### **SPECIAL SECTION: NEUROENDOCRINE NEOPLASMS**

# **PET/CT and PET/MRI in neuroendocrine neoplasms**

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### **Abstract**

Advanced molecular imaging has come to play an integral role in the management of gastro-entero-pancreatic neuroendocrine neoplasms (GEP-NENs). Somatostatin receptor (SSTR) PET has now emerged as the reference standard for the evaluation of NENs and is particularly critical in the context of peptide receptor radionuclide therapy (PRRT) eligibility. SSTR PET/ MRI with liver-specifc contrast agent has a strong potential for one-stop-shop multiparametric evaluation of GEP-NENs.  $^{18}$ F-FDG is a complementary radiotracer to SSTR, especially in the context of high-grade neuroendocrine neoplasms. Knowledge gaps in quantitative evaluation of molecular imaging studies and their role in assessment of response to PRRT and combination therapies are active research areas. Novel radiotracers have the potential to overcome existing limitations in the molecular imaging of GEP-NENs. The purpose of this article is to provide an overview of the current trends, pitfalls, and recent advancements of molecular imaging for GEP-NENs.

**Keywords** Positron emission tomography-computed tomography · Magnetic resonance imaging · Neuroendocrine tumors · Gallium radioisotopes · Fluorodeoxyglucose F18

# **Introduction**

Around two-thirds of all neuroendocrine neoplasms (NENs) originate in the gastrointestinal system [[1,](#page-11-0) [2](#page-11-1)]. Gastro-enteropancreatic (GEP) NENs can occur at any age; however, the incidence exceeds 10 per 100,000 population between 70 and 8[4](#page-11-3) years of age  $[3, 4]$  $[3, 4]$  $[3, 4]$ . There has been a steady rise in the incidence of GEP-NENs over the last decade, likely due to increased awareness and the wider use of advanced cross-sectional imaging [[5–](#page-11-4)[7](#page-11-5)]. Most GEP-NENs are nonfunctional and remain clinically indolent, but metastases are common and often the source of symptoms [\[8\]](#page-11-6). Conversely, a subset of GEP-NENs are functional and present at earlier stages due to clinical manifestations induced by hypersecretion of various bioactive hormones, which can

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be debilitating. The majority of GEP-NENs are sporadic. However, a small subset of NENs can arise in the context of syndromes such as Multiple Endocrine Neoplasia type 1 (MEN1), Von Hippel Lindau syndrome (VHL), Neurofbromatosis type 1 (NF1), and tuberous sclerosis complex (TSC) [\[9](#page-11-7)]. Despite the high prevalence of metastatic disease, GEP-NENs tend to have a good prognosis with a mean survival of around seven years [[10](#page-12-0)]. However, the prognosis substantially varies with the site of the primary tumor. For instance, the average 5-year survival is around 54% for pancreatic NENs and nearly 100% for gastric NENs [[10](#page-12-0), [11](#page-12-1)].

The 2019 WHO system classifes NENs based on their mitotic activity and Ki-67 proliferation index (Table [1\)](#page-1-0) [[12,](#page-12-2) [13](#page-12-3)]. High-grade (G3) NENs are now stratifed into two histologically and genetically distinct groups, i.e., the welldiferentiated and poorly diferentiated groups. The latter are now termed neuroendocrine carcinomas (NECs) [[12](#page-12-2)]. There have been signifcant recent advances in the diagnosis, staging, and multidisciplinary treatment of NENs. One of these is the molecular imaging of NENs with somatostatin receptor (SSTR)-targeted PET, which has largely supplanted conventional gamma SSTR scintigraphy and single-photon emission-computed tomography (SPECT). The purpose of this article is to provide an overview of the current trends,



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<span id="page-1-0"></span>**Table 1** Grading system for NENs (Based on WHO 2019 and AJCC 2017)



^ Percentage of cells with a positive reaction on immunocytochemistry with MIB1 antibody

Φ Number of mitotic fgures within ten high power felds

*NEN* Neuroendocrine neoplasm, *WHO* World Health Organization, *AJCC* American Joint Committee on Cancer, *NEC* Neuroendocrine carcinoma, *MiNEN* Mixed neuroendocrine–non-neuroendocrine neoplasm

pitfalls, and recent advancements of molecular imaging for GEP-NENs.

### **Molecular imaging of GEP‑NENs**

Successful targeted molecular imaging of GEP-NENs is dependent upon the overexpression of SSTRs by these neoplasms. There are six subtypes of SSTRs (1, 2A, 2B, 3, 4, & 5). Of these, subtype 2A has the highest expression in GEP-NENs, particularly low-grade (G1 and G2) NENs [[14](#page-12-4)].  $^{111}$ Indium ( $^{111}$ In)-diethylene-triamine-penta-acetic acid (DTPA)-pentetreotide had been the traditional radiopharmaceutical for planar somatostatin receptor scintigraphy (SRS) and SPECT imaging of NENs. However, it had a high false-negative rate in organs that show high physiological uptake (e.g., liver), low spatial resolution, required long scan times, resulted in relatively high radiation dose to the patient, and orders of magnitude lower affinity for SSTRs compared to SSTR-targeted PET radiotracers. Therefore, it has been largely replaced by SSTR PET, which has become the current reference standard for molecular imaging of GEP-NENs.

In current clinical practice, SSTR PET is performed with  $^{68}$ Gallium ( $^{68}$ Ga) or  $^{64}$ Copper ( $^{64}$ Cu)-tagged peptides such as -TATE (Tyr3-octreotate), -NOC (NaI3-octreotide), and -TOC (TyI3-octreotide), which are chelated with DOTA (1,4,7,10-tetra-azacyclododecane-1,4,7,10-tetraacetic acid) to produce <sup>68</sup>Ga-DOTATATE, <sup>68</sup>Ga-DOTANOC, and <sup>68</sup>Ga-DOTATOC, respectively. Although there are minimal differences in the SSTR affinity of these agents, there is no clear superiority of one over the other in clinical practice.  $^{68}$ Ga-DOTATATE and  $^{68}$ Ga-DOTATOC are approved by the US Food and Drug Administration (FDA).

Compared to SRS, SSTR PET has signifcantly higher sensitivity for the detection of metastatic NENs, which translates to a substantial impact on clinical management  $[15–17]$  $[15–17]$ . The superior sensitivity is due to multiple factors such as the higher affinity of PET radiopharmaceuticals for SSTRs coupled with the higher spatial resolution and physical sensitivity of PET cameras. Thus, SSTR PET can detect more and smaller lesions, including those with low-to-moderate SSTR expression (Fig. [1](#page-2-0)). PET also offers faster throughput and a shorter overall scan time (a few hours for SSTR PET versus 2–3 days for SRS), the ability to quantify radiotracer uptake through standardized uptake values (SUVs), and lower efective radiation doses [[17\]](#page-12-6). Therefore, recent guidelines recommend that SSTR PET replaces SRS for all clinical indications used previously (Table [2\)](#page-2-1) [\[18](#page-12-7)].

<sup>64</sup>Cu-labeled DOTATATE is another PET radiotracer that was more recently approved by the FDA. The longer physical half-life of  ${}^{64}Cu$ , 12.7 h, compared to 68-min for  $^{68}$ Ga, can be an advantage because it allows for its central production and transportation to peripheral facilities that lack access to <sup>68</sup>Ga. Second, it has a shorter positron range in tissue (0.6 mm versus  $3.5$  mm for <sup>68</sup>Ga) and lower physiologic uptake in the liver. These properties have the potential to provide superior imaging quality, especially at delayed time points (3–24 h after injection). One comparative study found higher detection of true positive lesions with  $^{64}$ Cu-DOTATATE than <sup>68</sup>Ga-DOTATOC, especially in the liver. However, a patient-based analysis revealed no signifcant difference [[19](#page-12-8)]. Second, a dual-time point imaging study of 64Cu-DOTATATE showed similar accuracy for 1 and 3 h time points. <sup>64</sup>Cu-DOTATATE is also prone to in vivo demetallation and transchelation, which may reduce image quality  $[20]$  $[20]$ . Finally, compared to  $^{68}Ga$ -DOTATATE,  $^{64}Cu$ -DOTATATE emits fewer positrons per annihilation event and emits beta emissions, which contribute to increased patient radiation dose and limit the permissible dose to the patient. Thus, to achieve image quality comparable to  ${}^{68}Ga-$ DOTATATE PET with an equivalent efective dose, the scan time needs to be increased for <sup>64</sup>Cu-DOTATATE PET. New sarcophagine-based chelators such as <sup>64</sup>Cu-SARTATE have shown high retention in the tumor at delayed time point imaging with progressive clearance from the liver and have the potential to provide better results than <sup>64</sup>Cu-DOTATATE [[21\]](#page-12-10).

<span id="page-2-0"></span>**Fig. 1** Incremental value of SSTR PET over somatostatin receptor scintigraphy (SRS). A 66-year-old male with a metastatic well-diferentiated NEN. Whole-body planar SRS image (**a**) shows multifocal radiotracer-avid hepatic metastases and a few scattered tracer-avid osseous lesions. Maximum intensity projection (MIP) image (**b**) of the  ${}^{68}Ga-$ DOTATATE PET/CT shows a substantially higher number of hepatic and osseous lesions with superior resolution



<span id="page-2-1"></span>

*SSTR* Somatostatin receptor, *NEN* Neuroendocrine neoplasm, *PRRT* Peptide receptor radionuclide therapy, *CI* Conventional imaging

# **PET/MRI**

imaging

PET/MRI is a hybrid imaging modality that enables simultaneous acquisition of PET and MRI. It became a reality mainly due to the advent of magnetic feld-insensitive solid-state photon detectors of scintillation events. Clinical use of PET/MRI has led to innovative changes in the way both PET and MR data are acquired [[22](#page-12-11)]. PET/MRI has a particularly strong potential for multiparametric evaluation of GEP-NENs. Despite the high accuracy of SSTR PET

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for imaging of GEP-NENs, evaluation of subtle or small hepatic metastases can be a challenge on SSTR PET/CT due to the high and variable degrees of physiologic hepatic radiotracer uptake (Fig. [2](#page-3-0)). SSTR PET also does not accurately detect poorly diferentiated lesions and tends to have false positives due to physiologic radiotracer uptake in pancreatic uncinate process or intrapancreatic splenules [[17](#page-12-6)]. MRI is the reference standard imaging examination for the evaluation of liver metastases in patients with GEP-NENs. However, characterization of tumor biology and treatment response assessment are known challenges on

<span id="page-3-0"></span>**Fig. 2** 68Ga-DOTATATE PET/ MRI for evaluation of hepatic metastases. A 76-year-old woman with a G2 ileal NEN. Maximum intensity projec tion (MIP) image (a) of the **68Ga-DOTATATE PET/MRI** shows the primary ileal mass with adjacent mesenteric nodal metastases (thin black arrows) and multiple radiotracer-avid liver metastases (blue arrow heads). Axial <sup>68</sup>Ga-DOTATATE PET/MRI ( **b**, **d**) shows three tracer-avid liver metastases (thick black arrows). The corre sponding 20 min delayed hepa tobiliary phase images ( **c**, **e**) show three additional tiny satel lite metastases (red arrowheads) adjacent to the lesions seen on PET (Color figure online)





MRI [[23](#page-12-12), [24](#page-12-13)]. Because of these advantages and limitations of individual imaging modalities, many patients with GEP-NENs often undergo both SSTR PET and liver MRI. The combination of PET and MRI into one comprehensive examination offers the prospect of synergistic imaging, streamlined workflow, and a better patient experience.

Appropriate patient selection and optimized imaging workflow are critical requirements for the clinical success of PET/MRI [[25\]](#page-12-14). For instance, patient body habitus is an important consideration. Since the solid-state PET detectors are part of the MR gantry, PET/MRI has a narrower bore (60 cm) compared to most stand-alone MRI scanners (70 cm). At our institution, only patients with body mass index<40 or anteroposterior abdominal diameter less than 32 cm are scheduled for PET/MRI. To balance patient comfort and scanner throughput, the SSTR PET/MR imaging protocol has been designed to last no more than 60 min. It has two components – the whole-body survey and a focused abdominal PET/MRI. The whole-body component includes multi-bed position PET with co-acquisition of 2-point Dixon three-dimensional (3D) fast-spoiled gradient-recalled echo (FSPGR) imaging at each bed position for anatomic colocalization and attenuation correction. This is immediately followed by focused abdominal PET/MRI, which includes single-bed, list-mode, respiratory-compensated PET acquisition with simultaneous dynamic post-contrast imaging with hepatocyte-specifc contrast agent (gadoxetate disodium), T2-weighted imaging, and diffusion-weighted imaging. This protocol offers a synergistic combination of wholebody SSTR PET and optimized multiphase abdominal MRI with dedicated liver PET and has rapidly gained traction in our clinical practice (Fig. [3\)](#page-4-0). Our referring providers use SSTR PET/MRI as an alternative to a combination of SSTR PET/CT and contrast-enhanced CT of the chest, abdomen (biphasic liver protocol), and pelvis. SSTR PET/MRI has the potential to be a sensitive and specifc imaging tool for the evaluation of GEP-NENs. Some studies have already shown the promise of PET/MRI for GEP-NENs, but there is a need

for validation in larger studies [[26–](#page-12-15)[29\]](#page-12-16). Further, evaluation of lung parenchyma can be suboptimal principally due to limitations of the MR component for detection of sub-centimeter nodules. Recent developments such as free-breathing ultrashort time of echo (UTE)-based PET/MR lung imaging have the potential to address this challenge [[30\]](#page-12-17). Other practical challenges are the high upfront investment that limits the widespread availability of PET/MR, the technical complexity of image acquisition compared with PET/CT, and the complex imaging workfow that often involves multiple radiology subspecialties.

#### **Scoring systems**

Krenning score: The Krenning score (Table [3](#page-4-1)) was initially developed for SRS to assess candidacy for peptide receptor radionuclide therapy (PRRT). However, the Krenning score in its modifed form is widely extrapolated to SSTR PET, although there is limited validation for its use with SSTR PET. Besides, the Krenning score from SRS has a limited relationship with the score from SSTR PET [[20](#page-12-9)]. Compared with the Krenning score from SRS, the score on SSTR PET (i.e., modifed Krenning score) tends to be higher, especially for lesions less than 2 cm [\[20,](#page-12-9) [31\]](#page-12-18). On the other hand, the score tends to be lower in patients with a very high tumor burden. This is because of the preferential radiotracer sequestration in the NEN lesions, which causes a decrease in the physiologic uptake by the spleen and liver; this is called the 'sink efect' (Fig. [4\)](#page-5-0). These nuances are

<span id="page-4-1"></span>**Table 3** Krenning score

Grade 1	Uptake similar to the background
Grade 2	Uptake greater than the background but less than or equal to liver
Grade 3	Uptake greater than liver but less than spleen
Grade 4	Uptake greater than spleen



<span id="page-4-0"></span>**Fig. 3** 68Ga-DOTATATE PET/MRI protocol at our institution. *FSPGR* Fast-spoiled gradient-recalled echo, *IDEAL IQ* Iterative Decomposition of water and fat with Echo Asymmetry and Leastsquares estimation, *MPH* Multiphase, *Ax* Axial, *DWI* Difusionweighted imaging, *HBP* Hepatobiliary phase. The total protocol duration is around 60 min



**Fig. 4** Normal biodistribution of 68Ga-DOTATATE and the sink effect. Maximum intensity projection (MIP) image of a <sup>68</sup>Ga-DOTA-TATE PET/CT shows the normal biodistribution of <sup>68</sup>Ga-DOTA-TATE (**a**). Note the pronounced physiologic uptake in the spleen (black arrow). MIP (**b**) and coronal 68Ga-DOTATATE PET/CT (**c**)

<span id="page-5-0"></span>particularly relevant when the modifed Krenning score is used to determine eligibility for PRRT.

SSTR-RADS: SSTR-RADS is a 5-point scale-based scoring system used for the standardized classifcation and reporting of SSTR PET. It seeks to provide an objective numerical grading based on the level of confdence in the presence of a lesion, the most appropriate next step in management, and potential eligibility for PRRT. Based on the uptake pattern, the lesions are classifed into fve groups, with recommendations for each group's next step in management (Table [4\)](#page-6-0). SSTR-RADS has been demonstrated to have a high interobserver agreement [\[32](#page-12-19)]. SSTR-RADS has several advantages over the Krenning score. The Krenning score only compares the uptake in a lesion to the uptake in the liver or spleen. In contrast, SSTR-RADS entails the assessment of the entire tumor burden while considering information from all available imaging modalities (both molecular and cross-sectional imaging). These advantages have the potential to infuence treatment decisions. For instance, the Krenning score does not account for SSTR-negative neoplasms.

images of a 62-year-old male with metastatic G2 GEP-NEN show sequestration of radiotracer in the extensive metastatic osseous and liver lesions (red arrowhead) with a consequent marked decrease in the physiologic splenic uptake (red arrow), this is called the 'sink efect' (Color fgure online)

Therefore, it does not provide information about disease heterogeneity, which can be a challenge in patients with both SSTR-positive and SSTR-negative lesions. These patients may be candidates for combination therapies such as PRRT with either chemotherapy or loco-regional therapy. The use of SSTR-RADS in clinical practice may face resistance from radiologists due to its complexity and the potential to impact their workfow negatively. Prospective multicenter studies are warranted to demonstrate the beneft of SSTR-RADS for response and outcome prediction, which will facilitate its adoption in clinical practice.

## **SSTR PET in the context of PRRT**

PRRT is the therapeutic use of radiolabeled molecules such as somatostatin analogs (SSA) that target the SSTRs on NENs. PRRT represents a precision medicine paradigm that tailors a minimally invasive treatment specifc to the biological profle of the tumor. SSTR PET is the new reference standard investigation for patient selection for PRRT,

#### <span id="page-6-0"></span>**Table 4** Overview of SSTR-RADS



\*Levels of uptake: 1-less than or equal to blood pool, 2-greater than blood pool but less than or equal to the liver, and 3-greater than the liver *SSTR-RADS* Somatostatin receptor PET-reporting and data system, *PRRT* Peptide receptor radionuclide therapy, *CI* Conventional imaging, *BPH* Benign prostatic hyperplasia, *NEN* Neuroendocrine neoplasm, *LN* Lymph node, *F/u* follow-up

endorsed by the National Comprehensive Cancer Network guidelines  $[33]$  $[33]$ . Only patients with tumors that sufficiently express SSTRs on SSTR PET qualify for treatment; this provides an optimal selection strategy. In contrast, patients with lesions that demonstrate lower SSTR uptake are not eligible for PRRT. Typically, the threshold for positive expression on SSTR PET that would lead to PRRT consideration is defned as tumor uptake more than the liver or a Krenning score  $>2$ [\[34,](#page-12-21) [35\]](#page-12-22). SUV-based thresholds of positive SSTR expression on SSTR PET have been proposed [[36,](#page-12-23) [37](#page-13-0)]. However, due to the signifcant variability and lack of standardization of SUV measurements on SSTR PET, clinical adoption of SUV-based criteria is not feasible. In addition to SSTR expression, SSTR PET also provides personalized information pertinent to management, like the detection of SSTRnegative lesions that may require additional targeted therapy.

#### **Response assessment and outcomes prediction**

Morphology or size-based response assessment criteria are suboptimal for NENs due to their low growth rate and since

systemic therapies tend to stabilize rather than shrink the tumor. Post-therapy SSTR PET has shown variable results for treatment response evaluation in NENs and is further confounded by other challenges. Standard PET response assessment criteria such as PERCIST and the EORTC criteria cannot be directly translated to SSTR PET due to the signifcant variability in SUVs on SSTR PET. In addition to scanner-related factors, this variability can also be attributed to the widespread therapeutic usage of long-acting SSAs, which tend to decrease physiologic radiotracer uptake and increase tumoral uptake after long-term use [[38](#page-13-1)]. Besides, the diverse treatment options, each with diferent tumor involution mechanisms, are not amenable to a single response assessment criterion. Due to these challenges, response assessment in clinical practice is often centered on the disappearance of known lesions to indicate favorable treatment response or the detection of new lesions to indicate disease progression. This paradigm is endorsed by multidisciplinary guidelines [[18](#page-12-7)]. In the future, a combination of molecular imaging and blood-based biomarkers may improve treatment response assessment in patients with NENs [\[39](#page-13-2)]. For instance, the NETest analyzes 51 specifc circulating mRNA sequences specifc to GEP-NENs and has a high accuracy for response assessment of small intestinal and pancreatic NENs [\[39](#page-13-2)[–42](#page-13-3)]. Recently, it has been demonstrated that a persistently positive NETest after a seemingly complete resection predicts early radiologic recurrence with high accuracy [[43](#page-13-4), [44](#page-13-5)]. Integration of this information with imaging parameters from SSTR PET could be incremental due to their mechanistic diferences.

On the other hand, the prognostic and predictive signifcance of SSTR expression has been validated. In general, higher uptake on baseline pre-therapy SSTR PET correlates with superior post-PRRT outcomes [[36](#page-12-23), [37](#page-13-0), [45](#page-13-6)[–47\]](#page-13-7). Furthermore, volumetric PET metrics such as SSTR-expressing tumor volume (SSTR-TV), which represents the total tumor volume with SSTR expression above a threshold (e.g., 50% of the  $\text{SUV}_{\text{max}}$ ), and total lesion SSTR expression (TL-SSTR), which is the product of SSTR-TV and  $\text{SUV}_{\text{mean}}$  correlate with post-PRRT outcomes such as progression-free survival and time-to-new treatment [[48–](#page-13-8)[51\]](#page-13-9).

### **Pitfalls of SSTR PET**

It is imperative to be aware of potential pitfalls and sites of physiologic uptake on SSTR PET that can bias its interpretation. The maximum physiologic uptake of  ${}^{68}Ga$ -DOTATATE is in the spleen, followed by the kidneys, adrenals, and liver with variable uptake in the stomach, pituitary gland, head of the pancreas, thyroid gland, and uterus (Fig. [4](#page-5-0)) [\[52](#page-13-10)]. Physiologic intense uncinate process uptake occurs in up to 30% of patients and can mimic a neoplasm [[53,](#page-13-11) [54](#page-13-12)]. This occurs due to the high physiologic density of SSTR expression in the islet cells of the uncinate process [[55\]](#page-13-13). This physiologic uptake can often be diferentiated from a neoplasm by its relatively non-circumscribed nature and characteristic curvilinear shape, which is best appreciated on coronal maximum intensity projection images. Apart from the uncinate process, low-level uptake can also be seen throughout the pancreas due to scattered islet cell clusters.

The liver shows high physiologic uptake of <sup>68</sup>Ga-labeled SSTR compounds, which can obscure small liver metastases on SSTR PET. Newer radiotracers like <sup>64</sup>Cu-DOTATATE have the advantage of lower physiologic liver uptake. A combined PET/MRI protocol with hepatobiliary contrast agents like gadoxetate also helps improve diagnostic confdence and accuracy (Fig. [2](#page-3-0)) [\[17](#page-12-6), [22\]](#page-12-11).

Splenunculi near the pancreatic tail can be confused with a NEN (either a primary tumor or a peritoneal deposit). Splenunculi often demonstrate lower SSTR uptake than the spleen, likely due to their lower vascularity, and diferentiation solely on SSTR PET is usually not possible. A denatured red blood cell SPECT or <sup>99</sup>Tc-labeled sulfur-colloid scan is confrmatory [\[35](#page-12-22)]. Splenunculi have high uptake on these scintigraphic studies, whereas NENs tend to be photopenic (Fig. [5\)](#page-8-0). In patients with a very high burden of SSTRavid metastatic disease, the combination of low background and high radiotracer uptake can lead to a "sink effect", which refers to high radiotracer sequestration in diseased organs with consequent reduction at sites of physiologic uptake (e.g., spleen). This phenomenon impacts PET-scoring systems (e.g., Krenning score) as well as PRRT dose considerations [[56\]](#page-13-14).

Osteoblasts also tend to have SSTR expression. Therefore, variable degrees of radiotracer uptake can be seen in osteoblastic lesions like fractures, osteoblastic metastasis, Paget's disease, and fbrous dysplasia. For instance, osseous hemangiomas can be mistaken for metastases as they often show tracer uptake on SSTR PET (Fig. [6\)](#page-9-0). In such instances, their characteristic appearance on the attenuation correction CT component—bone demineralization with thickened trabeculae manifesting as vertical striation on sagittal images ("corduroy sign") and as small punctate areas of sclerosis on axial images ("polka-dot" appearance) can help with correct interpretation [\[57](#page-13-15)]. However, diferentiation from metastasis can be difficult on PET/MRI because the characteristic morphology of these lesions may not be appreciated on the MR component. In addition, leukocytes and macrophages also express SSTR, which can result in variable radiotracer uptake at sites of infection or infammation.

Numerous non-neuroendocrine neoplasms such as meningiomas and epithelial tumors (e.g., lung, esophageal, breast, colorectal, and testicular) can show variable uptake on SSTR PET. In addition, benign lesions such as thyroid adenomas, hyperplastic prostate nodules, lymphoid hyperplasia, and serous cystadenomas of the pancreas may also show lowlevel uptake [[53,](#page-13-11) [58\]](#page-13-16).

# **18F‑FDG PET**

 $18$ F-FDG PET is complementary to SSTR PET for poorly diferentiated or high-grade NENs. Well-diferentiated and low-grade NENs tend to have low rates of glucose metabolism. Nevertheless, FDG uptake can be seen in up to 40% of such neoplasms [\[59](#page-13-17)]. As the NENs de-diferentiate towards high-grade NENs and NECs, there is upregulation of glucose transporters and downregulation of SSTRs, referred to as the 'fip-fop' phenomenon. There also tends to be signifcant intra-lesional and inter-lesional variability in any given patient (Fig. [7](#page-10-0)). Therefore, some clinical practices perform both SSTR and FDG PET in many patients to characterize disease heterogeneity, risk stratify disease groups, and assess the potential of response to PRRT. For instance, the combination of high SSTR and low FDG uptake portends a high likelihood of response to PRRT. Secondly, FDG PET can guide treatment options to augment PRRT, such as targeted <span id="page-8-0"></span>**Fig. 5** SSTR PET and sulfurcolloid SPECT for diferentiation of splenunculus from NEN. MR images (**a**–**d**) of a 50-year-old woman showed a well-circumscribed mass near the pancreatic tail with signal intensity and post-contrast enhancement mirroring that of the spleen on T2-weighted image (**a**), difusion-weighted image (**b**), arterial phase image (**c**), and coronal delayed postcontrast image (**d**). A <sup>99m</sup>Tc sulfur-colloid SPECT (**e**) demonstrated no radiotracer uptake in the mass, which excluded the possibility of a splenunculus and suggested NEN as the etiology. Subsequent 68Ga-DOTA-TATE PET/CT demonstrated intense radiotracer uptake in the mass and the diagnosis of well-diferentiated NEN was confrmed on histopathology evaluation of the distal pancreatectomy specimen



external radiation to FDG-avid but SSTR-negative lesions. Therefore, a combination of FDG and SSTR PET can facilitate personalized treatment decisions for NENs.

FDG PET also has strong prognostic utility in NENs [\[60](#page-13-18)[–62](#page-14-0)]. Lesions with high FDG and low SSTR uptake have a worse prognosis than those with high SSTR and low FDG uptake. In NECs, a maximum standardized uptake value  $(SUV_{max})$  > 3 on FDG PET is an independent risk factor for disease progression [\[59,](#page-13-17) [63\]](#page-14-1). FDG PET may also provide prognostic information incremental to the WHO grade. In patients with G3 NENs, uptake on FDG PET correlates strongly with overall survival  $(OS)$  [\[61](#page-13-19)]. This can potentially help stratify G3 NENs into low and high-risk groups, which is currently not possible on histology. Similarly, FDG may also stratify low-grade NENs into low and high-risk groups [[64\]](#page-14-2). Based on these data, some groups recommend FDG PET in the routine workup of NENs [\[61](#page-13-19)].

The NETPET score is a recently described imaging metric that seeks to incorporate information from both FDG and SSTR PET into a single index (Table [5\)](#page-11-8) [[65](#page-14-3)]. The lesion that shows maximum FDG uptake relative to its SSTR uptake is used as the index lesion for categorization since this lesion likely has the most aggressive phenotype. The NETPET score correlates with the WHO grade and the OS (independent of histological grade) [\[66](#page-14-4)]. Another metric, the FDZ score, can identify a subset of patients with <span id="page-9-0"></span>**Fig. 6** Vertebral hemangioma mimicking metastasis on 68Ga-DOTATATE PET/CT. 68Ga-DOTATATE PET/CT images in a 61-year-old woman with Multiple Endocrine Neoplasia type 2A. Focal radiotracer uptake is seen in a thoracic vertebral body (**a**) (white arrow), which was suggestive of being a metastasis. However, the attenuation correction CT (**c**) shows punctate sclerosis ("polka dot sign") in a pattern that is characteristic of a vertebral hemangioma. 68Ga-DOTATATE PET/CT obtained 6 months later (**b**, **d**) shows an increase in radiotracer uptake (**b**) but with a stable CT appearance (**d**). The stability and the characteristic morphology on CT confrmed the etiology as osseous hemangioma. The lesion remained stable on an MRI performed 1 year later (not shown)



G3 GEP-NENs with better outcomes [\[67](#page-14-5)]. The FDZ score normalizes the different reference  $\text{SUV}_{\text{max}}$  values from the dual-tracer PET to obtain a 'Z score' for each tracer (FDZ  $score = Z_{FDG} - Z_{DOTATATE}$ ). The FDZ score strongly correlates with OS in patients with G3 NENs, but prospective validation is needed. The clinical utility of these metrics remains uncertain because SSTR and FDG PET are not routinely performed together, and co-registration of data from both scans is needed for accurate calculation.

# **Other radiotracers**

18F-Fluorodihydroxyphenylalanine (18F-FDOPA)**,** a radiotagged precursor for serotonin biosynthesis, is preferentially taken up by NENs, particularly those arising from the midgut [[68,](#page-14-6) [69\]](#page-14-7). Small head-to-head comparison studies in patients with small intestinal NENs have shown higher sensitivity and superior lesion detection rates compared with  $^{68}$ Ga-labeled-SSAs [[70–](#page-14-8)[72](#page-14-9)]. Therefore,  $^{18}$ F-FDOPA can be a potential problem-solving tool in patients with a high index of suspicion for a midgut NEN and negative SSTR imaging [\[73\]](#page-14-10).

Radiolabeled glucagon-like peptide-1 receptor (GLP-1R) analogs (e.g., 68Ga-DOTA-exendin-4) are currently the most sensitive radiotracers for benign insulinoma localization. Insulinomas are the most common functioning NEN. Unfortunately, identification is often difficult on SSTR PET and cross-sectional imaging due to their poor SSTR expression and small size [\[74](#page-14-11)–[77\]](#page-14-12). The European Neuroendocrine Tumor Society (ENTS) guidelines endorse the use of GLP-1R PET for patients with life-threatening hypoglycemia in whom cross-sectional imaging and endoscopic ultrasound cannot localize the neoplasm [[78\]](#page-14-13). Malignant insulinomas, on the other hand, express GLP-1R in less than 40% of cases; fortunately, these neoplasms have high SSTR expression, which renders them amenable for detection on SSTR PET.

SSTR antagonists (e.g., 68Ga-NODAGA-JR11) are novel radiotracers that, unlike agonists, neither activate the SSTR nor are internalized, yet retain a high affinity for SSTRs due to the higher number of potential binding sites [[17](#page-12-6)]. Advantages include their rapid tumor binding, high tumorto-background ratio, rapid blood clearance, and optimal biodistribution profles in patients with metastatic NENs [\[79](#page-14-14)]. Despite early evidence that suggests <sup>68</sup>Ga-NODAGA-JR11 demonstrates a higher lesion-based detection sensitivity than 68Ga-DOTATOC, further comparative studies are needed to

<span id="page-10-0"></span>**Fig. 7** Dual-tracer PET imaging with <sup>18</sup>F-FDG and <sup>68</sup>Ga-DOTA-TATE. A 79-year-old gentleman with a metastatic large cell NEC<br>of GI origin. FDG PET/CT (a–c) shows multiple radiotracer-avid liver (asterisks) and osseous metastases (arrows). Subsequent <sup>68</sup>Ga-DOTATATE PET/MRI ( **d** – **f**) showed the absence of radiotracer uptake in both the liver (asterisks) and the osseous metastases (arrows) ( **e**, **f**) consistent with the expected receptor distribution of NECs. The NETPET score for this patient would be P5 since the target lesions (3 in the liver) were photopenic on SSTR PET but radiotracer avid on FDG PET. Note the high spatial coregistration of the PET and the MR data on the fused PET/MR image ( **e**, **f**) due to simultane ous co-acquisition of the two datasets











<span id="page-11-8"></span>**Table 5** NETPET scoring system for dual-tracer SSTR/ FDG PET



\*Grade P2 to P4 are further subclassified based on the number of lesions into a=1–2 lesions and b=  $\geq$ 3 lesions

*SSTR* Somatostatin receptor, *FDG* fuorodeoxyglucose

assess the diferences in the diagnostic performance of SSTR antagonists versus agonists [[80](#page-14-15)].

 $^{18}$ F-AlF-NOTA-octreotide ( $^{18}$ F-OC) is a novel  $18F$ -labeled-SSA with favorable kinetic and imaging characteristics compared to  ${}^{68}$ Ga-labeled-SSAs [[81,](#page-14-16) [82](#page-14-17)].  ${}^{18}$ F-OC has good tumor uptake and a higher liver tumor-to-background ratio than 68Ga-labeled SSAs, which is refected by the higher hepatic lesion detection rate [[81,](#page-14-16) [83](#page-14-18)]. If validated for imaging of NENs,  $^{18}$ F-OC has the potential to be an alternative to <sup>68</sup>Ga-DOTATATE in centers where <sup>68</sup>Ge/<sup>68</sup>Ga generators are not available.

# **Conclusion**

Advances in the molecular imaging of GEP-NENs have led to improved diagnosis, staging, understanding of their biology, and personalized patient management. SSTR PET is the new reference standard imaging examination for GEP-NENs and is particularly critical in the context of PRRT eligibility. SSTR PET/MRI with liver-specific contrast agent offers the prospect of one-stop-shop imaging for the evaluation of GEP-NENs. It is crucial to be aware of the potential pitfalls and areas of physiologic uptake on SSTR PET to avoid inadvertent interpretation errors. FDG PET is complementary to SSTR PET, especially in the context of high-grade NENs and NECs. Novel radiotracers under investigation have the potential to overcome existing limitations in the molecular imaging of GEP-NENs. Knowledge gaps in quantitative evaluation of molecular imaging studies and their role in response assessment are active research areas.

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# **Declarations**

**Conflict of interest** Dr. Rajamohan, Dr. Khasawneh, Dr. Singh, Dr. Suman, Dr. Majumder, Dr. Halfdanarson, and Dr. Goenka have no conflicts of interest.

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