2×10^5 HCE–T cells were seeded onto the surface of each dish. These dishes were then placed in larger (90-mm-diameter) outer dishes (Sumitomo Bakelite, Japan) containing 9 mL of complete medium in an air-liquid interface condition (Fig. 1d). To serve as controls, HCE-T cells were also seeded on collagen gel dishes without mesenchymal cells. Primary corneal keratocyte cells isolated from the corneal tissue of Wistar rats were cocultured with HCE-T, as previously described.

Fluid flow-generating system

The fluid flow–generating system was slightly modified from a method used previously [12]. One day after HCE–T cells were seeded, dishes were incubated in a system that generated fluid flow. The culture dishes were incubated in an atmosphere of 5% CO₂ and 20% O₂ at 37 °C in a CO₂ incubator; to generate flow, the dishes were placed on a gyratory shaker (MIR–S100C; Panasonic, Tokyo, Japan) that rotated at a speed of 45 rpm (Fig. 1e). Control dishes were placed in the CO₂ incubator when static, and the culture medium was changed every other day. In this way, the HCE–T cells were exposed to both an air–liquid interface and a fluid flow condition, which mimicked the in vivo physical microenvironment of the cornea.

Histology and immunohistochemistry

After 14 days of culturing, we performed histological examinations with hematoxylin-eosin staining. Tissues were fixed with 10% formalin, routinely processed, and embedded in paraffin, before deparaffinized sections were used for staining. A mouse monoclonal anti-pan-cytokeratin (CK) AE1/AE3 antibody was used to detect HCE-T cells, and a mouse monoclonal alpha-smooth muscle actin (aSMA) antibody (Dako, Glostrup, Denmark) was used to evaluate the myofibroblasts. Proliferative and apoptotic cells were labeled with a mouse monoclonal anti-Ki-67 antibody (Dako) and a rabbit monoclonal cleaved caspase-3 antibody (Cell Signaling Technology, Danvers, Massachusetts), respectively. For immunofluorescence analyses, a rabbit monoclonal anti- α SMA antibody conjugated with Alexa Fluor 488 was used. Alexa Fluor 568-conjugated goat anti-mouse immunoglobulin G (Invitrogen, Carlsbad, CA) was used as the antibody secondary to CK AE1/AE3 antibody. Images were analyzed with an Axio Imager 2 light microscope and Apotome.2 system (Carl Zeiss Co. Ltd., Oberkochen, Germany).

Morphometric analysis

A total of 1000 cells were counted (low magnification, \times 10 objective) at five randomly chosen noncontiguous and nonoverlapping fields of the stained sections. The percentages of Ki-67-positive cells and cleaved caspase-3–positive cells were then determined as indicators of proliferation and apoptosis, respectively. The epithelial cell layer thickness was measured at ten points in the five randomly chosen areas. The depth of HCE–T cell invagination was measured from the basement membrane to the deepest part of the HCE–T cells.

Western blot analysis

Experiments were performed with the samples in submerged conditions for the protein analysis. HCE-T cells and NIH 3T3 cells were cocultured in inserts with 8-µm pore sizes (Falcon Cell Culture Insert; Becton Dickinson, Franklin Lakes, N.J.). NIH 3T3 cells embedded in collagen gels were placed on the outside bottom of the inserts, and HCE-T cells were seeded inside the inserts. The inserts were then placed in 10-cmdiameter dishes in 20 mL of complete medium and were adjusted to the air-liquid interface condition. After culturing for 48 h, the collagen gels were stripped from the inserts. The HCE-T cells were lysed in 400 µL of M-PER Reagent (ThermoFisher Scientific, Waltham, Massachusetts) containing Protease/Phosphatase Inhibitor Cocktail (Cell Signaling Technology). Lysates containing an equal quantity of protein were separated by sodium dodecyl sulfate-polyacrylamide gel electrophoresis in 12% bis-tris gels and transferred to polyvinylidene difluoride membranes. The membranes were



50

40 30

20

10

0

Mono

+Fibroblast

+NIH3T3

6

4

2

0

Mono

+Fibroblast

+NIH3T3

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static flow

Mono

+Fibroblast +NIH3T3

Fig. 2 Effects of stromal cells and fluid flow on the cellular kinetics of HCE−T cells. a At day 14, both keratocyte and NIH 3T3 cells synergistically promoted cellular hypertrophy and thickened epithelium layer in HCE−T cells in conditions of fluid flow. HCE−T cells cultured with fibroblasts and NIH 3T3 cells invaded the corneal stroma. Upper and lower pictures show low and high magnification images, respectively. Abbreviation: Mono, monoculture. Bar, 100 µm. b Immunostaining of Ki-67 ad cleaved caspase-3. c Thickness of epithelial cell layers. d Immunostaining for Ki-67 and the percentages of positive cells. Data are shown as means ± standard deviation of the mean for three measures. **p* < 0.05. White and blue bar charts indicate the static and fluid flow conditions, respectively</p>

incubated overnight at 4 °C with antibodies against extracellular signal–regulated kinase (ERK) 1/2, p-ERK1/2, p38, and p-p38 (Cell Signaling Technology). A chemiluminescent immunodetection system (Western Breeze; ThermoFisher Scientific) was used to detect antibody-bound antigens on membranes. Band densities were determined using a Fusion system (Vilber–Lourmat, Eberhardzell, Germany), analyzed with Image J software (http://rsb.info.nih.gov/ij/), and presented as ratios relative to control values.

Statistical analysis

Data obtained from three to five independent experiments were analyzed with Student's *t* tests or Wilcoxon tests, depending on the results of equality of variance. Values are presented as means \pm standard deviations, together with the number of experiments carried out. Mean values of replicates in experiments were used to determine statistical significance; *p* values of less than 0.05 indicated statistically significant differences. All statistical analyses were performed using JMP 13 for Windows (SAS, Cary, N.C.).

Results

Synergism of mesenchymal cells and fluid flow in HCE–T cells at the air–liquid interface

Because the air-liquid interface is an essential microenvironment for corneal cell culture [10, 11], all experiments were performed in this condition.

To clarify mesenchymal paracrine and fluid flow stimulation effects, we cultured HCE–T cells with primary corneal fibroblasts derived from rat corneal tissue or NIH 3T3 fibroblasts in the static and fluid flow conditions, as mentioned previously. The HCE–T cells cultured without mesenchymal cells showed a flat cytoplasm with a one- to twolayer structure in the static conditions (Fig. 2a). When they were cultured with primary keratocytes, however, cellular hypertrophy was induced, and the thickness of the HCE–T cell layer increased. When they were cultured with NIH 3T3 cells in the static conditions, there was mild cytoplasmic hypertrophy with increased sheet-like thickness of cells. Both fibroblasts and NIH 3T3 cells triggered HCE– T cell invagination into the collagen gel layer, which was not present in the monoculture group, in both static and fluid flow conditions.

Next, we added fluid flow stimulation to the cell cultures to investigate the role of the physical microenvironment. HCE–T cells in the monoculture group showed cytoplasmic hypertrophy and a thickened cellular layer in conditions of fluid flow stimulation (Fig. 2a). The presence of fibroblasts or NIH 3T3 cells also induced greater cell numbers, a greater ratio of nuclear cells to cytoplasmic cells, and an increase in multistratified layers in HCE–T cells. The respective thicknesses of cellular layers in the groups in the static and fluid flow conditions were $16.3 \pm 7.1 \ \mu m$ and $28.0 \pm 13.3 \ \mu m$, respectively, for HCE–T monocultures; $29.7 \pm 7.9 \ \mu m$ and $116.8 \pm 5.1 \ \mu m$, respectively, for HCE–T cells plus fibroblasts; and $37.4 \pm 7.3 \ \mu m$ and $72.6 \pm 10.3 \ \mu m$, respectively, for HCE–T cells plus NIH 3T3 cells.

In static conditions, there was a difference between the groups cocultured with fibroblasts and those cocultured with NIH 3T3. Fluid flow significantly increased the ratio of Ki-67-positive HCE–T cells cocultured with either fibroblasts or NIH 3T3 cells, in comparison with these groups in static conditions. The respective Ki-67 labeling index percentages in the groups in static and fluid flow conditions were $40.7\% \pm 20.7\%$ and $52.9\% \pm 12.6\%$, respectively, for HCE–T monocultures; $27.5\% \pm 14.4\%$ and $54.6\% \pm 24.1\%$, respectively, for HCE–T cells plus fibroblasts; and $41.2\% \pm 5.2\%$ and $56.7\% \pm 9.8\%$, respectively, for HCE–T cells plus NIH 3 T3 cells (Fig. 2c).

Fibroblasts and NIH 3T3 cells had a lower labeling index of HCE–T cells positive for cleaved caspase-3 than did the monoculture group in static and fluid flow conditions (Fig. 2d). Fluid flow did not affect the cleaved caspase-3 labeling index in any group. The respective percentages for the cleaved caspase-3 labeling indexes in the groups in static and fluid flow conditions were $6.9\% \pm 4.3\%$ and $5.1\% \pm 3.8\%$, respectively, for HCE–T monocultures; $3.4\% \pm 2.4\%$ and $2.7\% \pm 1.2\%$, respectively, for HCE–T cells plus fibroblasts; and $3.6\% \pm 2.5\%$ and $2.3\% \pm 1.4\%$, respectively, for HCE–T cells plus NIH 3T3 cells.

Mesenchymal cells and fluid flow promote HCE–T cell invagination into collagen matrix at the air–liquid interface

Corneal damage induces keratocytes to differentiate into myofibroblasts [13]. These then regulate the deposition and organization of extracellular matrix in corneal wounds and are responsible for corneal wound contraction [14], and both the epithelial–mesenchymal transition of epithelial cells and the activated stromal niche regulate





Fig. 3 Stromal cells and fluid flow promote frequent myofibroblast emergence and HCE–T cell invagination **a** Myofibroblasts emerged beneath the epithelial layer in the group cocultured with fibroblasts or NIH 3T3 cells in the static condition. NIH 3T3 cells promoted more frequent myofibroblast emergence compared with the fibroblasts. Fibroblasts and NIH 3T3 cells induced HCE–T cells to invaginate into the collagen gel. Fluid flow enhanced this invagination of HCE–T cells. Immunofluorescence images of border area of epithelial cell layers and

mesenchymal cells (green, α SMA; red, cytokeratin [CK] AE1/AE3; blue, DAPI). α SMA and cytokeratin AE1/AE3 double–positive cell is difficult to detect. **b** Depth of epithelial cell invagination area. Data are shown as means ± standard deviation of the mean for three measures. Bar, 100 µm. *p < 0.05. White and blue bar chart indicates the static and fluid flow conditions, respectively. Abbreviations: Mono, monoculture; α SMA, alpha-smooth muscle actin

intrastromal invasion of limbal epithelial cells [15]. Any disarrangement of corneal epithelial cells and keratocytes then induces corneal opacity [16].

The monoculture group had no α SMA-positive cells in the static or fluid flow conditions, but aSMA-positive myofibroblasts emerged beneath the HCE-T cells in the groups cocultured with fibroblasts or NIH 3T3 cells in the static conditions (Fig. 3a). The frequency of myofibroblast emergence was higher in the group cocultured with NIH 3T3 than in the group cocultured with fibroblasts. Away from the epidermal layer, neither fibroblasts nor NIH 3T3 cells showed α SMA-positive phonotypes. Compared with the static condition, fluid flow increased the number of myofibroblasts in the affected area in both the keratocyte and the NIH 3T3 coculture groups. Compared with the static condition, fluid flow also increased the distributed range and depth of myofibroblasts from fibroblasts and NIH 3T3 cells in the affected area. Myofibroblasts emerged inside the thickened epithelial layers cocultured with fibroblasts and NIH3T3 cells under fluid flow condition, but the CK AE1/ AE3 and α SMA double-positive cell was not observed. During corneal regeneration, corneal epithelial cells often invaginate into the stroma in the manner of rete ridges of the skin [17]. To assess this, we measured the invagination depths of HCE-T cells into collagen gel. In the absence of mesenchymal cells, HCE-T cells did not invaginate into collagen gel in either the static or fluid flow condition. In contrast, the presence of fibroblasts and NIH 3T3 cells induced invagination, and this was promoted by fluid flow. The respective depths of invagination in groups in the static and fluid flow conditions were 0 µm and 0 µm, respectively, for HCE-T monocultures; $11.6 \pm 1.7 \mu m$ and $37.0 \pm 9.9 \mu m$, respectively, for HCE–T cells plus fibroblasts; and $21.0 \pm 6.0 \mu m$ and 43.9 \pm 3.9 μ m, respectively, for HCE–T cells plus NIH 3T3 cells.

Fibroblasts and fluid flow modulate ERK1/2 and p38 expression in HCE-T cells

Mitogen-activated protein kinase (MAPK) pathways are involved in the proliferation, epithelial–mesenchymal transition, and migration of many cell types, including those of the cornea [18]. To achieve reproducible results, we used NIH 3T3 cells as the representative mesenchymal cell, and we evaluated ERK1/2 and p38 expression to clarify the kinetics of HCE–T cells.

The total ERK expression of HCE–T cells did not differ significantly between the monoculture and NIH 3T3 cocultured groups in the static or fluid flow conditions (Fig. 4). Fluid flow caused significant downregulation of the total ERK expression in the monoculture group, in comparison with the static condition. There was no difference in the ratios of phosphorylated ERK1/2 to total ERK1/2 in the monoculture group in the static and fluid flow conditions. In comparison with the static condition, fluid flow caused significant upregulation of the ratio of phosphorylated ERK1/2 to total ERK1/2 in the monoculture group, in comparison with the NIH 3T3 coculture group.

There was no significant difference in total p38 expression of HCE–T cells between the monoculture and NIH 3T3 coculture groups in the static or fluid flow conditions. The ratio of phosphorylated p38 to total p38 was significantly lower in the monoculture group than that in the NIH 3T3 coculture group in the static condition. Fluid flow caused upregulation of the ratio of phosphorylated p38 to total p38 in the monoculture group in comparison with the static condition but caused downregulation of that ratio in the NIH 3T3 coculture group.

Discussion

In this study, we demonstrated that three microenvironments interaction between cells, stimulation by fluid flow, and the presence of an air–liquid interface—synergistically regulated the behavior of corneal epithelial cells. We assessed this synergy by using a new three-dimensional culture system.

Physical stress, especially fluid flow, has been implicated in the physiologic response to endothelial cells [19, 20]. Shear stress and fluid flow constitute critical microenvironmental factors in various cell types, including stem cells and cancer cells [21, 22]. In the eye, corneal epithelial cells and stromal cells are surrounded continuously by lacrimal and aqueous humor, respectively. These two fluids are involved in fluid flow during blinking, eye movement, and aqueous outflow. Several researchers have reported that the cell kinetics of corneal epithelial cells or endothelial cells are individually affected by the resulting shear stress [23-27]. However, these researchers used only two-dimensional, single-cell culture models and did not consider the air-liquid interfaces that are key for organs covering or covered by the body (e.g., eyes, skin, and gastrointestinal tract). According to previous reports, reconstructing this particular physical environment in a culture model affected cellular proliferation, apoptosis, differentiation, and stemness in several normal and cancer tissues [10, 28–30]. It is therefore essential that investigators replicate the tissue architecture, cell-cell interactions, and specific physical microenvironment in a three-dimensional culture system that in order to interpret cell kinetics and remodeling accurately.

Cell–cell interaction is critical for maintaining tissue homeostasis and regeneration of both normal and cancer tissue [31, 32], and a mesenchymal paracrine effect is attributed to cell–cell interaction and exerts proliferative, anti-apoptotic, and anti-inflammatory effects to parenchymal cells [33, 34]. Our culture model also replicated the anti-apoptotic paracrine effect of fibroblasts and NIH 3T3 cells in corneal epithelial cells independently of fluid flow stimulation. In contrast, the



< Fig. 4 Effect of NIH 3T3 cells and fluid flow on mitogen-activated protein kinase (MAPK) expression in HCE−T cells. Protein expression levels in HCE−T cells were evaluated with Western blot. Relative expression is depicted as the ratio of target protein expression to α- and β-tubulin expression. Data are presented as means ± standard deviations of 3–5 determinations. **p* < 0.05. White and blue bar charts indicate the static and fluid flow conditions, respectively. Abbreviations: ERK1/2, extracellular signal-regulated kinases 1 and 2; p-, phosphor-; Mono, monoculture

effect of physical stimulation on cell–cell interactions is not fully understood. In this study, we demonstrated that a phenotypic change from keratocyte or fibroblast to myofibroblast was promoted by fluid flow stimulation in the air–liquid interface. Moreover, MAPK signaling was synergistically or independently regulated by the interaction between cells and the stimulation by fluid flow. Our simple culture model helped us determine the factors that affected the behavior of corneal epithelial cells in order to evaluate the kinetics of corneal cells in a manner consistent with the in vivo environment.

Corneal ulceration can be highly detrimental to visual acuity, potentially causing loss of vision in the most severe cases [35]. Such ulcers have been attributed to the loss and deformation of the extracellular matrix material of corneal tissue. Several researchers have also reported that injury-induced activation and phenotypic transformation from fibroblasts to myofibroblasts regulate the deposition and organization of extracellular matrix in corneal wounds [14, 36]. Myofibroblasts play a central role in the control of an interconnected meshwork of cells and extracellular matrix that deposits regenerative matrix and contracts corneal wounds [37]. In addition, epithelial-mesenchymal transition is recognized to occur in a limbal site in cases of corneal injury and is involved in the fibrotic process of corneal regeneration. Pathological fibrotic and re-epithelizing processes cause vision-threatening diseases such as severe ocular surface fibrosis [38]. Although the importance of myofibroblasts is widely recognized, no suitable application for in vitro analysis was previously established. In this study, we proposed that replication of both corneal cell-cell interaction and the specific microenvironment is essential for understanding the corneal wound healing process.

The activation of MAPK signaling is a key factor in the transition of fibroblasts to myofibroblasts [39, 40]. However, our data showed that with fluid flow stimulation, the number of myofibroblasts increased and phosphorylation of ERK and p38 of HCE–T cells cocultured with NIH 3T3 cells decreased. We previously demonstrated that fluid flow stimulation promoted peritoneal fibrosis via epithelial–mesenchymal transition of mesothelial cells [12]. In addition, fluid flow stimulation ratio of ERK1/2 and p38 of mesothelial cells, and ERK and p38 inhibitors replicated the fibrotic change caused by mesothelial cells without fluid flow stimulation in the same manner.

Fluid flow stimulation may regulate non-ERK or non-p38 signaling, and the signaling of an unknown entity may increase the emergence of myofibroblasts and inhibit the expression of ERK and p38.

In conclusion, we established a reconstruction model for concurrently investigating the cellular and physical microenvironments of corneal tissue. This alternative culture model is a promising tool to aid with further therapeutic investigation into cornea-damaging disease.

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Compliance with ethical standards

All animal experiments complied with the guidelines of the Association for Research in Vision and Ophthalmology (ARVO) Statement for the Use of Animals in Ophthalmic and Vision Research.

Conflict of interest The authors declare that they have no conflict of interest.

Ethical approval All applicable international, national, and institutional guidelines for the care and use of animals were followed.

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