METHODS AND PROTOCOLS



Multiple amplification-based fluorometric aptasensor for highly sensitive detection of *Staphylococcus aureus*

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Abstract

Rapid and accurate detection and identification of *Staphylococcus aureus* (*S. aureus*) are of great significance for food safety, environmental monitoring, early clinical diagnosis, and prevention of the spread of drug-resistant bacteria. Herein, we design a fluorometric aptasensor for ultra-sensitive, specific, and rapid detection of *S. aureus*. The apasensor combines the enrichment and separation of magnetic nanoparticles (MNPs), the biotin-streptavidin conjugation system, and a single *S. aureus* can release four signaling probes for signal amplification. Aptamer acts as a specific biorecognition element of *S. aureus*. Four FAM-labeled partially complementary sequences (FAM-pcDNAs) were used as signaling probes. The aptamers were sequential hybridized with the four FAM-pcDNAs to form aptamer&pcDNAs, which were then bound to MNPs via the biotin-streptavidin. When the aptamer specifically recognizes and binds to *S. aureus*, the FAM-pcDNAs signaling probes are replaced and released into the supernatant. The concentration of *S. aureus* can be quantified by measuring the fluorescence intensity ($\lambda exc/em = 492/520$ nm) of the replaced signaling probe FAM-pcDNAs. The results show that the proposed fluorometric aptasensor displays good specificity, ultra-high sensitivity (1.23 cfu/mL), wide linear range (1 ~ 10⁸ cfu/mL), and fast detection speed (~ 1.5 h). The recovery test verifies further that the proposed fluorometric aptasensor can detect *S. aureus* in spiked blood samples. Since aptamers are easy to customize, we believe that fluorometric aptasensors based on multiple amplification of practical high-performance biosensors for bacterial detection.

Key points

- Multiple amplification-based fluorometric aptasensor for S. aureus is developed
- The aptasensor displays high specificity with a LOD of 1.23 CFU/mL
- The aptasensor can directly detect S. aureus in spiked blood samples

Keywords Aptasensor · Amplification · Fluorometric detection · S. aureus

Introduction

S. aureus is one of the most pathogenic pathogens in the world, and was first discovered and named by Dr. Alexander Ogston in 1880 (Ogston 1882). *S. aureus* naturally exists in

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water, sewage, air, environmental surfaces, and food (Lian et al. 2015), and produces one or more staphylococcal enterotoxins (SE), such as SEA, SEB, and SEC, etc (Principato and Qian 2014), which are the main causes of food-borne poisoning (Hulme 2017). *S. aureus* is also the most common pathogen which can cause skin and soft tissue infections (impetigo, folliculitis, and scalded skin syndrome), pneumonia, endocarditis, osteomyelitis, pseudomembranous enteritis, and even serious systemic infections such as bacteremia, sepsis and toxic shock syndrome (Tong et al. 2015). In recent years, methicillin-resistant *S. aureus* (*MRSA*) has posed a serious threat to global public health and the infection rate of *MRSA* remains high in developed countries ($40 \sim 60\%$) as well as developing countries (>70%) (Chen and Huang 2014; Fluit et al. 2001).





S. aureus has become a pathogen that seriously endangers global public health. Therefore, rapid and accurate detection and identification of S. aureus are of great significance to food safety, environmental monitoring, early clinical diagnosis, and prevention of the spread of drug-resistant bacteria. The gold standard for detecting S. aureus is still cultivation and identification, the results are accurate and reliable, economical and simple, but it is very time-consuming, usually taking $1 \sim 2$ days to form visible colonies on agar plates, and then $1 \sim 2$ days for biochemical identification and serological typing. There are many newly developed rapid and automated detection methods in recent years, such as enzyme-linked immunosorbent assay (ELISA) (Nouri et al. 2018), polymerase chain reaction (PCR) (Umesha and Manukumar 2018), next-generation sequencing, and matrixassisted laser desorption/ionization time-of-flight mass spectrometry (MALDI-TOF-MS) (Gill et al. 2019; Rajapaksha et al. 2019), etc., which require only $1 \sim 5$ h. However, these methods require expensive instruments, complicated sample preparation, and extensive experience, and most experiments also require culture enrichment and isolation to improve the detection sensitivity, thereby greatly extending the detection time. Therefore, it is still challenging to develop a rapid, specific, and ultra-sensitive detection method for S. aureus.

Aptamer technology has shown its promising application in the fields of medicine and life sciences since the RNAtype oligonucleotide aptamers were screened from a library containing approximately 10¹⁵ oligonucleotide molecules by Systematic Evolution of Ligands exponential enrichment (SELEX) (Ellington and Szostak 1990; Tuerk and Gold 1990). Aptamers are a specific oligonucleotide sequences (most commonly single-stranded DNA or RNA), usually ranging in length from 25 to 90 bases, and their binding to the target is based on the diversity of single-stranded nucleic acid structure and spatial conformation (Tok et al. 2000). Aptamers can not only bind to the corresponding ligand with strong affinity (the affinity dissociation constants are generally 1 pM ~ 1 mM) and high specificity similar to antibodies, but also have many advantages compared to antibodies, such as small molecular weight, low synthesis cost, easy of modification, wide selection of ligands (small molecules, ions, proteins, and even cells), no immunogenicity, and a higher specificity, stability, and reproducibility (Labib et al. 2016; Liu et al. 2021a; Moutsiopoulou et al. 2019).

In recent years, biosensors based on aptamers as specific biorecognition elements have been widely used for efficient and rapid identification of pathogens, and have been proposed as the most attractive alternatives for the traditional detection of pathogens (Cesewski and Johnson 2020; Furst and Francis 2019). Fluorometric aptasensor is one of the most commonly used biosensors, with high sensitivity, wide linear range, and fast detection, and has been widely used for pathogen detection (Chen et al. 2022). In this research, we have fabricated a fluorometric aptasensor for ultra-sensitive, specific, and rapid detection of S. aureus. The apasensor combines the enrichment and separation of magnetic nanoparticles (MNPs), the biotinstreptavidin conjugation system, and a single S. aureus can release four signaling probes for signal amplification. As shown in the Scheme 1, biotin-aptamer acts as a specific biorecognition element of S. aureus and forms a hybrid sequence (aptamer&pcDNAs) with four partially complementary sequences (FAM-pcDNAs) through base pairing. Aptamer&pcDNAs immobilize on the streptavidin-MNPs to form aptamer&pcDNAs@MNPs as detection probe due to the strong affinity interaction between biotin-streptavidin. When S. aureus is present in the sample, the aptamer can specifically recognize and binds to S. aureus, and the FAMpcDNAs signaling probes are replaced and released into the supernatant. The concentration of S. aureus in the sample can be quantified by measuring the fluorescence intensity $(\lambda exc/em = 492/520 \text{ nm})$ of the replaced signaling probe FAM-pcDNAs.

Materials and methods

Bacteria and reagents

S. aureus ATCC25923, Staphylococcus epidermidis ATC12228 (S. epidermidis), Klebsiella pneumoniae ATCC 700603 (K. pneumoniae), Acinetobacter baumannii ATCC 19606 (A. baumannii), Pseudomonas aeruginosa ATCC 27853 (P. aeruginosa), Escherichia coli ATCC 25922 (E. coli), Enterococcus faecium ATCC 29212 (E. faecium), Proteus mirabilis ATCC 12453 (P. mirabilis), Streptococcus pyogenes ATCC 19615 (S. pyogenes), and Streptococcus pneumoniae ATCC 49619 (S. pneumoniae) were obtained from the Xiangya Hospital of Central South University. From a pure culture, a single colony was selected for bacterial enrichment and different concentrations of bacteria were prepared with Tris–HCl (10 mM, pH 7.4). The standard plate count method was used to count the bacteria.

Streptavidin-MNP_S (50 mg/mL), LB broth medium, Tris–HCl, PBS, agarose, 4S Red Plus nucleic acid stain, running buffer, loading buffer, and rabbit whole blood were purchased from Shanghai Sangon Biological Engineering Technology and Services. The aptamer sequence, partially complementary sequence (pcDNA), and fully complementary sequence (fcDNA) required in this article are shown in Table 1, which were synthesized by Shanghai Sangon Biological Engineering Technology and Services. Washing buffer (10 mM Tris–HCl, with 2 M NaCl, 1 mM EDTA, pH 7.4), blocking buffer (0.1 M NaCl, 0.1 M PBS, 0.05% Tween-20, pH 7.4), and hybridization buffer (10 mM Tris–HCl, with 150 mM NaCl, 5 mM KCl, 2 mM MgCl₂, 1 mM CaCl₂, pH 7.4) were prepared according to the literature (Shi et al. 2019).

Preparation of the aptamer&pcDNAs

Add 100 μ L of different concentrations (2 μ M, 4 μ M, 6 μ M, 8 μ M, 10 μ M) of FAM-pcDNA1, FAM-pcDNA2, FAM-pcDNA3, and FAM-pcDNA4 to 100 μ L of biotin aptamer (5 μ M). Heat at 95 °C for 5 min to denature the *S. aureus* aptamer (Mazzaracchio et al. 2019), and then cool down naturally at room temperature in the dark with shaking (110 r/min) for hybridization. Twenty microliters of each sample were loaded on agarose gel (4%) and electrophoresis was performed at a constant potential of 120 V for 20 min. The gel was photographed, and the gray-scale of the DNA electrophoresis bands on the gel image was analyzed by gel imaging analysis software, thereby semi-quantitative analysis of the DNA content.

Preparation of aptamer&pcDNAs@MNPs

Streptavidin-MNP_S was washed three times with washing buffer and resuspended in hybridization buffer. Next, 200 μ L aptamer&pcDNAs (1 μ M) were added and incubated with 200 μ L streptavidin-MNP_S (0 mg/mL, 0.25 mg/mL, 0.5 mg/ mL, 1 mg/mL, 2 mg/mL, 4 mg/mL, 8 mg/mL, 16 mg/mL) at 37°C for 30 min in the dark under shaking (110 r/min) to generate aptamer&pcDNAs@MNP_S detection probe.

 Table 1
 The sequences of the used oligonucleotides

Name	Sequence (5'-3')		
Aptamer	Biotin-(CH2)6-GCAATGGTACGGTACTTCCTCGGCACGTTCTCAGTAG		
	CGCTCGCTGGTCATCCCACAGCTACGTCAAAAGTGCACGCTACTT		
	TGCTAA(Cao et al. 2009)		
pcDNA1	CGAGGAAGTACCGTACCATTGC-(CH ₂) ₆ -FAM	58.12 °C	
pcDNA2	GCGAGCGCTACTGAGAACGTGC-(CH2)6-FAM	64.08 °C	
pcDNA3	TGACGTAGCTGTGGGATGACCA-(CH ₂) ₆ -FAM	60.71 °C	
pcDNA4	TTAGCAAAGTAGCGTGCACTTT-(CH2)6-FAM	54.58 °C	
fcDNA	TTAGCAAAGTAGCGTGCACTTTTGACGTAGCTGTGGGATGACCAG	78.0 °C	
	CGAGCGCTACTGAGAACGTGCCGAGGAAGTACCGTACCATTGC		
	-(CH ₂) ₆ -FAM		

The aptamer&pcDNAs@MNP_S was further washed twice with 400 μ L washing buffer until no DNA was detected in the discarded solution. The fluorescence intensity (λ exc/ em=492/520 nm) in all isolated supernatants were measured to estimate the content of unbound aptamer&pcDNAs. Aptamer&pcDNAs@MNP_S were then resuspended in blocking buffer (37 °C, 30 min) to block the exposed unbound sites of the streptavidin-MNP_S. Prior to use, the aptamer&pcDNAs@MNP_S were resuspended in hybridization buffer and stored at 4 °C in the dark.

Procedure for S. aureus detection

First, *S. aureus* sample (300 μ L) was added to 300 μ L aptamer&pcDNAs@MNP_S probe solution, and co-incubated in the dark under shaking (110 r/min). After magnetic separation, centrifuge was performed to separate unbound *S. aureus* from FAM-pcDNAs in the detection solution. Finally, FAM-pcDNAs in the supernatant were transferred to Hitachi F4500 matching cuvette to measure its fluorescence intensity (λ exc/em = 492/520 nm).

Results

Preparation of aptamer&pcDNAs

Agarose gel electrophoresis was performed to prove the occurrence of the hybridization of biotin-aptamer with four

Fig. 1 a Agarose gel electrophoresis of aptamer (20 µL, 2 µM), pcDNAs (20 µL, 2 µM), and aptamer&pcDNAs (20 µL, 10 µM aptamer + 10 µM of each of the four pcDNA); **b** the gray value of aptamer&pcDNAs after different concentrations of pcD-NAs (2 µM, 4 µM, 6 µM, 8 µM, 10 µM) incubated with aptamer $(5 \mu M)$. The concentrations ratio of pcDNAs to aptamer was 0.4, 0.8, 1.2, 1.6, 2.0; c the typical UV-Vis absorption curves of the Tris- HCl (Blank), aptamer&pcDNAs, MPNs, and aptamer&pcDNAs@MPN_s; **d** the fluorescence intensity of all separated solution after aptamer&pcDNAs incubated (37 °C, 30 min) with different concentrations of streptavidin-MNPs (0 mg/mL,0.25 mg/ mL,0.5 mg/mL, 1 mg/mL, 2 mg/mL, 4 mg/mL, 8 mg/mL, 16 mg/mL). Error bars indicate standard deviation (n=3)

partially complementary sequences (FAM-pcDNAs). As can be seen in Fig. 1a, lanes 1, 3, and 5 represent aptamer, FAM-pcDNAs, and aptamer&pcDNAs, respectively. The lane 5 has a light band, and the size of the light band is larger than that of the aptamer and the partially complementary sequences (FAM-pcDNAs), indicating that the aptamer&pcDNAs hybrid sequence was successfully prepared. The size of aptamer&pcDNAs in agarose gel (about 200 bp) is larger than the size of one aptamer (88 bases) plus four partially complementary sequences (22 bases), which may be because the modification of $-(CH_2)_6$ -FAM on the pcDNAs affect the charge, molecular size, and shape in the aptamer&pcDNAs.

We tried to optimize the concentration ratio (0.4, 0.8, 1.2, 1.6, 2.0) between the FAM-pcDNAs (2 μ M, 4 μ M, 6 μ M, 8 μ M, 10 μ M) and biotin-aptamer (5 μ M) to improve hybridization efficiency. As shown in Fig. 1b, the gray-scale of aptamer&pcDNAs increased with the increase of concentration ratio of FAM-pcDNAs to biotin-aptamer from 0.4 to 2.0. When the concentration ratio of FAM-pcDNAs to biotin-aptamer increased up to 1.2, the gray value increased insignificantly. Therefore, the optimal concentration ratio of FAM-pcDNAs to biotin-aptamer is 1.2, and it will be used for subsequent experiments.

Preparation of aptamer&pcDNAs@MNPs

UV-Vis absorption spectroscopy analysis was performed to confirm the formation of the detection probe



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aptamer&pcDNAs@MNP_S. As shown in Fig. 1c, Tris–HCl (Blank) has no absorption peak, while streptavidin-MNP_S has an absorption peak at 206 nm, and the baseline is increased, which may be attributed to streptavidin and MNP_S respectively. Two absorption peaks were observed at 206 nm and 260 nm for aptamer&pcDNAs, which were characteristic absorption peaks of biotin and DNA respectively. The baseline induced by streptavidin-MNP_S also increased, providing evidence for the successful preparation of aptamer&pcDNAs@MNP_s.

We tried to optimize the concentration of streptavidin-MNP_S (0 mg/mL, 0.25 mg/mL, 0.5 mg/mL, 1 mg/mL, 2 mg/ mL, 4 mg/mL, 8 mg/mL, 16 mg/mL) to improve combining efficiency. As shown in Fig. 1d, the fluorescence intensity in the separated solution after aptamer&pcDNAs incubated with streptavidin-MNP_S decreased with the increase of concentration of streptavidin-MNP_S from 0.25 mg/mL to 16 mg/ mL. When the concentration of streptavidin-MNP_S was increased up to 8 mg/mL, the fluorescence intensity in the separated solution decreased insignificantly, indicating that almost all aptamer&pcDNAs in solution have been bound to the streptavidin-MNP_S. Therefore, the optimal concentration of streptavidin-MNP_S was 8 mg/mL, and it was used for subsequent experiments. According to the standard curve established by fluorescence intensity (λ exc/em = 492/520 nm) and aptamer&pcDNAs concentration, it can be calculated that about 21.27 pmol (11.50 µg) of aptamer&pcDNAs bind to 1 mg of streptavidin-MNP_S when the streptavidin-MNP_S concentration is 8 mg/mL.

Characterization of streptavidin-MNP_s and aptamer&pcDNAs@MNP_s

The streptavidin-MNP_S and aptamer&pcDNAs@MNP_S were characterized by FTIR, XPS spectra, and zeta potential to further confirm the successful assembly of aptamer&pcDNAs@ MNP_S. As shown in Fig. 2a, the main characteristic FTIR adsorption peaks of streptavidin-MNP_S are 3229 cm⁻¹ and

Fig. 2 a FT-IR spectra of MPN_S and aptamer&pcDNAs@MPN_S; b the narrow-scan C1s XPS of MPN_S and aptamer&pcDNAs@ MPN_S; c The narrow-scan N1s XPS of MPN_S and aptamer&pcDNAs@MPN_S; d the narrow-scan O1s XPS of MPN_S and aptamer&pcDNAs@ MPN_S; e the narrow-scan P2p XPS of MPN_S and aptamer&pcDNAs@MPN_S; f the zeta potential of MPN_S and aptamer&pcDNAs@MPN_S



3189 cm⁻¹ (stretching vibration of O–H and N–H), 2987 cm⁻¹ (stretching vibration of C–H), and 2600 cm⁻¹ (stretching vibration of S–H), 1630 cm⁻¹, 1551 cm⁻¹, and 1460 cm⁻¹ (skeleton vibration of benzene ring), 1403 cm⁻¹ (deformation vibration of -CH3), 1296 cm⁻¹ (deformation vibration of N–H), 1135 cm⁻¹ and 910 cm⁻¹ (stretching vibration of C–O–C), 1035 cm⁻¹ (stretching vibration of C–O–C), 1035 cm⁻¹ (stretching vibration of C–O–C), 1035 cm⁻¹ (stretching vibration of C–O), 664 cm⁻¹ (deformation vibration of C–H), and 581 cm⁻¹ and 468 cm⁻¹ (vibration of Fe–O). After the aptamer&pcDNAs immobilized on streptavidin-MNP_S, the new characteristic adsorption peaks 1180 cm⁻¹ (stretching vibrations of C–O and P-O-C which mainly in nucleic acids) and 1730 cm⁻¹ (stretching vibration of C=O which mainly in A/T/C/G base cyclic ketone) are observed, indicating the successful assembly of aptamer&pcDNAs@MNP_S.

The chemical composition and states of the chemical elements of streptavidin-MNP_S and aptamer&pcDNAs@ MNP_S were analyzed by XPS. We can clearly see the abundant C–O–C, C-O–H (Fig. 2b), and N–H (Fig. 2c) in the aptamer&pcDNAs@MNP_S, which are almost absent in streptavidin-MNP_S, indicating that the aptamer&pcDNAs@

MNP_S were assembled successfully. Similarly, we can see that the main form of O1s in aptamer&pcDNAs@MNP_S are O-C, O=C, and O–H, which are different from O-Fe in streptavidin-MNP_S as (Fig. 2d). What is more, there was a peak at 133.2 eV only for aptamer&pcDNAs@MNP_S not for streptavidin-MNP_S in the narrow-scan P2p XPS (Fig. 2e), which could be attributed to the phosphate skeleton in nucleic acids, further indicating the successful assembly of aptamer&pcDNAs@MNP_S. As shown in Fig. 2f, the zeta potential of Streptavidin-MNP_S is about – 26.87 mV, while the zeta potential of aptamer&pcDNAs@MNP_S is – 27.57 mV under the same pH condition. This is because the nucleic acid is negatively charged and could make the zeta potential of aptamer&pcDNAs@MNP_S more negative.

Optimization of experimental parameters for S. *aureus* detection

The incubation temperature (4 °C, 25 °C, 37 °C) and time (30 min, 60 min, 120 min) of aptamer&pcDNAs@MNP_S

Fig. 3 a Optimization of incubation temperature (4 °C, 25 °C, 37 °C) between the aptamer&pcDNAs@ MPNs and S. aureus for 120 min; b optimization of incubation time (30 min, 60 min, 120 min) between the aptamer&pcDNAs@MPNs and S. aureus at 37 °C; c, d, e, f the fluorescence emission spectra of the detection supernatant contained signaling probe after aptamer&cDNA@MPNs incubation (37 °C, 60 min) with different concentrations of S. aureus (10¹ cfu/mL, 10⁴ cfu/ mL, 10^7 cfu/mL): c only one FAM-fcDNA signaling probe, d two FAM-pcDNAs signaling probes, e three FAM-pcDNAs signaling probes, f four FAMpcDNAs signaling probes



with *S. aureus* are the critical experimental parameters that should be optimized to enhance the performance of the aptasensor. As shown in Fig. 3a, the fluorescence intensity of the detection solution increased with the increase of incubation temperature from 4 to 37 °C for 120 min. Therefore, 37 °C was the optimal temperature for the incubation of aptamer&pcDNAs@MPN_S with *S. aureus* and used for subsequent experiments. As shown in Fig. 3b, the fluorescence intensity of the detection solution increased with the increase of incubation time from 30 to 120 min at 37 °C. The fluorescence intensity increased insignificantly as the incubation time between the aptamer&pcDNAs@MPN_S and *S. aureus* was determined to be 60 min, and it was used for subsequent experiments.

Then, we compared the performance of four FAMpcDNAs signaling probes with one FAM-fcDNA signaling probes, two FAM-pcDNAs signaling probes, and three FAM-pcDNAs signaling probes. As shown in Fig. 3c, when one FAM-fcDNA signaling probes were used to react with low (10^1 cfu/mL), medium (10^4 cfu/mL), and high (10^7 cfu/mL) concentrations of *S. aureus*, the relatively low fluorescence intensities were obtained (51.19, 183.52, 747.85, respectively). The fluorescence intensity enhanced with the increase of FAM-pcDNAs bound on the signaling probe. When using the four FAM-pcDNA_S signaling probes, the corresponding fluorescence intensities were enhanced about twofold, reaching to 148.55, 596.81, and 2342.73, respectively, indicating that this strategy can be used to improve the detection sensitivity.

The morphology of aptamer&*S. aureus*@MNP_S was observed by scanning electron microscopy (SEM) to verify that the aptamer@MNP_S could specifically recognizes and binds to *S. aureus*, thereby releasing the FAM-pcDNAs signaling probe for detection. The morphology of streptavidin-MNP_S (Fig. 4a, b) has no significant difference from that of aptamer&pcDNAs@MNP_S (Fig. 4c, d). As shown in Fig. 4e, f, the aptamer@MNPs are obviously bound and aggregated on the surface of approximately spherical *S. aureus* with a diameter of about 0.8 µm by aptamer-specific biorecognition

Fig. 4 a, b SEM image of Streptavidin-MNP_S at different magnifications: $a \times 10,000$, $b \times 50,000$; c, d SEM image of aptamer&pcDNAs@MPN_S at different magnifications: $c \times 10,000$, $d \times 50,000$; e, f SEM image of aptamer&*S.aureus*@ MPN_S at different magnifications: $e \times 10,000$, $f \times 50,000$. The arrow points to the *S. aureus*



element after aptamer&pcDNAs@MNP_S incubated with *S. aureus* (10^8 cfu/mL) at 37 °C for 60 min. The results indicate that the FAM-pcDNAs signaling probe could be replaced and released from aptamer&pcDNAs@MNP_S by *S. aureus*, and the content of the replaced FAM-pcDNAs signaling probe is related to the concentration of *S. aureus*.

The linearity, sensitivity, and selectivity of fluorometric aptasensor

Figure 5a shows the fluorescence emission spectra of the detection supernatant after incubation of aptamer&pcDNAs@MNPs with different concentrations of S. aureus $(1 \sim 10^8 \text{ cfu/mL})$ at 37 °C for 60 min. The fluorescence intensity of the separated supernatant increased with the increase of S. aureus concentration from 1 to 10^8 cfu/ mL. It displays a good linear relationship between the logarithm of the fluorescence intensity and the logarithm of the S. aureus concentration from 1 to 10^8 cfu/mL as shown in Fig. 5b. The linear regression equation could be expressed as logF (a.u.) = $0.22\log C (cfu/mL) + 1.87 (R^2 = 0.99)$. The limit of detection (LOD) and limit of quantification (LOQ) were calculated according to the following equations (Zhou et al. 2017): LOD = $3\sigma/k$ and LOQ = $10\sigma/k$, where $\sigma = 0.0899$ (standard deviation of Tris-HCl solution), k = 0.22 (slope of the calibration curve). Our LOD and LOQ are calculated to be 1.23 cfu/mL and 4.09 cfu/mL, respectively.

The aptamer&pcDNAs@MPN_s were incubated with Tri-HCl (blank) at 37 °C for 60 min to determine whether the FAM-pcDNAs signaling probes would spontaneously detach from the aptamer. The results in Fig. 5c show that the probe FAM-pcDNAs detached hardly from the aptamer spontaneously as the fluorescence intensity of the separated supernatant changed little before and after the reaction between aptamer&pcDNAs@MPNs with Tri-HCl. In order to explore the specificity of the aptasensor, the prepared aptamer&pcDNAs@MPN_S were incubated with E. coli, A. baumannii, E. faecium, P. aeruginosa, P. mirabilis, S. epidermidis, S. pyogenes, S. pneumoniae, and K. pneumoniae at 37 °C for 60 min. As shown in Fig. 5c, the fluorescence intensity of S. aureus (10^4 cfu/mL) is much stronger than that of other bacteria (10⁸ cfu/mL), indicating that there is no non-specific binding between aptamer&pcDNAs@MPNs and other bacteria. The above results showed that the proposed aptasensor owns excellent specificity due to the high specificity of aptamer.

Blood sample analysis

The proposed fluorometric aptasensor was used for the recovery test of blood samples spiked with different concentrations of *S. aureus* from 10^3 to 10^6 cfu/ mL to validate the feasibility of the method. As shown in Table 2, compared



Fig. 5 a The fluorescence emission spectra of the detection supernatant contained FAM-pcDNAs after aptamer&pcDNAs@MPN_S incubation (37 °C, 60 min) with different concentrations of *S. aureus* $(1 \sim 10^8 \text{ cfu/mL})$; **b** the relationship curve between the logarithmic values of fluorescence intensity with the logarithmic values of *S. aureus* concentration $(1 \sim 10^8 \text{ cfu/mL})$; **c** selectivity of the aptasensor toward different bacteria. The concentration of *S. aureus* is 10^4 cfu/mL and the concentration of other bacteria is 10^8 cfu/mL ; error bars indicate standard deviation (n=3)

 Table 2
 Recovery results of the fluorometric aptasensor in blood samples containing *S. aureus* against the plate counting method

Spiked (cfu/mL)	Plate counting method \pm SD (cfu/mL)	Proposed method \pm SD (cfu/mL)	RSD%	Recovery%
1×10^3	$(0.981 \pm 0.054) \times 10^{3}$	$(0.906 \pm 0.068) \times 10^{3}$	7.51	90.6
1×10^4	$(1.023 \pm 0.061) \times 10^{4}$	$(1.062 \pm 0.047) \times 10^{4}$		106.2
1×10^5 1×10^6	$(1.045 \pm 0.048) \times 10^{5}$	$(1.085 \pm 0.059) \times 10^{5}$	5.44	108.5
	$(0.997 \pm 0.071) \times 10^{6}$	$(1.033 \pm 0.062) \times 10^{6}$	6.0	103.3

The standard deviations (SD) of the measurement were calculated from three independent experiments

with the plate counting method, the spiked recovery rate between 90.6% and 116.2% demonstrated the applicability of fluorometric aptasensor for the detection of *S. aureus* in blood samples.

Discussions

The aptamer has higher specificity and affinity, can specifically capture S. aureus and distinguish it from other bacteria, endowing the apatsensor good selectivity. The high sensitivity of aptasensors is usually achieved by using one or more signaling amplification methods (enzyme-catalyzed reactions and/or nanomaterials) (Table 3). However, the wide application of enzyme-catalyzed reactions such as rolling cycle amplification (RCA) (Xu et al. 2018), strand displacement reaction (SDA) (Cai et al. 2020), hybridization Chain reaction (HCR) (Chai et al. 2021), and hairpin DNA cascade hybridization reaction (HD-CHR) (Borum and Jokerst 2021) are limited due to their complex reactions, harsh conditions, and susceptibility to environmental factors. Nanomaterials, as efficient transducers and amplifiers, play an increasingly important role in electrochemical-based aptasensors (such as differential pulse voltammetry (DPV) and electrochemical impedance spectroscopy (EIS)) (Abbaspour et al. 2015; Ranjbar and Shahrokhian 2018), but their stability and reproducibility still need to be improved. Novel optical methods such as surface enhanced Raman scattering (SERS) were also limited by the tedious sample preparation and the expensive equipment required (Liu et al. 2021b). In our research, we design a fluorometric aptasensor with comparable high sensitivity (1.23 cfu/mL) to other conjugated enzymes or/and nanomaterials studies by simply combining the enrichment and separation of MNPs, the biotin-streptavidin conjugation system, and a single *S. aureus* can release four signaling probes. The proposed aptasensor also showed a wide linear range from 1 to 10^8 cfu/mL and fast detection speed (~1.5 h). In the follow-up study, we will explore the use of different fluorescently labeled detection probes to achieve simultaneous detection of multiple pathogens, which is of great significance in practical applications.

To be acknowledged, there are still some limitations need to be addressed when applying the proposed fluorometric aptasensor for real samples analysis. First, the fluorescent molecules (FAM) used in our proposed fluorometric aptasensor are unstable, have low fluorescence intensity, and are prone to photobleaching, so the entire experiment needs to be performed in the dark and is susceptible to interference by autofluorescence or background fluorescence, which is not conducive to practical applications. Compared with traditional organic fluorescent dyes (FAM, fluorescein isothiocyanate, and acridine orange), fluorescent nanomaterials such as quantum dots (QDs) (Fu et al. 2020; Tao et al. 2021), upconversion nanoparticles (UCNPs) (Ouyang et al. 2021a, 2021b) and carbon dots (Cui et al. 2019; Pebdeni et al. 2020) that have emerged in recent years have many advantages, such as wider absorption spectra, size-tunable narrower emission spectra, and better stability, which can be subsequently used to improve the proposed fluorometric aptasensor. Second, although the proposed fluorometric aptasensor achieved good results in buffers (simple components) and good recoveries in blood samples $(10^3 \sim 10^6 \text{ cfu}/$ mL) by optimizing the experimental conditions, the interferences from multiple substances (ions, small molecules, proteins or carbohydrates, etc.) in blood sample requires further optimization to ensure their compatibility in real samples.

Table 3	Performance of
differen	t aptasensor for the
detectio	n of S. <i>aureus</i>

Transducer	LOD (cfu/mL)	Linear range (cfu/mL)	Response time	Reference
Colorimetric	5	$5 \sim 10^4$	~2 h	(Xu et al. 2018)
Fluorometric	1.7	$7 \sim 7 \times 10^7$	~5 h	(Cai et al. 2020)
SERS	1.95	$10 \sim 10^{6}$	>3 h	(Liu et al. 2021b)
DPV	1	$10 \sim 10^{6}$	30 min	(Abbaspour et al. 2015)
EIS	1	$12 \sim 1.2 \times 10^8$	30 min	(Ranjbar and Shahrokhian 2018)
Fluorometric	1.23	$1 \sim 10^8$	~1.5 h	Present work

Third, simultaneous detection of multiple pathogens with the proposed fluorometric aptasensor in real samples still needs to be explored.

In summary, although there are still some challenges to be addressed, the proposed multiple amplification-based fluorometric aptasensor have broad prospects in the construction of practical high-sensitive biosensors for early detection of bacteria due to the easy replacement of aptamers.

Author contribution WC and ZCL conceived and designed research. WC, QTL, and YZL conducted experiments. WC and YKZ analyzed data and wrote the manuscript. All authors read and approved the manuscript.

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Data availability All data generated or analyzed during this study are included in this published article.

Declarations

Ethics approval and consent to participate This work does not involve any human participation nor live animals performed by any of the listed authors.

Conflict of interest The authors declare no competing interests.

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