

4D-MR flow analysis in patients after repair for tetralogy of Fallot

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Abstract

Objectives Comprehensive analysis of haemodynamics by 3D flow visualisation and retrospective flow quantification in patients after repair of tetralogy of Fallot (TOF).

Methods Time-resolved flow-sensitive 4D MRI (spatial resolution ~ 2.5 mm, temporal resolution = 38.4 ms) was acquired in ten patients after repair of TOF and in four healthy controls. Data analysis included the evaluation of haemodynamics in the aorta, the pulmonary trunk (TP) and left (lPA) and right (rPA) pulmonary arteries by 3D blood flow visualisation using particle traces, and quantitative measurements of flow velocity.

Results 3D visualisation of whole heart haemodynamics provided a comprehensive overview on flow pattern changes in TOF patients, mainly alterations in flow velocity, retrograde flow and pathological vortices. There was consistently higher blood flow in the rPA of the patients (rPA/lPA flow ratio: 2.6 ± 2.5 vs. 1.1 ± 0.1 in controls). Systolic peak velocity in the TP was higher in patients ($1.9 \text{ m/s} \pm 0.7 \text{ m/s}$) than controls ($0.9 \text{ m/s} \pm 0.1 \text{ m/s}$).

Conclusions 4D flow-sensitive MRI permits the comprehensive evaluation of blood flow characteristics in patients

after repair of TOF. Altered flow patterns for different surgical techniques in the small patient cohort may indicate its value for patient monitoring and potentially identifying optimal surgical strategies.

Keywords 4D MRI · Tetralogy of Fallot · Pulmonary haemodynamics · Vortices · Monitoring

Introduction

Tetralogy of Fallot (TOF), the most common cyanotic congenital heart defect, accounts for about 10% of all congenital heart diseases [1, 2]. These patients usually undergo surgery in the first year of life with a good clinical outcome. The number of long-term survivors requiring cardiac and vascular imaging for follow-up and circulatory monitoring continues to rise [3]. Pulmonary valve insufficiency with consecutive right ventricular volume overload is the most common and serious postoperative problem in patients with TOF [4, 5]. Conventional angiography during cardiac catheterisation used to be considered the gold standard for the evaluation of pulmonary function, but Magnetic Resonance Imaging (MRI) has evolved as a powerful method for evaluating cardiovascular function after surgery for tetralogy of Fallot [6, 7]. Both angiography and standard MRI protocols, however, provide neither a complete picture nor detailed information about 3D haemodynamics and flow alterations occurring in the right ventricular outflow tract and the entire pulmonary vascular system at different points in time.

Time-resolved 3D phase-contrast MRI with three-directional velocity encoding, also known as flow-sensitive 4D-MRI, has become a valuable method for comprehensively assessing vascular haemodynamics in the

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aorta and other vascular territories [8–12]. In this study, the feasibility of whole heart flow-sensitive 4D-MRI [13, 14] for the visualisation of 3D flow characteristics and flexible retrospective flow quantification was evaluated in ten paediatric patients after repair of TOF. It was the aim to visualise and understand changes in blood flow characteristics in the pulmonary arteries after complex surgical repair.

Materials and methods

Patients

Ten patients after repair of TOF (age 12.1 ± 8.1 years, range 2–24 years, 5 male) and four healthy controls (age 26 ± 0.8 years, range 25–27 years) underwent whole heart flow-sensitive 4D-MRI. The mean interval between surgery and MRI was 10.4 ± 7.9 years. The mean age of corrective surgery was 0.8 ± 1.2 years. Four patients underwent transannular repair with consecutive pulmonary valve insufficiency, four pulmonary valve-preserving surgery, and two valve conduit implantation. The study was approved by our local ethics committee, and written informed consent was obtained from each participant and his or her parents prior to MRI examinations.

Magnetic resonance imaging

MRI examinations were performed on 1.5T (eight patients) and 3T MR (two patients and four controls) systems (AVANTO or TRIO, Siemens, Germany). Flow-sensitive 4D-MRI acquisitions were synchronised to the heart rate and breathing using prospective ECG-gating and adaptive diaphragm navigator gating [9]. The MRI sequence consisted of a k-space segmented rf-spoiled gradient echo sequence with interleaved 3-directional velocity encoding. Data were acquired in a sagittal oblique 3D data volume individually adapted to include the entire heart, thoracic aorta, and main pulmonary arteries. Imaging parameters were as follows: velocity sensitivity = 150–200 cm/s, TE = 2.3–2.5, TR = 4.7–5.1, field of view (FOV) = 125–345 mm \times 250–460 mm, spatial resolution = 1.7–2.2 \times 1.8–3.2 \times 1.6–2.5 mm³, temporal resolution = 37.6–40.8 ms, flip angle = 7°–15°, scan time ~10–20 min, parallel imaging with reduction factor R = 2 [15].

3D flow visualisation

Data analysis included calculation of a 3D phase contrast (PC) MR angiogram (MRA) from 4D-MRI data combined with 3D blood-flow visualisation using commercially available software (EnSight, CEI, Apex, NC, USA).

Visualisation of aortic and pulmonary flow was achieved by traces of 3D virtual particles demonstrating time-resolved blood flow [16, 17]. Particle traces were emitted from interactively positioned planes in the ascending aorta (AAo), main pulmonary artery (TP), and right (rPA) and left pulmonary arteries (IPA). Traces along the measured velocities were colour-coded according to the local velocity in the different vessels of interest.

Flow pattern analysis

4D-blood flow visualisation was evaluated for each patient in consensus reading with regard to vortex formation, retrograde flow, and the presence of increased peak velocities. Time-resolved 3D particle traces were viewed dynamically and rotated or magnified for inspection in any chosen orientation as illustrated in the supplemental video. As illustrated in Fig. 1, vortices were defined as regional circular flow patterns deviating by more than 90° from the physiological flow direction along the vessel lumen. Vortex severity was graded in 3 categories: no vortex formation = 0, moderate vortex (flow rotation $<360^\circ$) = 1, pronounced vortex (flow rotation $>360^\circ$) = 2. Retrograde flow in the right ventricular outflow tract, right and left pulmonary arteries as well as the ascending aorta was evaluated using a 3-grade ranking: no retrograde flow = 0, moderate retrograde flow = 1, severe retrograde flow = 2. Presence of high peak velocities, defined as flow velocity >1.5 m/s, was evaluated as absent = 0 or evident = 1.

Flow quantification

Blood flow was quantified by retrospectively extracting the measured flow velocities in manually-positioned analysis planes from the flow-sensitive 4D-MR data [18]. Flow-time curves, total flow, and systolic peak velocities were analysed in the AAo approximately 1 cm above the aortic valve, in the TP above the pulmonary valve, and in the middle segment of the rPA and IPA. Flow-time curves were used to calculate the retrograde flow fraction in all vessels. Total flow to the left and right pulmonary arteries was used to derive the rPA/IPA flow ratio.

Results

3D blood flow visualisation

We observed a marked variation in flow characteristics in all patients, as exemplified in Fig. 1 (severe vortex formation) and 2 (severe retrograde flow and rPA/IPA flow asymmetry). See supplemental video (Fig. 5) depicting vortices of Fig. 1.

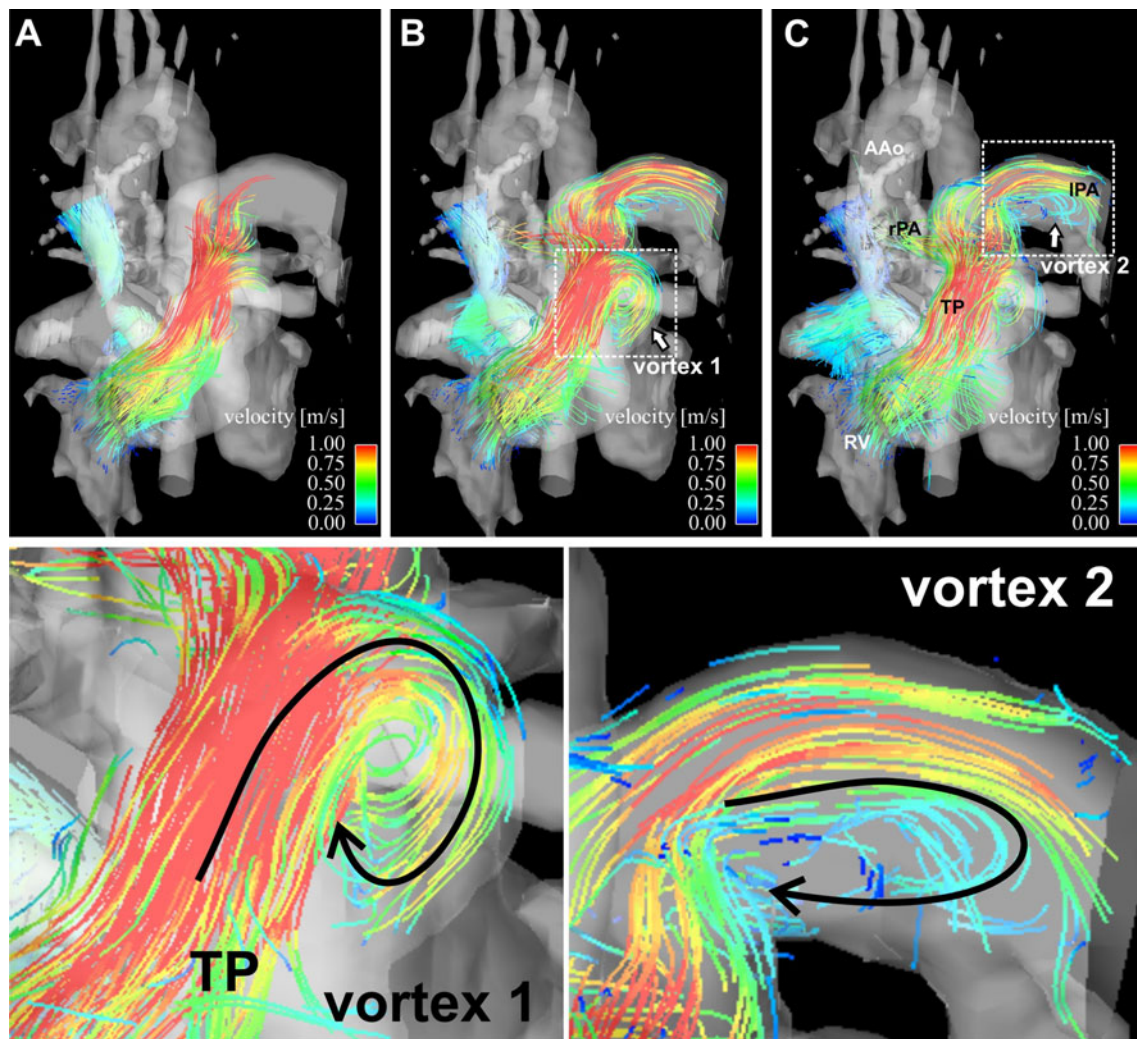


Fig. 1 Top row: 3D particle trace visualisation illustrating the dynamics of right ventricular outflow for three successive systolic time-frames (A-C). High systolic velocities (red colour) and vortex flow in the pulmonary trunk (TP) and the left pulmonary artery (IPA) can clearly be appreciated (white arrows). Lower row: Magnification of vortex flow in the TP (vortex 1) and IPA (vortex 2). Pronounced

vortex formation (vortex 1, grading = 2) in the TP coincided with a bulging enlargement of the outflow tract encompassing the circular flow. Additional vortex flow (vortex 2, grading = 2) was observed immediately distal to the IPA's branching point. 3D blood flow dynamics can be best appreciated in the supplemental video (Fig. 5). AAO: ascending aorta, RV: right ventricle, rPA: right pulmonary artery

Mean vortex severity in the TP was 0.9 ± 1.0 in patients, with less severe vortices in the rPA (0.2 ± 0.7) and IPA (0.7 ± 0.9). Pronounced vortices (grade 2) in the TP were detected in four patients and moderate vortices (grade 1) in two patients. Three patients presented mild-to-moderate vortices in the aorta. Flow visualisation in the aorta was impaired in one patient because of poor overall image quality. Evaluation of the pulmonary arteries was hindered in two patients due to artefacts caused by a stent within the IPA.

High peak velocities >1.5 m/s in the TP were apparent in eight patients (average grading = 0.8 ± 0.4) and in the rPA and IPA in seven and six patients, respectively (Fig. 2). One patient had high flow velocities in the ascending aorta.

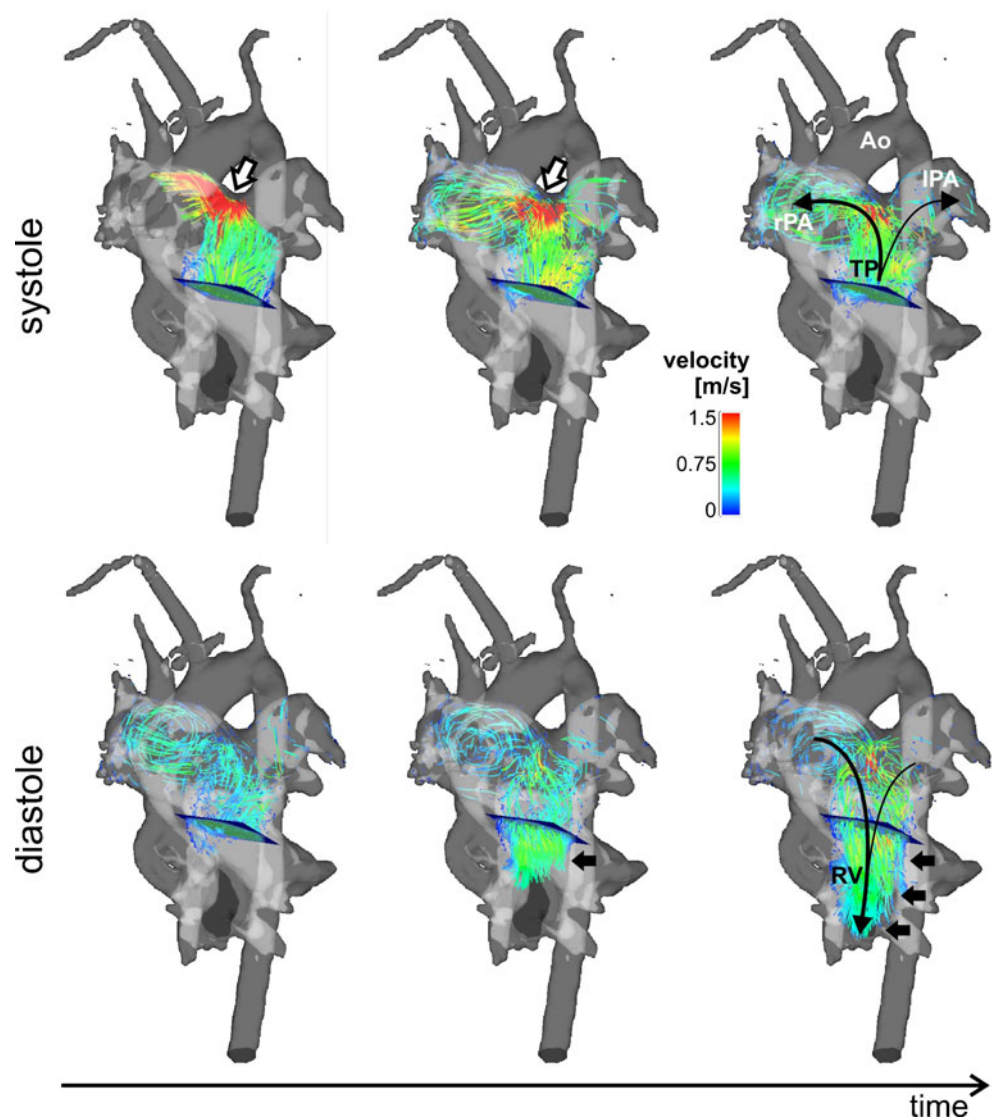
All patients presented unmistakable retrograde flow in the TP due to pulmonary insufficiency (average grading = 1.8 ± 0.4) estimated as moderate (grade 1) in two and severe (grade 2) in eight TOF patients (Fig. 2). Eight patients had retrograde flow in the rPA (average grading = 1.8 ± 0.7 , two moderate, six severe) and the IPA (average grading = 1.4 ± 0.7 , three moderate, five severe). No regurgitation was detected in the aorta.

Flow velocities above 1.5 m/s, vortices, and retrograde flow were not detected in the healthy volunteer group.

Flow quantification

Flow-time curves averaged over patients and controls in the aorta and pulmonary arteries are displayed in Fig. 3. As

Fig. 2 Time evolution of blood flow in the right ventricular outflow tract and pulmonary arteries during one cardiac cycle visualised by 3D particle traces originating from an emitter plane at the level of the pulmonary valve. Substantial flow acceleration during systole is clearly evident (*white arrows and red colours* = velocities >1.5 m/s). Pulmonary valve insufficiency resulted in marked diastolic retrograde flow (*small black arrows*, retrograde fraction = 39% in this patient example) into the right ventricle (RV). During both systole and diastole, particle traces visualised marked asymmetry of flow to and from the left (lPA) compared to the right (rPA) pulmonary artery. This finding was confirmed by quantitative analysis which revealed the highest rPA/lPA flow ratio = 8.2 in the study cohort, TP: pulmonary trunk, Ao: aorta



expected, we noted strong regurgitation in the TOF patients' pulmonary arteries (regurgitation fraction = $29\% \pm 11\%$) whereas no regurgitation was observed in controls. Systolic peak velocity in the pulmonary trunk was higher in patients ($1.9 \text{ m/s} \pm 0.7 \text{ m/s}$) than controls ($0.9 \text{ m/s} \pm 0.1 \text{ m/s}$), while aortic peak velocities were similar ($1.4 \text{ m/s} \pm 0.3 \text{ m/s}$ in patients versus $1.3 \text{ m/s} \pm 0.1 \text{ m/s}$ in controls). The rPA/lPA flow ratio was noticeably variable in TOF patients, with a tendency to higher blood flow in the rPA (rPA/lPA flow ratio = 2.6 ± 2.5). In contrast, the control group's blood flow was similar in both pulmonary arteries (rPA/lPA flow ratio = 1.1 ± 0.1).

To test the internal consistency of flow quantification based on flow-sensitive 4D MRI data, net aortic flow was compared to net pulmonary trunk flow and net pulmonary trunk flow was compared to net (RPA+LPA) flow using correlation analysis. As summarized in Table 1, significant ($p < 0.01$) and high correlation ($r > 0.9$) confirms the validity of the MR flow analysis.

Comparison of haemodynamics according to surgical repair technique

As illustrated in Fig. 4, groups were divided into healthy controls and patients with transannular (1), valve-preserving (2) and conduit repair (3). There was an obvious tendency towards higher regurgitation fractions in the lPA and rPA after transannular repair. No noticeable trends were found for vortex formation, rPA/lPA flow ratio, or peak velocities.

Discussion

The feasibility of whole heart 4D-MRI for the comprehensive evaluation of pulmonary haemodynamics was successfully demonstrated in a small cohort of children, teenagers and young adults who had undergone TOF repair. In contrast to older normal controls, potentially pathologic

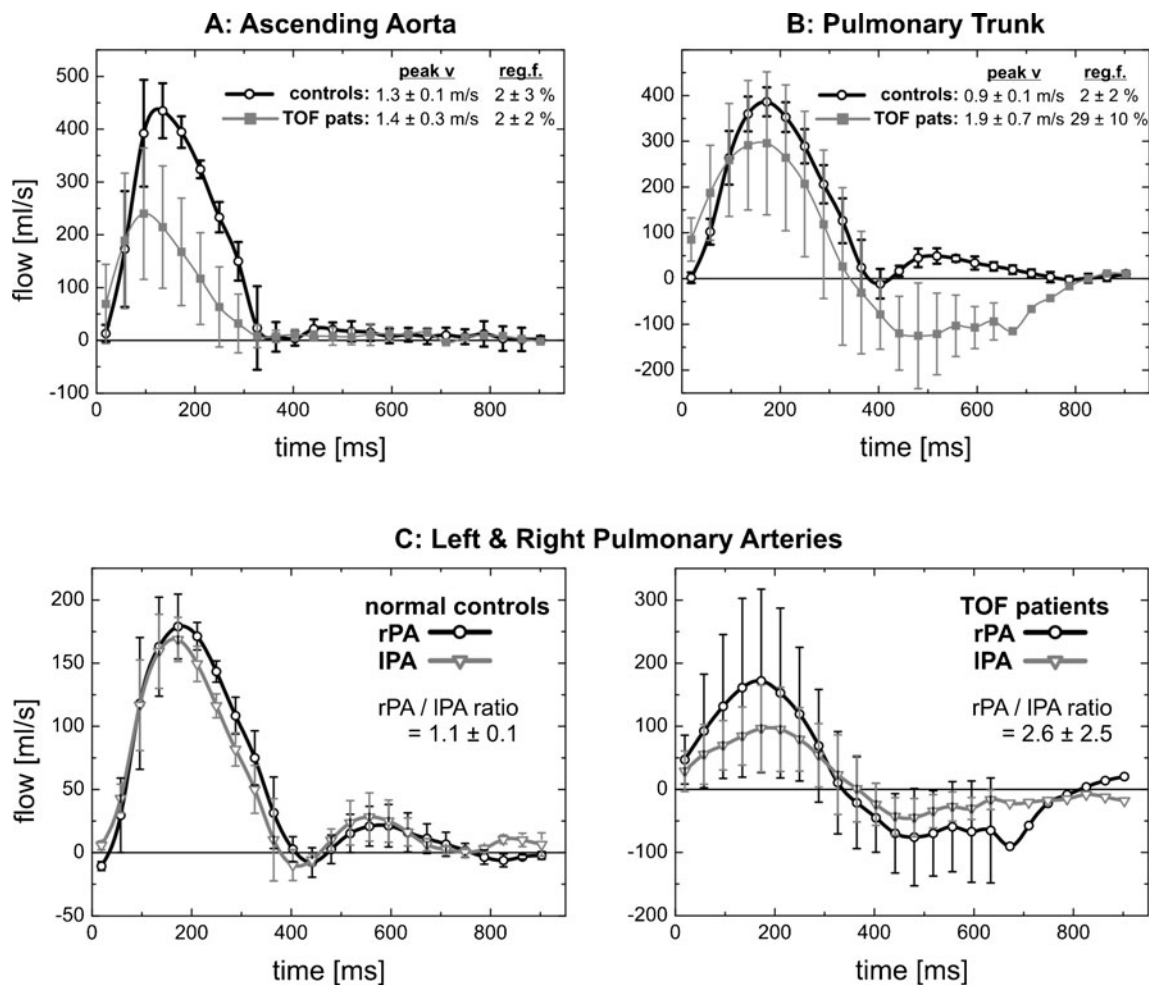


Fig. 3 Averaged blood flow-time curves in 10 patients with tetralogy of Fallot (TOF) and 4 normal subjects. **a:** Pulsatile flow-time curves in the ascending aorta (AAo) **b:** Flow-time curves in the pulmonary trunk clearly show regurgitant flow due to valve insufficiency in the TOF patient **c:** Flow to the left and right pulmonary arteries differed

considerably between normal controls and TOF patients. In comparison to volunteers, TOF patients showed pronounced diastolic retrograde flow and enhanced and more variable flow ratio to the left and right lung

vortex flow, substantial flow acceleration, pulmonary regurgitation, and abnormal flow ratios between right and left pulmonary arteries were our main findings.

In TOF patients, residual pulmonary stenosis, especially branch stenosis, and pulmonary regurgitation are

Table 1 Comparison of net flows in the ascending aorta (AAo), pulmonary trunk (TP) and left and right pulmonary arteries (LPA und RPA)

Net flow [ml/cycle]		correlation	
AAo	TP	p-value	r-value
55.6±28.0	59.9±29.0	< 0.01	0.95
TP	RPA+LPA	< 0.01	0.91
59.9±29.0	57.8±22.8		

the main problems in mid- and long-term follow-up. Progressive right ventricular dilatation or reduced ventricular function is an indicator of the need for valve replacement [19]. MRI is well suited to assess pulmonary vessel anatomy, using predominantly transverse black blood sequences such as HASTE or bright blood sequences, e.g. SSFP, or MRA, as recommended in the literature [6, 7, 20, 21]. Data available from echocardiography, however, are often incomplete, because pulmonary arteries are generally difficult to evaluate due to acoustic-window limitations [22]. We used the advantages of 4D-MRI, including complete volumetric coverage of the pulmonary trunk and flow-sensitive information on 3D blood flow to evaluate pulmonary haemodynamics, overcome the regionally-limited results of 2D phase-contrast MRI, and improve understanding of postoperative flow alterations [23].

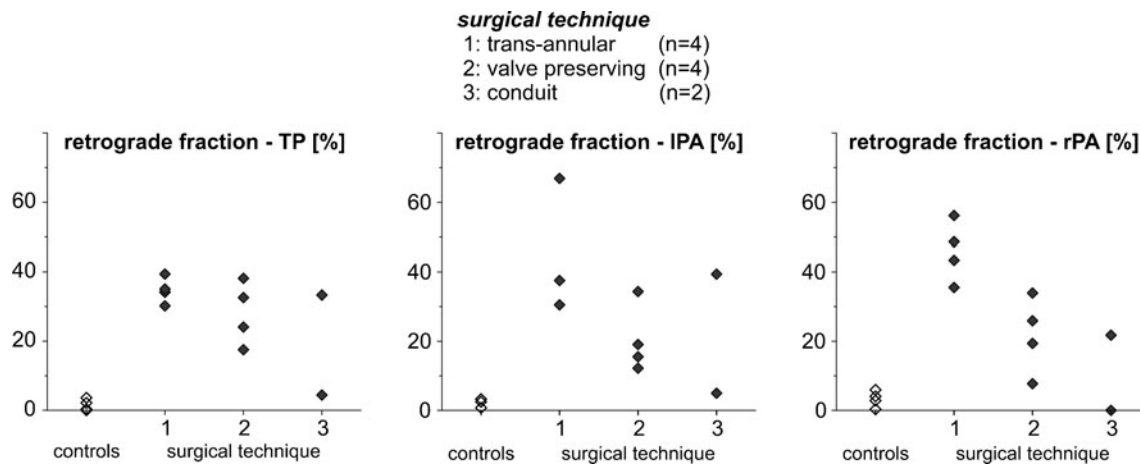


Fig. 4 Comparison of haemodynamic parameters between healthy volunteers (controls) and patients grouped according to the surgical technique employed for repair of tetralogy of Fallot (TOF)

The information on flow differences to the left and right lung found in our small patient cohort is similar to findings in previous studies [24, 25]. Using Doppler echocardiography data as a reference, normal pulmonary peak velocities range between 0.3 and 1.0 m/s, depending on the author [26–28]. In our survey, elevated peak velocities averaged 1.86 m/s in the patient group. No residual pulmonary stenosis, which could be the cause for flow acceleration, was detected in our investigation. We therefore assume that increased flow velocities may be compensating for blood reflux caused by pulmonary insufficiency which is a frequent long-term anomaly in 73% of TOF patients after repair [29].

A remarkable finding was the appearance of vortex flow patterns which cannot be detected by standard MRI scans or echocardiography. Reiter et al. detected a correlation between pulmonary hypertension and the appearance of vortex flow, followed by elevated pulmonary arterial pressure [30]. On the other hand, preexisting vortices may lead to pulmonary artery dilation. This concept is confirmed by previous 4D-MRI studies of the aorta, showing that vortices are associated with shear force alterations on the vessel wall, thus leading to changes in endothelial function, which is a predisposing factor for vascular remodelling and aortic dilatation [31, 32]. Similarly, pulmonary trunk abnormalities may influence the development of regurgitation and haemodynamic alterations. Using 4D-MR flow analysis, the complexity of vascular haemodynamics and its influence on morphology and function may be investigated more precisely than is possible using any other imaging tool.

Finally, we investigated the impact of the type of surgical repair and 4D-MR flow patterns. Although the number of patients in each group was limited, we found that transannular repair influences haemodynamics with

regard to regurgitation. Hence, when considering the long-term sequelae suffered by TOF patients, and current discussions concerning the ideal time for valve replacement [33, 34], patients' outcome might be additionally affected by the postoperative vessel dilation caused by vortices.

This study is limited by the small number of patients and the absence of an age matched control group. Larger patient cohorts and further follow-up examinations of our patients and long-term studies will be essential to learn more about the pathophysiological impact of the altered pulmonary haemodynamics and their link to prognostic and therapeutic consequences. Note that a validation of flow quantification based on the 4D data against standard flow measurements using the conventional 2D phase contrast MRI was not performed in the presented subjects. In a previous study we have demonstrated close agreement for flow derived from standard time-resolved 2D and 4D data [18]. A further disadvantage of the presented MRI methods is related to the long overall scan times on the order of 10–20 min which can be addressed using advanced parallel imaging techniques [35]. Nevertheless, we believe that the possibility for comprehensive visualisation of 3D haemodynamics and flexible retrospective flow quantification at any site within the 3D imaging volume justifies long scan times in cases of complex cardiac and vascular alterations as for TOF.

Conclusions

Beyond its unique potential to demonstrate the complexity of vascular morphology and function in TOF patients, 4D-MR flow analysis may prove valuable in clinical routine in the future by providing important data on both intracardiac and pulmonary vascular flow.

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