

Efficient In Vitro Electropermeabilization of Reconstructed Human Dermal Tissue

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Abstract DNA electrotransfer is a successful technic for gene delivery. However, its use in clinical applications is limited since little is known about the mechanisms governing DNA electrotransfer in the complex environment occurring in a tissue. The objectives of this work were to investigate the role of the extracellular matrix (ECM) in that process. Tumor ECM composition was shown to modulate in vivo gene electrotransfer efficiency. In order to assess the effects of ECM composition and organization, as well as intercellular junctions and communication, in normal tissue response to electric pulses, we developed an innovative three-dimensional (3D) reconstructed human connective tissue model. 3D human dermal tissue was reconstructed in vitro by a tissue engineering approach and was representative of in vivo cell organization since cell– cell contacts were present as well as complex ECM. This human cell model presented multiple layers of primary dermal fibroblasts embedded in a native, collagen-rich ECM. This dermal tissue could become a useful tool to study skin DNA electrotransfer mechanisms. As proof of the concept, we show here that the cells within this standardized 3D tissue can be efficiently electropermeabilized by milliseconds electric pulses. We believe that a better comprehension of gene electrotransfer in such a model tissue would help improve electrogene therapy approaches

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such as the systemic delivery of therapeutic proteins and DNA vaccination.

Keywords Tissue engineering · Electroporation · Gene electrotransfer - Connective tissue - 3D architecture

Introduction

The clinical development of gene therapy requires the use of safe and efficient methods to deliver therapeutic genes to the targeted cell. Contrary to viral vectors, plasmid DNA vectors offer many advantages. They are safer than viral vectors, cheaper and easier to mass-produce, they have a high DNA content, and their administration can be repeated since they are non-immunogenic (Pfutzner [2010\)](#page-5-0). However, their major disadvantage is their low effectiveness in vivo. Indeed, plasmid DNA vectors have to overcome several obstacles, namely, DNA diffusion through the extracellular matrix (ECM), uptake across the plasma membrane, intracellular migration to the nucleus, and through the nuclear envelope (Escoffre et al. [2010](#page-4-0)).

Physical techniques such as electroporation have been developed to improve the in vivo transfection rate and are now accepted in clinics. The method relies on the application of electric pulses to induce transient and localized cell permeabilization, a process that allows naked plasmid DNA uptake into cells (Neumann and Rosenheck [1972](#page-5-0); Neumann et al. [1982\)](#page-5-0). Thanks to electrogene transfer, safe local delivery can be achieved. A wide range of soft and hard tissues have already been successfully transfected using this method including skin, liver, muscle, joints, lung, spleen, brain, eyes, and tumors (Mir et al. [2005](#page-5-0)).

Electrogene transfer in skin, which is an easy organ to treat, allows multiple therapeutic approaches to be considered such as systemic delivery of therapeutic proteins and DNA vaccination (Rochard et al. [2011](#page-5-0); Vandermeulen et al. [2007](#page-5-0)). Indeed, human skin is largely microvascularized, allowing transfected cells to systemically secrete therapeutic proteins. Furthermore, skin contains a numerous antigen-presenting cells, allowing a strong immune response after DNA vaccination. Thus, the first published phase I study on metastatic melanoma found that IL-12 electrogene transfer led to tumor necrosis and regression of untreated distant metastases (Daud et al. [2008\)](#page-4-0).

In order to improve in vivo electrogene transfer efficacy in human skin and thus to develop clinical applications, we have to have a better understanding of the gene transfer mechanisms in a tissue context. A lot of in vitro studies performed on cells in culture have been used in an attempt to optimize the electrical parameters and thus to apply this technique in clinics. However, even though they are useful, none of these studies were able to access the complexity of in vivo tissues. Accumulating evidence underlines that three-dimensional (3D) cell models are superior to classical 2D cell culture to mimic and predict in vivo situations (Ghajar and Bissell [2010;](#page-4-0) Nyga et al. [2011;](#page-5-0) Pampaloni et al. [2007\)](#page-5-0).

This is why we and others have developed 3D cell culture models to study gene electrotransfer in vitro in a 3D context. The most common model, named the spheroid, is a 3D cellular model devoid of any exogenous material (Sutherland [1988](#page-5-0)). Even though mRNA for ECM components such as collagens, laminin, fibronectin, and glycosaminoglycans were found in spheroids, the model is especially relevant for intercellular junctions in a tumor context (Kunz-Schughart et al. [2006;](#page-4-0) Nederman et al. [1984;](#page-5-0) Stevens et al. [2009\)](#page-5-0). We previously demonstrated that although the electrotransfection rate reached values higher than 25 % for cells in suspension, the transfection rate of cells in spheroids hardly reached 1 % under the same electrical conditions (Chopinet et al. [2012\)](#page-4-0), a value which is close to in vivo tumor transfection rates (Rols et al. [1998\)](#page-5-0). Mellor and coll showed that transfected cells were only located on the outer layers of the spheroid, in direct contact with plasmid DNA (Mellor et al. [2006](#page-4-0)). Similarly, we noted that reporter gene expression was only detected in one cap of the spheroid, the one facing the negative electrode, which is direct evidence for the involvement of electrophoretic forces in DNA electrotransfer (Wasungu et al. [2009](#page-5-0)) and is in agreement with the in vitro process (Golzio et al. [2002](#page-4-0); Paganin-Gioanni et al. [2011](#page-5-0)). Interestingly, in another 3D cellular model, Haberl et al. confirmed that electrogene transfer within hamster cells dispersed in a type I collagen from rat tail gel was comparable to in vivo studies and depended on plasmid DNA concentration and pulse duration (Haberl and Pavlin [2010](#page-4-0)).

Thus, close contacts between cells and ECM deposition may act as a physical barrier that limits/prevents uniform DNA distribution and could explain the low gene electrotransfer efficiency in tissue.

Skin dermis is a connective tissue characterized by abundant ECM primarily synthesized by fibroblasts (Prost-Squarcioni et al. [2008\)](#page-5-0). Dermis ECM is composed of collagen and elastic fibers providing tissue resistance to tensile forces and the amorphous ground substance, allowing the flow of water and dissolved molecules. In order to study gene electrotransfer mechanisms in skin, we developed here an innovative in vitro 3D human model of normal dermal tissue, where primary dermal fibroblasts produce their own, complex physiological ECM.

Materials and Methods

Cell Culture

Primary human dermal fibroblasts were isolated from human foreskin biopsy after posthectomy as previously described (Gibot et al. [2010\)](#page-4-0). The cells were grown in Dulbecco's Modified Eagles Medium (Gibco-Invitrogen, Carlsbad, USA) containing 4.5 g/L glucose, L-glutamine, and pyruvate, supplemented with 10% (v/v) of heatinactivated fetal calf serum, 100 U/ml penicillin, and 100 μ g/ml streptomycin. Cells were maintained at 37 °C in a humidified atmosphere containing 5% CO₂.

Reconstruction of a Human 3D Dermal Tissue

The self-assembly approach (Auger et al. [2002](#page-4-0)) was used to produce human 3D dermal tissue in vitro. Schematically, primary human dermal fibroblasts were cultivated for 3 weeks in cell culture medium supplemented with $50 \mu g$ / mL of ascorbic acid (Sigma) as previously described (Gibot et al. [2010,](#page-4-0) [2013](#page-4-0)). Indeed, ascorbic acid is well known to improve collagen production, secretion, and maturation (Lyons and Schwarz [1984](#page-4-0); Schwarz [1985\)](#page-5-0). After 3 weeks, cells secreted enough ECM to form a cell sheet that was easy to manipulate. Since the cells used to produce the sheet are dermal fibroblasts, ECM is comparable to that found in the dermis compartment of the skin.

Histological Analysis

After fixation in formalin (Sigma-Aldrich) at room temperature for 1 h, transversal sections of cell sheet were embedded in paraffin for staining with Masson's trichrome (Sigma-Aldrich). The Masson's trichrome method stains cells red and collagens within the dermal tissue in blue (Masson [1929\)](#page-4-0).

Transmission and Scanning Electron Microscopy

For transmission electron microscopy, cell sheets were fixed in 2 % glutaraldehyde in 0.1 M Sorensen phosphate buffer (pH 7.4) for 4 h at 4 \degree C, washed overnight in 0.2 M phosphate buffer, and then post-fixed for 1 h at room temperature with 1 % osmium tetroxide in 250 mM saccharose and 0.05 M phosphate buffer. They were stained overnight in 2 % uranyl acetate. The samples were then dehydrated in a series of graded ethanol solutions and embedded in an Epon–araldite resin (Embed 812-Araldite 502, Electron Microscopy Sciences). Finally, ultra-thin sections stained with uranyl acetate were observed under a transmission electron microscope (Hitachi HU12A electron microscope). For scanning electron microscopy, cell sheets were fixed in 2 % glutaraldehyde in 0.1 M sodium cacodylate buffer for 4 h at 4° C. After two washes in the same buffer, the cell sheets were dehydrated in a graded ethanol series, dried by critical point drying with EMSCOPE CPD 750, coated with gold–palladium for 5 min at 100 \AA min⁻¹, and then observed with a S450 scanning electron microscope (Hitachi).

Collagens Detection by Second Harmonic Generation

Three dimensional stacks of $425 \times 425 \times 60 \mu m$ were acquired using a 7MP multiphoton laser scanning microscope (Carl Zeiss S.A.S., Jena, Germany), equipped with a $20 \times$ objective (NA 0.95) and coupled to a Ti-Sapphire femtosecond laser, Chameleon Ultra 2 (Coherent Inc) tuned to 800 nm. Organized fibrillar collagens were detected by second harmonic generation (SHG) at a wavelength of 400 nm. The acquired 3D images were stored and then analyzed off-line with Imaris software (Bitplane AG).

Electropermeabilization of 3D Human Dermal **Tissue**

Two flat parallel stainless steel electrodes (1 cm length, 1 cm width) were placed on the top of cell sheets and immersed in pulsing buffer (10 mM K_2HPO_4/KH_2PO_4 buffer, 1 mM $MgCl₂$, 250 mM sucrose, pH 7.4) containing $100 \mu M$ propidium iodide (PI) (Sigma-Aldrich). Electropulsation used an electro cell S20 generator (β Tech, Toulouse, France) which delivered square-wave electric pulses. An oscilloscope (Enertec, St. Etienne, France) was used to monitor pulse shape. The electrical conditions were as follows: eight pulses lasting 5 ms at a frequency of 1 Hz were applied from 0 to 600 V/cm at room temperature. Cell membrane permeabilization was assessed by multiphoton laser scanning microscopy on living tissues. An isosurface was made with Imaris software to visualize and isolate the permeabilized cells.

Results

Reconstruction of Human 3D Dermal Tissue Rich in Organized Collagens

In the first step, we visualized and characterized the ECM secreted by primary human dermal fibroblasts within our in vitro 3D reconstructed dermal tissue model. For this purpose, we identified collagens by different and complementary imaging tools. Primary human dermal fibroblasts cultured by the self-assembly approach are able to reproduce a physiological environment within 3 weeks, by secreting and organizing a dense 3D ECM rich in collagens (Fig. [1\)](#page-3-0). Dermal tissue cross sections showed several layers of fibroblasts embedded in a 3D ECM rich in collagens (Fig. [1a](#page-3-0)). Both scanning and transmission electron microscopy showed intact, organized collagen fibrils within our dermal tissue model (Fig. [1b](#page-3-0), c). Longitudinal sections of collagen fibrils showed the typical striation brought about by the arrangement of tropocollagen (Fig. [1](#page-3-0)d). In addition, multiphoton imaging allowed non-invasive highresolution in vitro, in situ imaging of organized ECM structures and cells in living intact tissue-engineered models. Thus, abundant organized collagens fibrils were distinctly observed by SHG (Fig. [1](#page-3-0)e).

Cells were Efficiently Electropermeabilized Within 3D Reconstructed Dermal Tissue

To study the effect of electrical pulse parameters (i.e., millisecond electric pulses) currently used for gene electrotransfer, the permeabilization state of cells within 3D human dermal tissue was assessed using PI penetration. Permeabilization was followed on live human dermal tissue by multiphoton imaging (Fig. [2](#page-4-0)). Biphoton microscopy allowed observation of the entire thickness of the fresh tissue. For the control, dermal tissues were incubated with PI without any electrical pulses. We only observed a few permeabilized cells, corresponding to dead cells (Fig. [2a](#page-4-0)). Indeed, there is some cell renewal in our model, and dead cells are trapped within the tissue. For the electropulsed condition, by increasing electric field intensity, we observed that cells could be gradually permeabilized (Fig. [2b](#page-4-0)–d). These experiments showed that electric pulse intensities between 300 V/cm and 600 V/cm led to an efficient and homogeneous permeabilization of the cells. Thus, using the gene electrotransfer electrical parameters (i.e., millisecond pulses), we are able to efficiently

Fig. 1 Human 3D dermal tissue characterization. a Cell sheet cross section stained with Masson's trichrome. Cells are red and collagens are blue. b Scanning electron microscopy showing fibroblast cells and extracellular matrix. c Transmission electron microscopy of cell sheet. Arrows indicate collagen fiber cross sections. d Transmission

electropermeabilize all the cells contained in the model tissue whatever their location in the cell sheet.

Discussion

In this study, we used a tissue engineering approach to in vitro reconstruction of human 3D dermal tissue rich in organized collagens. Indeed, primary human dermal fibroblasts cultured by the self-assembly approach reproduce a physiological environment within 3 weeks, by secreting and organizing a dense 3D ECM containing collagens and elastin, with characteristics similar to those observed in vivo (Pouliot et al. [2002\)](#page-5-0), (L'Heureux et al. [1998](#page-4-0)). Using self-assembly approach, we are able to produce in a reproducible manner several tens of sheets of 50 μ m average thickness. The production cost is less than 5ϵ for each cell sheet, which is dramatically cheaper than using rat tail collagen gel to mimic dermis compartment. The major limitation of self-assembly approach can be the time necessary for cells to produce handleable cell sheet, i.e., approximately 3 weeks, which can be overcome by a good logistical organization.

electron microscopy of cell sheet. Arrows indicate longitudinal section of collagen bundles. e Organized fibrillar collagens within cell sheet produce second harmonic generation signal (Color figure online)

To our knowledge, we are the first to implement and use these easily handleable cell sheets to study gene electrotransfer in tissue. We showed that using millisecond electric pulses, cells deep within the tissue were efficiently electropermeabilized.

After this proof of concept, we hope that our innovative model will be a valuable tool to assess the role of ECM secretion and organization, as well as intercellular junction and communication, in tissue responses to electric pulses. Indeed, it has already been proven in vivo that electric fields improve plasmid transport via electrophoresis across extracellular medium (Henshaw and Yuan [2008\)](#page-4-0). However, electrophoretic transport of plasmid DNA is inversely correlated with collagen content in solid tissues (Zaharoff et al. [2002\)](#page-5-0). Soft tumors containing few proteoglycans and collagens were found in vivo to be more efficiently electrotransfected with plasmid DNA than solid tumors with rich ECM (Mesojednik et al. [2007\)](#page-5-0). The underlying mechanism seems to be that collagen influences tumor tissue resistance to macromolecule transport by binding and stabilizing glycosaminoglycans (Netti et al. [2000](#page-5-0)). These in vivo studies were performed on mice and provided access to gene delivery in tissue, but mouse skin is

Fig. 2 3D dermal tissue electropermeabilization. Reconstructed human dermal tissue was electropermeabilized in the presence of propidium iodide (red) with the following electrical parameters: 8 pulses of 5 ms duration at 1 Hz. Electric field intensity was 0 V/cm (a), 200 V/cm (b), 300 V/cm (c), 400 V/cm (d), 500 V/cm (e), 600 V/cm (f) and observed under a fluorescent biphoton microscope. Collagens are blue (Color figure online)

very different from human skin (Pasparakis et al. [2014](#page-5-0)). Furthermore, most of these studies were performed in a tumor context. We think that a better understanding of the role of ECM in gene electrotransfer in a healthy human 3Drelevant context will help improve gene therapy and DNA vaccination efficiency.

In addition, tissue engineering approaches to reconstructing normal human tissue lends itself to the philosophy of the 4R's that promotes reliable alternatives to animal experiments in an attempt to reduce the numbers of animals used (responsibility, refining, replacement, and reduction). The simplicity of in vitro testing on reconstructed human dermal tissue will allow better development and adjustment of gene electrotransfer conditions in terms of plasmid DNA concentration and electrical parameters. With the development of dermal models reconstructed directly from patient cells, this technique could hold promise for the

development of patient-adjusted gene therapy, i.e., personalized medicine. It will become possible to evaluate and then adapt the electric field pulse parameters (pulse number, amplitude, and width) far beyond what can be done in animal studies.

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