

Can we produce an image of bacteria with radiopharmaceuticals?

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Introduction

Bacterial infection is nowadays one of the major causes of morbidity and mortality not only in developing countries but globally. Tuberculosis and multi-drug resistant bacteria are increasing and challenge the diagnostic approaches, the therapeutic schemes and the control of infection. Early diagnosis of infection and capacity to distinguish between bacterial and sterile inflammation is very important to efficiently treat patients and prevent the complications of pathology. Most infections are diagnosed by clinical history, physical examination, laboratory tests, identification of pathogens in body fluids and biopsies and by imaging techniques. There is a substantial difference in the use of non-nuclear medicine imaging techniques and the use of radionuclide techniques. The anatomical imaging

techniques such as plain radiography, ultrasonography and computed tomography are sensitive mainly in chronic stages of infection when there are significant anatomical changes. The detection of infection by nuclear medicine techniques relies on the physiological and biochemical changes at the site of lesions, which manifest much prior to the appearance of the anatomical changes.

Nuclear medicine has therefore contributed in the last years in the development of several radiopharmaceuticals, used like non-invasive tools, to discriminate between infection and sterile inflammation. However, none of these are “infection specific” because sensitivity and specificity can differ according to the type of infection, to the type of micro-organism, to the infection site and to the host clinical conditions/response. The number of micro-organisms available for targeting seems to be a major discriminating factor for nuclear medicine techniques. The paper by Akhtar and colleagues [1], published in this issue of the journal, describes the relation between bacterial number and ^{99m}Tc -UBI 29–41 uptake in mice. This provides important information about the specificity of this radiopharmaceutical but disappointingly evidences that it is difficult to discriminate between 2×10^4 and 2×10^6 bacteria, in this model, and it is probably difficult to image less than 2×10^4 bacteria, at least in a mouse. The question, therefore, arises about the minimum number of bacteria that can be detected in vivo, this being a relevant question to answer before routine clinical application of bacterial imaging in man.

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Radiopharmaceuticals for imaging bacteria

Many radiopharmaceuticals have been reported so far to detect and locate infection. These are very sensitive but do not show high specificity in the discrimination between

bacterial infection and sterile inflammation. This has been clearly summarised by Welling and colleagues [2] in a recent letter in reply to an editorial of G. Lucignani [3].

There is now a wide range of radiolabelled anti-microbial agents that are undergoing evaluation.

The first group consists of radiolabelled antibiotics such as ^{99m}Tc - or ^{18}F -ciprofloxacin [4–9], ^{99m}Tc -sparfloxacin [10], ^{99m}Tc -ceftizoxime [11, 12] and ^{18}F -fleroxacin [13], anti-fungal agents such as ^{99m}Tc -fluconazole and ^{99m}Tc -isoniazid [14] and the anti-*Mycobacterium tuberculosis* agent ^{99m}Tc -ethambutol [15]. The second group of radiopharmaceuticals for imaging infections is derived from the array of human anti-microbial peptides/proteins that binds to specific bacterial antigens [16], e.g. peptides derived from human lactoferrin [17], ubiquinidin (^{99m}Tc or ^{18}F -UBI) [18–23] and human neutrophil peptide 1–3 (^{99m}Tc -HNP1–3; members of the α -defensins) [24]. In this group, we can also include bacteriophages that specifically target bacterial antigens [25]. The third group of radiopharmaceuticals is represented by vitamins and bacterial growth factors that are necessary for bacteria growth as well as for human cell growth: in particular vitamin H, a group B vitamin, called biotin, that was labelled with ^{111}In [26].

^{99m}Tc -UBI 29–41

The anti-microbial peptides have a wide distribution throughout the animal and plant kingdom. They are produced by phagocytes, epithelial and endothelial cells and other cell types providing protection against microbial attacks [27]. Their expression is induced upon contact with micro-organisms or microbial products like lipopolysaccharides or pro-inflammatory cytokines such as tumour necrosis factor- α , interferon- γ and interleukin-1 and contributes to the innate resistance to infection. Although various anti-microbial peptides present different chemical structures, their mechanism of action is based on the interaction of the cationic charged domains of the peptides with the negatively charged surface of the outer membrane of the bacteria. Microbial membranes expose negatively charged phospholipids, e.g. lipopolysaccharide or teichoic acids, on their surface while mammalian cells segregate into the inner leaflet the lipids with negatively charged headgroups, thus explaining the poor binding of anti-microbial peptides to mammalian cells [28, 29]. A range of human anti-microbial peptides/proteins have been investigated as radiopharmaceuticals for imaging of infections. Amongst these, ^{99m}Tc -labelled ubiquinidin 29–41 peptide fragment (^{99m}Tc -UBI) is a cationic human anti-microbial peptide (MW 1.69 kDa) with the aminoacid sequence Thr-Gly-Arg-Ala-Lys-Arg-Arg-Met-Gln-Tyr-Asn-Arg-Arg and has six positively charged residues (5 Arg+1 Lys). In

animal studies, ^{99m}Tc -UBI labelled by direct method showed rapid visualisation of infections with Gram-positive and Gram-negative bacteria and little accumulation in sterile inflammation processes. ^{99m}Tc -labelled UBI 29–41 preferentially binds to bacteria and fungi in vitro and accumulates at the site of infection in experimental animal studies with fast renal clearance with minimal hepatobiliary excretion and shows the ability to detect infection foci in humans [20]. As compared to radiolabelled antibiotics, this radiopharmaceutical shows much lower uptake (as T/B ratio) in infected lesions and this raises the question whether this is due to a higher specificity and lower non-specific binding or whether it is due to the lower number of molecules bound per bacteria.

Further remarks on studies with radiopharmaceuticals for imaging bacteria

Given the previous considerations and by reviewing the literature, it emerges that it is still unclear whether it is possible to image bacteria in vivo with radiopharmaceuticals, particularly due to relatively low bacterial mass present in infection (can be less than 10^6 CFU) and, by consequence, due to the low number of targeting sites. Indeed, there is very limited published evidence that radiopharmaceuticals for bacteria bind to infected sites in a dose-dependent manner in relation to the number of bacteria. Akthar and colleagues [1], in this issue of EJNM&MI, try to answer this question but it is not possible to make a comparison with other radiopharmaceuticals of this kind. This is due, in part, to the difficulty of planning similar in vivo experiments, considering the fast bacterial doubling time in vivo, different biodistribution, affinity and specific activity of radiopharmaceuticals.

Overall, we lack basic studies to clearly prove the mechanism of action and binding of these radiopharmaceuticals to bacteria. As an example, the use of in vivo displacement studies (typically using large amounts of unlabelled products) are limited because of bactericidal activity of these compounds that, in large amounts, may significantly reduce the number of target sites [30]. Furthermore, since the growth of bacteria is logarithmic, it is possible to calculate the theoretical number of bacteria only up to 1 or 2 h after injection in animal models and therefore the radioactivity associated to bacteria at site of infection. In many papers, images have been acquired 4 h or even 24 h after bacterial inoculation.

What is the minimum number of bacteria that we can image?

In theory, it is possible to calculate the number of labelled molecules of some radiopharmaceuticals bound to bacteria

at the site of infection. This can be calculated on the basis of the molecular weight and specific activity of the radiopharmaceutical, the number, size and surface-to-volume ratio of bacteria. The specific activity of most anti-microbial radiopharmaceuticals can be obtained from data published by different authors in the literature as well as the number of bacteria at the time of imaging and the accumulated radioactivity at the site of injection (Table 1). Because of the small size of the majority of bacteria that are no larger than the average of eukaryotic cells (<20 μm), all bacteria have a large surface-to-volume ratio varying from about 3:1 (for bacteria with diameter of 2 μm) to 0.3:1 (for bacteria with diameter of 20 μm). This is an advantage if the binding site of radiopharmaceuticals is located on the cell surface. Bacteria volume and mass are more difficult to calculate and vary according to shape and size of bacteria. For example, *Staphylococcus aureus* has an average volume of about 1.76 μm^3 (0.5–1 μm cell diameter) while *Mycobacterium tuberculosis* has a volume of about 8.4 μm^3 (2–4 μm in length and 0.2–0.5 μm in width). The weight of an average bacterium is reported to be about $5\text{--}15 \times 10^{-7}$ g [31]. Therefore, the available targeting mass of 10^6 *S. aureus* is about 1.76 mm³, very small if compared to the mass of 10^6 granulocytes which is about 1.4 cm³ ($4/3\pi r^3$ for 14 μm diameter), 1,000-fold more than bacteria. Despite surface binding sites in bacteria being 10- to 50-fold more than those present on granulocytes, it is difficult to believe that we can image such a small mass of bacteria with the available technology.

If we then calculate the number of bound molecules of radiopharmaceutical per single bacteria, a wide range of results appear (Table 1) and this suggests that, at least for some radiopharmaceuticals, the majority of radioactivity

accumulated at the site of infection is non-specifically bound to bacteria and is due to the presence of plasma leakage from capillaries.

Host response to microbial infection

Another aspect that we should consider when attempting to image bacteria is that infection associated with prosthetic joints is typically caused by micro-organisms that grow in biofilms. Within biofilms, micro-organisms are enclosed in a polymeric matrix and develop into an organised, complex community with structural and functional heterogeneity. In the biofilm, microbes are protected from anti-microbial agents and host immune responses [32, 33]. In these conditions, the radiolabelled anti-microbial agents cannot interact with bacteria but only with the extra-cellular matrix giving information not suitable for specific antibiotic treatment of the prosthetic infection.

Last but not least, it is necessary to consider the host response to an infection process. Under the same conditions (with same number of bacteria), bacteria growth is dependent on host reaction, particularly on macrophage and monocyte response. These cells can control infection spreading in a fast or slow way in accordance with their number and functionality that change between different living beings and different tissues and psychological/metabolic condition of the host. In some cases, associated oedema and vascular leakage can also be readily induced by bacterial toxins produced by a very low number of bacteria (thus increasing the possibility of non-specific accumulation of radiopharmaceuticals) and, in other cases, a large number of bacteria may give rise only to a minor host response. Some radiolabelled anti-microbial agents

Table 1 Calculation of number of living bacteria at 4 h after injection in animal models and activity/bacteria of some radiolabelled anti-microbials

Radiolabelled anti-microbial	Specific activity (mean)	μCi per molecule	Type of bacteria	Calculated no. of bacteria at site of infection at time of imaging ^a	μCi per bacteria ^b	Calculated bound molecules per bacteria	Reference used for analysis
^{99m} Tc-UBI (29–41)	5 $\mu\text{Ci}/\mu\text{g}$	9×10^{-14}	<i>S. aureus</i>	2.58×10^8	4.18×10^{-9}	2,000,000	[1, 22]
^{99m} Tc-UBI (29–41)	6.7 $\mu\text{Ci}/\mu\text{g}$	4×10^{-16}	<i>S. aureus</i>	1.17×10^{12}	5.1×10^{-12}	10,000	[21]
^{99m} Tc-ciprofloxacin	5 $\mu\text{Ci}/\mu\text{g}$	29.7×10^{-20}	<i>S. aureus</i>	5×10^8	3.55×10^{-8}	241×10^8	[8]
^{99m} Tc-ciprofloxacin	5 $\mu\text{Ci}/\mu\text{g}$	32×10^{-20}	<i>S. aureus</i>	10^7	1.59×10^{-9}	105×10^9	[6]
^{99m} Tc-sparfloxacin	5.4 $\mu\text{Ci}/\mu\text{g}$	4×10^{-15}	<i>S. aureus</i>	5.83×10^{11}	7.4×10^{-11}	900,000	[10]
^{99m} Tc-isoniazid	5.4 $\mu\text{Ci}/\mu\text{g}$	1×10^{-15}	<i>S. aureus</i>	5.85×10^{15}	1.6×10^{-14}	300	[14]

Calculations have been made on the basis of information published by authors and of personal communication in the case of Tc-UBI kindly provided by Dr. M. Welling

^a This has been calculated using the following formula $b=B \times 2^n$, where b is the number of bacteria at time of imaging, B is the number of injected bacteria (CFU/ml) and n is the number of generations of bacteria, calculated on the basis of time interval occurred between injection and imaging. The number n is different for each type of bacteria

^b This has been obtained by calculating the ratio between the %ID at site of infection reported in each paper and the number of bacteria at site of infection at the time of imaging

have also shown to bind to monocytes and granulocytes [34–37].

From these considerations, it appears that we still need to investigate many basic aspects to better understand the mechanisms of binding and accumulation of radiopharmaceuticals to bacteria in the hope of finding a specific and reliable tool for imaging infection that can be used in clinical settings together or instead of the scintigraphy with radiolabelled autologous leukocytes or radiolabelled monoclonal antibodies to granulocyte antigens.

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