



Diffusion kurtosis imaging and dynamic contrast-enhanced MRI for the differentiation of parotid gland tumors

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Abstract

Objective To assess the usefulness of combined diffusion kurtosis imaging (DKI) and dynamic contrast-enhanced MRI (DCE-MRI) in the differentiation of parotid gland tumors.

Methods Seventy patients with 80 parotid gland tumors who underwent DKI and DCE-MRI were retrospectively enrolled and divided into four groups: pleomorphic adenomas (PAs), Warthin tumors (WTs), other benign tumors (OBTs), and malignant tumors (MTs). DCE-MRI and DKI quantitative parameters were measured. The Kruskal–Wallis H test and post hoc test with Bonferroni correction and ROC curve were used for statistical analysis.

Results WT demonstrated the highest K_{ep} value (median 1.89, interquartile range [1.46–2.31] min^{-1}) but lowest V_e value (0.20, [0.15–0.25]) compared with PAs (K_{ep} , 0.34 [0.21–0.55] min^{-1} ; V_e , 0.36 [0.24–0.43]), OBTs (K_{ep} , 1.22 [0.27–1.67] min^{-1} ; V_e , 0.28 [0.25–0.41]), and MTs (K_{ep} , 0.71 [0.50–1.23] min^{-1} ; V_e , 0.35 [0.26–0.45]) (all $p < .05$). MTs had the lower D value (1.10, [0.88–1.29] $\times 10^{-3}$ mm^2/s) compared with PAs (1.81, [1.60–2.20] $\times 10^{-3}$ mm^2/s) and OBTs (1.57, [1.32–1.89] $\times 10^{-3}$ mm^2/s) (both $p < .05$). PAs had the lower K^{trans} value (0.12, [0.07–0.18] min^{-1}) compared with OBTs (0.28, [0.11–0.50] min^{-1}) ($p < .05$). The cutoff values of combined K_{ep} and V_e , D , and K^{trans} to distinguish WT, MT, and PA sequentially were 1.06 min^{-1} , 0.28, 1.46×10^{-3} mm^2/s , and 0.21 min^{-1} , respectively (accuracy, 89% [71/80], 91% [73/80], 78% [62/80], respectively).

Conclusion The combined use of DKI and DCE-MRI may help differentiate parotid gland tumors.

Key Points

- The combined use of DKI and DCE-MRI could facilitate the understanding of the pathophysiological characteristics of parotid gland tumors.
- A stepwise diagnostic diagram based on the combined use of DCE-MRI parameters and the diffusion coefficient is helpful for accurate preoperative diagnosis in parotid gland tumors and may further facilitate the clinical management of patients.

Keywords Parotid gland · Parotid neoplasms · Magnetic resonance imaging · Diffusion · Perfusion

Nan Huang and Yu Chen are co-first authors and contributed equally to this study.

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Abbreviations

BCA	Basal cell adenoma
D	Diffusion coefficient
DCE-MRI	Dynamic contrast-enhanced MRI
DKI	Diffusion kurtosis imaging
iAUC	Initial area under the contrast agent concentration–time curve
IQR	Interquartile range
K	Diffusion kurtosis
K_{ep}	Rate constant from extravascular extracellular space to plasma
K^{trans}	Transfer constant from plasma to extravascular extracellular space
MT	Malignant tumor
OBT	Other benign tumor

PA	Pleomorphic adenoma
PGT	Parotid gland tumor
V_e	Fractional volume of the extravascular extracellular space
WT	Warthin tumor

Introduction

Parotid gland tumors (PGTs) contain abundant histological types and subtypes including pleomorphic adenomas (PAs), Warthin tumors (WTs), other benign tumors (OBTs), and malignant tumors (MTs). The treatment strategy and long-term prognosis vary widely depending on the histological type of the tumors [1]. Compared with benign tumors, total parotidectomy with radiotherapy is preferred in the malignancies [2, 3]. In the treatment decision of benign tumors, for patients with PAs, they may require complete surgical excision due to the potential for recurrence and malignant transformation [4], whereas patients with WTs and OBTs, local or superficial parotidectomy, or conservative observation may be sufficient [3]. Therefore, precise preoperative diagnosis is of great importance.

Conventional MRI can delineate lesions concerning the internal structure, morphology, accurate localization, locoregional extension, invasion, and perineural spread of tumors,

but the diagnostic performance is limited [3], particularly when benign tumors have similar imaging findings to low-grade malignant tumors showing low signal on T1WI and high signal on T2WI [5]. Advanced MRI techniques like diffusion MRI and perfusion MRI may provide the information of intratumoral water molecular diffusion, microstructural complexity, and capillary blood flows [6, 7]. DKI, a sophisticated modality that quantifies the non-Gaussian behavior of water molecule diffusion, can provide information about heterogeneity and cellularity in vivo with two parameters [8], including diffusion kurtosis (K) and diffusion coefficient (D), and has been proven to be useful in the field of parotid gland lesions [9, 10]. However, DKI used alone may not fully reflect the pathophysiological characteristics of PGTs. Moreover, DCE-MRI monitors T1 changes in tumor tissues over time after contrast administration of gadolinium to quantify the tumor perfusion and vessel permeability [11, 12]. A quantitative evaluation can be made with perfusion parameters including transfer constant (K^{trans}), rate constant (K_{ep}), fractional volume of the extravascular extracellular space (V_e), and initial area under the contrast agent concentration–time curve (iAUC) to identify benign and malignant lesions and monitor tumor responses to treatment in the head and neck [7]. Previous studies showed that quantitative DCE-MRI has played an important part in improving the diagnosis of parotid gland lesions [13–15]. However, those studies may

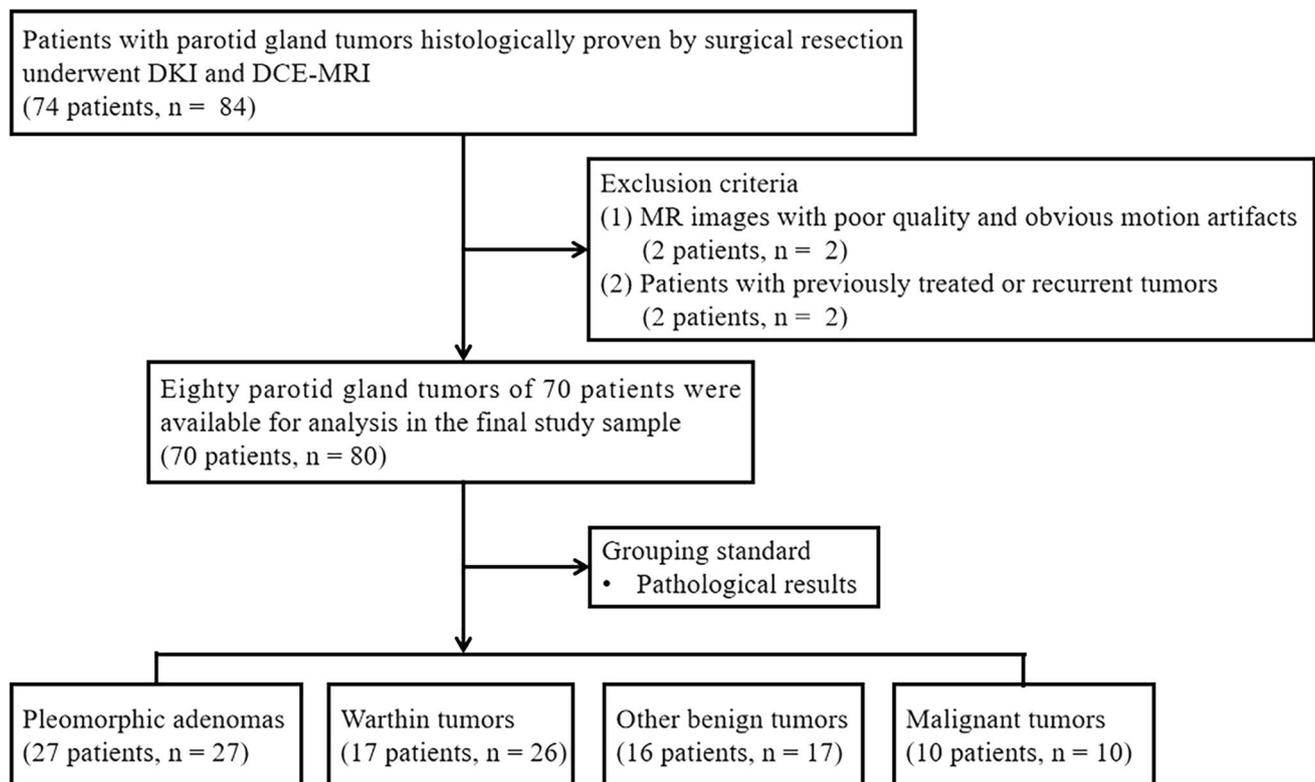


Fig. 1 Patients inclusion and exclusion flow diagram

have some limitations, such as the relatively small sample size. Up to now, none of the studies have demonstrated the added value of combining DKI and DCE-MRI for PGT characterization. We hypothesized that the combined use of DKI and DCE-MRI could reflect the discrepancies in diffusion and perfusion of PGTs. Therefore, the purpose of this study was to evaluate whether DKI and DCE-MRI quantitative parameters are beneficial for differentiating PGTs.

Materials and methods

Patients

The Institutional Review Board of our hospital approved this retrospective study, and the requirement of written informed consent was waived. Between January 2018 and September 2019, a total of 74 consecutive patients with PGTs histologically proven by surgical resection and available DKI and DCE-MRI sequences were retrospectively recruited. Of these patients, 4 were excluded because of MR images with poor quality and obvious motion artifacts ($n=2$), and previously treated or recurrent tumors ($n=2$). Finally, 70 patients with 80 lesions were included in this study and were divided into four groups including PAs ($n=27$), WTs ($n=26$), OBTs ($n=17$), and MTs ($n=10$) (Fig. 1). The OBTs group included 11 basal cell adenoma (BCA), 3 schwannoma, 1 hemolymphangioma, 1 oncocytic adenoma, and 1 cystadenoma. The MTs group included 4 mucoepidermoid carcinoma, 2 lymphoma, 1 carcinoma ex pleomorphic adenoma, 1 acinic cell carcinoma, 1 salivary duct carcinoma, and 1 mammary analog secretory carcinoma.

MRI protocol

All patients underwent MRI on a 3.0-T scanner (Skyra; Siemens Healthcare) with a 20-channel head/neck coil. Conventional MRI protocols were obtained first, then DKI using single-shot echo-planar imaging with fat suppression was performed with b-factors of 0, 1000, 1500, 2000, and 2500 s/mm^2 with diffusion gradient applied along all

three orthogonal gradient diffusion directions. T1 mapping was performed prior to DCE-MRI sequence. A dose of 0.1 mmol/kg of gadobenate dimeglumine (Gd-DTPA, MultiHance, Bracco Diagnostics) was intravenously administered through the median cubital vein at the rate of 2 ml/s, followed by a 15-ml flush of saline. The parameters of MR sequences are listed in Supplementary Material 1.

Image processing and analysis

The DCE-MRI processing was dealt with the commercial software tool (Tissue 4D, Syngo.via; Siemens Healthcare). The post-processing procedures are demonstrated in Supplementary Material 2.

DKI images were processed using prototype software (Body diffusion toolbox, Siemens Healthcare) and Diffusional Kurtosis Estimator (DKE, version 2.5.1, www.musc.edu/cbi). The DKI model is described as the following formula [16]:

$$\frac{S(b)}{S_0} = \exp\left(-b \cdot D + \frac{1}{6}b^2D^2 \cdot K\right),$$

where D represents the diffusion coefficient for non-Gaussian distribution and K represents the diffusion kurtosis coefficient [17].

For evaluation of DCE-MRI data, the values of quantitative parameters were automatically calculated by placing a single region of interest (ROI) manually in the largest enhanced solid portion of the lesion, excluding blood vessel, hemorrhagic, necrotic, and cystic regions referred to T2WI and contrast-enhanced T1WI. The corresponding ROIs were drawn on DKI maps for K and D values using the ImageJ software (version 1.8, National Institutes of Health). Image analysis was conducted separately by two radiologists blinded to histological diagnosis (Y.C. and N.H., with 2 and 8 years of experience in head and neck imaging, respectively). The quantitative measurement results of two readers were used to evaluate the interobserver agreement. The quantitative parameter results measured repeatedly by reader 1 with at least 1-month interval were used to evaluate intraobserver agreement. Finally, the measurement results of reader 1 were used for statistical analysis.

Table 1 Patient demographic information

Parameter	Pleomorphic adenomas	Benign tumors		Malignant tumors	Total	<i>p</i> value*
		Warthin tumors	Other benign tumors			
No. of patients	27	17	16	10	70	
No. of men	7	14	8	5	34	> .99
Age (year)	45 ± 13 (21–66)	59 ± 9 (42–78)	57 ± 15 (38–78)	46 ± 14 (21–69)	51 ± 14 (21–78)	.20

Mean values are ± standard deviation. Data in parentheses are ranges

**p* values are for the differences between benign and malignant tumors

Table 2 DKI and DCE-MRI parameters of PGTs and Kruskal–Wallis *H* test with Bonferroni correction

Parameters	<i>p</i> value ^a				<i>p</i> value ^b					
	PA	WT	OBT	MT	PA vs WT	PA vs OBT	PA vs MT	WT vs OBT	WT vs MT	OBT vs MT
DKI parameters										
<i>K</i>	0.51 (0.47–0.62)	0.99 (0.84–1.09)	0.64 (0.56–0.71)	0.87 (0.69–1.01)	<.001*	.06	.001*	<.001*	>.99	.12
<i>D</i> ($\times 10^{-3}$ mm ² /s)	1.81 (1.60–2.20)	0.97 (0.89–1.27)	1.57 (1.32–1.89)	1.10 (0.88–1.29)	<.001*	.90	<.001*	<.001*	>.99	.03*
DCE-MRI parameters										
<i>K</i> ^{trans} (min ⁻¹)	0.12 (0.07–0.18)	0.38 (0.28–0.45)	0.28 (0.11–0.50)	0.30 (0.14–0.50)	<.001*	.008*	.009*	.83	>.99	>.99
<i>K</i> _{ep} (min ⁻¹)	0.34 (0.21–0.55)	1.89 (1.46–2.31)	1.22 (0.27–1.67)	0.71 (0.50–1.23)	<.001*	.06	.20	.01*	.047*	>.99
<i>V</i> _e	0.36 (0.24–0.43)	0.20 (0.15–0.25)	0.28 (0.25–0.41)	0.35 (0.26–0.45)	<.001*	>.99	>.99	.001*	.001*	>.99
iAUC (mmol/s/kg)	0.13 (0.08–0.22)	0.25 (0.21–0.30)	0.24 (0.10–0.37)	0.32 (0.18–0.37)	<.001*	.09	.007*	>.99	>.99	>.99

DKI diffusion kurtosis imaging, DCE-MRI dynamic contrast-enhanced MRI, PGTs parotid gland tumors, PA pleomorphic adenoma, WT Warthin tumor, OBT other benign tumor, MT malignant tumor, *K* diffusion kurtosis, *D* diffusion coefficient, *K*^{trans} transfer constant from plasma to extravascular extracellular space, *K*_{ep} rate constant from extravascular extracellular space to plasma, *V*_e fractional volume of the extravascular extracellular space, iAUC initial area under the contrast agent concentration–time curve. Data are medians with interquartile ranges in parentheses. *p* values^a from Kruskal–Wallis *H* test. *p* values^b are adjusted for pairwise comparison by using post hoc test with Bonferroni correction

*Significant difference (*p* < .05)

Statistical analysis

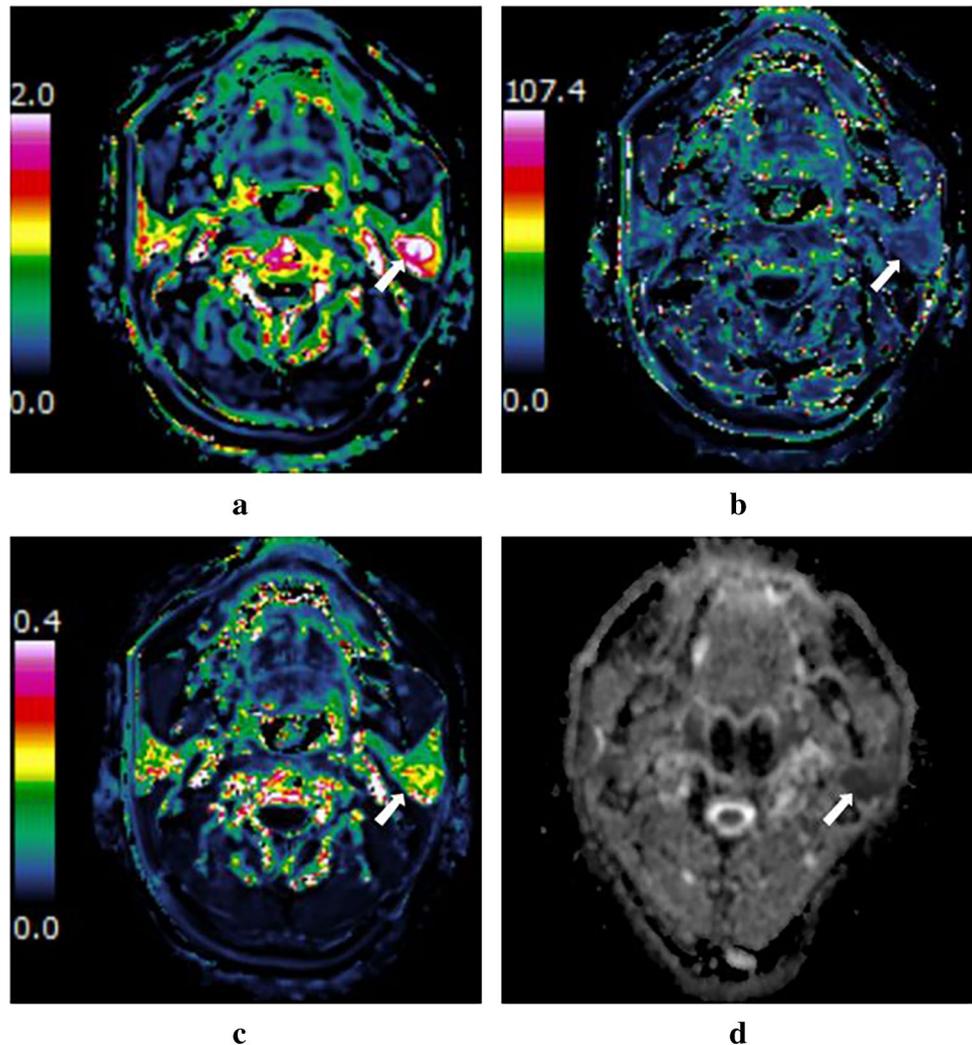
All numeric data were tested for normality using Kolmogorov–Smirnov’s test and for variance homogeneity using Levene’s test. The normally distributed variables were expressed as the means ± standard deviation and the non-normally distributed variables were expressed as medians (interquartile ranges, IQRs). A chi-square test was used to compare the discrepancy in sex between benign and malignant tumors. An independent samples *t*-test was made to compare the difference in age between the two groups. Mann–Whitney *U* test was used to compare DCE-MRI and DKI quantitative parameters between benign and malignant PGTs. The Kruskal–Wallis *H* test was made to test overall differences of quantitative parameters among four groups of PGTs. The post hoc test with Bonferroni correction was used for pairwise comparisons when the overall test was statistically significant. The intraclass correlation coefficient (ICC) with 95% confidence intervals (CIs) was used to assess the inter- and intraobserver agreement for quantitative parameters. The ICC > 0.61 was considered good agreement. The receiver operating characteristic (ROC) curve was drawn to ascertain diagnostic performance and optimal cutoff values of quantitative parameters. Then the area under the curve (AUC), sensitivity, specificity, positive predictive value (PPV), negative predictive value (NPV), and accuracy were further calculated. The combination of *K*_{ep} and *V*_e values for differentiating WTs from other three entities was based on the logistic regression analysis. The method developed by DeLong et al. [18] was used for comparisons of AUCs. Statistical analysis was performed using MedCalc statistical software (version 15.8, MedCalc), SPSS software (version 26.0, SPSS), and Graphpad Prism (version 6.0, GraphPad Software). *p* < 0.05 was considered statistically significant.

Results

Patients characteristics

The main demographic information of patients with PGTs is summarized in Table 1. The statistical results demonstrated that all numeric data were not normally distributed and equal variance except for the age. There was no significant difference in sex (*p* > 0.99) and age distribution (*p* = 0.20) between the benign and malignant groups. Fifty-six patients presented with palpable mass without tenderness, 11 patients felt swelling with pain, and the tumor was found during physical examination in 3 patients. One had facial nerve palsy.

Fig. 2 A 67-year-old man with Warthin tumor in the left parotid gland (white arrow). DCE-MRI parameter maps showed the K_{ep} (a), V_e (b), and K^{trans} (c) values of 2.02 min^{-1} , 0.19 , and 0.38 min^{-1} , respectively. **d** D map demonstrated that the mass showed hypointensity compared with neighboring normal-appearing muscle, with a D value of $0.90 \times 10^{-3} \text{ mm}^2/\text{s}$



DKI and DCE-MRI analysis between benign and malignant PGTs

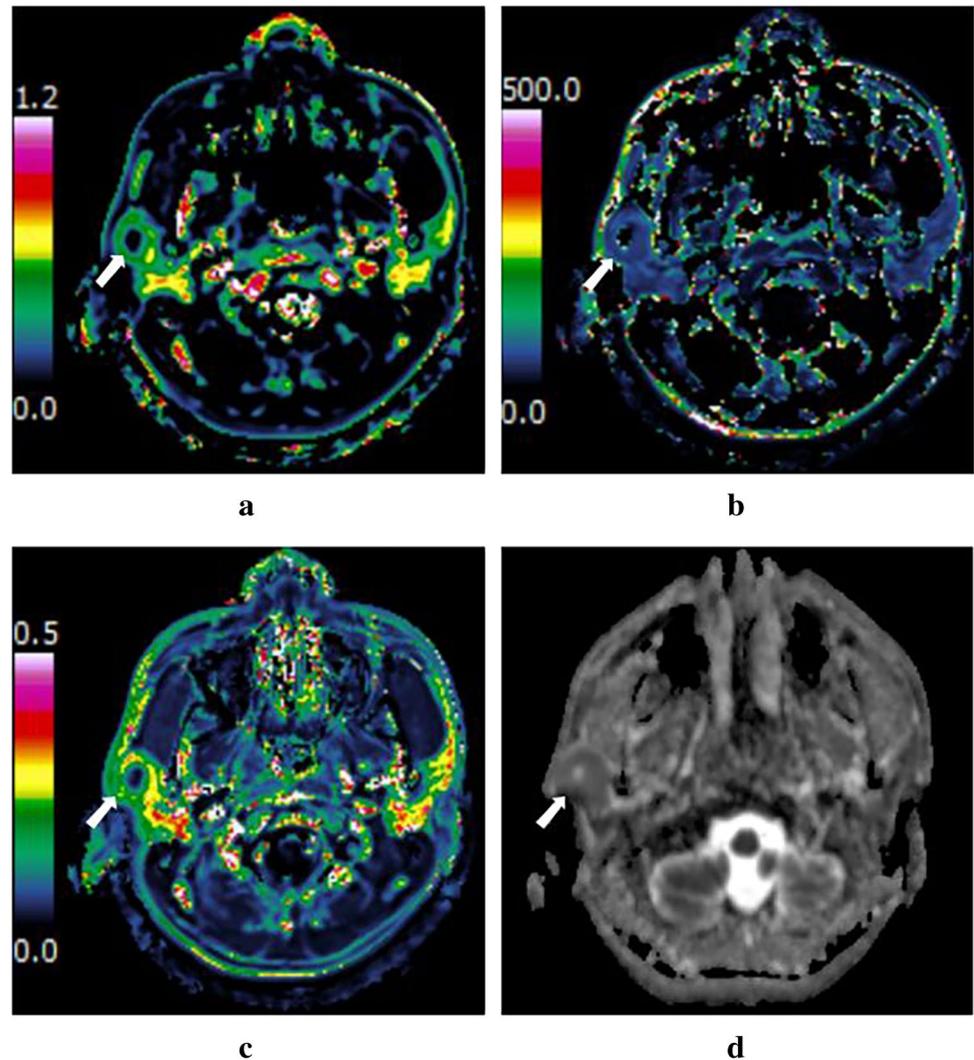
The comparisons of quantitative parameters between benign and malignant tumors are summarized in Supplementary Material 3 (Table E2). The D value of benign tumors (median 1.50 , IQR $[1.04\text{--}1.86] \times 10^{-3} \text{ mm}^2/\text{s}$) was significantly higher than that of malignant tumors (1.10 , $[0.88\text{--}1.29] \times 10^{-3} \text{ mm}^2/\text{s}$) ($p=0.02$). The cutoff value of D was $1.24 \times 10^{-3} \text{ mm}^2/\text{s}$ (AUC, 0.73 ; accuracy, 69% [$55/80$]) (Supplementary Material 3, Table E3). Additionally, there were insignificant differences in K , K^{trans} , K_{ep} , V_e , and iAUC values between the two groups (all $p > 0.05$).

DKI and DCE-MRI analysis between four groups of PGTs

The Kruskal–Wallis H test revealed that there were statistically significant differences in all quantitative

parameters among different groups of PGTs (all $p < 0.001$), and the comparisons of quantitative parameters of PGTs are summarized in Table 2. For DCE-MRI parameters, as exhibited in Figs. 2, 3, 4, and 5, the K^{trans} value of PAs (0.12 , $[0.07\text{--}0.18] \text{ min}^{-1}$) was significantly lower than that of WTs (0.38 , $[0.28\text{--}0.45] \text{ min}^{-1}$), OBTs (0.28 , $[0.11\text{--}0.50] \text{ min}^{-1}$), and MTs (0.30 , $[0.14\text{--}0.50] \text{ min}^{-1}$) (adjusted $p < 0.001$, $=0.008$, and 0.009 , respectively). Moreover, the K_{ep} value of WTs (1.89 , $[1.46\text{--}2.31] \text{ min}^{-1}$) was significantly higher than that of PAs (0.34 , $[0.21\text{--}0.55] \text{ min}^{-1}$), OBTs (1.22 , $[0.27\text{--}1.67] \text{ min}^{-1}$), and MTs (0.71 , $[0.50\text{--}1.23] \text{ min}^{-1}$) (adjusted $p < 0.001$, $=0.01$, and 0.047 , respectively). Meanwhile, the V_e value of WTs (0.20 , $[0.15\text{--}0.25]$) was significantly lower than that of PAs (0.36 , $[0.24\text{--}0.43]$), OBTs (0.28 , $[0.25\text{--}0.41]$), and MTs (0.35 , $[0.26\text{--}0.45]$) (adjusted $p < 0.001$, $=0.001$, and 0.001 , respectively). Additionally, the iAUC value of PAs (0.13 , $[0.08\text{--}0.22] \text{ mmol}\cdot\text{s}/\text{kg}$) was significantly lower than that of WTs (0.25 , $[0.21\text{--}0.30] \text{ mmol}\cdot\text{s}/\text{kg}$) and MTs (0.32 ,

Fig. 3 A 24-year-old man with mucoepidermoid carcinoma in the right parotid gland (white arrow). DCE-MRI parameter maps showed the K_{ep} (a), V_e (b), and K^{trans} (c) values of 0.90 min^{-1} , 0.61 , and 0.55 min^{-1} , respectively. **d** D map demonstrated that the solid portion of the mass showed hypointensity compared with neighboring normal-appearing muscle, with a D value of $1.46 \times 10^{-3} \text{ mm}^2/\text{s}$



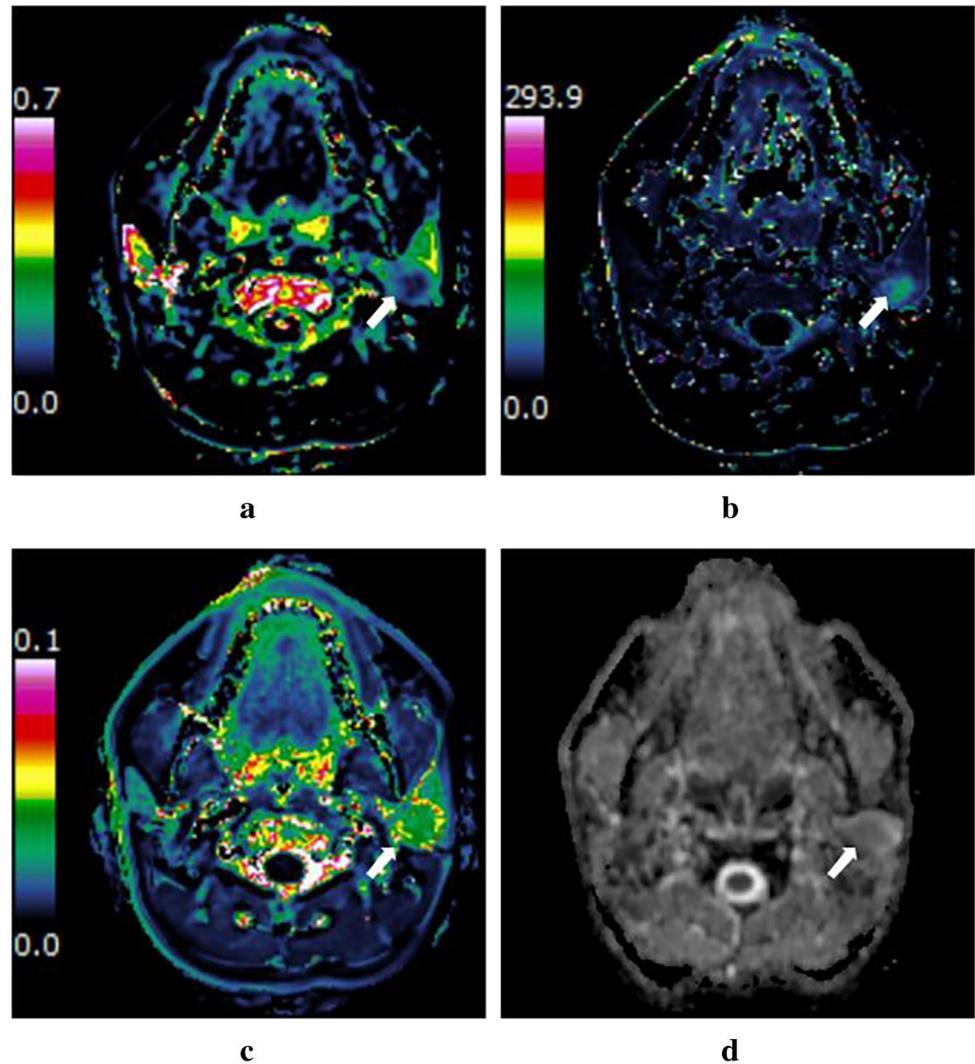
[$0.18\text{--}0.37$] $\text{mmol}\cdot\text{s}/\text{kg}$) (adjusted $p = 0.002$ and 0.007 , respectively).

For DKI parameters, the D values of both MTs (1.10 , [$0.88\text{--}1.29$] $\times 10^{-3} \text{ mm}^2/\text{s}$) and WTs (0.97 , [$0.89\text{--}1.27$] $\times 10^{-3} \text{ mm}^2/\text{s}$) were significantly lower than those of PAs (1.81 , [$1.60\text{--}2.20$] $\times 10^{-3} \text{ mm}^2/\text{s}$) (both adjusted $p < 0.001$ for MTs and WTs) and OBTs (1.57 , [$1.32\text{--}1.89$] $\times 10^{-3} \text{ mm}^2/\text{s}$) (adjusted $p = 0.03$ for MTs and < 0.001 for WTs), respectively. Moreover, the K value of PAs (0.51 , [$0.47\text{--}0.62$]) was significantly lower than that of MTs (0.87 , [$0.69\text{--}1.01$]) (adjusted $p = 0.001$); the K value of WTs (0.99 , [$0.84\text{--}1.09$]) was higher than that of PAs and OBTs (0.64 , [$0.56\text{--}0.71$]) (both adjusted $p < 0.001$).

The diagnostic performances between the four groups are summarized in Table 3. ROC analyses showed that in differentiating PAs from WTs, K (cutoff value, ≤ 0.72 ; AUC, 0.99 ; accuracy, 98% [$52/53$]) showed optimal diagnostic performance, which was better than that of V_e and iAUC (both $p = 0.003$), but the difference in AUC between K and

K^{trans} , K_{ep} , or D did not reach significance ($p = 0.08$, 0.50 , and 0.20 , respectively). In differentiating PAs from OBTs, the cutoff value of K^{trans} was 0.21 min^{-1} (AUC, 0.77 ; accuracy, 80% [$35/44$]). In differentiating PAs from MTs, D (cutoff value, $> 1.46 \times 10^{-3} \text{ mm}^2/\text{s}$; AUC, 0.96 ; accuracy, 92% [$34/37$]) showed optimal diagnostic performance, but the difference in AUC between D and K^{trans} , iAUC, or K did not reach significance ($p = 0.14$, 0.08 , and 0.40 , respectively). In differentiating WTs from OBTs, K (cutoff value, > 0.72 ; AUC, 0.97 ; accuracy, 93% [$40/43$]) showed optimal diagnostic performance, which was significantly better than that of K_{ep} ($p = 0.01$), but the difference in AUC between K and V_e or D did not reach significance ($p = 0.13$ and 0.11 , respectively). In differentiating WTs from MTs, V_e (cutoff value, > 0.23 ; AUC, 0.92 ; accuracy, 78% [$28/36$]) showed a higher AUC than K_{ep} , but the difference did not reach significance ($p = 0.33$). The cutoff value of D was $1.24 \times 10^{-3} \text{ mm}^2/\text{s}$ in differentiating OBTs from MTs (AUC, 0.88 ; accuracy, 82% [$22/27$]).

Fig. 4 A 34-year-old man with pleomorphic adenoma in the left parotid gland (white arrow). Dynamic contrast-enhanced MRI parameter maps showed the K_{ep} (a), V_e (b), and K^{trans} (c) values of 0.30 min^{-1} , 0.51 , and 0.15 min^{-1} , respectively. **d** D map demonstrated that the mass showed slightly hypointensity compared with neighboring normal-appearing muscle, with a D value of $1.85 \times 10^{-3} \text{ mm}^2/\text{s}$



Excellent inter- and intraobserver agreement for DKI and DCE-MRI parameters was achieved with ICCs ranging from 0.92 to 0.99 (see Supplementary Material 4 for details).

DKI and DCE-MRI analysis between solid and predominantly cystic of WTs

To overcome the possible influence in DKI and DCE-MRI parameters caused by heterogeneity of Warthin tumors, we further compared these parameters derived from the solid portion between Warthin tumors with solid and predominantly cystic forms. Of 26 Warthin tumors, 20 (77%) were presented as predominantly solid masses, which included completely solid or solid tumor with small cystic components, and 6 (23%) were presented as predominantly cystic entities. No significant differences were found in all parameters between predominantly solid and predominantly cystic Warthin tumors ($p=0.12, 0.05, 0.70, 0.98, 0.66$, and 0.22 for K^{trans} , K_{ep} , V_e , iAUC, D , and K value, respectively).

Stepwise discrimination among four groups of PGTs using DKI and DCE-MRI

Initially, PAs, OBTs, and MTs were classified as one group for the reason that there were significant differences in K_{ep} and V_e values between these three groups of tumors and WTs. Both K_{ep} and V_e values helped discriminate WTs from PAs, OBTs, and MTs, with a cutoff value of $> 1.06 \text{ min}^{-1}$ for K_{ep} (accuracy, 84% [67/80]) and ≤ 0.28 for V_e (accuracy, 74% [59/80]). Moreover, the combination of K_{ep} and V_e values generated the better diagnostic performance (accuracy, 89% [71/80]) than V_e (AUC, 0.93 vs 0.86; $p=0.03$) and was finally applied to distinguish WTs from the other three groups of PGTs (Table 4).

Subsequently, PAs and OBTs were classified as one group for the reason that lower D value was found in MTs than the other two entities. The D value was useful for differentiating MTs from PAs and OBTs, with a cutoff value of $\leq 1.46 \times 10^{-3} \text{ mm}^2/\text{s}$ (accuracy, 85% [46/54]) (Table 4).

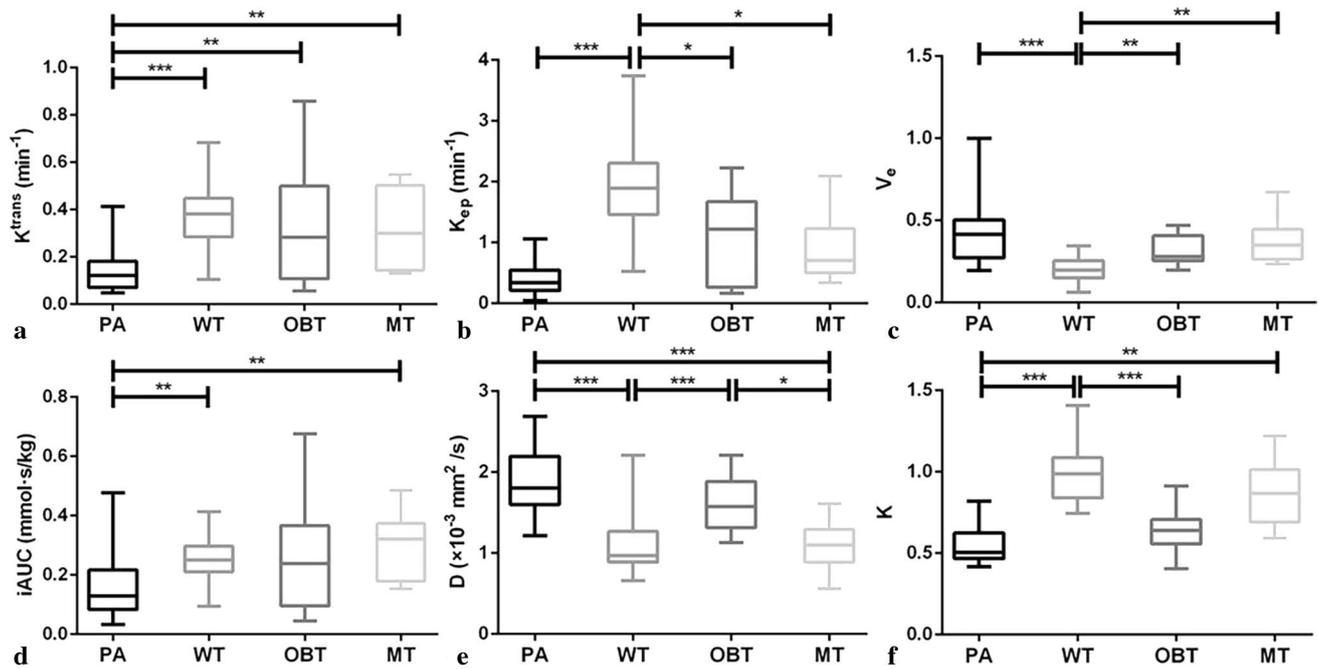


Fig. 5 Box-and-whisker plots show mean DCE-MRI and DKI quantitative parameters for all cases. Boundaries of boxes indicate 25th and 75th percentiles, and lines in boxes indicate medians. *PA* pleomorphic

adenoma, *WT* Warthin tumor, *OBT* other benign tumor, *MT* malignant tumor. * $p < .05$; ** $p < .01$; *** $p < .001$

Eventually, the K^{trans} value was used to differentiating PAs from OBTs resulted from the lower K^{trans} value of PAs with a cut-off value of $\leq 0.21 \text{ min}^{-1}$ (accuracy, 80% [35/44]) (Table 4). From this aspect, a stepwise distinguishable diagnostic diagram was put up for discriminating the four groups of PGTs consisting of PAs, WTs, OBTs, and MTs (Table 5 and Fig. 6). The diagnostic diagram provided high accuracy for the differential diagnosis of WTs and MTs of 89% (71/80) and 91% (73/80), respectively, and modest accuracy for both PAs and OBTs of 78% (62/80).

Discussion

DKI and DCE-MRI have been widely used in head and neck regions [19, 20]. However, to our knowledge, the diagnostic performance of combined DKI and DCE-MRI models in the field of PGTs has not been assessed in the existing studies. Our current study showed that DKI and DCE-MRI can elucidate the diffusion and perfusion characteristics of PGTs and provided a stepwise diagnostic diagram to distinguish common PGTs with modest to high accuracy (78–91%). These findings suggest that DKI and DCE-MRI quantitative parameters may facilitate the understanding of the pathophysiological characteristics of PGTs.

The D value derived from DKI is the corrected diffusion-related coefficient for non-Gaussian bias, and there is a strong inverse association with the tumor cellular density and nucleus-to-cytoplasm ratios [19]. Previously, Qian et al. [10] showed that no significant difference was found in the D value between the benign and the malignant tumors. They implied that low D value in WTs mainly accounted for low D value in benign PGTs and there was possibly a slight difference of D value by increasing the sample size. In this study, with a relatively big sample size, the mean D value was the only significant parameter in distinguishing the benignity from the malignancy, which was consistent with the hypothesis. In subgroup comparisons, a previous study [9] demonstrated that PAs had higher D value whereas WTs and MTs had relatively lower D value, which was in good agreement with our results. Histologically, the high D value in PAs resulted from the abundant myxoid and chondroid matrices [10]. Flourishing cells, enlarged nuclei, and smaller extracellular space in MTs [21] and high cellularity that resulted from rich lymphoid tissue-related interstitium in WTs [22, 23] help explain the low D value. Notably, in this study, D was used for the second step in the stepwise diagnostic diagram instead of K , due to the fact that the difference of K value between OBTs and MTs was not statistically significant, which was incompatible with the previous study [9]. The chief reasons for it may be different histopathological subtypes of OBTs and MTs and different b -value

Table 3 Optimal cutoff values and diagnostic performance of DKI and DCE-MRI parameters for differentiating four groups of PGTs

Parameters	Cutoff value	AUC	Sensitivity (%)	Specificity (%)	Accuracy (%)	PPV (%)	NPV (%)
Pleomorphic adenomas vs. Warthin's tumors							
K^{trans}	0.21	0.93	93 (25/27)	88 (23/26)	91 (48/53)	89 (25/28)	92 (23/25)
K_{ep}	1.06	0.99	100 (27/27)	92 (24/26)	96 (51/53)	93 (27/29)	100 (24/24)
V_e	0.28	0.82	63 (17/27)	96 (25/26)	79 (42/53)	94 (17/18)	71 (25/35)
iAUC	0.19	0.83	74 (20/27)	88 (23/26)	81 (43/53)	87 (20/23)	77 (23/30)
D	1.43	0.95	93 (25/27)	96 (25/26)	94 (50/53)	96 (25/26)	93 (25/27)
K	0.72	0.99	96 (26/27)	100 (26/26)	98 (52/53)	100 (26/26)	96 (26/27)
Pleomorphic adenomas vs. other benign tumors							
K^{trans}	0.21	0.77	93 (25/27)	59 (10/17)	80 (35/44)	78 (25/32)	83 (10/12)
Pleomorphic adenomas vs. malignant tumors							
K^{trans}	0.13	0.86	59 (16/27)	100 (10/10)	70 (17/37)	100 (16/16)	48 (10/21)
iAUC	0.15	0.84	59 (16/27)	100 (10/10)	70 (17/37)	100 (16/16)	48 (10/21)
D	1.46	0.96	93 (25/27)	90 (9/10)	92 (34/37)	96 (25/26)	82 (9/11)
K	0.54	0.93	70 (19/27)	100 (10/10)	78 (29/37)	100 (19/19)	56 (10/18)
Warthin's tumors vs. other benign tumors							
K_{ep}	1.51	0.79	73 (19/26)	76 (13/17)	74 (32/43)	83 (19/23)	65 (13/20)
V_e	0.23	0.88	69 (18/26)	94 (16/17)	79 (34/43)	95 (18/19)	67 (16/24)
D	1.05	0.90	73 (19/26)	100 (17/17)	84 (36/43)	100 (19/19)	71 (17/24)
K	0.72	0.97	100 (26/26)	82 (14/17)	93 (40/43)	90 (26/29)	100 (14/14)
Warthin's tumors vs. malignant tumors							
K_{ep}	0.98	0.86	92 (24/26)	80 (8/10)	89 (32/36)	92 (24/26)	80 (8/10)
V_e	0.23	0.92	69 (18/26)	100 (10/10)	78 (28/36)	100 (18/18)	56 (10/18)
Other benign tumors vs. malignant tumors							
D	1.24	0.88	82 (14/17)	80 (8/10)	82 (22/27)	88 (14/16)	73 (8/11)

DKI diffusion kurtosis imaging, DCE-MRI dynamic contrast-enhanced MRI, PGTs parotid gland tumors, AUC the area under the curve, PPV positive predictive value, NPV negative predictive value, K diffusion kurtosis, D diffusion coefficient, K^{trans} transfer constant from plasma to extravascular extracellular space, K_{ep} rate constant from extravascular extracellular space to plasma, V_e fractional volume of the extravascular extracellular space, iAUC initial area under the contrast agent concentration–time curve. Data in parentheses are the numerator and denominator used to calculate percentages. K_{ep} and K^{trans} values are expressed in min^{-1} ; iAUC values are expressed in $\text{mmol}\cdot\text{s}/\text{kg}$. D values are expressed in $\times 10^{-3} \text{mm}^2/\text{s}$

Table 4 Optimal cutoff values and diagnostic performance of DKI and DCE-MRI parameters for stepwise discrimination

Parameters	Cutoff value	AUC	Sensitivity (%)	Specificity (%)	Accuracy (%)	PPV (%)	NPV (%)
WTs vs. PAs + OBTs + MTs							
K_{ep}	1.06	0.90	92 (24/26)	80 (43/54)	84 (67/80)	69 (24/35)	96 (43/45)
V_e	0.28	0.86	96 (25/26)	63 (34/54)	74 (59/80)	56 (25/45)	97 (34/35)
$K_{\text{ep}} + V_e$	–	0.93	92 (24/26)	87 (47/54)	89 (71/80)	77 (24/31)	96 (47/49)
MTs vs. PAs + OBTs							
D	1.46	0.93	90 (9/10)	84 (37/44)	85 (46/54)	56 (9/16)	97 (37/38)
PAs vs. OBTs							
K^{trans}	0.21	0.77	93 (25/27)	59 (10/17)	80 (35/44)	78 (25/32)	83 (10/12)

DKI diffusion kurtosis imaging, DCE-MRI dynamic contrast-enhanced MRI, AUC area under the ROC curve, PPV positive predictive value, NPV negative predictive value, WTs Warthin tumors, PAs pleomorphic adenomas, OBTs other benign tumors, MTs malignant tumors, K_{ep} rate constant from extravascular extracellular space to plasma, V_e fractional volume of the extravascular extracellular space, D diffusion coefficient, K^{trans} transfer constant from plasma to extravascular extracellular space. Data in parentheses are the numerator and denominator used to calculate percentages. K_{ep} and K^{trans} values are expressed in min^{-1} ; D values are expressed in $\times 10^{-3} \text{mm}^2/\text{s}$

selection in DKI scan parameters in the two studies [24]. However, ROC curve analysis showed that the K value

can provide a high accuracy in differentiating WTs from PAs and OBTs. The K value can quantify the degree of

Table 5 Diagnostic accuracy with the combination of DKI and DCE-MRI parameters for the differentiation of PGTs

Parameters	DKI/DCE-MRI criteria			Diagnostic accuracy (%)
	$K_{ep} + V_e$	D	K^{trans}	
WT	$K_{ep} > 1.06, V_e \leq 0.28$	–	–	89 (71/80)
MT	$K_{ep} \leq 1.06, V_e > 0.28$	≤ 1.46	–	91 (73/80)
PA	$K_{ep} \leq 1.06, V_e > 0.28$	> 1.46	≤ 0.21	78 (62/80)
OBT	$K_{ep} \leq 1.06, V_e > 0.28$	> 1.46	> 0.21	78 (62/80)

DKI diffusion kurtosis imaging, DCE-MRI dynamic contrast-enhanced MRI, PGTs parotid gland tumors, WT Warthin tumor, MT malignant tumor, PA pleomorphic adenoma, OBT other benign tumor, K_{ep} rate constant from extravascular extracellular space to plasma, V_e fractional volume of the extravascular extracellular space, D diffusion coefficient, K^{trans} transfer constant from plasma to extravascular extracellular space. Data in parentheses are the numerator and denominator used to calculate percentages. K_{ep} and K^{trans} values are expressed in min^{-1} ; D values are expressed in $\times 10^{-3} \text{mm}^2/\text{s}$

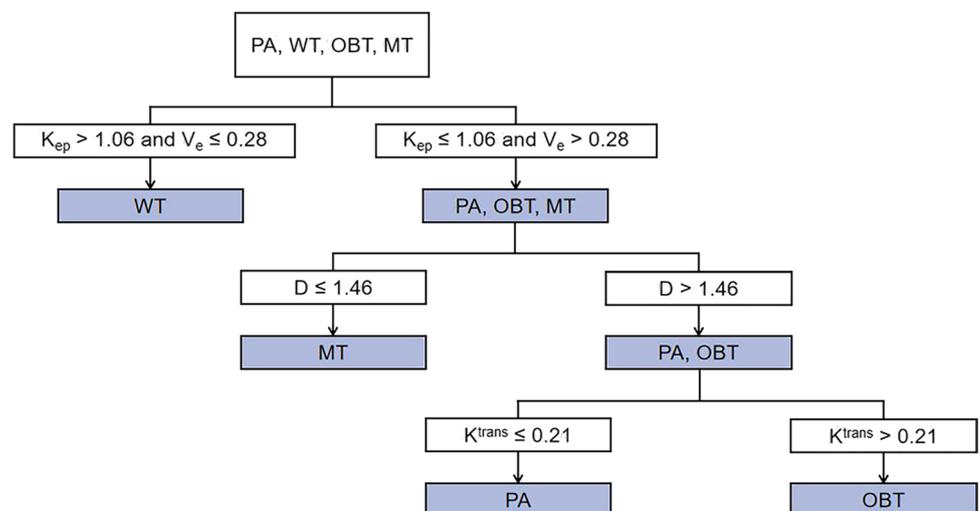
non-Gaussian distribution and tend to move together with cellular heterogeneity and tissue complexity [21]. The higher K value of WTs might be attributed to the complex microstructure within tumor, including various proportions of epithelia with papillary proliferation, lymphoid tissue, and cystic components filled with mucoid in histopathology [25]. Hence, our findings suggest that the K value evaluated preoperatively may aid in differentiating PGTs.

K^{trans} derived from DCE-MRI chiefly depends on blood flow in tissue and capillary permeability [19, 26]. Our findings discovered that K^{trans} was the only useful imaging

marker for distinguishing PAs from OBTs, which was inconsistent with the previous study [14]. In our study, BCAs accounted for the majority of OBTs, which possibly to some extent affected the K^{trans} value in the OBTs. Hence, the significant differences in K^{trans} value were related to the comparative higher K^{trans} value of BCAs. Histologically, compared with PAs, BCAs are short of mesenchymal component and chondromyxoid stroma but have a great deal of vascular architecture [27]. The different histological features may be the dominant reason; another one may be various pathological types but small sample size in OBTs in our study. Further studies with a bigger sample size are mandatory to analyze the differences of quantitative parameters between PAs and OBTs. V_e has a strong correlation with tissue necrosis and cellularity and K_{ep} is equal to the ratio of K^{trans} to V_e [19, 26]. In our study, WTs had the highest K_{ep} value but lowest V_e value than the other three groups, which was in accord with the previous study [13, 14]. In the study by Yabuuchi et al. [13], the differences in K_{ep} and V_e values reached statistical significance among four types of PGTs and particularly, the use of the K_{ep} value extremely promoted the diagnostic efficacy in the decision tree analysis. Histologically, limited extracellular and extravascular space in WTs [14] results in high K_{ep} value but low V_e value. Accordingly, with the characteristic presentations of perfusion parameters (high K_{ep} value and low V_e value), WTs could be effectively differentiated from the other three groups.

In our current study, the improved diagnostic performance was found in the combination of K_{ep} and V_e values for differentiating WTs from the other three groups, indicating K_{ep} and V_e values could be the optimal quantitative parameters for the diagnosis of WTs. Moreover, favorable sensitivity, specificity, and accuracy were also investigated in D value for the differentiation of MTs from PAs and OBTs, implying D value may conduce to the differential diagnosis. Furthermore, our study showed that K^{trans} value avails to

Fig. 6 Graph shows stepwise discrimination of four groups of parotid gland tumors, including Warthin tumors, malignant tumors, pleomorphic adenomas, and other benign tumors using DCE-MRI parameters and diffusion coefficient. PA pleomorphic adenoma, WT Warthin tumor, OBT other benign tumor, MT malignant tumor. Units for quantitative parameters: K_{ep} and K^{trans} are expressed in min^{-1} ; D are expressed in $\times 10^{-3} \text{mm}^2/\text{s}$



further discriminating PAs from OBTs. As a result, in the manner of the stepwise diagram combining DCE-MRI- and DKI-derived parameters, these common histological types of PGTs could be well differentiated. Regardless, the validation and correction of the criteria still need to be made with a larger sample size in further studies.

There are several limitations to our study. First, this was a retrospective study that may generate bias in case selection and the sample size of patients with malignant tumor was relatively small. Further study with a larger sample size is required to confirm our results. Second, magnetic susceptibility artifacts with anatomic distortions may inevitably exert an influence on the measurements and corresponding results. Various available DKI sequences like the readout-segmented echo-planar imaging (RS-EPI) technique may be offered as a solution. Third, our study applied DKI and DCE-MRI for PGTs. Further studies with multimodal imaging using intravoxel incoherent motion (IVIM) and arterial spin labeling (ASL) will improve the results.

In conclusion, our study demonstrated that DKI and DCE-MRI are useful for characterizing common PGTs. Additionally, a stepwise diagnostic diagram was put up based on the combined use of DCE-MRI parameters and the diffusion coefficient to improve the diagnostic ability. In the future, studies with a more abundant and larger sample size are necessary to help scrutinize, optimize, and validate our stepwise diagram and expand the applications of DKI and DCE-MRI to other parotid gland diseases.

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Declarations

Guarantor The scientific guarantor of this publication is Prof. Dairong Cao, MD, The First Affiliated Hospital of Fujian Medical University.

Conflict of interest The authors of this manuscript declare no relationships with any companies whose products or services may be related to the subject matter of the article.

Statistics and biometry No complex statistical methods were necessary for this paper.

Informed consent Written informed consent was waived by the Institutional Review Board.

Ethical approval Institutional Review Board approval was obtained.

Study subjects and cohort overlap Some patients in the present study cohort overlapped one of our studies, in which we used readout segmentation of long variable echo-trains diffusion-weighted imaging and quantitative dynamic contrast-enhanced MRI (DCE-MRI) with ROI measurements to differentiate parotid tumors. As for the DCE-MRI part, 69 cases (56.1%) overlapped in these two studies. In that study, the temporal resolution, duration of dynamic sequence and diffusion technique, and calculated mode were far different from our present study.

Methodology

- Retrospective
- diagnostic or prognostic study
- performed at one institution

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