



Atrial fibrillation ablation strategies and technologies: past, present, and future

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Received: 11 February 2020 / Accepted: 30 September 2020 / Published online: 22 October 2020
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Abstract

Catheter ablation is an established treatment option for atrial fibrillation (AF), and pulmonary vein isolation (PVI) has become the gold standard in AF ablation. AF recurrence after PVI remains an important clinical problem. Recovery of conduction from the pulmonary veins (PVs) is considered the dominant mechanism for AF recurrence in paroxysmal AF. However, the underlying mechanism of AF recurrence after PVI is more complex in patients with persistent and longstanding persistent AF. Different ablation technologies and energy sources have been developed aimed at improving lesion quality and durability with an acceptable safety profile. Novel technologies are under evaluation which have a great potential to produce permanent PVI after a single ablation procedure. However, clinical value of these novel devices needs to be tested in adequately powered randomized controlled trials. In this article, we review the history of catheter ablation for AF and discuss the present and future ablation technologies.

Keywords Atrial fibrillation · Ablation · Ablation technologies · Electrophysiology · Catheter ablation · Ablation techniques

Introduction

Atrial fibrillation (AF) is the most common supraventricular tachyarrhythmia [1] and is associated with reduced quality of life [2], increased mortality [3] and morbidity, including enhanced risk of stroke [4], heart failure [5], and repeated hospitalizations [6]. Due to its significant impact on cardiovascular morbidity and mortality, researchers have sought ways to successfully treat and even cure some types of AF. Over the past decades, percutaneous catheter ablation (CA) has become an important AF treatment modality to restore and maintain sinus rhythm. Pulmonary vein isolation (PVI) is now considered the cornerstone of catheter-based treatment for paroxysmal and early persistent AF [7, 8]. Since the introduction of CA, major advances have been made. Different ablation technologies and energy sources have been designed and the search for improving ablation safety and

clinical outcome continues. This article outlines the history and evolution of CA, reviews the currently available AF ablation technologies, and provides a glimpse into future ablation techniques.

History of catheter ablation

The first intra-cardiac use of catheters was described in the 1960s, where the application was limited to signal recording and cardiac stimulation. One of the earliest reports of catheter use is a study performed by Durrer et al. in which application of intracardiac electrical pulses and signal recording was described in patients with Wolff-Parkinson-White (WPW) syndrome [9]. Together with electrophysiological studies performed by Zipes and Wellens in the 1970s, insights into tachycardia mechanisms, including the WPW syndrome, markedly improved [10–12].

Probably the first described catheter-mediated ablation was permanent atrioventricular conduction (AV) block accidentally caused in a patient undergoing an electrophysiological study for recurrent syncope in 1979 [13]. During the procedure, the patient required electrical cardioversions for ventricular tachycardia while the intracardiac bipolar

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recording catheter was reportedly in contact with the bundle of His. Presumably, this led to inadvertent transfer of externally delivered direct current energy over the recording catheter electrodes resulting in complete AV block.

This unintended catheter-mediated induction of AV block was further investigated in the following years, leading to the first described in-human catheter ablation in 1982. In a study by Scheinman et al., five patients suffering from drug refractory supraventricular tachycardia received a permanent pacemaker followed by AV junction ablation using high-energy DC shocks [14]. From this point, the use of the electrode catheters was no longer limited to diagnostic electrophysiological studies alone, and DC ablation was applied in ablation of accessory pathways [15], atrial tachycardias [16], and ventricular tachycardias [17].

While these early results of high-energy DC catheter ablation appeared potentially promising, the occurrence of significant adverse events, including cardiac tamponade and sudden death, were major drawbacks of the technique [18–21]. High-energy DC shocks were associated with arcing, gas formation and shockwave generation leading to barotrauma [22–24].

In the late 1980s, radiofrequency (RF) energy for catheter ablation was introduced. In the early 1990s, many studies on RF ablation followed, showing better efficacy and safety in ablation of accessory pathways, atrial flutter, modification of the AV junction in AV nodal reentrant tachycardia and ventricular tachycardia [25–29]. The use of RF catheter ablation skyrocketed, and high-energy DC ablation became abandoned.

History of atrial fibrillation ablation

While insights obtained from electrophysiological studies led to surgical and catheter-based treatment of several supraventricular tachyarrhythmias, such as WPW syndrome and AV nodal reentrant tachycardia, treatment options for more complex arrhythmias like AF were limited to drugs or pacemaker implantation followed by AV junction ablation. In 1987, the first surgical strategy for AF treatment was reported by Cox and colleagues. Their group performed computerized mapping of atrial fibrillation in animals and man, eventually leading to the development of a surgical procedure for the treatment of drug refractory AF, known as the surgical Maze procedure [30, 31]. The original Maze procedure involved creation of multiple surgical incisions in the left and right atrium during open heart surgery. The rationale for the Maze procedure was derived from experimental studies by Allesie and Schuessler [32, 33]. Allesie et al. experimentally validated Moe's multiple wavelet hypothesis by mapping the activation pattern in isolated canine atria during rapid pacing-induced cholinergic atrial

fibrillation [34–36]. Complete mapping of both atria was performed, and it was estimated that a critical number of four to six simultaneously present wavelets were required to maintain AF. Although the underlying mechanisms involved in the initiation and perpetuation of AF were incompletely understood, the main goal of the initial Maze procedure was to compartmentalize the atria, thereby creating an electrical maze, using the “cut and sew” technique or alternative means of creating linear lesions of electrical block in both atria to eliminate reentrant wavelets and restore SR or an atrial rhythm within the atrial myocardium [30]. Further improvements to the surgical technique eventually resulted in the Cox Maze III procedure, which is still used today [37]. Long-term follow-up of 198 patients with paroxysmal and persistent AF who underwent a Cox Maze III procedure showed that 95% were AF free after a mean follow-up of 5.3 years. Major complications occurred in 12%, including two perioperative deaths [38]. Due to the complex and invasive nature of the Maze procedure several investigators in the early 90s tried to replicate the ablation lesion sets using the catheter. Morillo et al. performed a study with 22 dogs in which structural remodeling of the atria was achieved by rapid pacing for 6 weeks, resulting in inducibility of sustained AF. In 11 of the dogs, attempted cryoablation of an area in the posterior left atrium resulted in restoration of sinus rhythm and non-inducibility of AF [39]. In that same year, Elvan et al. published a study in which AF was induced by burst pacing in 27 dogs. The creation of epicardial and endocardial RF ablation lesions targeting the left and right atrium, the superior vena cava, and transverse sinus resulted in reduced inducibility of AF (by high doses of methacholine) [40]. In the mid-90s, feasibility of CA as treatment of AF in humans was reported by Haïssaguerre et al. The ablation involved the creation of multiple linear lesions in the right atrium using RF energy. After ablation AF could not be induced with pacing, and during short-term follow-up of 3 months the patient remained free of arrhythmias without antiarrhythmic drugs [41]. The first patient series on catheter ablation of AF soon followed. In a study by Swartz et al. patients with chronic AF received RF CA in both the left and right atria [42]. Arrhythmia-free survival after 12 months was considered satisfying; however, the complication rate was high including pericardial effusion and cerebrovascular accidents. In a study by Haïssaguerre et al. 45 patients with paroxysmal AF received RF ablation with the creation of linear lesions mainly in the right atrium. Follow-up showed a poor 1-year arrhythmia-free survival, but no serious complications were observed [43]. Long-term follow-up of clinical trials that applied transcatheter linear ablation lesions in the right atrium in a Maze-like approach showed limited success [44, 45]. An historically important AF ablation approach targeting foci that triggered AF was reported by Jai's et al. These arrhythmogenic foci were found near the

sinus node, at the coronary sinus ostium, and at the ostium of the left and right sided pulmonary veins, and were successfully eliminated by RF ablation [46]. In 1998, Haissaguerre and colleagues published their milestone study on ablation of AF initiating triggers that were mainly localized in the pulmonary veins (PVs) and which could be successfully eliminated using CA [7]. These findings led to a different approach of AF ablation, focusing on the elimination of AF triggers, and the Maze-like linear lesions in the right atrium became abandoned. Subsequently, a method was developed to electrically isolate AF triggers in the PVs by creation of circumferential ablation lesions in the PVs, now known as pulmonary vein isolation (PVI) [47].

Many studies on electrical isolation of the PVs as treatment for AF followed, and currently PVI has become the cornerstone treatment in catheter-based ablation of AF [8]. Randomized trials showed better efficacy rates for RF ablation compared to antiarrhythmic drugs [48–50]. Furthermore, PVI resulted in better quality of life compared to drug therapy [51]. However, AF recurrence after ablation was still frequently observed, especially in patients with persistent and long-standing persistent AF. In patients with persistent forms of AF, it was recognized that triggers that initiated and maintained AF frequently originated outside the PVs, including the PV antrum, the posterior wall of the LA, the superior vena cava, the crista terminalis, the coronary sinus, ligament of Marshall and the left atrial appendage [8]. Ablation strategies were adapted to wider ablations at the PV antrum, also known as wide-area circumferential ablation (WACA), and strategies complementary to PVI were investigated [52]. These strategies included linear lesions in the left and right atria, ablation of the left atrial appendage, and ablation of complex fractionated atrial electrograms (CFAE) [53, 54]. Some observational studies have suggested a beneficial effect of additional ablations on treatment outcome [55, 56]. However, results from the randomized STAR AF II trial demonstrated that additional ablation lines or CFAE ablation did not result in better efficacy in patients with persistent AF [57]. Whether selected groups of patients benefit from these additional ablation strategies remains uncertain and subject for future research.

Rationale behind AF ablation

The major impact of AF on cardiovascular morbidity and mortality has driven researchers and physicians to find ways to restore and maintain sinus rhythm. It is generally accepted that the pathophysiology of AF includes a trigger to initiate AF, a substrate to maintain AF, and modulating risk factors, ultimately resulting in progression to more persistent forms of AF [58]. Over the years, AF ablation strategies have targeted elimination of AF triggers or modification of

the arrhythmogenic substrate. Ablation lesions are created to produce non-conductive tissue isolating triggers that initiate AF, and interrupt arrhythmogenic pathways in patient-specific AF substrate, or modulate autonomic innervation of the atria [7, 59, 60].

Recent results from the randomized CABANA trial comparing ablative therapy to medical therapy for the treatment of AF showed no significant benefit of CA over medical therapy in reduction of the composite end point of death, disabling stroke, serious bleeding, or cardiac arrest [61]. However, treatment crossover and lower event rates than anticipated might have affected the disappointing results of the CABANA trial. Of note, the trial did show more favorable quality of life outcomes at 12 months following CA compared to medical therapy [62]. Therefore, whether AF ablation can reduce morbidity or mortality remains unclear. Meanwhile, symptom reduction and QOL improvement remain the primary indication for catheter ablation [8].

AF ablation and heart failure

Recent studies suggested AF ablation with restoration of sinus rhythm can improve morbidity and mortality in patients with heart failure. The AATAC study comparing CA with amiodarone resulted in reduction of hospitalization and mortality in persistent AF patients with heart failure [63]. The prospectively randomized CASTLE-AF trial reported similar results, in which CA of AF resulted in a lower rate of hospitalization and mortality in patients with heart failure compared to medical therapy [64].

Present AF ablation techniques and energy sources

3D mapping and creation of a transmural and contiguous ring of scar tissue around the PVs with point-by-point RF ablation can be technically challenging, particularly at less experienced centers. Over the past years, different 3D mapping and catheter ablation systems using various energy sources have been developed to improve catheter handling, thereby enhancing safety, efficiency and efficacy of these ablation procedures. Among these are balloon-based technologies using a variety of energy sources, circular multi-electrode, and contact force tip electrode systems. For surgical ablation, clamp devices have been developed to improve lesion quality. In this section, we will review different ablation technologies that are used for AF ablation.

Radiofrequency point-by-point ablation

RF myocardial ablation is a thermal-mediated method in which localized heat generation is used to create tissue

necrosis and formation of ablation lesions. Continuous lesions are created in a point-by-point manner usually guided by a dedicated 3D electro-anatomical mapping system. The thermal effect is generated by delivering an electrical current through myocardial tissue from the tip electrode of the ablation catheter to a large dispersive electrode patch (unipolar) or between a pair of electrodes from adjacent ablation catheters (bipolar), causing resistive heating of the underlying tissue at the electrode tip (unipolar) or resistive heating of tissue between two catheter electrodes (bipolar). Myocardial cells become irreversibly damaged when exposed to temperatures of 50 °C or higher, leading to necrosis and eventually to nonconducting myocardial fibrotic scar tissue. If the temperature at the electrode exceeds 100 °C, boiling of blood occurs, resulting in clot and char formation [65]. If the intramyocardial temperatures exceeds 100 °C, boiling of tissue can lead to steam formation (pop lesion) potentially causing intramyocardial rupture and tissue perforation [66]. Factors that affect lesion size include electrode size, temperature, electrode–tissue contact, power and duration of RF energy delivery [65, 67]. Furthermore, heat loss to circulating blood on endocardial side and to epicardial coronaries can compromise lesion formation [65]. RF ablation lesions in PVI often consist of a combination of myocardial necrosis and tissue edema, often resulting in partially reversible myocardial lesions [68]. This latter can appear as irreversible lesions but lead to PV-reconnection later, which is associated with recurrence of atrial arrhythmias after ablation [69–71]. Higher power RF energy delivery can increase lesion size and depth but also increases the risk of temperature rise and char formation and collateral damage to structures such as esophagus and phrenic nerve. To allow higher power RF energy delivery, saline irrigation of the catheter tip electrode was developed to improve conductive heating of the underlying tissue while reducing temperature rise in the circulating blood. Saline-irrigated RF ablation results in deeper and larger lesions [66]. Currently, point-by-point RF ablation is most commonly performed using ablation catheter tip electrode irrigation with saline. To improve electro-tissue contact, catheters have been developed that are capable of measuring contact force between the catheter tip and tissue during ablation [72, 73]. RF ablation catheters with a contact force sensor improved outcome of AF ablation in the hands of experienced operators. Contact force of more than 10 g was associated with higher rates of arrhythmia-free survival [74].

Although point-by-point RF ablation is the most commonly applied technique to achieve PVI, the procedure remains technically challenging, even in experienced centers. Potential complications associated with the RF point-by-point ablation technique include cardiac tamponade (0.2–5%) [8, 75], stroke and transient ischemic attack (0–2%) [8, 76], esophageal damage including atrio-esophageal

fistulae (0.02–0.11%) [8, 77], and PV stenosis (< 1%) [8, 78].

Multielectrode circumferential RF catheter

Multielectrode circumferential RF ablation catheters were designed to make PVI procedures less complex and time consuming. The currently available multielectrode PV ablation catheters contain nine to ten electrodes with a circular configuration when deployed. These catheters can be navigated to the PV ostium by fluoroscopy, enabling both mapping and ablation. The circumferential placement of the electrodes allows the creation of a circular ablation lesion at the PV ostium after multiple applications, eventually resulting in PVI. The first-generation multielectrode catheter is no longer in use due to its association with asymptomatic cerebral embolisms, which was related to overlap of the first and tenth electrode leading to tissue and blood overheating causing thromboembolisms [79, 80]. Currently, one multielectrode circumferential ablation catheter system is available for clinical practice; the second-generation gold multielectrode ablation catheter (PVAC GOLD™, Medtronic, Minneapolis, MN, USA) containing 9 gold-plated electrodes. PVI with the use of PVAC multielectrode ablation was associated with significantly shorter procedure, fluoroscopy, and radiofrequency energy times [81]. However, comparison of multielectrode PVAC PVI to standard point-by-point irrigated RF ablation PVI showed conflicting data; some studies showed comparable outcomes while others significantly lower long-term atrial arrhythmia-free survival with the PVAC. Currently, available data on efficacy of multielectrode PVAC ablation are scarce and conflicting. Therefore, more prospective and randomized studies on this subject are needed.

Cryoballoon ablation

In cryoballoon ablation (Arctic Front Advance™, Medtronic, Inc., Minneapolis, MN, USA; POLARx™ Cryoablation Catheter, Boston Scientific, Marlborough, MA, USA), PVI is achieved by freezing tissue using a pressurized balloon that occludes the PV ostium and injecting liquid nitrous oxide as refrigerant into the balloon. Freezing tissue below –40 °C causes irreversible cell death due to freezing of intracellular water that results in irreversible disruption of organelles and cell membranes [82]. The commonly used second-generation cryoballoon (Arctic Front Advance, Medtronic, Inc. Minneapolis, MN, USA) catheter has a refrigerant injection system with 8 injection jets. The catheter has a lumen that can be used to pass a guide wire or a mapping catheter to guide balloon position and record PV potentials during ablation. The balloon catheter can be placed at the PV ostia without the use of 3D electro-anatomic navigation systems, and the balloon design allows circumferential ablation in a so

called ‘single shot’ manner. The aim of this balloon design was to shorten and simplify PVI ablation procedures. Cryoablation has become the most frequently used alternative energy source to RF for AF ablation. In the multicenter randomized Fire and Ice trial, cryoballoon and point-by-point RF ablation were shown to be equally effective and safe for the treatment of paroxysmal AF [83]. However, procedure duration and left atrial dwell time were shorter in the cryoballoon group, whereas fluoroscopy time was shorter in the RF group [83]. The most commonly reported complication in cryoballoon ablation is phrenic nerve injury with a reported incidence between 2 and 5%, fortunately often of temporary nature [84, 85]. Recently, presented results from the YETI registry containing data from 5371 patients treated with second-generation cryoballoon shows an incidence of phrenic nerve injury incidence of 3.9%, of which 57.5% were resolved at the end of the procedure. After 12 months, most of the phrenic nerve injuries were recovered, with an incidence of persistent phrenic nerve injury of only 0.08% [86].

Laser balloon

Laser balloon ablation (Heartlight™, CardioFocus, Marlborough, MA, USA) is a balloon-based technology using laser energy to create circumferential cell necrosis and achieve PVI. The laser balloon consists of a compliant balloon that fits into the PVs irrespective of variability in PV sizes and shapes. Unique to the device is the incorporation of a fiber optic endoscope to provide direct visualization of the target tissue in the antrum of the PVs [87]. Once positioned in the PV, the laser source emits energy to the exposed PV antral tissue. The intensity of the laser energy application can be titrated from 5.5 to 12 W, usually during 20–30 s for the formation of each ablation lesion. Lower laser energy setting is usually applied to reduce the risk of heating blood and charring when the occlusion is suboptimal and blood is present in the targeted ablation field. Laser energy output is also lowered when the targeted tissue is in the vicinity of the esophagus or phrenic nerve. Higher laser energy dose can be applied to the remaining PV segments resulting in more durable PVI lesions [88]. A frequently observed complication in laser balloon ablation is phrenic nerve injury, fortunately often of a temporary nature [89]. In a meta-analysis, efficacy and safety of the laser balloon were comparable to other AF ablation techniques [89]. (Fig. 1).

Future ablation strategies and technologies

Over the past years, advances have been made in catheter-based AF ablation technologies and strategies. Achieving durable PVI lesions safely and rapidly remains challenging. Driven by AF recurrences after ablation and the occurrence

of severe complications including cerebral embolism, esophageal damage, phrenic nerve palsy, investigators continue their search for more effective and safe ablation strategies and technologies.

Ablation line contiguity index

Although contact force-guided PVI is associated with improved arrhythmia-free outcome compared to conventional RF, reconnection of the PVs after ablation is still observed. The PV reconnection is explained by discontinuous and insufficient lesion depth in the circular lesion sets. Optimized and protocolized ablation strategies are developed aiming at creating contiguous and transmural RF lesions that might improve PV isolation durability.

The ablation line contiguity index (ablation index) is a novel measure assessing both contiguity and lesion depth, which can be used as a measure to detect weak spots in the set of created PV antral ablation lesions and LA anterior lines [90, 91]. The ablation index incorporates ablation contact force, time, and power in one marker using a weighted formula, and provides an accurate estimation of lesion depth [92]. Studies that used target values of 550 for anterior and 400 for posterior LA regions demonstrated to prevent PV reconnection [93, 94]. The measure has been integrated in automated lesions tagging software for 3D electro-anatomic mapping to visualize lesion ablation index and target values. Performing contact force RF ablation according to a specific ablation protocol that incorporates the ablation index improved procedural and 1 year outcome of contact force PVI while shortening procedure time [95, 96].

High-power short-duration RF ablation

Recent studies investigated higher RF energy output with shorter pulses in AF ablation to improve safety and create more durable lesions [97–99]. This high-power short-duration (HPSD) ablation strategy comprises the use of higher RF power (45–50 W) and shorter duration of each RF energy application (5–15 s) instead of conventional lower RF power (25–30 W) and longer duration of applications (30–60 s). With HPSD, the short duration of RF energy application results in more local resistive heating and local atrial tissue destruction without conductive heating of more distant tissues, such as the esophagus, preventing collateral damage [99, 100].

The HPSD ablation strategy has been shown to improve contiguity and transmural of atrial linear lesions in animal models [97]. Furthermore, HPSD was associated with shorter procedural and RF time compared with conventional RF ablation and, appears to be a safe approach [98–100]. Recent studies have investigated even higher power settings. PVI is achieved with 90 W applications for 4 s per ablation

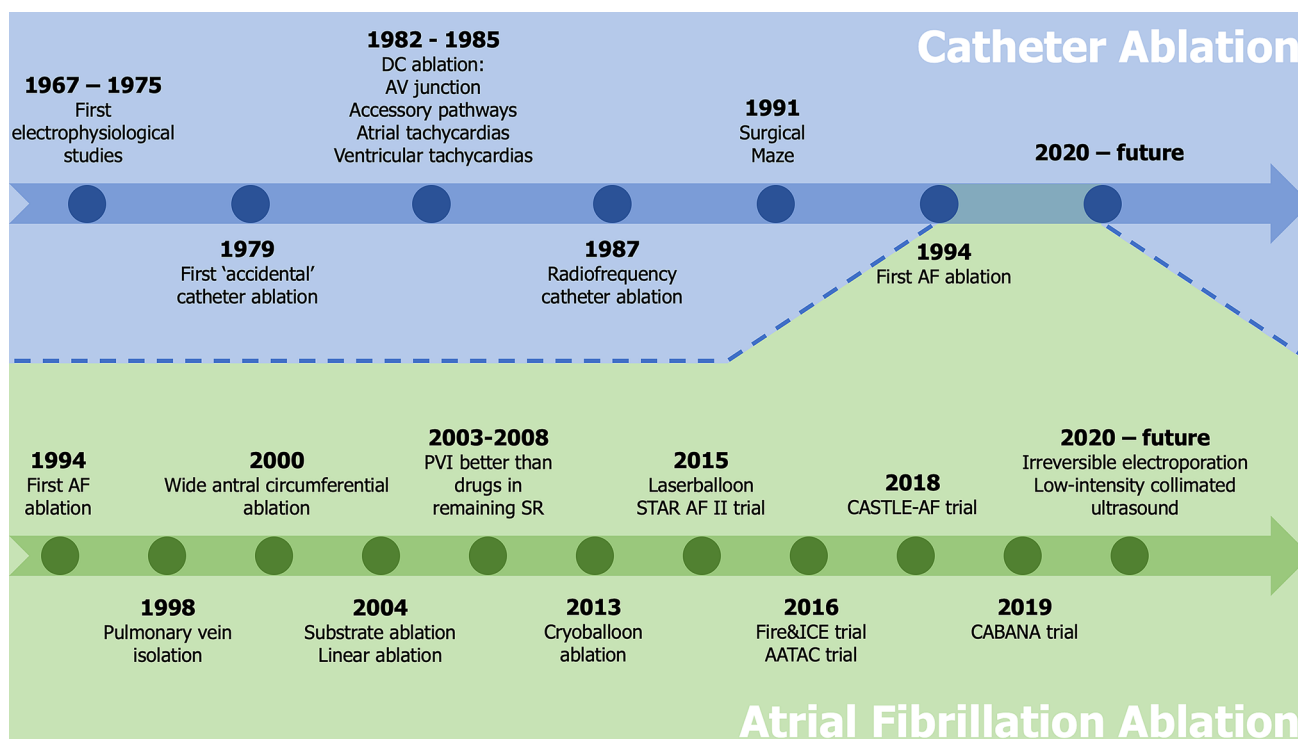


Fig. 1 Timeline of key findings in catheter ablation of atrial fibrillation research. AF atrial fibrillation, AV atrioventricular, DC direct current, PVI pulmonary vein isolation, SR sinus rhythm. AATAC Ablation versus Amiodarone for Treatment of AF in Patients With Congestive Heart Failure and an Implanted ICD/CRTD, CABANA Catheter Ablation versus Antiarrhythmic Drug Therapy for Atrial

Fibrillation, CASTLE-AF Catheter Ablation versus Standard Conventional Therapy in Patients with Left Ventricular Dysfunction and AF, FIRE&ICE Cryoballoon or Radiofrequency Ablation for Paroxysmal AF. STAR-AF II trial the Substrate and Trigger Ablation for Reduction of AF Trial Part II

point, with a computerized algorithm modulating power to maintain target temperature [97, 101]. A first-in-human study showed feasibility of achieving PVI with 90 W HPSD ablation in 52 patients. At 3 month follow-up, 49 patients (94.2%) were in sinus rhythm, and the occurrence of serious adverse events was low (3.8%) [101]. In another recently published study, a HPSD ablation protocol with 70 W for 5–7 s was compared to conventional (30–40 W for 20–40 s) ablation, in patients undergoing PVI for paroxysmal AF. The HPSD group showed significantly less AF recurrences 1 year after ablation, with 83.1% freedom from AF compared to 65.1% in the conventional group. Safety profiles were similar between the groups, and significantly shorter radiofrequency and procedural time were observed with HPSD [102].

Novel technologies in multielectrode RF balloon ablation

Several multielectrode RF balloon catheters have been developed for PVI. Similar to point-by-point RF ablation, PVI is achieved by RF energy resulting in thermal injury. The balloon design aims to shorten and simplify PVI ablation procedures. Data on these multielectrode RF balloon

systems are limited to experimental and first-in-human studies. The Heliostar multielectrode RF balloon catheter (Biosense Webster Inc, Irvine, CA, USA) contains 10 gold-plated and irrigated electrodes mounted around a balloon in a circular configuration. The RF balloon is advanced to the left atrium using an over-the-wire design and positioned at the PV ostia. Different RF energy settings can be programmed for each individual electrode to control temperature during ablation, particularly at sites that are in vicinity of sensitive structures (e.g. phrenic nerve and esophagus). This device allows the operator to create circumferential PVI lesions in a single shot manner without the need for catheter extensive manipulation, while preventing collateral damage. First-in-human results from the RADIANCE trial, showed feasibility and safety of achieving PVI in 39 patients with paroxysmal AF. Acute PVI was achieved in all the patients, and 79.6% of the PVs was isolated with a single application. In this limited series, one case of phrenic nerve palsy was observed [103].

The Luminize™, another RF balloon system (Boston Scientific, Marlborough, MA, USA) formerly known as the Apama RF balloon (Apama Medical Inc, Campbell, CA, USA), is an over-the-wire balloon catheter, containing 12 proximal (equatorial) electrodes and 6 distal electrodes.

The technology incorporates four built-in cameras and LED illumination that allows direct visualization of the targeted area of interest for ablation. Furthermore, both mapping and pacing from the ablation electrodes are possible. The first-in-human results presented at the European Heart Rhythm Association Congress (Lisbon, Portugal, 2019) demonstrated safety and efficacy in achieving PVI in patients with paroxysmal AF [104]. Successful PVI was achieved in 98% of all the PVs and no serious adverse events were observed during a follow up of 30 days.

The Globe system (The Globe[®] system, Kardium Inc., Burnaby, BC, Canada) is a multielectrode catheter containing globe-shaped expanding array of 122 electrodes that can be deployed in the left atrium. Each individual electrode can perform sensing, pacing, and measurement of tissue contact, temperature and impedance. Ablation is achieved using RF energy that can be applied on each individual electrode up to 24 electrodes simultaneously. The catheter is designed to combine diagnostic mapping capabilities of basket catheters with the simplicity of the use of balloon catheters for ablation. First-in-human experience showed that PV isolation could be performed using this new multielectrode array catheter [105]. The safety and efficacy of the catheter are still under investigation.

Although feasibility and safety were shown for these novel multielectrode RF balloon catheters, more patient data and long-term follow-up are warranted. Furthermore, randomized studies are needed to assess the potential benefit regarding procedural time, safety and efficacy of these novel catheters compared to other (balloon based) ablation techniques.

Irreversible electroporation

Irreversible electroporation (IRE), also referred to as pulsed field ablation, is a novel nonthermal ablative modality in which ultrarapid (< 1 s) electrical fields (monophasic waveforms 900–1000 V and biphasic waveforms, 800–2000 V per application) are applied to target tissue. This approach destabilizes cell membranes by forming irreversible nanoscale pores and leakage of cell contents, culminating in cell death [106]. Importantly, various tissues have specific characteristic thresholds to field strengths that induce necrosis by electroporation. Of note, myocardial tissue has the lowest threshold and is thus most sensitive tissue for irreversible electroporation. Therefore, in contrast to any other energy source, IRE spares collateral structures such as the esophagus, arteries and nerves while effectively ablating myocardial tissue. Potential benefits of IRE include the tissue selectivity of

the ablation, and the rapid delivery of the energy, potentially resulting in shorter procedure times. Experimental data demonstrated that IRE can be a safe treatment modality for ablation in the vicinity of important structures such as the coronary arteries, the right phrenic nerve, and the esophagus, consistent with the tissue selectivity data derived from animal studies [107–109]. The first-in-human experience with IRE ablation for PVI in patients with AF was recently reported [110, 111]. Feasibility of achieving acute PVI by IRE ablation was shown using different catheter designs, including a 14-polar circular catheter [110] and an over-the-wire catheter with a deployable basket containing 20 separate electrodes [112].

Low-intensity collimated ultrasound

Low-intensity collimated ultrasound (LICU) (VytronUS, Inc., Sunnyvale, California) is a novel ablation technique designed to integrate anatomic mapping and ablation capabilities in a single catheter [113]. The catheter contains an irrigated tip with an ultrasound transducer. The catheter tip allows automatic construction of two- and three-dimensional maps of the scanned left atrial area of interest with a maximal depth of 40 mm. Ablation is performed using a highly collimated ultrasound beam that is absorbed by the atrial tissue and results in thermal injury with an estimated maximum depth of 17 mm. Ablation is performed with the support of a robotic system after definition of the ablation trajectories on a two-dimensional map by the operator. Feasibility of producing continuous transmural lesions in PVI ablation was shown in a porcine model [113]. However, available data on this novel ablation technique are limited to an experimental study. Results from the first-in-human study are awaited (Table 1).

Conclusion

Catheter ablation is an established treatment option for AF. Isolation of the PVs is the gold standard of catheter ablation of AF, but reconnection and conduction from the PVs is the dominant mechanism of recurrences of AF after PVI, especially in patients with paroxysmal AF. Novel technologies are under evaluation that have a great potential to facilitate creation of durable lesions with permanent PVI after a single ablation procedure. However, many of these novel technologies need to be tested clinically in well powered RCTs.

Table 1 Overview of upcoming trials on various topics in AF ablation

Study	Intervention	Inclusion	Primary outcome	Study design	ClinicalTrials.gov Identifier:
Substrate and trigger ablation					
Low voltage-directed catheter ablation for atrial fibrillation	<ol style="list-style-type: none"> Pulmonary vein isolation (PVI) alone PVI plus total left atrial low voltage-directed ablation PVI plus non-voltage-directed posterior wall ablation 	Non-paroxysmal AF	Freedom from atrial arrhythmia recurrence at 12 months	Randomized, multicenter estimated enrollment: 180 pts estimated completion: September 2022	NCT03355456
Substrate versus trigger ablation for paroxysmal atrial fibrillation (SUBSTRATE)	<ol style="list-style-type: none"> Substrate ablation for AF, via ablation of rotors and focal sources alone Trigger-based ablation for AF, using PVI alone 	Paroxysmal AF	Freedom from AF recurrence at 12 months	Randomized, multicenter estimated enrollment: 120 pts estimated completion: September 2021	NCT02169037
Efficacy of delayed enhancement MRI-guided ablation vs conventional ablation of atrial fibrillation (DECAAFII)	<ol style="list-style-type: none"> Catheter ablation guided by cardiac delayed enhancement-MRI prior procedure Conventional PVI 	Persistent AF	Freedom from AF recurrence at 18 months	Randomized, multicenter estimated enrollment: 900 pts estimated completion: July 2021	NCT02529319
MARSHALL PLAN Vs. pulmonary veins isolation monocentric trial (PLAN-MARSHALL)	<ol style="list-style-type: none"> Destruction of Marshall bundles by ethanol infusion + coronary sinus ablation Conventional PVI Mitral, roof, and cavo-tricuspid isthmus ablation 	Persistent AF	Freedom from AF and AT recurrence at 12 months	Randomized, single center estimated enrollment: 120 pts estimated completion: December 2021	NCT04206982

Table 1 (continued)

Study	Intervention	Inclusion	Primary outcome	Study design	ClinicalTrials.gov Identifier:
Ectopy triggering ganglionated plexus ablation to prevent atrial fibrillation (GANGLIA-AF)	1. Conventional PVI 2. Left atrial ganglionated plexus ablation	Paroxysmal AF	Freedom from atrial arrhythmia recurrence at 12 months	Randomized, multicenter estimated enrollment: 180 pts estimated completion: September 2020	NCT02487654
Heart failure					
Atrial fibrillation treatment with cryoballoon in heart failureE (AFICHE)	1. Cryoballoon PVI +heart failure drugs 2. Rhythm control drugs + heart failure drugs	AF and LVEF <40% and heart failure symptoms (NYHA II or higher)	The time to AF burden exceeding 1% at 2 years	Randomized, single center estimated enrollment: 404 pts estimated completion: June 2022	NCT03573869
Ablation versus medical management of atrial fibrillation in HFpEF (AMPERE)	1. Conventional PVI 2. Medical management	Paroxysmal, persistent or long-standing persistent AF and heart failure symptoms (NYHA II or higher) and LVEF > 50%	Change in AF burden on ILR at 12 months	Randomized, single-center, pilot study estimated enrollment: 60 pts estimated completion: June 2025	NCT04282850
Treatment Of atrial fibrillation in preserved cardiac function heart failure (TAP-CHF)	1. Conventional PVI 2. Antiarrhythmic drug therapy	Paroxysmal or persistent AF and HFpEF	Time to composite of heart failure hospitalizations and/or cardiovascular mortality	Randomized, multicenter estimated enrollment: 360 pts estimated completion: June 2025	NCT04160000
Stroke prevention					
Stroke secondary prevention with catheter ablation and edoxaban for patients with non-valvular atrial fibrillation: STABLED study (STABLED)	1. Standard medical therapy with DOAC 2. Conventional PVI 1–6 months from cerebral infarction and DOAC	Nonvalvular AF and history of stroke in previous 6 months	Time to composite of recurrence of cerebral infarction, systemic embolism, all-cause death, hospitalization for heart failure at 5 years	Randomized, single center estimated enrollment: 250 pts estimated completion: September 2023	NCT03777631

AF atrial fibrillation, AT atrial tachycardia, HFpEF heart failure with preserved ejection fraction, ILR implantable loop recorder, PVI pulmonary vein isolation, MRI magnetic resonance imaging

Funding No funding.

Compliance with ethical standards

Conflict of interest The authors declare that they have no conflict of interest.

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