ORIGINAL ARTICLE

Predicting Fluid Responsiveness in Children Undergoing Cardiac Surgery After Cardiopulmonary Bypass

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Abstract Dynamic parameters of fuid responsiveness (FR), namely aortic blood fow velocity variation (delta V_{peak}), left ventricular velocity-time integral variation (delta VTI), stroke volume variation, and pulse pressure variation (PPV) have demonstrated good diagnostic performance for the prediction of response to fuid loading in mechanically ventilated critically ill adult patients. We aimed to evaluate these parameters in children undergoing cardiac surgery. A retrospective observational study of mechanically ventilated patients weighing less than 20 kg who received a volume expansion (VE) of 10 ml/kg after sternal closure was conducted. A 10% cardiac index (CI) increase divided patients into 7 responders (R) and 9 non-responders (NR). Transesophageal echocardiography and Pressure Recording Analytical Method data were retrieved. The percentage CI increase was 18.6 (12)% in R and 2.9 (5.7)% in NR $(p=0.037)$. Prior to VE, delta V_{peak} , delta VTI, PPV, and SPV difered between R and NR (*p*=0.045, 0.043, 0.048, 0,037 and 0.044, respectively). Systolic $(p=0.004)$, diastolic ($p=0.002$), mean blood pressure ($p=0.003$), delta V_{peak} ($p = 0.03$), delta VTI ($p = 0.04$), CI ($p = 0.01$), PPV $(p=0.04)$, SPV $(p=0.04)$, and dP/dt_{max} (maximal pressure-to-time ratio) $(p=0.02)$ changed the following VE in R patients. Delta V_{peak} decreased after VE in NR patients

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 $(p=0.004)$. Delta VTI and PPV showed the highest predictive values, with area under receiver operator characteristic curves of 0.76 ($p = 0.049$) and 0.76 ($p = 0.045$), respectively. Delta VTI and PPV were revealed to be potential predictors of FR in ventilated children after cardiac surgery. Their combined evaluation could be useful for fuid management after sternal closure.

Keywords Fluid responsiveness · Children · Echocardiography · Cardiac surgery

Introduction

Fluid handling is crucial for oxygen delivery optimization in children with congenital heart malformations after corrective or palliative surgery [\[1](#page-5-0)]. In particular, the evaluation of the adequate amount of fuid for administration is a central issue in neonates and infants afected by LCOS related to cardiopulmonary bypass (CPB). The aim is to minimize the fuid overload and tissue edema that is associated with worse outcomes in these patients [\[2](#page-5-1)].

Several hemodynamic indexes have been investigated as fuid responsiveness (FR) parameters [\[3](#page-5-2)]. A debate regarding the role of dynamic preload indexes (pulse pressure variation (PPV), stroke volume variation (SVV), systolic pressure variation (SPV)), and static parameters (blood pressure, heart rate (HR) central venous pressure (CVP), left atrial pressure) in mechanically ventilated children [[4](#page-5-3)[–6](#page-5-4)] is ongoing. Echocardiographic parameters of FR—namely respiratory variations of aortic blood flow velocity (delta V_{peak}) and aortic velocity-time integral (delta VTI)—have been described as reliable predictors of FR in both adults and children [[4,](#page-5-3) [7](#page-5-5)]. Moreover, a recent meta-analysis confrmed the

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ability of delta V_{peak} to predict the response to volume expansion (VE) in the pediatric population in various clinical settings. However, echocardiography requires expert clinicians to assess delta V_{peak} and its optimal cut-off value differentiating responders (R) and nonresponders (NR) to fuid loading, with exact values yet to be determined [[8\]](#page-5-6).

Powered by the Pressure Recording Analytical Method (PRAM), MostCare™ (Vygon, Vytech, Padova, Italy) is a continuous minimally invasive hemodynamic monitoring system based on arterial waveform pulse contour analysis sampled at a high rate (1000 points per second). PRAM estimates the stroke volume (SV) by analyzing the morphology and the area under the pressure waveform, including the post-dicrotic notch phase, and delivers averaged or beat-by-beat data [\[9\]](#page-5-7). The method also provides dynamic indexes of FR (PPV_{mc}, SPV_{mc} , dicrotic pressure variation, and SVV_{mc}). In addition, PRAM calculates the d*P*/d*t*max (maximal pressureto-time ratio or maximal slope of systolic upstroke (mmHg/ms) between two pressure points). The dP/dt_{max} value depends on both ventricular contractility and vascular impedance (ventriculo-arterial coupling) [\[10\]](#page-5-8).

The aim of our study was to test the ability of the dynamic indexes estimated by PRAM and measured with transesophageal echocardiography (TEE) to predict FR in a cohort of infants undergoing heart surgery with CPB soon after sternal closure.

Patients and Methods

A retrospective study was conducted. Data were retrieved from charts of patients scheduled for elective congenital heart surgery with CPB between February 2016 and May 2016. In our unit, PRAM and TEE monitoring are routinely applied for CPB weaning and the hemodynamic management of intraoperative care [[10](#page-5-8)]. Data were analyzed for patients meeting the following inclusion criteria:

- 1. Weight below 20 kg;
- 2. Biventricular anatomy after surgery;
- 3. Absence of spontaneous breathing;
- 4. Volume expansion of 10 ml/kg of blood products or crystalloids after chest closure, as per the management of clinically suspected hypovolemia in our institution; and
- 5. Recorded TEE measurements and MostCare™ data before and after a VE bolus administered after sternal closure and clearly identifed from clinical charts.

Exclusion Criteria

- 1. Postoperative supraventricular or ventricular arrhythmias;
- 2. Residual left ventricular outfow tract (LVOT) obstruction;
- 3. Moderate or severe valve stenosis or regurgitation;
- 4. Need to change inotrope/vasopressor doses during the study period or severe myocardial dysfunction;
- 5. Presence of arterial waveform artifacts (inappropriate identifcation of dicrotic notch, overdamping or underdamping of the transduced signal);
- 6. Delayed sternal closure;
- 7. Residual intracardiac shunts; and
- 8. Peak inspiratory pressure (PIP) above 30 cmH₂O and positive end expiratory pressure (PEEP) above 10 cmH₂O.

Anesthesia was induced with midazolam (0.1 mg/kg), rocuronium (0.6 mg/kg), and fentanyl (5–10 mcg/kg) and maintained by respective continuous infusions. Mechanical ventilation was set with a tidal volume of 8–10 ml/kg and a respiratory rate (RR) appropriate to age (between 15 and 40 breaths/min). Following the induction of anesthesia, a peripheral arterial catheter (24–22 G) was placed in the left or right radial, humeral, or femoral artery. At the end of anesthesia induction, the MostCare™ monitor retrieved the arterial waveform signal directly from the patient's monitor (Philips MX800) through an analogic output of the pressure transducer. A neonatal (bodyweight \leq 3 kg) or pediatric (bodyweight between 3.5 and 20 kg) echocardiographic transesophageal multiplane probe was inserted and connected to the echocardiography machine (Philips iE33). Using a longitudinal transgastric view at 110–130°, with an angle between the beam and the blood flow always inferior to 20°, pulse-wave Doppler on the LVOT was performed to measure velocity-time integral (VTI) and aortic peak velocity (V_{peak}) . Minimal and maximal values over a single respiratory cycle were recorded.

Demographic data (age, weight, height, diagnosis, type of surgery, hours of mechanical ventilation and ICU stay), mechanical ventilation setting data, and hemodynamic data were retrieved from clinical charts. PRAM data (cardiac index (Cl_{mc}) , SVV_{mc} , PPV_{mc} , SPV_{mc} , dP/dt_{max}) were obtained directly from a device that stores up to 50 patient recordings. TEE data (delta VTI and delta V_{peak}) were retrieved from an institutional database. Delta VTI was calculated as follows: delta VTI = $(VTI_{max} - VTI_{min})$ / $[(VTI_{max} + VTI_{min})/2] \times 100$. In the same way, delta $V_{\text{peak}} = (V_{\text{peakmax}} - V_{\text{peakmin}})/(V_{\text{peakmax}} + V_{\text{peakmin}})/2] \times 100.$

Hemodynamic data were analyzed at two time points following sternal closure: (1) before VE, with stable hemodynamics and controlled bleeding; (2) within 10 min after VE.

The primary objective of the study was to describe the performance of delta V peak, delta VTI, and PRAM dynamic indexes as FR predictors.

Secondary Objectives

- Evaluate static indexes (CVP, HR, invasive blood pressure) as FR predictors;
- Evaluate the modification of each index before and after VE in R and NR; and
- Compare the different behavior of each index between R and NR by comparing parameters collected before and after VE.

Statistical Analysis

Results are expressed as mean values (standard deviation). Unpaired and paired *t* tests were used to compare unmatched or matched data, respectively. Receiver operator characteristic (ROC) curves were generated and the area under each ROC (AUROC) curve was calculated to demonstrate the ability of delta V_{peak} , delta VTI, SVV_{mc}, PPV_{mc} , and SPV_{mc} to predict FR. A logistic multivariable regression was used to combine the best performers and to calculate the cumulative AUROC. A *p*-value ≤ 0.05 was considered statistically signifcant. Statistical analysis was performed using the GraphPad Prism 7.0 software package (GraphPad Software Inc., San Diego, CA, USA).

Results

Overall, 16 patients were enrolled in the analysis. Of these, 7 (44%) showed an increase in CI_{mc} \geq 10% after VE and were defned as R, while 9 (56.25%) showed an increase in CI_{mc} <[1](#page-2-0)0% and were defined as NR to VE. Table 1 describes the demographic characteristics of the included patients. Mean age was 1182 (1681) days in the R group and 371 (414) days in NR $(p=0.18)$. Mean Aristotle score was 7.7 (2) in R and 8.8 (2.2) in NR (*p*=0.3). CPB duration was 153 (67) min in R and 131 (52) min in NR $(p=0.47)$. Vasoactive inotropic score (VIS) was 11.6 (0.8) in R and 14.1 (7.8) in NR (*p*=0.56). Table [2](#page-3-0) describes all the considered hemodynamic variables before and after VE in R and NR patients. VE signifcantly increased systolic $(p=0.004)$, diastolic $(p=0.002)$, and mean blood pressure ($p=0.003$), dP/dt_{max} ($p=0.02$), CI_{mc} ($p=0.01$), and decreased delta V_{peak} ($p=0.03$), delta VTI ($p=0.04$), PPV_{mc} ($p=0.04$), and SPV_{mc} ($p=0.04$) in R. Only delta V peak signifcantly changed after VE in NR (*p* 0.004). The comparison of variables before VE (dP/dt_{max}) , delta V peak,

Table 1 Demographic, baseline, and outcome data	
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Data are expressed as means (standard deviation)

BSA body surface area, *CPB* cardiopulmonary bypass, *XClamp* crossclamp, *Mech Vent* mechanical ventilation, *VIS* vasoactive inotropic score, *PCICU* pediatric cardiac intensive care unit

delta VTI, PPV_{mc} , and SPV_{mc}) showed significant differences between R and NR (*p*=0.045, 0.043, 0.048, 0,037, and 0.044, respectively). After VE, only delta CI_{mc} differed between the two groups $(p=0.049)$ (Table [2\)](#page-3-0). Table [3](#page-3-1) and Fig. [1](#page-3-2) illustrate ROC curves analysis. In our population, FR was not predicted by SVV_{mc} and SPV_{mc} , whereas delta V_{peak} , delta VTI, and PPV_{mc} were able to predict a 10% increase in CI_{mc} after VE. Delta VTI and PPV_{mc} presented the highest predictive values. Delta VTI presented an AUROC of 0.76, a sensitivity of 83%, and a specifcity of 77%, while PPV_{mc} presented an AUROC of 0.76, a sensitivity of 67%, and a specificity of 100% ($p = 0.049$ and 0.045, respectively). The optimal cut-off values were 30% for PPV_{mc} and 16.5% for delta VTI. The combined application of PPV_{mc} and delta VTI significantly improved FR prediction: AUROC 0.83, *p*: 0.03 (Table [3\)](#page-3-1).

Discussion

This study is the frst assessment of FR indexes in a cohort of small children (bodyweight less than 20 kg) undergoing complex heart surgery (mean Aristotle score about 8). The main fndings of our study were as follows:

- I. Respiratory variation in left ventricular outfow tract velocity-time integral (delta VTI) measured with TEE is a sensitive predictor of FR in ventilated children after the correction of congenital heart disease.
- II. Pulse pressure variation (PPV_{mc}) measured using a pulse contour analysis method (PRAM) is a specifc predictor of FR.
- III. The combination of a sensitive and a specifc parameter further improved the accuracy of FR prediction in our cohort.

Table 2 Hemodynamic modifcations in responders and non-responders after fuid challenge

Data are expressed as means (standard deviation)

Statistically signifcant *p* values are highlighted in bold

VE volume expansion, *SAP* systolic arterial pressure, *DAP* diastolic arterial pressure, *MAP* mean arterial pressure, *HR* heart rate, *D* V_{peak} change in the peak velocity of aortic blood flow, *D VTI* change in the velocity-time integral of aortic blood fow, *CI* cardiac index, *D CI* change in the CI after VE, *PPV* pulse pressure variation, *SVV* stroke volume variation, *SPV* systolic pressure variation

 a_p < 0.05 responders before VE versus non-responders before VE

 $\rm{^{b}p}$ < 0.05 responders after VE versus non-responders after VE

Table 3 Area under the curve of receiver–operating characteristic (AUC–ROC) curves

Variables	AUC-ROC (std err) Cut-off		Sensitive- specific $%$ at cut-off	p
PPV	0.76(0.15)	30%	$67 - 100$	0.045
SVV	0.57(0.15)	17%	$100 - 33$	0.63
SPV	0.71(0.14)	11%	$57 - 85$	0.16
DVTI	0.76(0.13)	17%	$83 - 77$	0.049
$D V_{peak}$	0.70(0.14)	16.5%	$83 - 55$	0.19
$DVTI + PPV$	0.83(0.12)			0.03

Statistically signifcant *p* values are highlighted in bold

PPV pulse pressure variation, *SVV* stroke volume variation, *SPV* systolic pressure variation, *D VTI* change in the velocity-time integral of aortic blood flow, $D V_{peak}$ change in the peak velocity of aortic blood $flow$

- IV. Pre-VE absolute values of delta V_{peak} , delta VTI, PPV_{mc} , and SPV_{mc} showed a statistically significant diference between R and NR patients, and these might also be considered for a quick evaluation of FR.
- V. The modifcation of FR parameters after VE (essentially present only in the R group) can be considered as a positive response to fuid administration.

Fig. 1 Receiver operating characteristic curves of examined fuid responsiveness indexes. *PPV* pulse pressure variation, *SVV* stroke volume variation, *SPV* systolic pressure variation, *D VTI* change in the velocity-time integral of aortic blood fow, *D Vpeak* change in the peak velocity of aortic blood fow

FR assessment in critically ill children is currently considered a challenging task. There is certainly a lack of documented information regarding pediatric cardiac surgery patients undergoing correction for congenital heart diseases. Uncertainty regarding the reliability and accuracy of FR predictors has not been clarifed, despite several studies, systematic reviews, and meta-analyses having demonstrated the superiority of dynamic—as opposed to static—parameters for FR prediction [\[4](#page-5-3)[–6](#page-5-4)]. The study of

these parameters is based on the principle of heart–lung interaction in patients under general anesthesia and positive pressure mechanical ventilation. Positive pressure ventilation induces cyclical respiratory variations of systemic venous blood return and, consequently, inspiratory reduction or expiratory increases in left ventricular stroke volume. These variations depend upon the portion of the Frank–Starling curve on which the ventricles are working. They explain whether the patient will be a responder (CI increase after fuid loading) or a non-responder to VE.

Respiratory variation-derived parameters obtained by arterial waveform analysis (SVV, PPV, SPV) or by echocardiographic estimation (delta V_{peak} , delta VTI) have been widely validated as predictive parameters of FR in adult patients in diferent clinical settings [[7\]](#page-5-5). Recently, fuid therapy based on FR parameters in adult patients under general anesthesia showed a decrease in both post-surgical morbidity (infections, cardiac and abdominal complications) and the length of stay in ICU $[11]$ $[11]$.

Currently, there are not enough data to demonstrate the potential positive clinical impact of this advanced hemodynamic monitoring strategy both in optimizing fuid administration in post-cardio-surgical children and in preventing fuid accumulation. In the pediatric population, the main difficulties relate to ventricular systolic and diastolic function, which change markedly from the early neonatal period to the frst year of life [[12\]](#page-5-10). Cardiac function can be affected by the immaturity of neonatal myocardium that has a higher basal contractility, a reduced compliance and a greater sensitivity to changes in HR and afterload [\[13](#page-5-11)]. Furthermore, arterial elastic properties in neonates/ infants signifcantly decrease with age. In this context, we can speculate that SVV or SPV, obtained by pulse contour analysis, may fail to predict FR due to the complex interaction between "immature" myocardium and arterial compliance. Conversely, PPV calculation (the variation in the diference between systolic and diastolic pressures) may be less afected by such issues. However, both peripheral and proximal arterial wall elastance in children decline after birth [[14\]](#page-5-12), suggesting that there is an increase in arterial wall stifness as children grow older. It is possible that neonates have signifcantly diferent FR indexes and cut-ofs to older children, which may explain why the younger patients in our cohort tended to be enrolled in the NR group.

Lung compliance and elastic properties of the chest wall also change with age, leading to surfactant increase, alveolar maturation, improved compliance of lung parenchyma, and modifcation of the chest wall structure (rib ossifcation, diaphragm and abdominal wall tension, intraabdominal pressure) [[15\]](#page-5-13). This is certainly another reason why patients' age can afect dynamic indexes' ability to predict FR. For all these reasons, a minimum tidal volume of 8 ml/ kg is necessary to induce meaningful intrathoracic pressure swings and respiratory variation in LV stroke volume. In our study, to avoid falsely positive FR detection, we hence only included patients ventilated with a mean tidal volume of 8–10 ml/kg, PIP <30 cmH₂O, and PEEP <10 cmH₂O [\[16](#page-6-0)]. In an adult setting, it has also been demonstrated that delta VTI values are less afected by inspiratory tidal volume than are PPV values, and that the transesophageal route is less afected that the transthoracic approach in terms of the respiratory cycle [\[17](#page-6-1)].

Acute changes in afterload and hemodynamic instability can compromise the predictability of FR parameters. According to Desranges and coworkers, the use of inotropes or vasopressors may afect heart–lung interactions and aortic blood flow, altering the ability of delta V_{peak} to predict FR [[8\]](#page-5-6). However, a recent investigation by Pinsky and colleagues showed that both SVV and PPV appear to be unafected by varying doses of vasopressors and inotropic agents for post-cardiac surgery patients [[18\]](#page-6-2). In our population, no signifcant diferences in VIS were found and no change was made to vasopressor or inotrope doses during the study period. Vasoactive drug use in all patients of our population should hence not have afected FR indexes.

Baseline systemic ventricular contractility in cardiac surgery children recently weaned from CPB is another important factor infuencing FR. In a recent study [\[19](#page-6-3)], Saxena and colleagues reported that children with low contractility reach a positive delta SV in response to VE after a signifcantly higher fuid administration compared to patients with normal contractility. As reported elsewhere [\[8](#page-5-6)], we administered a fuid replacement bolus of 10 ml/ kg to all our patients, and it is possible that the amount of fluid administered might alter FR in patients with significantly diferent baseline contractility. Interestingly, in our population, we found a statistically signifcant diference in dP/dt_{max} before VE between R and NR patients and in R patients before and after VE. We speculated that FR patients with low contractility improved cardiac function after volume loading. In this context, dP/dt_{max} , integrated into a panel of hemodynamic data, may provide information that further assists clinicians in handling fuids and inotropes–vasopressors [[20\]](#page-6-4).

Limitations

The present study had several limitations. First, the cohort was small and heterogeneous involving diferent diagnoses and procedures. We limited enrollment to patients with biventricular anatomy weighing less than 20 Kg in order to include only neonates and patients below 2 years old—an original population by the standards of current literature. We specifcally wanted to extend Choi and coworkers' [[21](#page-6-5)] observation regarding FR prediction in cardiac surgery patients. In their preliminary study, only simple surgical procedures were included (ventricular septal defect correction), and we aimed to show that FR can be evaluated in diferent biventricular anatomies. Second, PRAM is not a validated technique for CI monitoring in the pediatric setting [[10](#page-5-8)]. However, our group make extensive use of it on a routine basis, and dynamic indexes are not subject to algorithm errors. Third, overor underdamping artifacts of the transduced signal can compromise the reliability of all the derived parameters. Even if we routinely check and carefully prevent waveform artifacts to alter hemodynamic monitoring, these may sometimes be difficult to identify or correct. Some of the enrolled patients' measurements may therefore have been affected by such bias (which is difficult to verify retrospectively) [\[22\]](#page-6-6). Nevertheless, we decided to use CI_{mc} to distinguish R from NR patients instead of TEE stroke volume measurement to avoid a potential source of bias being VTI, V_{peak} , and SV estimated by echo (LVOT area \times LVOT-VTI), as these are mathematically coupled [\[8\]](#page-5-6). Furthermore, our intention was to reduce intra- and inter-observer variability and echocardiographic measurement errors among clinicians dedicated to data collection. Finally, we decided to use an increase of 10% from the pre-VE value as a FR CI_{mc} cut-off, whereas other authors have used 15%. According to institutional protocol, however, we administer relatively low-volume boluses to our patients when fuid replacement is indicated. This is mainly due to patients' relatively limited tolerance to greater fuid boluses that, as discussed above, may not be able to increase CI above the threshold of 10%. Finally, no unequivocal cut-off for CI increase to defne FR has been recommended in the literature to date.

Conclusions

Echocardiographic dynamic indexes (delta VTI) and PPV measured by MostCare™ have revealed themselves to be reliable predictors of FR in ventilated children after correction of cardiac malformations with CPB. Integrated multiinstrumental and multi-parametric hemodynamic monitoring combining echocardiographic measurement and pulse contour analysis may be helpful in achieving a high predictive performance for these variables.

Compliance with Ethical Standards

Confict of interest All authors declare that they have no fnancial or non-fnancial confict of interest.

Informed Consent Formal consent is not required because we conducted a retrospective study.

Research Involving Human and Animal Participants All procedures performed in this study were in accordance with the ethical standards of the institutional and/or national research committee and with the 1964 Helsinki declaration and its later amendments or comparable ethical standards. This article does not contain any studies with animals performed by any of the authors.

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