# **Apoptosis-detecting radioligands: current state of the art and future perspectives**

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Abstract. This review provides a critical and thorough overview of the radiopharmaceutical development and in vivo evaluation of all apoptosis-detecting radioligands that have emerged so far, along with their possible applications in nuclear medicine. The following SPECT and PET radioligands are discussed: all forms of halogenated Annexin V (i.e. <sup>123</sup>I-labelled, <sup>124</sup>I-labelled, <sup>125</sup>I-labelled, 18F-labelled), 99mTc/94mTc-labelled Annexin V derivatives using different chelators and co-ligands (i.e. BTAP, Hynic, iminothiolane, MAG<sub>3</sub>, EDDA, EC, tricarbonyl, SDH) or direct 99mTc-labelling, 99mTc-labelled Annexin V mutants and 99mTc/18F-radiopeptide constructs (i.e. AFIM molecules), 111In-DTPA-PEG-Annexin V, 11C-Annexin V and 64Cu-, 67Ga- and 68Ga-DOTA-Annexin V. In addition, the potential role and clinical relevance of anti-PS monoclonal antibodies and other alternative apoptosis markers are reviewed, including: anti-Annexin V monoclonal antibodies, radiolabelled caspase inhibitors and substrates and mitochondrial membrane permeability targeting radioligands. Nevertheless, major emphasis is placed on the group of Annexin V-based radioligands, in particular 99mTc-Hynic-Annexin V, since this molecule is by far the most extensively investigated and best-characterised apoptosis marker at present. Furthermore, the newly emerging imaging modalities for in vivo detection of programmed cell death, such as MRI, MRS, optical, bioluminescent and ultrasound imaging, are briefly described. Finally, some future perspectives are presented with the aim of promoting the development of potential new strategies in pursuit of the ideal cell death-detecting radioligand.

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## **Introduction on cell death**

Apoptosis is a common and universal mechanism of cell death, which was originally defined by Kerr et al. in 1972 [1] and has since been widely accepted by the scientific community. However, the first pathological descriptions of the cell death process date from the end of the nineteenth century. Although apoptosis and necrosis are commonly described as the two major cell death processes, there is also a third distinct but closely related form of cell death, referred to as oncosis; this term is employed to describe the pre-lethal stages of necrosis.

Necrosis or accidental cell death, including oncosis, is the most frequent type of cell death and is induced by a variety of sudden and severe non-physiological insults, including chemical or physical noxious insults and ischaemic or inflammatory injury. The process is characterised by progressive cell swelling, denaturation and coagulation of cytoplasmic proteins, disintegration of subcellular organelles and irreversible collapse of the plasma membrane integrity; this causes the release of cytotoxic cell components, thereby provoking an inflammatory response around the necrotic centre. In general, cell death by necrosis involves groups of cells and is often followed by the development of fibrotic tissue with distortion of the local tissue's architecture [2–4].

Apoptosis, however, is an energy-dependent, genetically controlled process by which cell death is activated through an internally regulated suicide program. In contrast with necrotic cell death, apoptosis tends to occur during less intense, chronic tissue insult. Once initiated, apoptosis is characterised by a cascade of morphological and biochemical events which finally leads to the cell's demise if it has not previously been rescued by antiapoptotic agents. The most prominent hallmarks of cells entering apoptosis include: phosphatidylserine (PS) externalisation, cytoplasm shrinkage, chromatin and nucleus condensation, DNA degradation and fragmentation of the cell into smaller "apoptotic bodies" by a budding process [5–8]. Finally, these membrane-enclosed bodies are engulfed and phagocytosed by macrophages and neighbouring cells, which then remove the cell fragments without inducing any concomitant inflammatory response. An unusual failure in this final clearance step may cause these cell fragments to degrade in a way similar to necrosis, leading to an inflammatory response, and is therefore defined as secondary necrosis. Thus, the apoptotic process can be divided into at least four functionally distinct phases: initiation, execution, degradation and elimination [9, 10].

Currently, two distinct types of pathway have been described by which apoptotic cell death is initiated: through death receptors or via the mitochondria. Nonetheless, both of these exclusive pathways eventually culminate in a mutual proteolytic cascade consisting of cystein aspartic acid-specific proteases (i.e. caspases), which act as executioners of the induced cell death process.

The death receptor pathway, also defined as the extrinsic cell death pathway, mainly consists of soluble or membrane-bound death ligands such as tumour necrosis factor  $\alpha$  (TNF- $\alpha$ ), Fas ligand (FasL) or TNF-related apoptosis-inducing ligand (TRAIL) which bind to their corresponding receptors. Subsequently, trimerisation of the receptor and binding to the cytoplasmic Fas-associated death domain adaptor protein (FADD) result in the formation of a death-inducing signalling complex (DISC). Finally, the DISC complex triggers the recruitment and activation of procaspase-8 and procaspase-3 followed by cleavage and activation of important downstream effector caspases such as procaspase-6, procaspase-8 and procaspase-10. These activated caspases cause cytoplasmic proteolysis and activation of DNAses which induce systematic degradation of nuclear DNA into multiple fragments of typically 180–200 bp [11, 12]. To date, seven types of death receptor have been described, including the Fas (CD95 or APO-1), TNF and TRAIL death receptor families [13–15].

On the other hand, the mitochondrial or intrinsic pathway is initiated by a variety of biochemical factors like oxidative and genotoxic stress, ischaemia, DNA damage, increased Ca2+ levels and chemotherapeutic drugs which provoke the release of pro-apoptotic factors like apoptosis-inducing factor (AIF), Smac, procaspases and cytochrome *c* from the mitochondria into the cytoplasm. Afterwards, the rise in cytoplasmic cytochrome *c* activates procaspase-9 and procaspase-3 consecutively, thereby resulting in a convergence with the death receptor pathway [12, 16]. AIF is able to proteolytically activate caspase-3 and nuclear endonucleases by itself. In contrast, cytochrome *c* requires interaction with additional proteins, including Apaf-1 (which binds ATP) and caspase-9 (Apaf-3), which together can activate procaspase-3. This complex of interacting proteins is called the "apoptosome".

Although distinctly different from each other in their initial phase, significant cross-talk between the extrinsic and intrinsic pathways has been demonstrated [17, 18]. This interaction is primarily possible due to a protein called Bid. In particular, once the death receptor pathway has been initiated, activated caspase-8 is able to truncate Bid, which in turn translocates to the mitochondria in order to contribute to cytochrome *c* release. Furthermore, both pathways are capable of inducing cell membrane alterations like PS externalisation in the early phase of apoptosis, through common activation of caspase-3.

Apoptosis is a highly conserved form of programmed cell death (PCD) that plays an important role in multiple physiological processes like organ development, tissue homeostasis and regulation of the immune system since many organisms use this mechanism to selectively eliminate unwanted cells. However, when the physiological balance between survival and death signals tilts towards cell death, the apoptosis program is engaged and culminates in a variety of pathological conditions (Table 1) [19–23]. Excessive apoptosis is known to result in progressive loss in tissue functionality, as occurs in acute myocardial infarction (AMI), chronic heart failure, allograft rejection, stroke, neurodegenerative disorders (e.g. Alzheimer's, Parkinson's and Huntington's disease) and inflammation. In contrast, autoimmune diseases like systemic lupus erythematosus (SLE) and rheumatoid arthritis are characterised by insufficient apoptosis, which enables immunologically competent cells (i.e. autoreactive lymphocytes) to survive and to injure healthy organs inappropriately. In addition, pronounced loss in normal apoptosis leads to excessive cell proliferation and subsequent tumour development [18, 24–27]. Furthermore, the beneficial or detrimental effect of many drugs can be attributed to their action on the apoptotic process [28–33]. Accordingly, non-invasive in vivo monitoring of the rate and extent at which apoptosis occurs, may provide clinicians with relevant clinical information on disease activity and therapeutic efficacy [34–36].

## **PS-targeting radioligands**

## *Annexin V*

Annexin V is a member of the calcium and phospholipid binding superfamily of Annexin proteins, of which at least 13 members have been identified in a variety of organisms in the animal and plant kingdoms [37–40]. Since the protein was originally found to possess vascular





AMI, Acute myocardial infarction; ARVD, arrhythmogenic right ventricle dysplasia; CAD, coronary artery disease; CHF, congestive heart failure; MODS, multiple organ dysfunction syndrome; SLE, systemic lupus erythematosus

anticoagulant activity, various synonyms have been used in the literature, including: placental protein 4 (PP4), placental anticoagulant protein I (PAP I), vascular anticoagulant protein alpha (VAC $\alpha$ ), lipocortin-V, endonexin II and calcium-dependent phospholipid binding protein (CaBP33) [41–44]. Like the other Annexin members, Annexin V is widely expressed in eukaryotic organisms. The protein is mainly found intracellularly on the cytosolic side of plasma membranes, although very low concentrations (1–6 ng/ml) circulate in the blood compartment of healthy humans [45, 46]. Furthermore, the protein is ubiquitously expressed in a variety of cell types, including: cardiomyocytes, vascular endothelium, erythrocytes, thrombocytes, lymphocytes, glial cells, astrocytes, oligodendrocytes, Schwann cells, skeletal muscles, hepatocytes, bronchi, chondrocytes and osteoblasts [45–51].

The mature Annexin V molecule consists of 319 amino acids with a total molecular weight of 35.8 kDa. The protein is folded into a planar cyclic arrangement with a unique N-terminal region followed by four homologous repeats of approximately 70 amino acids, each of which is composed of five alpha-helical segments. Similar to the other Annexin family members, every tandem repeat contains a highly conserved sequence of 17 amino acids, termed the "endonexin fold", which harbours a characteristic  $Ca^{2+}$ - and phospholipid- binding site [50–54]. Furthermore, the 3D structure of Annexin V is characterised by a concave and a convex side. The concave surface of the protein harbours the amino terminal tail and carboxy terminal tail, whereas the convex side bears the calcium binding sites located within the endonexin loop sequences.

Over the past years many studies have focussed on elucidating the biological functions of Annexins. Originally, Annexin V was found to exhibit potent vascular anticoagulant activity due to its inhibitory effect on prothrombin activation [55] and its ability to effectively prevent thrombus formation under normal physiological conditions. In addition, the protein is capable of inhibiting phospholipase  $A_2$  (PLA<sub>2</sub>) activity, thereby exerting anti-inflammatory properties due to its ability to prevent arachidonic acid release by  $PLA_2$  [56, 57]. The protein also acts as an inhibitor of protein kinase C (PKC).

Most of the known biological functions of Annexin V can be attributed to its high affinity for negatively charged phospholipids in the presence of physiological concentrations of calcium. In particular, Annexin V is known to bind selectively with nanomolar affinity  $(K_d \approx 0.5-7 \text{ nM})$  to membrane bound PS residues [42, 55, 58]. Thus, PS binding of Annexin V not only proceeds very rapidly, but is also strongly dependent on the presence of Ca2+ ions. The molecular mechanism of action by which Annexin V binds to PS residues will be explained further (cf. 99mTc-Annexin V Mutants, below).

Based on these observations, Annexin V was originally labelled with different fluorescent tags (e.g. FITC) and is now routinely used for histological and cell-sorting studies to identify and quantify apoptotic cells [59–62]. However, all of these detection methods (i.e. microscopy, immunohistochemistry, flow cytometry) are either characterised by specific problems in detectability or exhibit restricted applicability in vitro and often require invasive sampling techniques like biopsies [63–66]. Other methods like the TUNEL assay (terminal uridine deoxynucleotidyl end-labelling) often lack sensitivity in quantifying the process since their detection mechanism only targets cells in a later stage of the apoptosis cascade, when phagocytosis of apoptotic cells is already occurring in vivo.

In analogy, Annexin V can also be radiolabelled with radionuclide tags such as <sup>99m</sup>Tc or <sup>123</sup>I for non-invasive detection and quantification of apoptosis in vivo [67–70]. Initial in vitro studies with normal and sicklecell erythrocytes, activated blood platelets and tissue factor (TF)-expressing fibroblasts or ovarian carcinoma cells clearly demonstrated the proof of concept that early apoptosis could be detected successfully with radiolabelled Annexin V [71]. Since then, extensive progress has been made in the in vivo evaluation of radiolabelled Annexin V in animals and humans and in the development of alternative cell death radioligands.

Annexin V was originally isolated from placental tissue of human or other origin [72, 73]. However, recombinant human Annexin V (rh-Annexin V) is currently being produced by cytoplasmic expression in *Escherichia coli* [74–76]. Due to its fairly low molecular weight, the recombinant protein can easily be generated in high (i.e. milligram) yields with excellent purity and is very unlikely to trigger an immune response compared with murine monoclonal antibodies or murine/bovine Annexin V. Furthermore, unlike Annexin V originating from human placentas, rh-Annexin V can be considered practically free of human plasma constituents while containing extremely low endotoxin levels, allowing its use in various clinical applications.

## *PS expression as a cell death target*

According to the existing major cell death pathways described in the literature, several of the involved processes may serve as a specific target for new apoptosis radioligands, including: PS exposure, caspase activation, mitochondrial permeability transition, FasR expression, and TNF-α-mediated cell death. Until now, interest has focussed on the phenomenon of PS externalisation. In general, eukaryotic plasma membranes exhibit significant phospholipid asymmetry, with choline-containing phospholipids such as phosphatidylcholine (PC) and sphingomyelin (SM) mainly being expressed on the extracellular side of the cell. In contrast, aminophospholipids like PS and phosphatidyl ethanolamine (PE) are largely confined to the inner side of the phospholipid bilayer, representing the two major lipid components in this compartment. In fact, PS residues are the only phospholipids which are virtually absent on the outer cell membrane layer [77, 78]. This asymmetrical phospholipid distribution is regulated enzymatically by aminophospholipid translocase activity which catalyses the transportation of PS and PE residues from the outer to the inner leaflet of the cell membrane under normal cellular conditions. Conversely, a second enzyme called scramblase controls the bidirectional transbilayer movement of all phospholipids [79–81].

One of the early hallmarks of cells entering the apoptosis cascade is the fast externalisation of PS residues from the cytoplasmic to the extracellular side of the membrane. This PS surface exposure results from a deactivation in the translocase and floppase activity in combination with an enhanced scramblase activity (Fig. 1). Although many chemical (e.g. chemotherapeutics, glucocorticoids) [82–84], physical (e.g. UV radiation, γ-radiation, heat) [85–87] and biochemical factors (e.g. hypoxia, osmotic imbalance, high  $Ca^{2+}$  levels, nitrogen oxide) [88] are able to induce apoptosis in vitro and in vivo, the basic mechanism of PS expression on the membrane of cells entering apoptosis always proceeds regardless of the apoptosis-inducing agent or cell type [89, 90]. Most interestingly, PS externalisation precedes most of the other events within the apoptosis cascade, including: cytoplasm shrinkage, condensation of the nucleus, DNA degradation and fragmentation of the cell into smaller apoptotic bodies [89–91]. Since the membrane-engulfed cell fragments are removed by phagocytic cells in the final stage of apoptosis, externalisation of PS residues to the surface of dying cells acts as a



**Fig. 1.** The regulation and physiology of membrane PS asymmetry. This model depicts how the membrane PS asymmetry is generated and drastically altered in PS-related (patho)physiological processes such as blood coagulation (including thrombocyte activation), thrombosis and apoptotic cell death. At physiological Ca2+ concentrations, the asymmetrical phospholipid distribution is enzymatically promoted by translocase and floppase activity and inactive scramblase. The ATP-dependent aminophospholipid-specific translocase catalyses the transportation of PS residues and PE residues from the outer to the inner leaflet of the cell membrane. Conversely, the ATP-dependent non-specific lipid floppase slowly transports lipids from the cell's inner to outer side whereas the Ca2+-dependent non-specific lipid scramblase controls the bidirectional transbilayer movement of all phospholipids. Elevated intracellular Ca2+ levels will facilitate membrane blebbing through calpain activation and induce PS externalisation by providing a deactivation in the translocase and floppase activity in combination with an enhanced scramblase activity. Subsequently, the apoptotic cells which express PS residues are recognised and eliminated by macrophages (adapted from Zwaal and Schroit [80])

"recognition and elimination" signal for macrophages which express the PS receptor [92–94]. Concordantly, apoptotic cell death represents a dynamic process, which provides a temporary time window for detection in vivo.

The number of PS-binding sites for Annexin V on human erythrocytes and resting platelets has been reported as 278 and 5,000 sites/cell, respectively, [95–97]. However, this number significantly increases to 2×105/cell for activated blood platelets and 8.8×106 per cell in the case of endothelial cells [98], whereas apoptotic tumour cells have been shown to express up to  $6-24\times10^6$  sites/cell [99]. Taking into account the stoichiometry of Annexin V binding to PS residues, four to eight Annexin V molecules are able to bind per exposed PS residue [100]. Hence, considering all these findings, the loss of PS asymmetry constitutes a very attractive target for early in vivo detection of PCD. Consequently, about 90% of the currently developed apoptosis radioligands consist of Annexin V-based PS-targeting molecules. Additionally, fast translocation of PS residues to the outer side of the cell membrane is also known to take place in sickle-cell erythrocytes and during the process of blood platelet activation since PS expression is essential for the platelet pro-coagulant activity. Therefore, fluorescent or radiolabelled Annexin V also appears very promising for in vivo detection of atherosclerotic plaques or thrombi which contain high amounts of activated platelets and apoptotic monocytes [96, 101–103].

With regard to the specificity of apoptosis detection by PS targeting, one should take into account the fact that cells dying by necrosis will also allow binding with Annexin V ligands since the intracellular PS residues become readily accessible for binding as soon as the plasma membrane ruptures. Consequently, in vivo discrimination between apoptotic and necrotic cell death using PS-targeting radioligands will be very difficult.

## *Radiolabelled Annexin V derivatives*

#### Halogenated Annexin V

Annexin V and its derivatives have been labelled with most halogens, including 123I, 125I, 124I and 18F, thereby providing a broad range of imaging applications in apoptosis research from single-photon emission computed tomography (SPECT) and autoradiography to positron emission tomography (PET). Somewhat similar to the group of 99mTc-Annexin V radioligands, halogenated Annexin V was produced by either direct or indirect radiolabelling methods, as described below.

*123I/125I-Annexin V.* Direct iodination of proteins and peptides by means of electrophilic aromatic substitution of the molecule's tyrosine residues has been used in radiochemistry for many years owing to the simplicity and easiness of the technique. The most commonly used techniques are the IodoGen, IodoBead, chloramine-T (CAT) or enzymatic lacto-, bromo- or myeloperoxidase methods.

Preparation of 123I-Annexin V and 125I-Annexin V using the IodoGen method [104] was originally described by the group of Tait et al. in the early 1990s [96]. Iodination of Annexin V usually consisted of a one-pot reaction in which the protein was radiolabelled at pH 7.5–8 at room temperature, using IodoGen-coated reaction vials, after which the reaction was quenched with sodium metabisulphite and/or NaI. Additional purification of the radioligand by gel filtration or extensive dialysis resulted in excellent radiochemical purities of greater than 99% while retaining full anticoagulant and phospholipid binding activity [105–107]. Only one study has reported so far on the preparation of 125I-Annexin V by means of the enzymatic lactoperoxidase-glucose oxidase method [108]. Similar to the IodoBead method, enzyme-coated beads were applied in this approach as solid phase oxidant generating significantly higher specific activities. Although radiolabelling of Annexin V according to the IodoGen or enzymatic method was not optimised, 123I/125I-Annexin V was used in many in vitro and in vivo studies for several years and its usefulness in detecting PS expression was clearly demonstrated. Most in vitro studies with iodinated Annexin V consisted of radioligand binding assays with normal and sickle-cell erythrocytes [74, 105], activated blood platelets [95, 96, 107, 108] and tissue factor (TF)-expressing fibroblasts [109] or ovarian carcinoma cells [110]. Originally, radioiodinated Annexin V was tested ex vivo as a potential platelet-directed thrombus imaging agent in rabbits and swine [76, 101, 106]. 125I/123I-Annexin V selectively targeted thrombi in rabbit iliac and swine carotid arteries, resulting in thrombus/blood ratios of 6.4 and 6.9, respectively, within 2 h post injection (p.i.). Left atrial thrombi were found to provide even higher thrombus/blood uptake ratios, of ca. 13.4, indicating the presence of a stronger detection signal in acutely formed intracardiac thrombi compared with thrombi induced in arteries. Other groups even developed prourokinase-Annexin V chimeras as potential thrombolytic agents based on the ability of Annexin V to bind activated platelets in thrombi with high affinity [111].

Thorough optimisation of the radiolabelling procedure for 123I-Annexin V was described by Lahorte et al. for both the IodoGen and the IodoBead method [112, 113]. Using recombinant human Annexin V, optimisation of all reaction parameters resulted in radiochemical yields of 75–85%, respectively, while preserving sufficient biological activity towards blood platelets and apoptotic lymphocytes. In addition, excellent radiochemical purities of >98% were obtained for both methods. Most interestingly, further improvement of the IodoGen method allowed routine production of clinical-grade 123I-Annexin V, achieving radiochemical yields of 87% and specific activities of 13.4 GBq/µmol [114]. Preliminary

studies in a rat model of sepsis-induced myocardial dysfunction clearly indicated significantly increased radioligand uptake in the myocardium compared with control animals [115]. Furthermore, myocardial tracer uptake could be decreased by about 80% by means of broadspectrum and selective caspase-3 inhibitors, thereby providing evidence for the specificity of the tracer signal [116, 117]. Most recently, the biodistribution and dosimetry of 123I-rh-Annexin V was evaluated in humans and compared with previously obtained data in mice applying the MIRD program [114]. 123I-rh-Annexin V was characterised by a fast bi-exponential clearance from the blood compartment (i.e.  $T_{1/2,\alpha} = 3.87 \pm 0.90$  min and  $T_{1/2, \beta} = 4.13 \pm 2.04$  h) and predominant uptake in the kidneys, liver and gastrointestinal tract followed by pronounced renal excretion. However, delayed whole-body images indicated progressive deiodination of the radioligand, which could impede in vivo detection of apoptosis in the abdominal region. From the dosimetry point of view, intravenous injection of 345 MBq 123I-rh-Annexin V resulted in moderate radiation doses for most organs, whereas the estimated effective dose received by the volunteers in this study represented 0.02 mSv/MBq administered. Thus, the effective dose received by the volunteers in this study (i.e. on average 6.9 mSv) is somewhat higher than the 5 mSv upper limit average effective dose of category IIa of the World Health Organisation and category IIb of the ICRP report [118, 119]. The results of this study also demonstrated that 123I-rh-Annexin V was well tolerated in humans  $(n=6)$  without provoking any adverse effects or complications despite the relatively high amount of radiolabelled protein delivered as bolus injection (i.e. 940±64 µg/volunteer). In addition, for most organs, the estimated absorbed radiation dose as well as the estimated effective dose for humans corresponded well with the extrapolated radiation dose estimates originating from the animal biodistribution studies.

Alternatively, Annexin V has been iodinated indirectly by applying the commonly known Bolton-Hunter method and compared with directly iodinated Annexin V prepared by the IodoBead method [120]. Iodination of the water-soluble Bolton-Hunter reagent with CAT and subsequent conjugation to Annexin V for 1 h at pH 9.2 resulted in relatively poor radiochemical yields of 40%. In vitro assays with irradiated neuroblastoma cells and immobilised PS residues indicated 50–75% preservation of the radioligand's PS-binding capacity. However, Bolton-Hunter-labelled 125I-Annexin V showed clearly improved in vivo stability compared with directly 125Ilabelled Annexin V at 2 h p.i. Furthermore, C3H mice treated with anti-Fas monoclonal antibody (MoAb) or irradiation showed significantly increased activity accumulation in the apoptotic organs. However, the Bolton-Hunter radioligand showed extensive accumulation in the liver and bowels owing to increased lipophilicity, which could seriously hamper in vivo apoptosis detec-

tion in these regions. So, although the Bolton-Hunter approach seems to offer improved in vivo stability over directly iodinated Annexin V, the method remains laborious and time-consuming while providing low radiochemical yields. Furthermore, the inherent biological behaviour of Bolton-Hunter-labelled Annexin V could restrict its applicability for apoptosis imaging in the abdominal region.

*[124I]Iodoannexin V, [124I]m-IBA-Annexin V, 124I-MBP-Annexin V and 124IB-MBP-Annexin V.* Additionally to the gamma-emitting radionuclides 123I and 125I, Annexin V has also been radiolabelled with the positron emitter <sup>124</sup>I (physical half-life of <sup>124</sup>I=4.18 days,  $E_{\text{max}}\beta^{+}=1.53$ , 2.14 MeV), by either direct or indirect iodination. In a first study, Glaser et al. reported on the 124I labelling of wild-type and polyhistidine-tagged recombinant Annexin V using two different methods [121, 122]. The modified Annexin V protein contained a tag with a tobacco etch virus (TEV) protease cleavage site linked to a hexahistidine residue. Both proteins were iodinated directly by using a variant of the well-established chloramine-T (CAT) method and optimised for reaction time and pH. When using a 10-min reaction time at pH 6.5, instant thin-layer chromatography (ITLC) analysis of the reaction mixtures indicated that nearly 80% of the radioactivity was incorporated with both unmodified and polyhistidine-tagged Annexin V, resulting in a 97.7% $\pm$ 1.0% radiochemical purity (RCP) and a specific activity of 14.5 GBq/µmol post purification. In spite of this relatively high radiochemical yield and specific activity, a poor overall yield of ca. 22.3%±2.6% was obtained for 124I-Annexin V after purification by means of gel filtration on a Sephadex column. Regardless of the higher RCP (>99%) obtained by fast protein liquid chromatography (FPLC) purification, the loss of radioligand was even more pronounced in such cases, indicating significant adsorption of the iodinated protein to the packing material of the TSK G3000 SWxl size exclusion column. In addition, direct iodination of Annexin V by means of CAT instead of IodoGen initially resulted in even lower radiochemical yields of near 4–6% [121].

Since Annexin V contains 21 lysine residues, the indirect iodination approach with N-acylation of amino residues was also investigated. For this purpose, Glaser et al. applied the pre-labelled reagent *N*-succinimidyl  $3-[124]]$ iodobenzoate ( $[124]$ ]m-SIB), generated from the stannyl precursor *N*-succinimidyl 3-(trimethylstannyl) benzoate (m-MeATE) in order to produce [124I]m-IBA-Annexin V with a high RCP of  $96.7\% \pm 2.1\%$  by means of a three-step procedure. The [124I]iododestannylation step was performed using IodoGen as solid phase oxidant whereas the final reaction step consisted of  $[124]$ ]m-SIB conjugation to the protein at pH 8.5. Similar to the direct labelling approach, [124I]m-IBA-Annexin V was obtained in poor overall radiochemical yields after purification by FPLC and gel filtration (i.e. 14% and

25%, respectively), which was, in part, attributed by Glaser et al. to the formation of unidentified radioactive side-products which are retained on the purification column. Efforts to increase the recovery of radiolabelled protein by using PBS primed with BSA during gel filtration provided only very limited success (i.e. 34% radiochemical yield). However, subsequent to the modified purification conditions the RCP dropped back to merely 76%, mainly due to poor column performance.

Furthermore, the specific activity of  $[124]$ m-IBA-Annexin (i.e. 1.6 GBq/µmol) was ninefold lower than that of directly 124I-labelled Annexin V and seems inherently linked to the use of multiple reaction steps involved in the indirect labelling approach. In particular, the pre-labelled active ester [124I]m-SIB is produced in a low and variable radiochemical yield (i.e. 39.3%±8.4% after HPLC purification) and can be considered as a major contributor to the low specific activity of the final [124I]m-IBA-Annexin V product. Nevertheless, [124I]iodoannexin V and [124I]m-IBA-Annexin V showed comparable in vitro stability (i.e. both compounds were stable up to 4 days when stored in PBS at 4°C, after which deiodination started to proceed). However, [124I]m-IBA-Annexin V should be expected to show superior stability over directly labelled Annexin V when uploaded with higher activities. The biological activity of both molecules was subjected to preliminary testing in an in vitro model of camptothecin-induced apoptosis in HL60 cells by using the <sup>125</sup>I counterparts of directly and indirectly iodinated Annexin V. Human leukaemic HL60 cells pre-treated for 6 h with campothecin showed increases in tracer uptake of 17% and 21% for [125I]iodoannexin V and [125I]m-IBA-Annexin V, respectively, compared with control cells. However, statistical significance for the 17% increased [125I]iodoannexin V binding was found in only one out of three experiments. Nevertheless, binding of [125I]m-IBA-Annexin V to control and pre-treated cells could be blocked by 60% and 68%, respectively, by pre-incubation with a 100-fold excess of unlabelled Annexin V. Based on these first in vitro results, one can conclude that these two radioligands seem to exhibit a rather comparable biopotency. However, when interpreting these data, it needs to be underscored that the minor difference in apoptosis observed between control and campothecin-treated cells (as reflected by the tracer binding) either indicates an inferior biopotency of the tracer or demonstrates that the DMSO solvent used for dissolving campothecin is capable of inducing apoptosis in the control cells to almost the same extent as in the campothecin-treated cells. Since [125I]m-IBA-Annexin V binding to control and pre-treated cells could be blocked to a similar extent (i.e. by 60% and 68%, respectively) by pre-incubation with a 100-fold excess of unlabelled Annexin V, the second hypothesis seems to be most likely. In this case the choice of in vitro model was less appropriate or the model would require further improvements and validation by alternative techniques to assess the amount of induced apoptosis accurately. This assumption was confirmed by a second in vitro model in which heat-induced PS exposure on HL60 cells resulted in a significant increase (i.e. by 56%) in [124I]m-IBA-Annexin V binding compared with control cells, thereby proving the biopotency of the radioligand [121].

From a clinical point of view, the long physical halflife of 124I offers broad possibilities for the (in)direct iodination of Annexin V and would allow monitoring and quantification of long-term biological processes. In contrast, in vivo administration of long-living 124I-labelled Annexin V to humans could contribute to high radiation doses to specific organs such liver, which is generally known to metabolise radiolabelled proteins, and subsequent accumulation of free iodine-124 in the thyroid and stomach due to deiodination of the protein. In this regard, 124I-labelled Annexin V ligands should display good in vivo stability and sufficient clearance from the body over time in order to minimise radiation burden to the patient, especially when considering the complex decay scheme of 124I, which produces several high-energy gamma emissions (0.60–1.69 MeV). Another disadvantage of the isotope that needs to be addressed is the low ratio of disintegrations, which results in 23% positrons, thereby requiring higher tracer doses to the patient or longer acquisition times in order to obtain highquality PET scans.

Most recently, a third type of 124I-Annexin V ligand was developed by Keen and Dekker et al., consisting of a maltose binding protein-Annexin V chimera (MBP-Anx 5) [123]. The molecule was radiolabelled by direct iodination applying the IodoGen method and evaluated in a mouse model of anti-Fas MoAb-induced hepatic apoptosis together with unmodified Annexin V, while iodinated MBP and albumin were used as corresponding control proteins. BDF1 mice pre-treated with anti-Fas MoAb 4 h prior to the tracer injection showed significantly increased hepatic apoptosis compared with control animals as determined morphologically. Furthermore, a correlation was found between the apoptotic index and the elevated liver uptake of both 124I-Annexin V and 124I-MBP-Anx 5 but not with that of the control proteins. Moreover, camptothecin-treated Jurkat cells had previously been demonstrated to exhibit an eightfold increase in 124I-MBP-Anx 5 binding compared with non-treated cells [124]. In spite of these promising results, the biodistribution of directly labelled 124I-MBP-Anx 5 in both normal and anti-Fas-MoAb-treated mice was characterised by rapid and extensive dehalogenation, as reflected by activity accumulation in the thyroid [123, 124]. This major drawback prompted Dekker et al. to iodinate MBP-Anx 5 indirectly by using [124I]-4-iodobenzylsuccinimide as a precursor molecule, which resulted in 124IB-MBP-Anx 5, applying the IodoGen method [125]. Comparative biodistribution experiments in normal mice at 2 h post tracer injection demonstrated significantly increased liver- and kidney-to-blood uptake ratios of 124IB-MBP-Anx 5 versus 124I-MBP-Anx 5. In contrast, urinary excretion was substantially lower in the case of 124IB-MBP-Anx 5, reflecting inferior renal excretion which could contribute to elevated residual background activity in the body. These preliminary data indicate that poor image contrast can be expected in the gastrointestinal region within the first few hours of tracer administration, which would seriously hamper clinical use. Furthermore, it remains unclear whether indirectly iodinated MBP-Anx 5 possesses better stability to in vivo dehalogenation compared with 124I-MBP-Anx 5 since the thyroid of all investigated animal groups was blocked prior to tracer injection [125].

In conclusion, preliminary in vitro and vivo results have provided the first evidence on the potential applicability of 124I-labelled Annexin V as a PET probe for imaging of apoptosis. Nevertheless, many of the problems mentioned above will need to be overcome before 124Ilabelled Annexin V, prepared by either direct or indirect iodination, could find its way into the clinic.

*4-[18F]fluorobenzoylannexin V.* Similar to the indirect radiolabelling method for [124I]m-IBA-Annexin V, a four-step synthesis has been described by three different research groups for production of 4-[18F]fluorobenzoylannexin V (4-[18F]FBA) by means of the *N*-succinimidyl-4-[18F]fluorobenzoate ([18F]SFB) precursor. The majority of the radiolabelling approaches have been based on the method of Wester et al. making use of ethyl-4-[18F]fluorobenzoate, 4-[18F]fluorobenzoic acid and [18F]SFB as intermediates [126, 127]. Although the same intermediate reaction products were generated in all methods mentioned below, different reagents, reaction conditions and purification methods were used in some of the synthesis steps, resulting in different overall radiochemical yields. The most technically advanced method was described by Zijlstra et al. making use of a microcomputer-controlled, automated module producing 4-[18F]FBA within 90 min in radiochemical yields of 15–20% (i.e. decay corrected) and with an RCP of at least 95%. Additionally, specific activities of more than 35 GBq/µmol were achieved, which is significantly higher than the value reported for <sup>124</sup>I-labelled Annexin V [128]. Despite the low overall yield, 4-[18F]FBA could be prepared by the automated system in batches of up to 2 GBq when starting from 25 GBq [18F]fluoride [129]. In contrast, the group of Mease et al. obtained significantly higher radiochemical yields ranging from 38% to 68%, in correspondence with an increased Annexin V concentration (i.e.  $1.25-5 \mu g/\mu l$ ) used for conjugation to [18F]SFB [130]. One of the major contributors to this difference is the 52–55% yield in which [18F]SFB could be produced compared with the 35% yield obtained by Zijlstra et al. Further optimisation of the [18F]SFB precursor synthesis resulted in radiochemical yields of up to 77% [131]. On the other hand, the third method present-

ed by Murakami et al. for production of 4-[18F]FBA requires 2 h of synthesis while generating the lowest radiochemical yields, in the range of 10%, with 99% RCP [132].

In vitro biological activity of 4-[18F]FBA was initially verified by Zijlstra et al. towards PS-containing liposomes and UV-irradiated Jurkat T-cell lymphoblasts. 4-[18F]FBA showed rapid and highly specific binding to liposomes containing 80–85% of PS residues whereas the Jurkat T-cell study revealed at least 60% increased tracer binding over time to apoptotic T cells versus nonapoptotic T cells. Furthermore, radioligand binding appeared to be time- and concentration-dependent and could be saturated. Mease and Grierson et al. demonstrated retention of the tracer's biological activity in a red blood cell assay in which 4-[18F]FBA binding to externalised PS residues was confirmed. In fact, 4-[18F]FBA exhibited a nanomolar affinity for red blood cells  $(K_d \approx 10.8 \pm 5.0 \text{ nM})$  [131]. At present, Murakami et al. were the first to evaluate 18F-labelled Annexin V in vivo in a rat model of myocardial ischaemia-reperfusion. Twenty-four hours after inducing ischaemia, a fourfold increase in tracer uptake in the infarcted area was seen compared with normal myocardial tissue. Specificity of the apoptotic signal was confirmed by the co-localisation of TUNEL-positive cells in the area of tracer accumulation. Most recently, preliminary biodistribution studies in normal Sprague-Dawley rats indicated that 4-[18F]FBA is rapidly cleared from liver, kidneys and heart within 1 h p.i., and provides high urinary excretion [131]. Moreover, 4-[18F]FBA PET images at 45 min p.i. did not show any thyroid uptake, which might reflect ongoing dehalogenation.

Based on the available data, 4-[18F]FBA seems to offer promise as a potential tool for PET imaging of PCD. PET studies with positron-emitting Annexin V radioligands not only could enhance the sensitivity and spatial resolution but would also allow better localisation and quantification of apoptotic areas compared with SPECT studies. Furthermore, 18F (physical half-life of <sup>18</sup>F=1.83 h,  $E_{\text{max}}\beta$ <sup>+</sup>=0.635 MeV) possesses a much shorter half-life and lower energetic positron emission compared with 124I, which is likely to contribute to a lower radiation burden to the patient considering the apparent superior biological clearance of 4-[18F]FBA.

### 99mTc-Annexin V

Beyond any doubt, 99mTc-Annexin V as a marker of PS expression is by far the most extensively investigated and broadly used apoptosis-detecting radioligand to date. Over recent years, numerous 99mTc-Annexin V radioligands have been developed by different groups using different types of chelators and co-ligands, each resulting in a different biological behaviour. The popularity and high interest in this group of Annexin-based radioligands



**Fig. 2.** Chemical structure of  $99 \text{mTc-N}_2$ S<sub>2</sub>-Annexin V ( $99 \text{mTc}$ -BTAP-Anx V)

is in part due to the substantial advantages of 99mTc compared with many other radionuclides. The <sup>99m</sup>Tc isotope is characterised by optimal radionuclidic properties for SPECT imaging (physical half-life of  $99mTc=6.01$  h,  $E_{\text{max}}$  $\simeq$  0.141 MeV), is inexpensive and is easily available. A thorough overview and discussion of the currently existing direct and indirect 99mTc-labelling methods for Annexin V and its derivatives is presented hereafter.

*99mTc-BTAP-Annexin V.* About 4 years after the development of radioiodinated Annexin V, 99mTc-4,5-bis- (thioacetamido)pentanoyl-Annexin V (99mTc-BTAP-Anx V) became the first  $99mTc$ -Annexin V radioligand to be described (Fig. 2).  $99mTc$  labelling of Annexin V was performed according to the pre-formed chelate approach in which a diamide dimercaptide  $N_2S_2$  chelate was used, based on the OncoTrac labelling method originally described by Kasina et al. [133, 134]. For this purpose, 99mTc was first converted in the presence of stannous gluconate to 99mTc-gluconate and reacted with the acidified phenthioate ligand under heating to form a stable  $^{99m}$ Tc-N<sub>2</sub>S<sub>2</sub> complex. In a final step, the  $^{99m}$ Tc-N<sub>2</sub>S<sub>2</sub>-TFP ester was conjugated to the protein at basic pH, after which the radioligand was purified by gel filtration, resulting in 25–30% overall radiochemical yields and a specific activity of 58.3 GBq/µmol. Subsequently, the production of  $99mTc-N<sub>2</sub>S<sub>2</sub>$ -Annexin V was further optimised in a kit formulation (Apomate, Theseus Imaging Corporation, Boston, USA) and evaluated in vivo in Yorkshire swine [101] and patients with acute cardiac transplant rejection [135, 136].

Initial studies in a swine model of trial thrombi indicated the potential use of 99mTc-BTAP-Anx V as a selective thrombus targeting agent generating thrombus/blood uptake ratios of 14.2, comparable to 125I-Annexin V [101]. More importantly, however, <sup>99m</sup>Tc-BTAP-Anx V provided the first evidence that in vivo detection of PS expression by means of SPECT was feasible. Early planar and tomographic images acquired within 140 min p.i. showed increasing tracer uptake over time in intracardiac thrombi, resulting in three- to fourfold higher uptake compared with control animals. Phase I clinical studies

investigating the biodistribution and dosimetry of 99mTc-BTAP-Anx V in a variety of patients clearly indicated predominant accumulation of radioactivity in the kidneys, liver and urine bladder over time [137]. However, the radioligand showed fast and extensive bowel excretion, precluding its clinical use for imaging apoptosis in the abdominal region. The high accumulation of radioactivity in the gastrointestinal tract as reported for  $123$ I-rh-Annexin V was even more pronounced for  $99$ <sup>m</sup>Tc-BTAP-Anx V. Nevertheless,  $99mTc-N<sub>2</sub>S<sub>2</sub>$ -Annexin V has proven most useful for in vivo detection of apoptotic and necrotic cell death in patients with acute cardiac transplant rejection [135, 136] and intracardiac tumours [70]. Furthermore, the radioligand has been used successfully to assess chemotherapy- and radiotherapy-induced apoptosis in patients with lung and breast cancer [35, 138] or lymphomas [139].

From the radiopharmaceutical point of view, the 99mTc-BTAP-Anx V kit formulation containing 11 kit components remains very elaborate and time-consuming since it requires multiple reaction steps at different temperature and pH conditions and a rather complex purification procedure. Furthermore, the preparation requires high (i.e. 4.4–5.5 GBq) start activities of <sup>99m</sup>Tc, thereby increasing the radiation exposure to the operator, while providing low radiochemical yields. For this multitude of reasons, an improved 99mTc-Annexin V ligand was required to address the major drawbacks of 99mTc-BTAP-Anx V.

*99mTc-Hynic-Annexin V.* In search of an alternative radiolabelling approach for Annexin V, the group of Blankenberg et al. applied the Hynic technology in 1998, which was originally developed by Abrams et al. [140]. The hydrazino-nicotinamide (Hynic) ligand, as a nicotinic acid analogue, is a bifunctional chelator capable of binding to the  $NH<sub>2</sub>$ -terminal amino acid and lysine residues of proteins on the one hand and of sequestering 99mTc on the other. Using tricine as co-ligand, the Hynic-Annexin V conjugate proved a most stable complex and allowed fast and efficient labelling with 99mTc in the presence of stannous ions (Fig. 3A). Consequently, the one-step reaction provides 99mTc-Hynic-Annexin in high radiochemical yields of typically 92–95% without requiring any additional purification step. Most interestingly, using the Hynic methodology, the Annexin V protein can be "uploaded" with 99mTc to very high specific activities of 198–265 GBq/µmol, making it most useful for in vivo imaging applications [141]. The radiolabelling procedure was further improved into a kit formulation of two vials requiring only 15 min of reaction (99mTc-Hynic-Annexin V, Theseus Imaging Corporation, Boston, USA). In comparison with  $99mTc-N<sub>2</sub>S<sub>2</sub>$ -Annexin V, the 99mTc-Hynic-Annexin V formulation offers a much simpler and faster preparation at room temperature, while providing significantly higher radiochemical yields. Consequently, the radiolabelling method requires



Fig. 3A, B. Chemical structures of <sup>99m</sup>Tc-Hynic-derivatised Annexin V using either tricine or EDDA as co-ligand: **A** 99mTc-Hynic(tricine)<sub>2</sub>-Annexin V, **B** <sup>99m</sup>Tc-Hynic-EDDA-Annexin V (99mTc-EDDA-Hynexin)

substantially lower start activities (e.g. 1.11–1.48 GBq), thereby improving radiosafety to the operator. All these advantages make 99mTc-Hynic-Annexin V much more suitable for routine production and fast application in a clinical setting. The coming of age of this second-generation kit represented a prelude to the impressive armamentarium of Annexin V-based radioligands that has been continuously expanding since then.

Undoubtedly, the development of 99mTc-Hynic-Annexin V can be considered as a benchmark in the field of apoptosis imaging since this tracer is by far the most extensively investigated and best characterised apoptosisdetecting radioligand thus far (Table 2). Numerous in vivo studies in animals have been published, demonstrating the broad applicability of  $99mTc$ -Hynic-Annexin V as a SPECT radioligand for imaging apoptotic cell death. Initially the radioligand was successfully used in animal models of Anti-Fas MoAb-induced hepatic apoptosis, allograft rejection of the heart liver and lungs, myocardial ischaemia-reperfusion injury, anthracycline-induced cardiomyopathy, rheumatoid arthritis, sterile inflammation, hypoxic brain injury and cyclophosphamide-induced intramedullary apoptosis [67, 142].<sup>1</sup> Moreover, Narula et al. provided first evidence that internalisation of 99mTc-labelled Annexin V in ischaemic myocardial tissue exceeds 50%, probably due to translocation of PS residues back to the inner sarcolemmal leaflet upon reperfusion [143]. Most interestingly, 99mTc-Hynic-Annexin V is increasingly being applied to monitor and evaluate the therapeutic effect of cardioprotective and immunosuppressive agents based on their ability to protect specific cells against apoptotic cell death [144, 145]. Conversely, the apoptosis marker has shown great potential for in vivo monitoring and prediction of anti-cancer treatment response.

<sup>&</sup>lt;sup>1</sup> A detailed list of preclinical studies is available from the author.

#### **Table 2.** List of clinical trials (phase I/III)



(A)MI, (Acute) myocardial infarction; IP, ischaemic preconditioning; MRI, magnetic resonance imaging; NSCLC, non-small cell lung cancer

At the beginning of 2002, 99mTc-Hynic-Annexin V entered phase I clinical trials to determine the safety, biodistribution and dosimetry of the molecule prior to clinical use in nuclear medicine [146]. Similar to the penthioate radioligand, 99mTc-Hynic-Annexin V showed strongest uptake in the kidneys, liver and urine bladder on early patient images. However, activity uptake in liver and kidneys was significantly higher (i.e. by a factor of 2–2.5 and 6–13, respectively) for both  $99mTc$ -Annexin V ligands compared with 123I-Annexin V. Like the iodinated protein, 99mTc-Hynic-Annexin V generally showed predominantly urinary excretion. Nevertheless, the total % injected dose found excreted in urine remained substantially lower than that observed with  $99mTc-BTAP-Anx$  V (i.e.  $22.5\% \pm 3.5\%$  ID vs  $65\% \pm 11\%$ ID at 20–24 h p.i.). Furthermore, the biodistribution of 99mTc-Hynic-Annexin was devoid of any bowel excretion, resulting in excellent imaging conditions in the abdominal region. Regardless of the applied radiolabelling method, both the 99mTc-Annexin V radioligands and 123I-rh-Annexin V generally exhibit a rapid, bi-exponential clearance from the blood circulation, although some differences do exist between the agents. Respectively 92%, 87% and 74% of the <sup>99m</sup>Tc-Hynic-, <sup>99m</sup>Tc-N<sub>2</sub>S<sub>2</sub>and 123I-Annexin V activity is cleared from the blood in a fast phase with a  $T_{1/2,\alpha}$ =24, 26 and 4 min whereas the remaining blood pool activity is slowly excreted with a  $T_{1/2,8}=35, 6.9$  and 4.1 h). From a dosimetry point of view, for 99mTc-Annexin V radioligands, the organs receiving the highest absorbed dose are kidneys, spleen and liver. However, in the case of 123I-rh-Annexin V, the absorbed dose to the kidneys and spleen was much lower whereas the absorbed dose to liver was comparable. Red bone marrow and urine bladder also received similar absorbed doses. In contrast, the high thyroid uptake observed for 123I-rh-Annexin V resulted in an 11- to 14-fold increase in the absorbed dose in comparison with 99mTc-labelled Annexin V. Furthermore, administration of 123I-rh-Annexin V to human subjects resulted in an effective dose about twofold higher than that reported for the  $99mTc$ -Annexin V radioligands.

Soon afterwards, phase I human studies were initiated with the most prominent clinical applications comprising in vivo detection of myocardial infarction [147–149], intracardiac tumours and infectious endocarditis [150] and spontaneous as well as chemotherapy- or radiotherapy-induced apoptosis in a variety of solid and haematological tumours [138, 139, 151, 152]. In this regard, systematic radionuclide detection of apoptosis during the course of tumour therapy would not only enable physicians to monitor the efficacy of treatment over time and patient outcome, but would also allow early prediction of therapy response, thereby avoiding unnecessary and time-consuming treatment courses. At present, <sup>99m</sup>Tc-Hynic-Annexin V is the only apoptosis-detecting radioligand that is currently being investigated in phase II/III trials in patients with non-small-cell lung cancer [138] and is likely to reach the stage of commercialisation for routine use in nuclear medicine.

*99mTc-i-Annexin V.* In the follow-up of 99mTc-BTAP-Anx V, a third type of 99mTc-Annexin V was developed and evaluated soon afterwards in human subjects [153]. Annexin V was derivatised with a monodentate *n*-1-imino-4-mercaptobutyryl side chain and subsequently labelled with 99mTc based on the earlier reported method of Goedemans and Panck [154]. The iminothiolane approach consists of converting amino groups within the protein into free thiol groups which can readily bind to 99mTc in the presence of stannous ions. Although this labelling method allowed fast and easy preparation of 99mTc-(*n*-1-imino-4-mercapto-butyl)-Annexin V (99mTci-Anx V, Mallinckrodt, Petten, The Netherlands), only low radiochemical purities of 79–82% could be obtained, making it less suitable for common use in clinical settings.

Biodistribution studies in human subjects injected with this iminothiolane preparation gave results for the most vital organs that were similar to those obtained with <sup>99m</sup>Tc-BTAP-Anx V. However, with the exception of the urinary bladder and large intestine wall, the absorbed radiation doses for most organs were higher in the case of 99mTc-i-Anx V owing to its substantial longer effective biological half-life in the total body (i.e. 62 $\pm$ 13 h vs 16 $\pm$ 7 h for <sup>99m</sup>Tc-BTAP-Anx V). Thus, 99mTc-i-Anx V seemed to be subject to slower clearance from most organs, resulting in two- to threefold higher radiation doses to the urinary bladder and large intestine wall. These findings were clearly reflected by slower clearance from the blood and less pronounced radioactivity accumulation in the bowels, as previously observed with <sup>99m</sup>Tc-BTAP-Anx V. Nevertheless, the radiopharmaceutical was applied successfully in patients with AMI who were receiving reperfusion therapy. Following 2 h of reperfusion, the infarcted area of the heart could be clearly detected on late SPECT images 17–22 h after tracer injection [69]. In contrast, increased radioligand uptake was seen neither in the heart outside the infarcted area nor in the heart of a control patient. Perfusion scintigraphy with sestamibi 6–8 weeks later demonstrated co-localisation of an irreversible perfusion defect with the area of increased 99mTc-i-Anx V uptake. However, on early SPECT images (i.e. 3–4 h p.i.), visualisation of myocardial tracer uptake was significantly hampered by the high blood pool activity. These findings indicate that reperfusion is associated with irreversible cell death in infarcted cardiac tissue and confirm previous studies which demonstrated the involvement of both apoptotic and oncotic cell death in myocardial ischaemia and reperfusion [63, 155].

 $^{99m}Tc-MAG_{3}$ -*Annexin V.* In an effort to decrease the high kidney and liver accumulation observed for most 99mTc-labelled Annexin V compounds, in particular 99mTc-Hynic-Annexin V, the protein was recently conjugated to mercaptoacetyl-glycyl-glycine  $(MAG_3)$  [156]. In fact, the  $MAG_3$  chelator has been applied in the  $99mTc$ 

chemistry of proteins and peptides many fold, often resulting in good renal clearance. Similar to the Hynic post-labelling methodology, NHS-MA $G<sub>3</sub>$  can be attached to Annexin V at room temperature in a single step. Radiolabelling of the purified  $N_3S$  chelate resulted in radiochemical yields of 90% under basic pH conditions, eliminating the need for further purification on a column. Preliminary biodistribution data in mice clearly showed significant decreases (by 62.8% and 52.6%, respectively) in the kidney and liver uptake of  $99mTc-MAG_3-Annexin$ V at 1 h p.i. compared with <sup>99m</sup>Tc-Hynic-Annexin V. Ongoing biodistribution studies in mice indicate an even more pronounced decrease in liver uptake of 84.6% (no results shown). Furthermore, the  $99mTc-MAG_3-Annexin$ V biodistribution was characterised by lower retention of radioactivity in the whole body whereas blood and intestinal uptake was threefold higher than that observed with 99mTc-Hynic-Annexin V. However, ongoing studies have revealed a sixfold higher tracer uptake in the small intestines for the  $MAG_3$  derivative at 1 h p.i., with blood pool activity being almost 1.4-fold lower than that of 99mTc-Hynic-Annexin V. These findings seem to confirm the expected improvement in renal and hepatic clearance of the  $MAG<sub>3</sub>$  radioligand, which could at least contribute to better imaging conditions for the study of apoptosis in kidney diseases. However, early in vivo detection of ongoing apoptosis in the liver might be hampered by the significantly increased activity uptake in the small intestines despite the improved hepatic clearance of  $99mTc-MAG_3$ -Annexin V.

*94mTc-Hynic-Annexin V.* Very recently a technetiumbased PET alternative to <sup>99m</sup>Tc-Hynic-Annexin V was studied by McQuade et al., applying <sup>94m</sup>Tc as the radionuclide [157]. Given the unique radionuclidic properties of this isotope (physical half-life of  $94mTc=53$  min,  $E_{\text{max}}\beta t = 2.5$  MeV), <sup>94m</sup>Tc-Hynic-Annexin V could be considered a valuable marker for in vivo detection of apoptosis by means of PET. Since 94mTc and 99mTc share identical physicochemical properties, 94mTc-Hynic-Annexin V can be produced using the same methodology as its SPECT counterpart, resulting in comparable radiochemical yields and purities >90%. Considering the superior resolution of PET over SPECT, positron-emitting apoptosis-detecting ligands seem very attractive, especially in cases where the ongoing apoptotic process is localised in small tissue areas (e.g. tumour nodules or focal ischaemic tissue zones) or in the presence of a weak apoptotic signal (e.g. subacute myocarditis). At present, 94mTc-Hynic-Annexin V is being evaluated in a mice model of anti-Fas MoAb-induced hepatic apoptosis [157].

*99mTc-EDDA-Hynexin.* In addition to tricine, several alternative co-ligands such as *N*,*N*-ethylenediamine diacetic acid (EDDA), tricine/nicotinic acid or isonicotinic acid can be considered for the 99mTc-labelling of HynicAnnexin V. The choice of co-ligand not only determines the number of possible isomers but also affects the lipophilic properties, in vivo stability and subsequent biological behaviour of the corresponding Hynic-technetium complexes [158].

In a study published by Verbeke et al., EDDA was used as co-ligand for labelling Hynic-derivatised Annexin V (Fig. 3B) [159]. Conjugation of the Hynic chelator to Annexin V and radiolabelling of the conjugate were performed similarly to the standard methods as described above. However, in contrast to the tricine-based preparations performed at room temperature, reaction mixtures for 99mTc labelling of EDDA-Hynexin required incubation at 37°C. Despite the heating process, poor radiochemical yields were obtained for 99mTc-EDDA-Hynexin (i.e. 28% and 35% after 20 and 60 min incubation time, respectively), whereas 99mTc-Hynic-Annexin V is consistently produced in radiochemical yields >90%. As a result, 99mTc-EDDA-Hynexin preparations require an extra purification step (e.g. by means of size-exclusion FPLC) in order to achieve adequate radiochemical purity prior to administration in animals. Biodistribution studies with 99mTc-EDDA-Hynexin in mice demonstrated a fairly rapid blood clearance and predominant uptake in kidneys and liver, as previously observed with 99mTc-Hynic-Annexin V. However, radioactivity accumulation in kidneys was significantly higher for 99mTc-EDDA-Hynexin, while liver uptake was much lower compared with that of 99mTc-Hynic-Annexin V. Furthermore, the two radioligands exhibited comparable, low urinary excretion 60 min after administration [160]. These findings could be explained by the lower lipophilicity of the EDDA co-ligand in comparison with tricine since decreased lipophilicity of co-ligands results in decreasingly lipophilic 99mTc-Hynic complexes which are generally known to provide lower abdominal excretion and organ uptake, particularly in the liver, followed by a higher renal excretion [158]. Nevertheless, the EDDA co-ligand does not appear to be a suitable alternative to tricine in the routine production of 99mTc-Hynic-Annexin V, considering the very low radiochemical yields.

*99mTc-EC-Annexin V.* An alternative method for preparing 99mTc-rh-Annexin V was described by Yang and Kim et al. making use of ethylenedicysteine (EC) as a bifunctional chelating agent. 99mTc-EC-Annexin V was produced by conjugation of EC to the protein, applying sulpho-*N*-hydroxysuccinimide (sulpho-NHS) and 1-ethyl-3-[3-(dimethylamino)propyl]-carbodiimide-HCl (EDC) as coupling agents [161, 162]. In a second step, the ethylene cysteine construct was radiolabelled with  $99mTc$  and SnCl<sub>2</sub> followed by purification through gel permeation, which resulted in overall radiochemical yields of 65–70% and purities near 100%. Furthermore, 99mTc-EC-Annexin V could be obtained in high specific activities of 185 GBq/µmol. In fact, radiopharmaceutical preparation of 99mTc-EC-Annexin V was based on the

 $N_2S_2$  bifunctional chelate approach, similar to preparation of the renal imaging agent 99mTc-EC, which is characterised by easy and efficient radiolabelling providing high radiochemical purity and stability. Although <sup>99m</sup>Tc-EC-Annexin V does not require any co-ligand for stabilising the radioligand, an additional purification step is necessary to obtain a sufficient radiochemical purity above 95%.

When evaluated in different animal models of spontaneous tumour apoptosis, highly apoptotic ovarian and breast tumour-bearing rodents showed moderate to high tumour radioligand uptake peaking within 15 min to 2 h post radioligand injection, after which the signal already started to decrease. These results seem to reflect an undesirable rapid tumour clearance of the tracer; this could be detrimental for clinical use of the tracer in nuclear medicine, which requires apoptosis imaging over longer periods (i.e. 6–24 h p.i.). Additionally, the specificity of the radioactivity uptake in the investigated tumours was unclear since 99mTc-L,L-ethylenedicysteine (99mTc-EC) was used as the control radioligand in these studies. Nevertheless, 99mTc-EC-metronidazole scintigraphic images in the same breast tumour-bearing rodents suggested a co-localisation of the area of tumour hypoxia with ongoing apoptosis, indicating the presence of hypoxiainduced apoptosis. In contrast, virtually no 99mTc-EC-Annexin V uptake could be documented in low apoptotic sarcomas within the same time frame.

Additional planar imaging studies were performed with implanted rat breast cancer tumours, which were treated with either paclitaxel or irradiation [162, 163]. Significantly increased tracer uptake was only observed in tumours 3 days after paclitaxel treatment; by contrast, tumour uptake was slightly lower at 5 days post therapy when compared with pre-therapy planar rat images. Furthermore, the overall tumour uptake of <sup>99m</sup>Tc-EC-Annexin V in paclitaxel-treated rats (i.e. 0.2–0.5% ID/g) within 0.5–4 h after tracer injection was rather low, resulting in poor tumour-to-blood ratios of 0.4–0.8. Considering the generally rapid clearance of apoptotic cells in vivo, early detection of chemo- or radiotherapyinduced apoptosis within 24 h post treatment would seem more likely to result in higher tumour-to-background ratios when the apoptotic tumour cells have not yet been extensively removed by macrophages and neighbouring cells. Indeed, several in vitro and in vivo studies have clearly demonstrated that a substantial rise in tumour cell apoptosis can occur within or around 24 h following chemotherapy or radiotherapy treatment [87, 164–166]. Again, these findings seem to confirm the necessity of determining the timing of PS exposure when studying chemotherapy- or radiotherapy-induced apoptosis in vivo.

*Directly labelled 99mTc-Annexin V.* In pursuit of a fast and simple method for 99mTc labelling of Annexin V, Zhu et al. recently described a direct labelling approach

in which the free thiol group of the protein was reduced in the presence of  $Sn^{2+}$  ions and citrate [167]. Reaction times of merely 10 min resulted in high radiochemical yields and purities above 95%, whereas the radioligand showed adequate in vitro stability at 10 h post labelling.

As previously reported in the literature, the direct 99mTc-labelling approach offers a quick and easy method for producing 99mTc-labelled antibodies and smaller proteins with high radiochemical yields and stability, often without requiring any additional purification steps. Subsequently, 99mTc complexation by reduced sulph-hydryl groups and free NH<sub>2</sub> groups is supposed to result in  $N_2S_2$ chelates whose radiochemical stability and biological activity greatly depend on the density of the thiol groups within the protein [168]. Considering the variety of amino acids involved in this type of chelation along with their complex location in the protein's structure, it remains difficult to predict the aforementioned characteristics. Since Annexin V exhibits only one cysteine residue buried within its tertiary structure, this approach is likely to generate a tracer with low specific activity, thereby making it less attractive for in vivo application. Thus, the preliminary data on directly 99mTc-labelled Annexin V require further evaluation in order to fully confirm the reproducibility of the radiolabelling method as well as the biopotency of the molecule.

*99mTc-SDH-Annexin V.* In addition to direct 99mTclabelling of Annexin V, a second simplified method was suggested by Subbarayan et al., also making use of a single reaction step [169]. In this pre-formed chelate approach, 99mTc was sequestered first by using succinic dihydrazide (SDH) along with tricine and nicotinic acid, after which the chelate was conjugated to the protein by heating at 90°C. The obtained radiochemical yield and purity both exceeded  $95\%$  initially, while  $94\%$  of  $99<sup>m</sup>$ Tc-SDH-Annexin V was recovered in saline and plasma 24 h post radiolabelling. Although Subbarayan et al. postulated that 99mTc-SDH-Annexin V production was significantly simpler than 99mTc labelling of Hynic-Annexin V, both types of kit preparation consist of one reaction step (i.e. starting from two kit vials) which provide comparable high radiochemical yields and purities, excluding any additional purification steps. However, the 99mTc-SDH-Annexin V radiolabelling requires extensive heating at 90°C for 10 min, which makes it less attractive for routine clinical use. Furthermore, it is very unlikely that the protein remains structurally intact at such a high reaction temperature. Previous studies have clearly demonstrated that many proteins, and Annexin V in particular, are very sensitive to elevated temperatures, which cause progressive denaturation and subsequent loss in biological activity. Moreover, some studies have even used heat-inactivated Annexin V as a negative control in ex vivo Annexin V binding assays. In such cases, heating at 56°C for 10 min was already sufficient to yield complete inactivation of the protein [90, 170]. These considerations could explain the apparent excellent stability of 99mTc-SDH-Annexin V in plasma compared with the in vitro stability in saline, since the protein has already been denaturated during radiolabelling, thereby making it virtually resistant to any further enzymatic breakdown in plasma. PD-10 size exclusion chromatography also revealed a clearly different elution profile of 99mTc-SDH-Annexin V compared with unlabelled Annexin V, indicating a discordance between the products' identities. In addition, HPLC analysis of the radioligand indicated two significant shoulder peaks, which were not identified.

All these findings raise serious doubts over the identity and radiopharmaceutical quality of <sup>99m</sup>Tc-SDH-Annexin V and over the relevance of the first biopotency data obtained in vitro [171] and in vivo in a tumour mice model of photodynamic therapy-induced apoptosis [169].

*99mTc-Annexin V mutants.* At the beginning of the 1990s, Huber et al. were the first to succeed in revealing the crystal and molecular structure of human Annexin V [52, 53, 172]. However, very soon afterwards the first mutant forms of the recombinant protein were developed by Tait et al. in order to study the structural basis for the high-affinity Annexin V membrane binding. Since His-204 and its adjacent residues in the third repeat of Annexin V (i.e. Arg-200, Arg-206 and Lys-207) were believed to be essential for anticoagulant activity, sitespecific mutagenesis of basic residues in this region by alanine seemed a promising approach for constructing short Annexin V derivatised peptides with increased anticoagulant properties [173]. Furthermore, such peptides, when radiolabelled, might prove most valuable as thrombus-detecting agents. Unfortunately, the produced 200A, 204A, 206A and 207A mutants exhibited unchanged binding affinity to phospholipids compared with the wild-type protein, indicating that the anticoagulant activity for short peptide sequences corresponding to this region was not related to their structural resemblance to the phospholipid binding region of unmodified Annexin V.

In pursuit of identifying new PS-recognising sites in Annexin V and studying their involvement in  $Ca^{2+}$ dependent membrane binding and their inhibitory effect on cytosolic phospholipase  $A_2$  (cPLA<sub>2</sub>) activation, several in depth studies were published more recently by the group of Russo-Marie et al. on a second group of Annexin V mutants [174, 175]. Based on the initial structure analyses of Huber et al., three high-affinity Ca2+-binding sites (i.e. Glu-72, Asp-144, Asp-303) had been identified in the domains I, II and IV of Annexin V. However, a fourth less essential  $Ca^{2+}$ -binding site (i.e. Glu-228) was discovered in domain III and appeared to be related to the presence of the Trp-186 and Trp-187 residues, which are located near the membrane surface in the Annexin V-phospholipid complex [176, 177]. Subsequent mutagenesis (i.e. Glu Gln or Ala, Asp Asn) of one

or more of these amino acids responsible for the bidentate attachment of calcium resulted in a class of single and multiple mutant constructs with different PS-binding properties and inhibitory effects on  $cPLA<sub>2</sub>$  activity. Of special interest were the quadruple mutant M1M2M3M4, containing all four defective Ca<sup>2+</sup>-binding sites (i.e. bearing one mutation in each Annexin V domain), and the M1M2M4 mutant, which had both completely lost their inhibitory effect on  $cPLA_2$  activation in comparison with wild-type recombinant Annexin V. These mutant proteins revealed that the  $Ca^{2+}$ -binding site located in domain I of Annexin V plays a major role in the inhibition of  $cPLA_2$  activity, whereas the fourth site is of secondary importance. In contrast, the  $Ca^{2+}$ sites located in domains II and III did not participate in this process while their overall molecular structure, as for the other mutants, was basically unaltered compared with the recombinant wild-type protein. Similar results were found when studying the inhibitory effect of wildtype and mutant Annexin V on cytosolic protein kinase C activity [178]. Additionally, enhanced mutational analysis in domain I of the M2M3M4 mutant has recently revealed a new PS-binding site which corresponds to a highly conserved consensus sequence present in the complete Annexin family [175].

Anyhow, the quadruple mutant M1M2M3M4 construct that became available through the increase in mutational analysis studies proved to be most suitable as a control protein for demonstrating the specificity of (wild-type) Annexin V binding to apoptotic cells or activated blood platelets. An increasing number of preclinical 99mTc-Hynic-Annexin V studies have started to use 99mTc-labelled M1M2M3M4 Annexin V as the control radioligand rather than radiolabelled human serum albumin, which has generally been used as a control protein in nuclear medicine for many years. Since M1M2M3M4 Annexin V possesses a very comparable molecular weight to wild-type Annexin V (MW 35,744 and 35,935, respectively), with a virtually unmodified overall molecular structure and only slight changes in physicochemical properties, it is probably the best control protein at present for demonstrating the specific nature of Annexin V binding.

Moreover, a new type of Annexin V mutant was recently developed by Tait et al. which carries an endogenous chelation site for 99mTc, thereby allowing direct 99mTc labelling of the protein [179]. The three mutant molecules, designated Annexin V-116, V-117 and V-118, were constructed by introducing seven amino acid sequences (i.e. containing either one or two cysteine residues) to the N-terminal side of Annexin V, whereas the naturally occurring Cys-316 was mutated to Ser in all three proteins (Fig. 4). Although radiolabelling of the mutant molecules was based on a simplified version of the method previously described for the  $99 \text{mT}c\text{-N}_2\text{S}_2$ -Annexin V, much higher radiochemical yields and purities were achieved while the overall reaction times were



Fig. 4A–C. Chemical structure of <sup>99m</sup>Tc-labelled Annexin V mutant molecules with endogenous chelation sites: **A** 99mTc-Annexin V-116, **B** 99mTc-Annexin V-117, **C** 99mTc-Annexin V-118. Y and X respectively represent the amino and carboxy terminal ends of the mutated Annexin V sequence

much smaller. This approach resulted in high specific activities of at least 66–132 GBq/µmol (i.e. especially for Annexin V-117 and Annexin V-118), which are more comparable with that of <sup>99m</sup>Tc-Hynic-Annexin V, while all radiolabelled mutants showed favourable in vitro stabilities over time. Both the non-radiolabelled and the 99mTc-labelled mutants demonstrated a fully preserved biological activity compared with Hynic-Annexin V and 99mTc-Hynic-Annexin V, respectively. Likewise, biodistribution studies in mice revealed predominant uptake in liver and kidneys for all radiolabelled mutants (ranging from 5.9% to 11.2% ID and from 5.9% to 17.9% ID, respectively), although the extent of uptake in these organs, along with spleen and bone marrow uptake, was significantly decreased in comparison with 99mTc-Hynic-Annexin V uptake (i.e. 16.6% ID and 39.1% ID for liver and kidney, respectively). In contrast, the abdominal clearance of the radiolabelled mutants was moderately increased [180–182]. Since Annexin V-116 and Annexin V-117 were assumed to form  $N_3S$  chelates whereas Annexin V-118 was believed to generate an  $N_2S_2$  chelate, it seems conceivable that these chelates resulted in a somewhat higher abdominal uptake, albeit much less pronounced than that previously observed with the  $99mTc-N<sub>2</sub>S<sub>2</sub>$ -Annexin V. Annexin V-117, which showed the most beneficial overall biodistribution properties, was further evaluated in a rat model of intramedullary cyclophosphamide-induced apoptosis. Significantly increased uptake was confirmed in femur and spleen 24 h post treatment due to ongoing apoptosis in bone marrow cells and splenocytes. In addition, cyclophosphamide**Table 3.** Primary structures of Annexin V mutants. Each mutant protein contains the indicated N-terminal sequence (italicised) followed by the amino acids 2–320 of human Annexin V. The initiator Met residue is removed post-translationally from all mutant

proteins and therefore not shown. In the Annexin V mutants 116, 117 and 118, the naturally occurring Cys residue at position 316 has also been mutated to Ser



All presented data were adapted from Tait et al. [179, 185] wt, Wild-type; NA, not applicable

<sup>a</sup> Membrane binding activity of unlabelled mutant Annexin V proteins.  $IC_{50}$  values for the mutant proteins were determined by a competition assay with FITC-Annexin V for binding to erythrocytes <sup>b</sup> Radiochemical yield and radiochemical purity (i.e. after purification by gel filtration) as determined by ITLC

treated mice showed substantially elevated tracer accumulation in the heart, spleen and bowels as early as 6 h post therapy. These results seem to suggest that <sup>99m</sup>Tc-Annexin V-117, owing to its lower basal overall uptake in healthy organs, might provide even higher targetto-background ratios than 99mTc-Hynic-Annexin V when imaging chemotherapy-induced apoptosis [180–182]. Nevertheless, the absolute tumour uptake of <sup>99m</sup>Tc-Annexin V-117 in cyclophosphamide-treated KDH-8 hepatomas reported by Kuge et al. [183] was threefold lower compared with earlier reported data for <sup>99m</sup>Tc-Hynic-Annexin V in the same rat model [184].

Soon afterwards, another class of Annexin V mutants emerged which was specifically designed to allow radiolabelling by means of the tricarbonyl  $99mTc(CO)$ <sub>3</sub> core [185]. For this purpose, N-terminal extentions containing either three or six histidine (His) residues were attached to the protein since His is known to form highly stable multivalent complexes with  $[99mTc(CO)_{3}(H_{2}O)_{3}]^{+}$ , thereby resulting in high specific activities. Similar to the previously described molecules, mutant forms of human Annexin V cDNA were cloned in an expression vector and expressed cytoplasmaticaly in *E. coli*, after which they were purified in high yields and purity.  $\frac{99 \text{m}}{\text{C}}(\text{CO})_3$ labelling of the Annexin V-122 and Annexin V-123 mutants resulted in similar radiochemical yields, in vitro stability and biopotencies as were observed for the mutants bearing endogenous chelation sites (Table 3). Although Annexin V-123 exhibited the most advantageous overall radiochemical properties, specific activies (i.e. at least 13–26 GBq/µmol) were nevertheless considerably lower compared with those reported for <sup>99m</sup>Tc-Annexin V-116, -117 and -118 mutants. Although less

<sup>c</sup> Membrane binding activity of 99mTc-labelled mutant Annexin V proteins. Binding to erythrocytes was determined similarly to the method described for the unlabelled mutant proteins

<sup>d</sup> Results from the tricarbonyl radiolabelling method

<sup>e</sup> Data originating from single measurements

complex and time-consuming than the multistep  $N_2S_2$ method, tricarbonyl labelling of His-tagged proteins still requires a two-step procedure in which the  $[{}^{99m}\text{Tc}(\text{CO})_3(\text{H}_2\text{O})_3]$ <sup>+</sup> chelate must be first formed in a separate step at 100°C. In contrast, recombinant proteins with endogenous chelation sites (i.e. in particular Annexin V-117), like Hynic-Annexin V, can be used for direct 99mTc labelling at room temperature or 37°C and therefore provide a faster and more simple labelling method for routine production in a clinical setting.

*99mTc-tricarbonyl Annexin V.* As with the abovementioned Annexin V-122 and Annexin V-123 mutants,  $99mTc(CO)$ <sub>3</sub> labelling has also been applied to native Annexin V by two different methods. In an effort to address the generally observed high renal and hepatic accumulation of 99mTc-labelled Annexin V, Han et al. developed the tricarbonyl ligand  $[99mTc(CO)_3$  PADA]-AV based on the previously established method of Alberto et al. [186]. For this purpose,  $[{}^{99m}\text{Tc}(\text{CO})_3(\text{H}_2\text{O})_3]$ <sup>+</sup> was complexed with picolylamine-*N*,*N*-diacetic acid (PADA), after which the pre-formed chelate was converted to an activated trifluorophenyl (TFP) ester and conjugated to Annexin V [187]. As reflected by in vitro stability experiments, tricarbonyl labelling of PADA resulted in a stable complex remaining fully intact at 16 h of excessive histidine challenge. Subsequently,  $[99mTc(CO)_3$  PADA]-AV exhibited fast uptake in kidneys, liver and spleen of mice early after administration (i.e. 78%, 36% and 31% ID/g at 0.25 h p.i., respectively), followed by a gradual clearance over time with, respectively, 2%, 3% and 2% remaining at 12 h p.i. Although lower early activity uptake was reported in all these organs for  $99mTc$ -Hynic-

Annexin V [141, 188, 189], the kidney accumulation of  $[99mTc(CO)$ <sub>3</sub> PADA]-AV at 3 h p.i. was already significantly lower whereas liver and spleen uptake remained slightly higher. Considering this finding in conjunction with a very fast blood clearance and low residual body retention,  $[99mTc(CO)_3$  PADA]-AV seems to be characterised by improved pharmacokinetic properties.

A second tricarbonyl method recently emerged which was applied to Hynic-derivatised DNA analogues [190] and proteins like Annexin V [191]. Since the Hynic chelator has been shown to sequester the  $99mTc(I)$  tricarbonyl ion easily,  $[99mTc(CO)_{3}(H_{2}O)_{3}]^{+}$  was coupled to Hynic-Annexin V in a single reaction step, yielding radiochemical purities of about 90% after additional purification. Preliminary biodistribution studies in Balb/c mice with anti-Fas MoAb-induced hepatic apoptosis showed predominant activity retention in liver and kidneys. Furthermore, the twofold increase in hepatic uptake of 99mTc(I)-Hynic-Annexin V compared with control animals was in the same order of magnitude as that observed with conventional <sup>99m</sup>Tc-Hynic-Annexin in 1 htreated Balb/c mice as reported by Blankenberg et al. [141]. Therefore,  $99mTc(I)$ -Hynic-Annexin V seems to hold potential for in vivo monitoring of apoptosis. However, in spite of the easy and kinetically fast complexation of  $[{}^{99m}\text{Tc}(\text{CO})_{3}(\text{H}_{2}\text{O})_{3}]^{+}$  to Hynic-Annexin V, the tricarbonyl approach provides a less stable radioligand compared with  $99mTc$  (V)O<sup>3+</sup>-labelled Hynic-Annexin V since only 70% of the molecule remains intact in saline or plasma 4 h after preparation. In this regard, the 99mTc-Hynic-Annexin V as originally developed by Blankenberg et al., based on the method of Abrams et al., remains a better choice of radioligand [140, 141].

#### 111Indium-DTPA-PEG-Annexin V

Following the initiation, execution and disintegration phases of the apoptotic cell death process, the remaining small "apoptotic bodies" will finally be recognised by macrophages and neighbouring cells which will engulf and eliminate the cell fragments by phagocytosis. Thus, externalisation of PS residues to the surface of dying cells eventually acts as a "removal" signal for macrophages which express the PS receptor. Concordantly, apoptotic cell death represents a dynamic process, which provides a temporary time frame for detection in vivo. In this context, apoptosis-detecting radioligands with a prolonged circulation in the blood compartment in theory might provide improved visualisation conditions for apoptosis detection in tumours. In search of such apoptosis markers with enhanced imaging properties, Li et al. developed a PEGylated Annexin V construct in order to increase the biological half-life of the protein [192]. Polyethyleneglycol (PEG) was used as a spacer between Annexin V and diethylene triamine penta-acetic acid (DTPA) as the chelating group, after which the molecule was radiolabelled with <sup>111</sup>In. <sup>111</sup>In-DTPA-PEG-Annexin V could be obtained in high radiochemical yields (i.e. 92%) with excellent radiochemical purity of >98%.

111In-DTPA-PEG-Annexin V was also evaluated in a tumour model of paclitaxel and anti-EGR MoAbinduced apoptosis in mammary MDA-MB468 tumourbearing nude mice. Paclitaxel-treated animals showed significantly increased tumour uptake 4 days post treatment, whereas a substantial decrease in radioligand tumour uptake was seen in nude mice treated with the anti-EGR MoAb. In addition, a good correlation was found between the radioligand uptake in tumours and the apoptotic index determined histologically ( $r^2$ =0.77). Wholebody gamma images of treated nude mice at 48 h following tracer injection clearly demonstrated an enhancement of the contrast in the tumours, thereby providing first evidence for the hypothesis that a prolonged circulation of radiolabelled Annexin V in the body might contribute to improved visualisation of tumour apoptosis. In this regard, the 111In radionuclide seems a good choice for diagnostic imaging of apoptosis, considering its prolonged half-life (physical half-life of  $\frac{111}{In}$ =2.81 days,  $E_{\text{max}}$  $\neq$  0.172, 0.247 MeV) and relatively low gamma energies.

#### 11Carbon-Annexin V

Another radioligand for PET imaging of apoptosis was proposed by Ito et al., who introduced 11C (physical half-life of <sup>11</sup>C=20.39 min,  $E_{\text{max}}\beta^2$ +=0.961 MeV) into the Annexin V protein [193]. In a first step,  $^{11}CH_{3}I$  was generated from the cyclotron product  ${}^{11}CO_2$  through autochemical synthesis. Afterwards  $^{11}CH<sub>2</sub>I$  was reacted with Annexin V dissolved in an MeOH solution at −20°C. The reaction was allowed to proceed for 5 min at 80°C, followed by solvent dry out under vacuum and reconstitution of the newly formed 11C-Annexin V in saline. Radiochemical yields were in the range 10–15% with an RCP above 95% as determined by HPLC. The biopotency of 11C-Annexin V was tested in vitro towards Gc-4SD cells (5% apoptotic) and Gc-4PF cells (34% apoptotic). Although the Gc-4PF cells were reported to show significantly increased tracer uptake over Gc-4SD cells, no data were provided to support these findings or to demonstrate the specificity of the radioligand uptake.

Furthermore, 11C-labelled Annexin V does not seem to be a suitable PET ligand for imaging cell death for several reasons: The physical half-life of 11C will undoubtedly be too short to allow repeated in vivo monitoring of the apoptotic process over time, thereby severely reducing the time window for detection almost to a single moment. As a result, much crucial information will be lost concerning the kinetics of the biological process. Secondly, the radiolabelling procedure for preparing 11C-Annexin V on a routine basis is rather complicated and time-consuming. In particular, the very poor radiochemical yields associated with the production of shortliving 11C-Annexin V represent a major constraint for the clinical applicability of the radioligand. Most importantly, 11C-labelling of Annexin V requires an extensive heating step similar to that described for 99mTc-SDH-Annexin V, which should result in substantial denaturation of the protein and a subsequent loss in biological activity. In this regard, alternative approaches for the proposed radiolabelling of 11C-Annexin V seem mandatory.

## 64Cu-DOTA-Annexin V

Along with 94mTc-Hynic-Annexin V, a new Annexin Vbased PET ligand recently emerged which was actually developed by the same research group. McQuade et al. reported on the radiolabelling of DOTA-conjugated Annexin V with 64Cu as an alternative PET radionuclide [157]. For this purpose, 1,4,7,10-tetraazacyclododecane-*N*,*N*′,*N*′′,*N*′′′-tetra-acetic acid (DOTA) was first activated with 1-ethyl-3-[3-(dimethylamino)propyl]-carbodiimide (EDC) and *N*-hydroxy sulphosuccinimide (sulpho-NHS) and afterwards conjugated to Annexin V. In a third step, DOTA-Annexin V was reacted with 64Cu under heating at 55°C for 40 min, which resulted in high specific activities (i.e. 106–132 GBq/µmol) and radiochemical purities in the range of 90–94% (Fig. 5). Furthermore, 64Cu-DOTA-Annexin V is being evaluated in the same animal model of anti-Fas MoAb-induced hepatic apoptosis as described for 94mTc-Hynic-Annexin V.

When compared with <sup>94m</sup>Tc, the longer half-life of <sup>64</sup>Cu (physical half-life of <sup>64</sup>Cu=12.7 h,  $E_{\text{max}}\beta^{\text{+}}=0.578$ , 0.65 MeV) should provide a significantly wider time frame for in vivo monitoring of apoptosis in humans, whereas the lower  $\beta$ <sup>+</sup> energy of the radionuclide should result in a decreased radiation burden to the patients' organs, in particular to the kidneys, spleen and liver. Hence, in spite of a slightly more complex synthesis, 64Cu-DOTA-Annexin V may be suitable for application as a PET ligand in apoptosis imaging, especially in clinical settings.

### 67/68Gallium-DOTA-Annexin V

Simultaneously with the development of 64Cu-DOTA-Annexin V, the protein has also been radiolabelled with  $67Ga$  and  $68Ga$  using the same methodology (Fig. 5) [194]. Activation of the DOTA chelator with EDC and sulpho-NHS was nearly identical, resulting in a conjugation ratio of 3.7 molecules of DOTA/Annexin V. The final radiolabelling step with the gallium isotopes showed only minor differences in reaction conditions and reagents compared with the 64Cu labelling. Immunoreactivity testing of the radioligands revealed comparable biological activity of 67Ga-DOTA-Annexin V with



**Fig. 5.** Chemical structure of DOTA-Annexin V with AX=64Cu, <sup>67</sup> Ga or 68 Ga

99mTc-Hynic-Annexin, which in turn was superior to 68Ga-DOTA-Annexin V.

Dual-isotope biodistribution studies in mice and rats injected with a mixture of 67Ga-DOTA-Annexin V and 99mTc-Hynic-Annexin V clearly revealed a rapid blood clearance over time for both tracers. However, the blood clearance was obviously better in the case of 99mTc-Hynic-Annexin V. In contrast, at 2 h p.i. the <sup>99m</sup>Tc radioactivity levels were significantly higher than the 67Ga levels in the lungs, liver, spleen and gastro-intestinal tract, whereas kidney and heart uptake were similar. These preliminary biodistribution results seem to suggest that 67Ga-DOTA-Annexin V could be useful as an alternative SPECT ligand for imaging apoptosis by providing higher signal-to-noise ratios. In addition, slower but more sustained tumour uptake might be achieved with 67Ga-DOTA-Annexin V owing to its longer retention time in the blood compartment relative to 99mTc-Hynic-Annexin V.

Alternatively, first micro-PET studies in rats treated with anti-Fas MoAb to induce hepatic apoptosis showed increased liver uptake of 68Ga-DOTA-Annexin V by a factor of 4.4 compared with control animals. Thus, the PET counterpart of <sup>67</sup>Ga-DOTA-Annexin V could offer new possibilities in PET imaging of apoptosis in spite of its lower in vitro biological activity. Nevertheless, the high-energy positron emission characteristics of <sup>68</sup>Ga (physical half-life of  $^{68}Ga=1.135$  h,  $E_{max}\beta^{\dagger}=1.9$  MeV) might hamper its application in the clinic by depositing a high radiation burden to specific organs such as the kidneys or liver. In contrast, 67Ga-DOTA-Annexin V (physical half-life of  $^{67}Ga=3.26$  days,  $E_{\text{max}} \neq 0.300$ , 0.393 MeV) exhibits a much longer half-life, allowing extensive in vivo monitoring of apoptotic processes over a wide time frame while emitting gamma rays at the upper detection limit of SPECT cameras.

#### 18F- and 99mTc-labelled radiopeptides

In the broad group of recently developed apoptosisdetecting radioligands, a radiopeptide construct was described, based on the AFIM molecule. Boisgard et al.

succeeded in engineering a small 8-kDa mini-protein derived from the specific PS-binding domain of the annexins which contains a multifunctional site for radiolabelling with either an 18F tag, such as the 18F-labelled maleimide reagent [195, 196], or 99mTc [197, 198]. Both radiolabelling methods yielded very high specific activities (i.e. 490–4,370 GBq/µmol) with excellent radiochemical purity of >99%. Furthermore, the AFIM construct was characterised by a high thermodynamic stability and high affinity for PS-containing membranes. Both tracers were also evaluated for tumour uptake in several melanoma mouse models of chemotherapy-induced apoptosis at various time points until 72 h following therapy administration [199]. 18F-AFIM was excreted predominantly through the kidneys, with minor uptake in the liver and gastro-intestinal tract whereas 99mTc-AFIM was exclusively excreted by the kidneys without showing uptake in any of the other organs. In addition, extremely fast blood clearance was reported for the 99mTc-AFIM molecule, with removal from the blood compartment within 10 min p.i. Tracer uptake was reported in treated tumours only at 72 h post chemotherapy and in some untreated tumours, presumably reflecting spontaneous ongoing apoptosis.

The biological rationale for engineering a small 8-kDa mini-protein derived from the specific PS-binding domain of the annexins is very interesting because such peptide-like molecules could benefit from the favourable biodistribution characteristics that small peptides in general exhibit over bigger proteins. However, reducing the molecular structure of Annexin V by stripping of most of its 319 amino acids in order to retain a PS-binding core seems a very challenging undertaking for many reasons. In particular, such a drastic reduction in molecular size and integrity could result in major conformational changes, thereby affecting the stability and high affinity of the protein for binding PS residues. Most surprisingly, Boisgard et al. reported that the AFIM construct was characterised by a high thermodynamic stability and high affinity for PS-containing membranes. Unfortunately, no real evidence was provided to support these preliminary findings. Additionally, no concrete data have so far been presented on the molecular structure of the AFIM mini-protein that would allow true comparison with Annexin V or with the highly conserved consensus sequence found in all Annexins, which contains two of the most important PS-binding sites [175]. Although the concept of a multipurpose radiolabelling site, allowing both 18F and 99mTc chemistry, is most interesting, the structural information on which this approach is based remains unclear. In spite of the very high specific activities obtained by this method, the in vitro and in vivo stability of the corresponding radioligands still needs to be fully demonstrated.

Both radiolabelled AFIM molecules, and 99mTc-AFIM in particular, seem to be cleared from the body more rapidly than 99mTc-Hynic-Annexin V owing to a very

fast blood clearance followed by a predominant and rapid kidney clearance. However, whether the significantly increased blood clearance will contribute to higher tumour-to-background ratios when studying chemotherapy-induced apoptosis will greatly depend on the tumour's extraction efficiency and clearance. The fact that Boisgard et al. were unable to demonstrate ongoing tumour apoptosis within 24 and 48 h post therapy, in contrast to many other in vivo studies, might indicate that the radiolabelled AFIM ligands are cleared from the body too quickly to allow sufficient uptake and subsequent visualisation of apoptotic tumour cells. Furthermore, the lack of any semi-quantitative biodistribution data for 18F-AFIM and 99mTc-AFIM in the described tumour models makes it impossible at present to compare organ and tumour uptake values with those reported for other apoptosis-detecting radioligands. Furthermore, the use of 2-deoxy-2-[18F]fluoro-D-glucose (18F-FDG) as a positive control tracer for 99mTc-AFIM tumour uptake does not seem to be a good choice for proving the specificity of the apoptotic signal. Although 18F-FDG is being widely used to measure the glucose metabolism in a variety of organs and disease states, this tracer is unable to detect apoptotic or necrotic cell death by a specific mechanism of action.

## *Anti-PS monoclonal antibodies*

Externalised PS residues as the primary target molecule for early detection of apoptotic cell death in vivo may also serve as antigen-binding sites for anti-PS antibodies. This type of antibody, in addition to anti-cardiolipin and lupus anticoagulant (LAC) antibodies, belongs to the family of anti-phospholipid antibodies which are known to inhibit the procoagulant and pro-inflammatory activities that externalised PS residues exert. The presence of anti-PS auto-antibodies circulating in the blood has been correlated with an increased risk of recurrent arterial and venous thrombo-embolism, recurrent foetal loss and thrombocytopenia. These symptoms are often related to the autoimmune disease SLE and many other conditions, which are generally referred to as the anti-phospholipid syndrome (APS). However, with the first PS-targeting MoAbs being described, such molecules, when radiolabelled, could be considered as alternative markers for apoptosis detection. The 3G4 mouse anti-PS MoAb  $(IgG_3)$  has shown equal affinity for PS residues and PI residues whereas the 9D2 rat MoAb (IgM) exhibits predominant affinity for PS residues ( $K_d \approx 0.1$  n*M*), which in fact appears to be 10- to 70-fold higher than observed for Annexin V. Nevertheless, the slow blood clearance associated with such antibodies, in some applications, could represent a major drawback to their use in nuclear medicine, indicating the need for construction of small PS-targeting antibody fragments with enhanced pharmacokinetic properties.

Most interestingly, anionic phospholipids such as PS have also been proposed as specific markers for tumour vasculature and consequently as potential targets for cancer imaging and therapy. Externalisation of PS residues not only seems to take place during PCD or platelet activation, but also can occur on the cell surface of viable endothelial cells in response to a variety of cellular stress factors and pathological conditions. The most prominent factors include inflammatory cytokines (e.g. IL-1 $\alpha$  or TNFα), hypoxia/reoxygenation, thrombin, acidic conditions,  $H_2O_2$  or combinations of hypoxia/reoxygenation and IL-1 $\alpha$  or TNF $\alpha$ . A recent study by Ran et al. demonstrated that PS becomes exposed on the vascular endothelial cells of different types of apoptotic solid tumours in mice and that such PS translocation is most likely caused by stress factors similar to those described for normal endothelial cells [200]. Although PS-positive tumour endothelium mostly was found to be nonapoptotic, PS-positive vessels appeared to be located particularly in and around regions of necrotic and apoptotic tumour cells, where hypoxia, acidity, thrombosed blood vessels, infiltrating host leucocytes and cytokine secretion are commonly present. Thus, the breakdown of PS asymmetry and subsequent exposure of PS residues to the cell surface of tumour blood vessels and malignant cells seems directly related to the necrotic and apoptotic status of the tumour microenvironment.

Taking these findings into account, PS-directed MoAbs such as the 3SB mouse antibody are being developed by Peregrine Pharmaceuticals Inc. (Tustin, CA, USA) as potential vascular targeting agents (VTAs). The 3SB IgM antibody shows major reactivity to PS but not to any other phospholipid, except for phosphatidic acid, which is only a minor component of the plasma membrane. According to Ran et al., PS residues are ubiquitously expressed on tumour endothelial cells (i.e. approximately 3×106 molecules per cell) and are located on the luminal surface of the tumour's blood vessel endothelium in all regions of the tumours, which makes them directly accessible for binding to VTAs administered in the blood [200]. In addition, PS residues are known to be abundantly present on endothelial cells of a variety of solid tumours while being absent from endothelium in nearly all the normal tissues. These characteristics make PS residues interesting targets for cancer imaging and therapy.

In spite of these interesting hallmarks, the potential use of anti-PS MoAbs and radioimmunoconjugates thereof in cancer imaging through vascular targeting is a difficult objective. In contrast to endothelial cells of murine or bovine origin, which were used as an in vitro model in the study of Ran et al., human vascular endothelial cells are likely to respond to similar cellular stress factors in a totally different way, possibly without causing any PS expression. Hence, extensive research is required to investigate the clinical applicability of using endothelial PS exposure as a target for vascular targeting

and cancer imaging. Previous studies on tumour neoangiogenesis have demonstrated that the vascular structure of neoplastic tissues is often characterised by many "leaky" blood vessels, easily allowing passive diffusion of molecules into the tumour's microenvironment [201]. On the other hand, the extent of neovascularisation might differ from one tumour type to another. Taking these considerations into account, it remains to be seen whether specific tumour uptake by radiolabelled anti-PS MoAbs can actually be achieved by significantly increased PS expression on the tumour's vasculature, rather than by increased vascular permeability or vascularisation contributing to a specific tracer uptake. Other potential risks related to the clinical use of radiolabelled anti-PS MoAbs, such as the HAMA response, might be circumvented by generating chimerised or fully humanised variants.

## **Alternative radioligands**

#### *Anti-Annexin V monoclonal antibodies*

Like the typical anti-phospholipid auto-antibody LAC, which is a well-known risk factor for thrombosis and recurrent spontaneous abortion, extracellular Annexin V can act as a pathogenic factor by providing an antigenic stimulus for auto-antibody formation. Thus, as for the anti-phospholipid auto-antibodies described earlier, significantly elevated concentrations of anti-Annexin V MoAbs have been found in sera from patients with rheumatoid arthritis, SLE, arterial or venous thrombosis, intrauterine fetal loss, pre-eclampsia and prolonged activated partial thromboplastin time. Furthermore, anti-Annexin V MoAbs present in sera from patients with SLE have been shown to exhibit anti-phospholipid and LAC properties [202–205].

As a result of these studies, several anti-Annexin V MoAbs were generated which could be radiolabelled for apoptosis imaging purposes. The majority of commercially available MoAbs are mouse (IgG<sub>1</sub> or IgG<sub>2a/K1</sub>), rabbit (IgG) and goat (IgG)-anti-human Annexin V specific MoAbs. At present, only one radiolabelled MoAb directed against human Annexin V has been described, by Kobayashi et al., who evaluated an 111In-DTPA anti-Annexin V MoAb in a rat model of myocardial ischaemia–reperfusion injury (IR) [206, 207] as well as in rats with myocardial infarction (MI) [208]. These studies assumed that Annexin V exists in the soluble fraction of the healthy myocardium and is translocated to the myocardial cell membrane after transient acute ischaemia, thereby becoming accessible for binding to Annexin Vdirected MoAbs. Twenty-four hour planar images of rats at 2, 7, 14 and 21 days post IR showed significantly increased tracer uptake in the heart compared with control animals. The difference in myocardial tracer accumulation was highest at 2 days after onset of ischaemia (i.e.

heart/lung ratio 3.32 vs 1.41 in controls) and gradually diminished over time until it became nearly insignificant at 50 days post IR. Macro-autoradiography revealed that 111In-DTPA anti-Annexin V MoAb radioactivity was mainly located in the ischaemic area of the myocardium and in the left anterior descending coronary region of ischaemic rats owing to the left coronary artery occlusion used to induce transient myocardial ischaemia. In rats with acute MI, the increase in myocardial tracer uptake was even slightly higher compared with the corresponding IR rat group at 7 days after onset. The radioligand accumulated predominantly in the marginal area of the infarcted tissue as demonstrated by autoradiography. These preliminary data seem to suggest that radiolabelled anti-Annexin V MoAbs might be used for in vivo detection of myocardial ischaemia and cell death. Nevertheless, additional information is required to clearly demonstrate the specificity of antibody binding to Annexin V molecules as well as its clinical applicability. Furthermore, the mechanisms by which intracellular Annexin V becomes translocated to the outer side of the cell membrane and the pathological conditions associated with this phenomenon still need to be elucidated. In fact, more recent studies have revealed that the endstage of heart failure in humans is characterised by a marked over-expression of Annexin II, V and VI along with a translocation of Annexin V from cardiomyocytes to interstitial cardiac tissue [209, 210].

A second approach in which radiolabelled anti-Annexin V MoAbs could be used as alternative radioligands for apoptosis imaging would consist in the pretargeting concept that has been successfully applied in radioimmunodetection and radioimmunotherapy of tumour growth for several years. Considering the stoichiometry of Annexin V binding to externalised PS residues, some studies have demonstrated that, in theory, four to eight Annexin V molecules can bind to a single PS residue [100]. Hence, the apoptotic signal initially generated by PS exposure in early apoptotic cells could be amplified through binding with exogenously administered "cold" Annexin V, which in turn would act as a secondary target molecule. In a second step, the radiolabelled anti-Annexin V MoAb would then be injected in order to bind to the Annexin V moeities locally presented in the region of ongoing apoptosis. Evidently, such an approach would need to overcome the classical problems associated with antibody pre-targeting. In this case, endogenous Annexin V molecules circulating in the blood might interfere with the MoAb binding, thereby contributing to a high overall background radioactivity and to a higher radiation dose to specific organs. Although extracellular Annexin V under normal physiological conditions is present in very low concentrations in the blood compartment (i.e. 1–6 ng/ml), it should be considered as a possible interfering factor, especially in pathological conditions such as myocardial infarction which are characterised by a more than tenfold increase

in the endogenous blood concentration of the protein [45, 211]. On the other hand, taking the fast bi-exponential blood clearance of human Annexin V into account, non-PS-bound Annexin V should be sufficiently cleared from the blood upon administration in order to provide a strong apoptotic signal for radioligand binding. Therefore, the use of radiolabelled antibodies directed against the Annexin V protein as target molecule might constitute an alternative approach in apoptosis imaging.

## *Radiolabelled caspase inhibitors and substrates*

Amongst the group of newly developed radioligands directed against alternative target molecules involved in the apoptosis cascade, the use of radiolabelled caspase inhibitors probably represents one of the most innovative but also most tantalising approaches. Caspases are a family of cysteine-containing aspartate-specific proteases which play a key role in the apoptotic process. The caspases are synthesised intracellularly as inactive proenzymes essentially in all animal cells and are activated by cleavage at specific aspartate-cleaving sites in order to release a N-terminal pro-domain, leaving a large (∼20 kDa) and a small subunit (∼10 kDa) to heterodimerise. The active enzyme is a tetramer composed of two such heterodimers, which are primarily associated through interaction of the small subunits. The active protease can in turn sequentially activate other caspases, thereby generating a cascade which will eventually cause mitochondrial release of pro-apoptotic molecules [212–214]. Since caspase activation occurs in the early phase of the intracellular signalling process of cells undergoing apoptosis, radiolabelled caspase inhibitors could offer a valuable and highly specific tool for early detection of apoptosis. Furthermore, targeting of activated caspases is believed to be more specific in apoptosis detection than the PS-targeting approach, where necrotic cells can also contribute to the cell death signal. Many types of caspase inhibitors and caspase substrates have been constructed for the different members of the caspase family, each with different specificity. However, the group of fluoromethylketone (fmk) caspase inhibitors exhibit the most favourable characterisitics since they are highly cell permeable, soluble and irreversible in action while possessing an extended biological half-life and lower cytotoxicity in vivo compared with other groups. Amongst these, benzyloxycarbonyl-Val-Ala-DL-Asp (*O*-methyl)-fmk, designated Z-VADfmk, is one of the most commonly used caspase inhibitors with broad-spectrum activity.

In a study published by Haberkorn et al., 131I-labelled Z-VAD-fmk was evaluated as an alternative in vivo marker for PCD through targeting and irreversible trapping by caspase inhibitors [215]. Successful radioiodination of the phenyl moiety of the *N*-terminal z-protection group clearly depended on the presence of carrier iodide,



**Fig. 6.** Chemical structure of the 4-iodophenyl derivative (Y) and 2-iodophenyl derivative  $(X)$  of  $\lceil 131 \rceil$ IZ-VAD-fmk which were generated in radiochemical yields of >60 and <40, respectively. X and Y both represent 131I

resulting in moderate radiochemical yields (i.e. 70%) and specific activities of about 3.3 GBq/µmol. However, the  $T1(TFA)_{3}/[131]$ iodide labelling method generated a mixture of 2-iodophenyl and 4-iodophenyl derivatives which could not be separated on RP-HPLC (Fig. 6). Changing the order in which Z-VAD-fmk was reacted with  $T1(TFA)$ <sub>3</sub> and  $[131]$  iodide did not affect the 4-iodophenyl product yield (i.e. 61%). Subsequently, in vitro [131I]IZ-VAD-fmk uptake was investigated in Morris hepatoma (MH3924Atk8) cells expressing the herpes simplex virus thymidine kinase (*HSVtk*) gene, in which apoptosis was induced by ganciclovir treatment. Intracellular uptake of [131I]IZ-VAD-fmk was increased merely twofold 24 h post treatment when compared with controls and remained nearly unchanged in both groups when the incubation time was increased up to 4 h. In contrast, 23% apoptotic cells were found in the TUNEL assay 24 h after ganciclovir therapy compared with 1.3% immediately after therapy administration, whereas "cold" IZ-VAD-fmk had shown a similar inhibition potency as Z-VAD-fmk towards apoptotic BJAB and SKW6 cells. In addition, the 131I-labelled oligopeptide exhibited a rather poor absolute cellular uptake (i.e. 0.76% of the activity accumulated in untreated MH3924Atk8 cells), characterised by a slow transport mechanism of passive diffusion.

In view of all these radiochemical and biological problems associated with radiolabelled caspase inhibitors, many hurdles still need to be overcome before successful apoptosis imaging can be achieved. Furthermore, it is unclear whether the concentration of activated caspases generated in apoptotic cells will be high enough to provide sufficient radioligand accumulation for in vivo imaging. In this regard, radiolabelled caspase substrates might be more attractive candidates for metabolic trapping. Such an approach would entail delivery of radiochelated caspase substrates into the apoptotic cell, which would then be cleaved by activated caspases, leading to accumulation of radioactive hydrophilic metabolites. Since all activated caspases can repeatedly cleave multiple substrates during the apoptotic cascade in the cell, this approach could result in a significant amplification of the tracer signal, thereby enhancing the target-to-background ratio. In fact, more than 280 caspase substrates have been identified to date, providing an impressive amount of target molecules for caspase cleavage [216]. In addition, further progress is being made on the 18F radiochemistry of fmk derivatives, which will provide new opportunities in the fluorination of fmk-based caspase inhibitors [217].

### *MMP-targeting radioligands*

As previously mentioned, the mitochondria play a key role in the initiation of both apoptotic and necrotic cell death. The mitochondrial permeability transition pore (MPTP) is assumed to represent a high-conductance unselective channel between the inner and outer mitochondrial membranes whose opening is triggered by several physiological effectors, such as elevated matrix  $[Ca^{2+}]$ , reduced concentrations of adenine nucleotides, reactive oxygen species or pH changes. The MPTP opening (i.e. often described as "mitochondrial permeability transition") causes a sudden increase in the permeability of the inner mitochondrial membrane to molecules smaller than 1.5 kDa, which results in uncoupling of the respiratory chain, immediate dissipation of the proton-dependent mitochondrial transmembrane potential ( $\Delta \Psi_m$ , MMP) and interruption in ATP synthesis followed by massive osmotic swelling of the mitochondria. Finally the outer mitochondrial membrane is disrupted with release of intermembrane components such as cytochrome *c*, procaspase-9, apoptosis-inducing factor and endonuclease G, which cause the cell to undergo apoptosis through caspase activation. In contrast, a high membrane potential, a low pH and cyclosporin A (CsA) provide protection against MPT [218–221]. During the apoptotic process, the MMP is being disrupted before caspase and endonuclease activation occur and this disruption even precedes PS exposure on the cell surface as well as morphological signs of apoptosis. The MMP collapse provoked at the high irreversible level of MPTP conductance is also considered as the point of no return in the apoptotic process and therefore represents an attractive and specific target for early detection of cells committed to die [9, 222–225].

Recently, Madar et al. developed a series of lipophilic MMP-dependent fluoro-phosphonium cations for PET imaging of apoptosis. For this purpose, several triphenyl methyl-phosphonium derivatives were radiolabelled with <sup>18</sup>F and evaluated for chemical and metabolic stability in vitro while their biodistribution was studied in rodents and mongrel dogs by PET imaging [226]. Among the group of fluorinated phosphonium analogues, [18F]*p*-fluorobenzyltriphenyl-phosphonium cation, [18F]*p*-FBnTP, showed the most favourable metabolic stability while exhibiting an extremely rapid blood clearance in mongrel dogs  $(T_{1/2}=12 \text{ s})$ . Furthermore, the high, sustained tracer accumulation in multiple organs

could be reduced by 87% when MMP loss was induced. Biodistribution studies in mice and rats revealed a fast and predominant radioactivity uptake in the heart, followed by lungs, kidneys, muscle and liver. In addition, a 40–60% regional decrease in myocardial [18F]*p*-FBnTP uptake could be documented in mongrel dogs with heart failure-induced cardiomyopathy. These findings were in accordance with the typical changes related to heart failure such as dilatation of the ventricles and thinning of the posterior heart wall [227]. These preliminary studies indicate that the heart represents the main target organ for [18F]*p*-FBnTP uptake. Consequently, radiolabelled MPP markers such as [18F]*p*-FBnTP show potential for in vivo detection of myocardial cell death by means of PET imaging.

In vitro models of taxotere-induced apoptosis in lung and prostate carcinoma cells also demonstrated a significant decrease in [18F]*p*-FBnTP uptake of 54% and 43%, respectively. Furthermore, the decrease in tracer accumulation correlated inversely with the extent of taxotere-induced apoptosis as determined by TUNEL staining. Additionally, breast carcinoma-bearing nude mice treated with taxotere showed 45% lower tracer uptake in tumours at 48 h post therapy compared with control animals [228]. Similar results were achieved in a rat model of prostatic apoptosis, where lobe-specific decrease in [18F]*p*-FBnTP accumulation (i.e. ranging from 45% to 58%) was observed between 2 and 4 days after androgen depletion [229]. Most interestingly, the differences in tracer uptake in the apoptotic prostate lobe were more pronounced than the changes in TUNEL-positive cells. Therefore, in vivo monitoring of the MMP collapse could represent a more sensitive method for early detection of apoptosis compared with existing methods such as the TUNEL assay directed against DNA laddering. Moreover, the MMP is considered to be a more accurate predictive parameter for cell death than caspase activation, which is often not required to generate apoptosis [220]. Taking these data into account, MMP-dependent biomarkers such as [18F]*p*-FBnTP could represent a useful group of new radioligands for early evaluation of chemo- or radiotherapy-induced apoptosis.  $\Delta \Psi_{\rm m}$  disruption is a constant hallmark of apoptosis which has been found in a broad variety of cell types [222, 224]. Nevertheless, some cell types have been reported to undergo apoptosis without demonstrating early changes in  $\Delta \Psi_m$ or inhibition of CsA [218]. Consequently, MMP-dependent radioligands might not be applicable for apoptosis detection in such cell types.

In addition to the MMP-targeting radioligands, the effect of apoptosis-inducing drugs which act on the  $\Delta \Psi_{\text{m}}$ can also be monitored indirectly by using radiolabelled Annexin V. The flavanoid quercetin in particular has been shown to induce apoptosis by triggering a secondary  $\Delta \Psi_{\rm m}$  decrease which could be detected by a 50% increase in 99mTc-Annexin V uptake in both sensitive and drug-resistant cells [230].

## **Alternative imaging modalities**

#### *MRS/MRI*

Apart from radionuclide imaging, magnetic resonance spectroscopy (MRS) is currently the only clinically available method for non-invasive in vivo detection and quantification of apoptosis. The changes in lipid structure and fluidity of the cell membrane which take place during the apoptotic process generate a number of small molecules (e.g. cytoplasmic lipid bodies, choline metabolites) which can be directly monitored by watersuppressed lipid 1H MRS techniques. Several in vitro studies have reported on the appearance of mobile lipid signals in 1H NMR spectra of cells induced to undergo apoptosis by treatment with chemotherapeutic drugs or anti-Fas MoAbs [231–234]. Furthermore, Blankenberg et al. demonstrated that lipid 1H MRS allows direct quantification of the present fraction of apoptotic cells based on the increase in intensity of the hydrocarbon chains' methylene over methyl signals [235]. Nevertheless, a more recent in vivo study from Valonen et al. clearly indicated that apoptotic brain tumours derived from *HSV-tk*-transfected BT2C glioma cells did not show any increase in  $CH<sub>2</sub>/CH<sub>3</sub>$  signal but rather a late occurring decrease [233]. Thus, these preliminary findings on MRS need to be addressed with some scepticism and require further investigation.

Apart from lipid 1H MRS, apoptosis can also be detected indirectly by means of  $31P$  and  $13C$  MRS [236, 237]. In this case, the detection mode is based on the impaired high-energy phosphate metabolism typically associated with apoptotic cell death. Nevertheless, lipid proton spectroscopy offers several advantages over phosphorus MRS, which requires longer acquisition times while providing an inferior resolution. In general, MRS seems not to be very suitable for routine use in critically ill patients, and in vivo detection of apoptosis through MRS is significantly limited by relatively low sensitivity and poor temporal and spatial resolution [235, 238, 239]. In this regard, non-invasive radionuclide imaging of apoptosis should prove more useful than lipid proton nuclear MRS.

Since the morphological features associated with apoptosis (i.e. cell shrinkage and membrane blebbing) induce alterations in tissue water T2 and T1ρ relaxation times and apparent diffusion coefficient (ADC), magnetic resonance imaging (MRI) has also been investigated as an alternative technique for the in vivo detection of apoptosis [236, 240, 241]. In comparison with MRS techniques, 1H MRI provides a much better spatial and temporal resolution along with a very high sensitivity. However, the changes in MR image contrast based on cell shrinkage and membrane blebbing are unable to provide an early indication of the ongoing apoptosis since these morphological features occur quite late in the apoptotic process. At present, the most successful approach in MRI for in vivo detection of apoptosis uses the highly specific and tight binding of Annexin V or synaptotagmin I to externalised PS residues. Since the  $C_2$  domain of synaptotagmin I is known to bind to membranebound anionic phospholipids similar to Annexin V [242, 243], the protein was recently conjugated with superparamagnetic iron oxide nanoparticles (SPIO) and evaluated in vitro and in vivo in a murine EL4 lymphoma tumour model [244]. In a comparable way, cross-linked iron oxide nanoparticles (CLIO) were attached to Annexin V and tested in vitro [245]. In the case of the  $C_2$ -labelled SPIO particles, T2-weighted MRI images of tumour-bearing C57/B16 mice treated with cyclophosphamide/etoposide showed a significant and progressive decrease in tumour signal intensity compared with control animals. Tumour regions displaying the biggest MRI changes correlated well with areas containing the highest amount of apoptotic and necrotic cells. Similarly, T2 weighted imaging sequences of camptothecin-treated Jurkat T cells (i.e. 65% apoptotic cells) incubated with increasing concentrations of Annexin V-CLIO particles indicated a stronger, dose-dependent decrease in signal intensity versus untreated control cells (i.e. 12% apoptotic cells). Analogous control experiments with nonlabelled CLIO did not show a significant decline in T2 relaxation times for apoptotic and control cells in any concentration. Thus both described contrast agents seem to offer considerable potential for successful detection of apoptosis by MRI. Furthermore, Gd-DTPA has been used successfully to assess the transmural extent of myocardial necrosis in patients with previous myocardial infarction by means of contrast-enhanced MRI [246].

### *Optical/bioluminescence imaging*

In effort to develop a non-invasive optical imaging modality for in vivo detection of tumour apoptosis, Annexin V was recently conjugated with a near-infrared fluorochrome, cyanine-5.5 (Cy5.5) [247]. First in vivo data in irradiated MCA-29 tumour-bearing nude mice showed increased Cy5.5-Annexin V accumulation in tumours compared with untreated animals. Most interestingly, optical imaging allowed repeated acquisitions over a time course of 10 days owing to the high stability of the fluorochrome. Consequently, this approach could resolve many of the problems related to several apoptosis-detecting radioligands, including high cost, limited stability and a limited time window for consecutive apoptosis detection due to a short physical half-life. However, its biggest advantage is undoubtedly its capacity to monitor ongoing apoptosis in real time, which permits examination of the affected organs as the imaging procedure is proceeding, without requiring any additional signal processing. Such real-time examinations are particularly valuable when studying organs in motion, like the beating heart. Furthermore, real-time imaging of spontaneous

or therapy-induced apoptosis could facilitate and speed up clinical decision-making in many pathological conditions. Therefore, near-infrared fluorescence imaging with Cy5.5-Annexin V seems to offer a promising new tool for in vivo detection of apoptotic cell death.

Another approach in bioluminescence imaging (BLI) that has emerged recently consists in using firefly luciferase, which is known as a useful reporter gene in vivo, allowing non-invasive detection of tumour growth or efficacy of drug treatment. Mandl et al. used this technique to investigate the spatial relationship over time between chemotherapy-induced tumour apoptosis and total tumour burden assessed by BLI [248]. Micro-SPECT images of Balb/c mice bearing luciferase-tranfected BCL-1 lymphomas indicated a significant increase in 99mTc-Hynic-Annexin V starting 3 h after doxorubicin treatment and peaking at 5 h post therapy. As shown by BLI, the tumour cell number started to decrease around 9 h post therapy. Thus, the luciferase reporter gene approach seems to offer new perspectives for monitoring apoptosis-related cell loss in tumour therapy.

Complementary to radionuclide imaging, biotinlabelled and fluorescent Annexin V has been applied with success for ex vivo detection and confirmation of ongoing apoptosis in different animal models of myocardial and cerebral ischaemia [155, 249, 250], atherosclerosis [251] and organ development [252]. Unfortunately, visible light (including fluorescent light) is by convention unable to penetrate more than 1–2 mm into biological tissue, which makes contrast agents like biotinylated or FITC-Annexin V unsuitable for in vivo detection applications. Even strongly fluorescent probes have been reported to visualise tumours only up to a maximum depth of 2.2 mm [253]. In contrast, near-infrared light probes are able to detect lesions as deep as 1.5 cm from the tissue surface [254] and therefore seem better candidates for in vivo apoptosis detection in superficial tumours (e.g. of the head and neck or breast region). Dumont et al. successfully applied the strong fluorescent probe Annexin V-Oregon Green to image cardiomyocyte apoptosis at the single-cell level in murine hearts [255]. Although this method is capable of detecting apoptotic cell death in real time, the imaging procedure required opening of the chest, making it unsuitable for routine clinical application.

#### *Ultrasound imaging*

An alternative detection method that would also allow real-time monitoring of apoptosis is high-frequency (40–50 MHz) ultrasound imaging. Ultrasonic detection of apoptosis is based on the subcellular nuclear changes (e.g. chromatin condensation and DNA fragmentation) which cells undergo during the apoptotic process. These nuclear changes provoke a significant increase in the ultrasound backscatter amplitude in ultrasonograms of

apoptotic cell samples, which results in much brighter images. First evidence that ultrasound imaging is able to differentiate living cells from apoptotic or dead cells was provided by Czarnota et al. using an vitro model of cisplatin-induced acute myeloid leukemia AML-3 cells [256]. Twenty-four hours of cisplatin treatment induced apoptosis in 95% of the AML-3 cells, which corresponded with a two- to fivefold increase in the ultrasound backscatter signal of apoptotic vs living cells. Furthermore, the increase in the ultrasound signal showed a linear correlation with the progression of nuclear condensation and fragmentation [257]. Nevertheless, it remains very questionable whether this imaging technique would provide a significant detection signal in tumours or other pathological conditions, which express a much lower degree of ongoing apoptosis. Similar experiments in a rat model of cerebral and epidermal apoptosis induced by photodynamic therapy gave similar results. However, in these experiments ultrasonic detection was performed ex vivo or at the skin surface of the animals [257]. Hence, considering the low focal detection range in tissue (i.e. 9 mm), high-frequency ultrasound imaging seems less appropriate for successful in vivo imaging of apoptosis.

## **Conclusion**

As our knowledge of the molecular mechanisms involved in PCD is rapidly expanding, small pieces of this immense, complex puzzle are being revealed day by day. These discoveries will provide researchers with new insights into the phenomenon of apoptosis which will guide them in their quest to create novel markers and imaging techniques that will allow non-invasive detection of this process. When all the presented data are reviewed, several important conclusions can be drawn which should facilitate the design of new strategies in the development and evaluation of apoptosis-detecting radioligands.

There is a high demand for well-defined in vitro and in vivo cell death models that fully reflect the ongoing apoptosis present in a variety of human pathological conditions. In this regard, the localisation, extent and kinetics of the PCD process over time need to be determined and compared very carefully. Hence, meticulous translation of animal data to human models remains very important in the design of clinical trials focussed on apoptosis imaging. Secondly, extensive characterisation of the optimal time frame for imaging chemo- and radiotherapy-induced apoptosis and determination of the optimal radioligand biodistribution time are still required. Complementary techniques such as flow cytometry, immunohistological staining methods and the TUNEL assay remain critical to assess the amount of ongoing apoptosis accurately in order to confirm the specificity of the apoptotic signal provided by the isotopic detection methods. In this regard, highly specific apoptosis-detecting radioligands that are able to discriminate apoptosis from other types of cell death would prove most valuable.

Continued efforts in the identification of novel molecular targets involved in the apoptotic cascade could contribute to new strategies that would allow early detection of the process by means of specific cell death radioligands. Furthermore, new imaging modalities are being explored in addition to the currently used radionuclide techniques, which will enable physicians to monitor in vivo apoptosis in real time. Evidently, such techniques will greatly improve clinical decision-making in apoptosis-related diseases. Furthermore, the therapeutic (i.e. apoptosis inhibition) or toxic (i.e. apoptosis induction) effect of new drugs can be evaluated by means of specific apoptosis tracers. Such markers could also allow physicians to monitor the efficacy of anti-cancer treatment and to select responding from non-responding patients at an early stage of chemo- or radiotherapy.

Finally, novel drug delivery approaches that would allow or facilitate sufficient administration of apoptosis markers like radiolabelled Annexin V into the brain could lead to successful cell death detection and quantification in many neurological disorders. Consequently, this methodology could open new frontiers in the diagnostic imaging of stroke, Parkinson's disease and Alzheimer's disease and further elucidate the role of neurological cell death in these pathologies.

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