ORIGINAL CONTRIBUTION

Coarse-grained simulation study of dual-stimuli-responsive nanogels

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Abstract In this work, the swelling of pH- and temperaturesensitive [poly(2-(diethylamino) ethyl) methacrylate]-based nanogels has been analyzed with the help of coarse-grained simulations employed in the last decade for polyelectrolyte gels. This computational approach, which is based on particle-particle interactions between polymer units, constitutes an alternative to thermodynamic formalisms. Polymer-polymer hydrophobic forces are accounted for in the model through a solvent-mediated interaction potential whose depth increases with temperature. This model qualitatively captures the swelling behavior of such nanogels when their degree of protonation varies from 0 to 1 without requiring changes in the potential parameters. In addition, our study quantitatively reveals that [poly(2-(diethylamino) ethyl) methacrylate]-based particles are more hydrophobic than those based on poly(*N*-isopropylacrylamide).

Keywords Coarse-grained simulations · Responsive nanogels

Introduction

Nanogels are nanometer-sized particles that consist of a crosslinked polymer network with the ability to swell in a thermodynamically good solvent [1]. More specifically, these soft

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² POLYMAT, Bionanoparticles Group, Department of Applied Chemistry UFI 11/56, Faculty of Chemistry, University of the Basque Country UPV/EHU, Donostia-San Sebastián, Spain nanoparticles can swell or shrink depending on many external stimuli such as temperature, pH, salt concentration, or solvent nature, which makes them very useful for many biotechnological applications [2]. In fact, there is a growing biomedical interest in multi-responsive nanogels that focuses to a great extent on their usage as controlled drug delivery systems, which are expected to overcome therapeutic issues such as poor intracellular delivery, lack of control over the release behaviors, or side effects. For instance, nanogels can be employed for siRNA Delivery [3], cancer therapy [4], and theranostic applications [5].

From a theoretical perspective, the classical Flory-Rhener (FR) formalism for gels and its refinements have been also applied to nanogels to achieve a better understanding of their swelling behavior (implicitly assuming that surface effects are negligible if nanogels are large enough) [6]. In the last decade, computer simulations within coarse-grained models have also been considerably useful for the analysis of certain nonspecific aspects on the swelling of gels and nanogels, such as size and charge effects, since excluded-volume and electrostatic interactions can be explicitly considered [7-20]. Coarsegrained models have also been extensively employed to shed light on issues of biotechnological interest, such as the adsorption and collapse of biopolymers [21–29], viral detection [30], or genome encapsidation [31]. It should be mentioned, however, that direct comparisons with experiments on specific microgels or nanogels have been scarcely done. In this sense, a solvent-mediated hydrophobic interaction was recently included in a coarse-grained model to capture the swelling of thermo-responsive microgels whose main comonomer was poly(N-isopropylacrylamide) (PNIPAM) [13]. This model succeeded in justifying why the transition from swollen to shrunken states was so gradual for these microgels, in contrast to abrupt volume changes previously reported for other PNIPAM-based gels and microgels. In particular, this work



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revealed that the abruptness of such transition is strongly conditioned by the number of monomer units per polymer chain. When this number is small, volume changes are very gradual and smaller in relative terms.

It should be pointed out, however, that the comparison performed by Quesada-Pérez et al. was restricted to slightly charged PNIPAM-based microgels with a high degree of cross-linking (small number of monomer units per chain) [13]. It would be desirable to find out if that coarse-grained model can justify (qualitatively at least) the swelling behavior of multi-responsive nanogels made of another stimuliresponsive polymers and/or under different conditions. In particular, it would be interesting to look into the case of nanogels with a high number of ionized monomer units per chain, since electrostatic interactions are not explicitly accounted for in most of the FR-inspired formalisms [6].

Recently, Pikabea et al. have reported an in-depth study of the swelling of multi-responsive nanogel particles based on poly(2-(diethylamino) ethyl) methacrylate (PDEAEMA) [32], which present thermo and pH sensitivity (tunable with the ionic strength). As a result of the protonation of amine groups in the monomer units, the degree of ionization of PDEAEMA chains can considerably increase when the pH decreases. In other words, slightly and highly charged nanoparticles can be achieved just changing the pH of the solution.

According to the preceding paragraphs, our main goal is to examine to what extent the abovementioned coarse-grained models for gels can capture the swelling of PDEAEMAbased nanogels with very different charges. We also want to test the hydrophobic potential (successfully applied to PNIPAM) with a different polymer.

Model and simulations

Model

The coarse-grained picture employed here is the so-called beadspring model for polyelectrolyte, in which monomer units and ions are represented as spheres, whereas the solvent is considered as a dielectric continuum [17, 33]. It should be mentioned that, even within this level of coarse graining, simulating charged nanogel particles with diameters greater than some tens of nanometers could require long times, particularly in the presence of salt, since a significant part of the electric double layer of such particles should also be included in the simulation cell. Just as an example, simulating nanogels of about 30 nm in the presence of an electrolyte at 100 mM [15] took nearly 2 months (within a conventional work station of 2.2 GHz).

For some purposes, however, simulating an inner piece of the polymer network might provide valuable information. This method, adopted here, supplies the value of intensive quantities such as the polymer volume fraction, which can be used to estimate the swelling ratio. In any case, the reader should keep in mind that this idealized representation of reality implicitly assumes that the inner structure of the network is replicated periodically and surface effects are negligible. A unit cell is schematically represented in Fig. 1.

If we consider the sequence of monomer units comprised between two cross-linker molecules as a single chain, molecules such as ethylene glycol dimethacrylate can be considered tetrafunctional cross-linkers (since four chains are linked to this molecule). Thus, a diamond-like topology was assumed (as usual in previous simulations of gels). N_{bead} stands for the number of monomer units (beads) per chain (between two cross-linker molecules or nodes), whereas N_{charged} represents the number of charged monomers per chain. In a model of ideal polymer network, N_{bead} and $N_{charged}$ are identical for all the chains of the network. In our simulations, Nbead=48 was employed. This value is of the order of the mean number of monomer units per chain that can be estimated from the synthesis recipe assuming an ideal network. The reader can find an example with PNIPAM-based microgels in a previous work [13]. In fact, it should be emphasized that the N_{bead} value used in these simulations is considerably greater than the value previously used comparing with PNIPAM-based microgels (N_{bead} =8). In other words, the degree of cross-linking of the nanogels studied here is significantly smaller. As we are interested in PDEAEMA chains with different degrees of ionization, simulations with several N_{charged} values were performed here.

Together with the beads of the polymer network, the simulation cell also contains a number of monovalent counterions that neutralize the charge of the protonated groups of the network. As the experiments with PDEAEMA-based nanogels were carried out in the presence of additional electrolyte, a monovalent electrolyte solution (at 10 mM) was also



Fig. 1 Snapshot of the simulation cell for a network with 48 monomers (*blue beads*) per chain and 2 ionized monomers (*red beads*) per chain. The snapshot also shows the cross-linkers (*green beads*) and the free counterions that neutralize the network charge (*orange beads*)

considered in simulations. For the sake of simplicity, the anion of the additional electrolyte was assumed to be identical to the counterion of the charged network, and both are collectively referred to as counterions. The solvent is only taken into account through its relative permittivity, ε_r .

Monomer units of polymer chains, cross-linker molecules, and ions are explicitly modeled as spheres of diameter σ_M , σ_{CL} , and σ_I , respectively. For PDEAEMA, σ_M was estimated from the molecular weight of the corresponding monomer and its density in the liquid state assuming that the volume fraction of such state is similar to that of close packing (0.74) [13, 34]. According to this prescription, previously used also for PNIPAM, σ_M =0.7 nm. This value was also assumed for cross-linker molecules. σ_I =0.7 nm was employed for all the ionic species. This ionic size can be considered representative for many hydrated monatomic cations and anions (if the hydration shell is included) and was estimated averaging results obtained from different experimental techniques [34].

At this point, let us comment the interactions between the different constituents of the model. The short-range repulsion between any pair of particles (monomer units, cross-linker molecules, and solute molecules) due to excluded volume effects is taken into account by means of the purely repulsive Weeks–Chandler–Andersen potential [8–10, 35]:

$$u_{WCA}(r) = \begin{cases} 4\varepsilon_{LJ} \left(\frac{\sigma^{12}}{r^{12}} - \frac{\sigma^6}{r^6} + \frac{1}{4} \right) & r \le \sqrt[6]{2}\sigma \\ 0 & r > \sqrt[6]{2}\sigma \end{cases}$$
(1)

where *r* is the center-to-center distance between a given pair of particles, $\varepsilon_{LJ}=4.11 \times 10^{-21}$ J, $\sigma=(\sigma_i+\sigma_j)/2$ (where *i* and *j* stand for interacting species). The beads of a given chain are connected by harmonic bonds, whose interaction potential is

$$u_{bond}(r) = \frac{k_{bond}}{2} (r - r_0)^2$$
(2)

where k_{bond} is the elastic constant and r_0 is the equilibrium bond length. In this work, we have assumed that $r_0 = \sigma_M$ and $k_{bond} = 0.4$ N/m. All the charged species (charged monomers and ions) interact electrostatically through the Coulomb potential:

$$u_{elec}(r) = \frac{Z_i Z_j e^2}{4\pi\varepsilon_0 \varepsilon_r r} \tag{3}$$

where *e* is the elementary charge, Z_i is the valence of species *i*, and ε_0 is the vacuum permittivity. Being interested in the thermo-responsive nanogels, the temperature dependence of the dielectric permittivity was also considered [36]:

$$\varepsilon_r = \frac{5321}{T} + 233.76 - 0.9297T + 0.4117 \cdot 10^{-2} T^2 - 0.8292 \cdot 10^{-6} T^3$$
(4)

Finally, we should keep in mind that, when nonpolar molecules (or macromolecules) are inserted into an aqueous medium, they tend to reduce the surface exposed to the solvent aggregating. The solvent-mediated attraction between nonpolar monomers required for this process is the so-called hydrophobic force, which is intrinsically temperature-sensitive and justifies why some polymer networks collapse upon heating. Admitting that the precise knowledge of hydrophobic forces is far from complete, other authors have employed phenomenological potentials for hydrophobic forces with different functional forms (square well, Lennard-Jones, and others) in previous simulations of flexible polymers [37-43]. In this work, the hydrophobic interaction was modeled through the same potential previously used for PNIPAM-based microgels [13], although some parameters were changed. In this way, the interaction potentials obtained for different polymers can be compared. The functional form $u_{hvd}(r)$ consists in a sigmoid approximation to the square well potential (also employed by other authors [39, 41, 44]):

$$u_{hyd}(r) = -\frac{\varepsilon_h}{2} (1 - \tanh(k_h(r - r_h)))$$
(6)

where r_h is the range of the potential and k_h is related to the slope of the sigmoid. As mentioned in previous works, the depth of this potential should increase with temperature. The function for the *T* dependence of ε_h previously proposed for PNIPAM was also adopted here:

$$\varepsilon_h(T) = \frac{\varepsilon_{\max}}{2} \left(1 + \tanh\left(k_{\varepsilon/2} \left(T - T_{\varepsilon/2}\right)\right) \right)$$
(7)

where ε_{max} is the maximum depth of the hydrophobic potential (reached at high temperatures), $T_{\varepsilon/2}$ is the temperature for which $\varepsilon = \varepsilon_{max}/2$ (inflection point) and $k_{\varepsilon/2}$ is proportional to the slope of the function at that point. Regarding the hydrophobic interaction, it should also be mentioned that charged chemical groups are usually hydrophilic rather than hydrophobic. Thus, the hydrophobic forces involving charged monomer units are expected to be considerably weakened. In addition, we also considered that hydrophobic forces are less intense for bonded monomeric units since their surface exposed to water molecules is smaller in this case. As a limiting case, we therefore assumed that the hydrophobic interaction only works between uncharged nonbonded monomeric beads.

Simulations

The simulation method of thermo-responsive gels in the presence of salt (in equilibrium with an external salt reservoir) has been described in detail elsewhere [35]. Here, its main features are outlined. First, the osmotic pressure and the activity coefficient of such reservoir were previously computed. The simulation cell consisted in a cubic box containing a piece of the polymer network (with a fixed number monomeric units), monovalent counterions neutralizing the charge of this network, and an electroneutral group of monovalent cations and anions in equilibrium with the salt reservoir. The equilibrium polymer volume fraction (φ) at a given temperature was calculated as follows. First, a set of systems at the same temperature but different polymer volume fractions were simulated adjusting the dimensions of the simulation cell. The osmotic pressure for each one of them was computed (see reference [35] for further details about the computation of this property). Then, φ was estimated as the polymer volume fraction for which the osmotic pressure of the simulation cell equaled the osmotic pressure of the electrolyte reservoir (previously determined, as mentioned before).

The Metropolis Monte Carlo (MC) protocol was used to generate Boltzmann-weighted gel configurations. Periodic boundary conditions were employed in the three directions of space. Translational MC moves were applied to all the particles in the simulation box adjusting their maximum displacements so that their acceptance ratios were of about 50 %. At least 1×10^7 and 2×10^7 trial moves were used for thermalization and statistics, respectively. It should be mentioned, however, that the electrolyte in equilibrium with the reservoir was simulated in the grand canonical ensemble implementing the method of Valleau and Cohen [45]. Accordingly, insertions and removals of ions were also attempted. As the condition of electrical neutrality of a system had to be preserved, electroneutral cation-anion pairs were inserted at random positions or were randomly selected from the ions present in the box and removed when such insertions and removals were attempted. The expressions for the probability of acceptance of these MC moves are again provided in reference [35].

Results

Given that the model employed here cannot provide extensive properties, comparisons between experiment and simulation will be done in relative terms defining the swelling ratio (S) as the quotient between the hydrodynamic diameters at a given state and at a reference state, which usually corresponds to the collapsed state. Figure 2 shows this parameter as a function of temperature for three pH values: 7.4, 6.3, and 5.6. The diameter of the nanogel at 353 K and pH=6.3 was chosen as reference to compute the swelling ratio. According to the titration curve reported by Pikabea et al. [32], the polyelectrolyte chains are slightly and highly protonated at pH=7.4 and 5.6, respectively. At pH=6.3, the degree of protonation is close to 50 %. Thus, these systems exhibit very different charges and three clearly differentiated swelling behaviors. At pH=7.4, nanogels are shrunken in the temperature window explored here, whereas at pH=5.6, they are swollen. At pH=6.3, a gradual transition from swollen to collapsed states is observed. The original results reported by Pikabea et al. [32] (which



Fig. 2 Swelling ratio observed in experiments with PDEAEMA-based nanogels (*solid symbols*) and predicted by simulations (*open symbols*) as a function of temperature at pH=7.4 (*solid* and *open squares*, respectively), 6.3 (*solid* and *open circles*, respectively), and 5.6 (*solid* and *open triangles*, respectively)

include data for other pH-values) also reveal that this transition shifts toward higher temperatures when the pH decreases and the nanogel charge increases. Finally, it should be mentioned that the swelling ratios observed in experimental data at pH=5.6 and 7.4 are similar to those observed at pH=6.3 when nanogels are swollen (low temperatures) or shrunken (high temperatures), respectively.

Can the simple model described above justify the behavior observed for PDEAEMA-based nanogels with very different charges? To give an answer to this question, $N_{charged}$ =2, 24, and 48 were chosen as representative number of ionized groups per chain for the slightly, moderately, and highly charged nanogels. Then, we tried to find a set of values for PDEAEMA-based nanogels that semiquantitatively captures their swelling behavior when their degree of ionization is 50 %. Such values were chosen taking as starting point the previously reported values for PNIPAM and/or from the experimental behavior observed for PNIPAM- and PDEAEMAbased nanogels. For instance, the lowest volume phase transition temperature (VPTT) observed for PDEAEMA-based nanogels (at 10 mM) by Pikabea et al. [32] is 292 K. As $T_{\varepsilon/2}$ is expected to be related to the VPTT (if $T_{\epsilon/2}$ increases, the VPTT will shifts towards larger values), two $T_{\varepsilon/2}$ values of this order were explored in our simulations (286 and 294 K). In relation to the depth and the range of the hydrophobic potential, r_h and ε_{max} , we explored a few values ranging from 0.9 to 1.4 nm and from 9.0×10^{-21} to 15.0×10^{-21} J, respectively. The swelling curves turned out to be quite sensitive to these parameters. As can be seen, such values are a bit larger than those reported for PNIPAM-based nanogels (see Table 1), in agreement with a recent work by Pelton [46] that concluded that PNIPAM chains have both hydrophobic and hydrophilic domains even above the lower critical solution temperature (LCST). In other words, this polymer is not as hydrophobic as many authors claim. $k_{\epsilon/2}$ is somehow related to the slope of volume phase transition observed in the collapse of the nanogels upon heating. The comparison of the experimental data shown in Fig. 2 for PDEAEMA-based nanogels with similar curves published for PNIPAM-based nanogels suggests that the slope of the transition is smaller for the former. Accordingly, we explored $k_{\varepsilon/2}$ values smaller than the $k_{\varepsilon/2}$ value reported for PNIPAM-based nanogels (0.03125 and 0.0385 K^{-1}) looking for the agreement between our results and simulation data. Finally, k_h is a technical parameter employed in constructing a differentiable approximation to the well square potential (which facilitates the computation of osmotic pressure). Swelling results are not expected to be very sensitive to this technical parameter. Thus, the same value reported for PNIPAM-based nanogels was used here. Indeed, this was not a strict fitting procedure, which would require a vast (and highly time-consuming) collection of simulation data at different conditions. However, it can provide some information about the hydrophobic forces inducing the collapse of PDEAEMA-based nanogels. Table 1 summarizes the values employed for the parameters of this potential for PNIPAM-based microgels (in a previous work) [13] and PDEAEMA-based nanogels.

In addition, Fig. 2 displays the swelling ratio obtained from simulations using the parameters included in Table 1. As mentioned before, this model cannot provide extensive quantities, such as the nanogel diameter. For an ideal network, however, the diameter is proportional to $\varphi^{-1/3}$, where φ is the polymer volume fraction. Thus, the swelling ratio can be computed as $S = \varphi^{-1/3} / \varphi_{ref}^{-1/3}$, where φ_{ref} is the φ value at the reference state.

Figure 3 shows the hydrophobic interaction potential, $u_{hyd}(r)$, computed from these parameters as a function of r for these two polymer units at the lower and upper temperatures explored here (283 and 353 K, respectively). As can be seen, both the depth and the range of the potential are greater for PDEAEMA. In fact, Fig. 3 also reveals that at 283 K, the depth for PDEAEMA is of the order of the thermal energy (k_BT) and very similar to the depth for PNIPAM at 353 K. This would justify why slightly charged PDEAEMA-based nanogels are shrunken at 283 K (since PNIPAM-based

 Table 1
 Parameters of the hydrophobic potential

Symbol	Unit	Value for PNIPAM- based microgels	Value for PDEAEMA- based nanogels
r_h	nm	0.9	1.3
k_h	nm^{-1}	12.0	12.0
$T_{\varepsilon/2}$	Κ	307.5	294
$k_{\varepsilon/2}$	K^{-1}	0.0667	0.02125
ε_{max}	J	5.5×10^{-21}	11.0×10^{-21}



Fig. 3 Hydrophobic potential between polymer units employed for PNIPAM (in a previous work [13]) and PDEAEMA at 283 and 353 K

nanogels are collapsed under similar hydrophobic forces at 353 K).

Concerning the predictions of the model using the parameters included in Table 1, Fig. 2 reveals that the model qualitatively and even semiguantitatively reproduces the gradual transition from swollen to shrunken states exhibited by the moderately charged nanogel (pH=6.3). The model also predicts that the highly charged nanogel is swollen in the temperature window explored, whereas the slightly charged system is collapsed. Both predictions are in qualitative agreement with the experimental swelling ratio observed. In relation to the qualitative agreement between simulation and experiment, it should be stressed that the predictions of the model displayed in Fig. 2 for PDEAEMA-based nanogels with different charges and those previously reported for PNIPAM-based microgels were obtained with hydrophobic potential's parameters that do not change when the nanogel charge varies. This is a strong point of the coarse-grained model as compared to FR-inspired formalisms, whose parameters can be extremely sensitive to the charge of the gel (even in the case of slightly charged systems) [13], which clearly limits the capability of prediction of these theoretical approaches.

It should be also mentioned, however, that there are quantitative discrepancies between simulation and experiment at pH=5.6 and 7.4, since the *S* value predicted for $N_{charged}$ =48 is considerably greater than that measured for pH=5.6, whereas the swelling ratio obtained for $N_{charged}$ =2 (pH=5.6) is significantly smaller than the one corresponding to the slightly charged nanogel.

Different aspects of real nanogels not included in this model could contribute to justify this quantitative disagreement. For instance, the reader should bear in mind that coarse-grained models are usually developed on polymer networks made of chains with the same number of monomeric units. However, high-resolution NMR measurements reveal a bimodal distribution of the PDEAEMA chain mobility inside the nanogel particles from which the coreshell model can be inferred [32]. Obviously, this also means that there is considerable heterogeneity in the PDEAEMA chain distribution, which is not considered in our coarse-grained model. Edgecombe et al. have observed that highly charged polymer networks with chain length polydispersity swell less than the ideal ones [47]. This could partly justify why simulation data overestimate the swelling ratio at pH=5.6. On the other hand, two factors might contribute to the numerical discrepancies reported for slightly charged systems (pH=7.4). First, it should be mentioned that our model did not consider chain stiffness. Thus, the compactness of shrunken networks might be overestimated by the model. In addition, the parameters employed in Eqs. 6 and 7 might overestimate the intensity of the hydrophobic interaction at high polymer volume fractions (collapsed nanogels), because the surface of polymer units exposed to water is smaller under such circumstances. At pH=7.4, simulations predict φ values of the order of 0.2. Thus, the hydrophobic interaction might have been overestimated to some extent in this case (predicting too shrunken nanogels). Finally, it should be kept in mind that we are simulating just an inner piece of the nanogel particle, which is identically replicated in the three directions of space. In other words, the core-shell structure inferred from NMR measurements is not included in the coarse-grained model either. Regarding this assumption (infinite and homogenous network), we should also point out that such hypothesis has been commonly employed in the study of microgels through classic RF formalisms as well as current sophisticated thermodynamic approaches [48-50]. However, a thermodynamic theory for core-shell particles has been recently proposed [51].

Conclusions

In this work, we have shown that coarse-grained simulations of polyelectrolyte gels qualitatively capture the swelling behavior of PDEAEMA-based nanogels with very different charges using a hydrophobic potential whose parameters do not depend on the degree of protonation, improving on the capability of prediction of those formalisms whose parameters are extremely sensitive to charge. Our simulations also suggest that the depth and the range of the hydrophobic interaction (responsible for the nanogel collapse) are greater for PDEAEMA polymer chains than for those of PNIPAM. In any case, the quantitative differences between simulation and experiment observed for highly and slightly charged nanogels could be reduced including some refinements in the model (for instance, chain length polydispersity, chain stiffness).

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Compliance with ethical standards

Conflict of interest The authors declare that they have no conflict of interest.

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