#### **KNEE**

# The posterior cruciate ligament: a study on its bony and soft tissue anatomy using novel 3D CT technology

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#### Abstract

*Purpose* The bony insertion sites of the PCL have been studied and described extensively using 2D technology such as macroscopic images, plain radiograph, computerized tomography (CT) and MRI. The purpose of this study is to visualize both the tibial and the femoral bony insertion sites but also the soft tissue anatomy of the native PCL using novel 3D CT imaging. In addition, new concepts of best-fit cylinder and central axis are introduced and evaluated.

*Methods* Nine unpaired knees of embalmed cadavers were used in this study. Following the dissection process, the PCL was injected with a contrast medium for computed tomography (CT) imaging. The obtained CT images were segmented and rendered in 3D allowing morphological and morphometric analysis of PCL. Femoral and tibial footprint surface area, best-fit PCL-cylinder intersection area, bestfit PCL-cylinder/footprint coverage ratio, best-fit PCLcylinder central axis projections at the tibial and femoral footprint were used to describe the anatomy of the PCL.

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P. C. M. Verdonk (⊠) Department of Orthopaedic Surgery, Monica Hospitals, Harmoniestraat 68, 2018 Antwerpen, Belgium e-mail: pverdonk@yahoo.com *Results* Mean footprint surface area of the tibial and femoral footprint were 189.1 and 293.3 mm<sup>2</sup>, respectively. The mean diameter of the best-fit cylinder was 10.5 mm. The mean coverage of the best-fit cylinder on the tibial and femoral footprint was 76.5 and 46.5, respectively. The best-fit cylinder central axis was located in the anterolateral AL bundle footprint on the femur and more centrally in the PCL footprint on the tibia.

*Conclusion* This study is the first to describe the detailed anatomy of the human PCL with respect to its course and footprints using a 3D approach. It confirms the large difference between the tibial and the femoral footprint area with the former being significantly smaller. In addition, a large inter-patient variability is observed. The best-fit cylinder and central axis concept offer additional insights into the optimal tunnel placement at the tibia and femoral footprint in order to cover the largest portion of the native PCL soft tissue.

**Keywords** Posterior cruciate ligament · 3D-computerized tomography · Anatomy

## Introduction

The strongest ligament in the knee, the posterior cruciate ligament (PCL), arises from the medial aspect of the medial femoral condyle and inserts posterior to the intercondylar eminence of the tibia.

The insertion sites of the PCL have been studied and described extensively using 2D technology such as macroscopic images, plain radiograph, computerized tomography (CT) and MRI [1, 3, 5, 7, 9, 15, 19–21].

Recently, 3D imaging and segmentation technology has been introduced into the orthopaedic field to improve the comprehension of the complex *osseous* anatomy of the human knee. Such information has led to the better understanding of the bony insertion sites of the native cruciate ligament and has been translated recently into the clinical practice as the anatomical ligament reconstruction concept. The definition of anatomical ligament reconstruction only includes bony references such as the following: a centre-tibial footprint to centre-femoral footprint tunnel position and at least 80 % footprint coverage. This concept, however, does not take into account soft tissue references such as the course and volume of the native ligament, as 3D visualization of *soft tissue* anatomical structures such as the PCL has not yet been performed using CT images [2, 14].

The purpose of this study is to visualize both the tibial and femoral bony insertion sites but also the soft tissue anatomy of the native PCL using novel 3D CT imaging. In addition, new concepts of best-fit cylinder and central axis are introduced and evaluated. The central axis represents the best-fit cylinder around the native PCL fibres as determined by an automated computerized process. The central axis bony insertion therefore depicts the ideal tunnel position to enclose the bulk of the PCL fibres. This information can be useful for ligament reconstructive purposes [2, 8, 11, 12, 16, 18, 23, 24].

## Materials and methods

Nine unpaired knees of embalmed cadavers (four from male cadavers and five from female cadavers) with no macroscopic degenerative or traumatic changes were used in this study. The mean age of the cadavers, at the time of death, was 79.4 years (range, 66–97 years).

#### Procedure

The knees were carefully dissected through anterior and posterior approach. For anterior approach, the knee was positioned in 90° of flexion and the patellar ligament was sectioned transversely at the level of the joint space. The infrapatellar fat tissue and the synovial sleeve embedding the PCL were carefully removed.

For the posterior approach, the knee was fully extended. In the popliteal fossa, the heads of the gastrocnemius muscles, the tendon of the semimembranosus muscle and deep popliteal neurovascular bundle were excised to the level of the oblique and the arcuate popliteal ligament and the popliteus muscle. The popliteal tendon was transected at its most lateral visible part where it disappears under the edge of the capsule. From this transection point, the posterior capsule was transversely opened until the tibial and femoral insertion sites of the PCL were clearly visible and accessible. The synovial sleeve was removed, and the posterior meniscofemoral ligament was kept intact. The anterior approach, craniomedially to the ACL, was integrated in the anatomical procedure for optimal accessibility of the femoral insertion site of the PCL. The dissection procedure (anterior and posterior approach) was performed with the preservation of the lateral and medial parts of the capsule in the manner that rotational stability was maintained in positioning the knee during CT scanning.

Following the dissection process, the PCL was injected with a contrast medium for computed tomography (CT) imaging, consisting of 80 % Barium sulphate, 10 % glycerine, 10 % water. Toluidine blue powder (0.1 g) was added to stain the solution which allows a visual control over dispersion and possible leakage of the mixture [6, 17, 22]. A needle (Terumo<sup>®</sup> needle  $0.45 \times 23$  mm) was inserted between the collagen fibres of the PCL, and the solution was injected with mild pressure until leakage occurred at the injection site or at spots further away along the ligament. Pieces of gauze swabs were wrapped around neighbouring structures and surfaces in order to prevent contamination of possible leaking contrast solution [4].

The injection needle subsequently was directed towards the femoral and tibial insertion site of the PCL as far as the contact point with the bony surface [7, 19]. On this spot, a small bolus of contrast was injected and this was repeated covering the complete insertion area. Then, a solid dissection needle—with identical diameter as the injection needle—was used for repeated pricking in this area to obtain maximal absorption of contrast solution in the bony PCL insertion area (footprint).

Additionally, the accessible exterior parts of the PCL were covered with an ethyl-acetate based solution containing lead dioxide to enhance surface contrast [7, 10, 22].

## CT scanning

After anatomical preparation, the specimens were studied by a helical CT scan (Siemens/volume zoom). The obtained CT images were then imported into a software package that is able to process any 2D stack of images (e.g., CT and MRI) and allows 3D reconstruction. In the present study, Mimics 14.11<sup>®</sup> (Materialise N.V., Heverlee, Belgium) was used for visualization and segmentation of CT images and 3D rendering of the knee joint with and PCL with a direct link to morphological and morphometric analysis of PCL and PCL reconstruction procedures [22].

#### Measurements

After the segmentation process, 3D reconstructions were calculated from the selected masks of the native PCL (Fig. 1), the distal part of the femoral shaft with the





condyles and the tibial plateau to a few centimetres distal from the tibial tuberosity.

Femoral and tibial footprint surface area, best-fit PCLcylinder intersection area, best-fit PCL-cylinder/footprint coverage ratio (Table 1) and best-fit PCL-cylinder central axis projections at the tibial (Fig. 2) and femoral (Fig. 3) footprint were used to describe the anatomy of the PCL.

#### Data analysis

Mean (SD) surface areas (mm<sup>2</sup>  $\pm$  1 SD) were calculated for the tibial and femoral native PCL insertion site. Then, the mean intersection areas (mm<sup>2</sup>  $\pm$  1 SD) of the best-fitted PCL-cylinder with the tibial and femoral footprint surfaces were calculated and expressed as a mean coverage (%  $\pm$  1 SD) in relation to the complete footprint areas.

**Table 1** Overview of the individual tibial and femoral footprint surface areas, the individual coverage of the best-fit cylinder on the tibial and femoral footprints in terms of percentage, the diameter of the best-fit cylinder and the femoral epicondylar width for each of the nine knees used

	Tib sfc (mm <sup>2</sup> )	Fem sfc (mm <sup>2</sup> )	Tib cov (%)	Fem cov (%)	Diameter (mm)	Fem epw (mm)
Knee 1	263.4	302.1	84.5	38.5	10.8	86.9
Knee 2	190.6	270.7	66.0	54.0	9.7	89.1
Knee 3	257.6	400.5	59.6	47.2	11.9	87.0
Knee 4	68.7	193.7	91.4	37.1	7.5	76.6
Knee 5	186.6	216.2	74.4	48.5	11.0	79.3
Knee 6	115.2	259.6	91.4	50.2	10.1	85.2
Knee 7	191.0	326.6	67.2	48.0	10.6	81.7
Knee 8	202.2	348.4	84.1	54.0	11.6	85.0
Knee 9	226.2	321.7	69.9	40.7	11.1	86.0
Mean	189.1	293.3	76.5	46.5	10.5	84.1

*Tib Sfc* tibial footprint surface area, *Fem Sfc* femoral footprint surface area, *Tib Cov* tibial coverage, *Fem Cov* femoral coverage, *Diameter* diameter of the best-fit cylinder, *Fem Epw* femoral epicondylar width. The data has a normal distribution; Shapiro–Wilk (*p* value n.s.)

The areas of the femoral and tibial footprints and native PCL diameter were compared to the femoral epicondylar mediolateral width, using a Spearman's rank correlation coefficient. The level of significance was set at p < 0.05.

## Results

Based on anatomical dissection, interpretation of specific collagen tissue contrasted CT, 3D reconstructions of the native PCL, tibial plateau and intersection area, we found that the posterior cruciate ligament was attached to the posterior intercondylar area between the tibial plateaus and posteriorly of the intercondylar eminences.

In line with the topographical studies of Forsythe et al. [7] and Tajima et al. [19], we also found the PCL consisting of two bundles inserting in different planes on the posterior intercondylar area. In almost every 3D native PCL, the anterolateral (AL) and posteromedial (PM) bundle is clearly detectable. Two slopes can be identified on tibial insertion area of the PCL: (1) an anterolateral slope, located at the superolateral aspect of the posterior intercondylar area, to which the AL bundle is attached; (2) a posteromedial slope in the inferomedial aspect of the fossa, which is the insertion area for the PM bundle [1, 5, 11, 13, 19].

In cranial direction, the PCL inserts on the lateral surface of the medial femoral condyle in the intercondylar fossa. This insertion area is bounded caudally by the rim of the articular surface of the medial condyle and cranially by the medial intercondylar ridge depicted in most knee samples. The medial bifurcate ridge, described in Forsythe et al. [7] as a small osseous prominence between the anterolateral and posteromedial bundles of the PCL, was not visible on the bony surfaces of the CT datasets and 3D reconstructions in the current study. On the other hand, it was possible to distinguish the anterolateral and posteromedial bundles in the 3D native PCL at the femoral insertion site [1–3, 5, 11, 13, 15, 19, 20]. **Fig. 2** Three-dimensional representation of the tibial footprint of the native PCL (*red*) for the nine knees used (**a–i**). In *blue colour*, the intersection area of the best-fit PCL-cylinder superimposed on the tibial footprint (*red*), and in *yellow colour*, the osseous intersection of the central axis superimposed on preceding footprint and intersection area (*red* and *blue*)

Fig. 3 Three-dimensional representation of the femoral footprint of the native PCL (*red*) for the nine knees used (**a**–**i**). In *blue colour*, the intersection area of the best-fit PCL-cylinder superimposed on the femoral footprint (*red*), and in *yellow colour*, the osseous intersection of the central axis superimposed on preceding footprint and intersection area (*red* and *blue*)



## Measurement of PCL footprint

Mean footprint surface area of the tibial and femoral footprint were 189.1 mm<sup>2</sup> (SD  $\pm$  63.0, range 68.6–263.4) and 293.3 mm<sup>2</sup> (SD  $\pm$  65.2, range 193.7–400.5), respectively. A high inter-patient variability was observed. No significant correlations were found between the femoral and the tibial footprint areas, the diameter of the native PCL in comparison with the femoral epicondylar width.

Spearman's rank correlation coefficient for the femoral footprint was 0.45 (n.s.); for the tibial footprint, 0.6 (n.s.); and for the native PCL diameter, 0.23 (n.s.).

Fitting of cylinders through the PCL

The mean diameter of the best-fit cylinder was 10.5 mm  $\pm$  1.299. The mean coverage of the best-fit cylinder on the tibial and femoral footprint was 76.5  $\pm$  11.7

and  $46.5 \pm 6.3$  %, respectively. The best-fit cylinder central axis was located in the AL bundle footprint on the femur and more centrally in the PCL footprint on the tibia.

#### Discussion

This study is the first to describe the detailed anatomy of the human PCL with respect to its course and footprints using a direct contrast-enhanced visualization methodology based on CT imaging in combination with a 3D approach. This unique approach offers valuable information on the bony insertion site but also offers new insights into optimal tunnel placement based on the new concept of best-fit tunnel and central axis. The latter technology is only possible through soft tissue visualization and allows maximum ligament soft tissue coverage in contrast to the mid-footprint anatomical approach which allows maximum bony footprint coverage. However, maximum footprint coverage does not necessarily encompass maximum soft tissue coverage. It is well known that the anterolateral bundle of the PCL is both functionally and anatomically more important [3]. A mid-footprint approach, however, will only incorporate equal parts of the AL and PM bundle and therefore underestimate the importance of the AL bundle [1-3, 5, 11, 13, 20]. In contrast, the best-fit cylinder approach would suggest a more balanced evaluation as it is not based on the mid-position of the footprints but rather on the bulk of the soft tissues of the PCL. Thus, since the bulk tissue of the AL bundle is larger than the PM bundle, the best-fit cylinder central axis will be closer to the AL bundle. This is confirmed by the observations made in this study. Nevertheless, while a mean best-fit cylinder of 10 mm diameter will cover almost 80 % of the tibial footprint, it will only cover 50 % of the femoral footprint. This observation suggests that single-bundle PCL reconstruction is never able to be considered anatomical on the femoral side [2, 8, 11, 12, 16, 18, 23, 24]. In addition, increasing the diameter of the PCL-cylinder in order to increase femoral footprint coverage would probably result in overstuffing the soft tissue compartment of the PCL and would result in impingement with the ACL.

This study also confirms the large difference between the tibial and the femoral footprint area with the former being significantly smaller. Nevertheless, the anatomy of the tibial footprint was characterized in all cases by 2 different planes. In contrast to a number of studies, we, however, were unable to discern the medial bifurcate ridge on the femur in between the AL and the PM bundle [7, 8]. In addition, a large inter-patient variability concerning footprint area is observed. Although most anatomical studies are limited by a low number of samples and thus low generalizability of these observations, such high variability should be incorporated into the treatment algorithm of PCL reconstruction as it can influence the graft choice and graft diameter [1, 5, 9, 20].

## Conclusion

This study is the first to describe the detailed anatomy of the human PCL with respect to its course and footprints using a 3D approach. It confirms the large difference between the tibial and the femoral footprint area with the former being significantly smaller. In addition, a large inter-patient variability is observed. The best-fit cylinder and central axis concept offers additional insights to develop improved techniques for restoring the function of the native PCL.

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