SCIENTIFIC ARTICLE

Quantitative assessment of anterior talofbular ligament quality in chronic lateral ankle instability using magnetic resonance imaging T2* value

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Abstract

Objective To determine T2^{*} normal reference values for anterior talofibular ligament (ATFL) and to investigate the feasibility of the quantitative ATFL quality evaluation in chronic lateral ankle instability (CLAI) using T2* values.

Materials and methods This study enrolled 15 patients with CLAI and 30 healthy volunteers. The entire ATFL T2* values from the MRI T2* mapping were measured. The prediction equation (variables: age, height, and weight) in a multiple linear regression model was used to calculate the T2* normal reference value in the healthy group. T2* ratio was defned as the ratio of the actual T2* value of the patient's ATFL to the normal reference value for each patient. A Telos device was used to measure the talar tilt angle (TTA) from the stress radiograph.

Results T2* values of ATFL in the healthy and CLAI groups were 10.82 ± 1.84 ms and 14.36 ± 4.30 ms, respectively, which are significantly higher in the CLAI group ($P < 0.05$). The prediction equation of the normal reference $T2^*$ value was [14.9] $+ 0.14 \times$ age (years) $- 4.7 \times$ height (m) $- 0.03 \times$ weight (kg)] ($R^2 = 0.65$, $P < 0.0001$). A significant positive correlation was found between the T2^{*} ratio and TTA ($r = 0.66$, $P = 0.007$).

Conclusion MRI T2* values in patients with CLAI were higher than those in healthy participants, and the T2* ratio correlated with TTA, suggesting that T2* values are promising for quantitative assessment of ATFL quality preoperatively.

Keywords Chronic lateral ankle instability · Anterior talofbular ligament · Quality · Magnetic resonance imaging · T2* value

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Introduction

An ankle sprain is one of the most frequent injuries during daily living and sports activities [\[1](#page-5-0), [2\]](#page-6-0), most commonly associated with anterior talofbular ligament (ATFL) injury. A common problem after ATFL injury includes chronic lateral ankle instability (CLAI), and surgery is indicated if conservative treatment fails. ATFL repair is the first-line CLAI surgical treatment when the residual ligament remains. Arthroscopic lateral ankle repair has been widely used to achieve good clinical results, such as providing stabilization, reducing postoperative pain, and facilitating early recovery [[3\]](#page-6-1). Michels et al. reported that the quality of the residual ligament infuences treatment outcome [[4\]](#page-6-2). Moreover, the previous study reported that a repair procedure against poor tissue quality in the ATFL remnant eventually required additional allograft reconstruction [\[5\]](#page-6-3). However, few studies have investigated a method of a preoperative quantitative ATFL quality assessment.

Magnetic resonance imaging (MRI) can provide a detailed morphological assessment of ligaments [\[6](#page-6-4)[–9](#page-6-5)] and has recently become available for quantitative assessment [\[10,](#page-6-6) [11](#page-6-7)]. T2* values refect the water content and collagen fiber content and orientation in the tissue $[12]$ $[12]$ $[12]$, which can quantitatively assess the ligament quality with shorter T2* relaxation times. The normal T2* value of the anterior cruciate ligament (ACL) is 11 to 19 ms [[13,](#page-6-9) [14](#page-6-10)], and the higher T2* value indicates the lower fascicle-specifc ACL surface in histomorphometry measurement [\[15](#page-6-11)] and increases anterior knee laxity [[14\]](#page-6-10).

Few studies have examined the T2* value of the ankle ligament. Surgeons appropriately may select the surgical procedure, such as ATFL repair or ATFL reconstruction if the ATFL quality can be assessed preoperatively using the T2* value, resulting in a better clinical outcome. Therefore, quantitative assessment is clinically important. This study aimed to determine T2* normal reference values for ATFL and investigate the feasibility of quantitative ATFL quality evaluation in CLAI using T2* values. We hypothesized that it would be possible to conduct a quantitative assessment of ATFL quality in CLAI using MRI T2* value. Furthermore, we also hypothesized that the MRI T2* values would be correlated with the anterior drawer distance as measured in patients.

Materials and methods

Patient cohort

The institutional review board of our hospital approved this study. This study enrolled 17 consecutive patients with CLAI and 30 healthy volunteers (16 males and 14 females; mean age, 39.8 ± 10.4 years [standard deviation]). The CLAI group consisted of patients who underwent surgery from November 2020 to November 2022, 3 months after ankle sprains, and those without ankle instability improvement after conservative treatment. The exclusion criteria include ankle osteoarthritis, rheumatoid arthritis, and incomplete MRI data. The fnal number of patients was 15 [6 males and 9 females; mean age, 34.7 ± 15.3 years (standard deviation)] based on these exclusion criteria. The healthy group consisted of participants with no history of sprain and no ankle pain during the MRI scan.

Imaging

All patients and healthy volunteers underwent 3.0-T MRI (Ingenia, Philips Healthcare, Netherlands) with a dStream FootAnkle 8ch coil consisting of structural three-dimensional (3D) T2-weighted images (repetition time/echo time = 1400/ 62 ms, voxel size = $0.5 \times 0.5 \times 0.6$ mm³) along with T2* map images in a neutral ankle position. The high-resolution T2* map image (multi-echo–Fast Field echo sequence) parameters were as follows: repetition time = 32 ms ; echo time = $2.3, 4.6, 6.9, 9.2, 11.5, 13.8$, and 16.1 ms; flip angle = 13° ; and voxel size = $0.6 \times 0.6 \times$ 0.6 mm³; compressed sensing acceleration factor = 4.6. The acquisition time was 5 min 4 s.

Imaging analysis

The entire ATFL of each ankle was manually segmented from the T2* map images using Ziostation2 (ZIOSOFT Inc., Tokyo, Japan) with reference to the 3D T2-weighted images by an MRI researcher with adequate ankle anatomy knowledge (Fig. [1](#page-2-0)). In this case, three planes were used for the identifcation and segmentation of the ATFL.

The T2* value of each ATFL was determined as the median value from these segmented pixels. Additionally, another MRI researcher performed image analysis to assess measurement interobserver variability. The prediction equation (variables: age, height, weight) in a multiple linear regression model calculated the T2* normal reference value in the healthy group. T2* ratio was defned as the ratio of the actual T2* value of the patient's ATFL to the normal reference value of ATFL obtained by substituting the patient's age, height, and weight into the prediction equation. Additionally, the MRI fndings on T2-weighted image were evaluated for the ATFL morphological characteristics classifed into the following categories: normal, wavy, thin, and thickened ATFL [\[16](#page-6-12)].

A Telos device was used to measure the talar tilt angle (TTA) and anterior drawer distance (ADD) from the stress radiograph in the CLAI group. Anterior translation (AT) was measured by a manual test using a capacitance-type strain sensor [\[17](#page-6-13)] in the healthy group and the CLAI group. All patients with CLAI underwent arthroscopic ATFL repair after an MRI examination [[18](#page-6-14)]. The ATFL tension (taut, mild laxity, and laxity) and quality (excellent, moderate, and poor) were evaluated from arthroscopic fndings by two foot and ankle orthopedic surgeons [[19](#page-6-15)].

Statistical analysis

All statistical analyses were performed using JMP 17.0 software (SAS Institute, Cary, NC, USA). The chi-squared test and Mann–Whitney *U* test for categorical and continuous variables, respectively, were used to evaluate the differences between the two groups. Accuracy was tested by analyzing the interinvestigator intraclass correlation coefficient (ICC) of the $T2*$ values, and the measured values were rated as follows: <0.50 (considered poor), 0.50 to Skeletal Radiology (2024) 53:733–739 735

Fig. 1 a Fusion oblique axial image of 3D T2-weighted image and T2* map image; **b**, **c**, **d** T2* map reconstructed images: oblique axial image, oblique coronal image, and oblique sagittal image. Red regions show the anterior talofbular ligament

0.75 (moderate), 0.75 to 0.90 (good), and >0.90 (excellent). First-order multiple linear regression analyses, with the T2* value as a dependent variable and age, height, and weight as independent variables, were used to determine the best-ft parameters and evaluate the relationship between the T2* value and age, height, or weight. The $R²$ values were reported as indicators of the relationship strength and goodness of ft, and the measured values were rated as follows: 0 to 0.25 (weak), 0.26 to 0.50 (moderate), and 0.51 to 1.00 (substantial) [[20](#page-6-16)]. Spearman correlation coefficients were used to investigate the correlation of the T2* value or T2* ratio and the TTA, ADD, or AT. The Kruskal–Wallis test was used to test the statistical signifcance of T2* values between arthroscopic fndings. *P* values less than 5% were considered statistically signifcant.

A prior power analysis (α error: 0.05, 1-β error: 0.85, number of predictors: 3, sample size: 29) was performed using the G*power program (version 3.1.9.6) to calculate the sample size for the healthy group. Additionally, post hoc analysis for correlation T2* ratio and TTA revealed that a sample size of 15 would achieve 88% power. A power level of more than 80% was considered sufficient. Thus, we determined that our study included a sufficient sample size.

Results

There were no signal changes of the ATFL on T2-weighted images in all healthy volunteers. T2* values of ATFL in the healthy and CLAI groups were 10.82 ± 1.84 ms (range, 7.54–14.09 ms) and 14.05 ± 4.60 ms, respectively, and were significantly higher in the CLAI group ($P = 0.0284$) (Table [1](#page-2-1)). The ICC index for the interobserver reliability of the T2* value between the two investigators was 0.94 (95% confdence interval: 0.83–0.99), indicating excellent

Table 1 T2* values and characteristics of healthy volunteers and patients with chronic lateral ankle instability (CLAI)

interobserver reliability. Multiple regression analysis revealed that the T2* value was predicted by age, height, and weight $(R^2 = 0.65, P < 0.0001)$ (Fig. [2](#page-3-0)). The prediction equation of the T2* normal reference value is shown as follows: T2* value (ms) = 14.9 + 0.14 × age (years) – 4.7 × height (m) $-0.03 \times$ weight (kg). The variance inflation factor (VIF) of each variable was 1.3 for age, 1.9 for height, and 2.2 for weight, indicating no problematic level of collinearity as the VIF was less than 10 $[21]$ $[21]$. Age showed significantly high positive [[22\]](#page-6-18) correlations with T2* value ($r = 0.72$, $P =$ 0.001). Also, R^2 was 0.51 in the parsimonious model where age was the only predictor variable $(P < 0.0001)$.

The mean AT of the healthy subjects was 3.8 ± 1.4 mm. The mean TTA, ADD, and AT were $13.1^\circ \pm 4.6^\circ$, 7.7 ± 1.9 mm, and 8.9 ± 3.0 mm, respectively, in the CLAI group. A signifcant positive correlation was found between the T2* ratio and TTA ($r = 0.66$, $P = 0.007$) and between the T2^{*} value and ADD ($r = 0.57$, $P = 0.033$) (Table [2\)](#page-3-1) (Fig. [3\)](#page-3-2). The T2* value for each morphologic fnding were 9.61 ms for normal thick without wavy contour in $1 (6.7\%)$, 13.80 ± 3.95

Fig. 2 Predicted normal reference $T2^*$ value versus actual $T2^*$ value $T2^$ using a multiple regression model as a function of the linear combination of age, height, and weight

Fig. 3 Relationship between Talar tilt angle and T2* ratio

ms for normal thick with wavy contour in 2 (13.3%), 13.58 \pm 4.21 ms for thickened ATFL in 6 (40%), and 18.18 \pm 8.87 ms for thin ATFL in $2(13.3\%)$ (Figs. [4](#page-4-0), [5](#page-4-1), and [6](#page-4-2)). There was no relationship between morphologic characteristics and T2* values. Arthroscopic fndings included ATFL tension (taut: 0, mild laxity: 10 cases, laxity: 5 cases) and quality (excellent: 3 cases, moderate: 8 cases, poor: 4 cases). A trend toward higher T2* values as the intraoperative fndings progressed from mild laxity to laxity, from excellent to poor, or from moderate to poor. No signifcant diferences were found between T2* values and intraoperative arthroscopic findings (Table [3\)](#page-5-1).

Discussion

To our best knowledge, this is the frst report related to the quantitative evaluation of ATFL using MRI T2* values. The most important fnding in this study was that the T2* ratio revealed a signifcant positive correlation with the TTA of

Table 2 Instability measurements and correlation coefficient with T2* value or T2* ratio

Abbreviation: *SD*, standard deviation; *CC*, correlation coefficient; *TTA*, talar tilt angle; *ADD*, anterior drawer distance; *AT*, anterior translation

ACL, posterior cruciate ligament, and patella tendon differ in collagen content and collagen fber orientation [\[23,](#page-6-19) [24](#page-6-20)], as refected by T2* values [\[25\]](#page-6-21). Previous prospective studies have shown longitudinal changes in graft maturation after ACL reconstruction using $T2^*$ values $[26, 27]$ $[26, 27]$ $[26, 27]$ $[26, 27]$ $[26, 27]$.

Additionally, direct measurement of T2* values of the ACL helped determine the elastic modulus [\[15](#page-6-11)] and the difference in anterior knee laxity in clinical practice [[14](#page-6-10)].

This study revealed that the T2* value of ATFL has a signifcant positive correlation with age in healthy groups.

Fig. 6 3D T2-weighted image

Fig. 5 3D T2-weighted image (**a**) and T2* map fusion image (**b**) in a 39-year-old man with CLAI. The T2-weighted image showed a thin ATFL and synovitis (arrow). The T2* value was 11.0ms. The normal reference T2* value for this patient was calculated to be 9.2 ms. Therefore, the T2* ratio was 1.2

(**a**) and T2* map fusion image (**b**) in a 25-year-old woman with CLAI. The T2-weighted image showed a thickened ATFL. The T2* value was 11.0ms. The normal reference T2* value for this patient was calculated to be 9.2 ms. Therefore, the T2* ratio was 1.2

Fig. 4 3D T2-weighted image (**a**) and T2* map fusion image (**b**) in a 37-year-old woman with CLAI. The T2-weighted image showed a normal thickness ATFL. The T2* value was 16.2 ms. The normal reference T2* value for this patient was calculated to be 10.0 ms. Therefore, the T2* ratio was 1.6

	ATFL tension			ATFL quality			
	Mild laxity	Laxity	Statistical analysis	Excellent	Moderate	Poor	Statistical analysis
N	10		$\overline{}$				-
$T2^*$ value, ms	13.28 ± 3.76	15.58 ± 6.16	- NS	13.24 ± 5.56	12.83 ± 3.32 17.07 ± 5.98		NS

Table 3 Comparison of T2* values and ATFL tension or ATTL quality in arthroscopic fndings

Values are expressed as means \pm standard deviation.

Abbreviation: ATFL, anterior talofibular ligament; *NS*, no significant differences.

A high percentage of age-related ACL histopathologic abnormalities had collagen fber disorientation [\[28\]](#page-6-24). Furthermore, higher T2* values refect collagen fber disorientation $[29]$. Therefore, the increase in T2 $*$ values with age may indicate degenerative changes in ankle ligaments. This study derived a substantial equation using age as a variable to calculate a normal reference value.

CLAI is a condition that is primarily characterized by insuffcient ATFL. Instability assessment using stress radiographs has been performed. Hashimoto et al. reported that the condition of the injured ligaments in patients with a TTA of more than 15° had almost avulsed and degenerated or completely absent injured ligaments [\[30](#page-6-26)]. However, stress radiographs have not directly assessed ATFL insufficiency. MRI T2* map images allowed a direct ATFL assessment. A signifcant correlation between TTA and the T2* ratios was found in the CLAI group. Therefore, the T2* value may provide a more robust ATFL insufficiency assessment. Additionally, a higher T2* value indicates a combination of less densely packed collagen fbrils, periligamentous scar tissue [[31](#page-6-27)], and a histological lower score [\[32\]](#page-6-28). No statistically signifcant diference was found in the arthroscopic fnding evaluation, but lower ATFL tension and quality revealed higher T2* values. The current fndings reported revealed ATFL quality can be objectively and quantitatively assessed preoperatively. Because there was a wide range of T2* value (7.54–14.09 ms) in the healthy group, the ATFL assessment of the CLAI patients using the pure $T2^*$ seemed to be difficult. Therefore, the use of $T2^*$ ratio should be considered for the assessment of ATFL quality in clinical practice.

Recently, ATFL arthroscopic is often performed, which is less invasive than open repair or reconstruction, and good clinical outcomes have been reported. Arthroscopic repair procedure also has the advantage of a shorter rehabilitation period [\[33](#page-6-29)]; therefore, surgical technique selection for arthroscopic repair, open repair, or reconstruction is important. Future work will need to investigate the relationship between time-dependent changes in T2* and the postoperative outcome with more participants to determine the cut-off value for surgical procedures.

This study has several limitations. First, the sample size in the CLAI group was small. Further investigations should be performed in a larger sample size when more patient data are available. Second, ATFL tissue samples were impossible to evaluate because all surgical procedures included a repair; therefore, the actual ATFL quality, such as collagen content and orientation is unknown. A histological evaluation may be possible in the case of ATFL reconstruction, but it also suffers from subject bias. Third, an arthroscopic evaluation of the entire ATFL is difficult to perform due to the limited field of view of arthroscopy, while MRI allows T2* value measurement for total ATFL. Forth, the T2* values may also difer for diferent vendors or diferent magnetic feld strength, and T2* values should probably be locally verifed for each center. Finally, the relationship between T2* value and clinical results is unclear. The clinical score and preoperative outcome should be investigated. However, to our best knowledge, the present study frst demonstrated measuring the T2* value of ATFL. Furthermore, the T2* ratio, defned as the ratio of normal calculation from the prediction equation, was correlated with TTA.

In conclusion, MRI T2* values in patients with CLAI were higher than those in healthy participants, and the $T2^*$ ratio correlated with TTA, suggesting that T2* values are promising for quantitative ATFL quality assessment preoperatively.

Data Availability The data that support the fndings of this study are available from the corresponding author, AT, upon reasonable request.

Declarations

Ethical approval Ethical approval for this study was obtained from the institutional review board in Sapporo Medical University Hospital (reference no: 322-250).

Informed consent Informed consent was obtained from all individual participants included in the study.

Conflict of interest The authors declare no competing interests.

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